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General estimates of the energy cost of walking in people with different levels and causes of lower-limb amputation: a systematic review and meta-analysis

Sanne Ettema^{1,2} , Elmar Kal³ and Han Houdijk⁴

Abstract

Background: Energy cost of walking (ECw) is an important determinant of walking ability in people with a lower-limb amputation. Large variety in estimates of ECw has been reported, likely because of the heterogeneity of this population in terms of level and cause of amputation and walking speed.

Objectives: To assess (1) differences in ECw between people with and without a lower-limb amputation, and between people with different levels and causes of amputation, and (2) the association between ECw and walking speed.

Study design: Systematic review and meta-analysis.

Methods: We included studies that compared ECw in people with and without a lower-limb amputation. A meta-analysis was done to compare ECw between both groups, and between different levels and causes of amputation. A second analysis investigated the association between self-selected walking speed and ECw in people with an amputation.

Results: Out of 526 identified articles, 25 were included in the meta-analysis and an additional 30 in the walking speed analysis. Overall, people with a lower-limb amputation have significantly higher ECw compared to people without an amputation. People with vascular transfemoral amputations showed the greatest difference (+102%) in ECw. The smallest difference (+12%) was found for people with nonvascular transtibial amputations. Slower self-selected walking speed was associated with substantial increases in ECw.

Conclusion: This study provides general estimates on the ECw in people with a lower-limb amputation, quantifying the differences as a function of level and cause of amputation, as well as the relationship with walking speed.

Keywords

energy cost of walking, lower-limb amputation, prosthesis, etiology, level, walking speed

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Background

In the Netherlands, the incidence of lower-limb amputations is 20 per 100,000 population.¹ Each year, about 3,200 lower-limb amputations are performed.² The group of people with a lower-limb amputation is heterogeneous, including persons with different levels and causes of amputation and concomitant factors. This heterogeneity is considered a main contributor to differences in the level of functioning between persons with a lower-limb amputation.³ Level of amputation can be roughly divided into amputations below and above the knee, with transtibial and transfemoral amputations being the most common. The etiology

of amputation can be roughly divided into vascular causes and nonvascular causes. Generally, lower-limb amputations with a vascular cause are performed in older persons with medical comorbidities including diabetes, whereas lower-limb amputations because of nonvascular causes often include younger persons with fewer comorbidities.⁴ It has been established that both level and cause of amputation have a major effect on walking ability in people with a lower-limb amputation.^{3,5-7}

Walking ability in people with a lower-limb amputation is often assessed in terms of energy cost of walking (ECw). ECw has shown to be related to quality of life and participation in social activities.⁸ It has frequently been found that people with a lower-limb amputation have increased ECw compared to persons without an amputation.⁶ After undergoing lower-limb amputation, one can choose to walk with or without use of a prosthesis, which will both increase the ECw.⁶ Walking without a prosthesis results in the highest ECw, as additional energy is needed to support body weight on crutches. Walking with a prosthesis also results in greater ECw, as the economy of gait is constrained by the prosthesis. People walking with a prosthesis show reduced ankle push-off power resulting from a reduced ability to plantar flex their ankle. Consequently, people with a lower-limb amputation need to use other, less efficient, strategies for propulsion and leg swing.⁹⁻¹¹ Impaired balance control is considered as another factor contributing to increased ECw while walking with a prosthesis.^{7,12} People with a lower-limb prosthesis are known to be less stable

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during steady-state walking compared to people without an amputation.^{12,13} This requires the use of compensatory strategies to maintain balance, resulting in increased energy demands.^{12,14-16}

