

# Electromagnetic fields counteract IL-1 $\beta$ activity during chondrogenesis of bovine mesenchymal stem cells

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## Abstract

Osteoarthritis (OA) is a common joint disease associated with articular cartilage degeneration. To improve the therapeutic options of OA, tissue engineering based on the use of mesenchymal stem cells (MSCs) has emerged. However, the presence of inflammatory cytokines, such as interleukin-1 $\beta$  (IL-1 $\beta$ ), during chondrogenesis reduces the efficacy of cartilage engineering repair procedures by preventing chondrogenic differentiation. Previous studies have shown that electromagnetic fields (EMFs) stimulate anabolic processes in OA cartilage and limit IL-1 $\beta$  catabolic effects. We investigated the role of EMFs during chondrogenic differentiation of MSCs, isolated from bovine synovial fluid, in the absence and presence of IL-1 $\beta$ . Pellets of MSCs were differentiated for 3 and 5 weeks with transforming growth factor- $\beta$ 3 (TGF $\beta$ 3), in the absence and presence of IL-1 $\beta$  and exposed or unexposed to EMFs. Biochemical, quantitative real-time RT-PCR and histological results showed that EMFs alone or in the presence of TGF $\beta$ 3 play a limited role in promoting chondrogenic differentiation. Notably, in the presence of IL-1 $\beta$  and TGF $\beta$ 3 a recovery of proteoglycan (PG) synthesis, PG content and aggrecan and type II collagen mRNA expression in the EMF-exposed compared to unexposed pellets was observed. Also, histological and immunohistochemical results showed an increase in staining for alcian blue, type II collagen and aggrecan in EMF-exposed pellets. In conclusion, this study shows a significant role of EMFs in counteracting the IL-1 $\beta$ -induced inhibition of chondrogenesis, suggesting EMFs as a therapeutic strategy for improving the clinical outcome of cartilage engineering repair procedures, based on the use of MSCs. Copyright © 2012 John Wiley & Sons, Ltd.

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## 1. Introduction

Osteoarthritis (OA) is a common disease of all the anatomical structures of the joint that is associated with articular cartilage loss, subchondral bone change and

synovitis leading to progressive joint degeneration (Aigner *et al.*, 2006). To date, cartilage damage is an irreversible process, because of the limited capacity of the adult articular chondrocytes to repair and regenerate the normal cartilage matrix architecture. Despite the large amount of active research to identify structure-modifying approaches to inhibit cartilage destruction in OA, there is an urgent need to improve the therapeutic options, because existing drug therapies reduce symptoms, primarily pain, but have a limited long-term efficacy (Goldring, 2006).

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In recent years, tissue engineering based on the use of mesenchymal stem cells (MSCs) has emerged as an alternative approach to current treatments for cartilage defects. Alternative cell sources with chondrogenic potential include MSCs derived from synovium, adipose tissue and periosteum, among others (De Bari *et al.*, 2001; Guilak *et al.*, 2004; Tuli *et al.*, 2004). Although cartilage engineering repair strategies that rely on the *in situ* differentiation of MSCs are attractive, existing methods fail to provide a reliably successful, long-term clinical outcome (Richter, 2009). A limitation of these procedures may be due to the presence of the inflamed environment in which chondrogenesis takes place. Intra-articular inflammation may result from disease, such as arthritis, or trauma, including the trauma during cartilage repair surgery itself. In inflammatory conditions, pro-inflammatory and catabolic mediators released from chondrocytes, synovial fibroblasts and inflammatory cells have been identified at high levels in the joint's inflammatory environment. Among them, the pro-inflammatory cytokine interleukin-1 $\beta$  (IL-1 $\beta$ ) plays a pivotal role in local inflammatory processes, and it has been shown that elevated IL-1 $\beta$  concentrations may be maintained in synovial fluid for a long time after injury (Catterall *et al.*, 2010). It has been also reported that the IL-1 $\beta$  levels, not detectable in healthy knee joints, show an increasing trend in cartilage lesions and reach a significantly elevated peak following the surgical cartilage-regenerating intervention (Schmal *et al.*, 2009). Furthermore, a frequent problem associated with cartilage repair strategies is the formation of fibrocartilaginous tissue. The formation of fibrotic tissue seems to be reduced by limiting the activity of inflammatory cytokines. In fact, it has been shown that a human MSC subpopulation expressing high levels of IL-1 receptor antagonist was able to inhibit bleomycin-induced inflammation and fibrosis within the lungs of mice (Ortiz *et al.*, 2007). In addition, IL-1 $\beta$  has been shown to inhibit the chondrogenic differentiation of human MSCs (Wehling *et al.*, 2009). Therefore, IL-1 $\beta$  activity might be strongly involved in the biological problems related to the regeneration of new cartilage tissue from MSCs.

Previous studies show that physical stimulation with electromagnetic fields (EMFs) represent a viable therapeutic approach to limiting cartilage degradation and to controlling inflammation associated with joint diseases, by stimulating anabolic chondrocyte functions and limiting the effects due to inflammatory activities of synovial fibroblasts (Ongaro *et al.*, 2012; Sellam and Berenbaum, 2010). In bovine and human cartilage explants, EMFs prevent the catabolic effect of the pro-inflammatory cytokine IL-1 $\beta$  and act in synergy with insulin-like growth factor-I (IGF-I), the main anabolic factor of cartilage (De Mattei *et al.*, 2003, 2004, 2007; Ongaro *et al.*, 2011). Further, in IL-1 $\beta$ -stimulated human osteoarthritic synovial fibroblasts, EMFs counteract the catabolic effects induced by the cytokine (De Mattei *et al.*, 2009), as EMFs reduce the synthesis of inflammatory mediators such as PGE<sub>2</sub> and pro-inflammatory cytokines (IL-6 and IL-8) (Ongaro *et al.*, 2012). *In vivo*, EMFs preserve the morphology of articular cartilage and retard the

development of osteoarthritic lesions in guinea pigs (Fini *et al.*, 2005). Also, EMFs favour the integration of osteochondral autografts in sheep, by decreasing IL-1 and tumour necrosis factor- $\alpha$  concentration in the synovial fluid, (Benazzo *et al.*, 2008a). In humans, EMFs show effectiveness in controlling joint inflammation after surgical procedures at the knee (Benazzo *et al.*, 2008b; Zorzi *et al.*, 2007).

