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Detection and staging of solid tumors with FDG-PET and FLT-PET

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Detection and staging of solid tumors with FDG-PET and FLT-PET



David C.P. Cobben

Detection and staging of solid tumors with FDG-PET and FLT-PET

David Catharina Petrus Cobben

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Cover: FDG-PET (left) and FLT-PET scan of a patient with metastatic non-small cell lung cancer

Ponsen & Looijen, Wageningen, The Netherlands © 2004 D.C.P. Cobben

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Stellingen

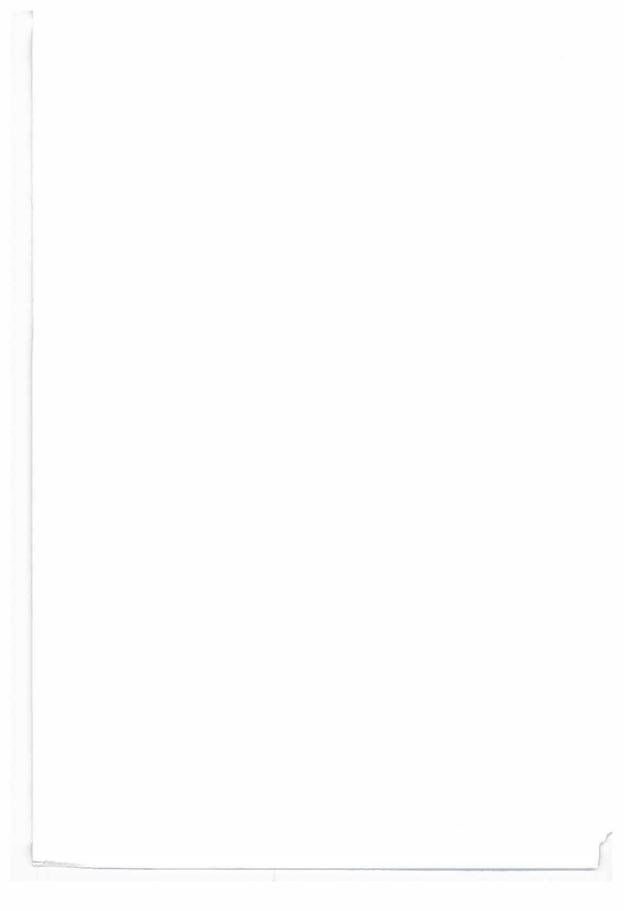
behorende bij het proefschrift

'Detection and staging of solid tumors with FDG-PET and FLT-PET'

- 1. FLT-PET meet de celproliferatie indirect.
- 2. De toekomst van FLT-PET ligt eerder op het gebied van de therapie-evaluatie dan op het gebied van tumordetectie en stadiëring.
- 3. De berekeningsmethode is het enige gestandaardiseerde aan de Standardized Uptake Value (SUV).
- 4. Vergelijking van "PET-data" wordt vaak bemoeilijkt door de summiere omschrijving van de methodologie in publicaties.
- 5. De ontwikkeling van de medische praktijk is een zaak van lange adem; PET en de ontwikkeling van diverse toepasbare tracers zijn hiervan voorbeelden.
- 6. De resectie-marge van het melanoom is nog steeds omstreden.
- 7. Na kinderen en ouderen met kanker, verdienen nu de adolescenten aandacht.
- 8. De epidemische toename van overgewicht lijkt gepaard te gaan met een endemische behoefte aan bariatrische chirurgie.
- 9. Er is een toenemende behoefte aan "novel food".
- 10. "Het zou misschien kunnen dat machines beslissen, maar we hebben nog steeds de dokter nodig om te helen". (Atul Gawande, 2002)
- 11. In de toekomst is het niet ondenkbaar dat de patiënt eerst informeert naar het aantal "Nintendo-uren" van de chirurg, alvorens enige vorm van "sleutelgatchirurgie" te willen ondergaan. (James Rosser, 2004)

David C. P. Cobben

Groningen, 12 mei 2004



Rijksuniversiteit Groningen

Detection and staging of solid tumors with FDG-PET and FLT-PET

Proefschrift

ter verkrijging van het doctoraat in de Medische Wetenschappen aan de Rijksuniversiteit Groningen op gezag van de Rector Magnificus, dr. F. Zwarts, in het openbaar te verdedigen op woensdag 12 mei 2004 om 13.15 uur

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Chapter 1

Introduction

The number of patients diagnosed with cancer is still increasing. In the Netherlands, approximately 328.000 new cancer patients are expected yearly and approximately 184.000 cancer patients die of their disease.¹ One of the most important causes is the proportional increase of the aging population. While accuracy and the impact of many novel diagnostic tools on survival of cancer patients are still under investigation, other new diagnostic tools are already being implemented and developed. The TNM-staging system, which is the universal approach for diagnostic tools. This approach will be discussed and used to explain some of the major technological advances in the diagnosis and staging of cancer. Positron Emission Tomography, which is one of these technological advances, will be discussed in detail.

TNM staging of cancer

Anti-cancer treatment depends on histological diagnosis and staging system of the anatomical site, size and extent of the tumor and presence of lymphatic and/or haematogenic metastases. The TNM-staging system is the universal staging method for all kinds of malignancies, which has been developed and updated since 1943 by international cancer societies. The goal of the TNM-staging system is to serve as a 'common language' for oncologists. The TNM-staging does not only stage cancer patients, but can also help with treatment planning, give an indication of prognosis, assist in treatment evaluation, facilitate exchange of information between treatment centers and contribute to the continuing investigation of human cancer.

The TNM-staging system consists of 3 levels. The Tumor stage, stands for the local progression of the tumor, Nodal stage for regional metastasis in the lymph node and the M stage for distant metastasis. Local progression of the tumor is expressed in numbers or as '*is*'. T_{is} stands for 'carcinoma in situ' and T₁, T₂, T₃ or T₄, express the increasing local progression of the tumor. In the same fashion does N₀, stand for no presence of regional lymphatic metastasis and N₁, N₂ and N₃ for progression of regional lymphatic metastasis. M₀ stands for no haematogenic metastasis present and M₁ for presence of haematogenic metastasis. The application of the TNM system in the clinical practice and the value of several diagnostic techniques will be discussed in the next paragraphs.

Clinical pathological staging

The clinical pathological staging of cancer is improving with the development of techniques such as immunohistochemistry (IHC) using antibodies and reverse transcriptase polymerase chain reaction (RT-PCR) for the sensitive detection of malignant cells in the pathological diagnosis of cancer. Computed tomography (CT), magnetic resonance imaging (MRI), ultrasonography (US) and positron emission tomograpy (PET) play a role in the anatomical or functional detection of tumors. However, all these techniques have their limitations. Fine needle aspiration can often distinguish between a benign and malignant process. To obtain a final histopathological diagnosis, a biopsy or an excision of the tumor is required. The pathologist will examine the specimen on several parameters, e.g. resemblance with normal tissue, number of mitotic figures, amount of necrosis and additional specific tissue or cell staining. The results of these examinations are histological specification and differentiation. The difficulty of obtaining a tissue biopsy of a tumor is the sampling error, especially in a non-palpable lesion. In addition the biopsy may not always be representative for the whole tumor regarding malignancy and proliferation activity, because many large tumors are heterogeneous with regard to proliferation activity and contain area(s) of necrosis.

Tumor extent

CT, MRI, US and surgery (e.g. laparotomy, laparoscopy and/or endoscopy) are used to investigate the extent of the tumor into the surrounding tissues. The difficulty of CT, MRI and US is that they play a very modest role in discriminating between malignant and normal tissue, especially in tumors that are highly differentiated and/or with a low proliferation grade. Furthermore, the detection of a recurrent malignancy on MRI and CT after previous cancer treatment is difficult, due to the tissue changes after surgery, radiation therapy and/or chemotherapy. These tissues changes are mostly caused by fibrosis, which can mimic or enclose malignant tissue. Surgery is in general a too invasive procedure to investigate the extent of the tumor prior to therapy.

Lymphatic metastases

CT, MRI, US and the sentinel lymph node (SLN) procedure can be used for the detection of lymphatic metastases. The method of choice, depends on the location of the primary tumor and location of the expected lymphatic metastases. The diagnosis of lymphatic metastases by MRI, CT and US depends mainly on the detection of enlarged lymph nodes. MRI, CT or US categorize lymph nodes larger than 1 cm as suspect for malignancy. However, enlarged lymph nodes can be reactive without containing metastatic cells and non-enlarged (< 1 cm) lymph nodes can contain metastatic cells. With respect to the last, it is interesting to mention new developments with lymph targeted MRI contrast agents, which may detect very small lymph node metastases.²

The advantage of the SLN technique is that it can detect the first echelon lymph node, which is thoroughly investigated by the pathologist with haematoxylin and eosin (HE) staining and if necessary, immunohistochemical (IHC) staining. However, the only indication for the sentinel node procedure is currently, limited and clinical node negative breast cancer. In the Netherlands, the clinical applications for melanomas, vulvar and cervical cancer, resectable non-small cell lung cancer, renal cell carcinoma and rhabdomyosarcoma, are still under investigation. The concept of the SLN represents a major opportunity to stratify patients for appropriate treatment, since the status of the SLN has been incorporated in the TNM classification of breast cancer and of melanoma. In short³, blue dye or [^{99m}Tc]-nano-colloid is injected intradermally (melanoma) or around the tumor or intradermally above the tumor (breast cancer) and taken up by the lymphatic system and transported to the lymph nodes. Scintigraphy detects [99mTc]-nano-colloid in the first draining lymph node(s) on the day prior to the surgery and its location(s) is/are marked on the skin. During surgery the draining lymph nodes may be stained blue and. when still radioactive, can be detected by the gamma probe, and is in this way indicated as "sentinel lymph node(s)" (Figure 1). The sentinel lymph node is excised and sent to the pathologist for histological and immunohistochemical analysis. When the sentinel lymph node contains malignant cells, all regional lymph nodes are excised, since these nodes have an increased risk to contain metastatic cells as well.

Figure 1. Sentinel lymph node in breast cancer



The blue dye and [^{99m}Tc]-nano-colloid are injected in the tumor and drain to the first lymph node: "sentinel lymph node" (arrow).

Haematogenic metastases

The presence of haematogenic metastases can be established by several techniques, depending on the site of the metastasis. Liver metastases can be detected by CT, MRI or US. Metastases in the lungs can be detected by conventional X-ray or CT and bone metastasis by [^{99m}Tc]-technetium-phosphate scintigraphy, conventional X-ray, CT and MRI. A drawback is that each site requires its own optimal technique(s) for detection of haematogenic metastases. In cancer patients disseminated tumor cells in the blood and bone marrow can often be detected by highly sensitive techniques such as RT-PCR. The presence (of subtypes) of these cells can be an indication for the prognosis. However, more studies with larger patient groups and the same design are needed, before the presence of metastatic cells in the blood and bone marrow can be incorporated in a staging system such as the TNM-staging system.

Restaging and therapy evaluation

Restaging of cancer patients and therapy monitoring, is solely based on a decrease in tumor size, which is not always feasible or quantifiable. US, CT and MRI are used to estimate the tumor response, based on change in tumor size. However, decrease in tumor size does not have to occur directly after treatment. Often a delay between response and tumor shrinkage can be seen. Furthermore, the size of tumor, increased or decreased, does not correlate with the presence or the amount of viable cancer cells. During and even after therapy tumors can consist of fibrosis, necrosis and/or viable cancer cells, which can differ in proliferation activity.

Developments in diagnostic tools

Because of the limitations of the current diagnostics for cancer, technological advances have led to new and improved diagnostic methods for staging cancer during the last decade. Especially the SLN biopsy and advanced radiodiagnostic imaging methods are recent developments in clinical oncology. The SLN procedure has been established as a reliable method for detection of lymphatic metastases in breast cancer and has reached the last investigational phase in melanoma. Functional imaging, such as functional CT, functional MRI, magnetic resonance spectroscopy, functional US and positron emission tomography (PET) are major recent advances in oncology.⁴⁻⁹ Functional CT, MRI and US focus on the quantification and alteration in the tumor vascularity. These techniques measure the behavior of specific and non-specific contrast agents in time in the tumor and may contribute in lesion characterization, tumor grading, predicting and monitoring of the response in radiation and chemotherapy, determine tumor prognosis and direct the optimal site for biopsy. However, today these techniques are not yet available in most clinical surroundings and are used mainly as a research tool.

Another functional imaging technique, Positron Emission Tomography (PET), has been investigated extensively in the last decades. PET has proven to be useful in diagnosing and staging of several cancers and is used increasingly in clinical oncology.

In general, the goal of all the individual and combined staging techniques is to provide an accurate diagnosis and TNM stage for the cancer patient for individually tailored cancer treatment.

Positron Emission Tomography

Positron Emission Tomography uses positron emitting radionuclides, which are incorporated into compounds that take part in physiological processes (tracers). Positron emitting radionuclides are generally produced by bombarding target materials with highly accelerated particles (deuterons or protons), using a cyclotron. The most frequently used radionuclides are carbon-11 (¹¹C), nitrogen-13, (¹³N), oxygen-15 (¹⁵O) and fluorine-18 (¹⁸F), which possess short physical half-lives (2-110 min.). These radioactive products can be used for the synthesis of radiolabeled tracers.

PET radionuclides have a surplus of positively charged particles in their nucleus (protons). To achieve stability within the nucleus, a positron is emitted. After travelling a small distance through the body, the positron encounters an electron and 'annihilates'.

During this process, the mass of these two photons is converted into energy ($E=mc^2$). This energy is liberated as two photons, each charged with 511 keV of energy, which emit under an angle of nearly 180 degrees.

The PET camera, which mostly consists of a full ring of detectors, registers only the simultaneously detected two photons (within 10 nanoseconds) on two opposite detectors. This is also known as coincidence detection. The camera is able to register the radiation in different angles, allowing establishment of the underlying distribution of radioactivity. When a radiopharmaceutical is administered (intravenously, orally or via inhalation) to a patient lying in the camera, the distribution of radioactivity within the field of view can be monitored in time, also known as a dynamic scan. By moving the bed, the whole body of the patient can be scanned to make a static "whole body" scan, which is used for tumor and metastases detection.

The PET imaging method has technical limitations. The resolution of the current generation of PET-cameras is 4-5 mm and is therefore unable to detect small tumors and micrometastases as is possible with the sentinel lymph node procedure.^{10,11} Moreover partial volume effects, influence the accuracy of the radioactivity measurement in small lesions by causing a spread of the signal over a larger area than it actually occupies. Depending on the spatial resolution of the camera the tracer accumulation can be significantly underestimated in small tumors.^{12,13}

Thus, PET visualizes metabolic processes as opposed to conventional imaging methods (CT, MRI and US), which are currently used for TNM staging and depend on structural or anatomical abnormalities.

Glucose metabolism

The most widely used PET tracer in oncology is 2-[¹⁸F]-fluoro-2-deoxy-D-glucose (FDG) and measures glucose utilization.¹⁴⁻¹⁷ FDG is a glucose analogue, that enters the cells via the same membrane transporters as glucose (Figure 2). Glucose as well as FDG are phosphorylated by the enzyme hexokinase. In contrast to glucose-6-phosphate, FDG-6-phospate is not a substrate for further metabolism in the glycolytic pathway. Therefore FDG-6-phosphate is trapped in the cells, in proportion to their glycolytic activity.

The indications for the use of FDG-PET in oncology are e.g. the diagnosis of pulmonary nodules, staging of lung cancer, end of treatment evaluation in lymphoma and

restaging of a suspected relapse of colon cancer.^{9,18} Furthermore, FDG-PET seems promising for staging stage III, IV and recurrent melanoma.¹⁹⁻²¹

FDG is not a tumor-specific tracer. It is also physiologically taken up in the heart and the brain and is excreted through the urinary system. The physiological uptake in the brain makes detection and interpretation of brain tumors difficult, while physiological uptake in the heart and urinary system makes the interpretation of lesions inside or in the vicinity of these organs difficult as well. High physiological FDG uptake, causing false positive results, can be seen in muscle tissue, macrophages and other cells in (local) inflammatory processes or activated after chemotherapy or radiation therapy. Decreased uptake can cause false negative results in hyperglycemic patients.^{9,10,22}

Therefore, there is a need for more specific tracers. Most research has been focused on the applicability of amino acid tracers and of pyrimidine analogues such as thymidine, which have the potential to be more specific. Besides these approaches several tracers, based on other molecular uptake mechanisms related to cancer, have been synthesized and evaluated. Examples are listed in Table 1. Some of these approaches are still in a preclinical phase, others have been investigated in small groups of patients.

Figure 2. Trapping principles of FDG and FLT

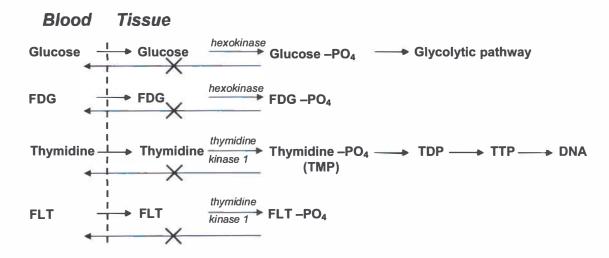


Table 1. Tracers and uptake mechanisms

| Tracer | Uptake Mechanism |
|---|--------------------------------|
| [¹⁸ F]-FDG ¹⁸ , [¹¹ C]-glucose ²³ | Glucose consumption |
| [¹⁸ F]-Fluoroethyltyrosine ²⁴ , [¹¹ C]-tyrosine ²⁵ , [¹¹ C]-methionine ²⁶ | Protein synthesis |
| [¹¹ C]-thymidine ²⁷ , [¹⁸ F]-Fluorouracil ²⁸ , [¹⁸ F]-Fluorothymidine ²⁹ | DNA-synthesis |
| [¹¹ C]-Choline ³⁰ , [¹⁸ F]-Fluoroethylcholine ³¹ | Membrane synthesis |
| [¹⁸ F]-Fluoromisonidazole ³² | Oxygenation |
| [¹⁸ F]-octreotide ³³ , [¹⁸ F]-Fluoroestradiol ³⁴ , [¹⁸ F]-neuropeptides ³⁵ | Signal transduction |
| [¹⁸ F]-phosphonium salts ³⁶ | Membrane potential |
| [¹⁸ F]-Fluorodihydroxyphenylalanine ³⁷ | Excretion of neurotransmitters |

Protein synthesis

Protein synthesis and amino acid transport are increased in tumors.²⁶ To measure these phenomena with PET, several amino acid tracers have been developed. The radiolabeled amino acids differ with regard to the production method and pharmacokinetics in vivo. For these reasons, mainly [¹¹C]-methionine (MET) has been studied in clinical trials.²⁶ MET is transported into the tumor cell, metabolized and irreversible incorporated into proteins. Low physiological uptake of MET can be seen in the brain, somewhat higher uptake in the pituary gland, pancreas, salivary glands, lacrimal glands, bone marrow and occasionally in the myocardium. Abdominal uptake in the liver and the pancreas can be seen as well as uptake in the intestines of varying degree. Preclinical data showed that MET is a selective tracer, which correlates with proliferative activity. However, preclinical data on the applicability of MET for evaluation of chemotherapy and radiation therapy are inconsistent.³⁸⁻⁴² More in vivo data are needed to investigate the background of METuptake for evaluation of several therapies. In clinical oncology MET has been applied in head and neck cancer, lung cancer and brain tumors.⁴³⁻⁴⁹ The physiological uptake in liver and salivary glands, makes MET a less attractive tracer for the detection of liver malignancies, liver metastases or metastases of head and neck cancer. The increased uptake in the pancreas makes it difficult for the detection of pancreatic cancer. From these studies can be concluded that FDG is a slightly more accurate tracer than MET, with the exception of brain tumors.²⁶ Most studies included few patients and did not investigate the value of MET for the detection of metastases. In nearly all tumor types more research is required, in larger patient series and in well defined clinical settings.

MET and other amino acid tracers, such as ¹¹C-tyrosine, also show non-specific uptake in ischaemic brain areas, stroke, scar tissue, abscess, irradiated areas, sarcoidosis and many other benign processes.²⁶ The tumor specific nature of amino acids is probably better than for FDG, but there is room for improvement.

DNA synthesis

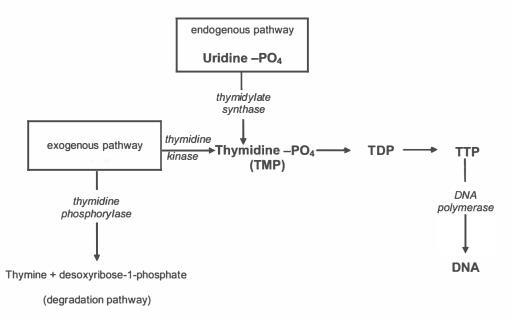
Since amino acid tracers and FDG seemed not specific enough, pyrimidine analogues, such as thymidine, were investigated. Pyrimidine analogues take part in the DNA synthesis and could therefore be more specific than the amino acid tracers. DNA is synthesized from nucleotides of four bases: cytosine, guanine, adenine and thymidine. Since thymidine is the only nucleotide that is not incorporated in the synthesis of RNA, using labeled thymidine as a substrate for growing cells, is a logical choice for specifically measuring cell proliferation. There are two pathways for the metabolism of thymidine (Figure 3). Thymidine is transported via facilitated diffusion by NBMPR-sensitive (es) and NBMPR-insensitive (is) transporters.⁵⁰ Once inside the cell, thymidine can be phosphorylated by thymidine kinase (TK), to thymidine monophosphate (TMP), followed by phosphorylation to thymidinediphosphate (TDP) and thymidinetriphosphate (TTP), prior to incorporation into the DNA. This is called the exogenous (salvage) pathway, since it allows the cell to use sources of thymidine produced elsewhere. Some of the thymidine used by cells is produced by endogenous (de novo) synthesis from uridylate. Deoxyuridine monophosphate is methylated to make TMP by thymidylate synthase (TS). Both TK and TS levels generally increase 5-10 times as cells enter the S-phase, which is the DNA synthesis phase of the cell.²⁷ Thymidine tracers take part in the exogenous pathway and are therefore dependent on the thymidine kinase concentration.

Labeled thymidine has been investigated in cell culture and animal studies for years. It seemed to be rapidly incorporated into newly synthesized DNA. [Methyl-¹¹C]-thymidine and [2-¹¹C]-thymidine have both been applied clinically in brain tumors, head and neck cancers, sarcomas, renal cancers and non-Hodgkin's lymphoma.^{51,51-59} However, [¹¹C]-thymidine is metabolized very rapidly and, depending on its labeling position, metabolites are being formed in tissue and blood. Therefore proliferation imaging with [¹¹C]-thymidine requires correction for labeled metabolites. Models have been developed for reliable estimates of cellular proliferation by measuring thymidine flux from the blood into DNA in tumors.²⁷ Because of the rapid metabolism, only a fraction of the

injected [¹¹C]-thymidine is incorporated into DNA and labeled metabolites impair image interpretation. Furthermore the short half-life of 20 min of carbon-11 and the relatively complicated production method prevents widespread use in a clinical setting. These aspects make thymidine difficult to apply as a tracer in general and in centers without a cyclotron in particular.

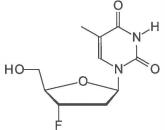
In the ongoing search for a new tracer that would not have the drawbacks of FDG, amino acid tracers and [¹¹C]-thymidine, [¹⁸F]-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT) was developed (Figure 4).²⁹





TDP=thymidine diphosphate; TTP= thymidine triphosphate

Figure 4. Chemical structure of FLT



FLT-PET

Shields et al. developed and tested FLT in canines and humans. FLT is resistant to degradation and was retained in proliferating tissues by the action of thymidine kinase 1 (TK₁), which causes phosphorylation of FLT (Figure 2 and 3). Approximately 30% of the circulating FLT is metabolized in the liver into its glucuronated form. FLT produced high-contrast images, visualizing normal bone marrow, liver and tumors. Thymidine kinase 1 (TK₁) is a principal enzyme in the DNA-salvage pathway (Figure 3) in cells,⁶⁰ and is especially upregulated just before and during the S-phase of the cell cycle.^{61,62} The TK₁ concentration increases 5-10-fold as cells enter the S-phase.⁶¹

In vitro research indicated that FLT uptake in tumor cells reflected TK₁ activity, percentage of cells in S-phase and tumor cell proliferation.⁶⁰ Little uptake of [³H]FLT (0.2%) was seen in DNA. The correlation between [³H]FLT uptake and percentage of cells in the S-phase varied between 0.76 and 0.91 and 0.86 for [³H]thymidine. Correlation between the [³H]FLT uptake and TK₁ activity was 0.63 in parental A549 (lung cancer) cells, 0.45 in A549 cells that were irradiated and 0.86 in A549 cells with abrogated p53 tumor suppressor gene.

