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Alternatives to amalgam: Is pretreatment necessary for effective bonding to dentin?



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ABSTRACT

Objective: The aim of this study was to determine whether pretreatment of the dentin surface is beneficial or not by analysis of the bond strengths of four self-adhesive restoratives and four restoration materials where pretreatment of dentin was necessary. Methods: Bovine incisors (n = 160) were ground flat on the labial surfaces to expose dentin using a grinder and silicon carbide (SiC) abrasive papers under running water. Between preparation and bonding procedures, the crowns were stored in Chloramine-T solution at 4 °C. Eight different restorative materials were studied: Activa BioActive (ABA), Cention Forte (CNF), Ceram.x Spectra ST (CXS), Riva self-cure (RSC), Equia Forte (EQF), Fuji II LC (FJI), Ketac Molar (KTM), Surefil one (SFO). Four materials required pretreatment of the dental hard tissue before placement, whereas the other four were self-adhesive (no pretreatment). The specimens were mounted vertically in plaster. A preload of 5 N was applied and the subsequent cross-head speed was 0.8 mm/min. Shear bond strengths (MPa) were calculated as the failure load divided by the bonding area. Failure modes were recorded as adhesive, cohesive or pretest. Data were statistically analyzed via ordinal regression for inference and Tukey's method to adjust for multiple comparisons. All computations were done using R version 4.1.2 (R Core Team 2021).

Results: S_{max} (failure stress in MPa) of the combined groups with pretreatment were significantly higher than the self-adhesive materials. The highest frequency of pretest-failure was seen with FJI. Glass-ionomer cements without pretreatment were the only restoratives with pretest failures. Amongst materials without pretreatment, SFO had the highest bond strengths. *Significance:* The further reduction of the placement steps for materials used as an amalgam alternative, namely the omission of pretreatment of the dentin, results in these self-adhesive materials having lower bond strengths than materials that require pretreatment of the dentin.

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1. Introduction

The search for reliable amalgam alternatives is continuing as the European Union changed its regulation to impose a stepwise reduction of amalgam use for children under 15 years and pregnant women. Strict regulation now exists regarding the disposal of waste amalgam (2017/852 article 10).

Although modern restorative materials, particularly resin composites, are reasonable alternatives to amalgam, it is difficult for them to compete with several beneficial characteristics of amalgam such as easy handling and extended durability. The clinical and mechanical properties of composite restoratives are often compromised by complicated handling procedures and unfavorable cavity conditions. The benefits of resin composite such as excellent esthetics, conservation of tooth structure, longevity, and reparability stand in contrast to their technique sensitivity, placement time and affordability. Especially for the group of patients affected by the above-mentioned regulation, children and pregnant women, placement time should be shortened to a minimum. This is sometimes impossible with the complicated handling procedures of composites.

Another group of dental restoratives, glass-ionomer cements (GIC) are often used instead of amalgam because they are easier to handle. But GIC fails to be considered as a proper alternative to amalgam along with resin composites due to its poor physical and chemical properties.

New materials with simplified handling, and shorter processing times compared to composites, are being developed by several major manufacturers. In some cases, they are rapidly introduced to the market. There is often insufficient time for prior long-term clinical studies. It is therefore important to conduct standardized laboratory investigations. These can be used to compare such new materials with conventional composite materials.

One such material is Surefil one, a self-adhesive hybrid composite, which is claimed to combine resin composite strengths with the easy handling of GIC-based materials. It is light cured, but depth-of-cure is not an issue because it is dual-activated. Cross-linking of structural monomers, combined with self-adhesive properties of GIC polyacids, is proposed to obviate the need for etching, bonding or layering.

Cention Forte is a self-curing radiopaque material for direct treatment of anterior and posterior cavities. Cention Forte has been termed an Alkasite and is claimed [1] to be bioactive and suitable for cavities where amalgam is contraindicated or not desired.

The aim of the study was to evaluate whether or not pretreatment of the dentin substrate is desirable. To address this question, bond strengths were measured of eight materials that are intended as amalgam alternatives. Four of these require pretreatment and four are specified as self-adhesive. Our null hypothesis is therefore that there is no difference in performance between the pretreatment and self-adhesive categories.