More recently, several studies have shown that EMFs can also influence the behaviour of MSCs, particularly their differentiation into the osteogenic lineage (Saino *et al.*, 2011; Schwartz *et al.*, 2008; Tsai *et al.*, 2009).

All of this evidence suggests that EMFs might have effects on MSC differentiation, thus limiting the catabolic activity of IL-1 $\beta$ , during cartilage-regenerating surgical interventions. Therefore, we first evaluated whether the chondrogenic differentiation of MSCs might be influenced by EMF exposure; then we investigated the role of EMFs during chondrogenic differentiation in the presence of IL-1 $\beta$ . As an experimental model we used MSCs isolated from bovine synovial fluid, since MSCs derived from the synovial membrane or the synovial fluid show higher chondrogenic potential than MSCs from other tissues (Sakaguchi *et al.*, 2005; Shirasawa *et al.*, 2006), suggesting that synovium is an excellent source of MSCs for cartilage regeneration. Our hypothesis was that EMFs might counteract the inhibition of the differentiation process induced by IL-1 $\beta$  during chondrogenesis.

## 2. Materials and methods

### 2.1. Collection of MSCs from synovial fluid and cell cultures

MSCs were isolated as previously reported by other authors, with minor changes in the experimental practice (Jones *et al.*, 2008; Jones *et al.*, 2004). Briefly, synovial fluid was aspirated from the metacarpophalangeal joints from eight bovines (females, 14–18 months old) using a syringe. For isolating cells, fresh synovial fluid ( $2 \pm 0.6$  ml for each animal) was diluted 1:4 with complete medium [Dulbecco's modified Eagle's/Ham's F12 (1:1) medium (DMEM/F12; Life Technologies, Paisley, UK)] containing 10% fetal bovine serum (FBS), centrifuged at 2000 rpm for 10 min and plated in 25 cm<sup>2</sup> culture flasks (Falcon, Becton-Dickinson, Franklin Lakes, NJ, USA). After 3 h, the medium was removed and fresh complete medium was added to the flasks. Immediately after cell isolation, a conventional colony-forming unit-fibroblast (CFU-F) assay was performed to evaluate the number of clonogenic cells (Jones *et al.*, 2004). At the beginning, cells isolated for the differentiation experiments were plated at about 500 cells/cm<sup>2</sup>, maintained in culture and then subcultured at 5000/cm<sup>2</sup> (Sakaguchi *et al.*, 2005). MSCs at passage 3 were used in chondrogenic differentiation experiments, according to previous studies on synovial MSCs (De Bari *et al.*, 2001; Jones *et al.*, 2004, 2008).

## 2.2. Chondrogenic differentiation

Cells (400 000) were centrifuged at 1000 rpm for 10 min in 15 ml tubes to form a pellet. The pellets were cultured in 0.5 ml chondrogenic differentiation basal medium containing dexamethasone, ascorbate, insulin, transferrin, selenium, penicillin/streptomycin, proline, sodium pyruvate and L-glutamine (Lonza Walkersville, Walkersville, MD, USA) at 37 °C, 5% CO<sub>2</sub>, alone (control) or supplemented with 10 ng/ml TGF $\beta$ 3 (Lonza), according to the manufacturer's protocol of chondrogenic differentiation. In a subset of pellets, 50 ng/ml IL-1 $\beta$  (PeproTech, London, UK) were added to the chondrogenic medium to evaluate the effects of the cytokine on chondrogenic differentiation. The IL-1 $\beta$  dose was chosen on the basis of our previous study performed on bovine cartilage explants (De Mattei *et al.*, 2003). In a parallel setting, the pellets were exposed to EMFs (75 Hz, 1.5 mT) inside an incubator during the whole period of culture. The medium was changed every 3 days. The pellets were harvested after 3 and 5 weeks of culture.

To evaluate chondrogenic differentiation, two series of pellets were used, one for biochemical assays and the other for quantitative real-time RT-PCR and histological analysis. Each series of pellets was derived from cells harvested from the same animal. Based on cell availability, when possible, cells from the same animal were used for all the experimental assays (biochemical, quantitative real-time RT-PCR and histological analysis). Furthermore, three pellets were prepared for each experimental condition tested. Four experiments for biochemical analysis and three for quantitative real-time RT-PCR and histological analysis were carried out.

## 2.3. Characteristics of EMF and exposure conditions

The EMF generator system was the same as used in previous studies (De Mattei *et al.*, 2003, 2004, 2009; Varani *et al.*, 2008). It consisted of a pair of circular Helmholtz coils of copper wire placed opposite to each other and in a signal generator (IGEA S.p.A., Carpi, Italy). The pellets were placed between the pair of Helmholtz coils. The power generator produced a pulsed signal with pulse duration of 1.3 ms and frequency of 75 Hz, yielding a duty cycle of 1/10. The intensity peak of the magnetic field was 1.5 mT and was detected between two coils from one side to the other, by the Hall probe of a Gaussmeter (LE, Gaussmeter DG500, USA) with a reading sensitivity of 0.2%. The shape of the induced electric field and its impulse length were kept constant. The intensity value of the magnetic field measured between two coils was uniform in the whole area in which the pellets were placed. In EMF-exposed pellets, the EMF exposure was maintained for the whole differentiation time (3 or 5 weeks). Control pellets were maintained in the same incubator, placed at a distance from

the coils where no difference from background magnetic field was observed when the EMF generator was turned on.