Recently, the correlation between FLT uptake and proliferation has been investigated *in vivo* by the research groups of Buck, Veselle, Barthel and Wagner.⁶³⁻⁶⁵ The groups of Buck (n=30) and Vesselle (n=11) confirmed in patients with solitary pulmonary nodules, that FLT uptake correlated with proliferation. The correlation between SUV and proliferation fraction varied between 0.78 and 0.87. The correlation between SUV and S-phase fraction varied between 0.36 and 0.69. Wagner et al. demonstrated a strong correlation with proliferation in B-cell lymphoma in mice and patients.⁶⁴ Barthel et al. used FLT for therapy evaluation in SCID mice with fibrosarcoma. They found a strong correlation between FLT and proliferation (r=0.71) and the therapeutic effect was better to evaluate with FLT than with FDG.⁶⁵ FLT may not have the same drawbacks as FDG (increased uptake in inflammation and benign lesions and little or no uptake in cancer of hyperglycemic patients) and amino acid tracers (physiological uptake in especially abdominal organs and salivary glands), and is correlated with proliferation. FLT may therefore be an interesting tracer for the detection and therapy evaluation of cancer.

Summary

Many diagnostic techniques are used and developed to investigate the extent of the tumor and the presence of lymphatic and haematogenic metastases in cancer patients. Especially, the sentinel lymph node (SLN) technique and functional imaging techniques, such as positron emission tomography (PET) are increasingly used. The SLN technique is a standard of care for staging breast cancer and might become a staging technique for other forms of cancers such as melanoma. FDG-PET, which measures glucose metabolism and is the most widely used PET-method in oncology. However, FDG is not a tumor-specific tracer. FLT-PET, which measures DNA-synthesis, has the potential to become a more specific tracer to apply in for the diagnosis and therapy evaluation of cancer.

Aim of this thesis

To investigate the scope and limitations of FLT-PET in solid tumors. Since FLT may be a more specific tracer than FDG, the applicability of FLT-PET for differentiation between tumor inflammation, tumor detection, tumor grading and tumor staging, was investigated. In all studies FLT-PET was compared with the standard diagnostic tool for the investigated type of cancer. In cancer types where FDG-PET is used routinely, FLT-PET is compared with FDG-PET as well. In order to fulfill these objectives the following studies have been carried out:

- Review the new diagnostic techniques for the staging of melanomas: sentinel lymph node biopsy, FDG-PET and pathology from a surgical point of view (chapter 2).
- To compare FDG-PET with sentinel lymph node biopsy for staging patients with melanoma (chapter 3).
- To investigate the value of FLT-PET for the detection of metastatic melanoma and staging melanoma patients with metastases (chapter 4).
- To investigate if FLT-PET can differentiate between cancer and inflammation in a rat model in comparison to FDG-PET (chapter 5).
- To study the correlation between FLT uptake and proliferation activity of low and high grade soft tissue sarcomas (chapter 6).
- To compare the value of FLT-PET with FDG-PET, CT and histopathology for the detection of primary and recurrent laryngeal cancer (chapter 7).

- To explore the value of FLT-PET with FDG-PET for staging patients with non-small cell lung cancer (NSCLC) (chapter 8).
- To summarize and describe the future perspectives of FLT-PET (chapter 9).

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Chapter 2

New Diagnostic techniques in staging in the surgical treatment of cutaneous malignant melanoma

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Summary

The emphasis of the research on the surgical treatment of melanoma has been on the resection margins, the role of elective lymph node dissection in high risk patients and the value of adjuvant regional treatment with hyperthermic isolated lymph perfusion with melphalan. Parallel to this research, new diagnostic techniques, such as Positron Emission Tomography and the introduction of the sentinel lymph node biopsy with advanced laboratory methods such as immuno-histochemical markers, and reverse transcriptase polymerase chain reaction, have been developed to facilitate early detection of metastatic melanoma. The role of these new techniques on the staging and surgical treatment of melanoma is discussed in this paper.

Introduction

The incidence of cutaneous malignant melanoma (CMM) in the Netherlands is 14 per 100.000, as compared to an incidence of approximately 33 in the United States, and is increasing approximately 5% per year.^{1.2} There have been changes in the distribution with regard to anatomic location, histology, race, socio-economic status and stage of CMM at diagnosis during the past decade, with an increase in thinner lesions, which have a more favourable outcome.²⁻⁴ The main problem in the surgical treatment of melanoma is the high tendency for recurrence local, regional or distant. The impact of surgical wounding and wound healing of melanoma with respect to tumour development and metastatic outgrowth is still unknown.⁵

During the last two decades extensive research has been performed on the surgical treatment of melanoma, with the focus on the extent of resection margins⁶⁻¹², the role of elective lymph node dissection in high risk melanoma patients¹³⁻¹⁶, and the value of adjuvant regional treatment with hyperthermic isolated limb perfusion (HILP) with melphalan.¹⁷⁻²³

New diagnostic techniques for the detection of melanoma and its metastases, such as Positron Emission Tomography (PET), as well as the sentinel lymph node (SLN) biopsy, with or without new laboratory methods such as immuno-histochemical (IHC) markers, and reverse transcriptase polymerase chain reaction (RT-PCR), made their introduction into the clinic. Their impact on the current surgical treatment of melanoma and their current status for the general surgical practice are reviewed and discussed in this paper.

Sentinel Lymph Node (SLN) Biopsy

Recently Morton et al defined that the first drainage lymph node from the primary tumour site and the first site of any nodal metastases, is the blue stained sentinel node, based on a standardised approach for the intra-operative lymphatic mapping with Tc-99m sulphur colloid and patent blue dye.²⁴

The concept of the sentinel lymph node represents a major opportunity to stratify patients for appropriate surgery in cancer and is explained in detail by Keshtgar et al and by Nieweg et al.^{25,26} In short, blue dye or 99mTc-nano-colloid is injected in or around the tumour or subdermally above the tumour and taken up by the lymphatic system and transported to the lymph nodes.^{27,28} Scintigraphy detects 99mTc-nano-colloid in the first

draining lymph node(s) on the day prior to the surgery and its location is/are marked on the skin (Figure 1).

During surgery the draining lymph nodes may be stained blue and when radioactive can be detected by the gamma probe, and indicated as "sentinel lymph node(s)". The sentinel node is excised and sent to the pathologist for histological and immunohistochemical analysis. The gamma probe together with patent blue dye can identify more SLNs (99.5%) than lymphatic mapping with patent blue dye alone (84%).²⁹ Because of the limited sensitivity (38%), frozen section analysis, is generally not performed from the SLN, since adequate histological analysis can be performed with HE and additional immunohistochemical staining only.³⁰⁻³² The accuracy of the SLN biopsy technique is increased if a more detailed and specific histopathological analysis of the SLN specimen is performed, using evaluation of multiple serial sections with hematoxylin and eosin (H&E), as well as IHC using antibodies detecting melanocytic antigens (S-100 and anti-HMB-45 proteins). In addition the SLN specimen may be evaluated using RT-PCR detecting mRNA for amongst others MART-1 and tyrosinase. This will be discussed more in detail in the paragraph on pathology.



Figure 1. (A) Posterior image 5 min after intradermal injection of Tc99m-nanocolloid around a melanoma scar, located on the lower back, showing tracer transport from the injection site through two lymph vessels to the left, and one to the right. (B) Anterior image of the same patient with body contours, obtained 2 hrs later, showing the injection site shining through from the back, and multiple sentinel nodes in both groins.

Accurate sentinel lymph node mapping requires close co-ordination and communication between surgeons, nuclear medicine physicians, and pathologists. Most institutions have established guidelines for the safe use of radioactive materials during localisation and resection of the SLN. Meticulously performed scintigraphy is essential to ensure correct imaging of the SLN.

The results of clinical research confirm the high accuracy and good clinical applicability of the SLN concept. In a study of Berman et al, all metastases were found in regional nodal basins, which were visualised by lymphoscintigraphy.³³ This was confirmed in a multicenter trial, in which the accuracy of lymphatic mapping and sentinel lymphadenectomy with blue dye and radiocoloid was 99.1%.³¹ Studies world-wide have confirmed the validity of the SLN concept, the accuracy of the SLN biopsy as a staging procedure, the biologic significance and therapeutic considerations. Most investigators report a high success rate for identification of the SLN (96-99,5%).^{28,29,31,34} The SLN concept, a minimal invasive surgical procedure allows to determine the nodal status accurately without the morbidity associated with lymphadenectomy. When applied in stage I and II patients, approximately 20% will have positive SLNs, similar to what would be expected after elective lymph node dissection (ELND).^{16,28,35} Regional nodal recurrence of early stage melanoma is rare when the SLN is negative. Therefore the SLN biopsy is an alternative to routine ELND or "watch and wait" policy.36-38 The importance of the prognostic role of a positive lymph node has been underlined and incorporated in the completely revised staging system for CMM.³⁹⁻⁴¹ Intra-operative SLN mapping and SLN biopsy is a cost-effective procedure, that allows an accurate identification of regional lymph nodes that contain metastatic disease.⁴²

Anatomical location and previous wide local excision (WLE), in which the defect was covered by flap rotation, influence the predictability of the lymph drainage pattern. Melanomas located on the lower and upper limb drain to a predictable area, the inguinal groin or the axilla, while those located at the proximal trunk, head and neck area often drain contralaterally and to unpredictable areas, such as internal mammary, para-aortic, chest wall lymph nodes, triangular intermuscular space and often to more than one lymphatic basin.⁴³⁻⁴⁶ Previous WLE of the melanoma does not appear to negate the reliability of the SLN biopsy, provided that no flap rotation was used to cover the defect.⁴⁷

In case of a negative SLN, close attention should be paid to all blue lymph nodes and lymph nodes with a low radioactivity. In a substudy of the Sunbelt trial an analysis was performed to determine the frequency of metastatic disease in less radioactive lymph nodes, when the most radioactive or "hottest" node did not contain metastatic disease, in order to determine which sentinel nodes should be removed. If only the most radioactive of all sentinel nodes in each basin would have been removed, 13.1% of the nodes would still contain micrometastases. However, it appeared that when all sentinel nodes, with a radioactivity level greater than 10% of the ex vivo count of the most radioactive node, were removed, no positive nodes were missed. Therefore it is recommended that all such nodes and all blue nodes should be removed.⁴⁸ Interval nodes are sentinel nodes in an unexpected node field between the primary lesion and the usual regional basin. These nodes have the same chance of harbouring micrometastatic disease as a sentinel node in this usual node field.^{49,50}

The status of the SLN is the best predictor of recurrence and therefore of utmost importance for the prognosis and treatment planning. A study of 565 patients with melanoma and identified SLN, unequivocally demonstrated that the disease free survival rates of the 85 patients with positive sentinel nodes were significantly worse than in the group of 480 patients with negative sentinel nodes.³⁵ Besides the detection of positive lymph nodes by ELND, even more and unexpected lymph nodes can be detected by SLNB. In fact in multivariant analysis, SLN status is the strongest predictor of recurrence. Therefore a positive SLN biopsy identifies patients most likely to benefit from therapeutic lymph-node dissection and adjuvant therapy. These are patients with nodal metastases.

The role of SLN mapping in the surgical treatment is currently further investigated in two major multi-institutional prospective trials. In the first study the SLN concept is studied. In a prospective randomised trial, consisting of wide local excision of the primary melanoma versus wide local excision and SLN biopsy, the therapeutic value of lymph node dissection in clinical node negative patients is investigated.⁵¹ The objective of the study is to determine if this surgical strategy can prolong the disease free and overall survival of melanoma patients. The value of regional lymphadenectomy and adjuvant interferon alfa-2b therapy in clinical node negative patients with occult nodal metastasis, detected by SLN biopsy, is being studied in the Sunbelt Melanoma Trial.⁵² Results of both studies are still pending.

The impact of the SLN on the final treatment and survival of melanoma patients is unknown and reason for controversy. Although in 20-25% of the patients nodal involvement is found and the patients therefore are upstaged, in 75% of the patients, undergoing this invasive procedure, the stage remained unchanged. One of the arguments of Thomas and Patocskai, who stated that SLNB should be confined to patients in clinical trails, is that there is no postsurgical treatment, which prolongs survival.⁵³ The arguments in favour of SLNB are described by McMasters et al.⁵⁴ One of the arguments is, that SLNB identifies patients eligible for adjuvant therapy with interferon alpha-2b. There is still some

controversy about the effect of interferon alpha-2b on survival.⁵⁵⁻⁵⁸ Therefore it is our belief that trials of patients to be treated with interferon alpha-2b and other novel agents, should continue to be based on a positive sentinel lymph node.

Positron Emission Tomography (PET)

Nearly together with the introduction of the sentinel lymph node concept, PET has emerged as another clinical modality to study staging, restaging and therapy monitoring of melanoma patients. Its high sensitivity and specificity may add to patient management, perhaps more than clinical examination and techniques that depict anatomy, such as computed tomography (CT), magnetic resonance imaging (MRI) and ultrasound. Clinical examination and techniques that depict anatomy (CT, MRI, ultrasound) are not adequate for the detection of metastatic melanoma.^{59,60}

Tumour metabolism may be a more accurate parameter to detect tumour deposits and to monitor the effect of various forms of therapy on tumour viability. Positron Emission Tomography (PET) is an excellent technique to investigate metabolism in vivo. The radiopharmaceutical ¹⁸F-fluoro-2-deoxy-D-glucose (FDG) is used worldwide for this purpose.

FDG is a glucose analogue that is taken up by cells, which are metabolically active and especially in tumour cells. It is trapped in the first step of glucose metabolism and accumulates in the cell after phosphorylation.⁶¹ Most melanomas have a very high glucose utilisation. In in vitro experiments melanoma cells demonstrate higher uptake than other tumour types.⁶²

In means of sensitivity and specificity for the detection of metastatic melanoma FDG-PET has shown to be superior to conventional imaging techniques (CT, MRI and ultrasound). PET demonstrated uptake of FDG in untreated melanoma deposits within lymph nodes and viscera.⁶² Initial clinical experience in the mid-nineties of FDG-PET in CMM suggested that PET scanning was an accurate modality to detect melanoma metastases with the exception of metastases in the brain.⁶²⁻⁶⁵ The effectiveness of PET scanning for detecting melanoma metastases was compared to CT and MRI in a series of 76 melanoma patients, AJCC Stage II to IV. The sensitivity was 94.2% and the specificity 83.3% for PET scanning, compared to only 55.3 and 84.4 respectively for CT scanning. There were only four false negative scans, which was probably due to very small areas of melanoma. PET scanning was particularly able to detect regional lymph node metastases.

The smallest nodules detected were 4-5 mm in diameter.⁵⁹ FDG-PET compared to clinical examination, CT, ultrasound, radiography, and liver function tests and pathological routine examinations or clinical follow up, proved to be a more sensitive method for detecting widespread metastases from malignant melanoma and useful as a supplement to clinical examination in melanoma staging (Figure 2).⁶⁰

Figure 2.

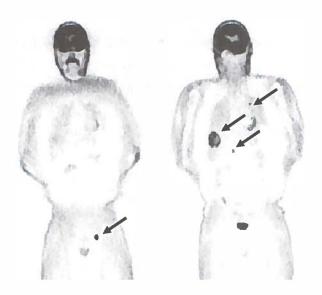


Figure 2. (A) Coronal FDG-PET image of a 44 year old patient with a penile melanoma, 7 months after partial amputation of the penis and right inguinal and para-iliacal lymph node dissections. A new lymph node metastasis in left inguinal area is clearly positive (arrow). (B) More dorsal slice of the same patient. A large metastasis with central necrosis can is found in the liver, and additional metastases in the left lung and para-aortal region (arrows). Further lymph node dissections were cancelled.

Despite this good performance of PET in staging of melanoma, sentinel lymph node biopsy proved to be even superior for the detection of metastases in regional lymph nodes in clinically node negative patients. FDG-PET imaging of regional lymph nodes in clinically node negative patients with AJCC stage I, II, and III melanoma, localised to the skin, was prospectively compared to SLN biopsy. Sensitivity of SLNB for detection of occult regional lymph node metastases was 94.4%, specificity 100%, positive predictive value (PPV) 100% and negative predictive value (NPV) 98.6%. The sensitivity of FDG-PET, however, was only 16.7%, specificity 95.8%, PPV 50% and NPV 81.9%.⁶⁶ As could be expected, the

failure to detect micrometastatic disease is the result of limitations of the imaging equipment and technique.⁶⁷⁻⁶⁹

A number of factors may interfere with the accuracy of PET scanning for metastatic melanoma. Apart from the detection limit of about 5 mm, false negatives may occur in patients with hyperglycaemia or after radiotherapy. Previous recent chemotherapy may influence the uptake of FDG due to cytostatic or cytolytic effects as well. False positives may be caused by non-specific uptake in inflammatory lesions, or mistaken for urinary excretion.⁵⁹

While less suited for primary staging, FDG-PET may be of value in stage III or IV, or for patients with recurrent melanoma.^{69,70} Patients may benefit from surgical removal of recurrences as long as no further metastases are present. To exclude the presence of additional metastases, FDG-PET may be useful, although more evidence is needed before FDG-PET data will influence therapeutic decision making.^{69,71,72} Detection of metastatic melanoma with new tracers needs to be further investigated, although it remains doubtful whether micrometastases will ever be detected, like in the sentinel node procedure.

Pathology

There are currently over 25 prognostic factors for CMM based on variables from the primary tumour. Tumour size, especially Breslow-thickness, invasion, ulceration, and site are the most important prognostic factors. There is also a growing interest in the impact of angiogenesis as a critical contributor to tumour growth, prognosis, and especially to metastatic potential. Based on multiple regression analysis the lymph node status of the melanoma patient is still the most powerful predicting factor for recurrence and survival.^{35,39,41}

The technique of examining the SLN has improved and different techniques are used for the detection of micrometastatic disease. Routine histological evaluation is based on conventional HE staining of one or two sections from the central cross-section of the node, and examination involves less than 1% of the volume of the node and thus could easily miss micrometastatic disease. Histological examination of a lymph node at several levels clearly results in an increased sensitivity.^{38,73,74} In addition, other techniques can be applied in order to increase the detection rate of (micro)metastatic cells.⁷⁵ Theoretically the presence of metastatic melanoma cells can be determined by demonstrating specific proteins using immunohisto- or cytochemistry; by demonstrating the presence of specific

changes in the DNA (translocations, mutations) using polymerase chain reaction (PCR), or detecting gene expression in the metastatic cells by identifying specific mRNAs using RT-PCR. In addition, relevance of serum tumour markers using immunochemical techniques in evaluation of therapy response and/or prognosis are investigated. ^{76,77}

Using immunohistochemistry, 1 tumour cell in 10⁵ cells in lymph nodes can be detected.⁷⁸ Using the SLN biopsy technique only one or two lymph nodes are analysed in detail for micrometastatic disease. Serial sectioning and immunohistochemical staining with the S-100 and the HMB-45 antibodies will increase the number of positive nodes identified (Figure 3).^{73,79} However, the S100 protein is a non-specific marker since it is also expressed in amongst others Schwann cells and dendritic reticulum cells normally present in the lymph nodes.⁸⁰ HMB-45 is variably expressed in melanomas.⁸¹ No melanoma specific antigen has been described yet.

Figure 3.

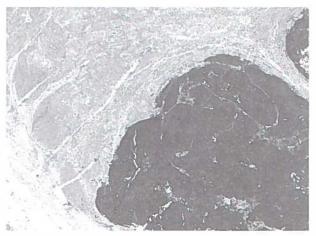


Figure 3. Metastatic melanoma cells in a lymph node: Immunohistochemical staining using anti HMB-45. Original magnification: 5x.

A breakthrough was the development of a highly sensitive method to reduce the already low false-negative rates of lymph nodes, by examining the lymph nodes for the presence of tyrosinase messenger RNA by RT-PCR. Fifty-eight percent of the histologic-negative SLN was upstaged with the RT-PCR.⁸² RT-PCR is an extremely sensitive, and reproducible, and efficient technique for the identification of micrometastases in melanoma patients.⁸³⁻⁸⁵ The technique of RT-PCR is also already successfully used on SLN's.⁸⁴⁻⁸⁷ With IHC or PCR techniques 9-44% of the negative lymph nodes by routine HE staining,

will be upstaged. Investigators have reported additional positive lymph nodes in lymphadenectomy specimens in 10-52% of cases.^{74,84,85,88} Tyrosinase is expressed in nonmalignant melanocytes and Schwann cells, which can be present in lymph nodes.⁸¹ Tyrosinase expression in lymph nodes can also be caused by 'illegitimate transcription', caused by imperfect transcription, as well.^{89,90} These two causes for tyrosinase expression in lymph nodes can dit is therefore advisable to use a panel of markers to increase the specificity.^{52,81,91,92}

Heterogeneity and specificity of gene expression and the importance of morphological control will influence test results. Regarding specificity, target genes should be selected that are exclusively expressed in the tumour cells and not in lymphatic cells. Examples are "illegal" expression of gp100, which was considered as a melanocytic lineage specific gene.⁹³ Finally, it is important to compose the right primer sets for the PCR to avoid amplification of pseudogenes^{94,95}, which may lead to false positive results. Regarding the heterogeneity of gene expression one should realise that most tumours, especially the poorly undifferentiated ones, may contain tumour cells which do not express specific differentiation genes as tyrosinase and MART-1.96 Approximately 17% of the advanced primary melanomas and melanoma metastases did not show positive tumour cells for any of these two differentiation markers.⁹⁶ In such cases the detection of tumour specific markers, i.e. MAGE's may yield useful.⁹⁷ The search for genes which play a role in malignant melanoma is difficult, but several important discoveries have been made.98-100 Several studies have compared the sensitivity of IHC and the RT-PCR on lymph node tissue and showed that PCR is more sensitive ^{74,84,85,88,101} A disadvantage of PCR is that there is no morphological control and false positives can occur. Furthermore, we should realise that in most of these studies IHC was performed on only one single thin section while for PCR several thick sections are used, increasing the odds of a positive PCR.

S100, Melanoma Inhibiting Activity (MIA) and tumour-associated antigen (TA90) have been detected as serum markers for malignant melanoma, which are valuable in therapy monitoring and in detecting tumour progression.^{76,77} Recently, a prospective study with 1,007 patients, confirmed that the new luminescence immuno assay (LIA) assay of S100-B protein in serum is correlated with clinical stage and is an independent prognostic marker in clinical stages II and III.¹⁰² RT-PCR based detection of tyrosinase in peripheral blood shows limitations in clinical relevance, and reproducibility.^{92,103,104} The use of a panel of markers will allow a better insight in prognostic classification.¹⁰⁵⁻¹⁰⁷

Nevertheless, 25% of the negative stage I and II melanoma patients will recur and die of their disease within 5 years of diagnosis, suggesting that some of these patients already have hematogenous metastases.

The value of the upstaging of the SLN with IHC or RT-PCR with respect to disease free survival, or the consequences for a lymph node dissection is currently unknown, but a combination of a panel with tumour specific markers with morphology will increase the accuracy. The search for specific makers, which indicate the genetic defects for melanoma, is still pending and will increase the accuracy as well. In addition proliferating markers of tumour progression may be of additional value. The place of the melanoma tumour marker S100-B via LIA in the clinical decision making of CMM needs further investigation.

Conclusions

The presence or absence of lymph node metastases is the most powerful predicting factor for recurrence and survival of melanoma. The 5 year survival rates for localised tumours for AJCC Stage I and II are 92.5 and 74.8%, respectively, Stage III 49.0%, and Stage IV only 17.9%.³ These figures have changed in the revised AJCC classification, because of the change in tumour-node-metastasis (TNM) criteria and stage groupings.⁴¹ The 5-years survival rate following therapeutic lymph node dissection ranges in the literature from 19% to 38%.¹⁰⁸ Lymphatic metastases are generally followed by hematogeneous metastases. Surgery for metastatic melanoma is usually palliative only, but in a selected group of patients with metastasis it prolongs survival, even for years.¹⁰⁹ At present surgery is the only curative treatment option for metastatic disease.¹¹⁰

Clinical research confirms the high accuracy and good clinical applicability of the SLN concept.^{31,33,111} The importance of the prognostic role of a positive SLN has been underlined by incorporation of the SLN status in the revised staging system for CMM.³⁹ Because the impact of the SLN on the final treatment and survival of melanoma patients is still unknown, we believe that more research is needed in that area.

FDG-PET is superior to conventional imaging techniques for staging metastatic melanoma (ultrasound, MRI and CT).^{59,60} FDG-PET has proven to be especially useful in stage III and IV disease.⁶⁹⁻⁷² The accuracy of detecting metastases can be interfered by different factors.⁵⁹ As expected, FDG-PET is inferior to SLN biopsy in clinically negative lymph node patients with AJCC stage I and II, especially because of the inability to detect

micrometastasis.⁶⁶⁻⁶⁸ FDG-PET as a diagnostic tool may especially be useful for stage III and IV disease.^{69,70,72}

The techniques of examining the SLN have improved the last decade, especially by increasing the number of dissection levels and using IHC and RT-PCR.^{38,73,74} By using immunohistochemical staining with S-100 and HMB-45, and RT-PCR on tyrosinase mRNA the number of positive nodes has increased to almost 50%.^{74,79,82,84,85,88} Nevertheless, in 25% of negative stage I and II patients the melanoma will recur and patients die within 5 years of diagnosis.

