

This is a provisional PDF only. Copyedited and fully formatted version will be made available soon.



ISSN: 0015-5659

e-ISSN: 1644-3284

Morphometrical features of left atrial appendage in the AF patients subjected to left atrial appendage closure

Authors: K. M. Slodowska, J. Batko, J. P. Holda, D. Dudkiewicz, M. Koziej, R. Litwinowicz, K. Bartus, M. K. Holda

DOI: 10.5603/FM.a2022.0080

Article type: Original article

Submitted: 2022-07-14

Accepted: 2022-08-19

Published online: 2022-08-25

This article has been peer reviewed and published immediately upon acceptance. It is an open access article, which means that it can be downloaded, printed, and distributed freely, provided the work is properly cited.

Articles in "Folia Morphologica" are listed in PubMed.

Morphometrical features of left atrial appendage in the AF patients subjected to left atrial appendage closure

K.M. Słodowska et al., Morphology of LAAs subjected to closure

K.M. Słodowska¹, J. Batko¹, J.P. Hołda¹, D. Dudkiewicz¹, M. Koziej¹, R. Litwinowicz², K. Bartuś², M.K. Hołda^{1,3}

¹Heart Embryology and Anatomy Research Team (HEART), Department of Anatomy, Jagiellonian University Medical College, Krakow, Poland

²Department of Cardiovascular Surgery and Transplantology, Jagiellonian University Medical College, Krakow, Poland

³Division of Cardiovascular Sciences, The University of Manchester, United Kingdom

Address for correspondence: M.K. Hołda, MD, PhD, DSc, Heart Embryology and Anatomy Research Team (HEART), Department of Anatomy Jagiellonian University Medical College, Kopernika 12, 31-034 Kraków. Poland, tel/fax: +48 12 422 95 11, e-mail: mkh@onet.eu

ABSTRACT

Background: This study aimed to evaluate the morphometrical features of left atrial appendage (LAA) in patients with atrial fibrillation, subjected to left atrial appendage percutaneous closure (LARIAT) for stroke prevention.

Materials and methods: Computed tomography (CT) scans of 51 patients with atrial fibrillation subjected to LARIAT procedure were comparatively evaluated with 50 patients with sinus rhythm (control group). Three-dimensional (3D) reconstructions were created using volume-rendering for evaluation.

Results: No differences were found in LAA types of distribution (cauliflower: 25.5 vs. 34.0%, chicken wing: 45.1 vs. 46.0%, windsock: 29.4 vs. 20.0%, all $p>0.05$) between groups. However, the study group was characterized by LAAs with a lower number of lobes. The LAA orifice anteroposterior and transverse diameters (19.3 ± 4.12 vs. 17.2 ± 4.0 mm, $p=0.01$ and 25.1 ± 5.1 vs. 20.5 ± 4.4 mm, $p=0.001$), orifice area (387.2 ± 133.9 vs. 327.1 ± 128.3 mm², $p=0.02$)

and orifice perimeter (70.2 ± 12.5 vs. 61.2 ± 11.6 mm, $p=0.04$) was significantly larger in atrial fibrillation patients. More oval LAA orifices was found in atrial fibrillation group (94.0 vs. 70.4%, $p=0.001$). No statistically significant differences were found in LAA body length (47.4 ± 15.4 vs. 43.7 ± 10.9 mm, $p=0.17$), body width (24.7 ± 5.6 vs. 24.4 ± 5.8 mm, $p=0.81$), and chamber depth (17.7 ± 3.5 vs. 16.5 ± 3.8 mm, $p=0.11$). Calculated LAA ejection fraction was significantly lower in study group compared to healthy patients (16.4 ± 14.9 vs. $48.2 \pm 12.9\%$, $p=0.001$).

Conclusions: Important morphometrical differences in LAA orifice have been found, which was significantly larger and more oval in patients with atrial fibrillation compared to healthy controls. Although no difference in LAA body type and size was observed; the LAA ejection fraction was significantly lower in atrial fibrillation rhythm patients.

