

1 **Comparative cytotoxicity of kaolinite, halloysite, multiwalled carbon nanotubes**  
2 **and graphene oxide**

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15  
16 **Abstract**

17 This study **aimed** at comparative examining of the interactions between conventionally  
18 used clay and carbon nanomaterials and human lung adenocarcinoma cells (A549 cells).  
19 The following platy and tubular nanomaterials **were** tested: carbon nanoparticles, i.e.  
20 multi-walled carbon nanotubes (MWCNTs) and graphene oxide nanosheets (GO) as well  
21 as nanoclays, i.e. halloysite nanotubes (HNTs) and kaolinite nanosheets (Kaol).  
22 Nanoparticle physicochemical properties and their internalisation into cells were  
23 examined using dynamic light scattering as well as atomic force, 3D laser scanning  
24 confocal and darkfield hyperspectral microscopies. Biological aspects of the  
25 nanomaterial-cell interaction **included** assessment of cellular toxicity, DNA damage,

26 metabolic activity, and physical parameters of the cells. Regardless of a shape, carbon  
27 nanomaterials demonstrated cell surface adsorption, but negligible penetration into cells  
28 compared to nanoclays. However, carbon nanomaterials were found to be the most toxic  
29 for cells as probed by the MTS assay. They also turned out to be the most genotoxic for  
30 cells compared to nanoclays as revealed by the DNA-Comet assay. GO significantly  
31 increased the fraction of apoptotic cells and was the most cytotoxic and genotoxic  
32 nanomaterial. Comparison of flow cytometry and MTS data indicated that a cytotoxic  
33 effect of MWCNTs was not associated with increased cell death, but was rather due to a  
34 decrease in cell metabolic activity and/or proliferation. Finally, no significant effect of the  
35 shape of the tested nanomaterials on their internalization and cytotoxicity was revealed.

36 **Key words:** halloysite, kaolinite, multiwalled carbon nanotubes, graphene oxide,  
37 cytotoxicity, genotoxicity

38

## 39 **1. Introduction**

40 The scope of nanoparticle (NP) applications and the types of nanomaterials used are  
41 constantly expanding. A particular attention is drawn to the nanospheres and nanotubes  
42 as potent systems for drug delivery (Lazzara et al., 2017). Nanotechnology has had an  
43 extremely important impact on nanobiomedicine, as well as on the diagnostics and  
44 treatment of various diseases (Marcano et al., 2018). The advantage of nanoparticles as  
45 carriers is their ability to bind certain ligands and deliver them to a specific cell population  
46 (Balthasar et al., 2005). They can also facilitate the penetration of drugs through the  
47 cellular membrane (Amai and Tsuji, 2000). Multifunctional carriers represented by carbon  
48 nanoparticles (Mohajeri et al., 2018; Choi et al., 2018), silicon- (Rahikkala et al., 2018)  
49 and chitosan- (Li et al., 2018) based nanomaterials, lipid and polymer-based  
50 nanoparticles (Allen and Cullis 2004) were described. The use of nanomaterials in the

51 treatment of cancer is promising since they can release drugs at required conditions: a  
52 given pH, temperature change, light or ultrasound (Thambi and Park, 2014).  
53 Nanostructures are also used for diagnostics of diseases and as tools for monitoring the  
54 tissue repair (LaVan et al., 2003).

55 The appearance and wide distribution of nanomaterials of various forms, chemical  
56 composition, and charge invoked the emergence of a new science - nanotoxicology -  
57 which aims at understanding the physicochemical properties of nanomaterials and  
58 assessing their toxic effects on humans and the environment (Xia et al., 2006). Clinical  
59 and experimental studies show that the properties of some nanomaterials, along with their  
60 value for materials science, can have a negative effect on human tissues and therefore  
61 their toxicological effects require a close attention. The effect of the nanomaterial shape  
62 on toxicity is still not fully understood, although numerous studies suggest that there exists  
63 a relationship between the substrate shape and its toxicity (Oh et al., 2010, Sharifi et al.,  
64 2012; Gatoo et al., 2014; Jeevanandam et al., 2018).

65 In this study we compare the toxic potential of nanoparticles having tubular and platy  
66 morphologies. They include carbon-based nanoparticles, i.e. multi-walled carbon  
67 nanotubes (MWCNTs) and graphene oxide (GO) nanosheets as well as clays, i.e.  
68 halloysite nanotubes (HNTs) and planar kaolinite particles (Kaol). Graphene is an  
69 allotrope of carbon consisting of a single layer of carbon atoms arranged in hexagonal  
70 lattice (Geim and Novoselov, 2007). One of the most important graphene derivatives is  
71 GO (Park and Ruoff, 2009), which has a large number of oxygen atoms on its surface in  
72 the form of carboxyl groups, epoxy groups, and hydroxyl groups (Dreyer et al., 2010). GO  
73 is a highly appraised material in electronics, energy, and materials science (Stankovich  
74 et al., 2006). Recently GO has actively been considered as an agent for biomedical  
75 research and drug delivery (Liu et al., 2008; Su et al., 2013; Chen et al., 2012). Single or  
76 multiple graphene sheets rolled into cylinders form single-walled and multi-walled CNTs,

77 respectively. CNTs are widely known for their unique physicochemical properties and  
78 practical applications (Yang et al., 2012); GO also play an important role in drug delivery  
79 as a carrier system (Kayat et al., 2011). Since the multi-ton production and use of these  
80 nanoparticles is envisioned, it is important to better understand and probe a possible  
81 toxicity of CNTs.

82 Kaolinite minerals are among the most common clay minerals on Earth. They are 1:1  
83 phyllosilicates of variable morphology with the theoretical formula of  $\text{Al}_2\text{Si}_2\text{O}_5(\text{OH})_4 \cdot n\text{H}_2\text{O}$ , where  $n = 0$  and  $2$ , for kaolinite and hydrated halloysite, respectively. The minerals  
84 find wide practical application for the transfer of drugs and enzymes, in cosmetics and  
85 tissue engineering, and are used as a suspending agent, white pigment and an additive  
86 to various materials to improve their mechanical strength, electrical resistance and  
87 appearance (Awad et al., 2017). Kaolinite is generally represented by stacked platelets  
88 which are hydrophilic and easily dispersible in water. Ionic and/or polar nonionic  
89 surfactants can be applied to the surface of kaolinite to make it hydrophobic or  
90 organophilic (Murray, 2000). Halloysite is found in soils and rocks and is a multilayer  
91 nanotube with an internal cavity diameter of about 50 nm and a length of up to 1  $\mu\text{m}$ .  
92 HNTs were also proposed as drug, cosmetics and gene delivery agents (Lvov et al., 2016;  
93 Panchal et al., 2018; Micó-Vicent et al., 2018; Massaro et al., 2019; Batasheva et al.,  
94 2020), as well as components of cell capturing devices (Kryuchkova et al., 2020) and  
95 tissue engineering scaffolds (Naumenko and Fakhrullin, 2019).

97 Not surprisingly, carbon and clay nanotubes and nanoplates are currently a kind of  
98 competing nanomaterials in the field of biomedicine. Although the unique properties of a  
99 given nanomaterial mostly determine the scope of its application, all the benefits  
100 conferred by the nanomaterial use must be weighed against its toxic potential. Numerous  
101 studies have already been published on the toxicity of pristine and surface-modified  
102 carbon and clay nanomaterials (Magrez et al., 2006; Cornejo-Garrido et al., 2012; Yang

103 et al., 2013; Cervini-Silva et al., 2013, 2015, 2016; Maisanaba et al., 2015; Kryuchkova  
104 et al., 2016; Tarasova et al., 2019; Rozhina et al., 2020). However, the toxicity results  
105 obtained in different studies are sometimes contradictory and difficult to collate and  
106 compare because of variability in cell lines used, cell culture and other conditions.  
107 Systematic investigation is needed in which carbon and clay nanomaterials would be  
108 compared in one study using the same cell type and at the same conditions.

