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A TCAD-based Methodology to Model the Site-Binding Charge at ISFET/Electrolyte Interfaces

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***Abstract*—We propose a new approach to describe in commercial TCAD the chemical reactions that occur at dielectric/electrolyte interface and make the ISFET sensitive to pH. The accuracy of the proposed method is successfully verified against available experimental data. We demonstrate the usefulness of the method by performing, for the first time in a commercial TCAD environment, a full two-dimensional analysis of ISFET operation, and a comparison between threshold voltage and drain current differential sensitivities in the linear and saturation regimes. The method paves the way to accurate and efficient ISFET modeling with standard TCAD tools.**

***Index Terms*—ISFET, TCAD, Modeling, Surface Reactions.**

I. Introduction

NANOELECTRONIC biosensors enable low-cost massively parallel detection of reaction by-products and analytes with unprecedented sensitivity [1], [2]. Among many sensor devices, the Ion Sensitive Field Effect Transistor (ISFET, [3], [4], [5]) has recently attracted renewed interest for its compatibility with standard CMOS technology [6], [7], [8], [9]. ISFET-based integrated circuits have been developed for DNA sequencing [10] and for quantitative and digital Polymerase Chain Reaction (PCR) [11]. For instance, the Ion Torrent^{TM} platform has been demonstrated down to the 110 nm CMOS technology node [12] and its further scalability has been investigated theoretically [13].

Until now ISFET modeling has mostly relied on analytical one-dimensional V_T calculations [14], [15], [16], [17], *ad-hoc* simulation programs [18], [19], [20], [21] or general purpose multi-physics platforms [22], [23], [24], [25]. Now that the ISFET has become the mainstream device of a few CMOS-based sensing platforms, accurate and versatile numerical device simulations in an integrated TCAD environment are desirable to support ISFET design, extract the ISFET equivalent circuit parameters and perform mixed device-circuit analysis. Unfortunately, the commercial TCAD of most widespread use [26], [27], [28] is not equipped with models for the complex and material-dependent electrochemical processes that govern ISFET operation [29], [30], [31].

This paper extends previous investigations [32], [33], [34], [35], [36] aimed at developing a commercial TCAD based methodology for the simulation of electronic biosensors. In particular, we present a strategy to describe in TCAD the chemical reactions at the ISFET oxide/electrolyte interface, which were not addressed previously, but are the main contribution to the ISFET threshold voltage sensitivity to pH. For demonstration purposes we adopt as vehicle TCAD the SDevice framework [28]; other platforms have similar limitations [26], [27], so the interest for the proposed approach extends to a broad community of TCAD users.

The paper proceeds as follows: the modeling framework and its verification against existing data is described in Section II. Simulation results about the sensitivity of short channel ISFETs featuring different gate dielectrics in the linear and the saturation regime are reported in Section III. Conclusions are summarized in Section IV.

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The research leading to this work was partially funded by the European Commission FP7 project NANOFUNCTION via the IUNET consortium.

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II. TCAD Models and methods

A. Electrolyte Model

Fig. 1 sketches the structure of an ISFET, where a fluid electrolyte replaces the gate of a conventional MOSFET.

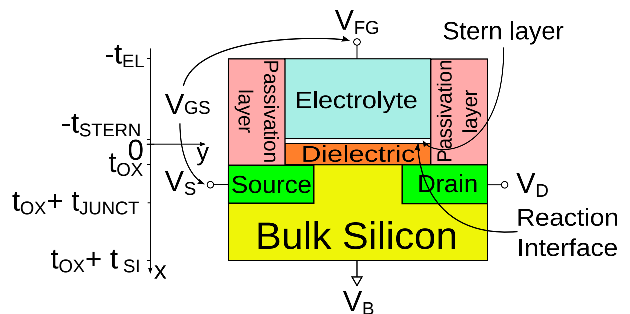

Fig. 1. Sketch of an ISFET device. The y-axis runs along the source-to-drain direction, whereas the x-axis is normal to the channel/dielectric interface. t_{STERN} denotes the thickness of the Stern layer, t_{OX}, t_{JUNCT}, t_{SI}, t_{EL} the thicknesses of the dielectric, S/D junctions, substrate and electrolyte, respectively.

We model the electrolyte as described in [35], that is: we exploit the similarity between the equations for cations and anions in the electrolyte at equilibrium and those for holes and electrons in a semiconductor. A monovalent symmetric (1:1) electrolyte is thus described as an undoped semiconductor with a zero band-gap (hence: $n \cdot p$=$N_C N_V$), a constant permittivity (ϵ_{el}≈80 ϵ_0) and an effective density of states

$$N_C = N_V = \begin{cases} 10^{-3} \cdot N_{av} \left(c_0 + cH_B\right) & \text{for } \mathrm{pH_B} \leq 7 \\ 10^{-3} \cdot N_{av} \left(c_0 + 10^{-14}/cH_B\right) & \text{for } \mathrm{pH_B} > 7 \end{cases}, \tag{1}$$

where N_C and N_V are expressed in cm^{-3}, N_{av}=6.02214·10^{23} mol^{-1} is Avogadro's number, c_0 the salt ion molar concentration (M = mol/l) in the bulk of the solution and

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cH_B=$[H_B^+]$=10^{-pH_B} is the hydrogen concentration in the bulk of the solution normalized to 1 M. As an example, for c_0=1mM and pH_B=3, we have N_C=N_V=$1.2 \cdot 10^{18} cm^{-3}$. The bulk electrolyte is defined as the region with constant potential and a zero net charge density as a result of equal total concentrations of positive and negative ions, respectively represented by p and n; hence n_B=p_B=N_C=N_V.

As shown in [35], provided all ions are monovalent and their mobility and diffusivity are not too different, an equivalent symmetric 1:1 electrolyte can be defined to mimic with good accuracy the electrostatic response of complex multi-ion solutions. Bivalent Mg and Ca ions are sometimes used in buffer solutions (e.g. for cell culture), but typically have much smaller concentration than that of monovalent ones (Na, K, Cl, etc.) [37]. Within these limits the proposed approach is thus applicable also to realistic electrolytes.