Key words: left atrial appendage closure, LAA shape, atrial fibrillation, stroke

INTRODUCTION

The left atrial appendage (LAA) is a small, irregular shape structure, outpouching from the left atrium of the heart [23]. LAA is a remnant of the primitive atrium developed in early gestation. It is proven that LAA takes part in the regulation of volume homeostasis through its mechanical function and neurohormonal secretion [12]. Moreover, the LAA is a well-established source of cardiac thrombogenesis and arrhythmogenesis [20]. For more than half of a century, the LAA is considered a primary source of cardioembolic events in patients with atrial tachycardia (atrial fibrillation) [28]. Numerous morphological features of the LAA, which include multilobular and trabeculated structure and small orifice with a narrow neck, predispose to turbulent blood flow and local blood stasis, thereby increasing the risk for thrombosis [20,21]. Nevertheless, no consensus was reached as to which specific LAA morphometric features increased the risk of thrombogenicity.

Anticoagulation therapy is a standard of care to prevent cardioembolic stroke in patients with atrial fibrillation [14]. In patients with a high risk of bleeding, contraindications to anticoagulants, intolerance, or low patient compliance the LAA closure was proposed as an alternative approach to eliminate cardioembolic stroke risk [11]. This led to the development of several surgical and percutaneous approaches to close/exclude the LAA based on three concepts: plug, pacifier principle, and ligation [4]. Among the ligation techniques, the LARIAT (SentreHEART, Inc., Redwood City, CA, USA) procedure is a distinguished

percutaneous adaptation of the surgical exclusion of LAA with a suture, used as an alternative to open-heart surgery [2]. Although the LARIAT procedure can be performed effectively with acceptably low complications, some short- and long-term complications of the intervention may occur [16]. The frequency of peri- and post-procedural complications can be lowered by adequate patients selection thanks to computed tomography (CT) evaluation of the LAA shape and size and detailed pre-procedural planning [26]. Morphology of the LAA can significantly affect pathophysiological properties of the LAA, choice of closure technique, the course of the procedure, its results, and complications [4, 23]. The present study aims to compare the LAA morphometrical features between patients with atrial fibrillation subjected to left atrial appendage percutaneous closure using LARIAT device and sinus rhythm patients using cardiac CT.

MATERIALS AND METHODS

The current study was conducted at the Department of Anatomy and the Department of Cardiovascular Surgery and Transplantology at the Jagiellonian University Medical College, Cracow, Poland. The study was conducted according to the principles expressed in the 1975 Declaration of Helsinki and was approved by the Bioethical Committee of the Jagiellonian University in Cracow, Poland (No. 1072.6120.4.2020).

Study population

The study evaluated 101 contrast-enhanced electrocardiograms (ECG) gated CT scans of hearts of which 51 were of consecutive adult patients with atrial fibrillation and who underwent percutaneous closure of the LAA with the LARIAT device (41.2% females, mean age of 61.0 ± 10.35 years) (study group). The CT scans were performed prior to the LARIAT procedure. The remaining 50 scans (control group) were of randomly selected adult patients subjected to non-invasive coronary arteries evaluation (50% females, mean age of 57.8 ± 14.45 years) of which inclusion criteria were: no history of ischemic stroke, no atrial fibrillation, and absence of any significant structural heart defects. All sample patients gave written informed consent. The medical history of all included patients was reviewed, and the following data were extracted: sex, age, body mass index, existing comorbidities (i.e., hypertension, hyperlipidemia, chronic heart failure, coronary artery disease, chronic

obstructive pulmonary disease, diabetes mellitus, history of stroke, and history of myocardial infarction), heart rhythm status, and the medication's usage. The following scores were calculated: Canadian Cardiovascular Society (CCS) grading of angina pectoris and New York Heart Association (NYHA) Functional Classification and CHA₂DS₂-VASc Score for Atrial Fibrillation Stroke Risk.