109 Recently a comparison of toxicity of MWCNTs and HNTs to human umbilical vein  
110 endothelial cells (HUVECs) *in vitro* and blood vessels of mice *in vivo* was reported (Wu  
111 et al., 2020). All of the toxic effects were more pronounced for MWCNTs in comparison  
112 with HNTs, implying that HNTs are probably safer nanocarriers compared with MWCNTs  
113 (Wu et al., 2020). However, the observed nanoparticle effects can be cell-type dependent  
114 (Pacurari et al., 2008) and greater safety of HNTs in comparison with MWCNTs should  
115 be verified in other cell types. In this study, for the first time the effects of carbon and clay  
116 nanomaterials of different shapes on human lung carcinoma cell line (A549) were  
117 compared side by side. The model of lung cells was chosen because inhalation is not  
118 only the most likely route of environmental nanoparticles exposure but the lung can be  
119 exposed to nanoparticles that are introduced to the body by any other administration route  
120 including gastrointestinal absorption and direct injection (Card et al., 2008). Cancer cell  
121 lines are widely used in the nanomaterial toxicity screenings because of their unlimited  
122 replication ability and wide distribution among researchers around the world, while their  
123 cell-to-cell variability can be addressed by application of statistical analyses.

## 124 **2. Materials and methods**

### 125 **2.1. Materials**

126 Kaol nanoparticles, MWCNTs and GO aqueous solutions, propidium iodide (PI) were  
127 purchased from Sigma Aldrich. All reagents were of analytical grade, and were used as

128 received without further purification. HNTs were received from Applied Minerals INC (NY,  
129 USA).

## 130 **2.2. Particle characterization**

131 NPs were resuspended in ultrapure H<sub>2</sub>O at a concentration of 40 mg mL<sup>-1</sup>. A sonication  
132 in a US-bath (Sonics & Material Inc., New Town, CT, USA) at 30 W for 10 min was applied  
133 to avoid NP aggregation. Hydrodynamic diameter and zeta-potential were determined at  
134 25°C in water using dynamic light scattering (DLS) in a Zetasizer Nano-ZS, Model  
135 ZEN3600 equipped with 633 nm laser of power of 4.0 mW (Malvern instruments Ltd.,  
136 Malvern, UK).

## 137 **2.3. Cell culture**

138 A549 cells were obtained from American Type Culture Collection (ATCC, Rockville,  
139 Maryland, USA) and cultured in minimal Eagle's medium Alfa (aMEM) (Paneco, RF)  
140 culture medium supplemented with 10% (v/v) fetal bovine serum (Gibco) and 100 U mL<sup>-1</sup>  
141 penicillin and 100 µg mL<sup>-1</sup> streptomycin at 37°C in a humidified atmosphere containing  
142 5% CO<sub>2</sub> and 95% air.

## 143 **2.4. Microscopic observations of NPs and cells**

144 Dark field microscopy images were obtained using a CytoViva® enhanced dark-field  
145 condenser attached to an Olympus BX51 (Japan) upright microscope equipped with  
146 fluorite 100x objectives and a DAGE CCD camera. Extra-clean dust-free Nexterion®  
147 glass slides and coverslips (Schott, Mainz, Germany) were used for enhanced dark-field  
148 microscopy imaging to minimize dust interference. For hyperspectral imaging of NPs and  
149 cell samples illuminated in the dark-field mode, scanning of the sample was performed  
150 automatically using a ProScan III (Prior) scanning module attached to the specimen table.  
151 Full field of view (901 image lines) images were collected at 0.1 s exposure time at

152 maximal halogen bulb light intensity. The hyperspectral data were collected using a  
153 Specim V10E spectrometer and PCOPixelFly CCD video camera. Spectra were collected  
154 within the 400 – 1000 nm region, spectral resolution was 2 nm. Hyperspectral data  
155 collection and mapping was performed using ENVI 4.8 software (Harris & Geospatial  
156 Solutions). Spectral libraries were obtained for pure nanoparticles (n = 20), which were  
157 then matched with hyperspectral images obtained from cells with internalized  
158 nanoparticles. This was done using the internal spectral mapping algorithm to determine  
159 the spectral matches between the image pixels in hyperspectral image of the cells and  
160 previously obtained nanoparticles spectral libraries. Spectral angle mapper threshold of  
161 0.3 radians was used. Individual colors were assigned to the pixels spectrally matching  
162 the NPs spectral signatures. ImageJ freeware (NIH) was used to calculate the area  
163 percentage of each individual color (expressed as number of pixels and percent of the  
164 whole image area).

165 The atomic force microscopy (AFM) images were obtained with Dimension Icon  
166 microscope (Bruker, USA) operating in the PeakForce Tapping mode. The ScanAsyst-air  
167 (Bruker) probes (nominal length 115  $\mu\text{m}$ , radius of tip 2 nm, spring constant 0.4  $\text{N m}^{-1}$ ).  
168 The images were obtained with 512-1024 lines/scanning at a speed of 0.8-0.9 Hz to  
169 provide high resolution images and display mechanical properties. Images were collected  
170 in the height (topography), peak force error, Young's modulus and adhesion imaging  
171 channels. The received data was processed using Nanoscope Analysis v.1.7. software  
172 (Bruker).

173 The topography of cells was studied using a laser scanning confocal microscope (LSCM)  
174 Keyence VK-X150 (Keyence, USA), as reported elsewhere (Panchal et al., 2018). The  
175 data obtained were processed using VK-Analyzer software (Keyence, USA).

## 176 **2.5. Cell viability**

177 The cell viability was evaluated by CellTiter 96® AQueous One Solution Cell Proliferation  
178 Assay, MTS (ProMega) according to the standard protocol. Briefly, A549 cells were  
179 seeded in the 96-well plates ( $2 \times 10^3$  cells per well) and incubated for 24 h. Then, NPs  
180 were added to the cells at different concentrations (11, 33, 100, 300 and 900  $\mu\text{g mL}^{-1}$ ).  
181 After 24 h of incubation cells were subjected to the incubation with MTS reagent and  
182 optical density (OD) of each well at 490 nm and 540 nm was measured by a Tecan Infinite  
183 200Pro (Tecan Trading AG). The cell viability (% to control) is expressed as the  
184 percentage of  $(\text{OD}_{\text{test}} - \text{OD}_{\text{blank}})/(\text{OD}_{\text{control}} - \text{OD}_{\text{blank}})$ , where  $\text{OD}_{\text{test}}$  is the optical  
185 density of the cells exposed to a nanoparticles sample,  $\text{OD}_{\text{control}}$  is the optical density  
186 of the control sample and  $\text{OD}_{\text{blank}}$  is the optical density of the wells without A549 cells.

