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## 3D-printed system optimizing dissolution of hyperpolarized gaseous species for micro-sized NMR†

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Dissolution of hyperpolarized species in liquids of interest for NMR is often hampered by the presence of bubbles that degrade the field homogeneity. Here a device composed of a bubble pump and a miniaturized NMR cell both fitted inside the narrow bore of an NMR magnet is built by 3D printing. <sup>129</sup>Xe NMR experiments performed with hyperpolarized xenon reveal high and homogeneous dissolution of the gas in water.

### Introduction

Today, nuclear magnetic resonance (NMR) is one of the most important modalities for molecular analysis and diagnosis. However, this technique intrinsically provides poor detection sensitivity, and recent years have seen the emergence of spin-hyperpolarization techniques designed to transiently boost nuclear magnetization, such as optical pumping of noble gases<sup>1</sup> and *para*-hydrogen-induced polarization.<sup>2</sup> The vast majority of NMR experiments involving gaseous hyperpolarized species include a dissolution step that most of the time is either manual (vigorous shaking<sup>3</sup>) or based on direct bubbling created by a peristaltic pump.<sup>4</sup> While the first method possesses some advantages such as simplicity or for instance the choice of magnetic field during mixing for *para*-hydrogen-induced polarization,<sup>5</sup> it sometimes lacks reproducibility and requires the use of fast NMR sequences to obtain maximal profit of the transient character of magnetization.<sup>6</sup> The bubbling method requires a waiting delay before the start of acquisition to avoid distortion of the magnetic field experienced by the nuclei of the solution linked to the strong susceptibility effects caused by the bubbles. In 2006, the use of hollow fibers<sup>7</sup> was shown to be a fast and robust method to efficiently dissolve hydrophobic gases such as xenon without bubbling, by increasing the exchange surface between the gas and the solution. The derived systems were powerful,<sup>8</sup> but the gas exchangers were necessarily placed inside large bore

apparatus or outside the NMR magnet. As far as a narrow bore magnet is concerned for a better spectral resolution, a compromise has to be found to place the reservoir containing the short-lived species (*para*-hydrogen, hyperpolarized noble gas) outside the magnet bore while minimizing the distance to the detection region. A mixing chamber outside the magnet implies a big volume of solution and causes a polarization loss, due to the fact that the magnetic field is much lower and also that the xenon relaxation rate is higher when the gas is dissolved.

We describe here a system using a microfluidic device for continuous- or stopped-flow delivery of gas, enabling its dissolution into a small volume as close as possible to the detection region for optimized magnetic resonance spectroscopy and imaging. We have developed a compact system that can be integrated into a conventional narrow-bore magnet in order to work with the high and homogeneous magnetic fields required for spectral resolution but also to reduce the sample volume. One of the technical challenges was to produce a complete system that integrates the gas exchange module, the pump and the NMR detection part in a small cylinder of 1.8 cm diameter and 4.3 cm height (upper part), without altering the magnetic field. Currently, integrated small devices are fabricated by conventional cleanroom techniques involving specialized resources and skills. Their development is usually cost and time expensive, which limits their design to a specific diagnostic application and hampers their diffusion to the market. Here we show that direct fabrication of 3D structures as milli/microfluidic systems by additive technologies such as 3D printing presents advantages such as fast and costless development with high achievable resolution on various materials, allowing rapid prototyping for a specific application. Moreover, we can then use our system as a disposable system to avoid contamination between experiments.

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† Electronic supplementary information (ESI) available: Movie of the bubble pump operation, <sup>129</sup>Xe magnetic resonance images recorded during its operation, and details of the time evolution of <sup>129</sup>Xe signals. See DOI: 10.1039/c5lc00193e

## Results

### Driven-flow device

A scheme of the whole device is given in Fig. 1. The plateau of a non-magnetic and programmable syringe pump (1) is fixed on top of an NMR magnet in a magnetic field of 100 G. Its console (2) is connected to the spectrometer console *via* a TTL port. At the beginning of the experiment, the syringe is filled with a buffer gas, such as nitrogen. Hyperpolarized xenon or other short-lived species, produced in batch mode, is contained in a Pyrex reservoir or glass coil (3). This reservoir is also fixed on top of the magnet; it is connected *via* silicon tubes to the syringe and to the fluidic part toward the solution placed inside the magnet, in the NMR detection region (4) (see next paragraph). After installation of the reservoir containing the hyperpolarized gas, primary vacuum is made.