Cardiac computed tomography

Every patient underwent a per-protocol contrast-enhanced ECG gated CT scan. All scans were performed in sinus rhythm. If the patient's heart rate was over 70 bpm before the cardiac CT examination, the patient was administered 10 or 40 mg of propranolol or 40 mg of verapamil, depending on the physician's recommendation. The examination was performed using a 64-row dual-source scanner (Siemens, Erlangen, Germany). The image acquisitions were collected during a deep inspiration breath-hold. The imaging parameters for dual-source CT were: a tube voltage of 100–120kV and an effective tube current of 350–400 mA. The collimation and temporal resolution were $2 \times 32 \times 0.6$ mm and 165 ms, respectively. The time of arrival of the contrast agent to the ascending aorta was determined at the level of the tracheal bifurcation and achieved with the test bolus method. Then, the 15 ml of contrast agent was infused, which was followed by 20 ml of saline. The contrast agent was injected at a dose of 1.0ml/kg at a rate of 5.5ml/s followed by a 40 ml saline chaser with the same infusion rate. In the test bolus, the acquisitions delay was the time of maximum density of the ascending aorta with an additional 6 s of delay. Images were reconstructed with a B26f and B46f kernel and an image matrix of 512×512 pixels. A multiphase reconstruction (from 10% to 100%) was done. Moreover, 30% (left ventricle end-systole) and 70% (left ventricle end-diastole) image reconstructions were evaluated. Then, the initial quality check was performed using multiplanar reconstructions.

Image postprocessing and analysis

Postprocessing analyses of CT scans were performed on dedicated workstations (Dell, USA). Three-dimensional (3D) reconstructions of the heart subcomponents (LAA, left atrium, and left ventricle) were created using volume-rendering and segmentation techniques using Innovation Suite 23 (Materialise, Belgium) software in both end-diastolic and end-systolic cardiac phases. Manual and semi-automatic methods of segmentation were used. Next, raw

data and visualizations were subjected to multidirectional morphological and morphometrical analyses.

First, two independent, blinded to patients history investigators classified LAA based on its shape into one of the three groups: cauliflower, chicken wing, or windsock as discussed previously (Figure 1) [23]. Additionally, some individual lobes have been established. The LAA orifice and body were measured on the 3D reconstructions in the end-diastolic phase of the heart using virtual calipers (Figure 2). Orifice shape, dimensions, area, and perimeter were measured. In addition, the maximal LAA body length (from orifice to the most far point) and width (in the widest point at the LAA base) were obtained. Depth of the LAA chamber was measured as a distance from the orifice plane to the last perpendicular and the orifice plane. For the chicken wing type, the angle of the bend and lengths from orifice to bend and from the bend to the LAA apex were also evaluated. The main dimensions of the left ventricle and atrium were estimated. The volume of the LAA left atrium and the left ventricle was measured in end-diastolic and end-systolic cardiac phases. Then, ejection fractions of the above-mentioned chambers were calculated.

To reduce human bias, all measurements were recorded by two independent, blinded to patients history investigators. If results between the two researchers varied by more than 10%, both measurements were repeated. The mean of the two new values was calculated and reported as the final value.

Statistical analyses

Data are shown as mean values with corresponding standard deviations (\pm SD) or in percentages. The Shapiro–Wilk test was used to determine if the quantitative data were normally distributed, and Levene's test was performed to verify a relative homogeneity of variance. The Student t-tests, Wilcoxon signed-rank tests, and the Mann–Whitney U tests with Bonferroni corrections were used to conduct statistical comparisons. The non-parametric Kruskal–Walli's test was used to compare values between groups. Bonferroni correction was applied because of multiple comparisons. Correlation coefficients were calculated to assess whether there was a statistical dependence between the analyzed parameters. A p-value lower

than 0.05 was considered statistically significant. Statistical analyses were performed using StatSoft STATISTICA 13.3 software for Windows (StatSoft Inc., Tulsa, OK, USA).