For the detection of metastatic cells in lymph nodes and in peripheral blood, it is advisable to use a panel of makers to increase specificity^{81,91,92,105-107,112} in combination with morphological control. The search for specific genes, which play a role in malignant melanoma, is ongoing, but several discoveries have been made.⁹⁸⁻¹⁰⁰

The surgical treatment of primary and recurrent melanomas, as well as lymphogenic and/or metastatic disease is well defined. The SNB concept is improving the staging of melanomas, but the clinical status is still experimental. The interferon therapy in an adjuvant setting is still not accepted as a standard therapy. PET has the potential to provide more insight in the amount of metastatic deposits in stage III and IV patients. Surgery is still the major corner stone in the treatment of melanoma. Further clinical and fundamental research may provide more insight in the treatment of a disease with a fast growing incidence. Melanoma is still an unimaginable and unpredictable disease.

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Chapter 3

Fluorodeoxyglucose-positron emission tomography and sentinel lymph node biopsy in staging primary cutaneous melanoma

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Summary

Aim: In this study we investigate the value of sentinel lymph node (SLN) biopsy and Fluorodeoxyglucose Positron Emission Tomography (FDG-PET) in relation to SLN biopsy in staging primary cutaneous melanoma.

Methods: 55 patients with primary cutaneous melanoma of more than 1.0 mm. Breslow thickness and no palpable regional lymph nodes underwent a FDG-PET scan before SLN biopsy.

Results: SLN's were retrieved in 53 patients. Melanoma metastases were found in the SLN of 13 patients. FDG-PET detected the lymph node metastases in two of the 13 patients with SLN metastases. In five patients FDG accumulation was recorded in a regional lymph node basin, while no tumor positive SLN was found. In 8 patients FDG-PET showed increased activity at a site of possible distant metastasis. Only in one patient metastatic disease was confirmed. In five of these patients no possible explanation for the positive FDG-PET result could be found.

Conclusion: FDG-PET should not be considered in this group. SLN biopsy reveals regional metastases that are too small to be detected by FDG-PET. The prevalence of distant metastases is too small to justify routine use of FDG-PET.

Introduction

Accurate staging of patients with cutaneous melanoma is important. After tumor thickness and tumor ulceration, lymph node status is the most important prognostic factor, as is emphasized in the completely revised staging system for cutaneous melanoma (1). Elective lymph node dissection has been proposed to increase survival in patients with isolated regional lymph node metastases. Although some studies failed to demonstrate the benefit of elective lymph node dissection, long term results from the Intergroup Melanoma Surgical Trial show a survival benefit for stratified subgroups of patients with non-ulcerated tumors, tumor thickness between 1.0 mm and 2.0 mm, or melanomas of the limb, undergoing elective regional lymph node dissection. (2). If regional lymph node dissection gives a survival benefit, it is likely to be in patients with metastases confined to the regional lymph node basin. Identification of patients with occult regional lymph node metastases may thus be important. Sentinel lymph node biopsy (SLNB) is widely used for this purpose. The value of early detection of lymph node metastases by SLNB, followed by therapeutic lymph node dissection, is currently prospectively studied in the Multicenter Selective Lymphadenectomy Trial (3) and the Sunbelt Melanoma Trial (protocol on http://www.sunbeltmelanoma.com/prot2000.htm). SLNB is an invasive procedure that gives no direct information on possible distant metastases, although a positive SLN has been shown to be the best predictor of tumor recurrence (4).

In recent years fluorodeoxyglucose - positron emission tomography (FDG-PET) may be a sensitive staging tool for melanoma. Initial results comparing FDG-PET with conventional diagnostic tests or with elective or selective regional lymph node dissection suggested a sensitivity and specificity of 90 percent or more (5-7).

This study was designed to investigate the value of FDG-PET scanning in the clinical treatment of primary cutaneous melanoma. The following questions were addressed: does FDG-PET predict lymph node metastasis in the SLN, and does FDG-PET provide useful information about extended disease outside the primary lymph node basin?

Patients and methods

Patients were selected with primary cutaneous melanoma \geq 1.0 mm Breslow thickness on the extremities or trunk, and no palpable regional lymph nodes. Fifty-five patients were entered in this study; 45 patients were treated at University Medical Center Nijmegen, and 10 patients were treated at the University Hospital Groningen, The

Netherlands. Twenty-six patients (47 percent) were male, 29 patients (53 percent) were female. Age range of the patients was 15 to 77 years, median age was 54 years. The primary lesions were located on the upper extremity in five patients (9 percent), on the lower extremity in 27 patients (49 percent), and on the trunk in 23 patients (42 percent). Mean Breslow thickness was 3.18 mm, ranging from 1.00 mm to 13 mm. Median Breslow thickness was 2.40 mm.

SLNB technique

All patients were scheduled to undergo sentinel lymph node biopsy. Preoperatively, lymphatic drainage patterns were defined by performing lymphoscintigraphy with ⁹⁹Tc nanocolloid. Probable sentinel nodes were marked at the skin. Before the incision, one to two milliliters patent blue dye was injected around the excision scar of the primary lesion. A gamma probe was used to identify the sentinel node during the operation, as is described in detail by Nieweg and Keshtgar (8,9). In Nijmegen a Europrobe (Euromedical Instruments, Le Chesnay, France) was used, in Groningen a Neoprobe 1000 and Neoprobe 2000 (Neoprobe Corporation, Dublin, Ohio, USA).

FDG-PET scanning technique

All patients underwent a FDG-PET scan before the operation. In Nijmegen, a dedicated, rotating half-ring PET-scanner (ECAT-ART, Siemens/CTI, Knoxville, TN, USA) was used for data acquisition. Prior to FDG-injection, patients were fasting for at least 6 h. Intake of sugar-free liquids was permitted. Immediately prior to the procedure, patients were hydrated with 500 ml of water. One hour after intravenous injection of 200-220 MBq FDG (Mallinckrodt Medical, Petten, The Netherlands) and 20 mg furosemide, emission and transmission images of the area between proximal femora and the base of the skull were acquired (10 minutes per bed position). The images were corrected for attenuation and reconstructed using the ordered-subsets expectation maximisation (OSEM) algorithm.

In Groningen, an ECAT 951/31 or an ECAT HR+ positron camera (Siemens/CTI, Knoxville, TN, USA) was used for data acquisition. After overnight fasting the patients were administered 422 MBq FDG (range 386 - 603 MBq) intravenously. Patients were hydrated in the same fashion. ¹⁸F-FDG was synthesized according to Hamacher by an automated synthesis module.(10,11) Data acquisition started 90 min after injection for 5

min per bed position. Both attenuation corrected and non-attenuation corrected images were reconstructed using OSEM.

Results

Sentinel node

Sentinel lymph node (SLN) biopsy was performed using ⁹⁹Tc nanocolloid in all patients and patent blue in 22 patients. SLN's were retrieved from one lymph node basin in 45 patients, and from a second lymph node basin in eight patients (15%). In two patients (4 percent), a SLN could not be retrieved. Melanoma metastases were found in the SLN of 13 patients (24%). Mean Breslow thickness of the primary tumour was 4.28 mm, ranging from 1.0 to 13.0 mm. Median Breslow thickness was 2.4 mm.

FDG-PET

FDG-PET detected the lymph node metastasis in only two of the 13 patients with proven SLN metastases. The diameter of the lymph node metastasis was 7 and 8 mm in these patients. The Breslow thickness of the primary tumour was 2.4 and 4.4 mm respectively. In the other 11 regional metastatic sites no abnormal FDG accumulation was seen. The diameter of the metastases in these 11 sentinel lymph node was: $\leq 2 \text{ mm (n=8)}$, 4 mm (n=1), 5 mm (n=1), and 11 mm (n=1). In the 32 SLN negative patients FDG-PET was negative in 27. However, in five patients FDG accumulation in a regional lymph node basin was recorded, while no tumor-positive SLN was found.

FDG-PET scan showed increased activity at a site of possible distant metastasis in eight patients.

- In one patient, increased activity in the mediastinum, liver and right adrenal gland was demonstrated to be caused by metastatic disease.
- In one patient increased activity in the mediastinum was demonstrated, later concluded to be due to a lung cancer.
- In two patients, increased activity was seen in the mediastinum and lung hilus. Analysis by CT scan in both patients and mediastinoscopy in one patient did not reveal any abnormalities.
- In one patient increased activity was seen at the splenic flexure of the colon. At colonoscopy no abnormalities were found.

- In one patient, increased activity was seen along the aorta and right iliacal vessels, cranial and posterior to the bladder. Sigmoidoscopy showed a hyperplastic polyp at 20 cm from the anal verge, which may explain the retrovesical hotspot. CT scan showed para-aortal lymph nodes with a diameter of 1.3 cm and several para-aortal, iliac, and peri-rectal lymph nodes with a diameter of 1 cm or less, which did not change in the following years.
- In one patient increased activity was demonstrated in the presacral area. After a followup of 38 months, the patient remains with no evidence of metastatic disease.
- In one patient increased activity was demonstrated caudal to the liver. A barium enema study showed a probable malignancy at the hepatic flexure for which the patient underwent a right hemicolectomy. Pathological examination revealed a T1N0 lesion in a large tubulovillous adenoma.

Discussion

In this study, we evaluated FDG-PET scanning in staging primary cutaneous melanoma \geq 1.0 mm Breslow thickness, and no palpable regional lymph nodes. SLN biopsy identified 13 patients with regional lymph node metastases, six of these patients had a micro metastasis (< 2 mm). FDG-PET scanning identified only two of these patients, with regional metastases of 7 mm and 8 mm in diameter. Furthermore, FDG-PET scanning suggested incorrectly a regional lymph node metastasis in 5 patients. Only one patient with generalized metastatic disease was identified by FDG-PET scanning.

Technical limitations of the FDG-PET are likely to cause these poor results (6,12,13). Only tumor loads of 80 mm³ or more can be visualized by FDG- PET (13) or expressed as a detection level of 4-5 mm (14). This is in contrast with SLN biopsy, where the pathologist is able to identify micro metastases (15).

Some studies have published favorable results of FDG-PET in staging primary melanoma (5,6). These studies compared FDG-PET with conventional diagnostics or lymph node dissection and not with SLN biopsy. In these studies accuracy rates of 88-98% were reported.

Ackland and co-authors evaluated FDG-PET and SLN biopsy in 50 patients with primary melanoma more than 1 mm in thickness or with lymphatic invasion. Fourteen positive regional lymph nodes were retrieved by SLNB. No regional lymph node metastasis was found with FDG-PET (12). Wagner and co-authors compared FDG-PET to

SLNB in 70 patients with primary melanoma with a thickness more than 1 mm or with localized regional cutaneous recurrence (16). In 17 patients, regional lymph node metastases were found with SLNB while in one additional patient a regional lymph node metastasis was found during follow-up examination. Only three of these 18 regional lymph node metastases were found with FDG-PET. Belhocine and co-authors also evaluated FDG-PET and SLN biopsy in 21 patients. FDG-PET detected only one of six sentinel node metastasis (17).

FDG-PET may be of value in stage III, IV, or for patients with recurrent melanoma (13,18). More research is needed before FDG-PET will influence therapeutic decision making (7,13,19,20).

In conclusion, FDG-PET should not be considered in patients with primary cutaneous melanoma \geq 1.0 mm Breslow thickness, and no palpable regional lymph nodes. SLN biopsy reveals regional metastases that are too small to be detected by FDG-PET. The prevalence of distant metastases in this group of patients is too small to justify routine preoperative FDG-PET.

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Chapter 4

¹⁸F-3'-fluoro-3'-deoxy-L-thymidine; a new tracer for staging metastatic melanoma?

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Summary

In this study the feasibility of ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine positron emission tomography (FLT-PET) for staging patients with clinical stage III melanoma was investigated.

Methods: 10 patients with melanoma and metastases to the locoregional draining lymph nodes, clinical stage III, based on physical examination, chest X-ray, LDH and histopathological confirmation underwent a whole-body FLT-PET scan 1 hour after injection of a median 400 (185-430)MBq FLT. Patients were staged according. All FLT-PET lesions were verified using the American Joint Committee on Cancer Staging System which includes physical examination, spiral computed tomography, ultrasound, chest X-ray and histopathological examinations. Size and mitotic rate of metastatic lymph nodes and skin metastases were determined.

Results: All histopathological samples and FLT-PET lesions were categorized over anatomical regions and correlated. All locoregional metastases were correctly visualized by FLT-PET. Region based sensitivity for detection of lymph node metastatic disease was 88%. There were 3 true negative and 2 false positive lesions. The detection limit for lymph node metastases appeared to be approximately 6 mm or a mitotic rate of 9 per 2 mm². Two patients were upstaged by FLT-PET, which was confirmed by CT. In three patients, FLT-PET detected a total of 3 additional lesions, with therapeutic consequences, without influencing staging. These lesions were initially missed by clinical staging.

Conclusion: FLT-PET seems promising for (re)staging purposes in clinically stage III melanoma. Further research is needed, in which FLT-PET should be compared with FDG-PET.

Introduction

Positron emission tomography (PET), using ¹⁸F-fluoro-2'-deoxy-D-glucose (FDG), has been accepted as a powerful non-invasive metabolic imaging method for the diagnosis and staging of cancer (1). The enzyme hexokinase causes intracellular entrapment of FDG, reflecting glucose metabolism. (2) FDG is transported into the cells, which are metabolically active, especially in the case of tumor cells (3).

Most melanomas have a very high glucose utilization. In vitro experiments demonstrate a high FDG uptake in melanoma cells (4). Therefore, almost parallel with the introduction of the sentinel lymph node biopsy (SLNB) in the staging of melanoma patients, FDG-PET emerged as a clinical modality for staging, restaging and therapy monitoring. Conventional imaging techniques, such as computed tomography (CT), magnetic resonance imaging (MRI), ultrasound (US) and physical examination are not as accurate for the detection of metastatic melanoma as SLNB and/or FDG-PET (5). For primary locoregional staging, FDG-PET is surpassed by the SLNB (6-9). FDG-PET may be of value in stage III or IV melanoma patients, or for patients with recurrent melanoma (5,10-14).

FDG is not a selective tracer, since it is also taken up in macrophages. Macrophages invade tumors and appear in inflammatory lesions, causing false positive results (*15*,*16*). Another problem is a decreased uptake in hyperglycemia (*17*). Furthermore, routine whole-body FDG-PET lacks sensitivity for imaging brain metastases, because glucose is avidly taken up by the normal brain.

Recently, ¹⁸F-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT) has been introduced as a PET-tracer by Shields and Grierson, which might not have these drawbacks (*18,19*). This pyrimidine analog, is phosphorylated by the enzyme thymidine kinase 1 (TK₁), which leads to intracellular trapping (*19*). During DNA synthesis, TK₁ activity increases almost tenfold and is, therefore, an accurate reflection of cellular proliferation (*20*). The aim of this study was to investigate the feasibility of FLT-PET for the staging of regionally metastasized melanoma.

Materials and Methods

Patients

This prospective study consisted of ten consecutive patients with clinically stage III melanoma (locoregional disease). Patients were included from April until November 2002. Two patients had a unknown primary and 2 patients had a primary melanoma, which was too small to assess the Clark level. All patients gave written informed consent. For inclusion, the liver and kidney functions and hematological parameters (Hb, Ht, erythrocytes, thrombocytes, leukocytes and white cell count) had to be within normal limits. Pregnant patients and patients with psychiatric disorders were excluded. All screened patients could be included in the study. The Medical Ethics Committee of the Groningen University Hospital approved the study protocol.

PET studies

Synthesis of FLT was performed according to the method of Machulla et al.(21) FLT was produced by [¹⁸F]fluorination of the 4,4'-dimethoxytrityl protected anhydrothymidine, followed by a deprotection step. After purification by reversed phase HPLC, the product was made isotonic and passed through a 0.22 μ m filter. FLT was produced with a radiochemical purity of >95% and specific activity of >10 TBq/mmol. The radiochemical yield was 6.7±3.7% (decay corrected).

Eight studies were performed using an ECAT EXACT HR+ (Siemens/CTI Inc., Knoxville, TN) and two studies on an ECAT 951/31 (Siemens/CTI Inc., Knoxville, TN). Prior to PET imaging, patients were instructed to fast for at least 6 hours to keep the study comparable with studies performed with FDG (22). They were also instructed to drink one liter of water prior to imaging to stimulate FLT excretion from the renal calyces and stimulate subsequent voiding. Surgery followed FLT-PET after a median period of 26 (7-45) days.

Sixty minutes after injection, a non attenuation-corrected whole-body scan was acquired from crown to femur with 8 minutes per bed position. Because detection or exclusion of malignant lesions, rather than the quantitative determination of uptake, is the main goal of this feasibility study, only non-attenuation corrected PET images were obtained. If the primary tumor was located under the level of the femur, the patient was

scanned from crown to foot. PET-images were iteratively reconstructed (ordered subset expectation maximization) (23).

Pathological evaluation and staging

The histology of all primary lesions and metastasis were evaluated according to the latest version of the American Joint Committee on Cancer (AJCC).(24) The emphasis of this classification is on tumor thickness, ulceration and number of positive lymph nodes. Breslow thickness and Clark level of the primary lesion were evaluated. In all metastatic lesions (in-transit and lymph node metastases), tumor size and mitotic rate were measured. Tumor size was expressed in mm or as micrometastasis if smaller than 2 mm. Mitotic rate was expressed in number of mitoses per 2 mm² at a 400 magnification.

The staging took place according to the last version of the American Joint Committee on Cancer (AJCC) (24). All patients were firstly staged clinically, by physical examination, LDH, chest X-ray and histopathological confirmation of the locoregional lymph node(s). Lastly, the patients were staged on the basis of the FLT-PET images only and finally staged pathologically after surgery. The included patients with stage III melanoma had locoregional metastases in the lymph nodes of the groin or axilla.

Data analysis

FLT-PET images were analyzed for uptake in malignant lesions and normal anatomical structures. Two experienced PET-physicians (PLJ, DCPC) evaluated the images independently only aware of the original location of the primary lesion, but blinded for other clinical information. They subsequently reached consensus on a lesion by lesion basis.

The pathologist (AJHS) was unaware of the results of the PET-images.

Because it is impossible to exactly match individual lesions on PET with the exact same lymph nodes as analyzed after resection or cytological aspiration, it was decided to categorized all histopathological and PET findings into relevant anatomical regions. The regions were defined as follows: superficial or deep groin, para-iliacal, obturator, popliteal, supraclavicular, axillar, mediastinal, skeleton, back, neck, arm, calf and heel. PET and histological data from these areas were correlated and sensitivity and specificity were calculated. Therefore only regions with histopathological confirmation were analyzed for accuracy. Per anatomical region all positive lymph nodes were measured in mm and the mitotic rate of the lymph node with the highest proliferation was calculated to estimate the detection level of FLT-PET.

The results of clinical staging (pre-surgery), staging with FLT-PET (pre-surgery) and pathological staging (post-surgery) were compared.

Results

FLT Distribution in patients

Ten patients were included. Patient and primary melanoma characteristics are shown in Table 1.

Patients received a median of 400 (185-430) MBq FLT. Intense FLT uptake was observed in the skeleton, with a distribution pattern that is typical for bone marrow uptake (Figure 1). Also the liver shows avid uptake. Minor uptake is observed in intestinal structures. All other organs and tissues show low grade and homogeneous uptake. No activity is present in the brain.

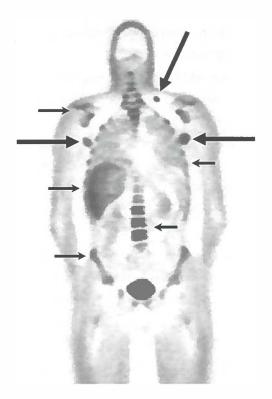
In all patients one or more abnormal lesions were found using FLT PET. Patient based sensitivity therefore was 100%.

| Patient | Age | Sex | Clark | Breslow | Locoregional |
|---------|-----|--------|-------|-----------|--------------|
| | | | Level | Thickness | Disease |
| | | | | (mm) | |
| 1. | 48 | Female | * | * | Groin |
| 2. | 39 | Female | IV | 1,8 | Groin |
| 3. | 42 | Male | IV | 4,1 | Axilla |
| 4. | 73 | Male | IV | 4,4 | Groin |
| 5. | 78 | Male | IV | 1 | Groin |
| 6. | 34 | Male | ** | 6 | Axillas |
| 7. | 40 | Male | IV | 1,35 | Axilla |
| 8. | 29 | Male | * | * | Groin |
| 9. | 40 | Female | III | 0,7 | Axilla |
| 10. | 54 | Male | ** | >4 | Groin |

Table 1. Patient Characteristics

* Unknown primary, **Primary melanoma to small to assess Clark level.

FIGURE 1.



F LT-PET of 34 year male (Pt 6) 2 months after resection of the primary melanoma on his back. Metastases can be observed in his left and right axilla and left supraclavicular area and are indicated by large arrows. Physiological uptake can be observed in liver and one marrow e.g. in the pelvis, vertebrae, ribs, and bony structures of the shoulder; indicated by small arrows; less intense, uniform tracer uptake was present in the lungs. Uptake of the tracer in the brain was negligible and no uptake was observed in the mediastinum and myocardium.

Region based analysis

Twenty-two true positive, 3 true negative, 3 false negative and 2 false positive regions were observed, resulting in pathological proven sensitivity of 88% (Table 2). There were 3 true negative and 2 false positive lesions.

Two of the three false negative results were caused by multiple cutaneous and subcutaneous malignant lesions (satellite or primary lesions) located on the back of 2 patients, with diameters ranging from 1 to 10 mm and mitotic rate ranging from 5 to 16 per 2 mm² (Table 3). The other false negative result was caused by a micrometastasis in a lymph node in the groin.

One of the two false positive lesions was located in the groin, but no positive lymph nodes were found after resection of the groin area. The other false positive lesion was located in the heel. This was the location of the primary melanoma, which was resected in toto 4 years earlier and is still clinically negative.

The three true negative regions, which displayed very little or no FLT-uptake were one region with negative lymph nodes after resection and two resected benign skin lesions; one located on the calf and one on the arm.

At the lesion level, analysis of tumor size and mitotic rate of metastatic lymph nodes, revealed that, the smallest detected lesion, consisted of three closely adjacent lymph nodes with in each lymph node a micrometastasis (<2mm). The detected lesion, with the lowest mitotic activity that was still detected, had a mitotic rate of 9 mitoses per 2 mm².

In two of the above mentioned true positive lesions, FLT-PET detected malignancy, which was initially missed with conventional staging techniques. In both patients this had therapeutic consequences as either dissection or radiation therapy was now indicated, but no influence on staging. These lesions were found in patient 1 and 2. In patient 1, a lesion in the fossa poplitea was indicated as malignant by FLT-PET and was confirmed on ultrasound guided aspiration cytology. The patient underwent a groin dissection and a resection of the popliteal lesion. In the supraclavicular region of patient 2, an additional lesion was detected, which was confirmed by ultrasound guided aspiration cytology. This patient received radiation therapy for locoregional control.

| | FLT + | FLT - |
|------------------|-------|-------|
| Histopathology + | 22 | 3 |
| Histopathology - | 2 | 3 |

| Table 2. Cross table of FLT-PET regions | compared with histopathological regions |
|---|---|
|---|---|

Sensitivity=88%; specificity=60%.

Additional lesions

Eleven previously unknown lesions were present on FLT-PET (Table 3). These were not histopathological confirmed, but analyzed with conventional staging techniques. Five lesions were true positive when compared with CT or physical examination. Two

mediastinal and two para-aortal lesions were confirmed as metastases (>1cm); one lesion in the supraclavicular lesion was confirmed on physical examination.

Four of these 11 unknown lesions were true negative based on a completely normal CT scan or clinical follow-up. One mediastinal and one para-aortal lesion were negative on CT (<1cm). Two lesions in the head and neck area were confirmed to be clinically negative as well during clinical follow-up.

Finally, two lesions detected by FLT-PET and interpreted as malignant, could not be evaluated. The lesion in patient 2, which was interpreted as benign was located in a lumbar vertebra, which was below the level of the CT-scan. The bone scan, which was performed 2.5 months later showed multiple lesions in the spine. It can be assumed that these lesions were already present at the time of the FLT-PET. The remaining lesion in patient 5, was located in the area of popliteal lymph nodes of the involved leg next to a vascular prosthesis. However, recently this patient developed brain metastases, for which he was palliatively treated. During a follow-up of period of 3 months, this lesion remained clinical negative. Although the above mentioned two lesions were malignant, since these patients developed disseminated disease within 12 weeks.