## 187 **2.6. Apoptosis assay**

188 Apoptosis kit (FITC Annexin V Apoptosis Detection Kit I, Invitrogen) was employed to  
189 detect apoptotic and necrotic cells. A549 cells were seeded in 6-well plates ( $1 \times 10^5$  cells  
190 per well) and incubated for 24 h. The NPs samples were added to the cells at the  
191 concentration of  $100 \mu\text{g mL}^{-1}$  and incubated for another 24 h. A549 cells were collected,  
192 washed twice with PBS, and re-suspended in Annexin V buffer ( $1 \times 10^6$  cells  $\text{mL}^{-1}$ ) and  
193 stained with 5  $\mu\text{L}$  of FITC-conjugated Annexin V (Annexin V-FITC) and 5  $\mu\text{L}$  of propidium  
194 iodide. Cells were analyzed on FACS Aria III flow cytometer (BD Biosciences, USA).

## 195 **2.7. Comet (single-cell gel electrophoresis) assay to detect damaged DNA**

196 The Comet assay was performed according to protocol described (Nandhakumar et al.,  
197 2011). Briefly, a stock lysis solution was prepared: 10 mM Tris, 2.5 M NaCl, 100 mM  
198 EDTA, pH 10. Working lysis solution was cooled down to  $4^\circ\text{C}$  before use. The solution of  
199 low-melting agarose was prepared (0.5 %). Cell suspension (about  $10^5$  cells) was mixed  
200 with low-melting agarose at  $37^\circ\text{C}$  and put on slides. Then the cells were distributed on  
201 the glass with the tip and left at  $4^\circ\text{C}$  for 10 minutes. The cells were lysed for 45 minutes



202 at 4°C and washed with TAE-buffer. Then electrophoresis was carried out for 20 min at a  
203 field strength of (1 - 10) V cm<sup>-1</sup> and a current strength of ~ 300 mA. The glasses were  
204 placed into 70% ethyl alcohol and washed with distilled water for 5 minutes at room  
205 temperature. The cells were stained with ethidium bromide (EtBr). The nuclear damage  
206 was analyzed with confocal microscopy LSM 780 (Carl Zeiss, Germany). For each  
207 treatment at least 100 of DNA comets were randomly analyzed. Data processing was  
208 implemented with the Comet Assay IV (Instem, UK) software.

## 209 **2.8. Statistical analysis**

210 The data is expressed as the mean ± standard deviation. The Student's t-test was applied  
211 to measure statistical differences in the data. A p-value of less than 0.05 was regarded  
212 as statistically significant.

## 213 **3. Results**

### 214 **3.1. Physicochemical characterization of particles**

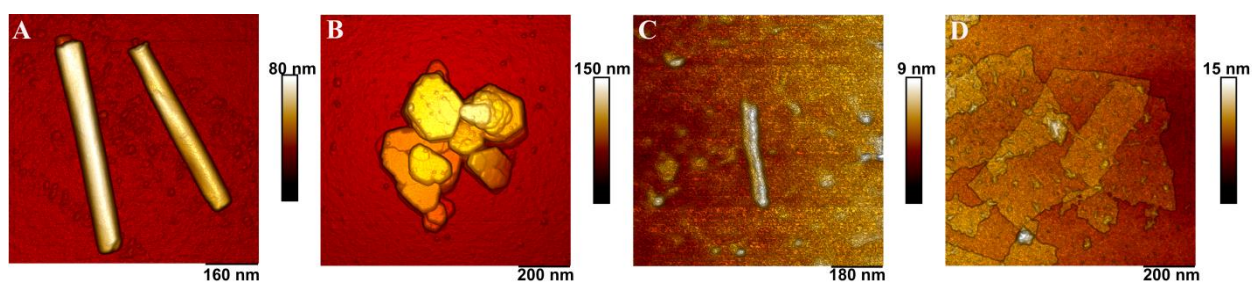
215 The effects of flat and tubular NPs on biological cells were analysed and compared in this  
216 study for different NPs. The study of electrophoretic mobility as well as the visualisation  
217 of nanomaterials using dark field microscopy allowed determination of the stability of the  
218 NP suspensions used and their dimensional characteristics (Table 1).

219 Table 1. **ζ-Potentials and sizes of nanoparticles measured by dynamic light scattering and**  
220 **AFM (Dispersions of the nanomaterials in deionized water were used for the**  
221 **measurements of ζ-Potentials and hydrodynamic diameters).**

Nanomaterial	Zeta potential (mV)	Size	
		DLS (d.nm)	AFM (nm)
Halloysite nanotubes	-31.8±3.7	310.5±4.1	626.5±176.4
Kaolinite	-31.5±0.6	753.1±34.9	526.9±206.8
Carbon nanotubes	-26.8±0.1	254.4±10.1	414.3±79.3
Graphene oxide	-48.6±2.4	1944±89.1	1065.8±251.5

222

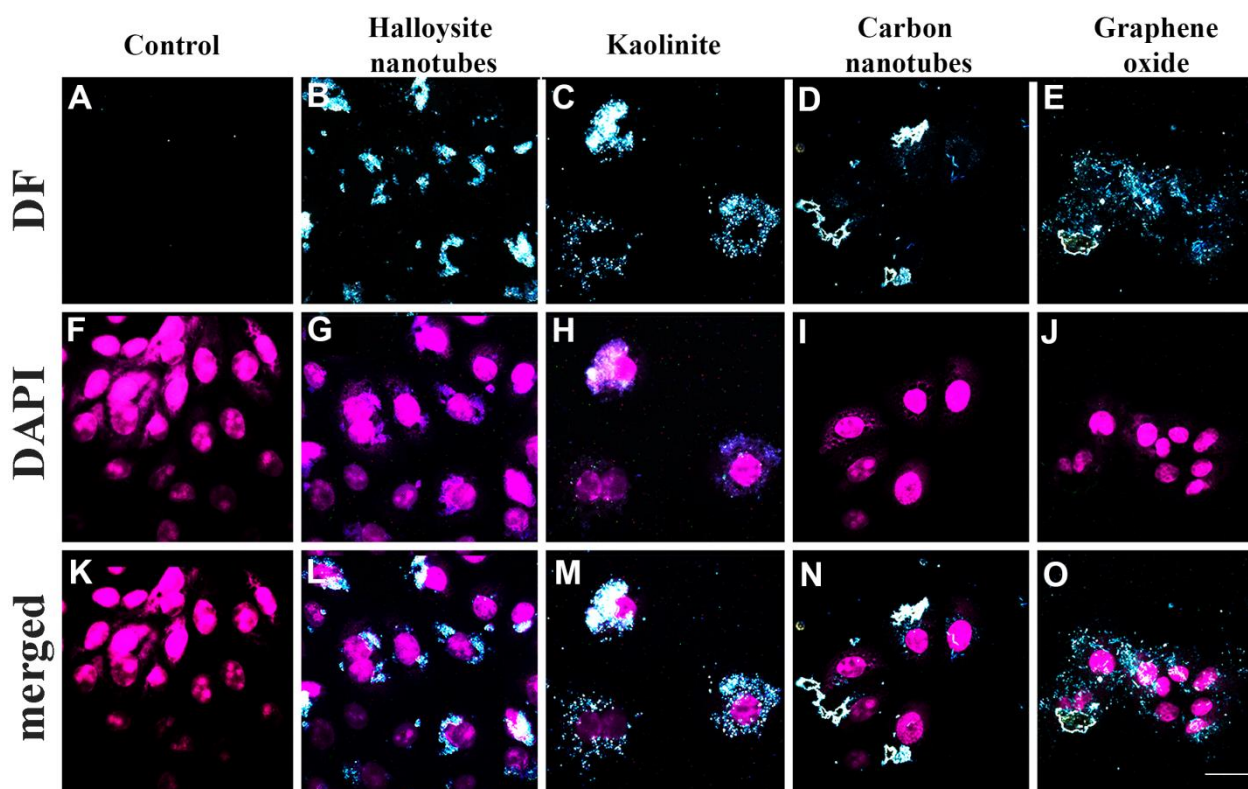
223 Carbon and clay nanotubes were similar in their size and zeta-potential. However, the  
 224 absolute value of the MWCNTs zeta-potential was lower than 30 mV, potentially  
 225 determining their lower colloidal stability. GO particles demonstrated the largest size and  
 226 the highest negative zeta-potential. It is hard to determine the real size of NPs using DLS  
 227 because the NPs tested here have different morphology. However, DLS did not reveal  
 228 any significant aggregation of NPs and the NP dimensions have further been probed  
 229 using AFM. The tubular morphology of halloysite and carbon nanotubes as well as platy  
 230 morphology of Kaol and GO particles was confirmed by AFM analysis (Figure 1).