## 2.4. Proteoglycan (PG) synthesis

PG synthesis was determined by radioactive sulphate incorporation into glycosaminoglycans (GAGs), which are biochemical components of PGs, after 3 or 5 weeks of culture, as previously reported (De Mattei *et al.*, 2004). Briefly, 5  $\mu$ Ci/ml Na<sub>2</sub>-<sup>35</sup>S<sub>4</sub> (2.2 mCi/ml; Amersham Pharmacia Biotech, Buckinghamshire, UK) was added to the culture media of both EMF-unexposed and -exposed pellets at time 0 and when the medium was replaced (every 3 days). After the radiolabelling, at the end of the culture period, the pellets were rinsed and digested in 20 mM phosphate buffer, pH 6.8, containing 2 mg/ml papain (Sigma-Aldrich, Milan, Italy) at 60 °C for 12 h. The content of <sup>35</sup>S-labelled newly synthesized PGs (<sup>35</sup>S-PGs) was measured following precipitation of the <sup>35</sup>S-PGs with cetylpyridinium chloride (Sigma-Aldrich) and filtration onto glass fibre filters (Whatman GF/C). The filters were dried and the radioactivity quantified by liquid scintillation counting. Data were normalized to the DNA content, measured fluorometrically by binding to Hoechst 33258 dye.

## 2.5. PG content

Total PG content within pellets was measured, using a spectrophotometer (Jenway, Zetalab Padova, Italy), as total sulphated GAGs, using the dimethylmethylene blue (DMMB) assay, with bovine chondroitin sulphate (Sigma-Aldrich Chemie, Steinheim, Germany) as the standard (De Mattei *et al.*, 2003), after digestion in papain as indicated above. The results were normalized to the pellet DNA content.

## 2.6. RNA isolation and quantitative real-time reverse transcription with polymerase chain reaction (RT-PCR)

Total RNA was extracted from formalin-fixed, paraffin-embedded pellets cultured for 3 and 5 weeks. For each sample, tissue slices were deparaffinized by two repeated incubations in xylene, followed by three repeated incubations in 100% ethanol, air-dried and homogenized in Qiazol lysis reagent in the RNeasy mini kit (Qiagen, Valencia, CA, USA). Total RNA was purified according to the manufacturer's protocol. RNA concentration and purity were determined using a NanoDrop 2000 spectrophotometer (Thermo Scientific). 75 ng total RNA was reverse-transcribed using the SuperScript™ III First-Strand Synthesis SuperMix (Invitrogen) and amplified using the PerfeCTa SYBR Green SuperMix, Rox (Quanta, 95055-02 K), with an initial 3 min incubation at 95 °C

followed by 40 cycles of amplification (95 °C for 15 s and 60 °C for 1 min), and examined on a 7500 Fast Real-Time PCR system (Applied Biosystems) (Rizzo *et al.*, 2008). Real-time RT-PCR was performed using primers for bovine collagen type II [ $\alpha$ 1(II)] and for aggrecan previously reported (Shintani and Hunziker, 2007). The real-time PCR data were analysed using the relative gene expression ( $^{\Delta\Delta C_T}$ ) method, as described in Applied Biosystems User Bulletin No. 2. Data are presented as the fold change in gene expression normalized to the endogenous reference gene (*18S* rRNA) and calculated relative to those of unexposed untreated pellets (control).

## 2.7. Histological analysis

At weeks 3 and 5 of culture, the pellets were fixed in a neutral-buffered, isotonic formalin solution at 4 °C overnight, embedded in paraffin and serially sectioned at 5  $\mu$ m, using a hard-cutting microtome (Leica RM2025, Leica Instruments GmbH, Nussloch, Germany). The sections were stained with haematoxylin and eosin (H&E) for morphological observations and with Alcian blue (Sigma-Aldrich) to assess for sulphated GAG content. Non-consecutive sections were immunostained with monoclonal antibodies against collagen type II and aggrecan (Abcam, Cambridge, MA, USA) individually. Immunohistochemical sections were deparaffinized, rehydrated and incubated for 1 h with 1 mg/ml collagenase from *Clostridium histolyticum* type VII (Sigma-Aldrich) in Tris-buffered saline (TBS), pH 7.2, at 37 °C. Then the sections were treated with 3% hydrogen peroxide for 10 min to inhibit endogenous peroxidase and incubated for 5 min with Ultra V Block at room temperature to block non-specific background staining. The primary antibody was applied to the sections and incubated overnight at 4 °C; then the sections were washed in buffer and incubated with primary antibody enhancer for 10 min at room temperature. This was followed by 15 min with horseradish peroxidase (HRP) polymer (Ultravision LP Large Volume Detection System HRP polymer, Thermo Scientific, Runcorn, UK). Finally, the sections were counterstained with haematoxylin. Normal bovine articular cartilage was used as the positive control. Twelve sections/treatment, i.e. three pellets/treatment and four non-consecutive sections/pellet, were examined.

## 2.8. Statistical analysis

Biological data shown in the Figures represent mean standard deviation (SD). Statistical analysis was assessed by one-way analysis of variance (ANOVA). Comparisons between groups were performed using Student's *t*-test. For statistical validation of the data, four independent experiments for biochemical analysis and three for quantitative real-time RT-PCR and histological analysis were carried out. In all experiments, each experimental condition was tested in triplicate.  $p < 0.05$  was considered statistically significant.

## 3. Results

### 3.1. Synovial fluid-derived MSC cultures

It has been previously reported that during the first week of culture, MSCs derived from the synovial fluid undergo several rounds of cell division, resulting in fibroblastic colonies clearly detectable by day 7 (Jones *et al.*, 2004, 2008). Accordingly, in our cultures we observed a progressive growth of cells derived from the synovial fluid. The cells appeared very sparse 24 h after seeding, then colony formation was detectable by days 3–5. Data obtained from the CFU-F assay ( $n = 5$ ) showed that CFU-F represented a mean  $\pm$  SD =  $0.32 \pm 0.08\%$  of total synovial fluid cells (about 240 cells/ml of synovial fluid). Under our experimental culture conditions, the expansion of synovial fluid MSC-derived colonies yielded typical spindle-shaped fibroblast-like cells, which were used at passage 3 for chondrogenic differentiation experiments (data not shown).

### 3.2. Effects of EMFs on chondrogenesis

To investigate the effects of EMFs on chondrogenic differentiation of synovium-derived MSCs, the pellets were cultured for 3 and 5 weeks in the absence and presence of 10 ng/ml TGF $\beta$ 3 and exposed or unexposed to EMFs for the whole period in culture.

