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Author	Family Name	Sparacello	
	Particle		
	Given Name	Vitale S.	
	Suffix		
	Division	Department of Anthropology	
	Organization	University of New Mexico	
	Address	Albuquerque, NM, USA	
Corresponding Author	Family Name	Marchi	
	Particle		
	Given Name	Damiano	
	Suffix		
	Division	Department of Biology	
	Organization	University of Pisa	
	Address	Via Derna 1, Pisa, 56126, Italy	
	Division	Evolutionary Studies Institute	
	Organization	University of the Witwatersrand	
	Address	Johannesburg, South Africa	
	Email	dmarchi@biologia.unipi.it	
Author	Family Name	Shaw	
	Particle		
	Given Name	Colin N.	
	Suffix		
	Division	McDonald Institute for Archaeological Research	
	Organization	University of Cambridge	
	Address	Cambridge, UK	
	Division	PAVE Research Group, Department of Archaeology and Anthropology	
	Organization	University of Cambridge	
	Address	Cambridge, UK	
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	Results reveal that Late Upper Paleolithic, Neolithic and Iron Age samples show high fibular rigidity and have values of relative fibular rigidity that are most similar to modern hockey players. The relative fibular diaphyseal rigidity of hockey players has been previously explained as the consequence of their dynamic and repetitive change of direction. Late Upper Paleolithic and Neolithic individuals are thought to have been highly terrestrially mobile, while Iron Age people were probably fairly sedentary. However, all of the three groups lived in areas of uneven terrain. We concluded that fibular rigidity and relative fibular rigidity are influenced by factors that increase foot eversion/ inversion such as frequent directional changes and uneven terrain. The results of this study suggest that inclusion of the fibula provides a valuable additional perspective that complements traditional predictions of mobility patterns based on the femur or the tibia alone.
Keywords (separated by "-")	Fibula - Tibia - Bioarchaeology - Cross-sectional geometry - Terrain conformation

Chapter 6 The Importance of Considering Fibular Robusticity When Inferring the Mobility Patterns of Past Populations

[AU1] Vitale S. Sparacello, Damiano Marchi, and Colin N. Shaw

Abstract In this chapter we investigate the lower limb structural rigidity (using 6 cross-sectional geometric properties of the diaphyseal midshaft) within a sample of 7 124 individuals from the Late Upper Paleolithic, Neolithic and Iron Age from Italy, 8 Medieval Germany, and twenty-first Century Britain (long distance runners, field 9 hockey players, and sedentary controls). Late Upper Paleolithic, Neolithic and Iron 10 Age samples were settled in rugged areas, whereas the other samples inhabited 11 plain areas. The aim of this study is to assess whether fibular diaphyseal properties 12 reflect mobility patterns or terrain properties in past populations. Both fibular rigid-13 ity and relative fibular rigidity ratio (fibula/tibia) have been analyzed. 14

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V.S. Sparacello

Department of Anthropology, University of New Mexico, Albuquerque, NM, USA

D. Marchi (🖂)

Department of Biology, University of Pisa, Via Derna 1, Pisa 56126, Italy

Evolutionary Studies Institute, University of the Witwatersrand, Johannesburg, South Africa e-mail: dmarchi@biologia.unipi.it

C.N. Shaw

McDonald Institute for Archaeological Research, University of Cambridge, Cambridge, UK

PAVE Research Group, Department of Archaeology and Anthropology, University of Cambridge, Cambridge, UK

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- a valuable additional perspective that complements traditional predictions of mobil-
- ity patterns based on the femur or the tibia alone.

Keywords Fibula • Tibia • Bioarchaeology • Cross-sectional geometry • Terrain
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29 6.1 Introduction

Although it constitutes one of the parameters that are most often investigated in 30 bioarchaeological research, mobility has not yet received a univocal definition. For 31 research aimed at the reconstruction of past activity patterns, mobility is usually 32 broadly defined as the habitual amount of traveling (either through walking or run-33 ning) that characterized a population. However, it is difficult to numerically quan-34 tify mobility in bioarchaeology, for example, through the reconstruction of home 35 ranges or trade networks. Qualitative assessments such as "high" or "low" mobility 36 are then usually used, and are linked to the logistic requirements of different subsis-37 tence strategies (see Wescott 2014) based on ethnographic analogies. 38

Since walking and running are the main causes of anteroposterior (AP) repetitive 39 mechanical loading on lower limbs, the amount of physical activity associated with 40 traversing the landscape can be indirectly quantified through its effects on long bone 41 diaphyses. Research that has investigated the relationship between mobility and 42 long bone diaphyseal structure has generally considered the AP-oriented loads as 43 the main cause of lower limb loading (Ruff 1999, 2000a; Shaw and Stock 2009; see 44 Wescott 2014 and references therein). However, experimental and nonexperimental 45 studies conducted on mammals-including primates-have demonstrated that dif-46 ferent "types" of mobility may considerably influence the amount of mediolateral-47 oriented loads to which the lower limb is subjected (Carlson et al. 2005; Demes 48 et al. 2006; Carlson and Judex 2007; Marchi 2007; Marchi and Shaw 2011; Marchi 49 et al. 2011). Following these findings, here mobility is considered as having two 50 components, both of which influence lower limb morphology. The first component 51 is the amount of traveling that people undertake to have access to resources: this is 52 the traditional definition of mobility. The second component is the type of move-53 ment, particularly focused on how movement influences mediolateral (ML) loading 54 (e.g., uphill/downhill and/or on even/uneven terrain). Untangling the concomitant 55 effect of the two components may improve the interpretation of lower limb skeletal 56 properties for behavioral reconstructions. 57

Cross-sectional geometry (CSG) is a biomechanical technique that studies the plastic behavior of long bone diaphyses to adapt to mechanical loads (for reviews, see Pearson and Lieberman 2004; Ruff et al. 2006b; and references therein). Various bioarchaeological studies have described a correspondence between femoral diaphyseal shape and levels of mobility dictated by subsistence patterns. In particular, highly mobile hunter-gatherers generally show