2. Materials and methods

2.1. Sample size

160 bovine incisors were used as substrates to measure the bond strengths of eight dental restoratives. A handsaw was used to separate the crowns from the roots. Buccal surfaces of the crowns were ground using a universal grinder (Metaserv 2000, Buehler, Düsseldorf, Germany) and silicon carbide (SiC) abrasive papers (grit 80, 400 and 1000, Buehler, Düsseldorf Germany) under running water. Grit 80 SiC paper was used to obtain a flat dentin surface, followed by grit 400 for 1 min. Between preparation and bonding procedures, the crowns were stored in Chloramine-T solution at 4 °C. Immediately before bonding, grit 1000 SiC paper was applied for 10 s.

Eight different restorative materials were each randomly placed on 20 dentin substrates. Four materials required pretreatment of the dental hard tissue before placement, whereas the other four were self-adhesive (no pretreatment) (Table 1).

2.2. Pretreatment and application

For the two resin-based composite restoratives (**CXS** & **ABA**) a universal self-etching adhesive material (Prime&Bond active (**PBA**), Dentsply, Konstanz, Germany) was applied with a microbrush and agitated lightly on the surface for 20 s. The adhesive was dispersed with water- and oil-free compressed air until a shiny and immobile film had formed and was light-cured for 10 s with a light-curing unit (SmartLite Pro (SLP), Dentsply, Konstanz, Germany; Irradiance: 1250 mW/cm²).

For the self-curing Alkasite (**CNF**), a two-component selfetching and self-curing primer (Cention Primer, Ivoclar Vivadent, Schaan, Liechtenstein) was applied to the dentin surface with a single-use applicator. After coating and scrubbing for 10 s, the primer was dispersed with water- and oil-free compressed air until a thin and shiny film had formed.

For the glass ionomer (**RSC**), the dentin surface was etched with Riva Conditioner (SDI, Victoria, Australia) – a polyacrylic acid conditioner and left on the surface for 10 s. The etching agent was rinsed, followed by gentle air-drying of the dentin surface.

After completion of the pretreatment steps, cylindrical specimens of the restorative pastes were produced in selfdissolving gelatin capsules and bonded perpendicularly to the dentin surface. Any excess was removed and the materials were cured according to the manufacturers' recommendations. For the light-activated materials, the light curing unit was used from 3 different directions for 10 s each (see Table 2).

For self-adhesive materials the dentin area was subject to gentle air-drying. Cylindrical specimens of the restorative in self-dissolving gelatin capsules were bonded perpendicularly

| Table | e 1 - Materials. | | | | | | |
|-------|-----------------------|-------------------------------------|------------------|----------------|------------------------------------|---|-------------|
| Code | Material | Type | Pretreatment Y/N | Curing mode | Manufacturer | Formulation | Lot numbers |
| ABA | Activa BioActive | Resin-based "bioactive" | Yes | Light | Pulpdent, Watertown, MA, USA | Powder: silanated bioactive glass and calcium, silanated silica, sodium fluoride | 210305 |
| | | contribostice | | | | uque, univertaine mounted by the insertion of a hydrogenated polybutadiene and other methacrylate monomers, modified polyacrylic acid | |
| CNF | Cention Forte | Self-curing "bioactive" Alkasite | Yes | Dual | Ivoclar Vivadent, Liechtenstein | Powder: barium aluminum silicate glass, ytterbium trifluoride, isofiller, calcium barium aluminum fluorosilicate glass, calcium | Z02CMP |
| | | | | | | fluoro silicate glass 1 inuid - urathana dimatharmlata tricrolodacandimathanol | |
| | | | | | | dimethacrylate, tetramethyl-xylylene diurethane dimethacrylate, polyethylene glycol 400 dimethacrylate, ivocerin, | |
| CXS | Ceram.x Spectra ST | Resin-based composite (RBC) | Yes | Light | Dentsply, Konstanz, Germany | Ethoxylated Bisphenol A Dimethacrylate, Urethane modified Bis- GMA dimethacrylate resin, 2,2'-ethylenedioxydiethyl | 210300526 |
| | | | | | | dimetharcylate, ytterbium trifluoride, 2,6-di-tert-butyl-p-cresol | |
| RSC | Riva self-cure | Bulk fill glass- ionomer | Yes | Self | SDI, Victoria, Australia | Powder: fluoroaluminosilicate glass, polyacrylic acid, iron oxide Liquid: polybasic carboxylic acid, water | A2104058EA |
| EQF | Equia Forte HT | Glass-ionomer | No | Self | GC, Tokyo, Japan | 2-hydroxyethyl methacrylate, polybasic carboxylic acid, urethane dimethacrylate, dimethacrylate, calcium-aluminum-fluoro-silicate alses, others | 210202A |
| FJI | Fuji II LC | Resin-modified Glass-ionomer | No | Light | GC, Tokyo, Japan | Powder: Ca, La, Al-fluorosilicate glass, pigments Liquid: Polycarbonic acid, tartaric acid, water | 210524B |
| KTM | Ketac Molar | Glass-ionomer | No | Self | 3 M, Neuss, Germany | Powder: Radiopaque fluroaluminosilicate glass, polyacrylic acid, pigments Liouid: Polvacrylic acid. tartaric acid. and water | 8048452 |
| SFO | Surefil one | Self-adhesive composite hybrid | No | Light | Dentsply, Konstanz, Germany | Powder: silanated aluminum-phosphor-strontiumsodium-fluoro- silicate glass, dispersed silicon dioxide, ytterbium fluoride, | 2104000853 |
| | | | | | | pigments Liquid: acrylic acid, polycarboxylic acid, bifunctional acrylate, self- cure initiator, camphorquinone, stabilizer | |
| | | | | | | | |