The program entered on the syringe pump console enables one to choose not only the infuse flow rate and duration, but also the waiting delays as well as the NMR spectrometer acquisition sequencing.

### Fluidic system and NMR chamber

Fig. 2 depicts the NMR cell used for this study. The cell was designed in four pieces to be easily assembled after prototyping. The upper part (caps with inlet and outlet channels, fluidic system and micro-coil) contains the fluidic system: gas exchanger, pump and circulation. The lower part is dedicated to connections between the micro-imaging probe and the rf antenna. It was intended to be easily removed when the solution of interest has to be changed or when cleaning the fluidic part. A 3D printer was used to build the NMR cell, which has the form of an insert that can be plugged into the probe head, like any commercial rf insert. The whole NMR cell fits into the gradient sleeve. In this way, the gradient system of the micro-imaging probe can be used without any modification. NMR detection is performed *via* a

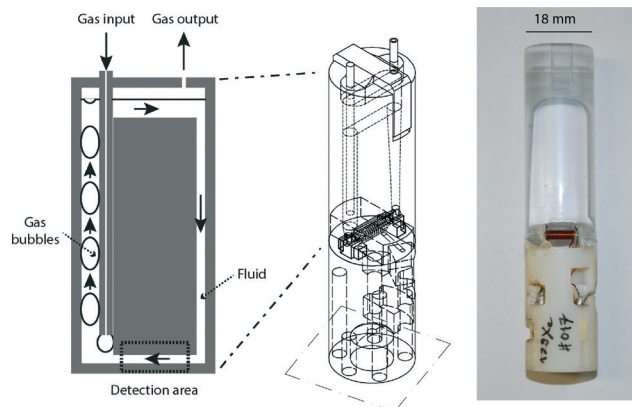


Fig. 2 The NMR cell. The principle of the bubble pump (in its top part) is depicted on the left. Middle: 3D drawing of the whole cell; right: picture of one of the cells equipped with a  $^{129}\text{Xe}$  solenoid coil.

horizontal solenoid; the electric circuit comprises pre-tuning and matching non-magnetic capacitors and is connected to the probe head. This enables easy tuning of the circuit in the common way using the rods of the probe. The gas output is made *via* a silicon tube exiting on top of the magnet while the solution flows into its chamber for a total volume of 500  $\mu\text{L}$  and for a detection volume of 5  $\mu\text{L}$ .

To overcome the drawbacks of an external pump, integration of a pumping element inside our NMR cell was investigated. Most microfluidic systems need a self-contained active micropump. Micropumps can be classified into two categories: mechanical (electrostatic, piezoelectric, thermo-pneumatic, electromagnetic actuations, *etc.*) and non-mechanical (magneto- and electro-hydrodynamic, electroosmotic, electro-wetting, electrochemical and bubble-type) pumping. Bubble-type micropumps appear as good candidates for our system. The pumping effect is based on the periodic expansion and collapse of bubbles generated in the region of higher diameter. The bubble outlet direction induces the flow direction of the solution.<sup>9</sup> Nevertheless in the literature this strategy uses a heating process to create bubbles, which is incompatible with our application. By combining the working principle of a bubble-type pump and the need for dissolution of our hyperpolarized gas, we created a non-heating bubble-type micropump by introducing the gas into the solution *via* a narrow tube (Fig. 2) positioned at one side of the chamber. This flow of xenon bubbles creates a flow of liquid in our NMR cell (see movie in the ESI<sup>†</sup>) and gas dissolution due to the large exchange area between the liquid and the gas.