B. Site Binding Model

Chemical reactions at the interface between the ISFET gate dielectric and the electrolyte generate a surface charge density [29], [38], [39], [14], [40], [15] which makes the ISFET sensitive to pH. As a first step toward the development of a general methodology, we implement the default formulation of the well known site-binding model [29] of the chemical reactions at the amphoteric silanol (SiOH) groups. These reactions generate a surface charge density [29], [5]

$$\sigma_0(\psi_0) = qN_{sil}\left[\frac{cH_S^2 - K_aK_b}{cH_S^2 + K_bcH_S + K_aK_b}\right] \quad , \qquad (2)$$

where q is the electron charge, N_{sil} is the number of amphoteric silanol surface sites per unit area, cH_S=10^{-pH_S} is the surface H^+ concentration, $K_a = \nu_{SiO^-} \cdot cH_S/\nu_{SiOH}$ and $K_b = \nu_{SiOH} \cdot cH_S/\nu_{SiOH_2^+}$ are the surface dissociation constants [5], where ν_{SiO^-}, ν_{SiOH} and $\nu_{SiOH_2^+}$ are the number of negative, neutral and positive silanol surface sites per unit area, respectively. Under equilibrium conditions, as it is most often the case in the electrolyte of an ISFET, and neglecting steric effects which are relevant only well above physiological salt concentrations ($c_0 \gg$100 mM), the surface and bulk concentrations of all monovalent ions are related by the same Boltzmann factor. For H^+ ions, this relation reads

$$cH_S = cH_B \exp\left(-\frac{q\psi_0}{kT}\right) \quad , \qquad (3)$$

where ψ_0 is the potential difference between the interface and the bulk of the solution.

Equations 2 and 3 are also valid for dielectrics other than SiO_2 where a metal (M) replaces Silicon, and amphoteric sites are generated by MOH groups. This category comprises most of the dielectrics used in the semiconductor technology, such as HfO_2, Al_2O_3 and Ta_2O_5, with the notable exception of Si_3N_4. In fact, besides the SiOH groups formed by oxidation of Silicon, the Si_3N_4 surface is characterized by additional basic sites formed by primary amine groups [41]. Dielectrics such as Si_3N_4 and Al_2O_3 are often preferred because they have better sensitivity, and yield more stable characteristics thanks to the reduced ion diffusivity [42], [43], [44], [45], [46].

A model for the Si_3N_4/electrolyte interface has been proposed in [41] under the assumption that silanol and amine sites behave independently from each other. The expression for the surface charge density then reads [41], [16]:

$$\sigma_0(\psi_0) = qN_{sil}\left(\frac{cH_S^2 - K_aK_b}{cH_S^2 + K_bcH_S + K_aK_b}\right) + \\ + qN_n\left(\frac{cH_S}{cH_S + K_n}\right) \quad , \qquad (4)$$

where N_n is the number of amine surface sites per unit area and K_n the corresponding surface dissociation constant. Eqs. 2, 3 and 4 express the surface charge as a function of the local surface potential, ψ_0.

C. TCAD implementation of the site-binding model

Commercial TCAD allows users to introduce bias dependent surface charges in the form of interface donor or acceptor traps. The charge corresponding to a surface trap density of N_S^a acceptor and N_S^d donor traps per unit area reads

$$\sigma_T = q\left(N_S^d f^d - N_S^a f^a\right) \qquad (5)$$

where f^d and f^a are the occupation probabilities for donor and acceptor traps, respectively. The occupation probability for an acceptor trap is expressed as [28]

$$f^a = \frac{c_C^a + c_V^a}{c_C^a + c_V^a + e_C^a + e_V^a} \quad , \qquad (6)$$

where c_C^a and c_V^a are the capture rates from the conduction and valence band, respectively, and e_C^a and e_V^a are the emission rates to the conduction and valence band, respectively. A similar expression holds for f_d [28].

We exploit this feature of TCAD to introduce the site-binding charge in the simulations self-consistently. Since the sites have amphoteric behaviour and σ_0 can be either positive or negative depending on pH_B and ψ_0, both acceptor and donor traps are necessary to map Eq. 2 into Eq. 5. In the following we analyze acceptor traps; similar considerations apply to donor traps.

SDevice TCAD allows the user to redefine c_C^a, c_V^a, e_C^a and e_V^a as arbitrary functions of the local carrier concentrations, but it is not possible to use ψ_0 as an independent variable, as prescribed by Eqs. 2 and 4. To overcome this difficulty and without loss of generality, we first make the assumption that acceptor (donor) traps exchange carriers only with the conduction (valence) band of the semiconductor representing the electrolyte, respectively; hence, we set c_C^d=e_C^d=c_V^a=e_V^a=0. We also note that (aside from a sign change) the Boltzmann factor in Eq.3 is the same for all monovalent anions (cations), and thus for the total anion (cation) concentration represented by the electron (hole) concentration. In formulae: n_S=$n_B \exp(\psi_0/V_{th})$ and p_S=$p_B \exp(-\psi_0/V_{th})$, where V_{th}=k_BT/q. Therefore, by reminding that n_Sp_S=n_Bp_B and that n_B=p_B, we obtain

$$\exp(-\psi_0/V_{th}) = p_S/\sqrt{n_Sp_S} = p_S/\sqrt{N_CN_V} \quad , \qquad (7)$$

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and we can re-write Eq. 2 as

$$\sigma_0 = qN_{sil}\frac{cH_B^2 p_S - K_a K_b n_S}{K_a K_b n_S + K_b cH_B\sqrt{p_S n_S} + cH_B^2 p_S} \quad . \qquad (8)$$

Eq. 8 eliminates the explicit dependence of σ_0 on ψ_0 in Eq. 2. Following a similar reasoning, it is straightforward to cast also Eq. 4 in the form of a function of n_S and p_S instead of ψ_0. Unfortunately, the default expressions for emission and capture rates in the TCAD do not allow us to match the n_S and p_S dependencies of Eq. 5 to those of Eq. 8.

