

1 **Skeletal muscle oxidative function *in vivo* and *ex vivo* in athletes with marked**
2 **hypertrophy from resistance training**

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15 **Running head:** Oxidative function in athletes with marked muscle hypertrophy

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25

26 **Abstract**

27

28 Oxidative function during exercise was evaluated in 11 young athletes with marked skeletal
29 muscle hypertrophy induced by long-term resistance training (RTA, body mass 102.6 ± 7.3 kg,
30 mean \pm SD) and 11 controls (CTRL, body mass 77.8 ± 6.0). Pulmonary $\dot{V}O_2$ and vastus
31 lateralis muscle fractional O_2 extraction (by near-infrared spectroscopy) were determined during
32 an incremental cycle ergometer (CE) and one-leg knee-extension (KE) exercise. Mitochondrial
33 respiration was evaluated *ex vivo* by high-resolution respirometry in permeabilized vastus lateralis
34 fibers obtained by biopsy. Quadriceps femoris muscle cross sectional area, volume (determined by
35 magnetic resonance imaging) and strength were greater in RTA vs. CTRL (by $\sim 40\%$, $\sim 33\%$ and
36 $\sim 20\%$, respectively). $\dot{V}O_{2peak}$ during CE was higher in RTA vs. CTRL (4.05 ± 0.64 L min^{-1} vs.
37 3.56 ± 0.30); no difference between groups was observed during KE. The O_2 cost of CE exercise
38 was not different between groups. When divided per muscle mass (for CE) or quadriceps muscle
39 mass (for KE) $\dot{V}O_{2peak}$ was lower (by 15-20%) in RTA vs. CTRL. Vastus lateralis fractional O_2
40 extraction was lower in RTA vs. CTRL at all work rates, both during CE and KE. RTA had higher
41 ADP-stimulated mitochondrial respiration (56.7 ± 23.7 pmol $O_2 \cdot s^{-1} \cdot \text{mg}^{-1}$ ww) vs. CTRL (35.7 ± 10.2),
42 and a tighter coupling of oxidative phosphorylation. In RTA the greater muscle mass and maximal
43 force, and the enhanced mitochondrial respiration seem to compensate for the hypertrophy-
44 induced impaired peripheral O_2 diffusion. The net results are an enhanced whole body oxidative
45 function at peak exercise, and unchanged efficiency and O_2 cost at submaximal exercise, despite a
46 much greater body mass.

47

48 **Key words:** skeletal muscle hypertrophy; mitochondrial respiration; oxidative metabolism during
49 exercise.

50

51 **Introduction**

52

53 Resistance training programs have been developed with the aim of improving variables of muscle
54 function such as strength, power, speed, local muscular endurance, coordination, and flexibility
55 (21). Resistance training is now considered an important part of training and rehabilitation
56 programs for healthy subjects and for various types of patients, such as cardiac patients (45),
57 patients with pulmonary diseases (10), patients undergoing prolonged bed rest periods (2), or
58 elderly subjects (28). In these populations, the combination of resistance training with the more
59 conventional endurance exercise improves the patients' outcomes and quality of life (45).

60 An increase in the cross sectional area of skeletal muscle fibers and a shift of fiber type
61 distribution towards type 2 fibers are typical adaptations induced by resistance training; these
62 adaptations enhance the muscle force-generating potential (12) but could represent an impairment
63 to skeletal muscle oxidative metabolism. On the other hand, muscles with higher maximal force
64 would need to recruit a lower number of motor units, and therefore more oxidative (and more
65 efficient) muscle fibers (20, 26). According to other authors strength training may increase
66 skeletal muscle efficiency (4) and enhance skeletal muscle "metabolic stability" (50). Other
67 studies reported, after resistance training, unchanged values of maximal O₂ uptake (6), as well as
68 unchanged (19) or lower (42, 43) mitochondrial volume density, oxidative enzyme activity, and
69 capillary density in the hypertrophic muscles. Thus, the specific effects of resistance training, with
70 the related changes in muscle phenotype, on oxidative metabolism appear difficult to reconcile in
71 a unifying *scenario*. The aim of the present study was to determine whether increases in muscle
72 mass induced by chronic resistance training are associated, in humans, with alterations in skeletal
73 muscle oxidative function and aerobic performance. Experiments were carried out on a group of
74 resistance-trained athletes (RTA), in whom muscle adaptations to resistance exercise are expected
75 to be particularly marked. An integrative approach was applied by analyzing oxidative metabolism

76 at different levels, spanning from pulmonary gas exchange to skeletal muscle function and
77 mitochondrial respiration. Oxidative function was assessed *in vivo* during incremental cycle
78 ergometer (CE) exercise and dynamic knee extension (KE) exercise with one leg (3). During KE
79 the recruitment of a relatively small muscle mass, *i.e.* the *quadriceps femoris* of one leg,
80 significantly reduces constraints to oxidative function deriving from cardiovascular O₂ delivery,
81 thereby allowing a more direct assessment of quadriceps muscle oxidative capacity *in vivo*. The
82 intrinsic properties of mitochondria were assessed *ex vivo*, in permeabilized muscle fibers
83 obtained by biopsy, by high-resolution respirometry (36).

84 We hypothesized, in RTA *vs.* control subjects (CTRL), an impaired skeletal muscle oxidative
85 function *in vivo* and an impaired mitochondrial respiratory function *ex vivo*.

86

87 **Materials and Methods**

88

89 **Subjects**

90 We evaluated eleven male RTA (age 25.4 ± 6.1 [mean \pm SD] years; body mass (BM) 102.6 ± 7.3
91 kg; stature 1.84 ± 0.04 m; body mass index (BMI) 30.1 ± 2.6 kg·m⁻²), who had been following for
92 at least 5 years resistance training programs specifically designed to increase quadriceps muscle
93 strength and power, and eleven physically active CTRL (age 25.4 ± 3.8 years; BM 77.8 ± 6.0 kg;
94 height 1.81 ± 0.05 m; BMI 23.8 ± 2.2 kg·m⁻²). A thigh circumference above 60 cm (with thigh fat
95 thickness below 10 mm) was taken as a criterion for including subjects in the RTA group. A diary
96 of the training regimen and physical activity, focused on the 8 weeks preceding the evaluation,
97 was collected. RTA practiced sport activities such as American football (tackle position), track
98 and field (throwing), and weightlifting for an average of 487 ± 204 minutes per week. Most of
99 them took part at national-level competitions and championships. In their training sessions RTA
100 included standard protocols of resistance exercise targeting all major upper body and lower body

101 muscle groups. The RTA training regimen could be categorized as high-intensity and low-volume
102 resistance exercise training (21). The RTA subjects also practiced aerobic exercise such as running
103 and cycling for about 127 ± 150 minutes per week. CTRL practiced running and cycling for about
104 153 ± 133 minutes/wk and sport activities such as tennis, handball or gym activities for 102 ± 143
105 minutes/wk, respectively, essentially for recreational purposes. They did not follow any resistance
106 training program or any other specific training schedule.

107 Careful medical and pharmacological histories were collected. RTA and CTRL were not affected
108 by any disease and were not taking any drug at the time of the study. RTA did not report any drug
109 misuse to support their training. Participants were informed about the aims and methods of the
110 investigation and gave their written informed consent. The experiments were carried out at the
111 Valdoltra Orthopaedic Hospital of Ankaran, Slovenia. All procedures conformed to the
112 declaration of Helsinki (2000) and were approved by the Slovenian National Medical Ethics
113 Committee.

114 All tests were conducted under close medical supervision and following standard safety
115 procedures, and the subjects were continuously monitored by 12-lead electrocardiography (ECG).

116

117 **Exercise protocols**

118 Incremental exercise protocols were carried out by utilizing a mechanically braked cycle (CE)
119 ergometer (Monark Ergomedic 839E), and a custom-built knee extension (KE) ergometer
120 (modified Monark cycle ergometer), as originally described by Andersen et al. (3). The exercise
121 protocols were conducted in random order during different experimental sessions separated by a
122 24h recovery period.