Over the past 50 years, many studies have investigated the ECw in people with a lower-limb amputation. The seminal study of Waters et al⁶ was one of the first studies to systematically investigate the ECw for people with different levels and causes of amputation. The results showed that the ECw in people with a lower-limb amputation is dependent on both level and cause of amputation. They reported increases of 25% and 55% in ECw, for persons with a nonvascular amputation at the transtibial and transfemoral level, respectively, compared to persons without an amputation. For persons with a vascular amputation, the reported values were even higher, with increases of 65% and 120% for persons with a transtibial and transfemoral amputation, respectively. These values as reported by Waters et al⁶—and reevaluated in a later review¹⁷—are still often used as reference values in clinical practice because the study of Waters et al is actually the only study that systematically compared ECw in subgroups stratified for all levels and causes of amputation within one study. However, it can be questioned whether the values provided by Waters et al^{6,17} are applicable to the current population of people with a lower-limb amputation because the sample size in the study was rather small (approximately 15 persons for each subgroup of people with an amputation and five people without an amputation) to generalize the results to the whole population of persons with a lower-limb amputation, which might limit precision of the provided estimates. Moreover, patient characteristics, prosthetic developments, and assessment methods may have changed over time. In the years following the seminal research of Waters et al,⁶ the ECw for people with a lower-limb amputation has been assessed in many other studies.^{9,18-20} However, these studies have predominantly focused on one specific cause or level of amputation.^{9,18-20} In addition, a great variety of types of prostheses has been analyzed, as ECw has often been used as an outcome to test a newly developed prosthesis.^{21,22} Few of these studies included a control group of people without an amputation. Moreover, studies differ in their experimental protocol, using different walking speeds and walking surfaces.^{23,24} Walking speed has been shown to substantially influence ECw, both in people with and without lower-limb amputation.²⁵ ECw is known to have a U-shaped relation with walking speed, increasing at both slow and fast walking speeds.²⁵ It has been shown that, in contrast to persons without an amputation, people with a lower-limb amputation walk at speeds slower than their most economic speed.²⁶ Therefore, differences in self-selected walking speed can be associated with differences between individuals and subgroups. This can be controlled by studies that use a fixed imposed walking speed rather than self-selected walking speed to assess the ECw. However, these ECw outcomes are not representative for walking in daily life.

Hence, despite the availability of a large (and still growing) amount of quantitative data on the ECw with a lower-limb prosthesis, general estimates on the magnitude of the difference in energy cost relative to walking in persons without a lower-limb amputation are difficult to derive from the available data because of the heterogeneity between study populations and designs. Still, clinical practice and prosthetic developments need such

information to set patient-specific expectations for ECw and to develop benchmarks and interventions to reduce the ECw. Therefore, the purpose of this study was to compare the ECw between people with and without a lower-limb amputation, and to assess to what extent ECw differs as a function of level and cause of amputation. In addition, we investigated the association between self-selected walking speed and ECw of people with a lower-limb amputation, to assess how self-selected walking speed might account for the variation in energy cost between and within subgroups.

Methods

Search strategy

We performed an electronic search via the following databases until March 2020: PubMed, Physiotherapy Evidence Database, and Cumulative Index to Nursing and Allied Health Literature. A detailed description of the applied search strategy is provided in Appendix 1 (Supplemental Digital Content 1, <http://links.lww.com/POI/A46>). Searches were prelimited using the following criteria: English language and abstract available. Articles were further selected by reading title and abstract, after which a final selection was made based on the full article. Articles were selected for two types of analysis. In *analysis 1*, we compared the ECw between people with a lower-limb amputation, stratified for level (transtibial vs transfemoral) and cause (vascular vs nonvascular) of amputation, and persons without an amputation. In *analysis 2*, we assessed the effect of self-selected walking speed on ECw. Articles selected for *analysis 2* did not need to include people without an amputation. All included articles needed to provide explicit data concerning average and standard deviation of ECw and walking speed and meet all other inclusion criteria described below. When an article had been selected for either *analysis 1* or *analysis 2*, but did not provide all required details, the author was approached to provide the exact data. One author (S.E.) selected articles and extracted data. Another author (H.H.) checked the selection and data extraction of all articles. If discrepancies existed, the authors conferred to reach consensus on the specific issue.

Inclusion criteria

The following inclusion criteria were used when selecting studies: (1) participants are at least 18 years of age; (2) inclusion of a control group without amputation (*analysis 1* only); (3) inclusion of participants with transtibial or transfemoral amputation; (4) measurement of energy consumption during walking (for people with an amputation: during walking with prosthesis); (5) energy consumption measured by indirect calorimetry; and (6) the article is not a case-study or a review article.

Data extraction, outcome measures, and risk-of-bias assessment

The following information was extracted from the selected articles: (1) subject characteristics (e.g. age and sex); (2) level of amputation; (3) cause of amputation; (4) system used for measuring oxygen consumption and calculation of the ECw; (5)

type of prosthetic component used; (6) study design (instructions, duration, and environment); (7) ECw; and (8) walking speed at which ECw was assessed.