There were four lesions, which were missed on FLT-PET without histopathological evaluation (Table 3). These four lesions were false negative on FLT-PET when compared with CT. Three of these lesions were interpreted as mediastinal lymph node metastases (>1cm) on CT and one a bone metastasis in a thoracic vertebra on CT.

| Location | # of | PA | Result | It Diagnostics | |
|------------------------|---------|-----|--------|---|--|
| | lesions | | | | |
| deep groin | 1 | pos | FN | Aspiration cytology | |
| dermal or subcutaneous | 9 | pos | FN | Histopathology | |
| metastases on the back | | | | | |
| back (primary tumor) | 1 | pos | FN | Histology | |
| deep groin | 1 | neg | FP | Histopathology | |
| leg (heel) | 1 | neg | FP | Re-resection in 1998 negative and clinical negative, | |
| | | | | follow-up of 5 years | |
| mediastinal | 3 | NP | FN | СТ | |
| thoracic vertebra | 1 | NP | FN | СТ | |
| lumbar vertebra | 1 | NP | NA | bone scan with multiple bone metastases (also spinal) | |
| | | | | 2.5 months after PET | |
| fossa poplitea | 1 | NP | NA | Clinical negative, follow-up of 4 months | |
| mediastinal | 1 | NP | TN | СТ | |
| para-aortal | 1 | NP | TN | СТ | |
| head and neck | 2 | NP | TN | Clinical negative, follow-up of 3 months | |
| mediastinal | 2 | NP | TP | СТ | |
| para-aortal | 2 | NP | TP | СТ | |
| supraclavicular | 1 | NP | TP | Physical examination | |

Table 3. False negative, false positive and additional FLT-PET findings

FN=false negative; FP=false positive; NA=not assessable; neg=negative; NP=not performed; pos=positive; TN=true negative; TP=true positive.

Effect of FLT-PET on staging

FLT-PET detected the extent of the locoregional disease correctly in all patients (Table 4). The clinical (pre-surgery), FLT-PET and pathologic (post-surgery) staging were compared. All patients were clinically stage III. However, one patient was upstaged to stage IV both by CT and FLT-PET, as both modalities detected mediastinal metastases. Another patient was upstaged by FLT-PET as compared with the clinical pre-surgery staging, which was confirmed by CT. The detected metastases, which caused the upstaging in the second patient, were located in para-aortal (lymphatic) region.

| Tal | ы | • | A | Cta | air | |
|-----|---|---|----------|-----|-----|----|
| I a | U | C | . | Sta | уıı | ıy |

| | Clin | ica | I staging | PET | st | aging | Pat | holog | gical | staging |
|---------|------|-----|-----------|-----|----|-------|-----|---------------|-------|---------|
| Patient | Т | Ν | Stage | N | Μ | Stage | Т | N^{\dagger} | Μ | Stage |
| 1. | * | + | III | + | 0 | | * | p2b | 0 | IIIB |
| 2. | 2a | + | III | + | 1 | IV | 2a | р3 | 1c | IV |
| 3. | 4b | + | III | + | 0 | III | 4b | р3 | 0 | IIIC |
| 4. | 4b | + | III | + | 1 | IV | 4b | р3 | 1c | IV |
| 5. | 1a | + | III | + | 0 | III | 1a | р3 | 0 | IIIC |
| 6. | 4b | + | 111 | + | 0 | ш | 4b | р3 | 0 | IIIC |
| 7. | 2a | + | Ш | + | 0 | Ш | 2a | p1b | 0 | IIIB |
| 8. | * | + | HI | + | 0 | HI | * | р3 | 0 | IIIC |
| 9. | 1a | + | Ш | + | 0 | III | 1a | p1b | 0 | IIIB |
| 10. | 4b | + | III | + | 0 | III | 4b | р3 | 0 | IIIC |

*Unknown primary.+=positive lymph nodes on physical or cytological examination. [†]All patients had loco-regional lesions visualized by FLT-PET.

Discussion

The study shows the feasibility of FLT-PET in the visualization of locoregional metastasized melanoma, as well as metastatic disease.

In ten patients, FLT-PET was compared with the histopathological results of the locoregional lymph nodes. All available resected tissue samples and lesions on FLT-PET were categorized in anatomical regions and were compared. The sensitivity was 88% and specificity 60%, based on 3 true negative and 2 false positive lesions. Due to the low number of false positive and true negative lesions, the specificity is less reliable. FLT-PET detected all locoregional metastases. Analyzing the effect of FLT on tumor stage, 2 (20%) of patients could be upstaged. However, also CT generated this upstaging.

The detection limit for lymph node metastases was lower than for the in-transit metastases. All in-transit metastases were below the detection limit of lymph node metastases of approximately 6 mm (3 lesions with micrometastases <2mm) and below detection limit of mitotic rate 9 per 2 mm² of FLT-PET. All in-transit metastases had a diameter of 1-10 mm and a mitotic rate of 5-10 per 2 mm². Taken the detection limit into account, sensitivity of FLT-PET increased to 90% when compared with histopathologically examined samples only. Comparing FLT with FDG, the detection limit of FDG-PET for lymph nodes with melanoma metastases also depends on tumor volume and imaging equipment and technique (*11-14,27-31*). A tumor volume larger than 78 mm³ is needed for

a sensitivity higher than 90% or a diameter of at least 6 mm for a sensitivity higher than 83% (*11,31*). These FDG data are in the same range as our FLT findings.

The role of FDG-PET for detecting melanoma has been evaluated extensively over the last decade. For staging patients with stage I and II melanoma, the sentinel node biopsy will remain the method of choice (5,28). FDG-PET can be of value in stage III and IV, or for patients with recurrent melanoma (10,32). In the literature there is a large variation in sensitivity and specificity of FDG-PET for the detection of melanoma metastases. A recent review by Mijnhout et al showed a sensitivity and specificity for the detection of melanoma metastases with of FDG-PET of respectively 79%(95%CI 66-93%) and 86%(95%CI 78-95%) (13). Recent reports show comparable results (10,24,32,33). FDG-PET displays false negative findings caused by small skin metastases or primary small skin lesions of melanoma as well (32,33). The cutaneous and subcutaneous lesions, which were missed by FDG-PET had a diameter between 1 and 10 mm (33). When comparing these figures with the performance of FLT-PET, FLT-PET appears to be equally accurate as FDG-PET and has the same detection limit (32).

In this study no patient had brain or liver metastases. The detection of liver metastases by FLT-PET could be disturbed by the physiological uptake in the liver. However, brain metastases could be detected, since there is no physiological uptake of FLT in the brain and FLT-PET has been able to detect brain tumors (*19,34,35*).

Conclusion

The results of this study indicate that FLT-PET could be a new method for staging melanoma patients with stage III and probably also for investigating the extent of stage IV disease. The question whether FLT-PET or FDG-PET performs best in the staging stage III melanoma patients remains to be answered.

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Chapter 5

Selectivity of 3'-deoxy-3'-[¹⁸F]fluorothymidine (FLT) and 2-[¹⁸F]fluoro-2-deoxy-D-glucose (FDG) for tumor versus inflammation in a rodent model

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Summary

Increased glucose metabolism of inflammatory tissues is the main source of false positive 2-[¹⁸F]fluoro-2-deoxy-D-glucose (FDG)-PET findings in oncology. It has been suggested that radiolabeled nucleosides could be more tumor-specific. To test this hypothesis, we compared the biodistribution of 3'-deoxy-3'-[¹⁸F]fluorothymidine (FLT) and FDG in Wistar rats, which were tumor-bearing (C6 rat glioma in the right shoulder) and also had a sterile inflammation in the left calf muscle (induced by injection of 0.1 ml turpentine). Twenty-four hours after turpentine injection, the rats received an intravenous bolus (30 MBg) of either [¹⁸F]FLT (n=5) or [¹⁸F]FDG (n=5). It proved necessary to pretreat the animals with thymidine phosphorylase (> 1000 U/kg, i.v.), before injection of FLT to reduce the serum levels of endogenous thymidine, in order to acquire satisfactory tumor uptake of radioactivity. Tumor/muscle ratios of FDG at 2 h post injection (13.2 ± 3.0) were higher than those of FLT (3.8 ± 1.3). FDG showed a high physiological uptake in brain and heart, whereas FLT was avidly taken up by bone marrow. FDG accumulated in the inflamed muscle, with 4.8 ± 1.2 times higher uptake in the affected thigh than in the contralateral healthy thigh, in contrast to FLT for which this ratio was not significantly different from unity (1.3 ± 0.4) . In FDG-PET images, tumor and inflammation were both visible, but FLT-PET showed only the tumor. Thus, the hypothesis of a higher tumor specifity of FLT was confirmed in our animal model.

Introduction

2-[¹⁸F]Fluoro-2-deoxy-D-glucose (FDG) is currently the most widely used radiopharmaceutical in clinical oncology. This analog of glucose is trapped in tissues after phosphorylation by hexokinase, but is not a substrate for glycolysis. Although the applications of FDG-PET in tumor detection, staging and therapy evaluation are rapidly expanding, FDG uptake is not tumor-specific. Various forms of inflammatory lesions also take up FDG and are a major cause of false positive results. Histological confirmation of FDG-positive lesions is therefore required in many types of tumors.(3,6,1,2,5,4) Macrophages, which invade tumors, especially after anticancer therapy, can induce high FDG uptake as well and can complicate the interpretation of FDG-PET.(9,8,1,7) A decreased uptake of FDG is seen in hyperglycemic patients which can cause false negative results.

Another approach for tumor visualisation is the use of radiolabeled nucleosides such as [¹¹C]thymidine. Since [¹¹C]thymidine is rapidly incorporated in newly synthesized DNA, this radiopharmaceutical can be used to image cellular proliferation. Animal and *in vitro* studies have suggested that thymidine shows considerable uptake in malignant tissue but much less uptake in inflammatory cells than FDG.(11,10) Unfortunately, the imaging quality of [¹¹C]thymidine is relatively poor and its clinical applications are limited, owing to rapid *in vivo* degradation and the short half-life of ¹¹C (20 min).(14,12,13)

However, the pyrimidine analogue 3'-deoxy-3'-fluorothymidine (FLT) can be labeled with ¹⁸F (half-life 109.8 min) and is resistant to metabolic breakdown.(15) FLT is transported by the same nucleoside carrier as thymidine and is also phosphorylated by the same enzyme, S-phase-specific thymidine kinase 1, which leads to intracellular trapping of radioactivity within the cytosol.(21,20,16,17,18,19) In contrast to thymidine, FLT remains in the cytosolic fraction as FLT-monophosphate and acts as a DNA chain terminator because of the 3' substitution (17). Thus, only a very small DNA incorporation of FLT has been observed in cell lines.(18)

Although inflammatory cells display a high metabolic activity and an avid uptake of FDG, they are recruited from elsewhere and do not divide at the site of inflammation. Since the mitotic activity of inflammatory cells is low, these cells can be expected to show a relatively low uptake of radiolabeled nucleosides. Thus, FLT may overcome one major drawback of FDG imaging.

To the best of our knowledge, no reports have appeared in the literature in which the selectivity of FDG and FLT for tumor and inflammation was compared. Therefore, we decided to examine the biodistribution of these radiopharmaceuticals in male Wistar rats which were tumor-bearing and also had a sterile inflammation. The inflammation was induced by injection of turpentine, which is known to result in exudation of plasma and migration of neutrophils within 24 hours.(22)

Materials and methods

Materials

[¹⁸F]FLT was produced by radiofluoridation of the 2,3'-anhydro-5'-O-(4,4'dimethoxytrityl)-thymidine precursor, with radiochemical yields of 5-10 %. [¹⁸F]FDG was produced by the Hamacher method (nucleophilic fluorination reaction followed by deprotection). The specific radioactivities of [¹⁸F]FLT and [¹⁸F]FDG were always > 10 (usually 50-100) TBq/mmol. Thymidine phosphorylase (from the bacterium *Escherichia coli*) was obtained from Sigma (St.Louis, MO, USA). Matrigel^R Basement Membrane Matrix was purchased from BD Biosciences (Bedford, MA, USA). Turpentine came from a local paint shop.

Animal model

The experiments were performed by licensed investigators in accordance with the Law on Animal Experiments of The Netherlands. Male Wistar rats (200-240 g body weight) were obtained from Harlan (Lelystad, The Netherlands). After one week of acclimation, C6 glioma cells (2 x 10⁶, in a 1:1 v/v mixture of Matrigel^R and Dulbecco's Minimal Essential Medium containing 5% fetal calf serum) were subcutaneously injected on the right shoulder. Matrigel^R was included to avoid migration of tumor cells to other sites than the place of injection. Ten days later, 0.1 ml of turpentine was intramuscularly injected into the thigh of the left hindleg. After an additional 24 hours, the radiopharmaceutical (either FDG or FLT) was intravenously administered (tail vein).

Phosphorylase pretreatment

In order to reduce the serum levels of endogenous thymidine, five rats were pretreated with thymidine phosphorylase (1000-1500 U/kg body weight), 45 min before

injection of the radiopharmaceutical FLT. The enzyme was administered by intravenous infusion via a tail vein. As phosphorylase is supplied in potassium phosphate buffer, a very slow rate of infusion was used (less than 50 µl per minute, total volume 0.6-1.0 ml) to avoid myocardial arrest. Plasma thymidine was measured using reversed-phase HPLC (24,23).

Biodistribution experiments

Twenty-four hours after the turpentine injection, the rats were anesthetized using (S)-ketamine (Ketanest^R, 50 mg/kg i.p.) and medetomidine (Domitor^R, 0.3 mg/kg i.p.). Animals were kept under anesthesia for the rest of the experiment. A bolus of either [¹⁸F]FLT or [¹⁸F]FDG (0.3 ml containing 30 MBg) was administered by intravenous injection into a lateral tail vein. The rats were sacrificed 120 min after radiotracer injection by extirpation of the heart (under general ketamine/ medetomidine anesthesia). Blood was collected and normal tissues (brain, fat, bone, heart, intestines, kidney, liver, lung, skeletal muscle, pancreas, spleen, submandibular gland and urinary bladder) were excised. Urine was collected and plasma plus a red cell fraction were obtained from blood centrifugation (5 min at 1000 g). The complete tumor was excised and carefully separated from muscle and skin. Inflamed muscle was recognisable by its pale color and could generally be distinguished from the surrounding darker tissue. A relatively small sample including the inflamed region (0.71 \pm 0.32 grams) was excised from the affected thigh. All samples were weighed, and the radioactivity was measured using a LKB-Wallac Compugamma^R CS 1282 counter (LKB, Bromma, Sweden, Wallac Oy, Turku, Finland), applying a decay correction. The results were expressed as dimensionless standard uptake values (dpm measured per g of tissue/dpm injected per g of body weight). Tissue/plasma and tumor/muscle concentration ratios of radioactivity were also calculated.

Histological examination of inflamed muscle and C6 tumors

Excised tumors and the inflamed parts of the thigh muscle were fixed in formalin and embedded in paraffin. Five µm-sections were stained with hematoxylin and eosin.

PET imaging

Ketamine/medetomidine-anesthetized rats were placed into a positron camera (Siemens ECAT 962/HR+, FWHM is 4.5 mm) and received a bolus injection of either [¹⁸F]FLT or [¹⁸F]FDG (30 MBq) via a tail vein. Data was acquired from 90-150 min. A zoom factor of 1.5 was applied during reconstruction (by filter-back projection) and the matrix size was 128 x 128.

Statistical analysis

Statistical analysis was performed using the software package Statistix (NH Analytical Software, Roseville MN, USA). Differences between the various groups (FLT, FLT with phosphorylase pretreatment, FDG) were tested for statistical significance using the two-sided Student t-test for independent samples. P-values < 0.05 were considered significant.

Results

Development of tumor and inflammation

The growth rate of C6 tumors in Wistar rats proved to be variable. Tumor mass at radiotracer injection was 1.61 ± 0.89 grams (mean \pm SD, range 0.41 to 2.97 grams). Turpentine injection resulted in visible swelling of the inflamed thigh after 24 hours, although behavior of the rats during this period was normal. Body weight of the animals during the biodistribution experiments was 325 ± 27 grams.

FLT uptake in untreated rats

In initial experiments on three rats, the radiopharmaceutical FLT was administered directly to the animals without any pretreatment. To our surprise, the nucleoside was not accumulated in any organ above plasma levels with the exception of bone marrow, small intestine, kidney and urinary bladder (Table 1). Even the C6 tumors did not accumulate radioactivity (Table 2). High serum levels of endogenous thymidine may have saturated tissue nucleoside transporters or thymidine kinase 1, and have blocked uptake or trapping of FLT. Drs A.F.Shields (Karmanos Cancer Institute, Detroit, MI), P.S.Conti and J.Bading (University of Southern California, Los Angeles) suggested to infuse thymidine phosphorylase before injection of FLT to circumvent this problem. The next five rats were pretreated in this way; the radiolabeled nucleoside was administered 45 min after the start of enzyme infusion. Data of untreated animals were compared to those in the thymidine phosphorylase-pretreated group.

| Tissue | FLT Untreated | FLT + phosphorylase | FDG | Effect phosphorylase | FLT + phosphorylase |
|---------------------|----------------------|------------------------|----------------------|-------------------------|------------------------|
| Cerebellum | (n=3) 0.06 ± 0.01 | (n=5) 0.04 ± 0.02 | (n=5) 1.23 ± 0.29 | on FLT uptake NS | vs. FDG < 0.001 |
| Cortex | 0.05 ± 0.01 | 0.04 ± 0.02 | 1.86 ± 0.45 | NS | < 0.001 |
| Rest brain | 0.06 ± 0.01 | 0.04 ± 0.02 | 1.45 ± 0.33 | NS | < 0.001 |
| Adipose tissue | 0.14 ± 0.16 | 0.03 ± 0.02 | 0.09 ± 0.04 | NS | < 0.05 |
| Urinary bladder | 0.74 ± 0.49 | 1.57 ± 0.68 | 1.65 ± 0.92 | NS | NS |
| Bone | 0.19 ± 0.03 | 1.18 ± 0.67 | 0.35 ± 0.11 | 0.06 | 0.09 |
| Bone marrow | 1.04 ± 0.54 | 6.67 ± 2.53 | 1.55 ± 0.41 | < 0.02 | < 0.05 |
| Heart | 0.46 ± 0.20 | 0.26 ± 0.15 | 5.84 ± 3.29 | NS | < 0.02 |
| Large intestine | 0.54 ± 0.25 | 0.55 ± 0.16 | 1.37 ± 0.32 | NS | 0.001 |
| Small intestine | 1.08 ± 0.45 | 1.28 ± 0.58 | 1.10 ± 0.23 | NS | NS |
| Kidney | 2.28 ± 0.69 | 1.19 ± 0.49 | 1.89 ± 0.43 | 0.06 | < 0.05 |
| Liver | 0.61 ± 0.28 | 0.39 ± 0.20 | 0.51 ± 0.11 | NS | NS |
| Lung | 0.46 ± 0.16 | 0.34 ± 0.19 | 1.15 ± 0.26 | NS | 0.0005 |
| Muscle | 0.42 ± 0.15 | 0.29 ± 0.09 | 0.18 ± 0,06 | NS | 0.05 |
| Pancreas | 0.41 ± 0.21 | 0.26 ± 0.12 | 0.32 ± 0.05 | NS | NS |
| Plasma | 0.58 ± 0.25 | 0.31 ± 0.15 | 0.43 ± 0.17 | NS | NS |
| Red blood cells | 0.55 ± 0.21 | 0.31 ± 0.15 | 0.31 ± 0.09 | NS | NS |
| Spleen | 0.56 ± 0.20 | 1.16 ± 0.63 | 1.64 ± 0.42 | NS | NS |
| Submandibular gland | 0.31 ± 0.11 | 0.34 ± 0.17 | 1.18 ± 0.30 | NS | < 0.001 |
| C6 tumor | 0.55 ± 0.06 | 1.14 ± 0.62 | 2.34 ± 0.72 | NS | < 0.05 |
| Inflammation | 0.51 ± 0.18 | 0.37 ± 0.16 | 0.82 ± 0.14 | NS | < 0.002 |
| Urine | 12.6 ± 2.0 | 16.3 ± 12.4 | 9.0 ± 2.0 | NS | NS |

 Table 1. Standard Uptake Values at 120 min post injection

NB The bone sample contained marrow, thus bone uptake does not reflect defluorination. NS=not significant.

FLT uptake after pretreatment

Pretreatment of animals with thymidine phosphorylase (i.v., 45 min before administration of the radiotracer) did not affect tissue/plasma ratios of FLT in brain, adipose tissue, urinary bladder, heart, kidney, liver, lung, normal and inflamed skeletal muscle, pancreas and red blood cells. However, infusion of the enzyme increased the accumulation of FLT in bone, bone marrow and the C6 tumor (Table 1 and 2). Plasma levels of radioactivity tended to be decreased after phosphorylase infusion. Thus, tissue/plasma ratios of radioactivity were significantly increased in bone, bone marrow, intestines, tumor, spleen and submandibular gland (values not shown in Table 1). Tumor/muscle ratios of radioactivity were also significantly increased after phosphorylase treatment (Table 2). Plasma levels of thymidine were measured in a parallel experiment on a single rat and were found to decrease from 0.15 µg/ml to undetectable levels after phosphorylase infusion.

| Parameter | FLT | FLT + | FDG | Effect | FLT + |
|----------------------|-----------|---------------|------------|---------------|---------------|
| | untreated | phosphorylase | | phosphorylase | phosphorylase |
| | (n=3) | (n=5) | (n=5) | | vs. FDG |
| Tumor/plasma | 1.0 ± 0.4 | 3.8 ± 1.4 | 6.1 ± 2.7 | < 0.05 | NS |
| Tumor/muscle | 1.4 ± 0.4 | 3.8 ± 1.3 | 13.2 ± 3.0 | 0.05 | 0.001 |
| Inflammation/ plasma | 0.9 ± 0.1 | 1.2 ± 0.3 | 2.1 ± 0.8 | NS | < 0.05 |
| Inflammation/ muscle | 1.2 ± 0.0 | 1.3 ± 0.4 | 4.8 ± 1.2 | NS | 0.0002 |
| Selectivity index* | 1.8 ± 1.7 | > 10.6 | 3.5 ± 1.2 | | |

 Table 2. Tissue/plasma and tissue/muscle ratios besides selectivity index

 (tumor vs. inflammation)

*Defined as (tumor uptake – muscle uptake)/(inflammation uptake – muscle uptake), i.e. tumor/inflammation ratio corrected for background. **Standard deviation cannot be given since in some animals, tracer uptake in inflamed and healthy contra lateral muscles was equal.

Biodistribution of FDG and FLT

The next five animals received FDG rather than FLT, in order to compare the biodistribution of both radiopharmaceuticals. The glucose analogue FDG showed physiological uptake in heart and brain. FDG showed higher uptake than FLT in C6 tumors, inflamed muscle, brain, adipose tissue, kidney, large intestine, lung, and submandibular gland (Table 1). In contrast, FLT accumulated more in bone, bone marrow and healthy muscle than FDG (Table 1).

Selectivity of FDG and FLT

FLT was not accumulated in inflammatory tissue (tissue/plasma and tissue/muscle ratios were not significantly different from unity). However, FDG accumulation in inflamed thigh muscle was 4.8-fold higher (p = 0.0002) than in the non-inflamed contralateral thigh (Table 2). The selectivity index (tumor/inflammatory tissue ratio corrected for the uptake in healthy muscle) was > 10.6 for FLT and 3.5 for FDG (Table 2).

Tumor/plasma ratios of FLT and FDG were not significantly different, but tumor/muscle ratios of FDG were significantly higher (p = 0.001) than those of FLT (Table 2).

Histology of inflamed muscle and C6 tumors

Histological examination of the muscle specimens excised 24 hours after turpentine injection showed an acute inflammatory reaction. Massive infiltration of neutrophils was seen in and between partially necrotic muscle fibers, the picture of an acute myositis (Fig.1). In the border of the inflammatory infiltrate, macrophages and few fibroblasts could be discerned.

Histological examination of the excised C6 tumors showed the picture of a malignant mesenchymal tumor (Figure 2). Spindled tumor cells with pleomorphic, hyperchromatic nuclei were arranged in short bundles. Many mitoses were found (range 25-40 per 2 mm²). Small areas of tumor necrosis were seen, comprising less than 10 percent of the total tumor volume.

Figure 1.

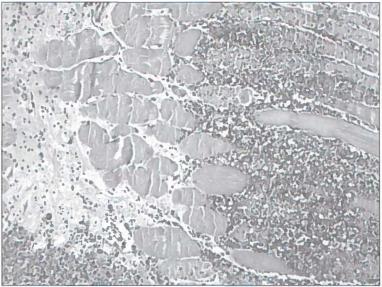


Figure 1. Microscopic image of a specimen of inflamed rat muscle, 24 hours after injection of turpentine.

Figure 2.