| Table 2 – Study variables. Mod | ified after and [2] | |
|--------------------------------|-----------------------------|---|
| Tooth substrate | Type and age of teeth | Bovine incisors of the lower jaw; average age 60 months |
| | Selected region | Superficial layers of facial incisal dentin |
| | Condition | Only sound dentin |
| | Collection and storage | Stored at – 20 °C; thawed 24 h before experiments; stored at 4 °C in |
| | | 0.5% chloramine-T solution |
| Restorative material | | Ceram.x Spectra ST, Activa BioActive, Cention Forte, Riva self-cure, |
| | | Surefil one, Ketac Molar, Fuji II LC, Equia Forte HT |
| Specimen preparation and pre- | Method | Grinder (Metaserv 2000, Buehler, Düsseldorf, Germany) and SiC |
| testing conditions | | abrasive paper (grit 80, 400 and 1000, Buehler, Düsseldorf, |
| | | Germany). Grit 80 used to create appropriate bonding dentin |
| | | surface; grit 400 for 1 min; grit 1000 for 10's right before bonding |
| | Postorativo shano and | Culindrical (internal diameter 4 mm height 8 mm) |
| | dimensions | Cymuncal (mternal diameter 4 mm, neight 8 mm) |
| | Restorative application and | Restorative material was inserted into self-dissolving gelatin |
| | curing conditions | capsules, pressed against the dentin surface at 90°. If material is |
| | 0 | light-activated, light-curing from 3 different directions for 10 s each |
| | | (total 30 s). |
| | Bonding and testing | 20 °C, 60% relative humidity |
| | environment | |
| | Post-bonding storage | 24 h, water, 37 °C |
| | Potting material | Tooth specimens were mounted vertically in hard plaster, type 3, |
| | | color blue (Heraeus Kulzer, Hanau, Germany) |
| Data reporting and analyses | Descriptive statistics | Results were expressed as means and with exact confidence |
| | parameters | intervals. |

to the dentin surface. The excess was removed and the materials were cured if required, according to the manufacturers' recommendations. **SFO** and **FJI** were light-cured from 3 different directions for 10 s each.

For encapsulated materials a Rotomix device was used (3 M, Neuss, Germany). All specimens were stored in distilled water at 37 °C for 24 h.

2.3. Shear bond strength measurements

The specimens were mounted vertically in plaster. Specimen cylinders were aligned horizontally, parallel to the surface of the hard plaster. A preload of 5 N was applied and the subsequent cross-head speed was 0.8 mm/min, using a Universal testing machine (Zwick/Roell, Ulm, Germany). The shear bond strength was calculated as the load at failure divided by the bonding area and was expressed in MPa. The mode of failure was recorded as adhesive, cohesive or pretest failure. The data were statistically analyzed.