RESULTS

Clinical characteristics of studied patients are presented in Table 1. Among the study group, 29.4% of patients had a history of ischemic stroke. Arterial hypertension was more common in the study group than in control subjects (90.2 vs. 38.0%, $p < 0.001$). The clinical manifestation of chronic heart failure symptoms was significantly more severe in study group patients (NYHA scale, Table 1). Moreover, patients subjected to the LARIAT procedure have significantly higher thromboembolic risk than control patients (CHA₂DS₂-VASc, Table 1). No other significant differences in patients' demographic and clinical data were found.

The chicken wing shape was the most common type of LAA both in the study and control group (45.1 vs. 46.0%, $p = 0.93$), followed by windsock (29.4 vs. 20.0%, $p = 0.27$) and cauliflower (25.5 vs. 34.0%, $p = 0.35$) (Table 2). Although no statistically significant differences in LAA type distributions were found between groups, the study group was characterized by LAAs with a lower number of lobes (Table 2).

In both analyzed groups, the LAA orifice was predominantly oval (study group: 94.0% vs. control group: 70.4%), and significantly fewer round orifices were found in the study group ($p = 0.001$, Table 2). Moreover, the size of the orifice was found to be significantly larger in LARIAT patients compared to the control group (higher diameters, orifice area, and orifice perimeter, Table 2).

Several major LAA morphometrical features were analyzed (body length, body width, and chamber depth). However, no statistically significant differences were found in those measured parameters between the two groups (all $p > 0.05$, Table 2). No differences between groups were noted in LAA end-systolic volumes, but a significant difference was observed in the end-diastolic cardiac phase (Table 2). The calculated LAA ejection fraction was significantly lower in the study group compared to healthy patients (16.4 ± 14.9 vs. $48.2 \pm 12.9\%$, $p = 0.001$). For the chicken wing type, the angle of the bend was significantly smaller in LARIAT patients than in the control group (62.1 ± 10.4 vs. $68.5 \pm 13.9^\circ$, $p = 0.011$). The LAA body lengths measured from orifice to bend and from bend to LAA apex showed no

differences between analyzed groups (to bend: 22.7 ± 3.8 vs. 18.4 ± 5.5 mm, $p = 0.103$; from bend: 28.1 ± 4.6 vs. 27.3 ± 5.8 mm, $p = 0.443$).

A significantly larger left atrium was observed in the study group compared to controls (larger anteroposterior diameter and volume) with reduced left atrium ejection fraction in LARIAT patients (13.9 ± 10.8 vs. $17.7 \pm 6.5\%$, $p = 0.04$) (Table 2). No differences were found in measured left ventricle dimensions, volumes, and ejection fraction between investigated groups (all $p > 0.05$, Table 2). No other significant correlations and differences were found between all measured morphometric parameters.

DISCUSSION

The LAA morphology plays a significant role in the pathogenesis of ischemic stroke. It was proven that complex LAA (non-chicken wing shape) is an independent risk factor for cryptogenic ischemic stroke [6,27]. However, little is known about the LAA anatomy that influences the course and results of the LAA closure procedures. Without a doubt, a significant morphologic remodeling of the left atrium occurs in patients with non-sinus rhythm [3]. Nevertheless, a lack of consensus is observed regarding the LAA structural alterations related to rhythm and hemodynamical disturbances [3,13]. Although it is hard to believe that the remodeling may concern the type (shape) of the LAA body, the changes in the LAA orifice shape and size, LAA body size, and LAA function may be substantial.