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higher values of femoral shape ratios $(I_x/I_y \text{ and } I_{\text{max}}/I_{\text{min}})^1$ than sedentary agriculturalists (e.g., Ruff and Hayes 1983; Ruff 1987, 1999; Larsen 1995; Stock and Pfeiffer 65 2001; Holt 2003; Ruff et al. 2006a). 66

However, research suggests that distance traveled is not the sole agent of lower 67 limb remodeling; other factors should be taken into account, and possibly factored out 68 when comparing skeletal samples and inferring habitual behavior patterns (Ruff 1999, 69 2000a; Sparacello and Marchi 2008). One of the confounding factors to consider 70 when interpreting lower limb robusticity is the potential influence of topography. Ruff 71 (1999) found that Native American groups characterized by different subsistence 72 economies (preagricultural and agricultural, with assumed differences in patterns of 73 mobility) were not differentiated in femoral diaphyseal robusticity. However, groups 74 coming from more rugged areas showed significantly more robust femora. Based on 75 these results, Ruff (2000a) proposed that once terrain is factored out, the influence of 76 subsistence strategies on lower limb bone robusticity greatly declines. 77

Diaphyseal cross-sectional robusticity may therefore be influenced by both the 78 activity performed and the topography upon which the activity is performed. Further 79 support to this hypothesis came from the comparison of two groups that adopted dif-80 ferent subsistence economies (herding and fishing-agriculture, respectively) settled 81 in the same rugged area (Sparacello and Marchi 2008). Despite differences in pre-82 sumed mobility levels, comparisons did not reveal significant differences in femoral 83 robusticity, but showed significant differences in diaphyseal shape (I_x/I_y) . This was 84 interpreted as reflecting the influence of mobility levels and terrain properties on 85 femoral midshaft robusticity and shape. The high femoral robusticity of both sam-86 ples was interpreted as dictated by terrain ruggedness. The more elliptical diaphyseal 87 shape (greater I_x/I_y ratios) of the Neolithic sample was interpreted as a consequence 88 of higher mobility levels (Sparacello and Marchi 2008). A similar pattern was 89 observed for the tibia in a comparison among several groups that adopted different 90 subsistence economies (hunter-gatherers and herders) who had settled in both plain 91 and mountainous regions (Sparacello et al. 2008). These results suggest that, when 92 comparing groups dwelling in areas with similar topographies, different subsistence 93 economies seem to generate less dramatic differences in lower limb robusticity. 94

Differently from the femur, there is not consistent correspondence between 95 tibial shape (as revealed by I_{max}/I_{min} ratio) and mobility patterns (cf. Stock and 96 Pfeiffer 2001; Holt 2003; Marchi 2008; Marchi et al. 2011). A comparison of 97 upper and lower limb CSG properties in Andaman Islanders and Later Stone 98 Age southern African foragers (Stock and Pfeiffer 2001) showed that 99 Andamanese people had significantly more robust upper limbs than Later Stone 100 Age people. Andamanese people incorporated a significant degree of marine 101 mobility into their behavioral pattern that included swimming and canoe pad-102 dling, which probably led to this result. Later Stone Age people were highly 103 mobile terrestrial hunter-gatherers and were characterized by significantly more 104

 $^{{}^{1}}I_{x}$ is the AP bending rigidity; I_{y} is the ML bending rigidity; I_{max} is the maximum moment of area; and I_{min} is the minimum moment of area of a bone at a cross section (Ruff and Hayes 1983). Femoral I_{x}/I_{y} is normally referred to as a mobility index.



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robust lower limbs, and more AP-strengthened femoral cross sections. However, 105 Later Stone Age people did not display statistically significant differences 106 (more) in platycnemic tibiae relative to the Andamanese people. It therefore 107 appears that femoral cross-sectional shape shows a more strict correspondence 108 with inferred mobility levels than the tibia. A similar pattern was observed in 109 European skeletal samples ranging from the Early Upper Paleolithic to the 110 Bronze Age (Holt 2003; Sládek et al. 2006a, b; Marchi 2008; Marchi et al. 2011; 111 see also Pearson et al. 2014, for an analysis of the weak correlation between 112 femoral and tibial shape indices). 113

In a study of the associated influence of activity, climate, and mechanical con-114 straints for tissue economy in the lower limb, Stock (2006) found that tibial diaphy-115 seal robusticity was less correlated than femoral diaphyseal robusticity with climate 116 and body shape, and showed less inherent variance in the samples. Stock (2006) 117 concluded that the strongest morphological correlates of terrestrial mobility are 118 femoral cross-sectional shape and tibial diaphyseal robusticity. A recent study on 119 modern athletes and a bioarchaeological sample also found a good correspondence 120 between tibial robusticity (relative to humeral robusticity) and mobility patterns 121 (Shaw and Stock 2013). 122

Recently, Shaw and Stock (2009) compared three modern human samples: cross-123 country runners, field hockey players, and sedentary controls. Results revealed that 124 the two highly mobile athlete samples had significantly more robust tibiae com-125 pared to controls. Further, diaphyseal shape differences between runners and hockey 126 players were significant, with runners showing higher values (more elliptical diaph-127 vseal cross sections). This result was interpreted as reflecting a greater degree of 128 AP-oriented bending stress in runners-whose mode of locomotion was mainly 129 linear-compared to field hockey players who performed frequent changes of direc-130 tion (Spencer et al. 2004, and references therein). The results of Shaw and Stock 131 (2009) suggest that tibial diaphyseal robusticity provides information about the 132 level of mobility, while tibial cross-sectional shape is more informative about the 133 directionality of loading. 134