To overcome this difficulty we then used the Physical Model Interface (PMI) [28], that allows the user to rewrite the emission and capture rates as arbitrary functions of electric field, temperature, electron and hole concentrations at the point where the traps are introduced. By using donor and acceptor trap densities N_S^d=N_S^a=N_{sil} and by assigning to the emission and capture rates the expressions

$$c_V^d = cH_B^2 p_S \quad , \qquad (9a)$$

$$e_V^d = K_a K_b n_S + K_b cH_B\sqrt{n_S p_S} \quad , \qquad (9b)$$

$$c_C^a = K_a K_b n_S \quad , \qquad (9c)$$

$$e_C^a = K_b cH_B\sqrt{n_S p_S} + cH_B^2 p_S \quad , \qquad (9d)$$

we obtain the same dependence of σ_T on pH_B and ψ_0 given by Eq. 8; hence, by Eq. 2 as well. Eq. 4 is also amenable to this TCAD implementation by introducing additional donor traps with area density N_n, and valence band capture and emission rates easily derived from Eq. 4 itself. The parameters K_a and K_b are easily derived from literature data (e.g. Table II) for many gate dielectrics commonly used in microelectronis, whereas cH_B is the hydrogen concentration in the bulk of the solution.

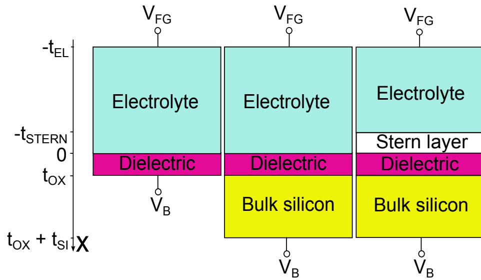

Fig. 2. Sketch of the 1D structure (left) used to validate the PMI implementation of the site-binding model and of a 1D electrolyte/insulator/semiconductor device (center). Right: Same as (center) with the Stern layer.

Fig. 3 compares Eq. 2 with its TCAD implementation for the same set of SiO_2 parameters (Tabs. I, II) for the structure on the left of Fig. 2. The ψ_0 in Eq. 2 is extracted at each V_B from the TCAD simulations. An excellent agreement is observed confirming the validity of the proposed approach.

D. Model of the Stern Layer

Ions in the electrolyte cannot approach the dielectric arbitrarily close, due to their finite ionic radius, and this results in a number of steric effects [47]. The electrolyte region next to the

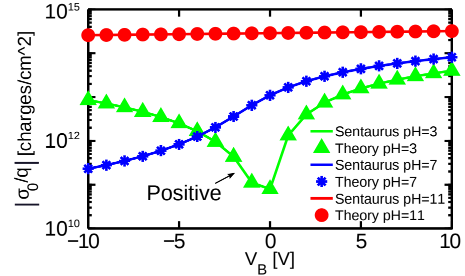

Fig. 3. Comparison between the PMI model (solid lines) and Eq. 2 (symbols) for different V_B, pH and the same set of model parameters. The charge density is always negative unless otherwise specified. V_{FG}=0 V, N_{sil}=5×10^{14} cm^{-2}, c_0=1 mM, SiO_2 gate dielectric.

surface where the net ionic charge is essentially null is called *Stern layer* [48], and it is usually modeled as a thin dielectric. Since for the dielectrics of interest the interface is most often negatively charged at high pH (Fig.3), the thickness (t_{Stern}) is typically assumed equal to the cation's atomic radius [49] and the dielectric constant is set to a value such that the Stern layer capacitance is approximately 20 $\mu F/cm^2$ [30]. A reasonable choice of t_{Stern} appreciably mitigates the inaccuracies due to the lack of specific models for steric effects [35], [34]. For all these reasons it is highly desirable to include the Stern layer in the ISFET model and adjust its capacitance to best fit the experiments. However, if traps as those necessary to mimic the site-binding reactions are located in between the Stern layer and the gate dielectric, then n=p=0 regardless of the ion concentration in the electrolyte. Consequently the capture and emission rates are zero and the trapped charge is not controlled by the pH.

To overcome this difficulty, differently from past literature we model the Stern layer as a thin *semiconductor* film with a low N_C=N_V corresponding to a 1 fM solution. Consequently the Stern layer has a negligible free charge and essentially behaves as a dielectric but, at the same time, it is still possible to define traps at its interface with the actual gate dielectric. We found this workaround quite robust provided the Stern layer is not too thin. In fact, although n_S and p_S are very small inside the Stern layer, TCAD can still calculate the correct trap occupation function and σ_T because the Boltzmann factor depends on the ratio between the carrier concentrations and the corresponding equilibrium values (Eq. 7), which are *both* very small in the Stern layer.

E. Model Validation

In order to check the validity of our model and to demonstrate the importance of the Stern layer, we extracted the threshold voltage V_T versus pH_B curve for the structures reported at the center and right of Fig. 2, and compared the results with the experimental data in [30]. To this end, V_T is defined as the V_{FG} at which the minority carrier concentration at the silicon interface (n) is equal to the doping concentration in the substrate (N_A) for V_B=0 V. The structure and the surface reaction parameters used in the paper are reported in Tabs. I and II. In general terms the parameters are extracted by fitting the model to experimental V_T or surface potential versus pH

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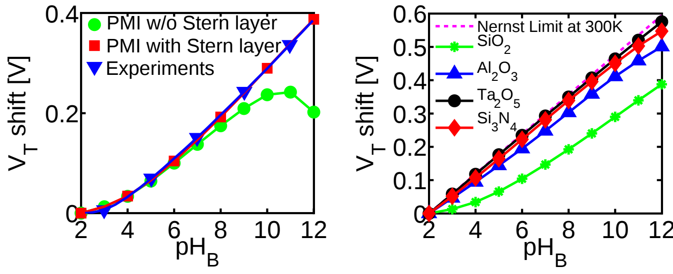


Fig. 4. Left: comparison between the TCAD simulations for the structure at the center of Fig. 2 with SiO_2 dielectric (○), the SDevice simulations of the structure on the right of Fig. 2 (square) and the experimental data of [30] (△). Right: V_T versus pH_B characteristics for different dielectric materials for the structure on the right of Fig. 2 at 1 mM salt concentration. V_B=0 V.

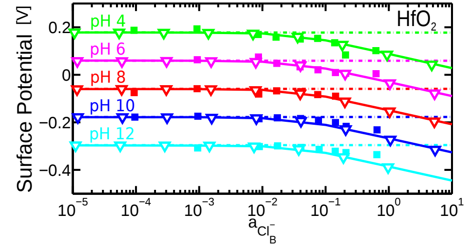


Fig. 5. Surface potential experimental data in [31] (squares) compared to the site-binding model (dash-dotted lines), the model of [31] (open triangles) and our TCAD implementation (solid lines). $a_{Cl_B^-}$ denotes the chlorine ion activity in the bulk of the solution. Following ref. [31], we compute the surface potential as $V_{T,PZC} - V_T$, where $V_{T,PZC}$ is the V_T for the pH of zero charge ($pH_{PZC} = -0.5 \ln K_a \cdot K_b$) at very low electrolyte concentration (10μM). K_a=K_b=10^{-7}, K_c=3.3$\cdot 10^{-6}$, N_{sil}=10^{15}cm^{-2}.

and ion concentration (see also Fig.5 in the following).