Regardless of the technique used, residual leaks after the LAA are commonly observed[9]. Our study shows that in atrial fibrillation patients, the biggest morphological changes are found in the LAA orifice, crucial for all LAA closure procedures. Left atria remodelling associated with enlargement in heart failure and arrhythmia patients changes the shape and size of the LAA opening. LAA orifices in diseased patients are significantly larger and more oval, which affects the risk of leakage [18]. An incomplete sealing may potentially occur in cases where an appropriately large device is used to close the LAA when implanted not in the round and when in oval or in irregular shape orifice [18]. Thus, operators should be aware of this change in LAA orifice morphology and choose the appropriate tool for the LAA closure to avoid danger to the health and life of patients' peri-device leaks. The observed reduced LAA ejection fraction in research group is another important observation emerging

from the current work. The LAA EF was decreased even despite performing tomography scans during sinus rhythm. This reduced contractile function of the LAA may be the indirect result of remodeling of the left atrium and altered atrial blood pressure, which influence structure of the LAA itself leading to impaired contractility of LAA. In paroxysmal AF remodeling of LA is most often negligible and reversible. The duration time of LA rhythm disturbances negatively affects the structure of the atrium. Persistent AF strongly promotes electrical remodeling and pressure/volume overload of LA promotes interstitial fibrosis leading to structural remodeling [23]. It follows that irreversible changes in LA morphology and consequently in LAA structure may start to develop in patients with AF lasting more than one week [1,5]. On the other hand, the increased left atrial pressure may create to high resistance for the LAA to generate the effective force of its contraction. Previous studies showed that LAA ejection fraction may be an independent predictor of cardiac thromboembolization [8,22], which alters LAA emptying and predisposes to local blood stasis and its increased thrombogenicity [19].

Cardiac CT seems to be the preferable tool for pre-procedural imaging of the LAA as it provides the most faithful, 3D image of the LAA [24]. Moreover, it helps visualize other important heart cavities and main vessels (together with coronary vasculature), in which knowledge of morphology is crucial to avoid serious peri-procedural complications [7,23]. Our study also indicates that LAA 3D visualization may provide useful information for the operator on the LAA morphology, thereby influencing the choice of the technique of its closure. The creation of a fully personalized virtual 3D model of the patient's LAA may be completed in less than an hour. This model can easily be subjected to multi-directional measurement or used to simulate procedures [10]. Moreover, the created model may be visualized using virtual or augmented reality techniques or using the 3D printed technique to better assist the clinicians [17]. Unfortunately, one of the obstacles to the use of this wonderful tool in all medical centers is the relatively low availability and high cost of software enabling the segmentation and visualization of the CT data, as well as the lack of experience of the staff in manufacturing the 3D models [15].

Some limitations to this study should be considered. First, this is a single-center study with a relatively small sample size. A limited number of patients in both groups does not allow a comprehensive statistical analysis to determine which LAA morphometrical factors may contribute to the occurrence of a stroke or are associated with success rate or

complications during the LARIAT procedure. Moreover, only Caucasian subjects were studied, and no inter-racial differences are studied. Despite these limitations, we believe that the current study has provided insight into the morphological characteristics of the LAA in different groups of patients.

CONCLUSIONS

Presented morphometrical data should be considered during planning and when performing procedures targeted to LAA closure, as significant differences in the anatomy of the LAA may be encountered in patients with atrial fibrillation. Substantial morphometrical differences in LAA orifice are found, which is significantly larger and more oval in patients with atrial fibrillation compared to healthy controls. Although no difference in LAA body type and size is observed, the LAA ejection fraction is significantly lower in atrial fibrillation patients.

Acknowledgments

Financial support and disclosure statement: This study was supported by the National Centre for Research and Development under the LIDER program (LIDER/7/0027/L-10/18/NCBR/2019).