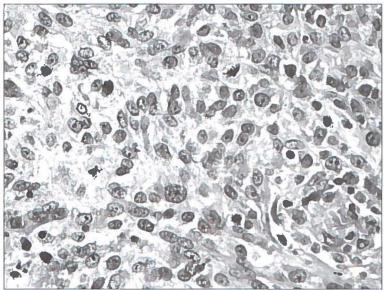


Figure 2. Microscopic image of a specimen of rat tumor, 11 days after inoculation of C6 cells. Histological examination of the excised C6 tumors showed the picture of a malignant mesenchymal tumor. Spindled tumor cells with pleomorphic, hyperchromatic nuclei were arranged in short bundles. Many mitoses were found (range 25-40 per 2 mm²). Small areas of tumor necrosis were seen, comprising less than 10 percent of the total tumor volume.

PET images

PET images of tumor- and inflammation-bearing rats, made with the two tracers, are shown in Figure3. The head of the animals is at the right hand side of the picture, and the rats are seen from below. Both FLT and FDG clearly visualized the C6 tumor in the right shoulder. FDG showed high, physiological uptake in the brain, in contrast to FLT. The inflammation in the left hindleg was visualized with FDG, but not with FLT.

Figure 3

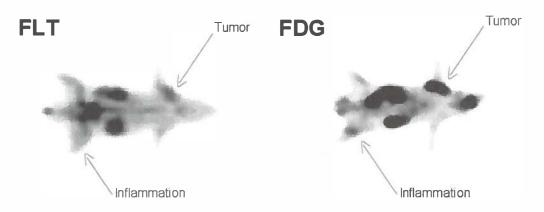


Figure 3. PET images of rats made with FLT and FDG. Note that FLT visualizes only the tumor, whereas both tumor and inflammation are visible after injection of FDG.

Discussion

This study confirms that the standard uptake value of FLT in inflammatory tissue is lower than that of FDG (see Table 1 and Fig.3). Although the tumor uptake of FLT is also considerably lower than that of FDG (Table 1), the selectivity of FLT for tumor vs. inflammation is nevertheless higher than that of glucose analogue: 10.6- vs. 3.5-fold at 120 min post injection, when the data are corrected for background (Table 2). Thus, the hypothesis of a higher tumor specificity of FLT was confirmed in our animal model. Apparently radiolabeled nucleosides have similar advantages as radiolabeled amino acids regarding tumor specificity.^{23,24}

Standard uptake values of FDG in C6 tumors were 2-fold higher than those of FLT. Tumor/muscle ratios of FDG (13.2 ± 3.0) were clearly superior to those of FLT (3.8 ± 1.3). These results are in accordance with clinical data from FDG and FLT-PET scans, where

colorectal cancers have been found to display a twofold higher uptake (SUV) of FDG than of FLT.²⁵

However, FDG showed relatively poor selectivity for tumor versus inflammatory tissue. The inflamed thigh was clearly visualized in a PET image (Fig.3). Tissue uptake of FDG in inflamed muscle was 4.8-fold greater than in the healthy contralateral leg, and the selectivity index of FDG for tumor vs. inflammation was 3.5 (Table 2). Since only part of the volume of the inflamed muscle samples consisted of neutrophils and macrophages, FDG uptake in these inflammatory cells may have been > 10-fold greater than in normal muscle cells.

FLT showed better tumor selectivity than FDG in our model. The inflamed thigh showed similar tracer uptake as the healthy contralateral thigh in a PET image (Fig.3). Biodistribution studies indicated that FLT accumulation in inflamed muscle was not significantly different from that in non-inflamed tissue of the contralateral thigh (ratio 1.3 ± 0.4 , see Table 2). The selectivity index of FLT for tumor vs. inflammation was 10.6 or greater (Table 2).

In Wistar rats, the glucose analogue showed a biodistribution as expected on the basis of clinical FDG-PET scans, i.e. high and physiological uptake in brain and heart, besides renal excretion and accumulation in the urine (Table 1). In contrast to FDG, FLT mainly accumulated in bone marrow (Table 1). Low levels of radioactivity in the brain are probably due to the fact that FLT does not cross the intact blood-brain barrier.

The data presented in the Tables indicate that endogenous thymidine can have a strong effect on the *in vivo* uptake of FLT. Low tissue uptake of FLT in untreated rats is probably a consequence of high levels of endogenous thymidine in rodent serum²⁶, since previous infusion of thymidine phosphorylase significantly increased uptake of the radiolabeled nucleoside in target organs (Table 1). Thymidine may compete with FLT for the active site of nucleoside carriers in cell membranes²⁷ and also for the active site of the trapping enzyme, thymidine kinase 1 (TK1). Affinity of human TK1 for thymidine has been reported to be 4-fold higher (0.5 μ M) than the affinity for FLT (2.1 μ M)²¹

Apparently, substantial plasma concentrations of endogenous thymidine can result in suppression of FLT uptake in most tissues (Table 1). In contrast to rats, humans have much (9-16 fold) lower levels of serum thymidine (0.01-0.02 vs. 0.15-0.27 μ g/ml).²⁶ Therefore, FLT-PET scans of cancer patients show adequate image contrast.^{19,20,25,28,29}

After infusion of a thymidine-degrading enzyme, physiological accumulation of FLT above plasma levels was observed in C6 tumors, bone, bone marrow, large and small intestine and spleen (Table 1). Many of these organs contain rapidly dividing tissue (malignant cells in the tumor, bone marrow in the skeleton, mucosa in the intestines). Thus, in pre-treated rats, FLT behaved as a tracer of cellular proliferation. This finding is in accordance with reports from the literature which suggest that there is a significant correlation between standardized uptake values of FLT and proliferative activity of various lesions.^{28,30,31} *In vitro* studies have shown that FLT uptake is related to thymidine kinase-1 activity and the percentage of cells in S-phase.^{16,17} FDG was accumulated in the same rapidly dividing tissues as FLT (Table 2) and showed even higher standard uptake values in tumor and large intestine.

Conclusion

In our animal model, FLT visualized only the tumor, whereas FDG delineated both tumor and inflammation. Based on these animal data, FLT scans of oncological patients can be expected to have more false negatives (because of lower tumor uptake) and less false positives (because of negligible accumulation in granulocytes) than whole-body FDG scans.

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Chapter 6

Detection and grading of soft tissue sarcomas of the extremities with ¹⁸F-'3-fluoro-'3-deoxy-L-thymidine

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Summary

Purpose The aim of the study is to investigate the feasibility of ¹⁸F-3'-fluoro-3'-deoxy-Lthymidine positron emission tomography (FLT-PET) for the detection and grading of soft tissue sarcoma (STS).

Experimental design Nineteen patients with 20 soft tissue sarcomas of the extremities were scanned, using attenuation corrected whole-body FLT-PET. Standardized uptake values (SUVs) and tumor/non-tumor ratios (TNTs) were compared with histopathological parameters using French and Japanese grading systems.

Results Mean SUV, max SUV and TNT could differentiate between low grade (grade 1; n=6) STS and high grade (grade 2 and 3; n=14) STS according to the French grading system (p=0.001). Mean SUV, max SUV and TNT correlated with mitotic score, MIB-1 score, the French and Japanese grading system (p=0.550-0.747).

Conclusions FLT-PET is able to visualize STS and differentiate between low grade and high grade STS. The uptake of FLT correlates with the proliferation of STS.

Introduction

Soft-tissue sarcomas (STS) form a heterogeneous group of rare malignancies, which arise from mesenchymal soft tissues and account for approximately 1% of all cancers. In the United States, 8300 new cases are diagnosed each year and in the Netherlands about 400.^{1,2} At first presentation, 13% of the patients with STS have metastases. The lung is the most common metastatic site, followed by bone, liver, and brain. Less common sites are regional lymph nodes, retroperitoneum and soft tissues.^{3,4} After treatment of the primary tumor, approximately 40% of the patients will develop recurrences either locally or distantly.

The presence or absence of metastases and the malignancy grade of the tumor will dictate the treatment. Grading is frequently performed according to the French grading system.⁵ In this grading system, points are scored for histological grade, tumor differentiation and amount of necrosis and number of mitotic figures. Recently, a Japanese grading system, using the MIB-1 score instead of the mitotic score, has been introduced, which correlates stronger with the prognosis than the French grading system.^{6,7}

Optimal management of STS depends on the anatomical site, local growth pattern, tumor size and grade and accurate staging of the disease, when first diagnosed. The site, growth pattern and size of the primary tumor are best determined by magnetic resonance imaging (MRI) or spiral computed tomography (CT). However, the clinical and radiological differentiation between benign soft tissue masses and soft tissue sarcomas, is difficult.⁸ Information regarding distant metastases is obtained primarily by chest radiography or a CT scan of the lungs, while bone-scintigraphy is of limited value.^{8,9} Distant metastases to the lungs are ruled out by CT. Physical examination, CT, MRI or ultrasonography are best used for the detection of local recurrences. However, after surgery and radiation therapy, physical examination and interpretation of the diagnostic images remains difficult.⁸

Therefore, the need for non-invasive detection, staging and grading of a soft tissue tumor mass, has increased. During the last decade the value of positron emission tomography (PET) in STS with several tracers, especially ¹⁸F-fluoro-2'-deoxy-D-glucose (FDG), has been investigated.¹⁰⁻¹⁶ However, the current potential of FDG-PET in the detection and/or grading is still unknown.^{10,11,15,17-32}

Several years ago ¹⁸F-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT) was introduced as PET tracer.³³ This tracer has theoretical advantages over the currently used FDG, since no

uptake in inflammatory cells is anticipated. The aim of this study is to investigate the feasibility of FLT-PET for the detection and grading of soft tissue sarcoma (STS).

Patients and methods

This prospective study, approved by Medical Ethics Committee of the Groningen University Hospital, consisted of 19 consecutive patients with a soft tissue sarcoma of the extremity. All patients were treated at the Groningen University Hospital and gave written informed consent. For inclusion, the liver and kidney functions and hematological parameters (Hb, Ht, erythrocytes, thrombocytes, leukocytes and white cell count) should be within normal limits. Pregnant patients or patients with psychiatric disorders were excluded from the study.

Synthesis of FLT was performed according to the method of Machulla et al.³⁴ FLT was produced by fluorination with [¹⁸F]fluoride of the 4,4'-dimethoxytrityl protected anhydrothymidine, followed by a deprotection step and purification by HPLC. FLT was produced with a radiochemical purity of >95% and specific activity of >10 TBq/mmol. The radiochemical yield was 5.6 \pm 2.8% (decay corrected).

Nineteen patients were examined in the period of February 2002 until July 2003, using an ECAT EXACT HR+ (Siemens/CTI Inc., Knoxville, TN). Prior to PET imaging, patients were instructed to fast for at least 6 hours in order to keep the study comparable with studies performed with FDG.³⁵ They were also instructed to drink one liter of water prior to imaging to stimulate FLT excretion from the renal calyces and stimulate subsequent voiding. For injection of FLT, a venous cannula was inserted in the forearm of the patient.

Patients received a median of 400 (115-430) MBq FLT. Sixty minutes after injection, the region of the tumor was imaged in emission-transmission-transmission-emission mode. After scanning the tumor region, a non attenuation-corrected whole-body scan was performed from crown to femur for 5 minutes per bed position. Data from multiple bed positions were iteratively reconstructed (ordered subset expectation maximization).³⁶

Histological typing of the tumors of all patients was performed on haematoxylin and eosin (HE) stained sections according to the WHO classification.³⁷ Immunophenotype was determined in poorly differentiated tumors. Tumors were graded using both the French and Japanese grading system.⁵⁻⁷

The number of mitotic figures was counted per 2 mm² in HE stained slides, after selecting the most cellular areas with the highest mitotic rate. Proliferating cells were detected with immunohistochemistry, using monoclonal antibody MIB-1 and antigen retrieval, as described earlier.¹² Monoclonal antibody MIB-1 recognizes the protein Ki-67 in all phases of the cell cycle with the exception of G₀.

The MIB-1 score was estimated by counting the percentage of MIB-1 positive cell nuclei per 1,000 tumor cells in the region of the tumor with the greatest density of staining, which in most instances corresponds to areas with the highest mitotic activity.

Data analysis

Region of interest (ROI)

Qualitative and quantitative evaluation of the PET scans was performed by analyzing the hypermetabolic zones on transaxial sections. The slice with the highest uptake was selected for ROI analysis.

Standardized uptake value (SUV)

After selecting the plane with the maximum SUV, a ROI was drawn manually. ROIs were placed at the 70% contour of the maximal SUV in the tumor. The same ROI was applied in the contralateral leg or arm. The mean SUV of the tumor was divided by SUV of the background region to produce the tumor/non-tumor ratio (TNT). In patients 3 and 13 it was not possible to let the ROI-tool calculate a mean SUV from 70% of the maximal SUV in the non-tumor region, because the calculated ROI was below the background uptake of FLT (Table 1). Therefore the highest mean of the manually drawn ROI, with the highest SUV, was used. TNTs and SUVs were compared with histopathological parameters.

The pathologist (AJHS) was unaware of the results of the PET-images. The images were analyzed independently by a clinical investigator (DCPC) unaware of histological typing and grading of the tumors. After calculating the SUVs and TNTs of the PET lesions, the PET data were correlated with the histopathological findings.

Whole body images

Whole body images were scored for presence/absence of lesions outside the location of the primary tumor, blinded for other clinical information. Lesions were

interpreted visually as malignant, if the FLT uptake in the lesion was higher than the surrounding tissue.

Statistical analysis

Kruskall Wallis non-parametric testing was used to see if the groups, as defined by the French or Japanese grading system, differed. Dunnett's T3 post-hoc multiple comparisons test was performed for variance analysis between the different groups, as defined by the French or Japanese grading system, for mean SUV, max SUV and TNT. Mann-Whitney testing was used to compare the mean SUV, max SUV and TNT between the French or Japanese grading system. Spearman's correlation coefficient was used to correlate mean SUV, max SUV and TNT, with mitotic score, MIB-1 score and the French or Japanese grading system. Two-tailed P-values <0.05 were considered significant.

Results

Patients

Nineteen patients with a median age of 58 (27-75) years, 7 women and 12 men, were included in this study (Table 1). Eighteen patients had one STS and one patient had two STS. Patient characteristics are presented in Table 1. Eighteen patients had a biopsy prior to the FLT-PET and one patient had a FLT-PET prior to the biopsy. A total of 17 incision biopsies and 2 true cut biopsies were performed.

Primary tumors

Twenty tumors in a total of 19 patients were clearly visible with high contrast and were interpreted as malignant. Figure 1 is an example of a FLT-PET whole body image (Pt 16). The sensitivity for detecting malignant lesions was 100%. The Kruskal-Wallis variance analysis showed significant different variance in mean SUV, max SUV and TNT between the groups, defined by the French or Japanese grading system.

The French and Japanese grading system were compared with mean SUV, max SUV and TNT. Mean SUV, max SUV and TNT could differentiate between grade 1 STS and grade 3 STS and between low grade and high grade STS (Tables 2A and 2B).

Mean SUV, max SUV and TNT were able to differentiate between low grade STS and high grade STS according to the French and Japanese grading system. Figure 2A is an

example of a FLT-PET of a low grade STS (Pt 6) and Figure 2B of a high grade STS (Pt 13).

| Pt | Sex | Age | Diagnosis | Max | Location | SUV | SUV | TNT | MS | FTG | MIB-1 | JTG |
|----|-----|-----|---------------------------------|----------|----------|-------|-----------|-----|----|-----|-------|-----|
| | | | | Diameter | | Tumor | Non-tumor | | 5 | 5 | Score | 0.7 |
| | | | | (cm) | | | | | | | 6,7 | |
| 1 | М | 55 | Well differentiated liposarcoma | 17 | leg | 0.2 | 0.1 | 2.4 | 1 | 1 | 1 | 1 |
| 2 | Μ | 55 | Myxoid liposarcoma | 10 | leg | 1.1 | 0.5 | 2.1 | 1 | 1 | 1 | 1 |
| 3 | Μ | 62 | Myxoid liposarcoma | 11 | leg | 1.5 | 0.6 | 2.4 | 1 | 1 | 1 | 1 |
| 4 | Μ | 71 | Recurrent MFH | 2 | leg | 1.0 | 0.6 | 1.7 | 1 | 1 | 1 | 1 |
| 5 | F | 61 | Well differentiated liposarcoma | 30 | leg | 0.4 | 0.7 | 0.6 | 1 | 1 | 1 | 1 |
| 6 | F | 73 | Well differentiated liposarcoma | 22 | leg | 0.9 | 0.6 | 1,5 | 1 | 1 | 1 | 1 |
| 7 | Μ | 27 | Epitheloid sarcoma | 7 | leg | 1.4 | 0.6 | 2.3 | 1 | 2 | 2 | 2 |
| 8 | Μ | 28 | Synoviasarcoma | 12 | leg | 0.8 | 0.4 | 2,1 | 1 | 2 | 2 | 2 |
| 9 | М | 33 | Myxofibrosarcoma | 17 | leg | 3.4 | 0.6 | 5.4 | 2 | 2 | 2 | 2 |
| 10 | М | 70 | Pleiomorphic MFH | 10 | leg | 3.7 | 0.6 | 5.9 | 2 | 2 | 2 | 2 |
| 11 | F | 71 | Leiomyosarcoma (recurrence) | 7 | arm | 2.1 | 0.6 | 3.4 | 2 | 2 | 2 | 2 |
| 12 | F | 75 | Myxofibrosarcoma | 14 | leg | 3,5 | 0.6 | 6.4 | 1 | 2 | 1 | 1 |
| 13 | М | 52 | Pleiomorphic MFH | 20 | Leg | 2.8 | 0.4 | 7.0 | 2 | 3 | 2 | 3 |
| | | | Pleiomorphic MFH (recurrence | 2 | Leg | 2.3 | 0.3 | 7.1 | 2 | 3 | 2 | 3 |
| | | | in opposite leg) | | | | | | | | | |
| 14 | М | 53 | Pleiomorphic liposarcoma | 28 | leg | 2.2 | 0.6 | 3.4 | 3 | 3 | 3 | 3 |
| 15 | М | 70 | Myxofibrosarcoma | 10 | leg | 2.3 | 0.5 | 4.7 | 2 | 3 | 3 | 3 |
| 16 | м | 71 | Pleiomorphic leiomyosarcoma | 20 | leg | 4.9 | 0.7 | 6.6 | 2 | 3 | 3 | 3 |
| 17 | F | 47 | Pleiomorphic leiomyosarcoma | 11 | arm | 4.8 | 0.9 | 5.3 | 3 | 3 | 3 | 3 |
| 18 | F | 56 | Extraskeletal osteosarcoma | 6 | leg | 2.8 | 0.3 | 9.3 | 3 | 3 | 3 | 3 |
| 19 | F | 58 | Pleiomorphic sarcoma NOS | 5 | leg | 3.7 | 1.5 | 2.5 | 3 | 3 | 3 | 3 |

Table 1. Patient characteristics mean SUV, TNT, mitotic score, MIB-1 score and grading

FTG=French tumor grade; JTG=Japanese Tumor Grade; MFH=malignant fibrous histiocytoma; MS=mitotic score; NOS=not otherwise specified; Pt=patient.

Figure 1.



Figure 1 demonstrates a whole body image of patient 16. Physiological uptake of FLT can be seen in the bone marrow of the pelvis, ribs, vertebrae and in the bones of the shoulder, in the liver and bladder (small arrows). The STS can be seen in the left upper leg and a lung metastasis in the mediastinum (large arrows).

| French | Grade 1* | Grade 2* | Grade 3* | Low grade [#] |
|-----------------------|---------------|---------------|---------------|------------------------|
| Grading | (n=6) | (n=6) | (n=8) | VS |
| System ⁵ | | | | High grade |
| Mean SUV | 0.9 (0.2-1.5) | 2.8 (0.8-3.7) | 2.8 (2.2-4.9) | 0.001 |
| Max SUV | 1.2 (0.3-1.7) | 3.4 (1.0-5.2) | 3.3 (2.8-6.7) | 0.001 |
| TNT | 1.9 (0.6-2.4) | 4.4 (2.1-6.4) | 6.0 (2.5-9.3) | 0.001 |
| Japanese | Grade 1* | Grade 2* | Grade 3* | Low grade [#] |
| Grading | (n=7) | (n=5) | (n=8) | vs |
| System ^{6,7} | | | | High grade |
| Mean SUV | 1.0 (0.2-3.5) | 2.1 (0.8-3.7) | 2.8 (2.2-4.9) | 0.011 |
| Max SUV | 1.3 (0.3-5.2) | 2.8 (1.0-4.7) | 3.3 (2.8-6.7) | 0.014 |
| TNT | 2.1 (0.6-6.4) | 3.4 (2.1-5.9) | 6.0 (2.5-9.3) | 0.008 |

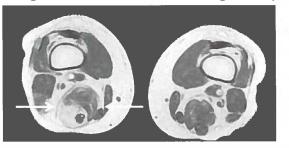
Table 2A. Mean SUV, Max SUV and TNT in the French or Japanese grading system

*Values expressed as medians (range); #statistic difference between medians (P values); Low grade=grade 1; High grade=grade 2+3.

| French | Grade 1 | Grade 1 | Grade 2 |
|---------------------------------|---------------|---------------|---------------|
| Grading | vs | vs | vs |
| System⁵ | Grade 2 | Grade 3 | Grade 3 |
| Mean SUV | 0.056 | 0.001 | 0.594 |
| Max SUV | 0.066 | 0.002 | 0.660 |
| TNT | 0.063 | 0.003 | 0.468 |
| | | | |
| Japanese | Grade 1 | Grade 1 | Grade 2 |
| Japanese Grading | Grade 1 vs | Grade 1 vs | Grade 2 vs |
| | | | |
| Grading | VS | VS | vs |
| Grading System ⁶⁷ | vs Grade 2 | vs Grade 3 | vs Grade 3 |

Table 2B. P values of Dunnett T3 comparisons for mean SUV, max SUV and TNT in the French or Japanese grading system

Figure 2A. MRI and FLT-PET images of a patient with low grade STS



1.

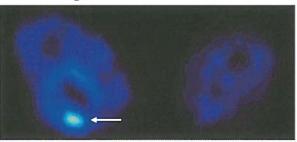
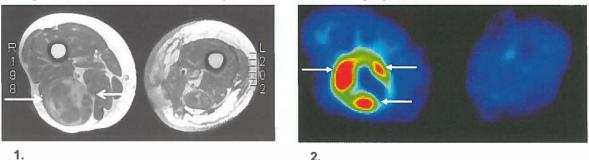




Figure 2B. MRI and FLT-PET images of a patient with high grade STS



2.

Figure 2A shows the MRI (1) and FLT-PET (2) images of a low grade STS (Pt 6) and Figure 2B of a high grade STS (Pt 13). The MRI images of both patients demonstrate a heterogeneous tumor. However, the FLT uptake in the high grade STS is higher (indicated as red) than in the low grade STS (indicated as blue).

All correlations between mean SUV, max SUV, TNT, mitotic score, MIB-1 score and the French and Japanese grading system were significant (Table 2B). The correlation coefficients varied from 0.550 to 0.747 with all p values <0.05. The strongest correlation was found between TNT and the French grading system.

| | | and MIB-1 score | | | | |
|----------|--------------------|----------------------|--------------------|-----------------------|--|--|
| | Mitotic | MIB-1 | French | Japanese | | |
| | Score ⁵ | Score ^{6,7} | Grading | Grading | | |
| | | | System⁵ | System ^{6.7} | | |
| Mean SUV | 0.721* | 0.652# | 0.724# | 0.647* | | |
| Max SUV | 0.668* | 0.610 [#] | 0.723 [#] | 0.627* | | |
| TNT | 0.646* | 0.550* | 0.747# | 0.668* | | |

Table 3. Spearman's correlations (ρ) between grade, Mean SUV, TNT, mitotic score

^{*}p<0.005; *p<0.05.

Additional findings with whole body FLT-PET

In four patients single or multiple lesions were seen or missed on the whole body FLT-PET. In two patients the lesions detected on FLT-PET were malignant. In patient 13, FLT-PET detected, besides a new primary STS in the right thigh, a 1.5 cm small local recurrence of a sarcoma in the left thigh, which was previously treated with surgery and radiation therapy. In patient 16, FLT-PET detected lung metastases, which were confirmed on CT as well.

In three patients the lesions seen on FLT-PET were not malignant according to pathological examination or follow-up. In patient 10, the lesions on FLT-PET in the groin and supraclavicular region were negative on physical examination and follow-up. In patient 13, the lesion on FLT-PET in the groin was histologically negative after lymph node dissection. In patient 14, the lesions on FLT-PET in the groin were indicated as lymph nodes with follicular hyperplasia after lymph node dissection.

In one patient a metastatic lymph node was missed on FLT-PET. In patient 7, a axillary lymph node dissection was performed. In the lymph node dissection, one lymph node contained two metastases with both a diameter of 5 mm with 11 mitotic figures per 2mm². This metastatic lymph node was not detected on whole-body FLT-PET.