123 During CE subjects performed an initial 4 min pedalling at 80 W, thereafter 20 W increments
124 were imposed every minute until voluntary exhaustion. Pedalling frequency was kept at ~ 60 rpm,
125 as imposed by a metronome. During KE subjects were constrained on an adjustable seat by a

126 safety belt, which anchored the angle of the hip at $\sim 90^\circ$. Subjects pushed on a padded bar attached
127 to a lever arm connected to the crank of the cycle ergometer, and allowing a knee extension
128 between ~ 90 to ~ 170 degrees. This type of exercise confines muscle contractile activity to the
129 *quadriceps femoris* muscle of one leg, which is activated during the extension phase. The return of
130 the leg to the starting position is brought about passively by the momentum of the flywheel of the
131 ergometer (see 37 for details). Before data collection, each subject was familiarized with the setup
132 environment and the exercise protocol by short preliminary practice runs. After an initial 3 min of
133 unloaded KE exercise, an incremental test was performed. Work rate increments were imposed
134 every minute, in order to allow the subjects to reach exhaustion in ~ 10 min. Work rate was applied
135 by adjusting the tension of a strap around the ergometer flywheel, as in a mechanically braked
136 cycle ergometer. Throughout the test the active KE and passive knee flexion cycle was carried out
137 ~ 40 times per minute, as imposed by a metronome. During each cycle (total duration 1.5 s) KE
138 lasted ~ 1 s. In other words muscle contraction corresponded to $\sim 65\%$ of the duty cycle.

139 All the exercises were conducted up to the limit of tolerance. The latter was defined as the
140 inability to maintain the imposed work rate at the required frequency, despite vigorous
141 encouragement by the operators. Mean values of cardiovascular, ventilatory, gas exchange and
142 muscle oxygenation variables (see below) were calculated during the last 20 seconds of each work
143 rate; values obtained during the exhausting work rate were considered “peak” values.

144

145 **Measurements**

146 *Anthropometry.* Fat-free mass (FFM) and total skeletal muscle mass were assessed by bioelectric
147 impedance analysis (BIA) performed by a tetrapolar device (Human IM, Dietosystem, Italy) in
148 accordance with the conventional standard technique (25).

149 *Anatomical CSA, muscle volumes and muscle force.* Anatomical cross sectional area (CSA) of
150 right thigh muscles and of the right quadriceps were measured from turbo spin-echo, T1-weighted,

151 Magnetic Resonance Images (MRI) obtained with a 1.5 Tesla (Magnetom Avanto; Siemens
152 Medical Solution, Erlangen, Germany). On each MRI slice, contours corresponding to the thigh
153 muscles and quadriceps were delineated by an expert of MRI imaging, using the image processing
154 tools available in the commercial software package AMIRA (v 4.1, Mercury Computer System
155 Inc., Chelmsford, MA, USA). The volumes of thigh muscles and quadriceps were then derived as
156 the geometrical volumes included in these contours.

157 Before the incremental tests, subjects performed two maximal voluntary isometric contractions
158 (MVC) of the knee extensors of the right leg at a 110° knee angle. Force was measured by an
159 electrical transducer (TSD121C, BIOPAC Systems, Inc., USA) implemented on a custom-built
160 chair for isometric contractions of knee extensor and flexor muscle groups. Force was sampled at
161 a frequency of 1 kHz (MP100, BIOPAC Systems).

162 *Measurements during the incremental tests.* Time to exhaustion was taken as an index of
163 performance. Pulmonary ventilation ($\dot{V}E$), tidal volume (VT), respiratory frequency (fR), O₂
164 uptake ($\dot{V}O_2$) and CO₂ output ($\dot{V}CO_2$) were determined on a breath-by-breath basis by means of
165 a metabolic unit (Quark b², Cosmed, Italy). Expiratory flow measurements were performed by a
166 turbine flow meter calibrated before each experiment by a 3 L syringe at three different flow rates.
167 Calibration of O₂ and CO₂ analyzers was performed before each experiment by utilizing gas
168 mixtures of known composition. The gas exchange ratio (R) was calculated as $\dot{V}CO_2 / \dot{V}O_2$. The
169 gas exchange threshold (GET) was determined by the V-slope method (5). All the data related to
170 GET were expressed as a percentage of $\dot{V}O_2$ peak.

171 During KE a biphasic pattern in the $\dot{V}O_2$ vs. work rate relationship was observed (see Richardson
172 et al., 34). During CE $\dot{V}O_2$ and $\dot{V}O_2$ peak values were expressed as L·min⁻¹ and normalized per
173 unit of whole body muscle mass (mL·min⁻¹·kg⁻¹), whereas during KE $\dot{V}O_2$ and $\dot{V}O_2$ peak values
174 were expressed as L·min⁻¹ and normalized as mL·min⁻¹·100g⁻¹ of quadriceps muscle mass (QM).

175 The latter was calculated on the basis of quadriceps muscle volume (see above), after assuming a
176 standard value for skeletal muscle density of $1.060 \text{ kg}\cdot\text{L}^{-1}$ (27).

177 Heart rate (HR) was determined by ECG. Stroke volume (SV) was estimated beat-by-beat by
178 impedance cardiography (Physio Flow, Manatec, Paris, France) (33). The accuracy of this device
179 has been previously evaluated during incremental exercise in healthy subjects against the direct
180 Fick method (33); in that study, the correlation coefficient between the two methods was $r = 0.946$
181 ($P < 0.01$), and the mean difference was equal to $-2.78 \pm 12.33\%$ (2 SD). Overall, the accuracy of
182 this method can be considered “acceptable” for the purpose of the study, that is to demonstrate
183 that the cardiac involvement during KE was not “maximal” also at peak exercise (as confirmed
184 also from HR measurements). Cardiac output (\dot{Q}) was calculated as $\text{HR}\cdot\text{SV}$. Cardiac index (CI;
185 $\dot{Q}/\text{body surface}$) was also determined in order to take into account the difference in body size
186 between RTA and CTRL.

187 Oxygenation changes in *vastus lateralis* muscle were evaluated by near-infrared spectroscopy
188 (NIRS) (7, 13). Reliability of tissue oxygenation indices obtained by NIRS, evaluated by the
189 intraclass correlation coefficient for repeated measurements on the same subject during different
190 days, was found to be very high for skeletal muscle (41). NIRS measurements in muscle tissue
191 have been shown to be well correlated with local venous O_2 saturation (48). A portable NIR
192 continuous-wave photometer (PortaMon, Artinis, The Netherlands) was utilized. Specific details
193 on the method can be found in recent papers by our group (32, 37). The instrument measures
194 micromolar (μM) changes in oxygenated haemoglobin (Hb) + myoglobin (Mb) concentrations
195 ($\Delta[\text{oxy}(\text{Hb}+\text{Mb})]$), and in deoxygenated [Hb + Mb] ($\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$), with respect to an initial
196 value arbitrarily set equal to zero and obtained during the resting condition preceding the test.
197 $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$ is relatively insensitive to changes in blood volume and has been considered an
198 estimate of skeletal muscle fractional O_2 extraction (ratio between O_2 consumption and O_2
199 delivery) (15, 18). A "physiological calibration" of $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$ values was performed by

200 obtaining a transient ischemia of the limb after the exercise period: data obtained during exercise
201 were expressed as a percentage of the values of maximal muscle deoxygenation obtained by
202 pressure cuff inflation (at 300-350 mm Hg), carried out at the inguinal crease of the thigh for a
203 few minutes, until $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$ increase reached a plateau (18). $\Delta[\text{deoxy}(\text{Hb}+\text{Mb})]$ kinetics
204 during the incremental tests were fitted by a sigmoid function, as proposed by Ferreira et al. (14).