231

232 **Figure 1.** AFM images demonstrating the morphology nanoclays and carbon  
 233 nanomaterials used in this study: HNTs (A); Kaol (B); MWCNTs (C); GO (D). All NPs were  
 234 prepared as water suspensions and further air-dried on clean glass surfaces.

235 Dark-field microscopy observations proved that the nanotubes and nanoplates were well-  
 236 dispersed and did not produce any aggregates during incubation with cells (Figure 2).



237

238 **Figure 2.** Dark-field (A-E), fluorescence (F-J) and merged dark-field and fluorescence  
 239 microscopy (K-O) images of NPs uptake by A549 cells after 24 h incubation. Control A549  
 240 cells (A, F, K) and A549 cells incubated with HNTs (B, G, L); Kaol (C, H, M); MWCNTs  
 241 (D, I, N); GO (E, J, O). The nuclei of cells were stained with DAPI (artificial color). Scale  
 242 bar is 25  $\mu$ m.

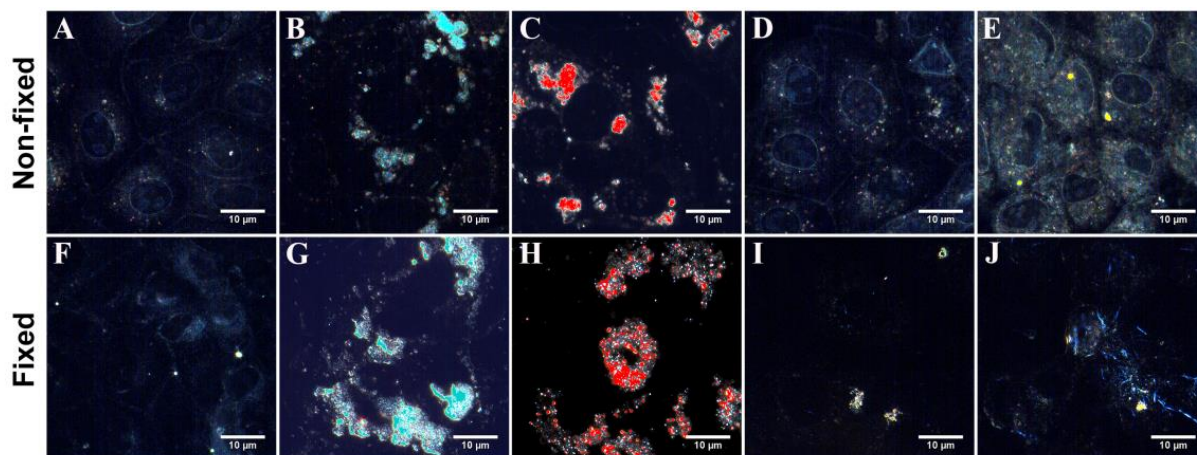
243 The dark-field microscopy is a convenient tool for visualisation and detection of  
 244 nanomaterials of different chemical nature and shape, based on registration of the  
 245 scattering signals of nanoparticles (Xu et al., 2020). Here, we managed to visualise the  
 246 carbon and halloysite nanotubes, kaolinite and graphene oxide in adherent A549 cells.

### 247 **3.2. Cell penetration and cytotoxicity of NPs**

248 Initially, we visualised the distribution of nanomaterials using dark-field microscopy. Then,  
 249 for each type of NPs, a hyperspectral profile of reflected light was obtained in the range  
 250 from 400 to 1000 nm, as described earlier (Akhatova et al., 2019) (Figure S1). The  
 251 reflectance spectra can be used as a signature allowing identification of specific NPs,

252 such as noble metal nanoparticles (Basnet et al., 2016), CNTs (Smith et al., 2014),  
253 graphene oxide (Kryuchkova et al., 2018) and nanoclays (Khodzhaeva et al., 2017) in  
254 biomaterials.

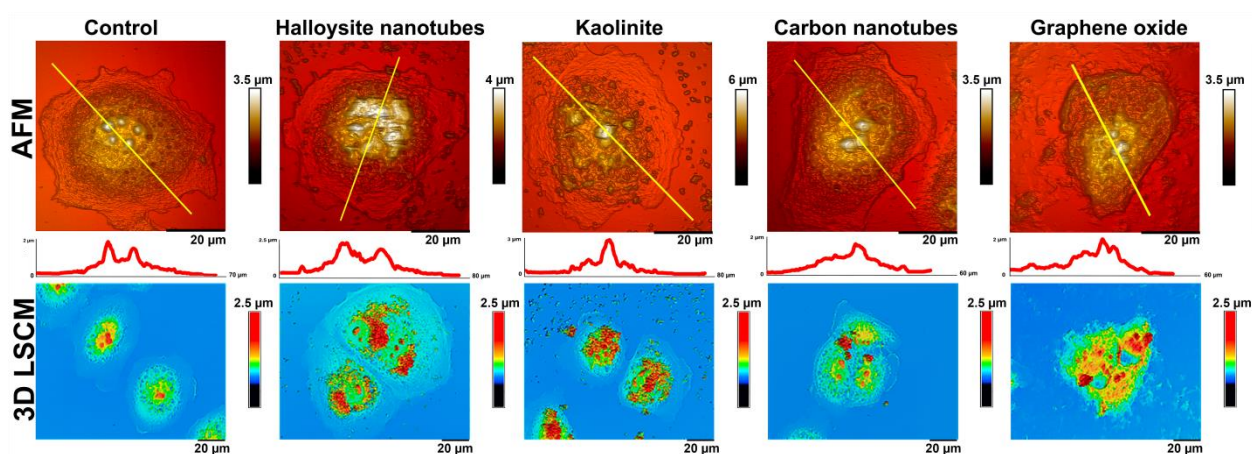
255 The intensity-normalised spectra from Figure S1 were then used to identify NPs in A549  
256 cells incubated for 24 h with NPs at concentration of  $100 \mu\text{g mL}^{-1}$  and fixed with  
257 paraformaldehyde. However, it was reported that cell fixation procedure itself can alter  
258 the NP interaction with cells (Richard et al., 2003). Therefore, cell penetration by NPs was  
259 additionally studied in non-fixed cells that were only washed three times with PBS to  
260 remove culture media and non-attached NPs. Similar results on NP localization were  
261 obtained for both fixed and non-fixed cells. The use of dark-field and hyperspectral  
262 microscopies revealed poor absorption of tubular MWCNTs and planar GO by A549 cells,  
263 in contrast to aluminosilicates with different surface geometries (Figure S2). Both planar  
264 and tubular forms of nanoclays were successfully visualised in the cell interior, but both  
265 types of carbon nanomaterials, despite the high intensity of the spectra, could hardly be  
266 identified in the cells. Before the analysis, the cells were thoroughly washed with a buffer  
267 three times in order to remove freely floating and weakly adhered to the cell surface  
268 aggregates of nanoparticles and analyze only those nanomaterials that were inside the  
269 cells or strongly interacted with the cell surface (Figure 3).