The results for an ISFET with SiO_2 dielectric are shown in Fig. 4 and illustrate the importance of the Stern layer in order to reproduce the experiments at high pH. This is because when the cations accumulate at the minimum distance from the dielectric/electrolyte interface a voltage drop develops across the Stern layer which explains the observed V_T increase. Without Stern layer, instead, at high pH the ions in the electrolyte screen the surface charge resulting in a weaker V_T increase and even a roll-off when pH becomes larger than 10.

The left plot in Fig. 4 reports the V_T shift versus pH for a few dielectrics of common use in microelectronics. The slope of these curves is the threshold voltage sensitivity S_{V_T}=dV_T/dpH_B. In agreement with the experiments in [50], [16], [30], [41], Si_3N_4, Ta_2O_5 and Al_2O_3 yield S_{V_T} values close to the theoretical 59 mV/pH Nernst limit (not shown), whereas the average sensitivity of SiO_2 is lower (≈40 mV/pH) especially for low pH_B values.

	Value	Units		Value	Units
t_{el}	10^{-6}	m	ϵ_{el}	80	1
t_{Stern}	1.1$\cdot 10^{-10}$	m	ϵ_{Stern}	2.5	1
t_{ox}	3$\cdot 10^{-9}$	m	ϵ_{ox}	3.9	1
T	300	K	N_A	10^{17}	cm^{-3}
c_0	10^{-3}	mol/l	ϵ_0	8.85$\cdot 10^{-14}$	F/cm

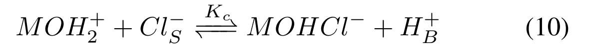
TABLE I
PARAMETER VALUES OF THE STRUCTURES IN FIG. 2.

Material	ϵ_{rel}	N_{sil}	K_a	K_b	N_n	K_n
		[cm^{-2}]			[cm^{-2}]	
SiO_2	3.9	5$\cdot 10^{14}$	10^{-6}	10^2	0	0
Al_2O_3	14	8$\cdot 10^{14}$	10^{-10}	10^{-6}	0	0
Ta_2O_5	22	10^{15}	10^{-4}	10^{-2}	0	0
Si_3N_4	7.5	3$\cdot 10^{14}$	10^{-6}	10^2	2$\cdot 10^{14}$	10^{-10}

TABLE II
VALUES OF THE SURFACE DISSOCIATION PARAMETERS USED IN SIMULATIONS. SiO_2 AND Al_2O_3 FROM [50], [30]; Ta_2O_5 FROM [30]; Si_3N_4 FROM [16].

F. High salt concentration effects

As pointed out in [31], the site-binding theory in the form previously discussed becomes inaccurate at high salt concentration. This discrepancy is clearly visible in Fig. 5 that compares the surface potential predicted by the conventional site-binding model to the experimental data from [31]. The discrepancy has been attributed to surface complexation reactions with the chlorine ions of the electrolyte salt (typically NaCl or KCl) of the form



$$MOH_2^+ + Cl_S^- \overset{K_c}{\rightleftharpoons} MOHCl^- + H_B^+ \qquad (10)$$

where M is the metal of the dielectric (e.g. Si, Ta, Al or Hf). Following [31], we should thus describe the dielectric/electrolyte interface of SiO_2, HfO_2, Al_2O_3 and Ta_2O_5 with three coupled chemical reactions. The additional dissociation constant is $K_c = \nu_{MOHCl^-} \cdot cH_B / (\nu_{MOH_2^+} \cdot cCl_S)$, where cCl_S=10^{-pCl_S} is the chlorine free-ions surface concentration and ν_{MOHCl^-} is the density of the negatively charged surface groups. The surface charge density is then given by

$$\sigma_0 = q \cdot \left(\nu_{MOH_2^+} - \nu_{MO^-} - \nu_{MOHCl^-} \right) \quad . \qquad (11)$$

Using the expression

$$N_{sil} = \nu_{MO^-} + \nu_{MOH} + \nu_{MOH_2^+} + \nu_{MOHCl^-} \quad , \qquad (12)$$

we derive:

$$\sigma_0 = qN_{sil} \left(\frac{cH_S^2 cH_B - K_a K_b cH_B - K_c cCl_S cH_S^2}{cH_S^2 cH_B + K_a K_b cH_B + K_c cCl_S cH_S^2 + K_b cH_S cH_B} \right) \quad . \qquad (13)$$

Eq. 13 is easy to implement in the TCAD via PMI considering two acceptor and one donor traps with suitable capture and emission rates as exemplified in Sect.II-C. The extra term, cCl_S, is (see Eq.7)

$$cCl_S = cCl_B \frac{n_S}{\sqrt{n_S p_S}} = cCl_B \exp\left(\psi_0 / V_{th}\right) \quad . \qquad (14)$$

Eq. 14 entails that the centroid of the bound chlorine ions charge (the so called inner Helmholtz plane) coincides with the dielectric/electrolyte interface where protonation/deprotonation reactions occur. This is a reasonable approximation that is justified by the good agreement with experiments shown in the following Section III.

The complete expression for σ_0 as a function of n_S and p_S is then given by Eq. 17 which extends Eq.8 to high chlorine concentrations. Note that for negligible cCl_B Eq. 17 yields back Eq.8, as it should be. The model parameters of this

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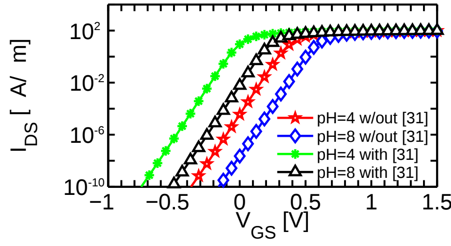

Fig. 6. I_{DS} versus V_{GS} characteristics of the ISFET in Fig.1 with and without the surface complexation reactions modeled as in [31]. Note the remarkable V_T shift associated to the chlorine concentration ($a_{Cl_B^-}$=c_0=100 mM) compared to the model without surface complexation. Al_2O_3 gate dielectric.

equation either are given in the caption of Fig. 5 (N_{sil}, K_a, K_b and K_c) or they should be computed according to the pH and chlorine concentration of the bulk solution (cH_B and cCl_B). Fig. 5 shows that the PMI implementation of Eq. 17 (solid lines) allows the TCAD to accurately reproduce the results of [31] (symbols and dashed lines) up to high salt concentration.