REFERENCES

1. Ausma J, Litjens N, Lenders MH et al. Time Course of Atrial Fibrillation-induced Cellular Structural Remodeling in Atria of the Goat. *J Mol Cell Cardiol.* 2001;33(12):2083-2094.
2. Bartus K, Podolec J, Lee RJ et al. Atrial natriuretic peptide and brain natriuretic peptide changes after epicardial percutaneous left atrial appendage suture ligation using LARIAT device. *J Physiol Pharmacol.* 2017; 68(1):117–123.
3. Floria M, Radu S, Gosav EM et al. Left Atrial Structural Remodelling in Non-Valvular Atrial Fibrillation: What Have We Learnt from CMR? *Diagnostics.* 2014; 10(3):137.
4. Glikson M, Wolff R, Hindricks G, Mandrola J, Camm AJ, Lip GYH, Fauchier L, Betts TR, Lewalter T, Saw J (2020) EHRA / EAPCI expert consensus statement on catheter-based left atrial appendage occlusion – an update. *EuroIntervention* 15(13):1133-1180.

5. Goette A, Honeycutt C, Langberg JJ. Electrical remodeling in atrial fibrillation. Time course and mechanisms. *Circulation*. 1996; 94(11):2968-2974.
6. Gwak DS, Choi WC, Kim YW, et al. Impact of Left Atrial Appendage Morphology on Recurrence in Embolic Stroke of Undetermined Source and Atrial Cardiopathy. *Front Neurol*. 2021; 12:679320.
7. Hołda MK, Koziej M, Hołda J et al. Anatomic characteristics of the mitral isthmus region: The left atrial appendage isthmus as a possible ablation target. *Ann Anat*. 2017; 210:103-111.
8. Iwama M, Kawasaki M, Tanaka R et al. Left atrial appendage emptying fraction assessed by a feature-tracking echocardiographic method is a determinant of thrombus in patients with nonvalvular atrial fibrillation. *J Cardiol*. 2012; 59(3):329–336.
9. Jang SJ, Wong SC, Mosadegh B. Leaks after left atrial appendage closure: ignored or neglected? *Cardiology*. 2021; 146(3):384–391.
10. Jia D, Jeon B, Park HB et al. Image-Based Flow Simulations of Pre- and Post-left Atrial Appendage Closure in the Left Atrium. *Cardiovasc Eng Technol*. 2019; 10(2):225–241.
11. John Camm A, Colombo A, Corbucci G, Padeletti L (2014) Left atrial appendage closure: A new technique for clinical practice. *Hear Rhythm* 11(3):514–521.
12. Karim N, Ho SY, Nicol E et al. The left atrial appendage in humans: structure, physiology, and pathogenesis. *Europace*. 2020; 22(1):5–18.
13. Kishima H, Mine T, Takahashi S et al. Morphologic remodeling of left atrial appendage in patients with atrial fibrillation. *Hear Rhythm*. 2016; 13(9):1823–1828.
14. Kleindorfer DO, Towfighi A, Chaturvedi S et al. Guideline for the Prevention of Stroke in Patients With Stroke and Transient Ischemic Attack: Guideline From the American Heart Association/American Stroke Association. *Stroke*. 2021. 52(7):364–467.
15. Lau I, Wong YH, Yeong CH et al. Quantitative and qualitative comparison of low- and high-cost 3D-printed heart models. *Quant Imaging Med Surg*. 2019; 9(1):107-114.
16. Litwinowicz R, Bartus M, Burysz M et al. Long term outcomes after left atrial appendage closure with the LARIAT device—Stroke risk reduction over five years follow-up. *PLoS One*. 2018; 13(12):e.
17. Litwinowicz R, Witowski J, Sitkowski M et al. Applications of low-cost 3D printing in left atrial appendage closure using epicardial approaches – initial clinical experience. *Polish J Cardio-Thoracic Surg*. 2018; 15(2):135–140.
18. Maan A, Kevin Heist E. Left Atrial Appendage Anatomy: Implications for Endocardial