270

271 **Figure 3.** The mages of A549 cells obtained using dark-field and hyperspectral  
272 microscopy after 24 h of incubation with NPs: native cells (A, F); A549 cells incubated  
273 with halloysite nanotubes (B, G); kaolinite (C, H); carbon nanotubes (D, I); graphene oxide  
274 (E, J). Upper and lower rows of images correspond to non-fixed and fixed cells,  
275 respectively.

276 The changes in the morphology and roughness of cells after 24 h incubation with  
277 nanomaterials (at concentration of  $100 \mu\text{g mL}^{-1}$ ) were also investigated using AFM and  
278 3D LSCM (Figure 4). The combination of different microscopic methods allows obtaining  
279 more information on the interaction of NPs of various shapes and nature with cell  
280 membranes. While 3D LSCM is completely non-contact and better than AFM in terms of  
281 operability, it has lower measurement resolution and thus is less powerful than AFM in  
282 detecting nanoparticles present on the cell surface. Therefore, here we have applied both  
283 AFM and 3D LSCM to get insights of cell surface morphology both at microscale and  
284 nanoscale.

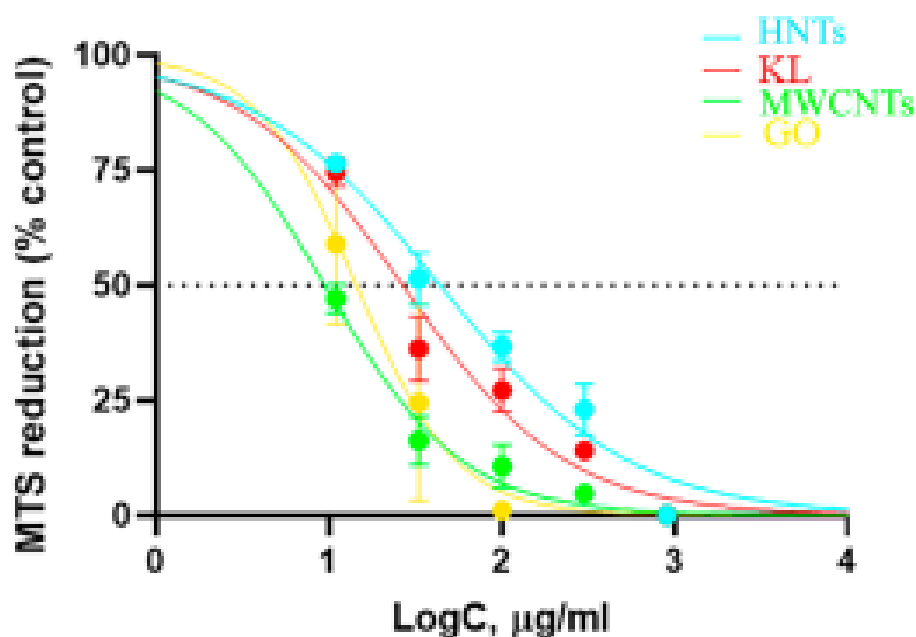


285  
286 **Figure 4.** Morphology of intact A549 cells (A, F) and A549 cells incubated with HNTs (B,  
287 G), Kaol (C,H), MWCNTs (D, I), GO (E,J ). Upper row of images shows the results  
288 obtained usinf AFM and the lower row by 3D LSCM. In between the images' rows, profiles  
289 taken along corresponding lines of the AFM images are presented.

290

291 Introduction of HNTs and Kaol into the incubation medium resulted in 2.23- and 1.86-  
292 times increase in the cell volume compared to the control experiment, respectively. After  
293 the introduction of MWCNTs and GO, a change in the cell volume of 1.68 and 1.14 times  
294 was observed, respectively. The data obtained can indicate the variable intensity of NP  
295 absorption by cells, as it was described previously for the increase in cell volume due to  
296 endocytosis of SPION (Zhou et al., 2018). Higher volume increase in the case of cell  
297 exposure to nanoclays points to their more efficient internalisation by cells; it is opposite  
298 to carbon nanomaterials which did not significantly affect the cell volume. However, the  
299 presence of carbon nanomaterials increased the cell surface roughness ( $R_a$  – average  
300 roughness) assessed using 3D-microscopy. The following  $R_a$  were obtained: A549 control  
301 cells ( $R_a=0.014\pm0.005 \mu\text{m}$ ), A549-MWCNTs ( $R_a=0.039\pm0.02 \mu\text{m}$ ), A549-GO  
302 ( $R_a=0.029\pm0.006 \mu\text{m}$ ). No statistically significant differences in cell surface roughness  
303 were observed between control cells and cells incubated with nanoclays: A549-HNTs  
304 ( $R_a=0.018\pm0.005 \mu\text{m}$ ), A549-Kaol ( $R_a=0.035\pm0.010 \mu\text{m}$ ), when calculated using the  
305 Student's t-test at the significance threshold  $P < 0.05$ .

306 To assess the cytotoxic potential of the studied nanomaterials, we evaluated the  
307 relationship between the applied dose of NPs and the viability of cells after 24 h incubation  
308 with nanomaterials. This was done using the MTS test with 3-(4,5-dimethylthiazol-2-yl)-  
309 5-(3-carboxymethoxy-phenyl)-2-(4-sulfophenyl)-2H-etrazolium inner salt (Figure 5).



310

311 **Figure 5.** The reduction of MTS by A549 cells after 24 h incubation with NPs. All NPs  
 312 show a decrease in MTS reduction by cells in a dose-dependent manner with semi-  
 313 inhibitory concentrations indicated by a dotted line. Error bars represent the standard  
 314 deviation of three parallel and independent tests.

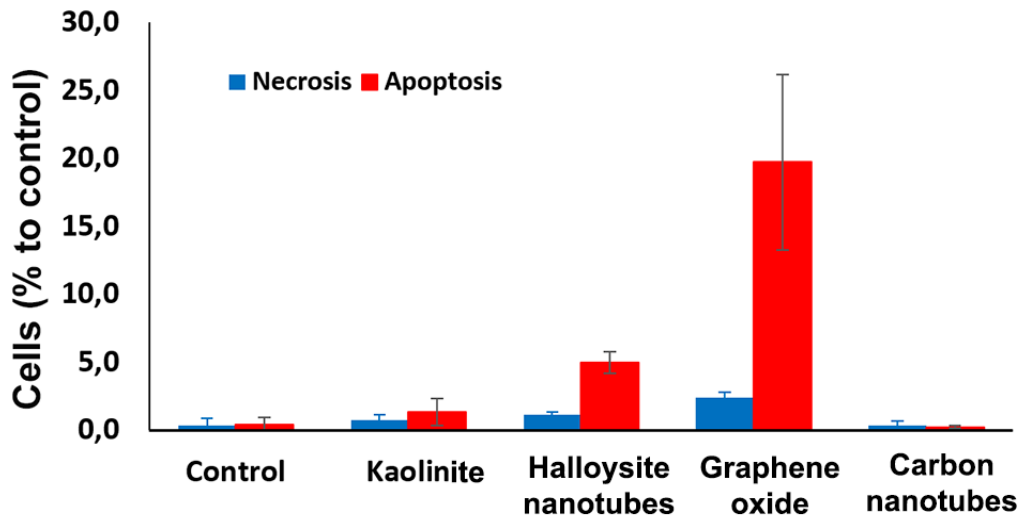
315

316 The dose-dependent inhibiting effect of all the studied types of nanomaterials was  
 317 revealed and IC<sub>50</sub> for each nanomaterial type was determined. MWCNTs and GO were  
 318 found to be the most toxic nanomaterials for cells. A semi-inhibitory concentration of  
 319  $9.4 \pm 0.9 \mu\text{g ml}^{-1}$  for MWCNTs and  $14.4 \pm 0.9 \mu\text{g ml}^{-1}$  for GO was found, compared to  
 320  $43.69 \pm 2.30 \mu\text{g mL}^{-1}$  for HNTs and  $26.6 \pm 1.1 \mu\text{g mL}^{-1}$  for Kaol, which indicates a lower  
 321 toxicity of aluminosilicates for A549 cells, in comparison with carbon materials.  
 322 Additionally, MWCNTs were more toxic than GO plates according to the results of MTS  
 323 test.