Discussion

The results of this study revealed that FLT-PET is able to visualize STS and recurrent STS and has the clinical potential to distinguish between low (grade 1) and high grade (grade 2 and 3) STS.

FLT uptake appeared to be related to proliferation and tumor grade. Mean SUV, max SUV and TNT correlated with mitotic score, MIB-1 score and the French and Japanese grading of STS. No difference between the French and Japanese grading system was found based on the correlations.

In the French grading system of STS, all three parameters (level of histological differentiation, amount of necrosis and mitotic index) are independent predictors of metastasis.³⁸ It has been demonstrated that when using the MIB-1 score instead of the mitotic score in the French grading system, the grading of soft tissue sarcoma improved. This modified Japanese grading system proved to be the most significant predictor of overall survival.^{6,7} Therefore, a PET-tracer that would reflect proliferation, could have the potential to visualize grading of STS. For this purpose ¹⁸F-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT) was developed.^{33,39} This pyrimidine analog, is phosphorylated by the enzyme thymidine kinase 1 (TK₁), which leads to intracellular trapping.³³ During DNA synthesis, TK₁ concentration increases almost tenfold and is, therefore, an accurate reflection of cellular proliferation.⁴⁰

Most previous studies for detecting sarcomas have been performed with ¹⁸F-fluoro-2'-deoxy-D-glucose-PET (FDG-PET) and have recently been critically reviewed in two meta-analyses.^{31,32} The sensitivity of FDG-PET for detecting primary and recurrent sarcomas varies from 88 to 92% and specificity varies form 73 to 87%.^{31,32} FDG-PET can be useful in tumor grading, but is, with the exception of a study of Eary et al, not able to differentiate between benign lesions and low grade sarcoma.^{16,17,31,32} The accuracy for the differentiation is influenced by technical limitations, time between injection and scanning, false negative and false positive findings.^{18,21,22,26,29} The SUV for FDG-PET for low grade (grade 1) STS varied between 1.6 and 2.6, as compared to 0.2 and 1.5 for FLT-PET; the SUV for FDG-PET for high grade STS (grade 2 and 3) varied between 8.0 and 9.4 as compared to 0.8 and 4.9 for FLT-PET.^{23,29} Despite the lower sensitivity of FDG-PET than FLT-PET, the uptake of FDG was higher than FLT. In a comparative study with FLT-PET, the correlation between FDG SUV and proliferation of the STS should be investigated. In conclusion, FLT-PET is able to visualize and differentiate high grade from low grade STS. The uptake of FLT correlates with the proliferation of soft tissue sarcomas.

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Chapter 7

¹⁸F-FLT-PET for the visualization of laryngeal cancer: comparison with ¹⁸F-FDG-PET

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Summary

Rationale: In this study the feasibility of ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine positron emission tomography (FLT-PET) for detecting laryngeal cancer was investigated and compared with FDG-PET.

Methods: Eleven patients with (or strongly suspected with) recurrent laryngeal cancer and 10 patients with histologically proven primary laryngeal cancer underwent one attenuation corrected FLT-PET, 60 minutes after injection of a median of 213 (175-400)MBq FLT, and one attenuation corrected FDG-PET, 90 minutes after injection of a median of 340 (165-650)MBq FDG. All patients were staged by endoscopy and CT according to the UICC TNM staging system. All patients underwent a biopsy of the laryngeal area after the PET-scans. Lesions on FDG-PET, and FLT-PET were compared with histopathological results. Mean SUV, max SUV and tumor/to non-tumor ratio (TNT) were calculated for FLT and FDG. Wilcoxon non-parametric testing was used for comparison of FDG with FLT uptake. Spearman's correlation coefficient was used to correlate mean SUV, max SUV and TNT of FDG-PET and FLT-PET. Two-tailed P-values <0.05 were considered significant.

Results: FDG-PET as well as FLT-PET detected laryngeal cancer correctly in 15 out of 17 patients. One lesion was judged as positive on FDG-PET, which turned out as normal tissue. Two lesions were judged as positive on FLT-PET, which turned out as inflammation in one lesion and normal tissue in the other lesion. Max SUV was 3.3 (1.9-8.5) for FDG and 1.6 (1.0-5.7) for FLT (p<0.001). Mean SUV was 2.7 (1.5-6.5) for FDG and 1.2 (0.8-3.8) for FLT (p<0.001). TNT was 1.9 (1.3-4.7) for FDG and 1.5 (1.1-3.5) for FLT (p<0.05). **Conclusion:** The number of laryngeal cancers detected with FLT-PET and FDG-PET was equal. In laryngeal cancer the uptake of FDG is higher than FLT.

Introduction

The current standard for staging of laryngeal cancer is direct laryngoscopy complemented with histological biopsy and computed tomography (CT) or magnetic resonance imaging (MRI) (1,2). The detection of tumors and metastatic lymph nodes by CT and MRI is solely dependent on changes in tissue structure and size of lymph nodes (2). Therefore, primary or recurrent tumors that do not distort tissue structures and non-enlarged metastatic nodes can be missed. In addition, tissue changes caused by radiation therapy can complicate interpretation of CT and MRI images as well. Despite the fact that a biopsy is the gold standard, locating the possible site of a recurrence for biopsy is still very difficult, since most recurrent head and neck cancers are located in the submucosa (1). Furthermore, the ENT-surgeon will be reluctant to obtain multiple blind biopsies, since biopsies could initiate or aggravate radionecrosis (2).

Positron emission tomography (PET), using 2'-¹⁸F-fluoro-2'-deoxy-D-glucose (FDG), is accepted as a powerful non-invasive metabolic imaging method for the diagnosis and staging of cancer (3-5). FDG-PET has been introduced as a non-invasive diagnostic tool in head and neck cancer, where it is especially accurate for the detection of cancer and provides prognostic information (6-8). However, experience with FDG-PET applied solely in patients with laryngeal cancer is limited. FDG-PET in patients with suspected recurrent laryngeal cancer has proven to be valuable to distinguish between benign and malignant tissue changes after radiation therapy (9-11). Even less data on FDG-PET is available in patients with untreated primary laryngeal cancer (9,12).

Since FDG is also metabolized in non-tumor tissue, false positive results can occur (13-15). These are the results of FDG uptake in inflammatory, reactive tissue or supraclavicular fat. In addition muscle uptake of FDG may interfere with FDG-PET interpretation. Furthermore, the time interval between radiation therapy and FDG-PET is essential for accurate diagnosis (1,9,16).

Recently, ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine (FLT) has been introduced as a PETtracer by Shields and Grierson, which might not have these drawbacks (*17*, *18*). This pyrimidine analog, is phosphorylated by the enzyme thymidine kinase 1 (TK₁), which leads to intracellular trapping (*18*). During DNA synthesis, TK₁ activity increases almost tenfold and is thus an accurate reflection of cellular proliferation (*19*). FLT uptake is probably related to TK₁ activity and therefore also related to proliferation. The aim of this study was to investigate the feasibility of FLT-PET for detection of primary and recurrent laryngeal cancer in comparison with FDG-PET. A second aim was to investigate possible differences in uptake of FLT and FDG in malignant and normal tissue.

Materials and methods

Patients

This prospective study consisted of 21 consecutive patients: 11 patients with suspected recurrent laryngeal cancer and 10 patients with primary laryngeal cancer, after informed consent was obtained. Patients were included from September 2001 until March 2003.

The 11 patients with suspicion of recurrent laryngeal cancer had initially been treated for a laryngeal squamous cell carcinoma with radiation therapy. These patients were suspected to have recurrent disease, because they developed increased hoarseness, edema, pain in the larynx or referred pain. All patients with suspected recurrent laryngeal cancer underwent a diagnostic laryngoscopy for a biopsy. The 10 patients with primary laryngeal squamous cell carcinoma were candidates for radiation therapy. All patients had been clinically staged according to the UICC TNM classification (20).

All patients underwent a physical examination of the head and neck, chest X-ray, endoscopic examination under general anesthesia, biopsies of suspected areas and a spiral CT of the neck. For inclusion, liver and kidney functions and hematological parameters (Hb, Ht, erythrocytes, thrombocytes, leukocytes and white cell count) had to be within normal limits. Pregnant patients and patients with psychiatric disorders were excluded. All screened patients could be included in the study. The medical ethics committee of the Groningen University Hospital approved the study protocol.

Tracer synthesis

Synthesis of FLT was performed according to the method of Machulla et al (21). FLT was produced by [¹⁸F]fluorination of the 4,4'-dimethoxytrityl protected anhydrothymidine, followed by a deprotection step. After purification by reversed phase HPLC, the product was made isotonic and passed through a 0.22 μ m filter. FLT was produced with a radiochemical purity of >95% and specific activity of >10 TBq/mmol. The radiochemical yield was 7.5 ± 5.1% (EOB).

Synthesis of FDG was performed according to the method of Hamacher et al by an automated synthesis module (22). The radiochemical yield was 65.9 ± 7.1% (EOB).

PET scanning

All studies were performed using an ECAT EXACT HR+ (Siemens/CTI Inc., Knoxville, TN). Prior to PET imaging, patients were instructed to fast for at least 6 hours. They were also instructed to drink one liter of water prior to imaging to stimulate FLT and FDG excretion from the renal calyces and subsequent voiding.

For injection of the radiopharmaceuticals, a venous cannula was inserted in the forearm of the patient. The interval between the FDG-PET and FLT-PET was maximal 16 days. All patients were scanned 4 positions from the nose down in emission-transmission-transmission-emission mode, with 3 and 5 minutes per bed position for transmission and emission scanning, respectively. Twenty-one patients with a median age of 65 (50-81) years, 20 men and 1 woman, were included in this study (Table 1). Patients received a median of 340 (165-650)MBq FDG and a median of 213 (175-400)MBq FLT. Patients were scanned sixty minutes after FLT and 90 minutes after FDG injection. Previous experience with FLT, indicated that the tumor over non-tumor ratios were constant from 60 minutes post-injection of the tracer. PET images were iteratively reconstructed (ordered subset expectation maximization) (23).

Pathological evaluation

Biopsies of the laryngeal area and surgical specimens of total laryngectomies were examined on haematoxylin and eosin (H and E) stained sections. The pathologist (AJHS) was unaware of the results of the PET images. In patients, in whom a total laryngectomy was performed, the maximum tumor diameter was obtained (Table 1). In the remaining patients only biopsies were performed and used for histological investigation.

Data analysis

FLT-PET and FDG-PET images were analyzed for uptake in malignant lesions and normal anatomical structures. An experienced PET-physician (DCPC) evaluated the images only aware of the location of the primary or suspected lesion, but blinded for other clinical information.

| | - | | | | | 1 | | | | | | | | | | |
|--------------------------------|----|-----|-----|-----------|------------|-------------|------|-----|-----|------------------|---------|----------|-----|---------|----------|-----|
| | Pt | Sex | Age | TNM | Treatment | Tx-interval | MDT | FDG | FLT | Pathology | FDG | FDG | FDG | FLT | FLT | FLT |
| | | | | PLC | PLC | Before | (mm) | | | | Max SUV | Mean SUV | TNT | Max SUV | Mean SUV | TNT |
| | | | | | | PET-scan | | | | | Tumor | Tumor | | Tumor | Tumor | |
| | 1 | F | 52 | T2N0 | RTX | 6 months | NA | - | + | Inflammation | NA | NA | NA | 1.4 | 1.1 | 1.1 |
| | 2 | м | 64 | T1N0 | RTX | 9 years | NA | - | - | No abnormalities | NA | NA | NA | NA | NA | NA |
| d D | 3 | М | 56 | T3N2c | Follow-up# | 3 months | 1,8 | + | + | RLC | 3.2 | 2.8 | 1.5 | 1.2 | 1.1 | 1.2 |
| gro | 4 | м | 70 | T1a/CISN0 | CO2 laser | 6 years | NA* | + | + | RLC | 1.9 | 1.5 | 1.5 | 1.5 | 1.2 | 1.5 |
| anca | 5 | м | 65 | T2N0 | RTX | 9 months | 18 | + | + | RLC | 3.0 | 2.3 | 1.5 | 1.3 | 1.1 | 1.4 |
| cure | 6 | м | 50 | T2N0 | RTX | 10 months | 15 | + | + | RLC | 8.5 | 6.5 | 4.1 | 2.9 | 1.9 | 3.2 |
| Suspected recurence group | 7 | м | 58 | T1N0 | RTX | 1.5 months | 40 | + | + | RLC | 3.7 | 2.9 | 2.4 | 1.5 | 1.3 | 1.4 |
| ecte | 8 | м | 66 | T4N0 | RTX | 3 months | 20 | + | + | RLC | 3.3 | 2.6 | 1.4 | 1.9 | 1.4 | 1.4 |
| usp | 9 | м | 56 | T3N1 | RTX | 16 months | 17 | + | + | RLC | 2.9 | 2.2 | 1.4 | 1.0 | 0.8 | 1.1 |
| 0) | 10 | м | 65 | T1aN0 | CO2 laser | 13 months | NA | + | + | No abnormalities | 1.9 | 1.6 | 1.3 | 1.5 | 1.2 | 1.1 |
| | 11 | м | 55 | T2N0 | RTX | 5 months | NA | - | - | Inflammation | NA | NA | NA | NA | NA | NA |
| - | 12 | М | 79 | T2N0 | RTX | NA | NA* | + | + | PLC | 2.5 | 1.8 | 1.3 | 1.7 | 1.2 | 1.7 |
| d n | 13 | м | 72 | T3-4N0 | RTX | NA | NA* | + | + | PLC | 5.8 | 4.4 | 3.1 | 5.7 | 3.8 | 3.5 |
| 2B | 14 | м | 66 | T1aN0 | RTX | NA | NA* | - | - | PLC | NA | NA | NA | NA | NA | NA |
| ncer | 15 | м | 55 | T2N0 | RTX | NA | NA* | + | + | PLC | 6.2 | 4.8 | 2.8 | 3.2 | 2.0 | 2.2 |
| Ca | 16 | м | 65 | T4N0 | RTX | NA | NA* | + | + | PLC | 5.8 | 4.4 | 2.3 | 3.7 | 2.6 | 2.2 |
| Bea | 17 | м | 79 | T4N0 | RTX | NA | NA* | + | + | PLC | 3.2 | 2.5 | 2.8 | 2,3 | 1.9 | 1.9 |
| aryr | 18 | м | 64 | T1aN0 | RTX | NA | NA* | + | + | PLC | 2.1 | 1.6 | 1.3 | 1.2 | 09 | 1.5 |
| Primary laryngeal cancer group | 19 | м | 72 | T1bN0 | RTX | NA | NA* | - | - | PLC | NA | NA | NA | NA | NA | NA |
| Ē | 20 | м | 53 | T2N0 | RTX | NA | NA* | + | + | PLC | 3.8 | 2.8 | 4.7 | 1.6 | 1.2 | 2,0 |
| | 21 | м | 81 | T2bN0 | RTX | NA | NA* | + | + | PLC | 4.6 | 3.5 | 2.9 | 1.6 | 1.1 | 1.6 |
| | 1 | | | | | | | | | | | | | | | |

Table 1. Patient characteristics

CIS=carcinoma in situ; MDT=maximum diameter of the tumor;NA=Not applicable; NP=not performed; PLC=primary laryngeal cancer; RLC=recurrent laryngeal cancer; Tx-interval= time interval between therapy of primary laryngeal cancer and PET-scan; *=only biopsies performed; *follow-up instead of RTX, because of primary treatment of lung cancer; -=negative; +=positive.

FLT-PET and FDG-PET images were first visually interpreted. Presence of a hypermetabolic lesion was judged as positive, absence of a hypermetabolic lesion as negative. After visual interpretation both the FLT-PET and FDG-PET images were analyzed randomly for hypo- and hypermetabolic lesions and sagittal sections. The slice with the highest uptake was selected for ROI analysis. After selecting the plane with the maximum SUV, a ROI was drawn manually. ROIs were placed at the 70% contour of the maximal SUV in the tumor when possible. In other cases ROIs were drawn manually. The same ROI method was applied on the same slice in normal laryngeal tissue above or below the tumor site, to calculate the background SUV. The mean SUV of the tumor was divided by the mean SUV of the background region to produce the tumor/non-tumor ratio (TNT). TNTs and SUVs of FLT-PET and FDG-PET were compared. Images were displayed on a SUN workstation. ROI calculation was performed Clinical Applications Programming Package version 5 (CAPP5, CTI, Knoxville (TN), USA).

Statistical analysis

The results of the visually interpreted PET images were compared with the histological data, which was used as standard. Wilcoxon signed rank test was used to compare mean SUV, max SUV and TNT between FDG-PET and FLT-PET. Spearman's correlation coefficient was used to correlate mean SUV, max SUV and TNT of FDG-PET and FLT-PET. Two-tailed P-values <0.05 were considered significant.

Results

Patients

Fifteen patients underwent a biopsy of the laryngeal area after the PET-scans in the Groningen University Hospital. However, patients 7, 8, 11, 12, 15 and 20 underwent a biopsy in a referring hospital. These biopsies were performed at 7 months, 17, 11, 27, 42 and 21 days prior to the PET-scans, respectively.

Visualization of laryngeal cancer

In patients 2, 11, 14 and 19 no uptake of FLT or FDG could be observed and therefore no SUV could be calculated. Histopathological investigation showed no

malignancy in patients 2 and 11. However, in patients 14 and 19 histopathological investigation showed two recurrent laryngeal cancers.

FDG-PET and FLT-PET detected 15 out of 17 laryngeal cancers. One lesion (Patient 10) was judged as positive on FDG-PET, which was normal tissue. FLT-PET and FDG-PET missed two T1 tumors of patient 14 and 19. Two lesions (Patients 3 and 10) were judged as positive FLT-PET on, which was inflammation in one lesion and normal tissue in the other lesion. Figure 1 demonstrates a FDG and FLT-PET image of a patient with primary laryngeal cancer.

Figure 1. FLT-PET and FDG-PET image of primary laryngeal cancer





Α

В

Coronal FDG-PET (A) and FLT-PET (B) image of patient 3, diagnosed with primary laryngeal cancer. With both imaging modalities, uptake of the tracer in the laryngeal region can be observed. Max FDG SUV was 3.2 and max FLT SUV was 1.2. Physiological FDG uptake can be seen in the muscles of the neck and physiological FLT uptake can be observed in the bone marrow of the ribs and bones of the shoulder.

Comparison between FDG and FLT uptake

The uptake of FDG, was significantly higher than FLT, when expressed in mean SUV, max SUV and TNT (Table 2). The correlations between mean SUV, max SUV, TNT, of FDG and FLT, varied between 0.613 and 0.705, and were significant (p<0.05).

| Table 2. Wilcoxon r | non-parametric test |
|---------------------|---------------------|
|---------------------|---------------------|

| | Max SUV | Mean SUV | TNT |
|---------|----------------|----------------|----------------|
| FDG-PET | 3.3 (1.9-8.5)* | 2.7 (1.5-6.5)* | 1.9 (1.3-4.7)* |
| FLT-PET | 1.6 (1.0-5.7) | 1.2 (0.8-3.8) | 1.5 (1.1-3.5) |

SUV expressed as median (min-max); *p<0.001; p<0.05.

Discussion

This study was conducted in 21 patients and shows that both FDG-PET and FLT-PET detected 15 out of 17 laryngeal cancers. The lesions of four patients, suspicious for laryngeal cancer turned out to be normal or inflammatory laryngeal tissue. FDG-PET detected one of those lesions as positive and FLT-PET detected two of those lesion as positive. The uptake of FDG, mean SUV of 2.7 (1.5-6.5), in laryngeal cancer was significantly higher than FLT, mean SUV of 1.2 (0.8-3.8).

Although little data are available, the limited FDG-PET data of this study, concerning the sensitivity, are in the same range as the FDG-PET data in the literature. Sensitivity for the detection of laryngeal cancer ranged between 80% and 97% (9,11,12,16,24,25), specificity ranged from 61% to 82% (10,11,16). The specificity, obtained in this study, which was 100% (3/3) for FDG-PET, is less reliable and not comparable with the literature, due to the low number of false positive and true negative lesions.

False positive results with FDG-PET can occur, since FDG is also trapped in normal tissue. Secretion of FDG in normal mucosa and saliva and pooling of saliva in the larynx may cause increased uptake in the laryngeal area (13). Increased uptake is also found in salivary glands, tonsil tissue, muscle tissue of the larynx and the neck, benign laryngeal papilloma and the base of the tongue (15). Moreover, wound healing after biopsies prior to the FDG-PET, local inflammation such as osteomyelitis, cellulitis or a polyp may cause increased local FDG uptake (9,10,13,26). Furthermore, the time interval between radiation therapy and the FDG-PET is essential for accurate diagnosis (9,10,16,27).

As an alternative for FDG, potentially more specific tracers have been developed, which take part in other metabolic processes. Several amino acids, imaging protein synthesis, have been developed as tracers. Most of these studies have been performed with L-[methyl-¹¹C-]-methionine (MET). The disadvantage of MET is substantial accumulation of non-protein related metabolites in tumor tissue (28). L-[1-¹¹C]-tyrosine (TYR) has also been used to detect tumors and determine protein metabolism. In laryngeal and hypopharyngeal cancer TYR was able to detect all primary tumors and there was a correlation between protein synthesis rate and SUV (29-31). However, the disadvantage of this tracer is the low tumor uptake and accumulation in salivary glands, which could impair the detection of metastatic lymph nodes in head and neck cancer (28,29). In 1998 Shields et al developed FLT, a pyrimidine analogue, which indirectly

measures DNA-synthesis through the DNA salvage pathway (18). Recent articles about FLT-PET focussed on the detection of colorectal and lung cancer and their metastases (32,33). A correlation was found between the SUV and proliferation in single pulmonary nodules (32,34,35).

Despite these promising properties of FLT, FLT-PET hardly detected a recurrent laryngeal tumor (patient 3), which displayed avid uptake of FDG. The tumor was a 1.8 mm large poorly differentiated tumor surrounded with ulcers. This could explain the low FLT uptake and avid FDG uptake in the surrounding inflammation tissue. FLT-PET and FDG-PET missed two T1 tumors, which were detected on CT. The size of these tumors could be below the detection level of PET and a partial volume effect could be involved. In the literature FDG-PET misses T1 to T4 laryngeal tumors as well. However, no (histological) explanation is given for these false negative findings (11,24,25). Unfortunately, it is impossible to obtain the size of a primary laryngeal cancer. This is because diagnosis and extent of the tumor are obtained by a laryngoscopically guided biopsy and CT, since almost all T₁-T₃ tumors are treated with radiation therapy. The size of the biopsy obtained from the tumor, is often too small to accurately assess the Ki-67 data for the correlation with FLT-uptake. In contrast, reliable Ki-67 data is possible in patients with a T₄ tumor, who undergo a total laryngectomy and are not palliatively treated with radiation therapy. In these patients the tumor can be fully histologically examined. However, a T₄ tumor often causes acute respiratory distress, urging an acute laryngectomy, making a PET-scan unethical and impossible.

Malignant tissue displayed a significant higher uptake of FDG as compared to FLT. The mean FDG SUV in the literature for patients with primary or recurrent laryngeal cancer ranges from 4.6 to 10.7 (9,12,13). These values are higher than the max FDG SUV of 3.3 (range 1.9-8.5) and mean SUV 2.7 (range 1.5-6.5) in this study. No literature is available on FLT-PET for detecting laryngeal cancer. However, in patients with colorectal cancer and lung cancer the SUV of FDG-PET and FLT-PET were compared. The mean FLT-PET SUV in colorectal cancer was 4.2 as compared with a mean FDG-PET SUV of 8.7; the FLT SUV in lung cancer ranged between 1.2 and 3.1 and FDG-PET SUV from 1.7 to 8.9 (32,33). Although these articles discuss different types of malignancies, they also report significantly lower uptake of FLT as compared to FDG, just as was found for the detection limit.

The correlation between FDG and FLT uptake was not very strong. The SUV is the net result of several uptake processes. The availability of the tracer in the blood pool, non-specific uptake, perfusion of the tumor, membrane transport, metabolic processes in which the tracer is involved and (ir)reversible trapping of the tracer flow over the membrane are factors which can influence the SUV. It is our impression that both FLT and FDG are taken up by the malignant cells, but that the demand for glucose is larger than for thymidine. The phosphorylation rate in vitro is about 30% of the phosphorylation rate of serum thymidine by thymidine kinase 1, which could be one explanation for a low FLT uptake in the tumor (36,37).

The number of patients in this study is too small to draw conclusions about the accuracy of FDG-PET and FLT-PET for detecting laryngeal cancer in general and for detecting primary or recurrent laryngeal cancer specifically. Larger groups of patients are needed with at least two observers to calculate the inter-observer agreement, which would reflect clinical reality more accurately.