When an article investigated the ECw for a group of people with mixed levels and/or causes of amputation, the author was approached to provide additional information needed to subgroup persons according to the level and cause of amputation. Subgroups with fewer than three participants were excluded from further analysis. When a particular study tested multiple types of prostheses in the same group of participants, the ECw and walking speed related to the prosthesis with the most widespread clinical use at the time of the study were used for further analysis (see Appendix 2, Supplemental Digital Content 1, <http://links.lww.com/POI/A46>, for detailed selection, not chosen options are provided in italics). The prosthesis with most widespread clinical use was selected by one author with longstanding experience in the field (H.H.). In the case that ECw had been assessed during both overground and treadmill walking, we used the ECw during overground walking for further analysis because this most closely resembles walking in daily life.²⁷ For each study, one combination of walking speed and ECw was used for analysis. If ECw had been assessed both at imposed and self-selected walking speeds, we used ECw values at self-selected walking speed for further analysis. Furthermore, when ECw had been measured only at multiple imposed walking speeds, we selected the ECw associated with the walking speed that was closest to the average self-selected walking speed of the specific subgroup. Average self-selected walking speed for each specific subgroup was based on the preferred walking speed found in other selected studies: transfemoral vascular: 0.52 m·s⁻¹; transfemoral nonvascular: 1.00 m·s⁻¹; transtibial vascular: 0.79 m·s⁻¹; and transtibial nonvascular: 1.34 m·s⁻¹. Summary information regarding study protocols of included studies is presented in Appendix 3 (Supplemental Digital Content 1, <http://links.lww.com/POI/A46>).

Two of the reviewers (S.E. and E.K.) independently assessed the risk of bias of the included studies with the Newcastle-Ottawa Scale (NOS²⁸), which was modified for the study purpose (see Appendix 4, Supplemental Digital Content 1, <http://links.lww.com/POI/A46>). The NOS contains items on participant selection, comparability of the study groups, and outcome assessment. The scale ranges from 0 to 11 for *analysis 1* and from 0 to 7 for *analysis 2*, as comparability items were not relevant for *analysis 2*. Higher NOS scores reflect a lower risk of bias.

Energy cost calculations

In this study, we analyzed the gross metabolic ECw expressed in ml O₂·kg⁻¹·m⁻¹. When studies only reported oxygen consumption ($\dot{V}O_2$; mL O₂·kg⁻¹·min⁻¹), ECw was calculated by dividing oxygen consumption by walking speed (in m·min⁻¹). When actual metabolic energy expenditure (EE) was provided in J·kg·s, it was converted into mL·O₂·kg⁻¹·m⁻¹ according to Equation (1), with walking speed (v) expressed in m·min⁻¹. Respiratory exchange ratio (RER) was assumed to be equal to 1.²⁹

$$ECw = \text{Joules} \frac{\dot{E}E \times 60 \times v}{(4.940 \times RER + 16.040)} \quad (1)$$

Meta-analysis calculations

To perform a meta-analysis with the data collected for *analysis 1*, the SD of ECw was needed. When articles did not report SD, 95% confidence interval (CI) was used to determine SD, according to Equation (2). Studies to which Equation (2) was applied are indicated with an asterisk (*) in Appendix 2 (Supplemental Digital Content 1, <http://links.lww.com/POI/A46>). When articles did not report SD nor 95% CI and when these data could not be retrieved from the original author, articles were excluded from *analysis 1*.

$$SD = \frac{\sqrt{N} \times (\text{upper limit } 95\% \text{ CI} - \text{lower limit } 95\% \text{ CI})}{3.92} \quad (2)$$

Meta-analysis

Meta-analyses were conducted with RevMan 5.3 (The Nordic Cochrane Centre, Copenhagen, Denmark). Since all included studies used the same outcome measure with similar (or converted to similar) units of measurement, data were pooled using the mean difference (MD). Significance level was set at $P < 0.05$. Random effects models were used (as a high level of heterogeneity was evident, and >5 studies were available). Statistical heterogeneity was confirmed by visual inspection of the forest plots, and with the I²-statistic, with heterogeneity considered to be present if χ^2 was significant ($P < 0.1$).³⁰ We subgrouped studies according to the level (transtibial vs transfemoral) and cause (vascular vs nonvascular) of amputation, to assess if ECw would be different for people with different combinations of levels and causes of amputation. When an article provided data for different subgroups of persons (i.e. different levels/causes of amputation) but for just one single control group, the means and SDs for this particular control group were used as many times in the same analysis, but we divided the sample size by the number of comparisons it was included in.³⁰

