

DEVELOPMENT OF A NEW ROBUST
HYBRID AUTOMATA ALGORITHM BASED
ON SURFACE ELECTROMYOGRAPHY
(SEMG) SIGNAL FOR INSTRUMENTED
WHEELCHAIR CONTROL.

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Doctor of Philosophy

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SUPERVISOR'S DECLARATION

I* hereby declare that I have checked this thesis and in my opinion, this thesis is adequate in terms of scope and quality for the award of the degree of Doctor of Philosophy in Mechanical Engineering



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I hereby declare that the work in this thesis is based on my original work except for quotations and citations which have been duly acknowledged. I also declare that it has not been previously or concurrently submitted for any other degree at Universiti Malaysia Pahang or any other institutions.

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Thesis submitted in fulfillment of the requirements
for the award of the degree of
Doctor of Philosophy

Faculty of Mechanical Engineering
UNIVERSITI MALAYSIA PAHANG

DECEMBER 2020

ACKNOWLEDGEMENTS

First and foremost, I would like to thank to my research supervisor, Assoc. Prof. Dr. Saiful Anwar Che Ghani. Without his assistance and dedication that involved in every steps throughout the process, this study would have never been accomplished. I would like to express my sincere appreciation for the support.

I would also like to show my deepest gratitude to the Universiti Malaysia Pahang for the facilities that they have provided and for the good services from their administrative staffs.

Getting through my dissertation required more than my academic support, and I would like to thank all of the people who were listening to me and at times, having to tolerate me over the past years. A special thanks to my family, my parents, my mother-in-law, my brothers, sister and all my big family. Words cannot express how grateful I am for all the sacrifices that you've made on my behalf. All of your prayers that had made me sustained everything so far.

At the end I would like to express my deepest appreciation to my beloved wife who always support me in the moments when there was no one to answer my queries and also my sons; whom were always understand and give me the inspirations.