Despite the abundance of work focused on the relationship between bone struc-135 ture and mobility, the fibula has been often overlooked in anthropological studies 136 because most of the body weight is supported by the tibia (Marchi and Shaw 2011 137 and references therein). Moreover, in bioarchaeological skeletal samples the fibula 138 is less frequently found intact compared to the tibia. Nevertheless, the fibula may 139 provide valuable information on mobility patterns. Studies on living hominoids 140 have demonstrated that the relative fibular diaphyseal robusticity (tibia/fibula) cor-141 responds with variation in locomotor patterns (Marchi 2007). Specifically, primarily 142 arboreal hominoids possess a relatively more robust fibula compared to primarily 143 terrestrial hominoids. These differences have been interpreted as a likely conse-144 quence of a more mobile fibula (Barnett and Napier 1953) and more adducted 145 hindlimb position in the former (Carlson et al. 2005), which is necessary for travel 146 in arboreal environments. 147

Marchi and Shaw (2011) analyzed fibular robusticity and tibio-fibular ratios in university varsity athletes and controls, in order to assess whether fibular properties

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are influenced by the intensity and type of mobility (i.e., straight line movement or 150 with frequent changes of direction). Results showed a trend of increased fibular 151 diaphyseal robusticity from controls to runners to field hockey players, with a signifi-152 cant difference (P < 0.05) between field hockey players and controls. Moreover, rela-153 tive fibular robusticity (fibula/tibia ratio) was significantly greater in hockey players 154 compared to runners. The authors concluded that fibular robusticity and relative 155 fibula/tibia robusticity may reflect adaptation to patterns of mobility that incorporate 156 high degrees of foot eversion and inversion. In field hockey players, foot eversion/ 157 inversion is likely to have been caused by constant and abrupt changes of direction. 158 When studying mobility patterns in bioarchaeological research, frequent foot ever-159 sion and inversion may have been caused by mobility in highly uneven terrains. 160 Comparison of Italian Neolithic and Iron Age skeletal series from individuals dwell-161 ing in mountainous terrains versus medieval and modern samples seems to provide 162 support for this interpretation (Marchi et al. 2011; see also Higgins 2014, who found 163 a similar effect of terrain properties on ML bending of bovid metacarpi). 164

In another study, Rantalainen et al. (2010) investigated the influence of locomo-165 tor patterns on tibial and fibular rigidity. The authors found that the repetitive loadings 166 associated with running appear to primarily influence tibial robusticity. According 167 to their model, runners would show low levels of relative fibular robusticity. This 168 prediction was empirically supported by the results of Marchi and Shaw (2011). By 169 contrast, Rantalainen et al. (2010) suggested that high impact activities involving 170 jumping influence the mechanical strength of both the tibia and the fibula. The 171 authors concluded that although the tibia and the fibula are spatially close, they 172 experience substantially different loading environments. Analyzing both the fibula 173 and the tibia may therefore help in obtaining a more thorough understanding of 174 mobility patterns. 175

In the present study we analyze tibial and fibular diaphyseal robusticity, and 176 tibio-fibular ratios within bioarchaeological and modern skeletal samples. The sam-177 ples are characterized by different levels of mobility: in the bioarchaeological sam-178 ples, mobility is inferred from archaeological evidence and femoral shape indices, 179 while modern samples include varsity athletes and sedentary controls (Shaw and 180 Stock 2009; Marchi and Shaw 2011). Three bioarchaeological samples come from 181 mountainous areas, while one bioarchaeological sample and the modern samples 182 come from areas associated with relatively flat terrain (see below). The aim of this 183 research is to assess whether fibular CSG properties can successfully be integrated 184 with the information drawn from femoral and tibial data to provide a more accurate 185 reconstruction of mobility levels and types in bioarchaeological populations. In par-186 ticular, the presence of samples characterized by varying degrees of mobility com-187 ing from both relatively flat and rugged areas gives the opportunity to untangle the 188 possible concomitant influence of mobility and terrain properties on the tibio-fibular 189 complex. On the basis of the above research on tibial and fibular robusticity, we 190 hypothesize that tibial robusticity will be influenced by both mobility levels and 191 terrain ruggedness, while fibular robusticity and relative fibular proportions will 192 mainly reflect foot eversion/inversion, associated with the terrain ruggedness. In 193 particular, we hypothesize that (1) when comparing groups dwelling in areas with 194



similar terrain properties, tibial diaphyseal robusticity will be higher in more mobile
groups; (2) when comparing groups with similar levels of mobility, tibial diaphyseal
robusticity will be higher in groups settled in mountainous (more rugged) terrain;
and (3) when fibular diaphyseal robusticity and the fibula/tibia robusticity ratio will
be higher in skeletal series drawn from more mountainous/uneven areas, indepen-

200 dent of mobility levels.

201 6.2 Materials and Methods

202 6.2.1 The Sample

The skeletal series analyzed here include four bioarchaeological and three modern 203 samples. Only male individuals were included in this study, given that, cross-204 culturally, most of the mobility-oriented activities were performed by males, at least 205 beginning with the Neolithic (Ehrenberg 1989). Bioarchaeological skeletal series 206 include 7 Late Upper Paleolithic, 15 Neolithic, 33 Iron Age, and 14 medieval indi-207 viduals (Table 6.1). Mobility levels for these samples are presumed based on archae-208 ological information and ethnographic analogy with modern or recent groups (e.g., 209 Hudson and Hudson 1980; Kelly 1983, 1995; Larsen 1995; Carlson et al. 2007). 210

The Late Upper Paleolithic sample (12,000–10,000 BP) (Alessio et al. 1967; Martini et al. 2004; Paoli et al. 1980) consists of individuals from the sites of Arene Candide (Liguria, Northwestern Italy) and Romito (Calabria, Southern Italy).