Future aspects for FDG-PET and FLT-PET for laryngeal cancer are only partly clear. The role for FDG-PET in the future for detecting laryngeal cancer seems to be in the differentiation between non-tumor and tumor tissue in patients suspected of recurrent laryngeal cancer (1,9-11,13). It is reasonable to delay biopsy on a negative FDG-PET and prevent unnecessary biopsies, which could initiate or aggravate radionecrosis (1,10,11). Imaging with PET lacks of anatomical detail, but could be overcome by a PET-CT. Too little data are available for the detection of untreated primary laryngeal cancer, which has not been treated with radiation therapy (9,24,25). Further research is needed to investigate if FDG-PET is an adequate tracer for the detection of primary laryngeal cancer. Because of the low uptake of FLT in laryngeal FLT-PET seems less adequate for the detection of laryngeal cancer (11).

The number of laryngeal cancers detected with FLT-PET and FDG-PET was equal. The uptake of FDG in laryngeal cancer is higher than FLT.

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Chapter 8

Is ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine useful for staging and restaging of patients with non-small cell lung cancer?

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Submitted

Summary

Rationale: To compare ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine positron emission tomography (FLT-PET) with clinical TNM staging, including FDG-PET, in patients with NSCLC.

Methods: Patients with NSCLC underwent a whole-body FDG-PET and whole-body FLT-PET, using a median of 360 MBq FDG (160-500) and 210 MBq FLT (130-420). FDG-PET was performed 1.5 hours post-FDG injection, FLT-PET 1 hour post-FLT-PET injection. Two independent viewers categorized all lesions independently on localization and intensity of tracer uptake. All FDG-PET and FLT-PET lesions were compared. Staging with FLT-PET was compared with clinical TNM-staging, based on history, physical examination, bronchoscopy, CT and FDG-PET. From eight patients SUVs were calculated. Maximal SUV (max SUV) and mean SUV were calculated.

Results: 16 patients with stage IB-IV NSCLC and one patient with strong suspicion of NSCLC were investigated. In 8 patients without pretreatment, on a lesion-by-lesion basis sensitivity was 80% and in the 9 patients with pretreatment before FLT-PET this number was 27%, using FDG-PET as the reference standard. As compared with clinical TNM staging, FLT-PET staged 8 of 17 patients correctly. In the group with previous therapy 5 out of 9 patients were staged correctly and in the group without pretreatment 3 out of 8 patients were staged correctly with FLT as compared to the TNM staging system. Max SUV of FLT-PET, 2.7 (0.8-4.5) was significantly lower than FDG-PET, 8.0 (3.7-18.8) (n=8; P=0.012). Mean SUV of FLT-PET, 2.7 (1.4-3.3) was significantly lower than FDG-PET, 6.2 (2.8-13.9) (n=6; P=0.027).

Conclusion: FLT-PET is not useful for staging and restaging patients with NSCLC.

Introduction

Positron emission tomography (PET), using 2-¹⁸F-fluoro-2-deoxy-D-glucose (FDG),has been accepted as a non-invasive metabolic imaging method for the staging of lung cancer.(1) FDG-uptake reflects glucose consumption.(2) However, FDG is not a selective tracer, since it also accumulates in inflammatory cells. Macrophages invade tumors and appear in inflammatory lesions, causing false positive FDG-PET results.(3-5) Another problem is a decreased uptake during hyperglycemia.(6) Furthermore, FDG-PET lacks sensitivity for imaging brain metastases, since it is avidly taken up by the brain.

In the search for more specific PET-tracers, ¹⁸F-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT) has been developed by Shields and Grierson. FLT may not have these drawbacks.(7,8) This pyrimidine analog, is phosphorylated by the enzyme thymidine kinase 1 (TK₁), which leads to intracellular trapping.(8) TK₁ concentration increases almost tenfold during DNA synthesis and FLT uptake may therefore accurately reflect cellular proliferation.(9)

Little data are available on the clinical comparison of FLT with FDG for staging and restaging of NSCLC.(*10-12*) The aim of the study was to compare ¹⁸F-3'-fluoro-3'-deoxy-L-thymidine positron emission tomography (FLT-PET) with clinical TNM staging in patients with NSCLC, including FDG-PET.

Materials and methods

Patients

In this prospective study, patients with histological and/or cytological confirmed NSCLC, who attended the outpatient department for various treatments, were included. All patients were staged according to the TNM staging system prior to FLT-PET scanning.(*13*) Clinical TNM staging was based on patient history, physical examination, bronchoscopy, chest X-ray, CT and FDG-PET. All patients were or would be included in chemo-/radiotherapy protocols at time of the inclusion. Organ functions such as liver, kidney and bone marrow should be within normal limits. Pregnant patients and patients with psychiatric disorders were excluded. The Medical Ethics Committee of the Groningen University Hospital approved the study protocol. All patients gave written informed consent.

Tracer synthesis

Synthesis of FLT was performed according to the method of Machulla et al.(14) FLT was produced by [¹⁸F]fluorination of the 4,4'-dimethoxytrityl protected anhydrothymidine, followed by a deprotection step. After purification by reversed phase HPLC, the product was made isotonic and passed through a 0.22 μ m filter. FLT was produced with a radiochemical purity of >95% and specific activity of >10 TBq/mmol. Synthesis of FDG was performed according to the method of Hamacher et al by an automated synthesis module.(15)

PET-scanning

All FLT-PET scans were attenuation corrected and performed on an ECAT EXACT HR+ (Siemens/CTI Inc., Knoxville, TN). Nine FDG-PET scans were attenuation corrected on an ECAT EXACT HR+ (Siemens/CTI Inc., Knoxville, TN). The remaining eight FDG-PET scans were non-attenuation corrected, of which four were scanned on an ECAT EXACT HR+ and four on an ECAT 951/31. It is our experience that the difference between both cameras and the use of attenuation and non-attenuation technique for FDG-PET is negligible for staging of patients with NSCLC. Since FLT was the experimental tracer and our experience with FLT in lung cancer was limited, we used only attenuation-corrected images made with the EXACT HR+ camera. Prior to PET imaging, patients were instructed to fast for at least 6 hours. They also were instructed to drink one liter of water prior to imaging to stimulate FLT and FDG excretion from the renal calyces. For injection of the radiopharmaceuticals, a venous cannula was inserted in the forearm of the patient. From this cannula, a 2 ml blood sample was taken to measure serum glucose level before each FDG-PET scan. The median interval (range) between FDG-PET and FLT-PET was 3 (1-63) days. Patients were injected with a median (range) of 360 (160-500) MBg FDG and 210 (130-420) MBq FLT. Ninety minutes post-FDG injection and sixty minutes post-FLT injection, interleaved attenuation-corrected whole-body scanning was performed from crown to femur with 3 and 5 minutes per bed position for transmission and emission scanning, respectively. Data from multiple bed positions were iteratively reconstructed (ordered subset expectation maximization) into attenuated and non-attenuated FLT and FDG whole-body PET images.(16)

Data Analysis

Two experienced PET-physicians evaluated the FLT-PET images independently and were unaware of patients' clinical information, including FDG-PET. The observers ranked the intensity of each lesion. The intensity was ranked as 0 (not visible), 1 (slight increase in uptake), 2 (moderate increase in uptake) and 3 (strong increase in uptake) as compared with the background uptake in the lungs. The observers reached consensus on a lesion-by-lesion basis according to the same intensity scale for differently scored lesions. Thereafter, lesions ranked as 0 or 1, were grouped as 'hypo/normometabolic' lesions and lesions that were ranked as 2 or 3 were grouped as 'hypermetabolic' lesions.

To compare the staging properties of FLT-PET with the clinical TNM system, the presence or absence of pulmonary, mediastinal and distant hypermetabolic lesions, were used. The mediastinal lesions were assigned according to the Mountain and Dresler classification of regional lymph nodes.(*17*) The exact location of N1 and N2 lesions is difficult to assess on PET and therefore these lesions were read in conjunction with CT, after all PET-scans had been evaluated. Lesions outside the mediastinum were described according to their anatomical locations.

After analysis of the lesions and the staging properties, SUV calculation was performed on the attenuation corrected FDG-PET and FLT-PET scans. The visually most hypermetabolic lesion on FLT-PET of each patient was compared with the corresponding lesion on FDG-PET on sagittal sections. The slice with the highest uptake was selected for ROI analysis. After selecting the plane with the maximum SUV, a ROI was drawn manually. ROIs were placed at the 70% contour of the maximal SUV in the tumor when possible. In other cases ROIs were drawn manually. SUVs of FLT-PET and FDG-PET were compared. Images were displayed on a SUN workstation. ROI calculation was performed Clinical Applications Programming Package version 5 (CAPP5, CTI, Knoxville (TN), USA).

Statistical Analysis

The degree of inter-observer agreement, for detection of FLT-PET and FDG-PET lesions, was quantified with kappa (κ) statistics. For analyses regarding the intensity of each lesion, the values from the consensus readings were used. Sensitivity was calculated on lesion level, using the number of pulmonary, mediastinal and distant hypermetabolic lesions. Sensitivity is expressed as mean with a 95% coincidence interval (CI). Staging

properties of FLT-PET based on the presence or absence of pulmonary, N1 or N2 lesions, or distant hypermetabolic lesions, were compared with the clinical TNM staging system. Wilcoxon signed rank test was used to compare max SUV and mean SUV, between FDG-PET and FLT-PET. Two-tailed P-values <0.05 were considered significant.

Results

Patients

From January 2002 until March 2003 seventeen consecutive patients were included in this study. Their characteristics are shown in Table 1. Nine patients were included for primary staging and eight patients were included for restaging. Seven of the restaged patients completed therapy before the PET-scans. Patient 3 was scanned during chemotherapy, because of clinical progression. All patients had histological confirmed tumors, with the exception of patient 17, who had no malignancy.

| | Pt Age | | Sex | Histology | TNM | Stage | Previous therapy | Time interval between | Consensus FDG | | | | Consensus FLT | | | |
|----------------------------|--------|----|-----|-----------|----------|-------|---|-----------------------|---------------|----|----|-----|---------------|----|----|----|
| | | | | | | | | treatment and PET | TL | N1 | N2 | D | TL | N1 | N2 | D |
| | 1. | 57 | F | AC | T2N2-3M1 | IV | Cisplatin and Gemcitabine | 27 months | 4 | 1 | 4 | 2 | 1 | 1 | 2 | 2* |
| | 2. | 56 | F | AC | T2N3M1 | IV | Docetaxel | 14 months | 1 | 0 | 1 | 3* | 2 | 0 | 0 | 3* |
| | 3. | 64 | F | AC | T4N0M1 | IV | Cisplatin and Gemcitabine and second line | Just before 3rd | 2 | 0 | 0 | 1 | 1 | 0 | 0 | 0 |
| | | | | | | | Paclitaxel and Docetaxel | cycle of Docetaxel | | | | | | | | |
| | 4. | 58 | М | SCC | T4N1M1 | IV | Epirubicin and Gemcitabine | 9 months | 1 | 1 | 0 | 1 | 1 | 0 | 0 | 0 |
| | 5. | 62 | М | LCUC | T4N2M0 | IIIB | Cisplatin and Gemcitabine | 17 months | 1 | 0 | 0 | 0 | 1 | 0 | 0 | 0 |
| Patients with pretreatment | 6. | 54 | F | AC | T4N2M1 | IV | Cisplatin and Gemcitabine and second line | 1 month | 4 | 0 | 1 | 11* | 2 | 0 | 1 | 2 |
| eatr | | | | | | | Docetaxel and Irinotecan | | | | | | | | | |
| oreti | 7. | 45 | Μ | SCC | T1N0M1 | IV | Radiotherapy on abdomen (in 1983), mediastinum | 20 months | 0 | 0 | 0 | 2 | 0 | 0 | 0 | 1 |
| ith _F | | | | | | | (in 1983) and head and neck and supraclavicular | | | | | | | | | |
| s) v | | | | | | | region (in 2000) | | | | | | | | | |
| tien | 8. | 61 | Μ | SCC | T2N2M1 | IV | Radiotherapy on recurrent tumor | 2 months | 1 | 0 | 1 | 1* | 0 | 0 | 0 | 1 |
| Ра | 9, | 53 | М | AC | TxN2/3M1 | IV | Radiotherapy on acetabulum | 1 week | 5 | 0 | 1 | 30* | 0 | 0 | 0 | 0 |
| t | 10. | 57 | М | SCC | T2N0M0 | IB | None | NA | 1 | 0 | 0 | 0 | 1 | 0 | 0 | 0 |
| without | 11. | 70 | Μ | SCC | T2N2M0 | IIIA | None | NA | 1 | 0 | 1 | 0 | 0 | 1 | 1 | 0 |
| 3 | 12. | 67 | М | SCC | T4N0M1 | IV | None | NA | 1 | 0 | 0 | 1* | 1 | 0 | 0 | 1* |
| | 13. | 73 | М | SCC | T4N2M0 | IIIB | None | NA | 1 | 0 | 0 | 0 | 1 | 0 | 0 | 1 |
| Ħ | 14. | 74 | М | SCC | T4N2M0 | IIIB | None | NA | 0 | 0 | 3 | 0 | 0 | 0 | 3 | 1 |
| t mei | 15. | 65 | М | LCUC | T4N2M1 | IV | None | NA | 1 | 1 | 1 | 1* | 1 | 0 | 0 | 0 |
| Patients pretreatment | 16. | 43 | F | AC | T4N2M1 | IV | None | NA | 2 | 0 | 3 | 2 | 1 | 1 | 2 | 0 |
| Pat pre | 17. | 52 | М | NM | NM | | None | NA | 0 | 0 | 0 | 0 | 0 | 0 | 0 | 0 |
| | | | | | | | | Total | 26 | 3 | 16 | 55 | 13 | 3 | 9 | 12 |

Table 1. Patient characteristics and detectability of hypermetabolic lesions on FLT-PET as compared with standard FDG-PET

*including pulmonary lesions located outside the lobe with the primary tumor. AC= adenocarcinoma; D=distant hypermetabolic lesion(s); LCUC= large cell undifferentiated carcinoma; N= lesion(s) at N1 and/or N2 location; N1=lesion(s) located at N1 node location; N2= lesion(s) located at N2 node location; NA=not plicable; NM=no malignancy; SCC= squamous cell carcinoma; TL= lesion(s) in lung(s).

Accuracy of FLT-PET

FLT-PET demonstrated easily interpretable images (Figure 1). Most prominent physiological uptake of the tracer was observed in liver, bone marrow, intestines and bladder. Negligible and uniform tracer uptake was present in the lungs. No uptake of the tracer was observed in the brain, mediastinum and myocardium.

Figure 1. FDG and FLT uptake in patient with post-obstructive pneumonia

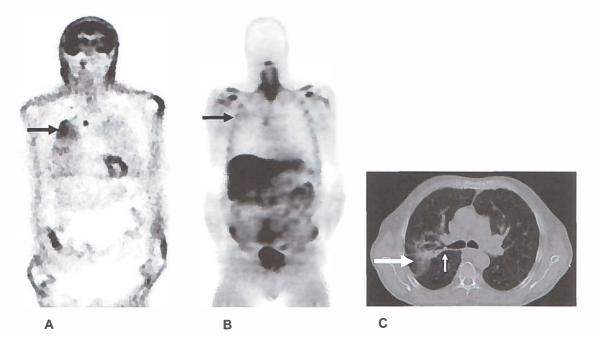


Figure 1. Coronal FDG-PET (A), FLT-PET (B) and CT image (C) of patient 11, diagnosed with squamous cell carcinoma in the right upper bronchus (small white arrow) and distally with suspected post-obstruction pneumonia (large white arrow) on CT. Avid uptake of FDG can be seen in a pre-tracheal lesion and the primary tumor, located in an area of elevated uptake, probably post-obstructive pneumonia (black arrow). Less avid uptake of FLT can be seen in the area of the tumor and little FLT uptake can be seen in the suspected infected area (black arrow). In the bone marrow of the ribs, shoulder bones, liver and intestine, there is physiological FLT uptake.

The inter-observer agreement for the detection of lesions (kappa) was 0.51 (SE=0.06) for FLT-PET and 0.55 (SE=0.06) for FDG-PET.

Overall sensitivity of FLT-PET for the detection of all hypermetabolic lesions was 37% (95% CI., 29-45%) as compared with those lesions on FDG-PET (Table 2). Sensitivity of FLT-PET for the detection of pulmonary, mediastinal (expressed as N1 and N2 lesions) and distant hypermetabolic lesions was respectively 50% (95% CI., 34-66%), 100%, 56%

(95% CI., 37-75%) and 21% (95% CI., 12-30%), using FDG-PET as the reference standard. Sensitivity was calculated on a lesion-by-lesion basis for FLT-PET using FDG-PET as the reference standard. In 8 patients without pretreatment sensitivity was 80% (95% CI., 67-93%), in 9 patients with pretreatment sensitivity was 27% (95% CI., 3-51%).

FLT-PET staged 8 of 17 patients correctly compared with clinical TNM staging (Table 1). In 8 patients without pretreatment, FLT-PET staged 3 patients correctly and 5 in 9 patients with pretreatment, compared with the clinical TNM staging.

The uptake of FDG was significantly higher than FLT, when expressed in max SUV and mean SUV (Table 2).

| Pt | lesion | FLT | FLT | FDG | FDG | | |
|-----|--------|-----------|---------|----------------|-------|--|--|
| | | Max | Mean | Max | Mean | | |
| | | SUV | SUV | SUV | SUV | | |
| | | Tumor | Tumor | Tumor | Tumor | | |
| 1. | N | 4.5 | 3.3 | 9.9 | 6.9 | | |
| 2. | Р | 3.0 | 2.4 | 9.2 | 7.3 | | |
| З. | P | 1.6 | NA | 6.7 | 5.4 | | |
| 4. | Р | 3.9 | 3.1 | 18.8 | 13.9 | | |
| 10. | Р | 3.1 | 2.9 | 10.0 | 7.8 | | |
| 13. | Р | 0.8 | NA | 54 | 4.4 | | |
| 14. | N | 2.4 | 1.9 | 5 1 | 3.7 | | |
| 16 | Р | 1.8 | 1.4 | 3.7 | 2.8 | | |
| | | Max SU | v | Mean SUV | | | |
| | | (n=8) | | (n=6) | | | |
| FLT | -PET | 2.7 (0.8- | -4.5)* | 2.7 (1.4-3.3) | | | |
| FDC | -PET | 8.0 (3.7- | -18.8)* | 6.2 (2.8-13.9) | | | |

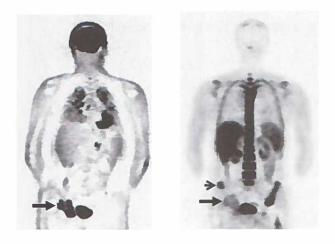
Table 2. Maximum and Mean SUV and Wilcoxon non-parametric test

[#]P=0.012; *P=0.027; N=mediastinal lesion; NA=not assessable; P=pulmonary lesion; SUV expressed as median (min-max).

Additional FLT-PET findings

In patient 11, CT showed a T1 tumor suspicious for malignancy in the right upper lobe. On both FDG-PET and FLT-PET mediastinal hypermetabolic lesions were detected (Figure 1). On FDG-PET and CT the primary tumor was located within an area, suspicious for post-obstructive inflammation. On FDG-PET this area showed diffuse FDG uptake. In contrast, on FLT-PET this inflammation was not visible, as would be expected. Patient 9 was treated with radiation therapy on the acetabulum. The field of radiation therapy and the remnant of the metastasis showed up with slightly decreased FLT activity. This lesion was ranked as hypometabolic lesion, because the observers were blinded to the clinical history of the patient (Figure 2). On FDG-PET this area showed up as a hypermetabolic lesion, bearing in mind that this could be caused by locally increased uptake of inflammatory tissue (Figure 2). Patient 4 demonstrated a photopenic defect in the liver, which corresponds with the photopenic defect in the hypermetabolic lesion on FDG-PET in the liver (Figure 3). Vital tumor tissue in the margin cannot be discriminated from the surrounding tissue because of the high physiological FLT uptake in the liver. This lesion was suspicious for a liver metastasis seen on CT.

Figure 2. FDG-PET versus FLT-PET for pulmonary malignancy

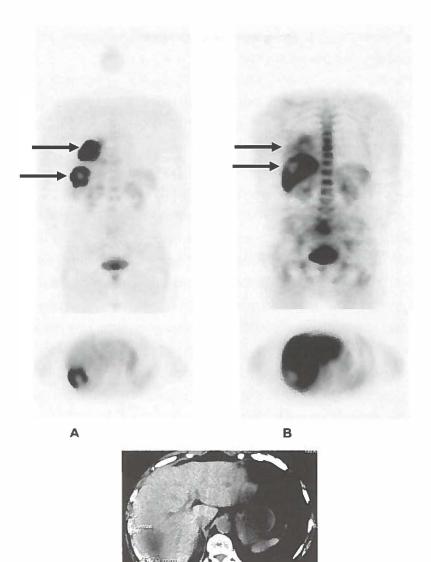


Α

В

Figure 2. Coronal FDG-PET (A) and FLT-PET (B) image of patient 9, with multiple lesions in both lungs on FDG-PET and no lesions on FLT-PET. The metastasis in the right acetabulum, which had been irradiated 1 week earlier, is very prominent on FDG-PET (large arrow), but less intense on FLT-PET (large arrow). In addition, the irradiated bone marrow, cranial of the tumor, has become metabolically inactive, visible as less intense FLT uptake as compared to the non-irradiated bone marrow (small arrow).

Figure 3. FDG-PET versus FLT-PET for liver metastasis



С

Figure 3. Coronal and transaxial FDG-PET (A), FLT-PET (B) and CT (C) images of patient 4, diagnosed with a large tumor in the right lower lung and a large metastasis in the liver on CT (large arrows). FDG-PET showed avid uptake in the lung tumor and liver metastasis (large arrows), while FLT uptake was slightly less in the pulmonary lesion and almost absent in the liver metastasis.

Discussion

Despite the potential of FLT for imaging proliferation of cancer, our results indicate that FLT is inferior to FDG for staging NSCLC. This is consistent with two recently published abstracts and one article.(*10-12*)

This article focuses solely on the staging properties of FLT-PET in patients with NSCLC. Sensitivity of mediastinal and distant hypermetabolic lesions was low, which resulted to incorrect staging in 9 of 17 patients (5 in the group with pretreatment and 4 in the group without pretreatment). Most visible FLT lesions were categorized as less intense lesions than the comparable lesions on FDG-PET. Other studies confirm that FLT-PET is not an accurate tracer for staging patients with NSCLC.(*10-12*)

FLT uptake is related to cellular proliferation, while FDG uptake is related to increased glucose metabolism. Since most cancer cells are metabolically active, but fewer cells are proliferating, a higher net uptake of FDG than FLT in the tumor can be expected. Besides tumor cells, usually many inflammation cells are present in malignant lesions, resulting in a higher FDG uptake compared to FLT.(3) Moreover, it is known that the FLT phosphorylation rate in vitro is about 30% of the phosphorylation rate of serum thymidine by thymidine kinase 1. This could explain the low FLT uptake in the tumor.(*18,19*) In this study, in a small and heterogeneous group of patients, the max SUV of FLT ranged from 0.8 to 4.5 as compared to 3.7 to 18.8 for FDG. Vesselle et al also found low FLT uptake, with max SUVs ranging from 0.9 to 6.9 (*20*); Buck et al found max SUVs ranging from 1.3 to 10.4.(*12*) Lesions with a low SUV can increase the risk for misinterpretation and thus influence the accuracy of staging with FLT-PET.

Other mechanisms could explain the low sensitivity of FLT-PET for the detection of NSCLC lesions. One explanation for the low sensitivity of FLT-PET in this study could be that nine patients had received chemotherapy and/or radiation therapy prior to the PET-scans. The effects of chemotherapy on FLT uptake have been studied in vitro and in vivo in animals. This was performed in esophageal cells, 24 and 72 hours with four different types of chemotherapy and in mice with a fibrosarcoma 24 and 48 hours after 5-FU.(*21,22*) These studies showed that the increase or decrease of FLT uptake in the tumor after chemotherapy depends on the type of chemotherapy. However, no clinical data are available to explain the (decreased) uptake of FLT in NSCLC patients with progression after first and second line chemotherapy. Next to this, in the 8 patients, who did not receive previous therapy, the results for staging were also poor, which is in

concordance with the preliminary results of Yap et al, who found a poor sensitivity for FLT-PET in untreated NSCLC patients as well.(*10*) On one hand, a decrease of FLT after therapy could be a major advantage for FLT-PET compared to FDG-PET and should not per se be interpreted as a lack of sensitivity. On the other hand, the group of pretreated patients showed clinical progression, indicating lower sensitivity of FLT-PET. The ideal situation would be to obtain pathological confirmation of the lesions, to correlate the cellular activity with FLT uptake.

Conclusion

Our study indicates that not only the pulmonary lesions, but also mediastinal and distant metastatic lesions are not well identified by FLT-PET. Therefore, staging with FLT-PET in patients with NSCLC is not recommended.