- Catheter-based Device Closure. *J Innov Card Rhythm Manag.* 2020; 11(7):4179-4186.
19. Masci A, Barone L, Dedè L et al. The impact of left atrium appendage morphology on stroke risk assessment in atrial fibrillation: A computational fluid dynamics study. *Front Physiol.* 2019; 9:1938.
 20. Naksuk N, Padmanabhan D, Yogeswaran V et al. Left Atrial Appendage: Embryology, Anatomy, Physiology, Arrhythmia and Therapeutic Intervention. *JACC: Clin Electrophysiol.* 2016; 2(4):403–412.
 21. Patti G, Pengo V, Marcucci R et al. The left atrial appendage: From embryology to prevention of thromboembolism. *Eur Heart J.* 2017; 38(12):877-887.
 22. Shimizu T, Takada T, Shimode A et al. Association between Paroxysmal Atrial Fibrillation and the Left Atrial Appendage Ejection Fraction during Sinus Rhythm in the Acute Stage of Stroke: A Transesophageal Echocardiographic Study. *J Stroke Cerebrovasc Dis.* 2013; 22(8):1370–1376.
 23. Słodowska K, Szczepanek E, Dudkiewicz D et al. Morphology of the Left Atrial Appendage: Introduction of a New Simplified Shape-Based Classification System. *Heart Lung Circ.* 2021; 30(7):1014-1022.
 24. Taina M, Korhonen M, Haataja M et al. Morphological and Volumetric Analysis of Left Atrial Appendage and Left Atrium: Cardiac Computed Tomography-Based Reproducibility Assessment. *PLoS One.* 2014; 9(7):e101580.
 25. Thomas L, Abhayaratna WP, Left Atrial Reverse Remodeling: Mechanisms, Evaluation, and Clinical Significance. *JACC Cardiovasc Imaging.* 2017; 10(1):65-77
 26. Wilkins B, Fukutomi M, De Backer O et al. Left Atrial Appendage Closure: Prevention and Management of Periprocedural and Postprocedural Complications. *Card Electrophysiol Clin.* 2020; 12(1):67–75.
 27. Yamamoto M, Seo Y, Kawamatsu N et al. Complex left atrial appendage morphology and left atrial appendage thrombus formation in patients with atrial fibrillation. *Circ Cardiovasc Imaging.* 2014; 7(2):337–343.
 28. Zuo K, Sun L, Yang X et al. Correlation between cardiac rhythm, left atrial appendage flow velocity and CHA2DS2-VASc score: Study based on transesophageal echocardiography and 2-dim speckle tracking. *Clin Cardiol.* 2017; 40(2):120 125.

Table 1 Clinical characteristics of studied patients (number / [%] or mean [SD]).

Variable		Study group (n=51)	Control group (n=50)	p-value
Females (%)		41.2%	50.0%	0.09
Age (years)		61.04 (10.35)	57.80 (14.45)	0.20
Body mass index (kg/m ²)		28.8 (5.4)	28.6 (4.9)	0.83
Non-sinus tachycardia		51 / 100.0%	0 / 0.0%	<0.001
Arterial hypertension		46 / 90.2%	19 / 38.0%	<0.001
Hyperlipidemia		3 / 5.9%	2 / 4.0%	0.67
Chronic heart failure		10 / 19.6%	6 / 12.0%	0.30
Coronary artery disease		11 / 21.6%	6 / 12.0%	0.20
Chronic obstructive pulmonary disease		2 / 3.9%	4 / 8.0%	0.39
Diabetes mellitus type II		6 / 11.8%	5 / 10.0%	0.78
History of myocardial infarction		1 / 2.0%	2 / 4.0%	0.55
History of ischemic stroke		15 / 29.4%	0 / 0.0%	<0.001
CCS	I	5 / 9.8%	3 / 6.0%	0.48
	II	8 / 15.7%	4 / 8.0%	0.24
	III	0 / 0.0%	1 / 2.0%	0.31
	IV	0 / 0.0%	0 / 0.0%	-
NYHA	I	14 / 27.5%	6 / 12.0%	0.05
	II	20 / 39.2%	8 / 16.0%	0.01
	III	3 / 5.9%	0 / 0.0%	0.08
	IV	0 / 0.0%	0 / 0.0%	-
CHA ₂ DS ₂ -VASc	0 (males) or 1 (females) - "low risk"	2 / 3.92%	22 / 44.0%	<0.001
	1 (males) – "low-moderate risk"	11 / 21.6%	5 / 10.0%	0.11
	≥2 - "moderate-high risk"	38 / 74.5%	23 / 46.0%	0.01