Analysis of walking speed

The relationship between walking speed and ECw was analyzed descriptively by fitting a polynomial through the available data of ECw and self-selected walking speed of different subgroups. The curves were second-order polynomial fits through all data points of a specific subgroup, which were described by the function: $ECw = av^2 + bv + c$. Walking speed was expressed in m·s⁻¹. For each study, only one specific estimate of ECw (i.e. at actual or approximated self-selected walking speed) was added to this analysis. These analyses were performed in Matlab (The Mathworks, Natick, MA) using the function *polyfit*.

Results

Literature search

Figure 1 shows the flow of study selection. In total, our search identified 526 articles. After screening of titles and abstracts, 40 potential articles were selected for *analysis 1* and 87 additional potential articles for *analysis 2*. Application of the inclusion and exclusion criteria eventually resulted in the inclusion of 35 articles

in *analysis 1* and 41 additional articles in *analysis 2*. Most common reasons for exclusion at this stage were unavailability of full-text paper, measurement of energy consumption by other means than indirect calorimetry, and data for a group of persons that had already been presented in an earlier published article that was already included (Figure 1). Regarding *analysis 1*, the results of 10 articles were only descriptively synthesized, but not included in the meta-analysis. Reasons for this were that the required data could not be extracted reliably and missing data could not be obtained by contacting the authors³¹⁻³⁶ (N = 6), standard deviations could not be obtained^{20,37} (N = 2), outlying data (extremely high ECw values³⁸; N = 1), or analysis of ECw in the presence of external

stimuli³⁹ (N = 1; referred to as “other” in Figure 1). In *analysis 2*, 11 articles were fully excluded from analysis because no accurate data extraction was possible (N = 11).

In sum, we selected 25 articles for the meta-analyses in *analysis 1* and 30 additional articles for the walking speed analysis in *analysis 2*.

Study characteristics

Participant characteristics

In total, 367 persons with a lower-limb amputation and 282 persons without an amputation participated in the selected articles