### On-flow $^{129}\text{Xe}$ NMR experiments

In order to test the performance of the integrated NMR cell (the fluidic and the detection parts),  $^{129}\text{Xe}$  NMR experiments with laser-polarized gas were performed. Besides its NMR sensitivity, hyperpolarized xenon-129 has the advantage of exhibiting a very large chemical shift bandwidth (more than 300 ppm for monoatomic species) and of being reversibly

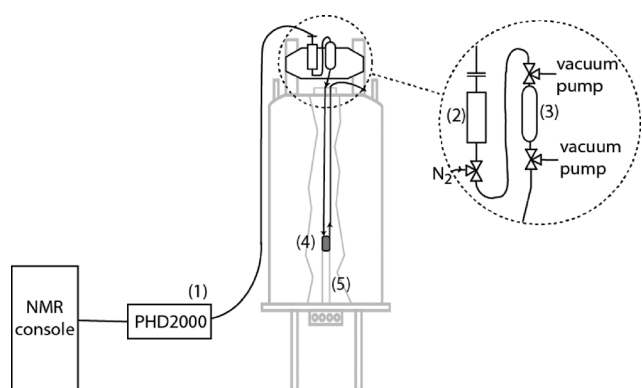
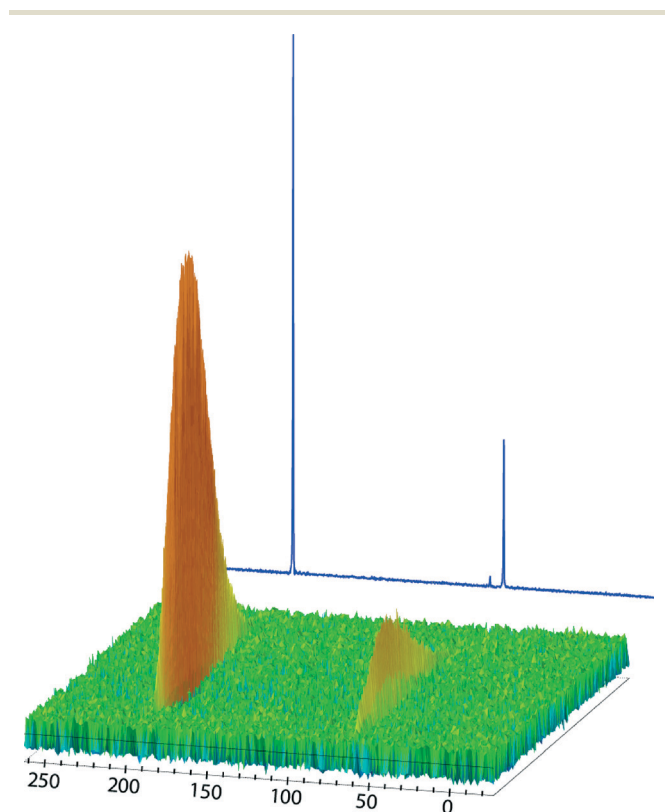


Fig. 1 Device for driven-flow of gas-loaded solutions into an NMR magnet. A syringe pump, whose console (1) is connected to the NMR console, pushes in a controlled way *via* a buffer gas (2) the gas of interest contained in the reservoir (3) to the NMR cell containing the solution (4). This cell is connected to the NMR probe head (5).

encapsulated in host systems in which it takes a specific resonance frequency.<sup>10</sup> The spectral resolution obtained for the dissolved gas and the performance in terms of the rate of gas loading of the solution, a value rarely given in the literature, were the two important parameters that we wanted to estimate. Therefore a molecular system in which xenon appears in slow exchange on the NMR time scale with known thermodynamics and in-out exchange kinetics was chosen. Aqueous solutions of cryptophane-222-hexacarboxylate were prepared and introduced with a syringe into the NMR cell. With such a molecular system for which the xenon binding constant is known ( $K = 6800 \text{ M}^{-1}$  at 293 K),<sup>11</sup> the instantaneous concentration of xenon in solution can be estimated.

Fig. 3 displays the  $^{129}\text{Xe}$  NMR spectra recorded on a 0.5 mM solution of cryptophane-222-hexacarboxylate in  $\text{D}_2\text{O}$  with the integrated NMR system. For this experiment, the flow rate was 10 mL per minute. Two consecutive spectra were separated by 1 second, and  $90^\circ$  rf pulses were used. Several observations can be made. When hyperpolarized xenon reaches the detection region, two signals appear: the signal at 195 ppm corresponds to the gas dissolved in water, and the