205 *Skeletal muscle biopsy and high-resolution respirometry.* Muscle samples were obtained from the
206 *vastus lateralis* muscle of the left limb by percutaneous biopsy which was taken, for all subjects, 5
207 h after the last incremental test. Biopsy was done after anesthesia of the skin, the subcutaneous fat
208 tissue and the muscle fascia with 2 mL of lidocaine (2%). A small skin incision was then made to
209 penetrate skin and fascia, and the tissue sample was harvested with a purpose-built rongeur (Zepf
210 Instruments, Tuttlingen, Germany). The muscle samples were divided into two portions. One
211 portion (~10 mg wet weight) was immediately frozen in liquid nitrogen and stored at -80°C until
212 enzymatic determination of citrate synthase (CS) activity. The other portion (~10 mg wet weight)
213 was used to measure mitochondrial respiration *ex vivo* and was immediately placed in an ice-cold
214 relaxing solution containing: EGTA-calcium buffer (10 mM) (free Ca^{2+} concentration 100 nmol L^{-1}),
215 imidazole (20 mM), taurine (20mM), $\text{K}^{+}/4$ morpholinoethanesulfonic acid (K-MES; 50 mM),
216 dithiothreitol (DTT; 0.5 mM), MgCl_2 (6.56 mM), ATP (5.77 mM), phosphocreatine (15 mM), pH
217 7.1.

218 The fiber bundles were separated with sharp-ended needles, leaving only small areas of contact,
219 and were incubated in 5 mL of the above solution (4°C) containing $50 \mu\text{g mL}^{-1}$ saponin for 30 min
220 with continuous gentle stirring, in order to ensure complete permeabilization. After being rinsed
221 twice for 10 min in a respiration medium (MiR05, Oroboros, Innsbruck, Austria; 0.5 mM EGTA,
222 60 mM potassium lactobionate, 3 mM $\text{MgCl}_2 \cdot 6\text{H}_2\text{O}$, 20 mM taurine, 10 mM KH_2PO_4 , 20 mM
223 HEPES, 110 mM sucrose and 1 g/L BSA, pH 7.1), permeabilized fibers were measured for wet

224 weight and immediately transferred into a respirometer (Oxygraph-2k; Oroboros Instruments,
225 Innsbruck, Austria) for the analysis.

226 Mitochondrial respiratory function was evaluated by measuring O₂ consumption polarographically
227 by high-resolution respirometry (17, 29). Data were digitally recorded using DatLab4 software
228 (Oroboros Instruments). The instrumentation allows for O₂ consumption measurements with small
229 amounts of sample in closed respiration chambers containing 3 mL of air-saturated respiration
230 medium at 30°C; 3-5 mg of muscle fibers were used for the analysis. Standardized instrumental
231 and chemical calibrations were performed to correct for back-diffusion of O₂ into the chamber
232 from the various components, leak from the exterior, O₂ consumption by the chemical medium,
233 and sensor O₂ consumption (29). The O₂ concentration in the chamber was maintained between
234 250 and 400 μM to avoid O₂ limitation of respiration. Intermittent reoxygenation steps were
235 performed during the experiments by adding a 200 mM hydrogen peroxide solution into the
236 medium containing catalase (29). A substrate-uncoupler-inhibitor-titration protocol with a
237 substrate combination that matches physiological intracellular conditions was applied (17). Non
238 phosphorylating resting mitochondrial respiration was measured in the presence of malate (4
239 mM), glutamate (10 mM), and succinate (10 mM), without ADP, so that O₂ consumption was
240 mainly driven by the back leakage of protons through the inner mitochondrial membrane (“leak”
241 respiration). ADP-stimulated mitochondrial respiration (“state 3” respiration) was measured after
242 the subsequent addition of ADP (2.5 mM) as phosphate acceptor with malate, glutamate and
243 succinate as substrates. The addition of cytochrome *c* (10 μM) had no additive effects on
244 respiration, with minor increases of ~2%, thereby confirming the integrity of the outer
245 mitochondrial membrane. We also examined electron transport system capacity by stepwise
246 addition of the chemical uncoupler protonophore carbonylcyanide-p-
247 trifluoromethoxyphenylhydrazone (FCCP) to optimum concentration (1.25 μM). Rotenone (1 μM)
248 and antimycin A (2.5 μM) were added to inhibit complexes I and III, providing a measure of

249 residual O₂ consumption, indicative of non-mitochondrial O₂ consumption. Mitochondrial
250 respiration was then corrected for O₂ flux due to the residual O₂ consumption. The respiratory
251 acceptor control ratio (RCR), taken as an index of coupling between electron transfer and
252 phosphorylation, was obtained by dividing state 3 respiration by leak respiration.

253 CS activity was determined in frozen fiber bundles (~5 mg wet weight), which were homogenized
254 in buffer (2,5% w/v) containing 250 mM sucrose, 40 mM KCl, 2 mM EGTA, 20 mM Tris HCl
255 (pH 7.4) and supplemented with 0,1% Triton X-100. CS activity was assayed according to Sreer
256 (40) by spectrophotometric methods (Lambda 14 Spectrometer; Perkin Elmer) and was expressed
257 as micromoles of substrate per minute per gram of total protein content. Protein content was
258 estimated by Bradford assay (8).

259

260 **Statistical analysis**

261 Results were expressed as means ± standard deviation (SD). Statistical significance of differences
262 between groups (RTA vs. CTRL) was checked by two-tailed Student's *t* test for unpaired data.
263 Bonferroni correction was used for multiple comparisons. The level of significance was set at
264 *P*<0.05. Statistical analyses were carried out with software packages (GraphPad Prism 4.0,
265 GraphPad Software Inc.; SPSS, Statistical Package Social Sciences, 13.0.1).

266

267 **Results**

268

269 Values of the anatomical cross-sectional area (CSA) of quadriceps muscle, calculated at 50%
270 femur length, are shown in **Figure 1A**. As expected on the basis of the selective inclusion criteria
271 of the study, CSA in RTA was significantly greater (by 37%) than in CTRL. Also the volume of
272 the quadriceps was significantly greater (by 33%) in RTA vs. CTRL (**Figure 1B**). Values of BM,
273 BMI, fat-free mass, skeletal muscle mass, and quadriceps muscle mass are reported in **Table 1**.

274 For all variables, values in RTA were significantly (by about 30%) greater in RTA vs. CTRL.

275 Also the percentage of body fat was slightly but significantly greater in RTA vs. CTRL.

276 The mean force exerted by the knee extensors during MVC was significantly higher (by 18%;

277 $P=0.026$) in RTA (998 ± 163 N) vs. CTRL (811 ± 188 N). Once normalized per unit of CSA,

278 values did not differ between groups (7.9 ± 0.8 N·cm⁻² in RTA vs. 8.7 ± 1.9 N·cm⁻² in CTRL).

279

280 Peak values of the main ventilatory and gas-exchange variables determined at the limit of

281 tolerance during CE and KE are presented in **Table 2**. Ventilatory variables were not different in

282 the two groups, both during CE and KE, with the exception of a higher VT peak in RTA during

283 CE. When expressed in L·min⁻¹, $\dot{V}O_2$ peak was higher in RTA vs. CTRL during CE; no

284 significant difference was observed during KE. When $\dot{V}O_2$ peak was expressed per unit of body

285 mass or body muscle mass (for CE) and per unit of quadriceps muscle mass (for KE), values were

286 significantly lower (by ~15-20%) in RTA vs. CTRL. Peak work rate was slightly but not

287 significantly higher during CE in RTA vs. CTRL; time to exhaustion values were not different in

288 the two groups, either during CE or KE. R peak values were higher than 1.1 in both groups during

289 both types of exercise. Peak values of HR, \dot{Q} and CI were similar between RTA and CTRL, either

290 during KE or during CE (Table 2). As expected, in both groups peak values of cardiovascular

291 variables obtained in KE were significantly lower than in CE.

292

293 Pulmonary $\dot{V}O_2$ values (mL min⁻¹) are plotted as a function of work rate in Figure 2, during CE

294 (left panel) and during KE (right panel). To obtain these figures, individual $\dot{V}O_2$ values were

295 grouped for discrete work rate intervals, which were determined in order to have, in each interval,

296 each subject represented by one data point. When the subject had more than one “original” data

297 points in the interval, mean individual values were calculated, both for the x and the y variables,

298 and were taken in consideration to obtain the figure.