t1.2	Period	Ν	Necropolis	Terrain	Subsistence	Mobility level
t1.3	Late Upper	7	Arene Candide 2, 4, 5, 10	Mountainous	Hunting	High
t1.4	Paleolithic		Romito 3, 7, 8			
t1.5	Neolithic	15	Arene Candide 2 Tinè, E VI,	Mountainous	Herding	High
t1.6			7, 8, IX, XIII			
t1.7			Arma dell'Aquila II			
t1.8			Bergeggi 2, 3			
t1.9			Boragni 2			
t1.10			Pollera 10, 13, 30, 32, 6246			
t1.11	Iron Age	35	Alfedena 1, 4, 5, 6, 9, 18, 19,	Mountainous	Agriculture-	Moderate-Low
t1.12			21, 40, 41, 53, 66, 67, 68,		herding	
t1.13			73, 82, 83, 84, 88, 89, 90,			
t1.14			91, 97, 98, 102, 105, 109,			
t1.15			114, 115, 116, 119, 121,			
t1.16			126, 130, 132			
t1.17	Medieval	14	Neuburg 24, B21, B26, 61,	Plain	Agriculture	Low
t1.18			65_57, 75, 80, 101_73,			
t1.19			109, 111, 167, 175, 176,			
t1.20			189			

t1.1 Table 6.1 Bioarchaeological skeletal samples composition

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Subsistence for these peoples was based on hunting mid-sized ungulates such as red214deer, roe deer, and ibex (Mussi 2001; Martini et al. 2009), an activity pattern that215required a high level of mobility (Kelly 1983, 1995).216

Neolithic individuals date to 6,000-5,500 BP (Maggi 1997) and were unearthed 217 from a series of neighboring caves including Arene Candide (Liguria, Northwestern 218 Italy). The main subsistence activity for Neolithic people was sheep herding, 219 although agriculture played a minor role (Marchi et al. 2006, 2011, and references 220 therein). In general, pastoral systems rely on both seasonal movements among vari-221 ous pasture zones (ranging from 20 to more than 300 km), as well as daily dispersal 222 from encampments (Niamir-Fuller 1999). Herder mobility is predicated on the 223 availability of pasture and water. For example, in arid areas cattle herders may walk 224 8–9 km per day (Coppolillo 2000; Turner and Hiernaux 2002) and, during the dry 225 season, up to 17 km per day (Adriansen and Nielsen 2005). Therefore, the most 226 mobile herders perform both high logistic and high residential mobility. This level 227 of mobility overlaps with that of modern hunter-gatherers (Kelly 1983, 1995; 228 Marlowe 2005). The Ligurian Neolithic people were part of a small-scale transhu-229 mance system in a region that virtually lacked pastures (Marchi et al. 2006, 2011), 230 a subsistence strategy that likely required logistic mobility. High mobility of the 231 Ligurian Neolithic people was supported by previous analysis performed on their 232 femoral CSG (Marchi et al. 2006). 233

Iron Age individuals date back to 2,600–2,400 BP and were unearthed from the necropolis of Alfedena in Abruzzo (central Italy). The economy at Alfedena was based on agriculture, while a small subset of the population was involved in herding. This subsistence strategy would have required lower population level mobility levels (Sparacello et al. 2011). Accordingly, the Iron Age sample is associated with a relatively circular femoral shape.

Medieval individuals (1,300 BP) were mainly agriculturalists (Marchi 2007; 240 Benjamin Höke, pers. comm.) and were unearthed from the necropolis of Neuburg 241 in Bavaria (Southern Germany). Historical studies indicate that early medieval 242 peasants had little or no opportunity for residential mobility and lived the majority 243 of their lives close to the field (Le Goff 1988, 1990). Furthermore, previous comparisons of hunter-gatherer and agricultural skeletal remains suggest decreased levels of mobility in agricultural populations (Larsen 1995; Ruff et al. 2006a). 246

The modern samples include 15 field-hockey players, 15 cross-country runners, 247 and 21 sedentary control individuals (Shaw and Stock 2009). Two additional indi-248 viduals practicing rugby were included in the field hockey players' sample, given 249 the similarity of the movements involved in the two sports (Marchi and Shaw 2011). 250 The two athlete samples are characterized by high levels of mobility. However, in 251 general, runners travel in a relatively straight-ahead direction, while hockey players 252 perform frequent and abrupt changes of direction (Shaw and Stock 2009; Marchi 253 and Shaw 2011). 254

Bioarchaeological samples come from areas that are easy to categorize topographically, being either flat or fairly rugged. Modern samples performed their sports in mainly flat terrain. However, we (Sparacello et al. 2008) developed a protocol to assess terrain ruggedness in an objective way using the freeware program 258

Google EarthTM. A circle with a diameter of 5 km is drawn, with the archaeological 259 site at the center. An altimetry profile is calculated using a function of Google 260 EarthTM for the four paths drawn along the directions N-S, E-W, NW-SE, SW-NE of 261 the circle (Sparacello et al. 2008). The altimetry profile provides the sum of the 262 elevation gain and loss along the path. We consider the average of this value among 263 the four paths as an effective measure of terrain ruggedness. In fact, the value pro-264 vides a standardized assessment of the amount of vertical traveling (either uphill or 265 downhill) imposed by traversing a landscape. Moreover, the value is not dependent 266 on the altitude of the starting point. After testing the method on several landscapes, 267 it was decided to consider "flat" terrain as having an average value between 0 and 268 500 m for the sum of elevation gain and loss. "Moderately hilly" was defined as a 269 sum between 500 and 1,000 m; "hilly-mountainous" as a sum between 1,000 and 270 1,500 m. Finally, we consider "mountainous" territory to have a sum above 1,500 m. 271 For example, the Black Hills in Wyoming (United States) and the iconic landscape 272 of the Tuscany hills (Italy) both average ~1,000 m, while the Himalayan village of 273 Chukhung, Nepal, at the fringes of Mount Everest, averages 2,512 m. Using this 274 method, the site of Neuburg falls in the "flat" category, averaging 202.5 m, while 275 Alfedena (average 1,580 m), Arene Candide (average 1,868 m), and Romito (aver-276 age 1,875 m) fall in the "mountainous" category. 277