**Fig. 3**  $^{129}\text{Xe}$  NMR experiment performed with the driven-flow device. Two consecutive spectra are separated by 1 second. 500  $\mu\text{L}$  of a 0.5 mM aqueous solution of cryptophane-222-hexacarboxylate fills the reservoir of the NMR cell. Hyperpolarized xenon, prepared in batch mode, is pushed by the syringe containing nitrogen. The peak at 195 ppm corresponds to xenon dissolved in water, and the peak at 64 ppm to xenon in cryptophane. The displayed 1D spectrum corresponds to the projection. Note that the small peak at 73 ppm reveals the presence of residual cryptophane.

one at 64 ppm to xenon encapsulated in the cryptophane cavity. Remarkably, there is absolutely no signal at 0 ppm, proving that no xenon bubble is present in the detection region. Also the FWHM of the NMR peaks is less than 50 Hz, confirming the high magnetic field homogeneity. Integration of the xenon signals leads to estimation of the instantaneous total xenon concentration in solution (see Fig. S4 in the ESI†).

## Discussion

The system we have developed has many advantages.

First of all, it is very versatile, as it can be installed on a classical micro-imaging probe head with few adaptation steps. This is in particular the reason for the design represented in Fig. 1. We could have imagined introducing the gas from the bottom of the magnet in an LC-NMR-like fashion.<sup>12</sup> In this case, the magnetic field outside the magnet would have been higher, and the distance between the gas reservoir and the solution sample would have been lower. But this solution would have lacked flexibility, and would have been reserved to only one probe head. With our system, every change in sample or even rf coil is straightforward. For the same reason, the usual capabilities of a classical probe head can be employed: i) tuning of the electric circuit is performed using tuning rods, and ii) spectrally resolved spectra and spatially resolved images can be recorded.

Second, no bubble is present in the detection area, as testified by the absence of signal near 0 ppm in the  $^{129}\text{Xe}$  NMR spectra. The dissolution yield is high (see below) as well as the xenon polarization level. We have tested various mixtures of nitrogen-xenon in the glass coil without noticeable difference.

Third, both the design of the gaseous reservoir and that of the sample chamber are optimized for short-lived or precious species. The location of the gaseous reservoir can be freely chosen according to the desired magnetic field. The location of the chamber not only minimizes the volume of the solution, but also allows one to conserve it in a high and homogeneous magnetic field. This can be of importance for applications dealing with hyperpolarized xenon. The design of the chamber enables the use of a horizontal solenoid micro-coil of maximal sensitivity, and avoids the usual convection problems linked to temperature regulation from the bottom of the probe.

The efficiency of the bubble pump is high, and infuse flow rates between 1 and 10  $\text{mL min}^{-1}$  give successful results with hyperpolarized xenon. The experiment shown in Fig. 3, performed with a high flow rate value of 10  $\text{mL min}^{-1}$ , was intended to show that even in such conditions no bubble was observed, but did not use in an optimized manner the hyperpolarized gas (see Fig. S2 in the ESI†).<sup>13</sup> In another – more realistic – example shown in Fig. 4, the flow rate was 1  $\text{mL min}^{-1}$ ; two consecutive  $^{129}\text{Xe}$  spectra were separated by 500 ms, and  $90^\circ$  rf pulses were used. Under such conditions, it was possible to observe the dissolved xenon signals for about 8 minutes. As mentioned above and detailed in the