Fig.6 shows how surface complexation reactions shift the devices threshold voltage to much smaller values, essentially bacause the chemical reaction in Eq.10 with K_c=3.3·10^{-6} increases the density of positively charged MOH_2^+ groups at the interface.

The extension to surface complexation reactions illustrates the versatility of the proposed method, which lends itself to the inclusion of many, possibly coupled, surface reactions, provided equilibrium holds in the electrolyte so that it is legitimate to substitute the Boltzmann factor for all monovalent ions with suitable ratios between the surface and bulk free carrier concentrations as in Eqs.7 and 14.

III. Results

To demonstrate the versatility of the proposed method, we present a full two-dimensional analysis of the V_T and I_{DS} sensitivity to pH changes for the planar ISFET architecture shown in Fig. 1 in the linear and saturation regions of operation. In fact, biasing the ISFET in the triode region is often the preferred choice in readout circuits designed to detect the threshold voltage sensitivity S_{V_T}=$\Delta V_T/\Delta pH_B$ at constant I_{DS}. However, several read-out circuits operate the ISFET in the saturation region, for instance when the device is part of a differential pair [6], or part of an inverter [45]. Furthermore, integrated arrays typically feature a unique fluid gate electrode for numerous ISFETs exposed to many analyte samples in parallel [10], [11]: sensing the V_T shift of the single wires in parallel is then difficult; consequently, the sense amplifiers detect changes in the drain current at constant V_{GS} and demand a large current sensitivity $S_{I_{DS}}$=$\Delta I_{DS}/[I_{DS}\Delta pH_B]$.

The dimensions of the simulated ISFET are reported in Tab. III. The source/drain doping profile decays at approximately 5 nm/decade toward the channel region; if not otherwise stated the surface reaction model parameters are those in Tab. I. Compared to the results of the previous Section, the Stern layer thickness has been increased to 3 Å while keeping the same 20μF/cm^2 capacitance [30] to facilitate numerical convergence. We verified that the current-voltage curves and the threshold voltage shifts are not affected by this choice.

	Value	Units		Value	Units
t_{Stern}	3	Å	ϵ_{Stern}	6.82	ϵ_0
t_{ox}	3	nm	N_A	10^{17}	cm^{-3}
$N_{D,source}$	10^{19}	cm^{-3}	$N_{D,drain}$	10^{19}	cm^{-3}
L_{source}	200	nm	L_{drain}	200	nm
$L_{channel}$	200	nm	t_{junct}	40	nm

TABLE III
Simulation parameters for the ISFET of Fig. 1.

A. Threshold voltage sensitivity

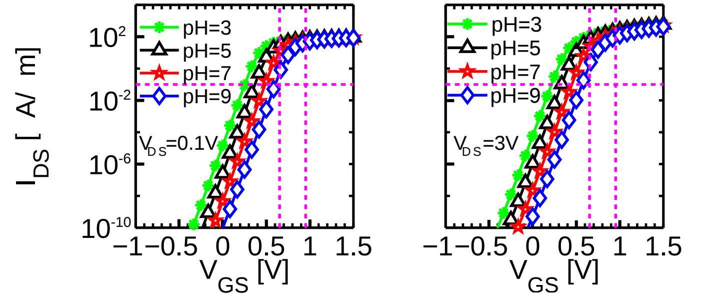

Fig. 7. Left: I_{DS}-V_{GS} curves of the device in Fig. 1 with parameters from Tabs.I and III, and considering a Si_3N_4 gate dielectric in the linear (left, V_{DS}=0.1 V) and saturation (right, V_{DS}=3 V) regions of operation. 1 mM salt concentration. The vertical and horizontal dashed lines mark the voltage and current levels used to extract the pH sensitivities.

Fig. 7 reports the I_{DS}-V_{GS} curves for the device with Si_3N_4 dielectric in the linear (left, V_{DS}=0.1 V) and saturation (right, V_{DS}=3 V) region. Due to a well-tempered device design and negligible short channel effects (subthreshold swing $SS \simeq$ 65.8 and 66.7 mV/dec at V_{DS} $\simeq$0.1 V and 3 V, respectively, DIBL $\simeq$ 13 mV/V), the curves shift rigidly for increasing pH both in the linear and saturation regimes, as we verified by checking explicitly that the g_m=$[\partial I_{DS}/\partial V_{GS}]$ versus V_{GS}-V_T characteristics overlap exactly.

Fig. 8 (top plot) shows the lateral potential profile at the dielectric/Stern layer interface, $\psi_0(y)$ and the surface potential at the channel/dielectric interface, $\psi_s(y)$. The surface potential decays with a short screening length $\lambda\simeq$ 14 nm due to the thin oxide and high channel doping. The lateral voltage drop remarkably modulates the negative site-binding charge (lower plot) which peaks at the source and drain side of the channel and in turn tends to equalize $\psi_0(y)$ and the potential at the

$$\sigma_0 = qN_{sil}\frac{cH_B^2 p_S - K_aK_bn_S - K_ccCl_B\sqrt{n_Sp_S}cH_B}{cH_B^2p_S + K_aK_bn_S + K_ccCl_B\sqrt{n_Sp_S}cH_B + K_b\sqrt{n_Sp_S}cH_B} \quad . \tag{17}$$

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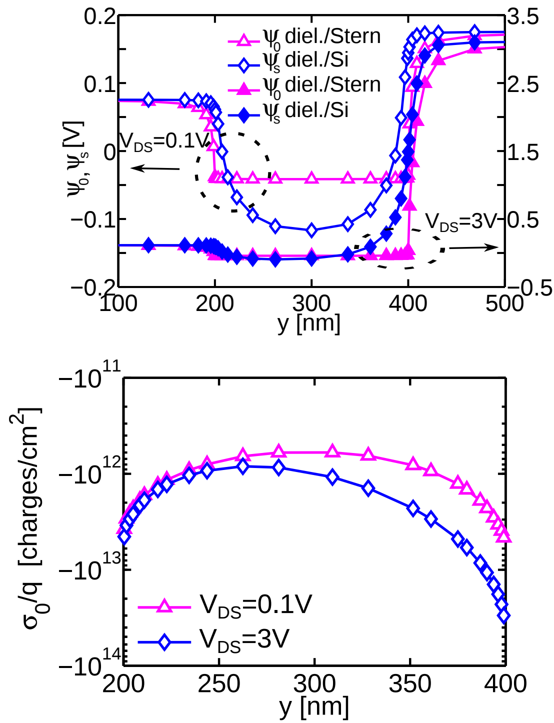