324 However, the rate of tetrazolium reduction depends on viable cell number (which is  
 325 determined by both cell death and cell proliferation level) and general metabolic activity  
 326 of cells (Berridge and Tan, 1993; Berridge et al., 2005). Thus, cell viability data obtained

327 by MTS assay must be corroborated by a more direct viability probing method such as  
328 flow cytometry. Additionally, using flow cytometry and cell staining with annexin and  
329 propidium iodide, the mechanism of the toxic effect of the studied nanomaterials can be  
330 evaluated (Figure 6).

331



332

333 **Figure 6.** Effect of carbon and clay nanomaterials on cell viability assessed by flow  
334 cytometry. The fraction of apoptotic and necrotic cells is presented as a percentage to a  
335 total cell number.

336 According to the flow cytometry data, MWCNTs did not induce cell death and apoptosis  
337 at the concentration of  $100 \mu\text{g mL}^{-1}$ . However, the cell death is not the only indicator of  
338 cellular dysfunction and thus nanomaterial toxicity to cells. MWCNTs significantly  
339 inhibited the reduction of tetrazolium by cells in MTS assay, which implies the negative  
340 impact of carbon nanotubes on the cell proliferation or metabolic activity. As the rate of  
341 tetrazolium reduction depends on viable cell number and general metabolic activity, it can  
342 be concluded that a high cytotoxic effect of MWCNT demonstrated in the MTS assay was  
343 not associated with cell death, but was rather due to a decrease in cell metabolic activity  
344 or proliferation.



345 Another reason of the discrepancy between the results of cell viability assessment by a  
346 colourimetric test and flow cytometry can be related with CNT interaction with indicator  
347 dyes. A fake strong cytotoxic effect of CNT within the MTT assay was observed previously  
348 in CNT treated A549 cells (Wörle-Knirsch et al., 2006), which was related to a reduction  
349 in MTT-formazan content in solution because of formation of insoluble MTT-formazan  
350 crystals covering the nanotubes. The authors did not find a similar effect when using  
351 water-soluble MTT analogues (like WST-1) and recommended water-soluble dyes for cell  
352 viability testing in the presence of carbon nanotubes (Wörle-Knirsch et al., 2006). MTS,  
353 used in our study, is another water-soluble analogue of MTT, which was previously  
354 applied for assessment of CNT cytotoxicity (Guo et al., 2008; Meindl et al., 2013).  
355 However, even water soluble MTT analogues (WST-1) can interact with CNTs, which may  
356 result in false positive toxic effect similar to that observed in the MTT assay (Casey et al.,  
357 2007). Moreover, the authors concluded that a whole range of indicator dyes (Coomassie  
358 Blue, Alamar Blue TM, Neutral Red, MTT and WST-1) were not appropriate for the  
359 quantitative toxicity assessment of carbon nanotubes because of nanotubes interaction  
360 with the dyes, resulting in the reduction of the associated absorption/fluorescent emission  
361 (Casey et al., 2007). Thus, using only colourimetric assays is obviously not enough for  
362 evaluating the cytotoxicity of carbon nanotubes.

363 In case of GO, high cytotoxicity observed in MTS test was confirmed by flow cytometry  
364 data. The highest proportion of dead (primarily apoptotic) cells was detected after the  
365 addition of graphene oxide, which coincides with the earlier data (Rozhina et al., 2019).  
366 The tubular nanoclay induced a higher rate of cell death compared to the platy one,  
367 according to the flow cytometry data, but the inhibition of tetrazolium reduction was higher  
368 in case of kaolinite, evidencing lower proliferation and/or cell metabolic activity in the  
369 presence of platy nanoclays.

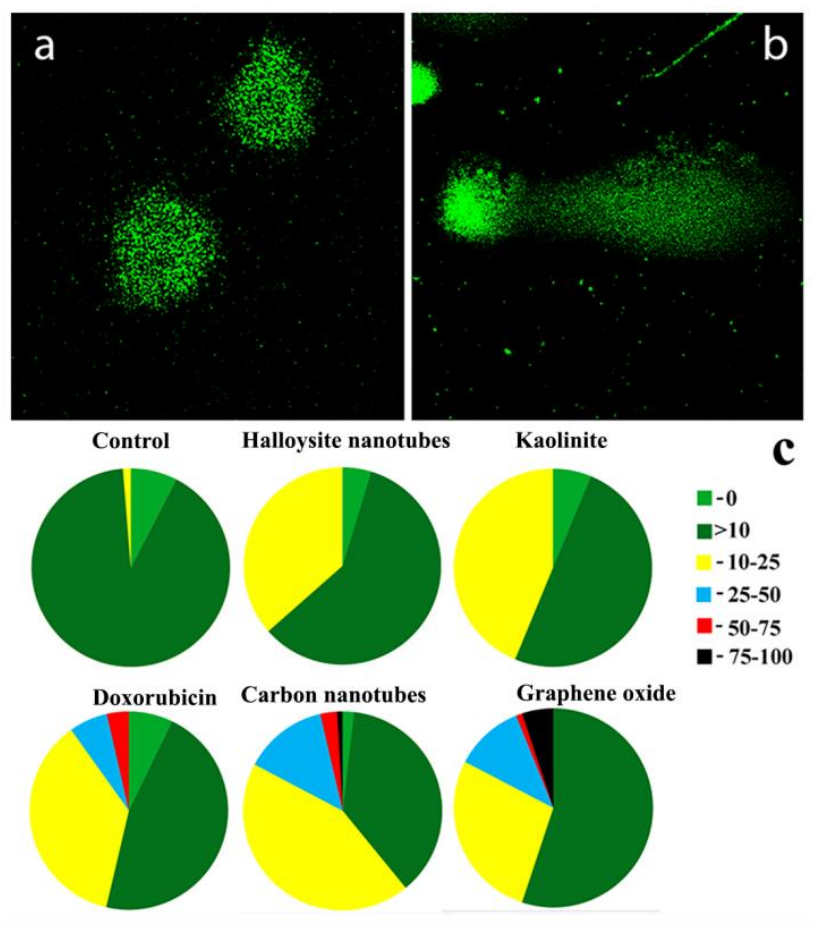
370

### 371 **3.3. Genotoxicity of carbon and clay nanoparticles**

372

373 Next, the genotoxicity of nanomaterials was investigated using the DNA-Comet assay  
374 (Figure 7). Comet assay (single cell gel electrophoresis assay) is a sensitive and effective  
375 method for analyzing DNA damage in cells (Dhawan et al., 2009) and it is the most used  
376 assay in assessing the genotoxic potential of nanomaterials (Azqueta and Dusinska,  
377 2015). In this method DNA damage becomes visible as a "tail" of DNA fragments  
378 migrating in an electric field away from the undamaged DNA remaining within the  
379 nucleoid. Analysis of the intensity of the comet tail relative to the nucleoid is related to the  
380 number of DNA breaks that have occurred in a particular cell. By counting the relative  
381 intensity of tail and nucleoid in 100 cells per sample, we evaluated the percentage of DNA  
382 damage in each sample. The percentage of DNA damage was presented as a diagram,  
383 where 100 is a maximal DNA content in "tail" and 0 is an absence of DNA damage (Figure  
384 7, C). As a positive control the doxorubicin ( $2 \text{ mg mL}^{-1}$ ) was used, which induces specific  
385 oxidative damage of DNA.