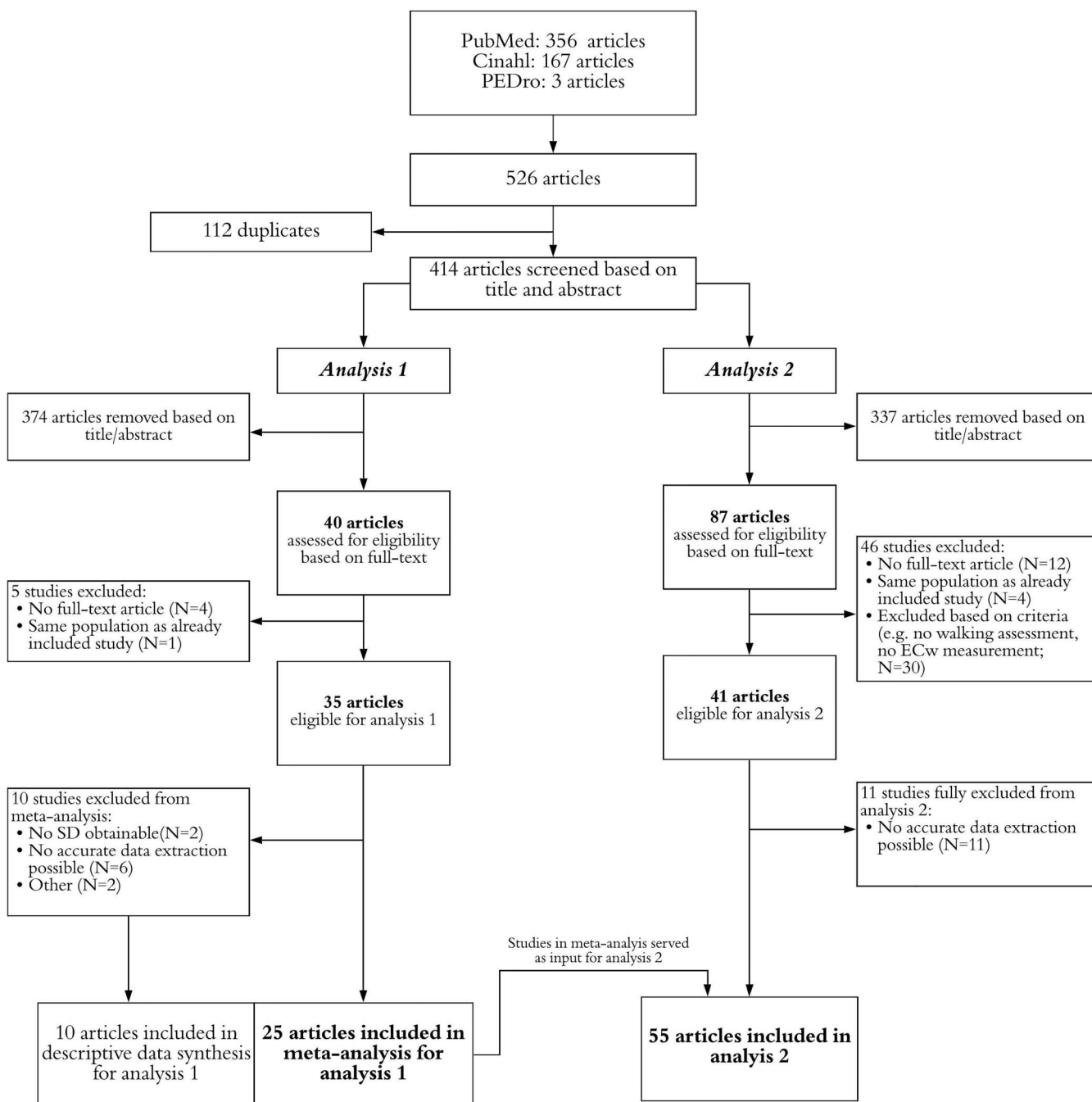


Figure 1. Flowchart of inclusion of articles.

Table 1. Overview of number of articles included in the different analyses by level and cause of amputation.

| | Analysis 1 – influence of level and cause of amputation on ECw (25 articles, describing 37 subgroups) | Analysis 2 – influence of walking speed on ECw (55 articles, describing 78 subgroups) |
|----------------------------|--|--|
| Transfemoral – vascular | 3 | 5 |
| Transfemoral – nonvascular | 15 | 32 |
| Transtibial – vascular | 3 | 9 |
| Transtibial – nonvascular | 16 | 32 |

Abbreviation: ECw, energy cost of walking.
NB: Please keep in mind that the number of articles and subgroups shown for analysis 2 is equal to the sum of the articles in analysis 1 and the additionally included articles in analysis 2.

for *analysis 1* and 362 additional persons with a lower-limb amputation participated in the selected articles for *analysis 2*. Table 1 shows the number and type of specific subgroups that were described in the included articles for *analysis 1* and *analysis 2*. Most of the included articles investigated persons with a non-vascular transtibial or transfemoral amputation. Considerable heterogeneity was noted in terms of participants' characteristics, such as mean age (range controls: 23–60 years; range people with amputation; 22–73 years), sex (85% male), walking speed (range controls: 0.83–1.56 m·s⁻¹; range people with amputation: 0.45–1.50 m·s⁻¹), and time since amputation (range: 9 weeks–31 years). For details for each of the studies, please see the overview tables in Appendix 2 and Appendix 3 (Supplemental Digital Content 1, <http://links.lww.com/POI/A46>).

Experimental protocol

In *analysis 1*, 18 articles assessed ECw using preferred walking speed, whereas 7 articles used an imposed fixed walking speed. Regarding walking surface, 12 articles performed their measurements on a treadmill and 13 articles performed overground measurements, either indoor or outdoor. In *analysis 2*, 20 articles studied ECw while walking at preferred walking speed, whereas 10 articles studied ECw at an imposed fixed speed. In *analysis 2*, 20 articles investigated ECw using a treadmill and 10 articles investigated ECw during overground walking. The duration of the walking trials varied between 2 and 20 minutes. All studies, except for two, did report the requirement of steady state walking. In both *analysis 1* and *analysis 2*, 14 studies used the average value over the last 2 or 3 minutes of their walking trials for analysis of the energy cost. Other studies took the average over shorter periods, whereas two studies in *analysis 1* and 3 studies in *analysis 2* did not provide clear information about the use of averaging methods when calculating the energy cost.