Biochemical results concerning pellet PG synthesis and PG content obtained after 3 and 5 weeks of differentiation time are shown in Figure 1. In the absence of TGF $\beta$ 3, control pellets showed a very low PG synthesis and PG content. Pellets exposed to EMFs had behaviour similar to that of unexposed control pellets, suggesting that EMF exposure alone does not influence pellet culture differentiation. In the presence of the chondrogenic growth factor TGF $\beta$ 3, a significant increase in PG synthesis and PG content was observed in EMF-exposed and -unexposed pellets compared with TGF $\beta$ 3-untreated and the EMF-unexposed control at both differentiation times, in a time-dependent fashion. The enhancement observed in the TGF $\beta$ 3-treated pellets compared with control was 305% at 3 weeks and 547% at 5 weeks in PG synthesis, and 50% at 3 weeks and 254% at 5 weeks in PG content. Similarly, pellets cultured in the presence of TGF $\beta$ 3 and exposed to EMFs showed a time-dependent increase in PG synthesis (274% at 3 weeks and 469% at 5 weeks, compared to control) and in PG content (28% at 3 weeks and 201% at 5 weeks, compared to control) and no significant differences were observed between EMF-exposed and -unexposed pellets in the presence of TGF $\beta$ 3.

Type II collagen and aggrecan gene expressions were measured by quantitative real-time RT-PCR to assess the expression of chondrocyte-specific genes in pellets cultured under the same experimental conditions. As shown in Figure 2, TGF $\beta$ 3-treated pellets showed 55- and 262-fold increases in type II collagen gene expression, compared to control, at 3 and 5 weeks, respectively.

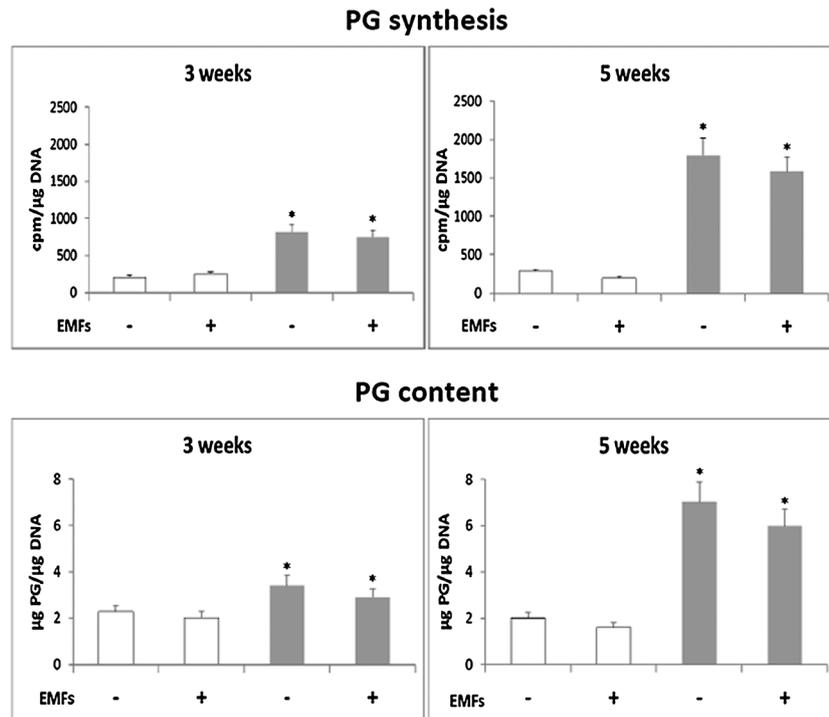


Figure 1. Effects of EMFs on chondrogenic differentiation of MSCs: biochemical data ( $n = 4$ ). PG synthesis and PG content in pellets cultured in the absence (white bar) and presence (grey bar) of 10 ng/ml TGF $\beta$ 3 for 3 and 5 weeks and exposed or unexposed to EMFs. All data are expressed as mean  $\pm$  SD. \*Statistical significance vs TGF $\beta$ 3-untreated and EMF-unexposed pellets (control)

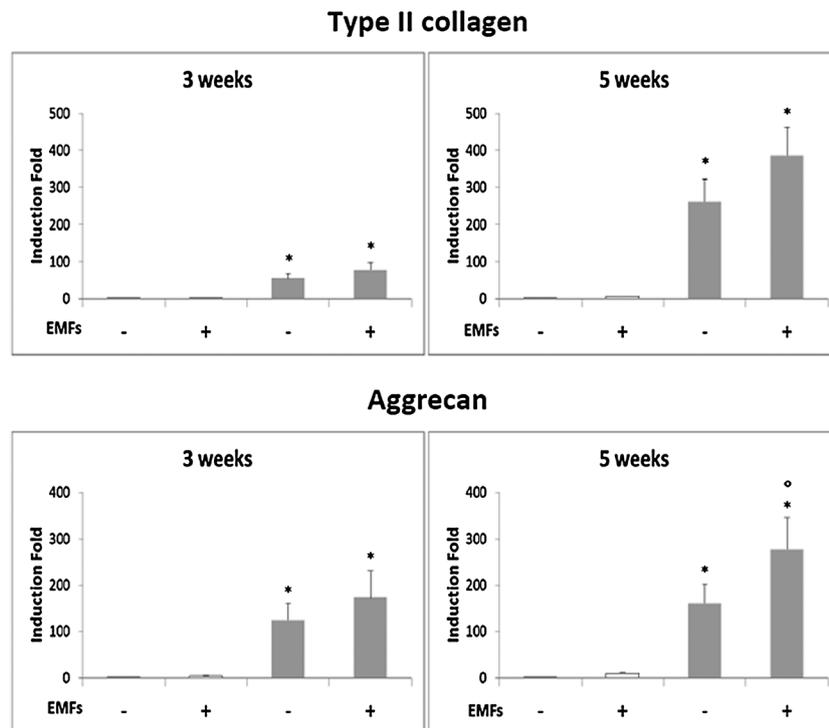


Figure 2. Effects of EMFs on chondrogenic differentiation of MSCs: quantitative real-time RT-PCR data ( $n = 3$ ). Type II collagen and aggrecan gene expression in pellets cultured in the absence (white bar) and presence (grey bar) of 10 ng/ml TGF $\beta$ 3 for 3 and 5 weeks and exposed or unexposed to EMFs. All data are expressed as mean  $\pm$  SD. \*Statistical significance vs TGF $\beta$ 3-untreated and EMF-unexposed pellets (control); °statistical significance vs TGF $\beta$ 3-treated and EMF-unexposed pellets