386



387

388

389 **Figure 7.** DNA damage in cells after 24 h incubation with carbon and clay nanomaterials  
 390 assessed by the Comet assay. Images of typical "comets" representing intact DNA (a)  
 391 and damaged DNA (b). Circular charts (c) displaying fractions of cells with various  
 392 degrees of DNA damage (100 - maximal DNA content in the comet tail, 0 – no tail).  
 393 Doxorubicin was used as a positive control.

394 The minimal cell DNA damage was observed after introduction of kaolinite and halloysite  
 395 ( $100 \mu\text{g mL}^{-1}$ ) into the cultivation medium. The introduction of GO and MWCNTs led to an  
 396 increase in the degree of DNA degradation, while in control, DNA damage was less than  
 397 10%. As can be seen in the graph, the addition of GO to the medium led to an almost  
 398 complete degradation of DNA in some cells. Thus, both forms of natural nanoclay (planar  
 399 and tubular) turned out to be the least genotoxic for cells.

400

#### 401 **4. Discussion**

402 The morphology of NPs, their size and chemical nature are known to play important roles  
403 in the delivery of therapeutic agents (Wang et al., 2018). Despite the widespread use of  
404 nanoscale materials in various fields, there are numerous reports of their side effects on  
405 biological systems and cell compartments. According to results obtained in this study,  
406 both platy and tubular carbon nanomaterials possess higher general toxicity than  
407 nanoclays for A549 cells. To date, there is a lot of inconsistency in the published results  
408 on MWCNTs toxicity studies due to permutations in NP dimensions, composition and  
409 surface chemistry, cell lines, concentration, time points and assays used (Nerl et al.,  
410 2011). The data on the toxicity and genotoxicity of GO are also quite contradictory; there  
411 are reports of both low toxicity of GO (Bengtson et al., 2016) and its significant toxicity for  
412 different types of cells such as stem cells, germ cells, lung cells, skin cells, endothelial  
413 cells and macrophages (Akhavan et al., 2012; Pelin et al., 2017; Ali et al., 2018;  
414 Gurunathan et al., 2019).

415 It is suggested that the toxic effect of NPs can correlate with their ability to penetrate into  
416 the cells (Sun et al., 2019). The surface charge of nanomaterials can affect their  
417 internalization: positively charged nanomaterials are internalized by cells to a greater  
418 extent than are neutral and negatively charged ones (Cho et al., 2009; Sun et al., 2019).  
419 Negatively charged membrane proteins directly or indirectly associated with cytoskeleton  
420 actin filaments interact with positively charged NPs resulting in NP absorption due to the  
421 retrograde motion of microvilli (Orr et al., 2007). According to the zeta-potential data, all  
422 the particles used in the present study were negatively charged. However, only clay  
423 nanoparticles were readily internalized by cells, while hyperspectral mapping failed to  
424 locate carbon nanomaterials inside the cells. The preferential presence of MWCNTs and  
425 GO on the cell outside was supported by insignificant changes in cell volume

426 accompanied by increased cell surface roughness found in AFM and 3D microscopy  
427 studies.

428 Despite the abundance of information on the uptake of nanomaterials by cells, a detailed  
429 mechanism of adsorption is not known (Iversen et al., 2011; Sahay et al., 2010). In the  
430 study of the transport mechanisms of HNTs in A549 cells it was found that FITC-labeled  
431 HNTs were readily internalized into A549 by both clathrin- and caveolae-dependent  
432 endocytosis, and the transport pathway of HNTs is an actin- and microtubule-associated  
433 process via Golgi apparatus and lysosome (Liu et al., 2019). CNTs can be absorbed  
434 through clathrin and/or caveolae-mediated endocytosis/phagocytosis pathway (Verma et  
435 al., 2008). The authors of a recent comparative study of MWCNTs and HNTs in cultured  
436 endothelial cells and blood vessels concluded that MWCNTs were possibly internalized  
437 via clathrin-mediated endocytosis, whereas HNTs were absorbed via energy-dependent  
438 non-endocytic uptake (Wu et al., 2020). The less efficient MWCNTs uptake by cells in our  
439 study can be explained by both different sizes of the nanotubes (the measured MWCNT  
440 hydrodynamic size in the cited study was lower than in our study and averaged around  
441 179.5 nm in water) and cell-specific differences.

442 The penetration of GO particles can also depend on the cell type. In this work, we  
443 observed a low absorption of GO nanoparticles by A549 cells, while GO particles were  
444 reported in HCT116 cells and rat skin fibroblasts (Rozhina et al., 2019) as well as in  
445 human fibroblast cells (Wang et al., 2010). The absence of GO inside A549 cells was  
446 previously mentioned by other researchers (Chang et al., 2011), and the authors  
447 suggested that GO interacted with cells on the cell surface or indirectly through other  
448 pathways, and partially blocked metabolism in A549 cells. Carbon nanomaterials are  
449 prone to agglomeration when prepared without dispersant, which can explain the  
450 variability in penetration and toxicity effects observed in different studies (Simon-Deckers  
451 et al., 2008), as well as disturbances in the carbon nanotube dose-effect curve (Hirano et

452 al., 2008). High cytotoxic effect of MWCNTs at low concentrations was observed when  
453 penetration of MWCNTs to A549 cells was achieved by dispersing the nanotubes using  
454 Arabic gum (Simon-Deckers et al., 2008) or gelatin (Magrez et al., 2006). Oppositely, no  
455 acute toxicity on cell viability (WST-1, PI-staining) upon incubation with aggregated  
456 MWCNTs was observed, but a dose- and time-dependent increase of intracellular  
457 reactive oxygen species (ROS) and decrease of the mitochondrial membrane potential  
458 were registered (Pulskamp et al., 2007).

459 Despite the pronounced internalization of nanoclays by cells, nanoclays demonstrated  
460 low cytotoxicity in a colorimetric MTS test which was confirmed by flow cytometry data.  
461 Very low toxicity of HNTs was evidenced by many years of research (Vergaro et al.,  
462 2012). Platy K particles were previously found to be non-toxic for *Paramecium caudatum*  
463 and cancer cell lines and even capable of decreasing the toxicity of GO nanosheets to  
464 cells during joint incubation (Kryuchkova et al., 2016; Rozhina et al., 2019). Both clay  
465 nanoparticles induced a slight DNA damage, and the tubular nanoclay demonstrated less  
466 DNA damaging potency than the platy one. The %tail DNA values found previously in  
467 different studies for kaolinite treated cells depended not only on the cell type and the Kaol  
468 concentration, but also on the size and morphology of platy Kaol particles (Kato et al.,  
469 2017; Kawanishi et al., 2020). Thus, one-hour treatment with Kaol particles increased  
470 DNA damage in Chinese hamster ovary CHO AA8 cells and in human primary epidermal  
471 keratinocytes and fibroblasts, with Kaol nanoparticles (200 nm) having higher DNA  
472 damaging potency and inducing more ROS than Kaol microparticles (4.8 µm) (Kawanishi  
473 et al., 2020). Although the low direct genotoxicity of platy Kaol particles towards A549  
474 cells was observed previously (Kato et al., 2017), DNA damaging capacity of Kaol  
475 particles to lung cells may be increased *in vivo* (Totsuka et al., 2009; 2011) by Kaol  
476 interaction with macrophage cells (Kato et al., 2017).