Risk-of-bias assessment

Appendix 5 (Supplemental Digital Content 1, <http://links.lww.com/POI/A46>) shows the NOS scores of each study for *analysis 1* and *analysis 2*. Mean score and SD were 6.4 ± 2.2 (range: 2–9) for *analysis 1* and 4.5 ± 0.9 (range: 2–6) for *analysis 2*. For most studies, stars were awarded for clear descriptions of the study groups and the applied protocol. Overall, stars were often withheld for items relating to the selection and follow-up of study groups, as this was often not explicitly described. In *analysis 1*, comparability of the groups was often achieved in terms of age and sex of the

participants, but only in a few studies were groups comparable in terms of physical fitness or physical activity levels.

Data analysis

Meta-analyses

A total of 25 studies (describing 37 comparisons) were included in the meta-analysis that investigated the difference in ECw between people with and without an amputation at self-selected walking speed. The results showed that persons without an amputation overall have significantly lower ECw compared to people with a lower-limb amputation (MD = 0.06 mL·O₂·kg⁻¹·m⁻¹, 95% CI = [0.04–0.07], Z = 8.80, P < 0.001; Figure 2). Considerable heterogeneity was present (I² = 88%). Subgroup analyses revealed that the difference in ECw was significantly different as a function of levels and causes of amputation ($\chi^2(3) = 165.92$, P < 0.001, I² = 98.2%). ECw was significantly higher compared to controls in all four subgroups (Figure 2). The highest ECw was observed for people with a vascular transfemoral amputation (MD = 0.18 mL·O₂·kg⁻¹·m⁻¹, 95% CI = [0.16–0.21]), followed by the nonvascular transfemoral group (MD = 0.07 mL·O₂·kg⁻¹·m⁻¹, 95% CI = [0.06–0.08]) and the vascular transtibial group (MD = 0.06 mL·O₂·kg⁻¹·m⁻¹, 95% CI = [0.03–0.09]), whereas the smallest (yet still significant) difference in ECw was observed for the nonvascular transtibial group (MD = 0.02 mL·O₂·kg⁻¹·m⁻¹, 95% CI = [0.01–0.03]). As can be seen in Table 2, the increase in ECw was significantly different between all subgroups (P ≤ 0.02), except for the comparison of the nonvascular transfemoral group and vascular transtibial group (P = 0.58).

When expressed as a percentage of the weighted average of ECw of the respective control groups, the ECw for people with a lower-limb amputation at self-selected walking speed was 35% higher compared to people without an amputation. When separately assessed for each of the subgroups, ECw values were 12% higher for the nonvascular transtibial group, 36% for the vascular transtibial group, 41% for the nonvascular transfemoral group, and 102% for the vascular transfemoral group.

Descriptive synthesis

We descriptively synthesized the results of the 10 articles that were excluded from the meta-analysis because no reliable data extraction was possible. All of the excluded articles investigated the ECw related to level of amputation and did not directly compare groups with different causes. Most of the articles showed