ABSTRAK

Kerusi roda beralat yang beroperasi berdasarkan elektromiografi di permukaan (sEMG) merupakan salah satu alternatif membantu golongan kurang upaya untuk bergerak. SEMG menjadi pilihan kerana ketepatan yang baik dan persediaan untuk meletakkan elektrod yang lebih mudah. Sel saraf menghantar isyarat yang mengandungi potensi elektrik ke otot untuk mengarahkan agar mengecut secara isometrik, sepusat dan eksentrik. Perubahan potensi elektrik ini disebut sebagai Potensi Tindakan Unit Saraf (MUAP) yang dapat diperoleh elektrod yang terletak diatas otot, diperkuat, dirakam dan dianalisa oleh peranti sEMG. Penyelidikan ini bertujuan untuk mengembangkan kebolehan peranti pemerolehan data sEMG yang berasaskan Arduino yang merupakan sumber terbuka dengan algoritma automata hibrid bagi membezakan aktiviti MUAP semasa mengayuh kerusi roda. Penambahan algoritma automata hibrid untuk menjalankan kaedah kawalan berdasarkan pengecaman corak dan bukan corak merupakan kelebihan bagi meningkatkan ketepatan membezakan aktiviti kayuhan ke hadapan atau gerakan mengemablikan tangan. Elektrod diletakkan pada otot Biceps (BIC), Triceps (TRI), Extensor (EXT), Flexor (FIX) dan aktiviti MUAP direkodkan bagi 30 peserta yang sihat tubuh badan. Kemudian, hasil eksperimen disahkan dengan hasil simulasi menggunakan perisian pemodelan bioperubatan OpenSim. Purata, standard deviation (SD) confidence interval (CI) dan titik maksimum berbeza (MPD) MUAP akan dikira dan digunakan sebagai penentu untuk kaedah kawalan pengecaman bukan corak untuk eksperimen pemilihan kaedah kawalan. Sementara itu, pengecaman corak menggunakan Fungsi Ketumpatan Kebarangkalian (PDF) untuk menentukan MUAP mengikut jenis aktiviti. Kaedah ambang ganda dan saluran melintang yang dilaksanakan untuk mengurangkan peralihan elektrod yang akan mempengaruhi kualiti isyarat sEMG dan meningkatkan ketepatan klasifikasi. Sebanyak sepuluh kaedah kawalan yang ditentukan daripada data populasi dan individu diuji terhadap 10 orang yang sihat untuk menilai prestasi algoritma. Penilaian setiap kaedah kawalan yang dilakukan oleh matrik salah klasifikasi melihat Positif Benar (TP) dan Negatif Salah (FN) untuk mengaktifkan sistem bantuan kuasa. Peranti pemerolehan data sEMG yang dibangunkan dikendalikan oleh Arduino MEGA 2560 dan sensor otot Myoware dengan kadar pengambilan sampel melebihi 400Hz untuk merekodkan MUAP dari otot lengan. Selanjutnya, 2.5ms kelewatan purata untuk peranti merakam, menganalisis, mengesahkan dan membuat arahan untuk mengaktifkan sistem bantuan kuasa. Data yang diperoleh dari peranti menunjukkan bahawa otot yang paling aktif semasa mengayuh kerusi roda adalah TRI, diikuti oleh BIC dan keputusan ini sepadan dengan hasil simulasi OpenSim. Dalam eksperimen pemilihan kaedah kawalan, 96.28% ketepatan purata dicapai dan kaedah kawalan yang berbeza dipilih oleh matriks salah klasifikasi untuk setiap orang. Kaedah yang terpilih ini akan menjadi kaedah kawalan untuk mengaktifkan sistem bantuan kuasa dan berdasarkan syarat yang ditetapkan dalam algoritma. Penemuan ini menunjukkan bahawa Arduino mampu menjalankan secara langsung kaedah kawalan berasaskan pengecaman corak dan tanpa corak dengan menghasilkan ketepatan klasifikasi hingga 99.48% walaupun ia hanya dikenali sebagai pengawal mikro yang mempunyai batasan untuk menjalankan pengklasifikasi yang kompleks. Pada masa yang sama, peranti yang berharga kurang dari USD200 memiliki 400 sampel kadar pensampelan per saat adalah sama baiknya dengan peranti sumber tertutup yang mahal harganya. Berdasarkan keputusan penilaian algoritma yang menunjukkan bahawa satu kaedah kawalan tidak sesuai untuk semua peserta seperti yang terbukti dalam eksperimen pemilihan kaedah kawalan. Individu yang berbeza mempunyai kaedah kawalan yang berbeza yang sesuai dengan mereka. Terakhir, BIC dan TRI boleh dijadikan otot rujukan untuk mengaktifkan alat bantuan di kerusi roda beralat yang menggunakan kayuhan untuk mengaktifkannya.