299 As for CE, mean (\pm SD) values of the intercepts and of the slopes of the individual linear
300 regression lines (shown in the Figure legend) were not significantly different in RTA vs. CTRL.
301 The mean slopes of the individual regression lines were 10.6 ± 0.9 mL min⁻¹ watt⁻¹ in RTA, and
302 10.3 ± 0.7 mL min⁻¹ watt⁻¹ in CTRL (no significant difference). Peak $\dot{V}O_2$ and peak work rate
303 values are described in Table 2. As for KE, whereas the mean values of the slopes (submaximal
304 work rates) were not different in the two groups, the intercepts values were higher in RTA. The
305 mean slopes of the individual regression lines were 9.5 ± 1.1 mL min⁻¹ watt⁻¹ in RTA, and $9.7 \pm$
306 1.9 mL min⁻¹ watt⁻¹ in CTRL (no significant difference). Peak $\dot{V}O_2$ and peak work rate values are
307 described in Table 2. Peak $\dot{V}O_2$ values normalized for muscle mass (for CE) or quadriceps
308 muscle mass (for KE) are shown in Figure 3.

309

310 Values of NIRS-obtained $\Delta[\text{deoxy(Hb+Mb)}]$, which was taken as an estimate of *vastus lateralis*
311 muscle fractional O₂ extraction, are shown in **Figure 4** as a function of work rate, during CE (left
312 panel) and KE (right panel). Work rate intervals were defined according to the principles
313 described above for Figure 2. Both in RTA and CTRL, either during CE or KE, the dynamics of
314 $\Delta[\text{deoxy(Hb+Mb)}]$ followed a sigmoid pattern, with a tendency to plateau at $\sim 85\%$ of peak work
315 rate. At all work rate levels, values of $\Delta[\text{deoxy(Hb+Mb)}]$ were significantly lower in RTA vs.
316 CTRL, both during CE and KE; peak values were $\sim 30\%$ lower in RTA (vs. CTRL) either during
317 CE or KE.

318

319 ADP-stimulated mitochondrial respiration (state 3 respiration), fueled by malate, glutamate and
320 succinate, as determined by high-resolution respirometry, was significantly higher (by $\sim 60\%$) in
321 RTA vs. CTRL (**Figure 5A**). CS activity, taken as an estimate of mitochondrial content (24), was
322 similar in the two groups (**Figure 5B**). Maximal mitochondrial respiration induced by the
323 chemical uncoupler FCCP, reflecting the maximal oxidative capacity of the electron transport

324 system (ETS), was not significantly different in RTA ($68.0 \pm 31.4 \text{ pmolO}_2 \cdot \text{s}^{-1} \cdot \text{mg}^{-1}$ wet weight) vs.
325 CTRL (52.1 ± 22.3). No differences between groups were found in “leak respiration” (**Figure**
326 **5C**), reflecting the basal O_2 consumption not coupled to ATP synthesis, thereby suggesting that in
327 RTA and in CTRL the rate of “energy” dissipated by the membrane proton leak was similar. The
328 “respiratory acceptor control ratio” (RCR), that is the ratio between state 3 respiration and leak
329 respiration, was taken as an index of coupling of mitochondrial respiration for a specific substrate
330 supply (malate, glutamate, succinate in this study). A significantly higher RCR was observed in
331 RTA vs. CTRL (**Figure 5D**), suggesting a tighter coupling between oxidation and phosphorylation
332 in RTA.

333

334 **Discussion**

335

336 The present study provides an integrative evaluation of oxidative metabolism in a group of young
337 resistance-trained athletes (RTA) characterized by a marked skeletal muscle hypertrophy.
338 Different variables of oxidative function were evaluated, spanning from pulmonary gas exchange
339 and skeletal muscle function *in vivo* to mitochondrial respiration *ex vivo* in permeabilized fibers.
340 We hypothesized, in RTA vs. control subjects (CTRL), an impaired oxidative function *in vivo* and
341 an impaired mitochondrial respiratory function *ex vivo*. The obtained results did not confirm these
342 hypotheses.

343

344 Whole body peak oxidative function was enhanced in RTA vs. CTRL. Figure 2 (left panel), in
345 which pulmonary $\dot{V}\text{O}_2$ data are expressed in L min^{-1} shows that during CE $\dot{V}\text{O}_2$ peak was indeed
346 *higher* (by ~15%) in RTA vs. CTRL, in association with a slightly higher (by ~10%) peak work
347 rate. Moreover, despite the significantly greater body mass, during CE no impairment of oxidative
348 function was seen in RTA at submaximal work rates: the efficiency and the “ O_2 cost” of exercise

349 (as indicated by the slopes and the intercepts of the $\dot{V}O_2$ vs. work rate relationships) were indeed
350 the same in the two groups. This finding is of interest, also in comparison to what is usually seen
351 in another population characterized by a significantly greater body mass, such as obese patients, in
352 which the $\dot{V}O_2$ vs. work rate relationship is shifted upward compared to that seen in normal
353 controls (22), indicating a higher O_2 cost of CE exercise deriving from the excess in body mass.

354 The situation was in part different for KE (right panel of Figure 2): the slopes of the $\dot{V}O_2$ vs.
355 submaximal work rates relationships were again similar in the two groups, but the intercept was
356 higher in RTA (suggesting a higher O_2 cost for KE exercise), and $\dot{V}O_2$ peak and peak work rate
357 values were only slightly higher in RTA. No clear-cut explanation can be given for the higher O_2
358 cost of exercise observed in RTA during KE, but not during CE. Cardiovascular constraints cannot
359 be hypothesized, since they were by definition much lower in KE vs. CE. It can be hypothesized
360 that the work of accessory muscles (see Richardson et al., 34) during KE was overall higher in
361 RTA vs. CTRL. We indeed measured pulmonary $\dot{V}O_2$ and not $\dot{V}O_2$ across the leg, and as a
362 consequence of this we cannot discriminate between $\dot{V}O_2$ attributable to the legs and $\dot{V}O_2$
363 attributable to the rest of the body.

364

365 On the other hand, after we normalized $\dot{V}O_2$ peak per whole body muscle mass (for CE) or
366 quadriceps muscle mass (for KE) values were significantly lower (by ~15-20%) in RTA vs. CTRL
367 (see Figure 3). This finding could be interpreted from two different perspectives: despite a lower
368 $\dot{V}O_2$ peak per unit muscle mass, RTA reached slightly higher (during CE) or similar (during KE)
369 peak work rate levels than CTRL, suggesting a higher muscle/metabolic efficiency (see below).

370 On the other hand, it should also be recognized that $\dot{V}O_2$ peak/ muscle mass was substantially
371 lower in RTA, suggesting a substantial impairment of peak oxidative function *in vivo* when
372 normalized for the markedly greater muscle mass. Or, to put it in other words, in RTA (vs. CTRL)
373 the increase in muscle mass was more pronounced than the increase in maximal oxidative power.

374

375 How to interpret all these findings in a reasonably coherent *scenario*? The answer may come both
376 from some literature data and from data obtained in the present study.

377 First of all, strength training may have positive effects on aerobic performance and muscle
378 oxidative metabolism. In the present study RTA had greater maximal isometric force *vs.* CTRL.
379 For the same force (and power) output, muscles with higher maximal force would need to recruit a
380 lower number of motor units, and therefore more oxidative (and more efficient) muscle fibers (20,
381 26). Previous literature data confirm that strength training may increase skeletal muscle efficiency
382 (4) and enhance skeletal muscle “metabolic stability” (50). This would also be in agreement with
383 our high-resolution respirometry data, suggesting an enhanced mitochondrial respiratory function
384 in RTA (see below).