Fig. 8. Top: Potential profiles along the y direction at the oxyde/electrolyte (ψ_0) and at the silicon/oxide (ψ_s) interfaces for a few V$_{DS}$ at V$_{GS}$=V_T and pH=7. Bottom: corresponding surface charge density σ_0. c_0=1 mM. Si_3N_4 gate dielectric.

electrolyte/Stern layer interface (not shown). As a consequence of the almost constant $\psi_0(y)$ for both low and high V$_{DS}$ values, the change of the pH results in an amost rigid voltage shift as in Fig.7, regardless of the V$_{DS}$ value.

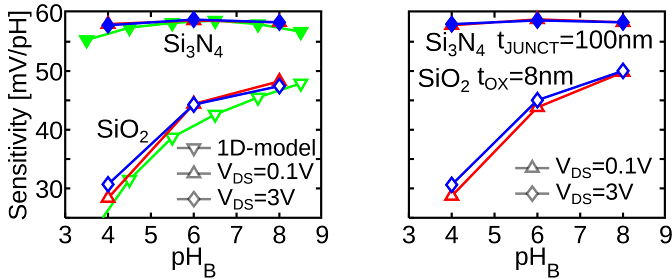

Fig. 9. Left: Differential V_T sensitivity versus pH for the ISFET with Si_3N_4 dielectric (filled symbols) and with SiO_2 dielectric (open symbols) in the linear (V_{DS}=0.1 V) and saturation region (V_{DS}=3 V). Calculations with the one-dimensional model [14], [15], [16], [17] (green) and with the TCAD. Right: S_{V_T} for the same devices as in the left plot, except that the junction depth is 100 nm for the Si_3N_4 device and the gate dielectric thickness is 8 nm for the SiO_2 device.

In fact, Fig.9 (left plot) shows the threshold voltage sensitivity S_{V_T}=$\Delta V_T/\Delta pH_B$ at constant I_{DS}=100 nA/μm for an ISFETs with Si_3N_4 gate dielectric. S_{V_T} values are almost insensitive to pH_B, and very close to the Nernst limit, as in the experiments of refs.[41], [30]. The S_{V_T} for a device with SiO_2 gate dielectric is much smaller than for Si_3N_4, especially at low pH_B, in agreement with [50]. The results demonstrate the ability of the proposed approach to describe different ISFET technologies. We also note that the 2D TCAD model agrees well with the 1D approximation in both the linear and the saturation region, the discrepancy being in the order of only 5%-10%. This is understood based on the discussion above, and further corroborated by the data in the right plot of Fig.9. As can be seen the threshold voltage sensitivity for devices not as well-tempered as the one in Fig.7 (because of deeper junctions, 100 nm, or thicker gate dielectric, 8 nm) is essentially the same than for the device in Fig.7.

The general purpose methodology developed here highlights that, despite the internal variables are non uniform and depend on V$_{DS}$, the resulting V$_T$ sensitivity is almost independent of V$_{DS}$ and equal to the predictions of the 1D model.

B. I_{DS} sensitivity

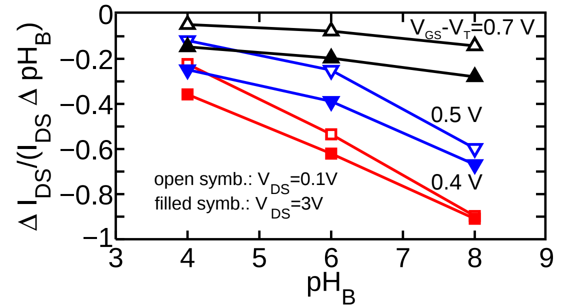

Fig. 10. Drain current sensitivity to pH changes $S_{I_{DS}}$ at constant V_{GS} values such that V$_{GS}$-V$_{T,pH=3}$ is the same at both V_{DS}=0.1 V and V_{DS}=3 V. Minimum and maximum V_{GS} are marked with vertical lines in Fig.7. Si_3N_4 gate dielectric.

As already mentioned, drain current sensitivity is also relevant for applications. To investigate this aspect, Fig. 10 plots the $S_{I_{DS}}$ versus pH_B value and for constant V_{GS}, corresponding to different V_{GS}-V_T depending on pH. The minimum and maximum V_{GS} are marked by dashed vertical lines in Fig.7. The gate voltage is chosen in such a way that V$_{GS}$-V$_{T,pH=3}$ is constant. At the highest V$_{GS}$-V$_{T,pH=3}$ the ISFET operates in strong inversion for all pH values. We see that the absolute value of the drain current sensitivity at constant V_{GS} increases at larger pH, and it varies with the bias point, being larger in the saturation region than in the triode region, and at small gate overdrive. In fact, $S_{I_{DS}} = S_{V_T} g_m/I_{DS}$ and g_m/I_{DS} increases for V$_{GS}$ values approaching V$_T$. At high pH, the V$_T$ is larger than for pH=3, so that for the same V$_{GS}$ we work closer to the threshold with larger g_m/I_D. This explains the large current sensitivity at large pH in Fig. 10.

Working in saturation thus provides clear advantages compared to the linear region only at moderate V$_{GS}$-V$_T$, but no advantages in voltage sensitivity.

IV. Conclusions

We proposed a general methodology to describe the surface charge density generated by reactions at the dielectric/electrolyte interface of ISFETs by means of commercial TCAD. By mapping the total anion and cation concentrations

DOI: 10.1109/TED.2015.2464251, © 2015 IEEE

(including H^+ and OH^- groups) into the hole and electron concentrations, we can then express the Boltzmann factor as the ratio between surface and bulk concentrations. The surface potential dependent charge is replaced by surface traps with modified concentration dependent capture and emission rates, and then solved self-consistently by the TCAD.