In TGF $\beta$ 3-treated pellets exposed to EMFs, a further induction in type II collagen expression compared to control was observed (78- and 387-fold at 3 and 5 weeks, respectively),

although differences between EMF-exposed and -unexposed pellets were not significant. A similar trend was found on aggrecan gene expression. TGF $\beta$ 3-treated pellets showed

124- and 161-fold increases, compared to control, at 3 and 5 weeks, respectively. In TGF $\beta$ 3-treated pellets, a further significant increase of 72.7% in aggrecan gene expression was induced by EMFs at 5 weeks.

In line with quantitative results showing that TGF $\beta$ 3 enhances cartilage extracellular matrix production and chondrocyte-specific gene expression, histological data supported that supplementation with the growth factor stimulated chondrogenic differentiation. Histological results obtained at 5 weeks of differentiation are shown in Figure 3. The pellets cultured without TGF $\beta$ 3 appeared smaller than those cultured with TGF $\beta$ 3 and they had no visible staining for Alcian blue, type II collagen or aggrecan, regardless of the differentiation time considered. In contrast, pellets cultured in the presence of TGF $\beta$ 3 exhibited a rounded shape and positive staining for Alcian blue, type II collagen and aggrecan compared to controls. In the pellets, a difference in the distribution of type II collagen and aggrecan was observed because the first preferentially accumulated at the edges of the pellets, whilst the second was distributed within the pellets. Pellets cultured in the presence of TGF $\beta$ 3 and exposed to EMFs did not show significant differences in morphology and staining for Alcian blue and type II collagen compared with EMF-unexposed pellets. Only a little more intense staining for aggrecan was observed in EMF exposed TGF $\beta$ 3-treated pellets compared with unexposed pellets.

### 3.3. Effects of EMFs on chondrogenesis in IL-1 $\beta$ -treated pellets

In order to evaluate whether EMFs can counteract the action of IL-1 $\beta$  during chondrogenesis, an untreated set and a TGF $\beta$ 3-treated set of pellets were cultured for 3 and 5 weeks in the presence of 50 ng/ml IL-1 $\beta$  and exposed or unexposed to EMFs. In the absence of TGF $\beta$ 3, the pellets cultured with IL-1 $\beta$  presented quantitative and histological results similar to the control pellets (data not shown).

In the presence of IL-1 $\beta$  and TGF $\beta$ 3 into the culture medium, significant time-dependent decreases in PG synthesis ( $-52\%$  and  $-74\%$  at 3 and 5 weeks, respectively) and PG content ( $-35\%$  and  $-71\%$  at 3 and 5 weeks, respectively) were observed compared to TGF $\beta$ 3-treated pellets (Figure 4). Interestingly, in the presence of both TGF $\beta$ 3 and IL-1 $\beta$ , EMF-exposed pellets showed a recovery of 40% at 3 weeks and of 88% at 5 weeks in PG synthesis, when compared to EMF-unexposed pellets. In addition, at 5 weeks a recovery of 138% in PG content was observed in the EMF-exposed TGF $\beta$ 3- and IL-1 $\beta$ -treated pellets compared to EMF-unexposed pellets. This suggests that the pro-inflammatory cytokine inhibited PG biosynthesis in our pellet cultures and EMF exposure was able to partially reverse this inhibition.

Quantitative real-time RT-PCR analysis showed that IL-1 $\beta$  induced a significant inhibition in both type II

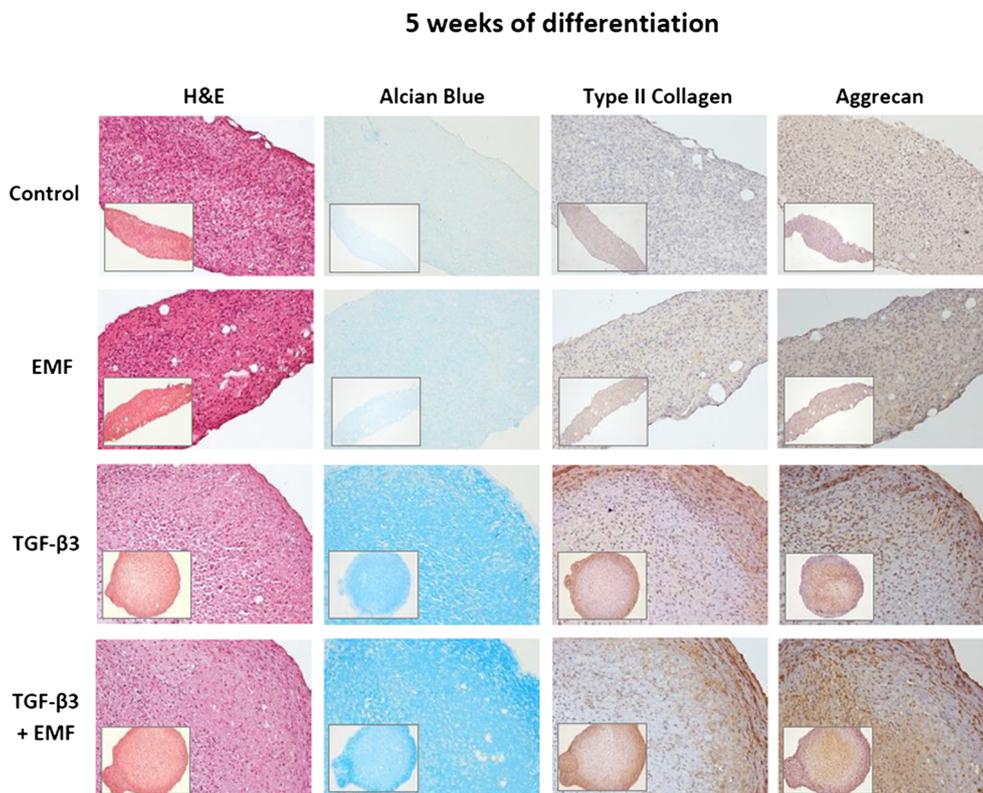


Figure 3. Effects of EMFs on chondrogenic differentiation of MSCs: histological data ( $n = 3$ ). Haematoxylin and eosin (H&E) and alcian blue staining and immunohistochemistry for type II collagen and aggrecan in pellets cultured in the absence and presence of 10 ng/ml TGF $\beta$ 3, for 5 weeks and exposed or unexposed to EMFs. Higher-magnification images ( $\times 200$ ) of the boxed areas (original magnification  $\times 100$ ) are shown