278 6.2.2 Methods

Cross-sectional properties were calculated at 50 % bone length, using three differ-279 ent methods: (1) polysiloxane molds and measurements of biplanar radiographs of 280 the diaphysis for the Late Upper Paleolithic sample and the majority of the Ligurian 281 Neolithic sample (O'Neill and Ruff 2004); (2) polysiloxane molds of the cortical 282 contour and regression equations for some Ligurian Neolithic individuals and the 283 Iron Age sample (Sparacello and Pearson 2010); (3) pOCT scans for the modern 284 athlete and control samples (Shaw and Stock 2009). Previous research has demon-285 strated the compatibility of results obtained using different techniques (Stock 2002; 286 Stock and Shaw 2007; Sparacello and Pearson 2010; Davies et al. 2012). For the 287 first two methods, dry bones were positioned following Ruff (2002) and Marchi 288 (2007); for the third method, limbs of the living individuals where held in place 289 using purpose-designed clamping devices as described in Shaw and Stock (2009). 290

The cross-sectional variable Z_p (section modulus) is used here to evaluate overall 291 bone rigidity in both the tibia and the fibula. Z_p is calculated by raising the polar 292 second moment of area (J) to the power of 0.73 (Ruff 1995, 2000b). Mechanical 293 loading of long bones is a function of physical activity, bone length, and body mass 294 (Ruff 2000b). Thus, to identify behaviorally significant differences in robusticity, it 295 is necessary to control for the effects of body size. Z_p was scaled for body size by 296 dividing it by bone mechanical length and body mass (Ruff 2000a, b). Body mass was 297 calculated from femoral head superoinferior (SI) diameter by averaging the values 298 obtained using equations in Grine et al. (1995), McHenry (1992), and Ruff et al. (1991). 299



Diaphyseal shape in CSG refers to the ratios of second moment of areas (SMAs), 300 which are proportional to bending rigidity. For the tibia, I_{max}/I_{min} (ratio of the maximum and minimum SMA) was used, while for the femur, I_x/I_y (ratio of SMAs calculated about ML and AP planes) was used. Relative fibular robusticity was calculated as $100 \times (J$ fibula/J tibia). Shape indices and relative fibular robusticity are derived from unstandardized data. 305

Statistical analysis consisted of a one-way ANOVA for each variable considered 306 in this study, and both Fisher LSD and Tukey HSD post-hoc tests. Using Fisher LSD 307 with seven groups increases the risk of Type I errors, because it does not correct for 308 multiple comparisons. Tukey HSD corrects for multiple comparisons, but given the 309 small sample size of several samples included here, this test may be too restrictive 310 for the purposes of this study. We present results for both tests and base our discus-311 sion on the LSD test. However, we note instances for which LSD and HSD tests 312 provide different results. In those cases, results should be further verified using a 313 larger sample size. All statistical analyses were carried out with STATISTICA 10 314 (Statsoft Inc. 2011). 315

6.3 Results

Table 6.2 shows the mean, standard deviations, Fisher LSD, and Tukey HSD posthoc results for comparisons of femoral, tibial, and fibular CSG variables. Figure 6.1 318 displays the femoral shape index (I_x/I_y) of those bioarchaeological samples for 319 which the femur was available (Late Upper Paleolithic, Neolithic, and Iron Age). 320 The Late Upper Paleolithic and Neolithic samples show midshaft femora that are more elliptical and AP oriented, while the Iron Age sample displays significantly more circular sections (Fig. 6.1 and Table 6.2). 321

Figure 6.2 displays variation in tibial Z_p across all samples. Tibial Z_p is higher in 324 the bioarchaeological samples settled in mountainous areas (Late Upper Paleolithic, 325 Neolithic, and Iron Age samples) when compared with the sedentary sample settled 326 in a flat terrain (medieval individuals). However, only the comparison between the 327 Neolithic and medieval sample is significant after correcting for multiple compari-328 sons. Within the samples settled in a rugged terrain, the less mobile Iron Age indi-329 viduals have the lowest average value of tibial Z_p , and the difference is significant 330 when compared with Neolithic individuals. Late Upper Paleolithic, Neolithic, and 331 Iron Age individuals are not significantly different from runners (which have the 332 highest values among modern samples) and have significantly higher tibial Z_p than 333 the sedentary control sample (Table 6.2). 334

Figure 6.3 displays variation in tibial shape (I_{max}/I_{min}) . Tibial shape reveals a diachronic decreasing trend from the Late Upper Paleolithic sample to the medieval sample, and all pairwise comparisons are significant according to LSD post-hoc analyses, but not according to the Tukey HSD post-hoc analyses (Table 6.2). When compared with the modern athlete samples, the Late Upper Paleolithic sample shows a significantly higher shape index than runners, while the Neolithic and 340

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t2.1	Table 6.2 Temporal diffe:	rences in	diaphyseal geo.	metric proper	ties of the fen	nur, tibia, and fibu	ıla			
t2.2	$I_{\mathcal{M}}$ Femur	Ν	Mean	SD	NEOL	IRONAGE				
t2.3	LUP	7	1.32	0.21	NS^{a}	***				
t2.4	NEOL	13	1.34	0.20		***				
t2.5	IRONAGE	27	1.03	0.14						
t2.6	Z_p Tibia	Ν	Mean	SD	NEOL	IRONAGE	MEDGER	HOCKEY	RUNNERS	CONTROL
t2.7	LUP	7	101.39	52.08	NS	NS	(NS)*	NS	NS	$^{**}(*)$
t2.8	NEOL	15	110.22	14.48		$^{***}(*)$	***	* *	NS	* *
t2.9	IRONAGE	33	98.39	10.59			(NS)**	NS	NS	* *
t2.10	MEDGER	14	88.5	12.71				NS	***(**)	NS
t2.11	НОСКЕҮ	17	92.27	9.33	2				(NS)**	NS
t2.12	RUNNERS	15	103.4	10.1						***
t2.13	CONTROL	21	85.28	9.7						
t2.14	I_{max}/I_{min} Tibia	Ν	Mean	SD	NEOL	IRONAGE	MEDGER	HOCKEY	RUNNERS	CONTROL
t2.15	LUP	7	3.55	0.57	***	***	***	***	** *	***
t2.16	NEOL	15	2.55	0.44		*(SN)	***	(NS)*	NS	(NS)*
t2.17	IRONAGE	33	2.27	0.37		2	(NS)**	NS	(NS)**	NS
t2.18	MEDGER	14	1.93	0.29				(NS)*	**	(NS)*
t2.19	HOCKEY	17	2.22	0.26					(NS)**	NS
t2.20	RUNNERS	15	2.61	0.50						(NS)**
t2.21	CONTROL	21	2.26	0.28						
t2.22	Z_p Fibula	Ν	Mean	SD	NEOL	IRONAGE	MEDGER	HOCKEY	RUNNERS	CONTROL
t2.23	LUP	L	14.58	3.66	NS	NS	***(**)	(NS)*	(NS)**	***(**)
t2.24	NEOL	15	15.17	3.10		NS	***	**(**)	***(**)	***
t2.25	IRONAGE	21	13.39	3.12			***(**)	(NS)*	(NS)*	***(**)
t2.26	MEDGER	14	10.01	2.01				NS	NS	NS
t2.27	HOCKEY	17	11.6	2.40					NS	NS