The method is versatile and easily applicable; many independent or coupled chemical reactions can be described provided a closed form expression can be found for σ_0 in terms of surface and bulk ion concentrations. The method enables full two- and three-dimensional analysis of planar, fin or nanowire ISFET device architectures in a TCAD environment. A critical re-examination of the bias dependent threshold voltage and drain current sensitivity of planar ISFETs in two dimensions has been carried out. The results highlight that a rigid shift of the $I_{DS}-V_{GS}$ characteristics versus pH has to be expected regardless of the operating region and, consequently, the g_m/I_{DS} parameter rules the relation between V_T and I_{DS} sensitivities regardless of the bias point.

The model represents a significant step forward in the accurate modeling of ISFETs by means of commercial TCAD and paves the way toward the practical use of these tools in the design and optimization of integrated ISFET devices.

ACKNOWLEDGMENTS

The authors would like to thank Paolo Scarbolo for many helpful discussions.

REFERENCES

[1] M. A. Reed and N. Haven, "CMOS Biosensor Devices and Applications," in *IEEE IEDM Technical Digest*, 2013, pp. 208–211.

[2] A. Matsumoto and Y. Miyahara, "Current and Emerging Challenges of Field Effect Transistor Based Bio-sensing," *Nanoscale*, vol. 5, pp. 10 702–10 718, 2013.

[3] P. Bergveld, "Development of an Ion-Sensitive Solid-State Device for Neurophysiological Measurements," *IEEE Trans. on Bio-medical Engineering*, no. 1, pp. 70–71, 1970.

[4] ——, "Thirty years of ISFETOLOGY What happened in the past 30 years and what may happen in the next 30 years," *Sensors and Actuators B: Chemical*, vol. 88, no. 1, pp. 1–20, 2003.

[5] ——, "ISFET, Theory and Practice," in *Proceedings IEEE Sensor Conference*, 2003, pp. 1–26.

[6] Y.-L. Chin, J.-C. Chou, T.-P. Sun, W.-Y. Chung, and S.-K. Hsiung, "A Novel pH Sensitive ISFET with on Chip Temperature Sensing Using CMOS Standard Process," *Sensors and Actuators B: Chemical*, vol. 76, no. 1-3, pp. 582–593, June 2001.

[7] C. Stagni, C. Guiducci, L. Benini, B. Riccò, S. Carrara, B. Samorí, C. Paulus, M. Schienle, M. Augustyniak, and R. Thewes, "CMOS DNA Sensor Array With Integrated A / D Conversion Based on Label-Free Capacitance Measurement," *IEEE Journal of Solid State Circuits*, vol. 41, no. 12, pp. 2956–2964, 2006.

[8] C. Jakobson, U. Dinnar, M. Feinsod, and Y. Nemirovsky, "Ion-Sensitive Field Effect Transistors in Standard CMOS Fabricated by Post-Processing," *IEEE Sensors Jou.*, vol. 2, pp. 279–286, 2002.

[9] C. Jimenez-Jorquera, J. Orozco, and A. Baldi, "ISFET based microsensors for environmental monitoring." *Sensors*, vol. 10, no. 1, pp. 61–83, Jan. 2010.

[10] J.M. Rothberg *et al.*, "An integrated semiconductor device enabling non-optical genome sequencing." *Nature*, vol. 475, no. 7356, pp. 348–52, July 2011.

[11] C. Toumazou and *et al.*, "Simultaneous DNA amplification and detection using a pH-sensing semiconductor system," *Nature Methods*, vol. 10, pp. 641–646, 2013.

[12] J. Bustillo, K. Fife, B. Merriman, and J. Rothberg, "Development of the Ion Torrent CMOS Chip for DNA Sequencing ," in *IEEE IEDM Technical Digest*, 2013, pp. 196–199.

[13] P. Dak, P. Nair, J. Go, and M. Alam, "Extended-gate biosensors achieve fluid stability with no loss in charge sensitivity," in *Proceedings Device Research Conference*, vol. 20, 2013, pp. 105–106.

[14] W. Siu and R. Cobbold, "Basic Properties of the EIectrolyte-SiO_2-Si System: Physical and Theoretical Aspects," *IEEE Trans. on Electron Devices*, no. 1, pp. 1805–1815, 1979.

[15] C. Fung, P. Cheung, and W. Ko, "A Generalized Theory of an Electrolyte-Insulator-Semiconductor Field-Effect Transistor," *IEEE Trans. on Electron Devices*, no. 1, 1986.

[16] M. Grattarola, G. Massobrio, and S. Martinoia, "Modeling H^+-Sensitive FET's with SPICE," *IEEE Trans. on Electron Devices*, vol. 39, no. 4, pp. 1–6, 1992.

[17] A. Matsumoto and Y. Miyahara, "Analytical Modeling of Biotransistors," *IET Circuits, Devices and Systems*, vol. 2, pp. 158–165, 2008.

[18] Y.Wang and G.Li, "Performance Investigation for a Silicon Nanowire FET Biosensor Using Numerical Simulation," in *Proc. IEEE Nanotechnology Materials and Devices Conference*, 2010, pp. 81–86.

[19] W. R. Frensley, "Performance Analysis of Si Nanowire Biosensor by Numerical Modeling for Charge Sensing," *IEEE Transactions on Nanotechnology*, vol. 11, no. 3, pp. 501–512, May 2012.

[20] S. Baumgartner, C. Heitzinger, A. Vacic, and M. A. Reed, "Predictive simulations and optimization of nanowire field-effect PSA sensors including screening," *Nanotechnology*, vol. 24, no. 22, p. 225503, 2013. [Online]. Available: http://stacks.iop.org/0957-4484/24/i=22/a=225503

[21] F. Pittino and L. Selmi, "Use and comparative assessment of the cvfem method for poissonboltzmann and poissonnernstplanck three dimensional simulations of impedimetric nano-biosensors operated in the dc and ac small signal regimes," *Computational Methods in Applied Mechanics and Engineering*, pp. 902–923, 2014.

[22] K. B. Parizi, A. J. Yeh, A. S. Y. Poon, and H.-S. P. Wong, "Exceeding Nernst Limit (59 mV/pH): CMOS-Based pH Sensor for Autonomous Applications," in *IEEE IEDM Technical Digest*, 2012, pp. 557–560.

[23] COMSOL, "Comsol Multiphysics Ref. Manual," Tech. Rep., 2013.