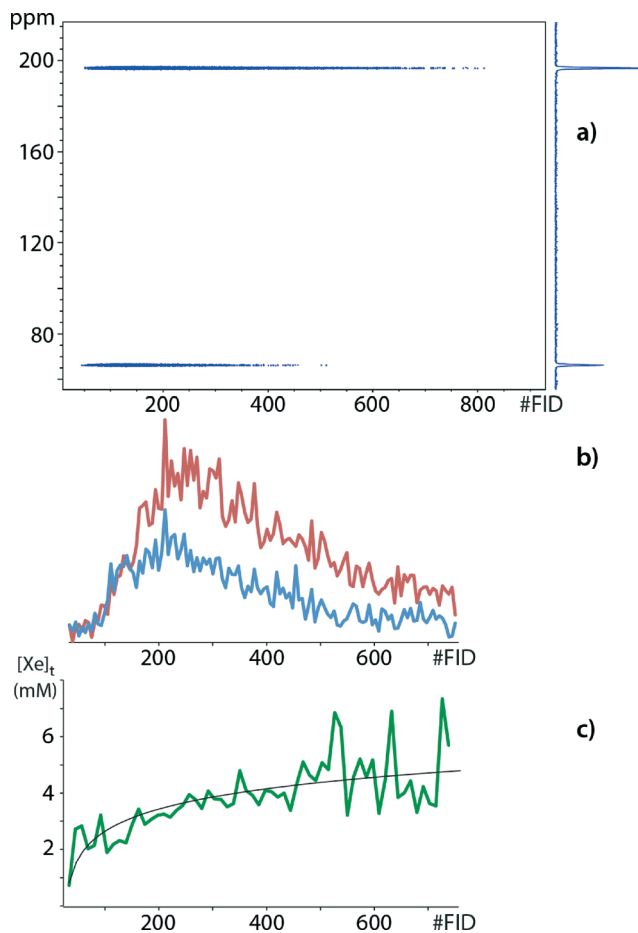


Fig. 4 a)  $^{129}\text{Xe}$  NMR experiment performed with a 1.3 mM solution of cryptophane-222-hexa-carboxylate and a gas flow rate of  $1 \text{ mL min}^{-1}$ . Two consecutive spectra are separated by 0.5 second. b) Areas of the signals of dissolved xenon (in red) and of xenon in cryptophane (in blue). c) Estimation of the instantaneous concentration of xenon in solution from these signal areas.

ESI,<sup>†</sup> the instantaneous total concentration of xenon can be estimated (green curve) from the ratio between the signals of dissolved xenon (in red) and the xenon@cryptophane signal (in blue). Remarkably, at this flow rate the xenon concentration is nearly constant, with an average value of  $4.0 \pm 0.5 \text{ mM}$ . Given that the detection volume is known ( $5 \mu\text{L}$  according to the recorded magnetic resonance images, see Fig. S1 in the ESI<sup>†</sup>), and that hyperpolarization is systematically destroyed by each  $90^\circ$  rf pulse, the total number of moles of xenon detected can be estimated and compared to the initial amount of gas in the syringe (which can be estimated through simple weighing of the glass coil before the transfer and after evacuation). In the experiment in Fig. 4, the measurement indicates that *ca.* 15% of the quantity of xenon in the syringe has been detected in the dissolved state, a value that is satisfying for us.

A detailed look at the results in Fig. 4 reveals the oscillatory character of the xenon signals (see Fig. S3 in the ESI<sup>†</sup>), which is always observed at such flow rates (but not for high rates as in the experiment in Fig. 3). This is due to the

discrete nature of bubbling, and is related to the inner diameter of the capillary for the gas input. In the next version of the bubble pump, the capillary will end with many small holes in order to reduce the size of the bubbles and to induce a continuous flow rate, even at low speed.

The ratio between the two peaks remains nearly constant all throughout the series. It means that hyperpolarization disappears before a significant decrease in the dissolved xenon concentration is detected. Therefore it is possible to extract from the second part of the curves the apparent xenon relaxation time  $T_1$  (see Fig. S3 in the ESI<sup>†</sup>). A value of 294 s was found.

## Conclusion

We have conceived an integrated solution to optimize the dissolution of a short-lived or precious gas in small quantities of liquids, and to optimize NMR detection of the resulting solution. By using 3D printing, the problems related to cleanroom techniques are avoided, and a cheap device that enables easy replacement of not only the solution of interest but also of the rf detection part is proposed. Such a low-cost and disposable system is fully compatible with spectroscopy and imaging, as the spectral and spatial resolutions are not significantly degraded. Our device is composed of a solenoid coil of millimetric size for rf detection as it is the most sensitive design and is perfectly adapted to our experiments, but obviously, further miniaturization could be applied *via* the use of planar or microslot probes,<sup>14</sup> at the price of a worse rf homogeneity. In this work, xenon is hyperpolarized in batch mode, but of course a further step could also be to miniaturize the optical pumping step<sup>15</sup> and insert it in the NMR magnet, close to the bubble pump and the NMR chamber.