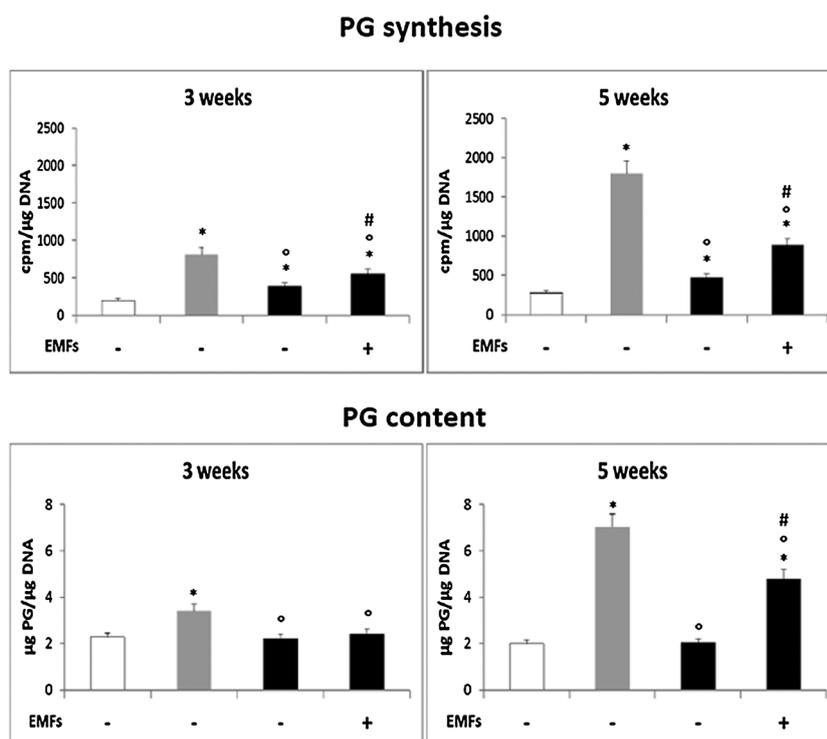


Figure 4. Effects of EMFs on chondrogenic differentiation of MSCs in the presence of the pro-inflammatory cytokine IL-1 $\beta$ : biochemical data ( $n = 4$ ). PG synthesis and PG content in pellets cultured in the absence (white bar) and presence (grey bar) of 10 ng/ml TGF $\beta$ 3 and 50 ng/ml IL-1 $\beta$  (black bar), for 3 and 5 weeks and exposed or unexposed to EMFs. All data are expressed as mean  $\pm$  SD. \*Statistical significance vs TGF $\beta$ 3-untreated and EMF unexposed pellets (control); °statistical significance vs TGF $\beta$ 3-treated and EMF unexposed pellets; #statistical significance vs unexposed pellets cultured in the presence of TGF $\beta$ 3 and IL-1 $\beta$

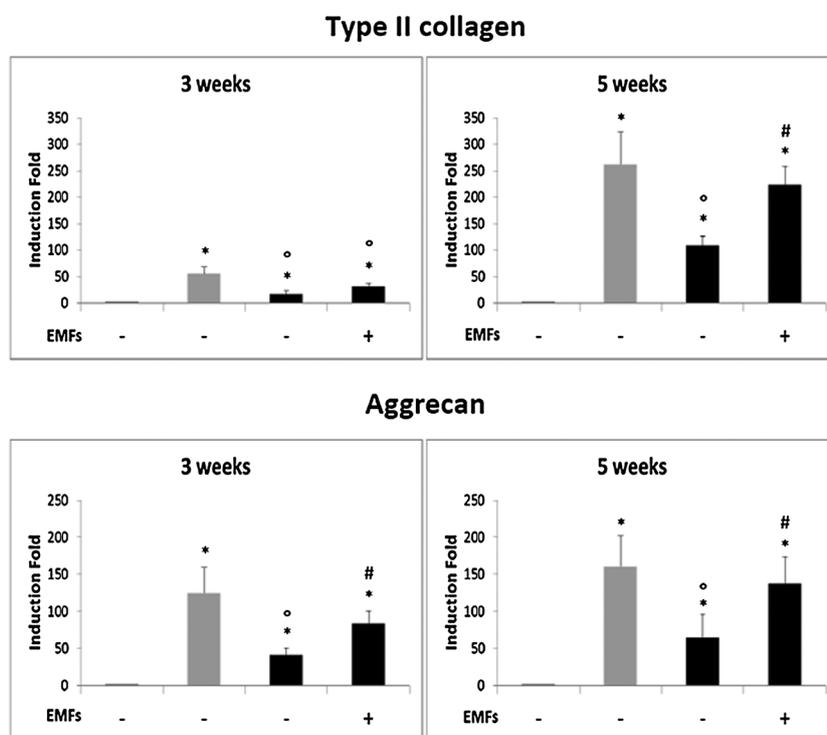


Figure 5. Effects of EMFs on chondrogenic differentiation of MSCs in the presence of the pro-inflammatory cytokine IL-1 $\beta$ : quantitative real-time RT-PCR data ( $n = 3$ ). Type II collagen and aggrecan gene expression in pellets cultured in the absence (white bar) and presence (grey bar) of 10 ng/ml TGF $\beta$ 3 and 50 ng/ml IL-1 $\beta$  (black bar), for 3 and 5 weeks and exposed or unexposed to EMFs. All data are expressed as mean  $\pm$  SD. \*Statistical significance vs TGF $\beta$ 3-untreated and EMF-unexposed pellets (control); °statistical significance vs TGF $\beta$ 3-treated and EMF-unexposed pellets; #statistical significance vs unexposed pellets cultured in the presence of TGF $\beta$ 3 and IL-1 $\beta$