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CONTROL 21 10.1 2.23 (J Fibula/ J Tibia) × 100 N Mean SD NEOL IRONAGE MEDGER HOCKEY RUNNERS CON LUP 7 7,45 2.57 NS NS (NS)* NS (*)** (NS) NEOL 15 7.04 1.77 NS (NS)* NS (*)** (NS) NEOL 15 7.04 1.77 NS (NS)** NS (*) NS NEOL 17 6.18 1.77 NS (NS)** NS (NS)* NS MEDGER 14 5.45 1.32 NS	RUNNERS	15	11.13	2.61						NS
$ \begin{array}{c c c c c c c c c c c c c c c c c c c $	CONTROL	21	10.1	2.23						
$ \begin{array}{cccccccccccccccccccccccccccccccccccc$	(J Fibula/ J Tibia)×100	Ν	Mean	SD	NEOL	IRONAGE	MEDGER	HOCKEY	RUNNERS	CONTRC
NEOL 15 7.04 1.77 NS (NS)* NS (**)*** (NS IRONAGE 21 7.04 2.00 (NS)** NS (**)**** (NS) MEDGER 14 5.45 1.32 NS NS NS NS NS HOCKEY 17 6.18 1.72 NS NS NS NS NS HOCKEY 17 6.18 1.72 NS NS NS NS NS RUNNERS 15 4.91 1.23 NNNERS 1.23 NS NS NS CONTROL 21 5.70 1.72 NS NS NS NS **0.01 2.00 1.72 NS NS NS NS NS ***0.01 $p < 0.001$; **** $p < 0.001$ *** $p < 0.001$; **** $p < 0.001$;	LUP	7	7.45	2.57	NS	NS	(NS)*	NS	$^{**}(*)$	$(NS)^*$
IRONAGE 21 7.04 2.00 (NS)** NS (NS) MEDGER 14 5.45 1.32 NS NS NS NS HOCKEY 17 6.18 1.72 NS NS NS NS RUNNERS 15 4.91 1.23 NS NS NS NS RUNNERS 15 4.91 1.23 NS NS NS NS RUNNERS 15 4.91 1.23 NS NS NS CONTROL 21 5.70 1.72 NS NS NS Fisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant; $*_r$ * **0.01 $-p < 0.001$; **** $p < 0.001$ **** $p < 0.001$ *** NS NS	NEOL	15	7.04	1.77		NS	(NS)*	NS	**(*)	(NS)*
MEDGER145.451.32NSNSNSHOCKEY176.181.72(NS)*NSRUNNERS154.911.23NSCONTROL215.701.72NSFisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant: ***0.01 < $p < 0.001$; ******0.01 < $p < 0.001$; ******0.01	IRONAGE	21	7.04	2.00			(NS)**	NS	***(**)	(NS)*
HOCKEY17 6.18 1.72 $(NS)*$ NS RUNNERS154.911.23 NS CONTROL21 5.70 1.23 NS Fisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant; $*_{I}$ **0.01 < $p < 0.001; ***p < 0.001$	MEDGER	14	5.45	1.32				NS	NS	NS
RUNNERS154.911.23NSCONTROL21 5.70 1.72 Prisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant: $*_1$ **0.01 < $p < 0.001$; *** $p < 0.001$	носкеу	17	6.18	1.72					(NS)*	NS
CONTROL 21 5.70 1.72 ^a Fisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant; $*_{t}$ **0.01 < $p < 0.001$; **** **0.01 < $p < 0.001$; ****	RUNNERS	15	4.91	1.23						NS
Fisher LSD post-hoc test and Tukey HSD post-hoc test (in parentheses) are both reported in cases where results were different. <i>NS</i> nonsignificant; $*_{I}$ *0.01 < p < 0.001; *** p < 0.001	CONTROL	21	5.70	1.72						
0.01p<0.001; *p<0.001	^a Fisher LSD post-hoc test	and Tuke	y HSD post-he	oc test (in p	arentheses) are	e both reported ii	a cases where rea	sults were differe	ent. NS nonsignifi	cant; $*p<0.05$
	0.01< <i>p</i> <0.001; * <i>p</i> <0	0.001		•	0)	•
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6 The Importance of Considering Fibular Robusticity...