2.4. Statistical analysis

Because of concerns with normality of residuals, ordinal regression was used for inference and Tukey's method was used to adjust for multiple comparisons. All computations were done using R version 4.1.2 (R Core Team 2021).

3. Results

 S_{max} (failure stress in MPa) for all material are depicted in Fig. 1. Pooled data are shown in Fig. 2. Types of failure are shown in Fig. 3. Descriptive statistics are summarized in



Table 3. Fig. 2 shows that the combined groups with pretreatment had a significantly higher S_{max} compared to the self-adhesive materials. As shown in Figs. 1 and 2, three of the four materials with pretreatment outperformed all the others. Mean S_{max} ranged from 1.7 MPa for KTM to 17.4 MPa for CNF.

As shown in Fig. 3, the highest frequency of pretest-failure was seen with FJI. The glass-ionomer cements without pretreatment were the only restoratives with pretest failures.

Except for **RSC**, the materials with pretreatment showed the highest S_{max} (Fig. 1). All three glass-ionomer cements showed the lowest S_{max} . The greatest range of S_{max} was seen in **CXS**. For materials without pretreatment, **SFO** showed the highest bond strengths.







Fig. 3 - mode of failure.

4. Discussion

This study compared the SBS of eight different materials to bovine dentin. Four materials required pretreatment and four were self-adhesive. In the case of **ABA** and **CXS** the pretreatment entailed the use of a bonding agent (**PBA**) upon the dentin surface. The dentin surface was treated with a primer before placing **CNF** and for the placement of **RSC** a conditioner was used.

The SBS of materials with pretreatment were significantly higher than self-adhesive materials. This is in accordance with previous studies where SBS to pretreated surfaces were compared with self-adhesive materials [3–7]. ABA showed significantly higher SBS than conventional glass-ionomer materials, which is in agreement with previous studies [8]. Etch and rinse with a phosphoric acid was used for RSC, a glass ionomer. The use of a dentin conditioner prior to glass-

| Table 3 – Descriptive statistics. Missing values = failure before measurement. | | | | | | |
|--|------|-----|----|---------|--|--|
| Material | Mean | SD | Ν | Missing | | |
| ABA | 17.1 | 4.0 | 20 | 0 | | |
| CNF | 17.4 | 4.0 | 20 | 0 | | |
| CXS | 16.1 | 6.1 | 20 | 0 | | |
| EQF | 4.2 | 2.7 | 20 | 1 | | |
| FJI | 2.2 | 2.6 | 20 | 12 | | |
| KTM | 1.7 | 1.5 | 20 | 3 | | |
| RSC | 7.3 | 1.5 | 20 | 0 | | |
| SFO | 9.1 | 2.6 | 20 | 0 | | |
| All | 10.2 | 7.0 | 20 | 16 | | |

ionomer placement proved to be an important step in improving the bond strength [9].

ABA, CNF and SFO were introduced recently. Previous measurements have shown that specimens without pretreatment had lower SBS than after applying Scotchbond Universal adhesive [10]. Although the pretreatment agents in our study were PBA for ABA, Cention Primer for CNF and no pretreatment for SFO, our mean bond strengths (Table 3) for these three materials correlate with the previous study [10], but are clearly 10–30% lower. If no adhesive was applied, SBS for SFO was highest compared to the other two materials [10].

The manufacturer's recommendation is to wait for the **ABA** material to self-cure for 20–30 s before proceeding with low-intensity light curing. This is to reduce polymerization stress and exothermic reaction. However, in our in vitro study, both polymerization stress and exothermic reaction can be neglected. Therefore, the same irradiance was used for all materials in order to obtain comparable results. The manufacturer of **ABA** does not give a concrete indication of how much mW/cm² energy output can be considered "low intensity".

Specimens used in this study were stored in water at 37 °C for 24 h. Although the storage time of specimen after bonding procedures is considered clinically relevant [11], it has been shown that long-term storage had only a small effect on bonding [12].