[24] M. Webster, I. Timoshkin, S.J.MacGregor, and M. Mattey, "Computer Aided Modeling of an Interdigitated Microelectrode Array Impedance Biosensor for the Detection of Bacteria," *IEEE Trans. on Dielectrics and Electrical Insulation*, vol. 16, pp. 1356–1363, 2009.

[25] Integrated Engineering Software, "ELECTRO/COULOMB Ref. Manual," Tech. Rep., 2013.

[26] Silvaco, "ATLAS user's manual," Tech. Rep., 2013.

[27] TMA, "MEDICI user's manual," Tech. Rep., 2013.

[28] Synopsys, *Sentaurus Device User Guide*, 2013.

[29] D. Yates, S. Levine, and T. Healy, "Site-binding model of the electrical double layer at the oxide/water interface," *Journal of Chemical Society, Faraday Transactions*, vol. 70, pp. 1807–1818, 1974.

[30] R. van Hal, J. Eijkel, and P. Bergveld, "A general model to describe the electrostatic potential at electrolyte oxide interfaces," *Advances in Colloid and Interface Science*, vol. 69, no. 1-3, pp. 31–62, Dec. 1996.

[31] A. Tarasov, M. Wipf, R. Stoop, and K. Bedner, "Understanding the electrolyte background for biochemical sensing with ion-sensitive field-effect transistors," *ACS Nano*, no. 10, pp. 9291–9298, 2012.

[32] I.-Y. Chung, H. Jang, J. Lee, H. Moon, S. M. Seo, and D. H. Kim, "Simulation Study on Discrete Charge Effects of SiNW Biosensors According to Bound Target Position Using a 3D TCAD Simulator," *Nanotechnology*, vol. 23, no. 6, p. 065202, 2012.

[33] D. Welch, S. Shah, S. Ozev, and J. B. Christen, "Experimental and Simulated Cycling of ISFET Electric Fields for Drift Reset," *IEEE Electron Device Lett.*, vol. 34, pp. 456–458, 2013.

[34] P. Palestri, R. Sette, F. Pittino, F. Saccon, D. Esseni, and L. Selmi, "Simulation of nano-biosensors based on conventional TCAD," in *Proceedings 14th International Conference on Ultimate Integration on Silicon (ULIS)*, Mar. 2013, pp. 77–80.

[35] F. Pittino, P. Palestri, P. Scarbolo, D. Esseni, and L. Selmi, "Models for the use of commercial TCAD in the analysis of silicon-based integrated biosensors," *Solid-State Electronics*, vol. 98, pp. 63–69, 2014.

[36] D. Passeri, A. Morozzi, K. Kanxheriand, and A. Scorzoni, "Numerical Simulation of ISFET Structures for BioSensing Devices with TCAD Tools," in *Proceedings IWBBIO*, 2014, pp. 425–435.

[37] F. Spiga, "Private Communication," Tech. Rep., 2014.

[38] J. Davis, R. James, and J. Leckie, "Surface ionization and complexation at the oxide/water interface. I. Computation of Electrical Double Layer Properties in Simple Electrolytes," *Jou. of Colloid and Interface Science*, vol. 63, no. 3, pp. 480–499, Mar. 1978.

[39] J. Drzymala, J. Lekki, and J. Laskowski, "Surface dissociation constants for solid oxide/aqueous solution systems," *Colloid and Polymer Science*, vol. 772, pp. 768–772, 1979.

DOI: 10.1109/TED.2015.2464251, © 2015 IEEE

[40] L.J.Bousse and N. De Rooij and P. Bergveld, "The influence of counter-ion adsorption on the ψ_0/pH characteristics of insulator surfaces," *Surface Science*, vol. 135, pp. 479–496, 1983.

[41] D. Harame and L. Bousse, "Ion-sensing devices with silicon nitride and borosilicate glass insulators," *IEEE Trans. on Electron Devices*, no. 8, pp. 1700–1707, 1987.

[42] H. Abe, M. Esashi, and T. Matsuo, "ISFET's using inorganic gate thin films," *IEEE Trans. on Electron Devices*, vol. 26, pp. 1939–1944, 1979.

[43] P. Bergveld and A. Sibbald, *Analytical and biomedical applications of ion-selective field effect transistors*, Elsevier, Ed. Elsevier, Amsterdam, 1988, vol. 23.

[44] B. Jr., B. Dorvel, J.Go, P. Nair, O. Elibol, G. Credo, J. Daniels, E. Chow, X.Su, M.Varma, M. Alam, and R.Bashir, "High-k dielectric Al_2O_3 nanowire and nanoplate field effect sensors for improved pH sensing," *Biomed Microdevices*, vol. 13, pp. 335–344, 2011.

[45] J. Lee, S. Hwang, B. Choi, J. H. Lee, D. Moon, M. Seol, C. Kim, I. Chung, B. Park, Y. Choi, D. M. Kim, D. H. Kim, and S. Choi, "A Novel SiNW/CMOS Hybrid Biosensor for High Sensitivity/Low Noise," in *IEEE IEDM Technical Digest*, 2013, pp. 385–388.

[46] K. Bedner, V. A. Guzenko, A. Tarasov, M. Wipf, R. L. Stoop, D. Just, S. Rigante, W. Fu, R. A.Minamisawa, C. David, and *et al.*, "pH Response of Silicon Nanowire Sensors: Impact of Nanowire Width and Gate Oxide," *Sensors and Materials*, vol. 25, no. 8, pp. 567–576, 2010.

[47] M. S. Kilic, M. Z. Bazant, and A. Ajdari, "Steric effects in the dynamics of electrolytes at large applied voltages. ii. modified Poisson-Nernst-Planck equations," *Phys. Rev. E*, vol. 75, p. 021503, Feb 2007.

[48] O. Stern, "Zur Theorie der elektrolytischen Doppelschicht," *Z. Elektrochem.*, vol. 30, pp. 508–516, 1924.

[49] Y. Marcus, "Ionic radii in aqueous solutions," *Chemical Reviews*, vol. 88, p. 147S, 1988.

[50] A. V. den Berg and P. Bergveld, "Sensitivity Control of ISFETs by Chemical Surface Modification," *Sensors and Actuators B: Chemical*, vol. 8, pp. 129–148, 1985.

DOI: 10.1109/TED.2015.2464251, © 2015 IEEE