477 The introduction of MWCNTs and GO into the incubation medium led to maximum  
478 damage to DNA strands in the cells. Moreover, platy GO nanoparticles were found to be  
479 the most toxic to A549 cells according to both MTS and flow cytometry data. A high  
480 percentage of apoptosis in GO-treated cells was supported by a high degree of DNA  
481 damage induced by GO treatment. DNA damage observed in case of CNT treatment did  
482 not result in increased apoptosis, indicating that the DNA lesions were probably not  
483 irreparable in this case; otherwise they would trigger apoptotic cell death (Norbury and  
484 Zhivotovsky, 2004).

485 The alkaline Comet assay allowed us to assess the general genotoxicity of nanomaterials  
486 while further researches are needed to determine the mechanisms of DNA damage in the  
487 presence of various nanomaterials. There are two variants of the Comet assay: the  
488 neutral and the alkaline one. The alkaline Comet assay is applied to detect DNA single  
489 strand breaks, double strand breaks and alkali labile sites, while the neutral assay detects  
490 double strand breaks. However, the double-strand break specificity of the neutral Comet  
491 assay was put into doubt because the appearance of a DNA segment either in the tail or  
492 head of the comet is essentially determined by the relaxation of DNA supercoils and  
493 extension of DNA loops, which do not depend on pH (Collins et al., 2008). Instead, such  
494 methods as the analysis of foci produced by phosphorylated histone 2A family member  
495 X ( $\gamma$ -H2AX) and tumor suppressor p53 binding protein 1 (53BP1) by  
496 immunofluorescence microscopy can be applied to detect double-strand breaks of DNA  
497 (Rothkamm et al., 2015).

498 It is likely that the observed DNA damage was associated with the formation of ROS in  
499 the presence of carbon nanomaterials in cell media. It was shown that G and GO  
500 nanosheets caused DNA damage by generating ROS both in cells and in zebrafish larvae  
501 (Lu et al., 2017). Numerous studies have shown that CNT can induce ROS generation in  
502 multiple cell lines and activation of ROS-related intracellular signaling pathways

503 (Shvedova et al., 2012; Clift et al., 2014). GO induced genotoxicity in normal lung  
504 fibroblast cells assessed using the Comet assay at concentration as low as  $1\mu\text{g mL}^{-1}$   
505 (Wang et al., 2013). MWCNTs also induced DNA damage (according to the results of the  
506 Comet assay and Micronuclei assay) and cytotoxicity in healthy male human peripheral  
507 blood lymphocytes, associated with elevated intracellular ROS level (Kim et al., 2016).  
508 MWCNTs were found to be more cytotoxic and genotoxic for immortalized Chinese  
509 hamster lung fibroblast V79 cell line and SHE (Syrian hamster embryo) cells than single-  
510 walled and double-walled carbon nanotubes, and genotoxicity was seen to increase with  
511 CNT width (Darne et al., 2014). In addition, it was reported that CNTs can adsorb nutrients  
512 from the medium, resulting in serious toxicity to HepG2 cells (Guo et al., 2008). This effect  
513 was not observed for GO, when it was introduced into the A549 cell incubation medium  
514 (Chang et al., 2011).

515 Thus, despite the lower cell penetration of carbon nanomaterials, they had a higher  
516 cytotoxic and genotoxic effect than tubular and platy nanoclays. Induction of intracellular  
517 oxidative stress is a key event in the toxic effect of nanomaterials (Sharifi et al., 2012). **It**  
518 **was demonstrated that GO can cause a dose-dependent oxidative stress in A549 cells**  
519 **even without entering the cells, by inducing generation of reactive oxygen species in**  
520 **culture medium, which then promotes ROS production inside cells (Chang et al., 2011).**

521 In turn, oxidative stress caused by particle exposure can trigger a cascade of responses,  
522 for example, stimulate an increase in the concentration of cytosolic calcium (Brown et al.,  
523 2007) or induce translocation of transcription factors (e.g., NF- $\kappa$ B), regulating anti-  
524 inflammatory genes such as TNF- $\alpha$  and iNOS, into the nucleus (Castranova, 2004).  
525 Excessive oxidative stress can also alter proteins, lipids, and nucleic acids, which further  
526 stimulates the antioxidant defense systems or lead to cell death as a result of apoptosis,  
527 necrosis, or inflammatory reactions (Simm and Brömme, 2005; Samuel et al., 2020).

## 528 **5. Conclusion**



529 The purpose of this study was to compare the absorption and cytotoxic effects in lung  
530 cancer cells (A549) of four commonly used nanomaterials: carbon nanomaterials  
531 (MWCNT and GO) and aluminosilicates (HNT and Kaol). This allows determination of  
532 NPs which are the most suitable for use as a carrier system for the delivery of therapeutic  
533 agents. All nanomaterials evoked some cytotoxic effects in cells, but the mechanisms of  
534 cytotoxicity varied depending on the type of nanomaterial. Despite the lower cell  
535 penetration of carbon nanomaterials, they had higher cytotoxic and genotoxic effects,  
536 while aluminosilicates were actively absorbed by cells without causing serious damage.  
537 Generally, for a certain nanomaterial, the higher its cell penetration, the higher the  
538 cytotoxic effect. But when different nanomaterials are compared, the relative toxicity of a  
539 nanomaterial is influenced by various factors such as the nanomaterial shape, size and  
540 surface chemistry (Sun et al., 2019). As the shapes and sizes of clay and carbon  
541 nanoparticles were similar, the higher toxicity of carbon nanomaterials was probably  
542 related to their surface chemistry. Although the penetration of carbon nanomaterials was  
543 negligible, single CNTs and GO particles were still detected inside cells. We suggest that  
544 even this low penetration of carbon nanomaterials was enough to cause some toxic  
545 effects, while a much higher penetration of clay nanoparticles was safer to cells. The  
546 lower toxicity of the nanoclays allows for considering aluminosilicates of different  
547 morphologies as perspective candidates for the delivery of drug compounds or  
548 nucleotides. However, *in vitro* assays are only a necessary early step in screening NP  
549 cytotoxicity due to their speed, convenience and low cost in comparison with *in vivo* tests  
550 (Fard et al., 2015). After finding the safest nanoparticulate candidates for drug delivery in  
551 preliminary screenings, more complex studies are required, including co-culture models,  
552 3D models and eventually *in vivo* assays, because the interaction with serum proteins  
553 and formation of a "protein corona" can dramatically change NP properties. At the same

554 time, the interaction of NPs with immune cells, patrolling most of the body parts, can  
555 cause unexpected effects, not foreseen in *in vitro* studies.

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559

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563

#### 564 **Declaration of Competing Interest**

565 The authors declare no conflict of interest.

566

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