385 On the other hand, the marked muscle hypertrophy *per se* could impair the peripheral diffusion of
386 O₂, if it is not accompanied by a proportional increase in muscle capillary supply. In the present
387 study quadriceps muscle mass and cross sectional area were ~35% greater in RTA than in CTRL.
388 It is generally assumed that the increase in muscle mass and size obtained by resistance training is
389 mainly determined by hypertrophic processes involving single muscle fibers (12). According to
390 Aagaard et al. (1), in the hypertrophic muscle the increase of CSA of individual fibers is more
391 pronounced (by ~6%) to that observed for the muscle as a whole, as a consequence of changes in
392 the pennation angle of fibers within the muscle. Thus, CSA of individual fibers in the RTA of the
393 present study could have been 40-45% greater than that of CTRL, possibly representing an
394 important impediment to muscle O₂ diffusing capacity (see below). Muscle capillary supply was
395 not determined in the present study, and literature data are not univocal. According to some
396 authors skeletal muscle hypertrophy induced by strength training could determine a capillary
397 “dilution” in the tissue (43). A lower microvascular surface area available for gas exchange and/or
398 an increased diffusion distance from the capillary to mitochondria would impair peripheral O₂

399 diffusion (46). In the present study we did not determine muscle capillarity, or peripheral O₂
400 diffusion; the latter could be determined by the invasive method developed in Dr. Wagner's
401 laboratory over the years (see *e.g.* 46). These approaches could be attempted in future studies. In
402 the hypertrophic skeletal muscles also an altered matching between O₂ delivery and O₂ utilization
403 within the muscles could lead to the lower muscle O₂ availability.

404 Evidence in favor of this phenomenon is provided, in the present study, by the observation in RTA
405 of lower fractional O₂ extraction values, both at submaximal and at peak work rates, both during
406 CE and KE (Figure 4). As nicely discussed by Poole et al. (31), it would be an oversimplification
407 to interpret fractional O₂ extraction simply as a result of "muscle factors"; indeed, this variable
408 may be affected by a combination of interrelated factors responsible for perfusive O₂ transport to
409 and within active muscles and diffusive O₂ transport within fibers. In the present study, however,
410 the lower O₂ extraction cannot be accounted by cardiovascular O₂ delivery (the impaired O₂
411 extraction was described both during CE and KE, in which, by definition, cardiovascular
412 constraints are reduced or eliminated), nor by an impaired mitochondrial respiratory function,
413 which was enhanced, at least in *ex-vivo* conditions, in RTA vs. CTRL. Thus, the "bottleneck" of
414 oxidative metabolism in RTA would reside "downstream" of bulk cardiovascular O₂ delivery, but
415 "upstream" of intracellular oxidative metabolism. The main impairment could then reside in the
416 diffusing capacity of the muscle for O₂ and/or in the intramuscular matching between O₂ delivery
417 and O₂ utilization, which could be altered as a consequence of the marked muscle hypertrophy.

418 By measures of high resolution respirometry carried out in permeabilized skeletal muscle fibers
419 (experimental conditions of unlimiting O₂ availability), we indeed observed higher values of
420 ADP-stimulated mitochondrial respiration in RTA vs. CTRL, associated with a higher degree of
421 coupling between oxidation and phosphorylation. These observations suggest an enhanced *ex vivo*
422 respiratory function in RTA. These data were obtained in the presence of a similar CS activity in
423 the two groups. Although the method has some limitations (see Leek et al., 24), the activity of the

424 enzyme is frequently utilized to estimate mitochondrial content. Thus, in the markedly
425 hypertrophic skeletal muscles of RTA mitochondrial biogenesis occurred proportionally to
426 contractile protein synthesis. The finding appears consistent with studies on molecular signaling
427 showing that the mammalian target of rapamycin (mTOR) kinase, which is known to be activated
428 by resistance training and to be involved in the signaling pathway of protein synthesis and muscle
429 growth, also regulates the expression of mitochondrial genes and may have a critical regulatory
430 role on mitochondrial biogenesis and function (38, 47). State 3 mitochondrial respiration was
431 higher in RTA vs. CTRL, whereas no differences were described between the two groups in terms
432 of leak respiration. These data suggest a tighter coupling of mitochondrial respiration and an
433 improved efficiency of the phosphorylation system in RTA. Similar findings have been observed
434 by other authors after long-term exercise training (44, 51), in association with a more efficient
435 control of mitochondrial respiration by the creatine kinase system. These adaptations are expected
436 to limit perturbations of cellular homeostasis during exercise and to delay the increased reliance
437 on substrate level phosphorylation for ATP regeneration, thus preserving exercise tolerance (51),
438 and are likely associated with the concept of muscle “metabolic stability” (49).

439 Which could be the cause(s) responsible for the improved mitochondrial respiratory function *ex*
440 *vivo* in RTA? Apart from the direct effects of training, it can be hypothesized that the impaired
441 peripheral O₂ diffusing capacity and/or the impaired matching between O₂ delivery and O₂
442 utilization, discussed above, could determine within the exercising hypertrophic muscles areas of
443 relative lack of O₂, that is of hypoxia. An improved coupling of mitochondrial respiration could
444 then result from adaptive responses of mitochondria to repeated hypoxic stimuli. In skeletal
445 muscle, a hypoxia-sensitive signal activation of transcription may occur in the myocellular
446 compartment as a direct consequence of a drop in tissue oxygenation, in order to maintain the
447 homeostasis of PO₂ at the levels considered critical for the function of cell (11). The multi-gene
448 hypoxia-inducible transcription factor (HIF)-1 is recognized as the master transcription regulator

449 of cell hypoxic signaling (39). HIF-1 drives the expression of a variety of genes involved in
450 mitochondrial metabolism in skeletal muscle under hypoxic exposure, among which those
451 controlling the efficiency of cytochrome *c* oxidase enzyme (COX) in the mitochondrial respiratory
452 chain. HIF-1 would coordinate a switch from COX4-1 subunit to COX4-2, thereby increasing the
453 efficiency of electron transfer to O₂ at complex IV, and minimizing electron leakage at complexes
454 I and III. This switch would also enhance the efficiency of ATP synthesis, by increasing proton
455 pumping into the mitochondrial intermembrane space (16). By this way, electron transfer and
456 phosphorylation would result more tightly coupled, and the efficiency of oxidative
457 phosphorylation improved.

458

459 ***Methodological considerations***

460 In the present study the values of ADP-stimulated mitochondrial respiration and maximal
461 uncoupled respiration were in the low-end of values for healthy subject's quadriceps muscle. A
462 wide range of values for mitochondrial respiratory capacity can be found in the literature (17).
463 This could be attributable to the investigated population, to intrinsic metabolic characteristics of
464 tissue samples, and to methodological procedures, such as titration protocol, sequence and
465 combination of administered substrates, [ADP], experimental temperature, wet or dry state of
466 tissue mass utilized for normalization, fresh or frozen tissue samples, etc (17). In any case, the
467 data obtained in the present study are similar to those obtained, after following substantially the
468 same protocol of the present study, in the healthy control subjects of recent studies (9, 23, 30). In
469 the present study, after adding cytochrome *c* to the measuring chamber, the increase in
470 mitochondrial respiration was very small (~2%). A small increase in respiration after adding
471 cytochrome *c* is a standard criterion to check the absence of a significant damage of the outer
472 mitochondrial membrane, possibly occurring during the preparation of samples.

473 At first sight a comparison of $\dot{V}O_2$ between the two groups at submaximal work rates may not be
474 warranted since the two groups presumably have different $\dot{V}O_2$ kinetics (slower in the resistance-
475 trained athletes), and as a consequence different rates of adjustment to the work rate increments.
476 However, as elegantly discussed in the recent review by Rossiter (35), during a standard
477 incremental test different time-constants of the $\dot{V}O_2$ kinetics do not affect the slope of the $\dot{V}O_2$
478 vs. work rate relationship, but only shift the linear relationship to the right (in case of a slower
479 $\dot{V}O_2$ kinetics) or to the left (in case of a faster $\dot{V}O_2$ kinetics), the “horizontal distance” between
480 these linear relationships being reflected by the difference in time-constants. We did not determine
481 the $\dot{V}O_2$ kinetics in the two groups of subjects of our study. However, if we assume a slower
482 $\dot{V}O_2$ kinetics in the strength-trained group, imagine a difference in time-constants of 15 seconds
483 (this is likely an exaggeration, considering that both groups had a common endurance training
484 background), and assume the same gain in the two groups (as actually observed in this study), the
485 small horizontal shifts of the $\dot{V}O_2$ vs. work rate relationships do not change data interpretation:
486 same slopes and intercepts between the two groups during CE, same slopes but higher intercepts
487 in RTA during KE, suggesting a slightly higher O_2 cost of KE exercise in this group.