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Chapter 9

Summary

In this thesis the applicability of 2-[¹⁸F]-fluoro-2-deoxy-D-glucose positron emission tomography (FDG-PET) and [¹⁸F]-'3-fluoro-'3-deoxy-L-thymidine PET (FLT-PET) in solid tumors was explored. FDG-PET has become an important diagnostic tool in clinical oncology with many proven indications. One indication, which is being explored, is FDG-PET for the staging of melanoma patients. The sentinel lymph node (SLN) procedures might become a standard of care for staging melanoma patients with stage I and II disease, but results of a prospective trial are still pending. Since the diagnostics in oncology for staging melanoma patients, e.g. FDG-PET, SLN procedure and histopathological staining techniques, have improved in the last decade, a review of the literature was performed to gain more insight in these techniques. The value of FDG-PET for staging melanoma patients with clinical negative regional lymph nodes is limited. A comparison of FDG-PET with the SLN procedure in these patients could be of value and was therefore performed. Because FDG is not a tumor specific tracer, several potentially more specific tracers are under investigation. FLT is one of those tracers, which could be more tumor specific and less sensitive for inflammation than FDG, since it measures cell proliferation. Since melanomas have a high proliferation activity, a feasibility study was performed to stage patients with metastatic melanoma with FLT-PET. The results of this study were encouraging. Therefore FLT-PET was compared with FDG-PET in a tumorinflammation rat model. To further explore the applicability, FLT-PET was used to correlate FLT uptake with proliferation activity in soft tissue sarcomas (STS). Next to this FLT-PET was compared with FDG-PET in two solid tumors, in which FDG-PET is performed frequently in clinical TNM staging. These tumors were non-small cell lung cancer (NSCLC) and primary and recurrent laryngeal carcinoma.

In the **introduction**, staging of cancer patients, positron emission tomography (PET), PET tracer basics, PET indications in oncology and the background of ¹⁸F-fluoro-3'-deoxy-3'-L-fluorothymidine (FLT), are described.

FDG-PET, SLN biopsy and new pathological markers for the detection of metastatic melanoma are reviewed in **chapter 2**. The current histopathological techniques have improved and are able to detect up to 1 tumor cell in 10⁵ cells. Therefore, the SLN biopsy is superior to FDG-PET for detecting micrometastasis, especially in patients with stage I and II melanoma. Although the SLN concept is improving the staging of melanoma patients, at this moment the clinical application is still under investigation. FDG-PET might

be superior to conventional imaging, such as ultrasound, MRI and CT, in the staging of patients with stage III and IV melanoma.

In chapter 3, the value of FDG-PET for the detection of lymphatic melanoma metastases, is compared with the SLN biopsy. Fifty-five patients with primary cutaneous melanoma, \geq 1.0 mm Breslow thickness and no palpable regional lymph nodes, underwent a FDG-PET before SLN biopsy. SLN biopsy identified 13 patients (23%) with regional lymph node metastases. FDG-PET identified only 2 of these 13 patients. The lesions detected with FDG-PET were regional metastases of 7 mm and 8 mm in diameter. In addition, FDG-PET suggested incorrectly a regional lymph node metastasis in five patients. FDG-PET should not be considered for staging of patients with stage I and II melanoma, since SLN also reveals regional metastases, which are too small to be detected by FDG-PET.

The value of FLT-PET for staging patients with clinical stage III melanoma, is described in **chapter 4**. Ten patients underwent a whole-body FLT-PET. All PET lesions and histopathological lesions were categorized into anatomical regions and compared with each other. The sensitivity was 88% and the specificity was 60% (3/5), comparable with the results for FDG-PET. FLT-PET could therefore be used as a diagnostic method for staging patients with stage III melanoma. However, large studies are required, in which FLT-PET is compared with FDG-PET, before a final conclusion can be drawn.

The theoretical advantage of FLT, no uptake in inflammatory cells, was investigated in a tumor-inflammation-rat model and compared with FDG (**chapter 5**). Twelve rats with a C6-glioma tumor in one leg and a turpentine induced acute inflammation in the opposite leg, were studied with FDG-PET (n=6) and FLT-PET (n=6). Uptake of both tracers in several tissues, including the C6 tumor, inflammatory tissue and muscle, were compared. The tumor/muscle ratio of FLT was 3.3, which was fourfold lower than the FDG. The inflammation/muscle ratio of FLT uptake was only 1.2 as opposed to 4.6 for FDG. PET images confirmed that the inflammation was visualized with FDG, but not with FLT. The tumor was visible with both tracers. Thus, the hypothesis that FLT is a more tumor-selective tracer than FDG, was confirmed in this experimental rat model.

The application of FLT-PET for the detection and grading of soft tissue sarcomas (STS) in the extremities of nineteen patients is described in **chapter 6**. The measure for FLT uptake, standardized uptake value (SUV), was compared with proliferation markers of the tumor. These proliferation markers are the mitotic score and the MIB-1 score. The

survival and metastatic potential of a sarcoma is related to malignancy grade, which is largely based on proliferation scores. FLT-PET was able to visualize and differentiate high grade from low grade STS according to two clinical grading systems. The SUV correlated well with the proliferation of STS, expressed as mitotic score and MIB-1 score.

The value of FDG-PET and FLT-PET for the detection of primary and recurrent laryngeal carcinoma, compared histopathology, was studied in 21 patients and described in **chapter 7**. FDG-PET and FLT-PET detected 15 out of 17 laryngeal cancers correctly. FLT-PET was false positive in two cases and FDG-PET in one case. The SUV and TNT were lower for FLT than for FDG. The uptake of FDG is higher than FLT in laryngeal cancers.

FDG-PET is the current standard for staging patients with NSCLC. FDG-PET even surpasses CT for the staging of NSCLC in the mediastinum. In **chapter 8** the value of FLT-PET for staging and restaging of patients with non-small cell lung cancer in seventeen patients is described and compared with clinical TNM staging, including FDG-PET. On a lesion-by-lesion basis, the overall sensitivity of FLT-PET was 37% as compared to FDG-PET. Especially pulmonary lesions and distant metastatic lesions were missed with FLT-PET. Only 5 of the 17 patients were staged correctly with FLT-PET compared to the clinical TNM-staging system, including FDG-PET. It may be concluded that FLT-PET is therefore inadequate for staging and restaging of patients with NSCLC.

Overall conclusions and future perspectives

This thesis describes the evaluation of 2-[¹⁸F]fluoro-2-deoxy-D-glucose-PET (FDG-PET) and [¹⁸F]-'3-fluoro-'3-deoxy-L-thymidine PET (FLT-PET) in solid tumors. Over the last decade the number of indications for FDG-PET has increased, and many new indications are under investigation. FDG-PET, which is superior to conventional imaging (ultrasound, MRI and CT), might be useful for staging patients with stage III and IV melanoma. Large patient studies are being conducted to investigate the value of FDG-PET for staging patients with stage III, IV and recurrent melanoma and the value of SLN biopsy for staging patients with stage I and II melanoma. The data obtained thus far confirm the value of FDG-PET and the SLN biopsy in patients with metastatic melanoma. This has resulted in implementing the SLN biopsy as a staging procedure for patients with metastatic melanoma and including the outcome of the sentinel node in the latest TNM-staging system for melanoma. The final results on the value of FDG-PET for staging melanoma

patients with palpable lymph nodes are pending, before it might become a standard diagnostic tool.

Although FDG-PET is superior to many conventional diagnostic techniques, it has drawbacks as well. Especially physiological uptake in the brain, heart, urinary system, inflammatory tissues and muscle can make the interpretation of the lesions difficult or cause false positive lesions. Therefore, new and more specific tracers are under investigation. One of those tracers is FLT.

What role can FLT-PET play in clinical oncology? FLT-PET is able to detect solid tumors and distinguish between tumor and inflammation in an animal model and some clinical studies. The study to measure the selectivity of FLT, was only performed in one specific (acute) inflammation model. Therefore, to investigate the claim that FLT is not taken up in inflammatory cells, more research with FLT-PET is required in different inflammation models (e.g. in lymph nodes of rats or canines), in patients with different inflammatory diseases (e.g. sarcoidosis, ulcerative colitis, Crohn's disease, etc) and in patients with proven metastatic lymph nodes.

Since FLT uptake is lower than FDG uptake in most investigated cancers, the role of FLT-PET in clinical oncology will be limited to cancers with a high proliferative activity. These forms of cancer, like oesophageal cancer, high grade soft tissue sarcomas and B-cell lymphomas, are currently under investigation. Preliminary reports on FLT-PET for the detection of lymphoma and oesophageal cancer, are promising. Both tumor types expressed a SUV of five on FDG-PET and on FLT-PET. FLT could also become a promising tracer for brain tumors, because low physiological uptake can be seen in the brain, whereas brain tumors have a high proliferation rate. When FDG-PET, CT or MRI scans are unable to differentiate between irradiation induced fibrosis and suspected recurrent tumor, FLT-PET can be a complementary diagnostic tool, before performing a biopsy.

Because FLT uptake reflects DNA synthesis, it can become a challenging tracer for therapy evaluation. The scarce data available on FLT-PET for the evaluation of chemotherapy indicates that FLT uptake is dependent on the dosage and the type of chemotherapeutic agent. FLT uptake in the tumor can either increase or decrease after chemotherapy, because these agents interfere with DNA synthesis. More research is needed on the uptake mechanisms of FLT in relation to the different chemotherapeutic agents to understand what changes in FLT uptake during and after therapy evaluation mean for the treatment efficacy. The preliminary results of high grade STS for the therapy evaluation of isolated limb perfusion is promising as well. Since these tumors express a high initial FLT uptake, these tumors are likely to be valuable to investigate therapy evaluation.

FLT has disadvantages as well. Thus far, relatively low radiochemical yields, make it impossible to prepare multi-patient doses. However several reports have appeared, describing optimized production methods. Only a fraction of malignant cells in a tumor is in the late G₁ or S-phase, resulting in FLT uptake in a fraction of the cells. In contrast, the majority of malignant cells in a tumor. Therefore, a high FDG uptake can be expected in tumors. This may be an important reason why the FLT uptake is lower than the FDG uptake in tumors. Moreover, the phosphorylation rate of FLT is 30% of the phosphorylation rate of thymidine, which may result in decreased intracellular trapping. When FLT uptake is below the visual threshold, tumors are easily missed with FLT-PET. Because FLT is metabolized in the liver and physiologically taken up in bone marrow, it is not an accurate tracer for the detection of liver malignancies, liver metastases and bone metastases. False positive lymph nodes in patients with laryngeal cancer and in a sarcoma patient were found. False-positive FLT-PET findings of lymph nodes and high FLT uptake in the hilar regions of a sarcoidosis patient, were also mentioned by the group of Shields et al.

In conclusion, future research with FLT-PET should focus on the selective detection of highly proliferative cancers and its therapy evaluation. For these indications and the staging of cancer, FLT-PET could become a valuable complementary diagnostic tool.

Chapter 10

Samenvatting

Positron emissie tomografie (PET) is een 'in vivo imaging' techniek die in toenemende mate wordt toegepast bij de diagnostiek en stadiëring bij patiënten met kwaadaardige tumoren. Dit proefschrift beschrijft de toepasbaarheid van 2-[¹⁸F]-fluoro-2-deoxy-D-glucose PET (FDG-PET) en [¹⁸F]-'3-fluoro-'3-deoxy-L-thymidine PET (FLT-PET) bij diverse solide tumoren, zoals het melanoom, weke-delen tumoren, larynx carcinoom en niet-kleincellig longcarcinoom. Daarnaast wordt een experimenteel tumor-ontstekingsmodel in de rat beschreven. De specifieke eigenschappen van de beide tracers met betrekking tot de differentiatie tumor versus ontsteking werden in dit model onderzocht.

In de **inleiding** wordt allereerst ingegaan op de stadiëring van patiënten met kanker. Daarnaast wordt de techniek van PET, de diverse PET-tracers en de huidige indicaties van PET in de oncologie beschreven. Ten slotte worden de achtergrond en de diverse aspecten van de nieuwe PET-tracer [¹⁸F]-'3-fluoro-'3-deoxy-L-thymidine (FLT) belicht.

Voor het stadiëren van patiënten met een melanoom zijn de laatste jaren diverse technieken beschikbaar gekomen, zoals PET, de schildwachtklier (SWK) biopsie en nieuwe pathologische markers. In **hoofdstuk 2** wordt een overzicht gegeven van de huidige toepassingsmogelijkheden van deze technieken bij de behandeling van het melanoom.

In hoofdstuk 3 wordt de waarde van FDG-PET voor de detectie van lymfkliermetastasen bij het klinisch niet-regionaal-gemetastaseerde melanoom vergeleken met de SWK biopsie. Vijfenvijftig patiënten met een primair melanoom, Breslow dikte van > 1.0 mm zonder palpabele lymfklieren, ondergingen een FDG-PET voorafgaand aan de SWK biopsie. Met de SWK biopsie werden bij 13 patiënten (23%) regionale lymfkliermetastasen aangetoond. Daarentegen identificeerde FDG-PET lymfkliermetastasen bij slechts 2 van deze 13 patiënten. De laesies die gedetecteerd werden met FDG-PET bestonden uit regionale lymfkliermetastasen met een diameter van respectievelijk 7 en 8 mm. FDG-PET detecteerde bij 5 patiënten onterecht lymfkliermetastasen. Voor het stadiëren van patiënten met een klinisch stadium I en II melanoom is de SWK procedure beter dan FDG-PET. Er is daarom geen plaats voor FDG-PET in de diagnostiek van patiënten met een klinisch stadium I en II melanoom.

De waarde van FLT-PET voor de stadiëring van patiënten met klinisch stadium III melanoom wordt beschreven in **hoofdstuk 4**. Tien patiënten ondergingen een whole-body

FLT-PET. Alle laesies op FLT-PET en histopathologische laesies werden ingedeeld in anatomische regio's en met elkaar vergeleken. De sensitiviteit was 88% en de specificiteit 60%. Dit is vergelijkbaar met de resultaten uit de literatuur voor FDG-PET bij de stadiëring van stadium III melanoom. FLT-PET zou daarom gebruikt kunnen worden bij het stadiëren van patiënten met stadium III melanoom. Welke tracer de uiteindelijke voorkeur heeft bij de stadiëring van stadium III melanomen, zal in een vergelijkend onderzoek met een groter aantal patiënten onderzocht moeten worden.

Het theoretische voordeel van FLT ten opzichte van FDG is, dat FLT wel in tumorcellen, maar niet in ontstekingscellen zou worden opgenomen. Teneinde dit te onderzoeken werd een experimenteel tumor-ontstekingsmodel in de rat gebruikt. In **hoofdstuk 5** wordt een experimentele studie met dit model beschreven waarin FLT wordt vergeleken met FDG. Twaalf ratten met een C6-glioom in een voorpoot en een door terpentine geïnduceerde acute ontsteking in een achterpoot, werden onderzocht met FDG-PET (n=6) en FLT-PET (n=6). De opname van beide tracers in verschillende weefsels werd bepaald. De tumor/spier ratio voor FLT was 3.3, welke vier keer lager was dan de ratio van FDG. De ontsteking/spier ratio van FLT was 1.2 in tegenstelling tot 4.6 voor FDG. De PET-afbeeldingen bevestigden dat de ontsteking werd gedetecteerd met FDG, maar niet met FLT. De tumor was detecteerbaar met beide tracers. De hypothese dat FLT een meer tumorspecifieke tracer is dan FDG werd in dit model bevestigd.

De toepassing van FLT-PET voor de detectie en gradering van weke-delen sarcomen (WDS) in de extremiteiten van negentien patiënten wordt beschreven in **hoofdstuk 6**. De mate van FLT-opname, uitgedrukt in standardized uptake value (SUV), werd vergeleken met afgeleiden van de delingsactiviteit van de tumor, zoals de mitotische score en de MIB-1 score. Met FLT-PET konden alle sarcomen worden afgebeeld en kon het onderscheid gemaakt worden tussen hoog- en laaggradige WDS. De SUV correleerde met de proliferatiegraad van WDS, uitgedrukt als mitotische score en MIB-1 score. Hoewel FLT-PET kan differentiëren tussen hoog- en laaggradige sarcomen, zal de plaats van FLT-PET in de diagnostiek en behandeling van weke-delen tumoren nog nader moeten worden onderzocht.

In **hoofdstuk 7** wordt het gebruik van FDG-PET en FLT-PET voor de detectie van primair en recidief larynxcarcinoom beschreven. Bij 21 patiënten werd de waarde van beide tracers onderzocht en werden de resultaten vergeleken met de huidige klinische standaard, de combinatie van CT en pathologie. FDG-PET en FLT-PET detecteerden 15 van 17 larynxcarcinomen correct. FLT-PET was vals-positief in 2 gevallen en FDG-PET in 1 geval. De SUV en tumor/non-tumor ratio waren lager voor FLT dan voor FDG. FLT-PET en FDG-PET waren even nauwkeurig voor de detectie van larynxcarcinomen, echter de opname van FLT in de tumoren was lager dan FDG.

Bij de stadiëring van patiënten met een niet-kleincellig longcarcinoom (NSCLC) is FDG-PET een standaardonderzoek. In **hoofdstuk 8** wordt de toepasbaarheid van FLT-PET voor het stadiëren en restadiëren van patiënten met NSCLC beschreven. Zeventien patiënten met een NSCLC ondergingen een FDG-PET en een FLT-PET en werd de klinische TNM-stadiëring van beide onderzoekstechnieken bestudeerd. Op basis van gedetecteerde laesies, was de sensitiviteit van FLT-PET slechts 37%, ten op zichte van FDG-PET. Door FLT werden vooral laesies in de longen en op afstand niet gedetecteerd. Slechts 5 van de 17 patiënten werden correct gestadieerd met FLT-PET, vergeleken met de klinische TNM-stadiëring. FLT-PET is daarom een inadequate methode om patiënten met NSCLC te stadiëren en te restadiëren.

Conclusies en toekomstperspectieven

Dit proefschrift beschrijft de toepassingsmogelijkheden van FDG-PET en FLT-PET bij melanomen, weke-delen sarcomen, primair en recidief larynxcarcinomen, en nietkleincellige longcarcinomen. Het experimentele onderzoek heeft aangetoond dat FLT-PET inderdaad meer tumor specifiek is dan FDG-PET.

Gedurende het laatste decennium is een aantal indicaties voor FDG-PET gedefinieerd, zoals het diagnostiseren van solitaire laesies in de longen, stadiëren van lymfomen herstadiëren recidief longkanker, therapie evaluatie van en van coloncarcinomen. In de naaste toekomst zullen waarschijnlijk ook nieuwe indicaties gedefinieerd worden. Zo heeft een whole-body FDG-PET de potentie om ongeveer 25% van de patiënten met een stadium III melanoom te 'upstagen'. De vraag is nu, hoe kan een patiënt met een stadium III melanoom het best gestadieerd worden? Hiertoe worden momenteel 'whole body FDG-PET' en 'whole-body spiraal-CT' bij het stadium III melanoom prospectief met elkaar vergeleken. De waarde van FDG-PET bij stadium IV melanoom is vooral gelegen in het vaststellen van de uitgebreidheid van de metastasering, ten einde de meest optimale kankerbehandeling te kunnen vaststellen. De SWK procedure is tot nu toe een stadiërende ingreep bij het stadium I en II melanoom en is inmiddels opgenomen in de gereviseerde TNM-classificatie. Of deze verbeterde stadiëring van de regionale lymfklierstations en de daarbij horende therapeutische lymfklierdissectie ook zal lijden tot een verbeterde overleving wordt momenteel onderzocht.

Een beperking van de toepasbaarheid van FDG-PET is gelegen in de fysiologische opname van FDG in de hersenen, hart, urinewegen, spierweefsel en ontstekingsweefsel waardoor de interpretatie van de gevonden afwijkingen met FDG-PET bemoeilijkt kan worden of vals-positieve uitslagen kan veroorzaken. Daarom wordt er naar nieuwe, meer specifieke PET-tracers gezocht. FLT is hiervan een voorbeeld. Welke rol zou FLT-PET kunnen spelen in de klinische oncologie? FLT-PET kan solide tumoren detecteren en onderscheid maken tussen tumor en ontsteking zoals aangetoond is in een diermodel en in een aantal klinische pilot studies. De selectiviteit van FLT werd slechts in één specifiek (acuut) ontstekingsmodel onderzocht. Er is vervolgonderzoek nodig in verschillende tumor-ontstekingsmodellen en verschillende vormen van ontsteking in patiënten om meer inzicht te verkrijgen in de achtergronden en toepassingsmogelijkheden van FLT.

De rol van FLT-PET in de klinische oncologie zal vooral beperkt blijven tot kankervormen met een (zeer) hoge delingsactiviteit. De opname van FLT in tumoren met een lage delingsactiviteit is namelijk lager dan die van FDG; tumoren met een lage delingsactiviteit worden beter afgebeeld met FDG dan met FLT. Daarom zal het vervolgonderzoek naar de toepassingsmogelijkheden van FLT gelegen zijn bij tumoren met een hoge delingsactiviteit zoals het oesofaguscarcinomen en B-cellymfoom. FLT-PET dient daarnaast onderzocht te worden bij de detectie van hersentumoren. Immers hersentumoren hebben een hoge delingsactiviteit terwijl er een lage fysiologische opname van FLT in het brein is. Wanneer FDG-PET, spiraal-CT of MRI geen onderscheid kunnen maken tussen door bestraling veroorzaakte fibrose en een mogelijk tumorrecidief, zou de waarde van FLT-PET als complementaire afbeeldingtechniek onderzocht kunnen worden.

De mate van FLT-opname weerspiegelt de DNA-synthese, die een afspiegeling zou kunnen zijn van het effect van behandeling. Onderzoek is nodig om de opnamemechanismen van FLT in relatie tot de verschillende chemotherapeutica bij diverse tumorsoorten te begrijpen en te onderzoeken wat de veranderingen in FLT-opname gedurende en na chemotherapie betekenen voor de effectiviteit van de behandeling.

FLT heeft ook nadelen. Bij de bereiding van FLT is de radiochemische opbrengst te laag om meerdere patiënten uit één opbrengst te kunnen scannen. Het is te verwachten

dat er betere productiemethoden ontwikkeld zullen worden. Vooralsnog is het daarom niet mogelijk om grootschalig onderzoek met deze tracer uit te voeren.

Slechts een fractie van maligne cellen is in de late G₁- of S-fase. Een beperkt aantal cellen zal dus FLT kunnen opnemen. De meerderheid van de maligne cellen is, net als ontstekingscellen die de tumor omgeven, metabool actief, wat leidt tot een hoge FDG-opname. Dit is waarschijnlijk een belangrijke reden waarom de FDG opname hoger is dan de FLT-opname in tumoren. De fosforyleringssnelheid van FLT is slechts 30% van die van thymidine, wat ook een reden voor verminderde intracellulaire FLT-opname kan zijn. Wanneer de FLT-opname in tumoren onder de detectiegrens komt, worden deze tumoren niet met FLT-PET gedetecteerd. FLT wordt gemetaboliseerd in de lever en daarnaast opgenomen in het beenmerg. FLT is daarom een onnauwkeurige tracer voor de detectie van levertumoren, levermetastasen en botmetastasen. Het is nog onduidelijk waarom er false-positieve opname worden gevonden in lymfklieren.

Toekomstig onderzoek met FLT-PET zal zich moeten richten op de selectieve detectie, stadiëring en therapie-evaluatie van kankervormen met een hoge delingsactiviteit. Met name voor deze indicaties zou FLT-PET mogelijk een waardevolle complementaire diagnostische techniek kunnen zijn.

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Curriculum Vitae

David Cobben werd geboren op 8 juni 1974 te Maastricht. Na het behalen van het VWO diploma in 1992 te Meerssen begon hij met de studie Geneeskunde aan de Universiteit Maastricht. Vanaf zijn tweede studiejaar werkte hij als student-onderzoeker achtereenvolgens bij de afdelingen Bewegingswetenschappen, Neurologie en Heelkunde. Zijn wetenschappelijke stage volgde hij bij de afdeling Heelkunde in het Academisch Ziekenhuis Maastricht (AZM), getiteld "The role of renal arginine during endotoxemia in the rat". In 1999 behaalde hij na een stage Emergency Medicine in Toronto, Canada, het artsexamen. Hierna werkte hij een half jaar als arts-onderzoeker bij de afdeling Heelkunde aan de Vrije Universiteit in Amsterdam. Daarna was hij 7 maanden werkzaam als arts-assistent bij de afdeling Heelkunde in het Academisch Ziekenhuis Groningen (AZG). Van 1 september 2000 tot 1 september 2003 is hij werkzaam geweest als arts-onderzoeker bij het PET-centrum en de afdeling Chirurgische Oncologie in het AZG, waar dit proefschrift tot stand kwam. Op 1 september 2003 is hij begonnen met de opleiding Heelkunde in het AZG (opleider Prof. Dr. H.J. ten Duis).

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