collagen and aggrecan expression (Figure 5). Specifically, when compared with TGF $\beta$ 3-treated pellets, the decrease in type II collagen expression was 68% and 59% at 3 and 5 weeks, respectively, and in aggrecan expression 67% and 60% at 3 and 5 weeks, respectively. These reductions were in part counteracted by EMF exposure. In particular, a total recovery in type II collagen gene expression was induced by EMFs at 5 weeks (107% increase compared to EMF-unexposed TGF $\beta$ 3- and IL-1 $\beta$ -treated pellets) and in aggrecan expression at both differentiation times (105% and 111% increase at 3 and 5 weeks, respectively, compared to EMF-unexposed TGF $\beta$ 3- and IL-1 $\beta$ -treated pellets).

These findings were confirmed by histological and immunohistochemical results showing a reduction in staining for Alcian blue, type II collagen and aggrecan in pellets cultured in the presence of IL-1 $\beta$  and TGF $\beta$ 3, compared with pellets cultured with TGF $\beta$ 3 alone. Interestingly, at 5 weeks of differentiation, in EMF-exposed pellets an appreciable recovery of the histological parameters analysed was observed compared to unexposed pellets (Figure 6).

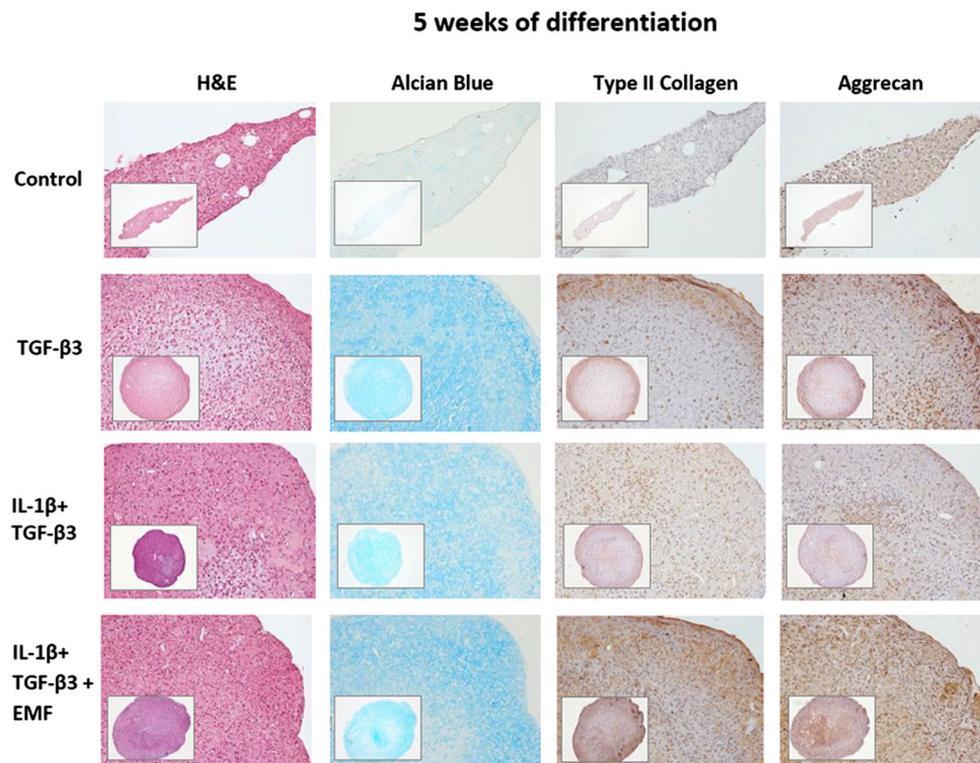
## 4. Discussion

In this study we employed the pellet culture system of synovial fluid derived-MSCs to evaluate the effects of EMF

exposure on chondrogenesis. MSCs used for cartilage engineering repair strategies have been identified in various adult tissues: bone marrow (Jiang *et al.*, 2002), periosteum, fat, synovial membrane (Pei *et al.*, 2008) and synovial fluid (Jones *et al.*, 2004, 2008). Furthermore, a chondrocyte progenitor population isolated from the surface zone of articular cartilage appears to be a promising cell source for cell-based cartilage repair (McCarthy *et al.*, 2012; Williams *et al.*, 2010).

The choice of our experimental model is due to the observation that MSCs isolated from the synovium and synovial fluid of animals or humans have been shown to have a higher chondrogenic potential than MSCs derived from other tissues (De Bari *et al.*, 2001; Jones *et al.*, 2004, 2008; Park *et al.*, 2005; Shirasawa *et al.*, 2006), thus making them a suitable source for studies on chondrogenesis (Sakaguchi *et al.*, 2005).

Several growth factors, including TGF $\beta$ 1, TGF $\beta$ 3, insulin-like growth factor-1 (IGF-1) (Longobardi *et al.*, 2006) and bone morphogenetic proteins (BMPs) (Park *et al.*, 2005), are commonly used to induce chondrogenesis in synovial-derived MSCs or MSCs from other tissues. In our study, we stimulated chondrogenic differentiation by adding 10 ng/ml TGF $\beta$ 3 to the culture medium. It has been reported that the TGF $\beta$  subtypes are equally active chondrogenic factors (Richter, 2009), and both TGF $\beta$ 1 and TGF $\beta$ 3 stimulate *in vitro* chondrogenesis (Fortier *et al.*, 2011). For synovium-derived stem cells-based chondrogenesis, TGF $\beta$ 1 (De Bari *et al.*, 2001; Pei *et al.*, 2008)