ABSTRACT

Instrumented wheelchair operates based on surface electromyography (sEMG) is one of alternative to assist impairment person for mobility. SEMG is chosen due to good in accuracy and easier preparation to place the electrodes. Motor neuron transmit electrical potential to muscle fibre to perform isometric, concentric or eccentric contraction. These electrical changes that is called Motor Unit Action Potential (MUAP) can be acquired and amplified by electrodes located on targeted muscles changes can be recorded and analysed using sEMG devices. But, sEMG device cost up to USD 2,100 for a sEMG data acquisition device that available on market is one of the drawback to be used by impairment person that most of them has financial problem due to unable to work like before. In addition, it is a closed source system that cannot be modified to improve the accuracy and adding more features. Open source system such as Arduino has limitation of specifications that makes able to apply non-pattern recognition control methods which is simpler and easier compared to pattern recognition. However, classification accuracy is lower than pattern recognition and it cannot be applied to higher number participants from different background and gender. This research aims are to develop an open-source Arduino based sEMG data acquisition device by formulating hybrid automata algorithm to differentiate MUAP activity during wheelchair propulsion. Addition of hybrid automata algorithm to run pattern and non-pattern recognition based control methods is an advantage to increase accuracy in differentiating forward stroke or hand return activity. Electrodes are placed on Biceps (BIC), Triceps (TRI), Extensor (EXT), Flexor (FIX) and MUAP activity recorded for 30 healthy persons. Then, experiment result was validated with simulation result using OpenSim biomedical modelling software. Mean, standard deviation (SD), confidence interval (CI) and maximum point different (MPD) of MUAP were calculated and to be used as thresholds for non-pattern recognition control method in method selection experiment. Meanwhile, pattern recognition is using Probability Density Function (PDF) to determine MUAP according to type of activities. Total of ten control methods determined from population and individual data were tested against another 10 healthy persons to evaluate the algorithm performance. Assessment of each control method done by misclassification matrix looking at True Positive (TP) and False Negative (FN) of power assist system activation period. Developed sEMG data acquisition device that is operated by Arduino MEGA 2560 and Myoware muscle sensors with sampling rate of above 400Hz successfully recorded MUAP from four arm muscles. Furthermore, 2.5 ms of average data latency for device to record, analyse, validate and creating commands to activate the power assist system. Data obtained from the device shows that most active muscle during wheelchair propulsion is TRI, followed by BIC and matched to OpenSim simulation result. In method selection experiment, 96.28% of average accuracy was achieved and different control methods were selected by misclassification matrix for each of persons. This method would be a control method to activate power assist system and selected based on conditions set in the algorithm. These findings indicated that open source Arduino board is capable of running real time pattern, non-pattern recognition based control methods by producing classification accuracy up to 99.48% even though it is known as just a microcontroller that has limitation to run complex classifiers. At the same time, a device that cost less than USD200 has 400Hz of sampling rate is as good as closed source device that is come with expensive price tag to own it. Based on algorithm evaluation, it shows that one control method couldn't fit to all persons as per proven in method selection experiment. Different person has different control method that suit them the most. Lastly, BIC and TRI can be reference muscles to activate assistive device in instrumented wheelchair that is using propulsion as indication.

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LIST OF SYMBOLS

N	Total number of phases
\bar{x}	Mean
σ	Standard deviation
e	Euler's number 2.71828
π	Pi = 3.14159
μ	Mean for PDF calculation
X	MUAP reading

LIST OF ABBREVIATIONS

SBPWM	Simple Boost Pulse Width Modulation
ZSI	Z source inverter
MUAP	Motor unit action potential
BIC	Biceps
TRI	Triceps
EXT	Extensor
FIX	Flexor
SD	Standard Deviation
MPD	Maximum point different
TP	True Positive
FN	False Negative
TN	False Positive
IoT	True Negative
AR	Augmented reality
EEG	Electroencephalography
ECG	Electrocardiography
EMG	Electromyography
EOG	Electrooculography
CWA	Collaborative wheelchair assistant
SENIAM	Surface EMG for non-invasive assessment of muscles
DP	Door Passage Mode
GOA	General Obstacle Avoidance Mode
NNA	No Navigation Assistance
IW	Intelligent Wheelchair
FSPAC	Force sensor less power assist control
LZM	Left zygomaticus muscles
NI	National instrument
EEPROM	Electrically Erasable Programmable Read-Only Memory
SRAM	Static random access memory
I/O	Input/Output
PWM	Pulse Width Modulation

DC	Direct current
UE	Upper extremity
Pt	Platinum
Cr	Chromium
Ni	Nickel
AG	Silver
Ag/AgCl	Silver/silver chloride
TAC	Target Achievement Control
HD-Semg	High Density surface EMG
DT	Decision Trees
kNN	k-th Nearest Neighbor
MLP	Multi-layer Perceptrons
LDA	Linear Discriminant Analysis
SVM	Support Vector Machines
PDF	Probability Density Function
t	Processing time
d	Decision
MAV	Mean absolute value
RMS	Root mean square
WL	Wavelength length
VAR	Variance
ZC	Zero crossing (ZC)
BoB	Biomechnaics of Bodies
DOF	Degree of freedom
ADC	Analog-to-digital converter
Arduino IDE	Arduino integrated development environment
N	Number of cycle
CP	Contact phase
RP	Recovery phases
P _{CONTACT}	Probability of contact phase
P _{RECOVERY}	Probability of recovery phase
W	Weight/Load
F _f	Friction force

*susun ikut
alphabetical
order.*

AD	Average Deviation
s	Second
ms	Millisecond
μV	Microvolt
mV	Millivolt
V	Voltage
RM	Ringgit Malaysia
USD	US dollar

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