SD – standard deviation, n – number, CCS – The Canadian Cardiovascular Society grading of angina pectoris, NYHA – New York Heart Association Classification of Heart Failure, CHA₂DS₂-VASc – risk stratification score for estimation of stroke risk for nonvalvular atrial fibrillation in adults

Table 2. Comparison of corresponding parameters measured in both groups (% or mean [SD]).

Parameter		Study group (n=51)	Control group (n=50)	p-value
LAA shape (%)	cauliflower	25.5	34.0	0.35 *
	chicken wing	45.1	46.0	0.93 *
	windsock	29.4	20.0	0.27 *
Number of LAA lobes (%)	1	39.2	16.0	0.01 **
	2	33.3	20.0	0.13 **
	3	19.6	34.0	0.10 **

	≥ 4	7.8	30.0	0.01 **
LAA orifice shape round/oval (%)		6.0 / 94.0	29.6 / 70.4	0.001
LAA orifice antero-posterior diameter (mm)		19.3 (4.12)	17.2 (4.0)	0.01
LAA orifice transverse diameter (mm)		25.1 (5.1)	20.5 (4.4)	0.001
LAA orifice area (mm ²)		387.2 (133.9)	327.1 (128.3)	0.02
LAA orifice perimeter (mm)		70.2 (12.5)	61.2 (11.6)	0.04
LAA body length (mm)		47.4 (15.4)	43.7 (10.9)	0.17
LAA width at the base (mm)		24.7 (5.6)	24.4 (5.8)	0.81
LAA chamber depth (mm)		17.7 (3.5)	16.5 (3.8)	0.11
LAA end-diastolic volume (ml)		9.0 (3.4)	5.4 (3.8)	0.001
LAA end-systolic volume (ml)		10.9 (3.6)	10.6 (4.3)	0.69
LAA ejection fraction (%)		16.4 (14.9)	48.2 (12.9)	0.001
Left atrium end-diastolic antero-posterior diameter (mm)		40.1 (6.9)	36.0 (7.1)	0.001
Left atrium end-diastolic volume (ml)		109.5 (38.9)	93.8 (30.8)	0.02
Left atrium end-systolic volume (ml)		129.5 (41.7)	112.5 (34.3)	0.04
Left atrium ejection fraction (%)		13.9 (10.8)	17.7 (6.5)	0.04
Left ventricle end-diastolic inner diameter (mm)		45.5 (6.8)	46.4 (6.3)	0.47
Left ventricle end-diastolic volume (ml)		124.5 (48.1)	133.5 (39.1)	0.15
Left ventricle end-systolic volume (ml)		68.7 (40.5)	65.7 (25.0)	0.56
Left ventricle ejection fraction (%)		46.7 (14.3)	50.7 (12.2)	0.14

LAA – left atrial appendage, SD – standard deviation, n – number

* Results are considered statistically significant at p<0.017 to allow for a Bonferroni correction accounting for the multiple comparisons

** Results are considered statistically significant at p<0.013 to allow for a Bonferroni correction accounting for the multiple comparisons

Figure 1. Representatives for 3D reconstructions of each left atrial appendage (LAA) type (cauliflower, chicken wing, and arrowhead type), left atrium (LA) and left ventricle (LV) segmented from contrast-enhanced computed tomography of the heart (Mimics Innovation Suite 22, Materialise).

Figure 2. 3D visualizations of left atrial appendages (LAA) with marked measurements (Mimics Innovation Suite 22, Materialise). **A.** Body length and width, **B.** Depth of LAA chamber, **C.** Orifice dimensions (D1 and D2), area and perimeter, **D.** Angle of the bend and body lengths for chicken wing type.