**Figure 6.** Effects of EMFs on chondrogenic differentiation of MSCs in the presence of the pro-inflammatory cytokine IL-1 $\beta$ : histological data ( $n = 3$ ). H&E and alcian blue staining and immunohistochemistry for type II collagen and aggrecan in pellets cultured in the absence and presence of 10 ng/ml TGF $\beta$ 3 and 50 ng/ml IL-1 $\beta$ , for 5 weeks and exposed or unexposed to EMFs. Higher-magnification images ( $\times 200$ ) of the boxed areas (original magnification  $\times 100$ ) are shown

and TGF $\beta$ 3 (Jones *et al.*, 2004; Sakaguchi *et al.*, 2005; Shirasawa *et al.*, 2006) have both been used successfully as chondrogenic factors in different experimental models. In line with these studies, in our TGF $\beta$ 3-treated pellets the MSCs assumed chondrocyte-like characteristics by synthesizing PGs, type II collagen and aggrecan, as shown by biochemical, quantitative gene-expression and histological results. Regarding treatment times in *in vitro* differentiation experiments, several times of chondrogenic differentiation are reported in the literature, from 2 to 6 weeks (Sakaguchi *et al.*, 2005; Shintani and Hunziker, 2007; Shirasawa *et al.*, 2006). Specifically, in bovine synovial explants a time-dependent chondrogenic differentiation was observed (Shintani and Hunziker, 2007). Therefore, to analyse chondrogenic differentiation in our experimental model during an early and a later differentiation time, we maintained the pellets in culture for 3 and 5 weeks. We observed a time-dependent increase in the parameters investigated, showing that TGF $\beta$ 3 induces progressive differentiation with increasing culture time. Regarding the analysis of the EMF effects, the results indicate that under our experimental conditions EMF exposure had limited effects on TGF $\beta$ 3-induced chondrogenesis, as shown by quantitative and histological data, although it could increase aggrecan gene expression, at least at 5 weeks. Although there is growing evidence showing the impact of EMF exposure on human MSCs during *in vitro* osteogenic differentiation (Schwartz *et al.*, 2008; Tsai *et al.*, 2009), conversely, there is a lack of research addressing whether the chondrogenic potential of human MSCs can be increased *in vitro* by the application of low-frequency EMFs. However, the study of Mayer-Wagner *et al.* (2011) focused on this aim and analysed, by real-time PCR, the expression of chondrogenic differentiation-related genes. They found that low-frequency electromagnetic stimulation (15 Hz, 5 mT) led to a significant increase in type II collagen mRNA expression in human MSCs at passage 6, but it did not modify aggrecan, SOX 9 and type X collagen mRNA expression. In our study, in the pellets exposed to EMFs, we did not find a significant increase of type II collagen expression analysed by real-time PCR and immunostaining, whilst we observed an increase in aggrecan gene expression. These apparently different results may be related to the tissue source of MSCs or the different cell passage number, as well as to differences in the characteristics of the electromagnetic field.

Regarding the efficacy of cartilage-regenerative procedures, a relevant problem is the presence in the site of the lesion of several pro-inflammatory and catabolic mediators. Among these factors, the cytokine IL-1 $\beta$  plays a crucial role, not only in the inflammatory process but also in the inhibition of *in vitro* chondrogenic differentiation of MSCs (Wehling *et al.*, 2009). Accordingly, in our experimental model IL-1 $\beta$  also strongly inhibited chondrogenesis induced by TGF $\beta$ 3, by reducing PG synthesis and PG content accumulation, type II collagen and aggrecan expression. Notably, in pellets treated with TGF $\beta$ 3 in the presence of the cytokine, EMF exposure could

counteract the inhibitory IL-1 $\beta$  effects on chondrogenesis by sustaining the expression of type II collagen, aggrecan and PGs, although EMFs were not able to completely re-establish the level of chondrogenic differentiation observed in the absence of IL-1 $\beta$ .

These data indicate that synovial MSCs are sensitive to EMFs, in agreement with the results of previous studies on MSCs obtained from different tissues (Mayer-Wagner *et al.*, 2011; Schwartz *et al.*, 2008). The ability of EMFs to counteract IL-1 $\beta$  activity is in line with previous data showing similar effects in differentiated cartilage (De Mattei *et al.*, 2003; Ongaro *et al.*, 2011). In fact, in both bovine (De Mattei *et al.*, 2003) and human cartilage explants (Ongaro *et al.*, 2011) cultured in the presence of IL-1 $\beta$ , EMF exposure counteracted the inhibitory effect on PG synthesis and PG content induced by the cytokine, suggesting an EMF chondroprotective role under inflammatory conditions. Similar anti-inflammatory effects have been also observed in bovine and human synovial fibroblasts, in which EMFs reduced the production of pro-inflammatory mediators and cytokines induced by IL-1 $\beta$  (De Mattei *et al.*, 2009; Ongaro *et al.*, 2012). In agreement with these previous studies, the results of this study show that EMFs also maintain the capability to inhibit the catabolic activity of IL-1 $\beta$  in MSCs. Although the mechanisms through which EMFs may counteract the inhibitory effects of IL-1 $\beta$  on chondrogenesis remain to be elucidated, these effects might be mediated by an EMF-induced increase of anti-inflammatory adenosine receptors. Indeed, it has been previously reported that EMFs stimulate an increase of A<sub>2A</sub> and A<sub>3</sub> adenosine receptors, which are involved in the regulation of inflammatory processes in both chondrocytes and synovial fibroblasts (De Mattei *et al.*, 2009; Ongaro *et al.*, 2012; Varani *et al.*, 2008, 2010).

In conclusion, the results of this study support the hypothesis that EMF therapy may maintain and favour chondrogenic differentiation under inflammatory conditions. Low-frequency EMFs are a non-invasive therapy that has not been linked with any side-effects (Benazzo *et al.*, 2008b; Zorzi *et al.*, 2007). EMFs can be applied during cell culture and beyond under *in vivo* conditions. In regenerative medicine, after implantation of the tissue substitute, physical stimuli could have a primary role, by preventing the catabolic effects of the inflammatory microenvironment and instead favouring the anabolic activities of the implanted cells and surrounding tissues.

Taken together, these results suggest EMF exposure as a possible strategy for improving the clinical outcome of cartilage repair procedures, based on tissue engineering and the use of MSCs.

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## Conflicts of interest

Stefania Setti is an employee of IGEA S.p.A. (Carpi, Italy).

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