Fig. 6.1 Femoral shape index I_x/I_y . I_x =anteroposterior bending rigidity; and I_y =mediolateral bending rigidity. *LUP* Late Upper Paleolithic, *NEOL* Neolithic, *IRONAGE* Iron Age



Fig. 6.2 Tibial section modulus Z_p : size-standardized diaphyseal torsional rigidity. *LUP* Late Upper Paleolithic, *NEOL* Neolithic, *IRONAGE* Iron Age, *MEDGER* Medieval, *HOCKEY* field hockey players, *RUNNERS*, cross-country runners, *CONTROL* sedentary control





Fig. 6.3 Tibial shape index I_{max}/I_{min} : I_{max} = maximum bending rigidity; I_{min} = minimum bending rigidity. *LUP* Late Upper Paleolithic, *NEOL* Neolithic, *IRONAGE* Iron Age, *MEDGER* Medieval, *HOCKEY* field hockey players, *RUNNERS* cross-country runners, *CONTROL* sedentary control

runner samples show comparable values. Iron Age individuals have a shape index 341 that is comparable with hockey players and the control sample. 342

Figure 6.4 displays variations in fibular Z_p . As seen for tibial Z_p , within bioar-343 chaeological samples, fibular Z_p of the samples settled in mountainous areas (Late 344 Upper Paleolithic, Neolithic, and Iron Age) is significantly higher than values in the 345 sedentary control sample and those settled in flat terrain (medieval sample). These 346 results are still significant after correcting for multiple comparisons with the Tukey 347 HSD test. The bioarchaeological samples settled in mountainous areas also display 348 higher values of fibular Z_p than most of the modern samples. After correcting for 349 multiple comparisons by using the Tukey HSD test, comparisons of the Late Upper 350 Paleolithic and Iron Age samples with hockey players and runners are not signifi-351 cant at the 0.05 level. Among the samples settled in rugged terrains, the less mobile 352 Iron Age individuals display the lowest average fibular Z_p , but differences from 353 other samples settled in rugged terrains are not statistically significant. 354

Figure 6.5 displays variations in relative fibular rigidity $[100 \times (\text{fibula } J/\text{ tibia } J)]$. 355 All of the bioarchaeological samples settled in mountainous areas (Late Upper 356 Paleolithic, Neolithic, and Iron Age samples) have a relatively more robust fibula 357 when compared to the medieval, runner, and control samples. However, after cor-358 recting for multiple comparisons, the same groups show a significantly higher value 359 of relative fibular rigidity only in comparison to runners. No significant difference 360 is present when compared with hockey players. Finally, no differences in relative 361 fibular robusticity are present within samples settled in a rugged terrain. 362



Fig. 6.4 Fibular section modulus Z_p : size-standardized diaphyseal torsional rigidity. *LUP* Late Upper Paleolithic, *NEOL* Neolithic, *IRONAGE* Iron Age, *MEDGER* Medieval, *HOCKEY* field hockey players, *RUNNERS* cross-country runners, *CONTROL* sedentary control



Fig. 6.5 Fibular relative robusticity: ratio between fibular J (polar moment of area) and tibial J. *LUP* Late Upper Paleolithic, *NEOL* Neolithic, *IRONAGE* Iron Age, *MEDGER* Medieval, *HOCKEY* field hockey players, *RUNNERS* cross-country runners, *CONTROL* sedentary control

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6.4 Discussion and Conclusion

The purpose of this research was to investigate the concomitant effects of mobility 364 level and mobility type on lower limb mechanical properties, and in particular, fibu-365 lar robusticity and tibio-fibular robusticity ratios. We compared bioarchaeological 366 and modern samples, each with different levels of mobility (known or inferred on 367 the basis of subsistence), and with or without factors influencing ML loadings 368 (sport-induced changes in direction or terrain ruggedness). Overall, the results sug-369 gest that including the fibula in bioarchaeological behavioral reconstruction may 370 provide insights on the "type" of mobility performed. 371

Femoral shape indices could be calculated for Late Upper Paleolithic, Neolithic, 372 and Iron Age individuals and confirm the expectations based on previous research: 373 Late Upper Paleolithic and Neolithic individuals show similarly elliptical and 374 AP-oriented femoral midshaft cross sections that are likely the result of high mobil-375 ity levels, while Iron Age people display a significantly more circular midshaft 376 shape. This finding is in agreement with Ruff's work (1999, 2000a), which con-377 cluded that femoral shape indices are good indicators of mobility levels after terrain 378 is factored out. Tibial cross-sectional properties provide a less clear correspondence 379 with mobility levels. Given the same terrain, tibial Z_p is generally higher in more 380 mobile groups, as evidenced by the comparison between Neolithic and Iron 381 Age individuals, and between modern athletes and controls. However, if mobility was 382 the only factor responsible for tibial diaphyseal robusticity, we would expect the Late 383 Upper Paleolithic individuals to be significantly more robust than Iron Age individuals 384 and that Iron Age individuals should not be significantly more robust than medieval 385 individuals. Instead, we did not find any significant difference between Late Upper 386 Paleolithic and Iron Age individuals, while the latter showed significantly more robust 387 tibiae than medieval individuals (although the comparison is nonsignificant after cor-388 recting for multiple comparisons). For the comparison between Late Upper Paleolithic 389 and Iron Age samples, the small sample size of the Late Upper Paleolithic sample 390 could have played a role. We propose that terrain plays a major role in determining 391 tibial diaphyseal robusticity. As Ruff (1999, 2000a) suggested for the femur, when 392 comparing groups settled in similar terrains, the influence of different mobility levels 393 seems to decline. This would also explain why the Iron Age individuals, who we 394 assume were not very mobile but were settled in a mountainous area, show tibial Z_p 395 values significantly higher than medieval individuals and sedentary modern controls, 396 and comparable with the ones shown by hockey players. 397