Amongst the self-adhesive group of materials, SFO had the highest shear strengths: S_{max} of 9.1 MPa (Table 3). Previous research showed poor bond strengths with GICs including EQF, FJI and KTM [13,14]. Incorporating lightactivated monomers to GIC improved their physical and mechanical properties - now known as resin-modified glass ionomer cements (RMGIC) [13-16]. Other formulations exist that either include reactive glass fillers but set by photopolymerization (polyacid-modified resin-composites: PMRCs or compomers) or that incorporate prereacted GIC filler in a photocured resin matrix (GIOMER) [10]. Bond strengths for PMRCs are up to 12 MPa [16,17] in contrast to conventional GICs which range between 3 and 7 MPa [14,18] or, as shown in the present study, ranging between 1.7 and 4.2 MPa (Table 3). The application of conditioner for the three materials EQF, FJI and KTM is described by the manufacturer as "optional" or "recommended". Since this study deals with amalgam alternatives, rapid treatment is essential. Therefore, in this study, the quickest possible handling procedure was applied, which is also applied by most dental practitioners.

Conventional polyacids lack polymerizable groups, therefore they cannot form a polymerized network [19,20]. SFO has been formulated as a modified polyacid system of high molecular mass to merge the classical self-adhesive feature of glass-ionomer cement with a structural polymerized network [19–21]. Recent 1-year clinical recall results of 41 patients suggest that SFO gave a clinically satisfactory performance in load-bearing class I, II and non-retentive class V cavities [21].

CNF is presented with a two-component self-etching and self-curing primer. **CNF** had the highest mean shear strengths of the investigated materials (Table 3).

A previous in-vitro study [22] showed that in terms of marginal quality, Surefil one behaves similar to conventional resin composite bonded with self-etch adhesives. The wear behavior of Surefil one outperformed other amalgam alternatives, such as **ABA**, **Equia Forte Fil** and **FJI** [22].

A recent clinical trial [21] showed that 84% of SFO restorations (class I, II and V cavities in permanent teeth) were satisfactory after 1 year with a recall rate above 80% and an annual failure rate (AFR) of 2%. Results were evaluated at baseline using the USPHS criteria, developed by Cvar and Ryge in 1971. Moderate hypersensitivity and partial fracture of the restoration were recorded as failures [21]. In another clinical study postoperative sensitivity (POS) was shown for ABA (4.2%), EQF (12.5%) and CNF (29.2) 24 h after placement in class I maxillary and mandibular premolars and molars, which decreased significantly after 1 month (ABA (0%), EQF (4.2%) and CNF (10.4%)) [22].

Two-year clinical performances of a high viscosity GIC (Equia, GC) and a nanohybrid resin composite (GrandioSO, Voco) were compared in a randomized, split-mouth study. A total of 112 restorations were done on both mandibular second molars (class I). GICs showed a success rate of 96%, while all resin composite restorations succeeded after 2 years. Significantly higher wear was observed for Equia [23]. Restorations were evaluated using modified USPHS criteria. An in-vitro study on localized and generalized wear showed that self-cured SFO in its experiment stage (ASAR-MP4) showed similar results to ABA, FJI and EQF [24].

The link between appropriate in-vitro properties and long term in-vivo success is the clinician's ability to handle and manipulate the material (technique sensitivity), which has an enormous impact on the quality and on the longevity of dental restoratives [25]. Several dental materials for posterior restoration have failed, either because of their technique sensitivity, or pure mechanical properties to withstand load in large posterior cavities [25,26]. Self-adhesive restoration materials are preferred as amalgam alternatives because no technique-sensitive and time-consuming bonding procedure is required [27].

Laboratory measurements on bond strength remain a useful tool to compare systems. However, no correlations between in vitro performance and clinical success can be demonstrated and if so, they are poor at best [28]. The absence of direct correlation to clinical outcomes, however, should not invalidate in-vitro trials [29]. Clinical studies remain the ultimate tool to evaluate the performance of new materials shown in this study.

5. Conclusion

- 1. In this study, the bond strength of materials requiring pretreatment of dentin is superior to that of self-adhesive materials.
- 2. Pre-test failures were only observed with glass-ionomer cements.

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