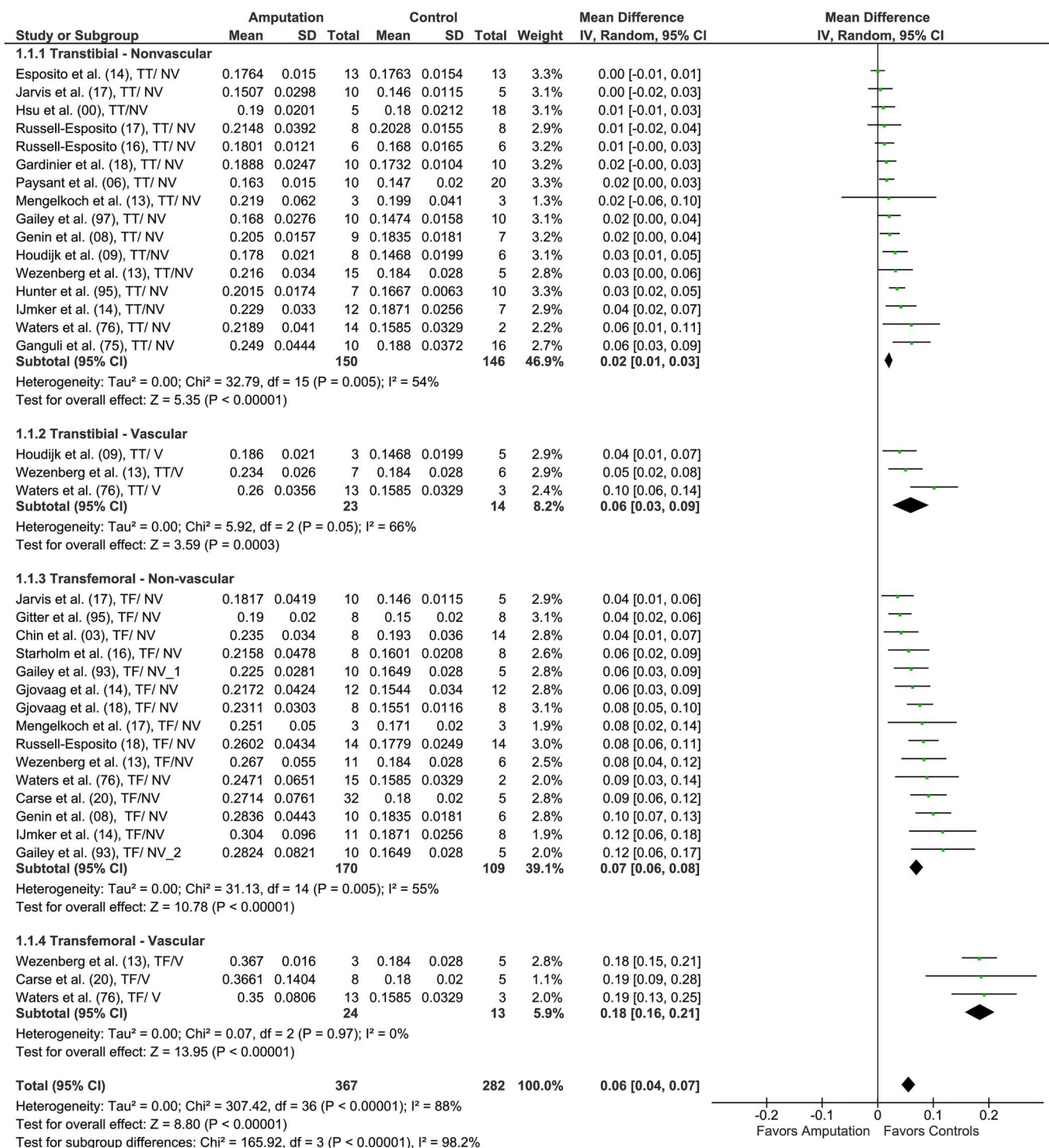


Figure 2. Pooled results of studies that investigated energy cost of walking in people with a lower-limb amputation. TF/NV, transfemoral, nonvascular amputation; TF/V, transfemoral, vascular amputation; TT/NV, transtibial, nonvascular amputation; TT/V, transtibial, vascular amputation. NB1: Average preferred walking speed for each group was as follows: transtibial nonvascular: $1.20 \pm 0.51 \text{ m}\cdot\text{s}^{-1}$; transtibial vascular: $0.82 \pm 0.15 \text{ m}\cdot\text{s}^{-1}$; transfemoral nonvascular: $1.02 \pm 0.20 \text{ m}\cdot\text{s}^{-1}$; and transfemoral vascular: $0.62 \pm 0.11 \text{ m}\cdot\text{s}^{-1}$. NB2: For two of the included studies,^{55,59} SD was obtained using Equation (2), as no other methods could be applied. However, this equation is typically recommended for studies with larger samples. To investigate whether using this equation influenced our results, we performed the meta-analysis also without these two studies, but this had minimal effect on the outcomes, and the main and subgroup effects remained unaffected.

results that were similar to the results found in the meta-analysis. Do Nascimento Garcia et al,³⁸ Herr and Grabowski,³⁶ Gailey et al,²⁰ Jaegers et al,³³ Schnall et al,³⁹ and Ladlow et al³⁵ all showed significant increases in ECw for persons with a nonvascular amputation at the transtibial or transfemoral level compared to

persons without an amputation, with the largest increase found for persons with a transfemoral amputation. This result was also found by Ganguli et al,³² but they did not report any significance values. Similar results were reported by Pinzur et al,³⁷ in people with vascular transtibial and transfemoral amputations, but they did not