488

489 ***Conclusions***

490 In a group of young resistance-trained athletes characterized by a marked skeletal muscle
491 hypertrophy, the greater muscle mass and maximal force, and the enhanced mitochondrial
492 respiratory function seem to compensate for the hypertrophy-induced impaired peripheral O_2
493 diffusion. The net results are an enhanced whole body oxidative function at peak exercise, and
494 unchanged efficiency and O_2 cost at submaximal exercise, despite the much greater muscle mass
495 and body mass.

496

497

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499

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- 635

636 **Author contributions**

637 The experiments were carried out at the Valdoltra Hospital, Ankaran, Slovenia. B.G., S.L.
638 conceived the study and obtained the financial support. All authors contributed to the design of the
639 experiments. R.P., S.L. and B.S. were responsible for the recruitment of the subjects and for the
640 logistics of the study. Data were collected and analyzed by D.S., R.D., S.P., J.R, G.R. and B.S.
641 D.S. and B.G. interpreted the data and wrote the first draft of the manuscript. All authors
642 contributed to the critical revision of the manuscript and approved its final version.

643

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TABLE 1 Anthropometric and body composition characteristics of subjects.

	RTA	CTRL
Body mass (kg)	102.6 ± 7.3*	77.8 ± 6.0
Stature (m)	1.84 ± 0.04	1.81 ± 0.05
BMI (kg·m⁻²)	30.1 ± 2.6*	23.8 ± 2.2
FFM (kg)	90.4 ± 6.1*	66.8 ± 11.0
Body muscle mass (kg)	46.1 ± 3.1*	35.2 ± 2.8
Quadriceps muscle mass (kg)	3.26 ± 0.44*	2.45 ± 0.26
Body fat (%)	12.2 ± 3.5*	9.9 ± 0.8

Data are expressed as means ± SD. RTA: resistance-trained athletes; CTRL: controls. BMI: body mass index. FFM: fat-free mass.

*: significantly different vs. CTRL ($P < 0.05$; unpaired Student's t test).

652 **TABLE 2** Peak values of investigated variables during cycle ergometer (CE) and knee-extension
 653 (KE) exercise.

	CE		KE	
	RTA	CTRL	RTA	CTRL
$\dot{V}E$ peak ($L \cdot \text{min}^{-1}$)	161.6 ± 27.5	145.9 ± 28.3	69.6 ± 18.9	62.0 ± 18.0
VT peak (L)	3.2 ± 0.5*	2.7 ± 0.3	1.8 ± 0.5	1.5 ± 0.5
fR peak ($\text{br} \cdot \text{min}^{-1}$)	51.3 ± 8.2	55.3 ± 10.0	41.2 ± 7.4	43.8 ± 6.0
$\dot{V}O_2$ peak ($L \cdot \text{min}^{-1}$)	4.05 ± 0.64*	3.56 ± 0.30	1.59 ± 0.23	1.50 ± 0.33
$\dot{V}O_2$ peak/BM ($\text{mL} \cdot \text{min}^{-1} \cdot \text{kg}^{-1}$)	39.6 ± 5.3*	45.9 ± 3.0	-	-
$\dot{V}O_2$ peak/muscle mass ($\text{mL} \cdot \text{min}^{-1} \cdot \text{kg}^{-1}$)	87.9 ± 11.7*	101.5 ± 6.7	-	-
$\dot{V}O_2$ peak/QM ($\text{mL} \cdot \text{min}^{-1} \cdot 100 \text{ g}^{-1}$)	-	-	51.5 ± 9.1*	63.7 ± 13.0
R peak	1.15 ± 0.06	1.17 ± 0.04	1.17 ± 0.14	1.13 ± 0.11
GET (% $\dot{V}O_2$ peak)	76.7 ± 3.8	73.8 ± 4.1	78.7 ± 3.6*	72.4 ± 3.9
Work rate peak (W)	314 ± 56	284 ± 15	103 ± 16	98 ± 13
Time to exhaustion (min)	15.7 ± 2.8	14.2 ± 0.7	14.3 ± 2.2	13.5 ± 1.7
HR peak ($\text{b} \cdot \text{min}^{-1}$)	184 ± 8	186 ± 11	142 ± 13	146 ± 11
\dot{Q} peak ($L \cdot \text{min}^{-1}$)	29.1 ± 3.9	27.2 ± 2.8	18.9 ± 4.5	17.9 ± 3.2
CI peak ($L \cdot \text{min}^{-1} \cdot \text{m}^{-2}$)	12.8 ± 1.6	13.7 ± 1.4	8.3 ± 1.9	9.1 ± 1.4

Data are expressed as means ± SD. RTA: resistance-trained athletes; CTRL: controls. $\dot{V}E$: pulmonary ventilation. VT: tidal volume. fR: respiratory frequency $\dot{V}O_2$ /BM: oxygen uptake per unit of body mass. $\dot{V}O_2$ /muscle mass: oxygen uptake per unit of whole body muscle mass. R: gas exchange ratio. GET: gas exchange threshold. HR: heart rate. \dot{Q} : cardiac output. CI: cardiac index. See text for further details.

*: Significantly different vs. CTRL ($P < 0.05$; unpaired Student's t test).

Figure captions

654 **Figure 1 (A)** Anatomical cross-sectional area (CSA) of the quadriceps muscle, obtained by
655 magnetic resonance imaging at 50% femur length, and (B) quadriceps muscle volume in resistance
656 trained athletes (RTA) and control subjects (CTRL). Mean (\pm SD) values are shown. *: $P < 0.05$ vs.
657 CTRL. See text for further details.

658

659 **Figure 2** Mean (\pm SD) $\dot{V}O_2$ values during CE (A) and KE (B) are plotted as a function of mean
660 (\pm SD) work rate (Watt) for resistance-trained athletes (RTA) and control subjects (CTRL).
661 Individual $\dot{V}O_2$ values were grouped for discrete work rate intervals. As for CE, the mean (\pm SD)
662 values of the slopes of the individual regression lines were 10.6 ± 0.9 mL min^{-1} watt^{-1} in RTA and
663 10.3 ± 0.7 in CTRL (n.s.); the mean values of the intercepts were 652 ± 96 mL min^{-1} in RTA and
664 613 ± 83 in CTRL (n.s.). As for KE, the mean values of the slopes of the individual regression lines
665 (submaximal work rates) were 9.5 ± 1.1 mL min^{-1} watt^{-1} in RTA and 9.7 ± 1.9 in CTRL (n.s.); the
666 mean values of the intercepts were 545 ± 71 mL min^{-1} in RTA and 421 ± 81 in CTRL ($P < 0.05$). *: $P < 0.05$
667 vs. CTRL. See text for further details.

668

669 **Figure 3** Peak $\dot{V}O_2$ values normalized for whole body muscle mass during CE (A) or quadriceps
670 muscle mass during KE (B), in resistance-trained athletes (RTA) vs. controls (CTRL). *: $P < 0.05$
671 vs. CTRL.

672

673 **Figure 4** Mean (\pm SD) values of the NIRS-obtained muscle deoxygenation index
674 ($\Delta[\text{deoxy(Hb+Mb)}]$), which estimates *vastus lateralis* fractional O_2 extraction, as a function of
675 work rate, during CE (A), and KE (B), in resistance trained athletes (RTA) vs. controls (CTRL).
676 $\Delta[\text{deoxy(Hb+Mb)}]$ data are expressed as a percentage of values obtained during a transient limb

677 ischemia at the end of the test. The sigmoid functions (see 14) fitting the data are also shown. *:
678 $P < 0.05$ vs. CTRL (Student's t test with Bonferroni correction). See text for further details.