Previous research hypothesized that tibial shape may be influenced by both 398 mobility level (increasing AP bending rigidity, and thus I_{max}) and frequent inversion/ 399 eversion of the foot caused by frequent changes of direction or terrain unevenness 400 (increasing the ML bending rigidity, and thus I_{\min}) (Marchi et al. 2011; see also 401 Higgins 2014, for a comparable result in bovid metacarpals). Taking into account the 402 influence of both mobility and terrain conformation on tibial shape, we would pre-403 dict that, when comparing groups settled in areas with similar topographies, more 404 mobile groups will show higher shape indices (less circular diaphyseal cross sec-405 tions). Our results partially support these expectations, but some pairwise differences 406

are difficult to explain in this framework and call for more investigation on the 407 reliability of tibial shape as an indicator of mobility levels. Within groups settled in 408 a mountainous terrain, the more mobile Late Upper Paleolithic and Neolithic indi-409 viduals show a higher shape index than Iron Age individuals. However, Late Upper 410 Paleolithic individuals have extremely platycnemic tibiae (Fig. 6.3); if tibial shape 411 was strictly correlated with mobility, this would signal that these individuals were 412 much more mobile than Neolithic individuals. Although this explanation may be 413 possible, the signal should have been similar when comparing femoral shape and 414 tibial robusticity. Even more problematic is the result of comparisons involving 415 medieval and control individuals. It is difficult to imagine a more sedentary lifestyle 416 than the one performed by modern college students who work out less than one hour 417 a week (Shaw and Stock 2009). The medieval agricultural lifestyle required at least 418 some degree of mobility due to farming activities. Yet, medieval individuals show 419 significantly less elliptical tibial cross-sectional shape than control individuals. Both 420 samples dwelled on flat terrain, which excludes the possibility that the higher shape 421 in medieval individuals is due to traversing rugged terrains. It is more likely that, as 422 Stock (2006) suggested, tibial shape is influenced by factors in addition to mobility 423 and terrain, causing the extreme values found here in Late Upper Paleolithic and 424 medieval German individuals (Fig. 6.3). 425

Mobility as generally implied in bioarchaeological studies, i.e., the amount of 426 traveling due to subsistence activities, is probably only one of the factors that char-427 acterize lower limb robusticity and shape. The type of substratum, different inten-428 sity and repetitiveness of activity, and the linearity or nonlinearity of the movement 429 should be taken into account when analyzing mobility (Carlson and Judex 2007; 430 Shaw and Stock 2009; Carlson 2014). For the Late Upper Paleolithic and medieval 431 samples, activities such as long distance running or plowing, or other factors hith-432 erto not investigated, may have had an influence on shaping lower limb properties. 433 However, it is difficult to incorporate information on the type of movements per-434 formed by past populations for subsistence tasks. It appears that the inclusion of the 435 fibula in the study of lower limb bone structure can provide useful insights when 436 developing behavioral interpretations in bioarchaeological contexts. 437

While tibial Z_p is significantly higher in the Neolithic sample when compared 438 with the Iron Age sample (a difference that we interpreted as due to different levels 439 of mobility in similar terrains), the groups settled in mountainous areas show more 440 robust fibula compared with non-mountainous samples, regardless of the assumed 441 level of mobility (although some of the pairwise comparisons would not be signifi-442 cant after correcting for multiple comparisons). Furthermore, while runners have 443 the highest tibial rigidity among modern samples (Fig. 6.2), no significant differ-444 ence in fibular robusticity is present among modern groups, and the highest value is 445 displayed by hockey players (Fig. 6.4). Fibular Z_p appears, therefore, not signifi-446 cantly influenced by the level of mobility, but mainly correlated with terrain proper-447 ties and with sport-dictated frequent changes of direction. 448

The pattern described above for fibular diaphyseal rigidity is more apparent when considering the ratio between fibular and tibial diaphyseal rigidity. All the groups settled in a mountainous terrain show significantly higher fibula/tibia ratios

than all other groups (with the exception of hockey players). This ratio appears not 452 to be influenced by mobility levels given equivalent terrain conditions. In fact, Late 453 Upper Paleolithic, Neolithic, and Iron Age individuals display similar values, and 454 also medieval, modern runners, and control individuals are not significantly differ-455 ent from each other. Hockey players show the highest fibula/tibia ratio among 456 groups settled in plain areas, and the result is significant when compared to the ratio 457 of runners. It therefore appears that what drives the increase in relative (to the tibia) 458 fibular robusticity may be either terrain ruggedness or sport-related abrupt changes 459 of direction, i.e., activities that have in common high levels of foot eversion/inversion. 460 It should be noted, however, that after correcting for multiple comparisons the 461 bioarchaeological samples settled in mountainous areas show significantly higher 462 fibula/tibia ratios only in comparison to runners, whose ratio is low due to high 463 tibial robusticity (Fig. 6.2). This calls for further verification of the results found 464 here using a larger sample size. 465

The above results suggest a clear and coherent correspondence between fibular 466 cross-sectional properties, relative fibular proportions, and factors increasing the 467 frequency of foot eversion/inversion, such as frequent and abrupt changes of direc-468 tion (Marchi and Shaw 2011) and traveling on uneven surfaces (Marchi et al. 2011). 469 Rugged terrain may also increase fibular loading using a different mechanism than 470 increasing the frequency of foot eversion/inversion: traveling downhill on particu-471 larly rugged terrain may increase the frequency of high-impact ground reaction 472 forces that enhance fibular robusticity compared to traveling on level rugged terrain 473 (Rantalainen et al. 2010). The apparent specificity of the response of the tibio-474 fibular complex should be further verified through experimental studies and larger 475 sample sizes. However, the study of the tibio-fibular complex in bioarchaeology 476 may integrate additional inferences about past population mobility. For example, in 477 areas with mixed relief, with plains and mountains, a robust fibula with a high fib-478 ula/tibia ratio may indicate a preferential subsistence-related exploitation of moun-479 tainous areas. The same properties can be used to assess degree of exploitation of 480 inland resources by coastal hunter-gatherers, provided that the inland region is 481 mountainous. 482

Femoral shape and, to a lesser extent, tibial robusticity are integral to inferences 483 of mobility patterns in past populations. Results presented here suggest that fibular 484 analyses also have the potential to improve these inferences by providing anatomical 485 information that may reflect variation in loading directionality and ankle mobility. 486

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AU4	Please provide the citation for references: Lovejoy et al.(1976); Marchi (2004).	

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