In the current article, the proof-of-concept has been made *via* hyperpolarized  $^{129}\text{Xe}$  NMR experiments, but we have checked that for other gases such as  $\text{H}_2$  or  $\text{N}_2$  the bubble pump still works. Here a judicious choice of the molecular system enabled us to (roughly) estimate the instantaneous concentration of dissolved xenon during the operation of the bubble pump, and in the future will enable us to optimize the experimental conditions. Also future studies will be directed towards further minimization of the solution volume, as well as optimization of the experimental conditions (pressure in the syringe, flow rate, *etc.*) and finally simultaneous NMR detection of  $^{129}\text{Xe}$  and  $^1\text{H}$  nuclei.

## Experimental

### Materials and methods

**Driven-flow device.** A non-magnetic syringe pump (2) (Harvard Apparatus, MRI-compatible model PHD2000) is fixed on top of the NMR magnet in a magnetic field of 100 G. At the beginning of the experiment, the syringe is filled with nitrogen. The gas of interest – hyperpolarized noble gas or *para*-hydrogen – is produced in batch mode and is contained in a Pyrex reservoir or glass coil (3). This reservoir is also fixed on top of the magnet; it is connected *via* silicon tubes

to the syringe and to the solution placed inside the magnet in the NMR cell. Vacuum can be made in these silicon tubes through a remote primary pump placed beyond the 5 gauss fringe field line. The console of the syringe pump (1) is connected *via* a TTL port at the TCU3 board of the Bruker Avance II NMR console, precisely on the T2-E slot. The program set on the syringe pump console trigs the NMR sequence, enabling the use of synchronized acquisition during continuous- or stopped-flow infusion.

**NMR cell fabrication *via* additive prototyping.** Initially, designs of the cell were created using the open source 3D computer-aided design program FreeCAD 0.14. The resulting file (STL format) was used by the Stratasys software to create slices of our 3D device. The printing parts were performed with an Objet30 pro 3D printer (Stratasys, Prairie, Minnesota) using PolyJet technology (ink jet technology). The 3D printer jets fine droplets of a liquid photopolymer followed by UV polymerization. Fine layers accumulate on the build tray to create a precise 3D model. The top part of the NMR cell, including the exchange module, was printed in a PMMA-like photopolymerizable resin, which presents high resolution (VeroClear RGD810 resin (Stratasys), deposited layer of 14  $\mu\text{m}$ ) using default support material setting. The lower part (for connection to the micro-imaging probe head) was printed in an ABS-like photopolymerizable resin that withstands higher temperatures to solder connections (RGD525 resin (Stratasys) deposited layer of 28  $\mu\text{m}$ ) using default support material setting. This support material was physically removed with high-pressure water after being weakened in 2 wt.% aqueous NaOH solution for 1 hour at room temperature. To obtain the best properties for the different polymers, a post-process treatment was necessary. Polymerization of the PMMA parts was completed under light (a classic desk lamp) at 40 °C for 6 hours. Polymerization of the ABS parts was ended by an annealing procedure that consists of a first stage at 50 °C for 2 hours, a second stage at 60 °C for 2 hours and a final stage at 70 °C for 1 hour.

The rf antenna consisted of a solenoid obtained by rolling up a 250  $\mu\text{m}$  diameter copper wire around a fine glass tube (1.8 mm exterior diameter and 1.0 mm interior diameter). The number of turns depends on the resonance frequency of the observed nucleus and the probe head used. For example, for proton measurement in an 11.7 T narrow bore magnet with a micro-5 Bruker probe head, use of a solenoid of 9 turns was used and addition of a 0.8 pF capacitance in series was necessary to tune it at 500 MHz. Under the same conditions, for hyperpolarized  $^{129}\text{Xe}$  measurement at 138 MHz, 29 turns without any capacitance added were necessary.

**Production of hyperpolarized xenon.** Xenon enriched with 83% isotope 129 (Euriso-Top, France) is spin-polarized in batch mode *via* spin-exchange optical pumping, using our home-built setup previously described.<sup>16</sup> Then after separation from helium and nitrogen, frozen xenon is stored in a glass coil placed inside a 3 kG solenoid immersed in liquid nitrogen. The glass coil is then transferred to the spectrometer, where it cools down to room temperature in a fringe field

value of 100 G delivered by an 11.7 T NMR magnet. It is then connected to the silicon tubing (position (3)).

**NMR data processing.** All xenon spectra have been apodized by a 10 Hz Lorentzian function before Fourier transformation. The curves displayed in Fig. 4 have been obtained using an automation program in Bruker Topspin 3.1.

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