679

680 **Figure 5 (A)** Mean (\pm SD) values of mitochondrial state 3 respiration (with glutamate, malate, and
681 succinate as substrates) per unit tissue mass (wet weight) measured in permeabilized muscle
682 fibers, and **(B)** citrate synthase activity (in $\mu\text{mol}\cdot\text{min}^{-1}\cdot\text{g}^{-1}$ protein), in resistance trained athletes
683 (RTA) and controls (CTRL). **(C)** Mean (\pm SD) values of leak respiration (respiratory rate in the
684 presence of substrates without ADP), and **(D)** respiratory acceptor control ratio (RCR, state 3
685 respiration/ leak respiration), denoting the degree of coupling of mitochondrial respiration, in RTA
686 and CTRL. *: $P < 0.05$ vs. CTRL. See text for further details.

Figure 1

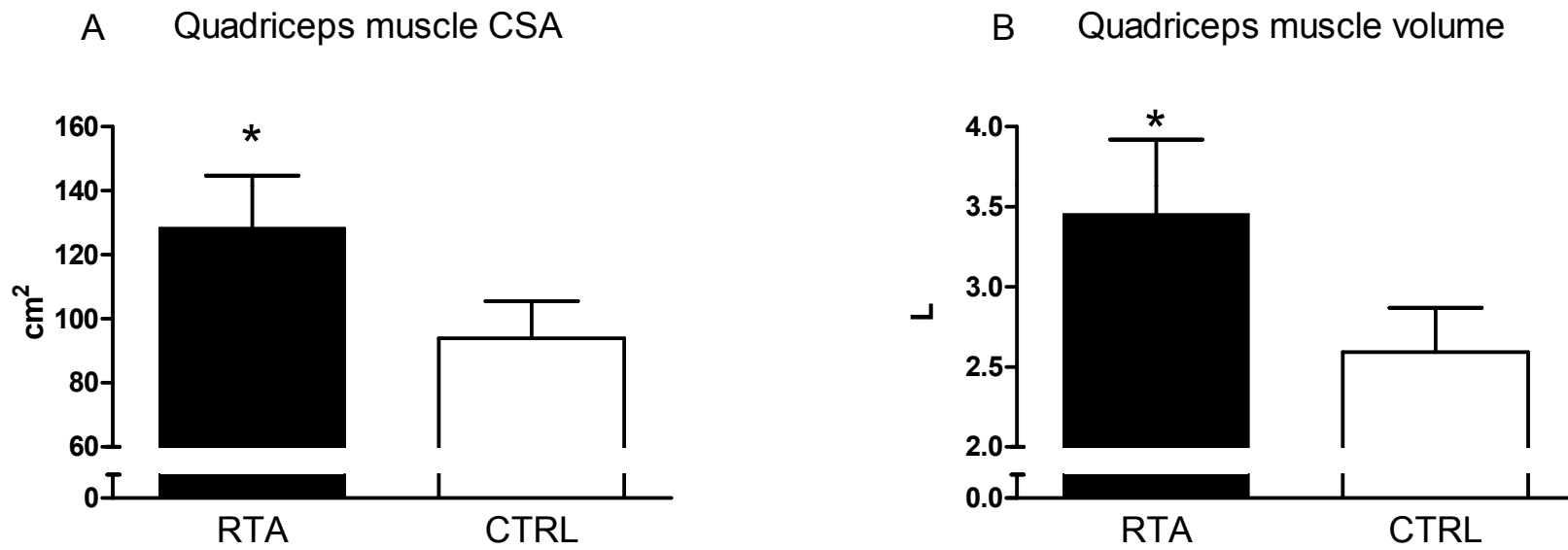


Figure 2

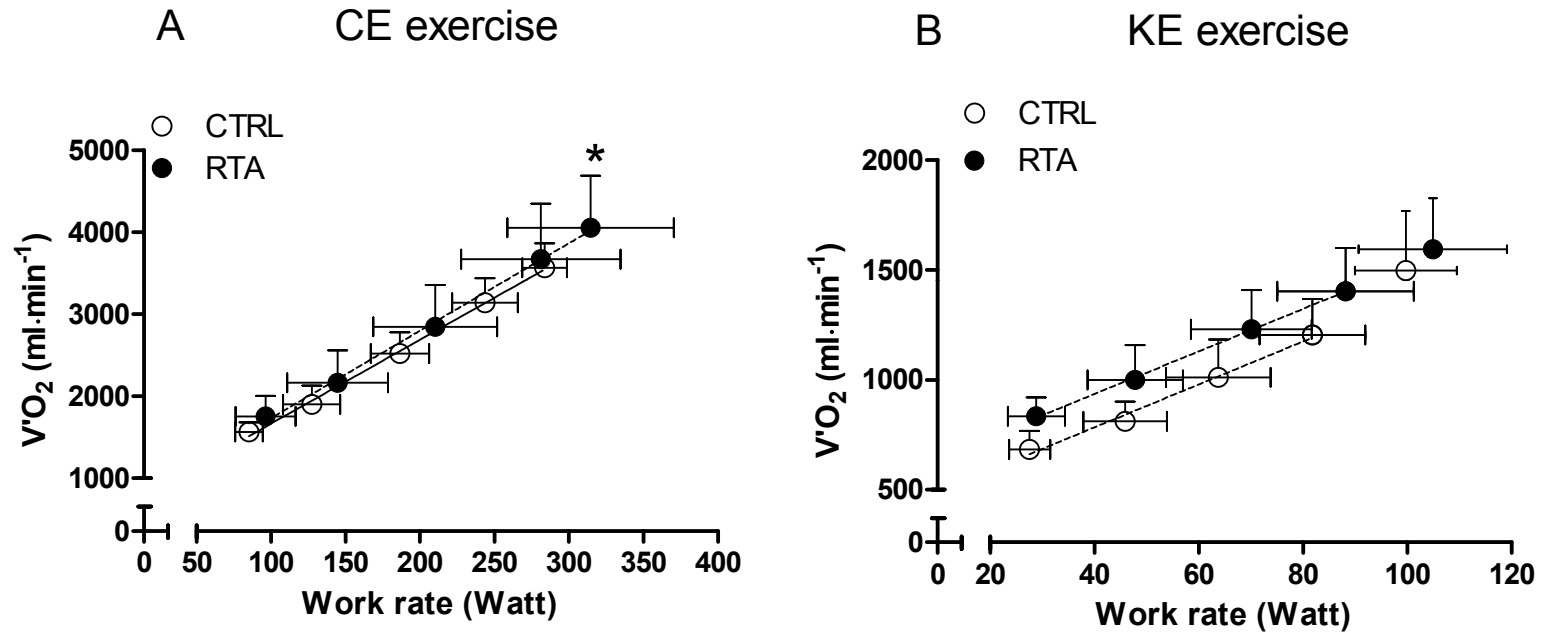


Figure 3

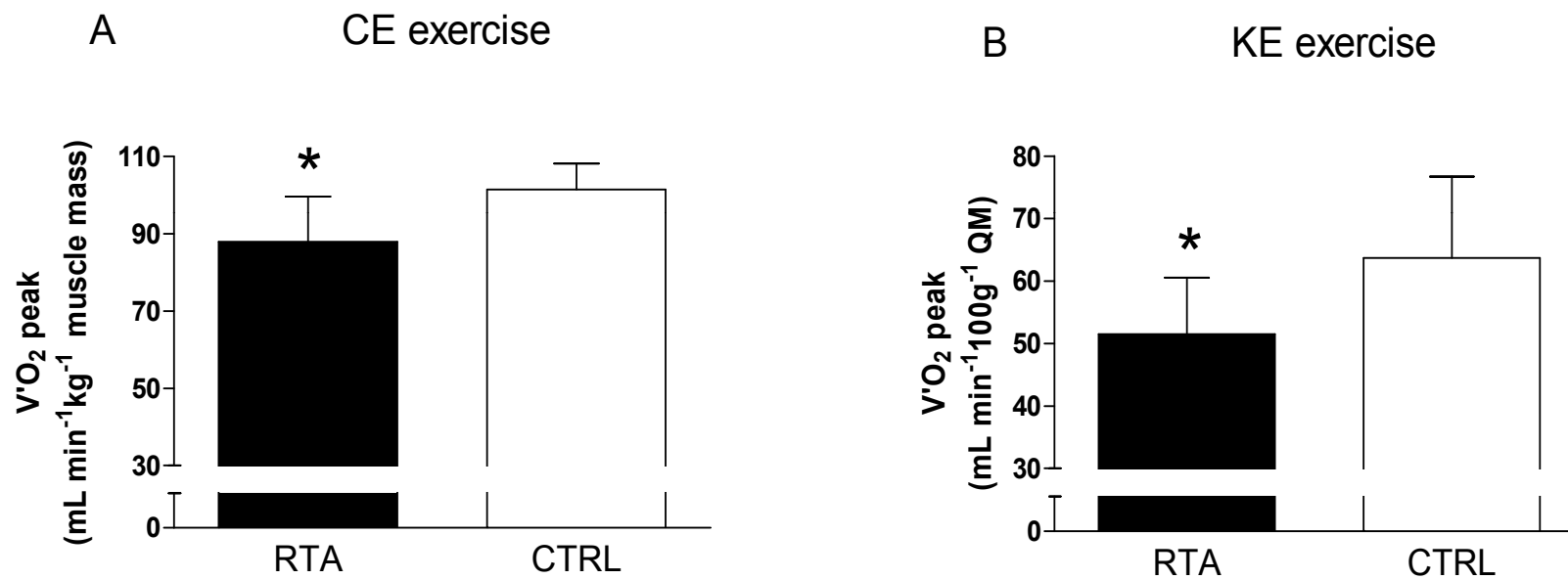


Figure 4

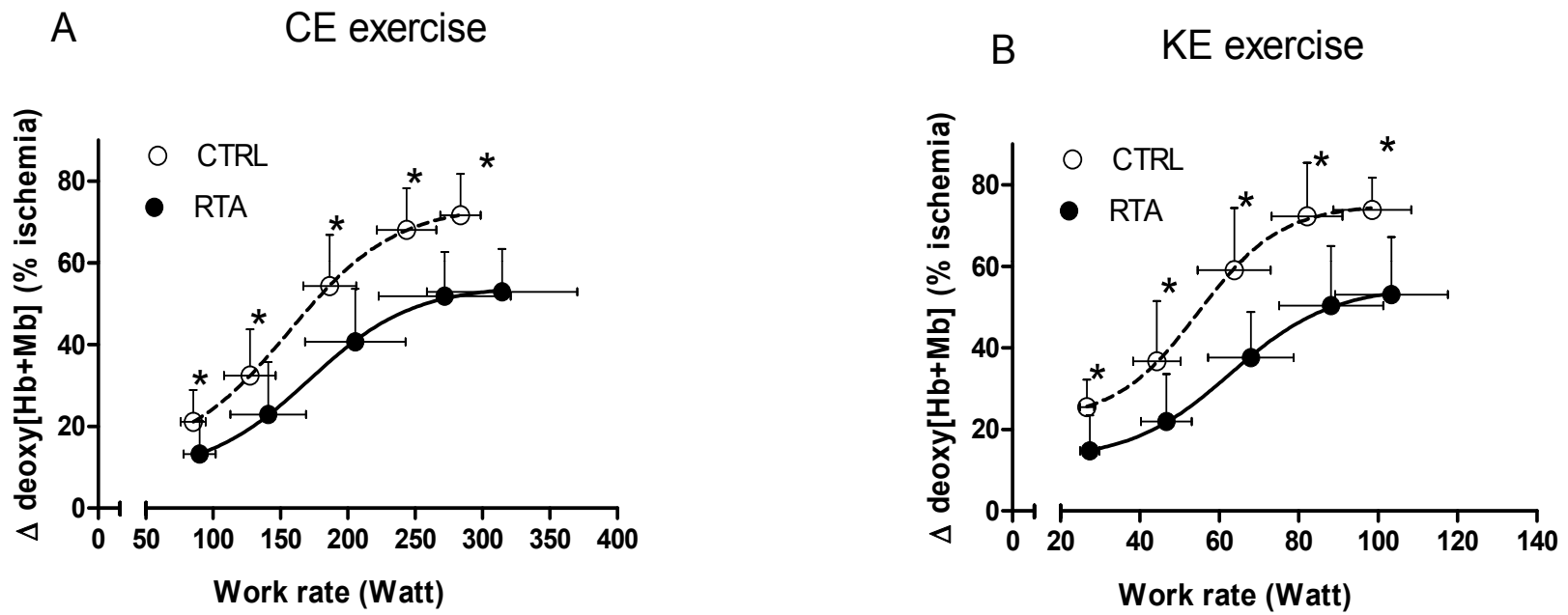


Figure 5

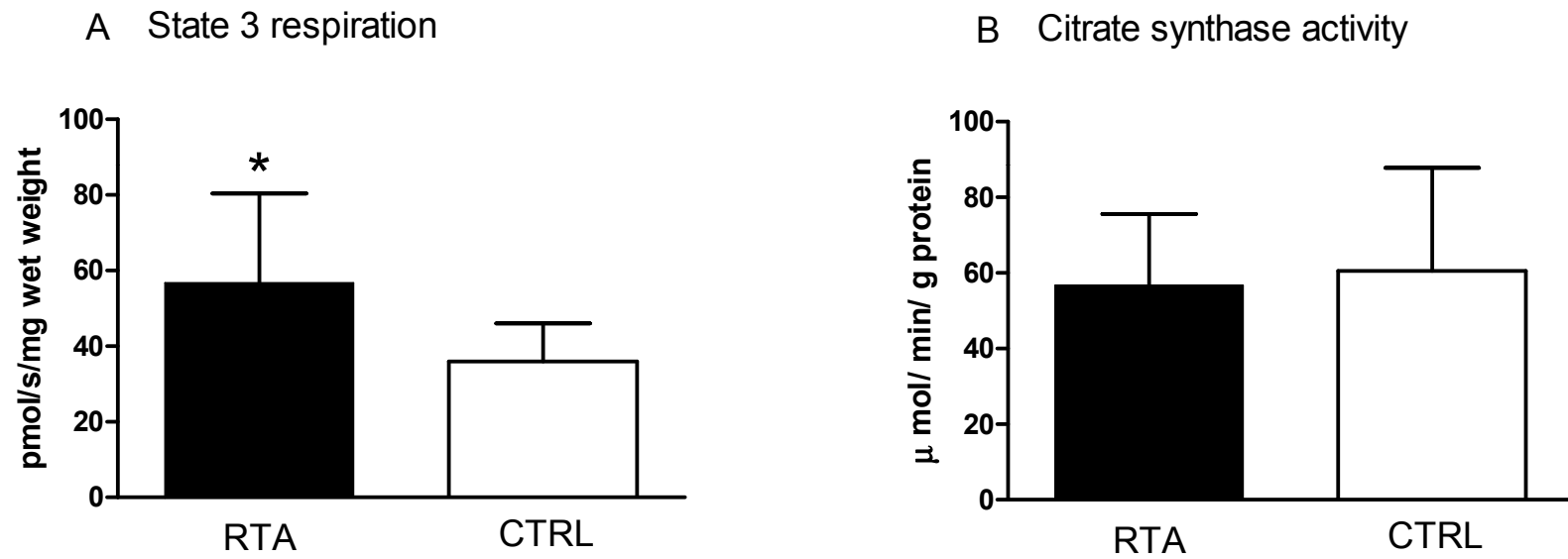


Figure 5