Table 2. Overview of pairwise comparisons of energy cost of walking between different subgroups.

| | <i>TF – vascular</i> | <i>TF – nonvascular</i> | <i>TT – vascular</i> | <i>TT – nonvascular</i> |
|-----------------------------|--------------------------|--|--|---|
| <i>TF – vascular</i> | | $\chi^2(1)=60.05$ $p<0.00001^*$ $I^2=98.3\%$ | $\chi^2(1)=33.78$ $p<0.00001^*$ $I^2=97\%$ | $\chi^2(1)=141.11$ $p<0.00001^*$ $I^2=99.3\%$ |
| <i>TF – nonvascular</i> | | | $\chi^2(1)=0.30$ $p=0.580$ $I^2=0\%$ | $\chi^2(1)=42.63$ $p<0.00001^*$ $I^2=97.7\%$ |
| <i>TT – vascular</i> | | | | $\chi^2(1)=5.28$ $p=0.020^*$ $I^2=81\%$ |
| <i>TT – nonvascular</i> | | | | |

Significant effects (p<0.05) are indicated with an asterisk ().*

report significance values either. The studies of Kark et al³⁴ and Eckard et al³¹ seemed to deviate slightly from the results in the meta-analysis. Kark et al³⁴ investigated ECw in transtibial amputees and transfemoral amputees with different causes of amputation, but only found significantly increased ECw for transfemoral amputees compared to people without an amputation. Eckard et al³¹ did not find any differences in ECw in a group consisting of both people with transtibial and transfemoral nonvascular amputations compared to persons without an amputation.

The relation between ECw and self-selected walking speed

Figure 3 shows the association between self-selected walking speed and ECw across different causes and levels of amputation and people without an amputation. Average preferred walking speed for each group was as follows: transfemoral vascular: $0.62 \pm 0.11 \text{ m}\cdot\text{s}^{-1}$; transfemoral nonvascular: $1.02 \pm 0.20 \text{ m}\cdot\text{s}^{-1}$; transtibial vascular: $0.82 \pm 0.15 \text{ m}\cdot\text{s}^{-1}$; and transtibial nonvascular: $1.20 \pm 0.51 \text{ m}\cdot\text{s}^{-1}$. The results indicate that ECw is moderately to strongly associated with self-selected walking speed in all subgroups, as shown by the R² values. It can be observed that especially persons with an amputation because of vascular reasons generally walk below their most economic walking speed, which contributes to their increase in ECw compared to persons without an amputation. Note that the variation in ECw that could be accounted for by differences in walking speed (i.e. a shift of a specific group on their speed-ECw curve to the left ascending flank) seems substantial relative to the variation accounted for by cause or level of amputation alone (i.e. an upward shift of the speed-ECw curves between groups).

Discussion

The aim of this study was to provide quantitative estimates of differences in ECw between people with and without a lower-limb

amputation and to investigate the influence of cause of amputation, level of amputation, and walking speed using a systematic review and meta-analysis of previous literature. In agreement with our expectations and previous research,⁶ the results of this study showed that ECw is significantly higher in people with an amputation who walk with a lower-limb prosthesis compared to people without an amputation (35%). On average, the difference in ECw is most pronounced in people with a transfemoral amputation because of vascular reasons (102%), followed by nonvascular transfemoral amputation (41%), vascular transtibial amputation (36%), and lowest after nonvascular transtibial amputation (12%). Furthermore, results suggest that reductions in self-selected walking speed seem to be a major contributor to the higher ECw in people with an amputation.

In total, we included 25 articles in the meta-analysis, which described 37 comparisons between designated subgroups of people with a lower-limb amputation and people without an amputation. These comparisons were, however, not distributed equally between subgroups. Specifically, people with amputations because of vascular problems were underrepresented in literature. Only four articles in the meta-analysis investigated ECw for persons with a vascular amputation, together including 47 persons with an amputation. From these articles, data on three vascular-transtibial groups (n = 23) and three vascular-transfemoral groups (n = 24) could be derived. It should be acknowledged that this limited amount of data reduces the reliability of the estimates for these subgroups. Please note that most articles that were only included in the descriptive synthesis showed similar results to those in the meta-analysis, both in terms of ECw and in terms of relative underrepresentation of people with a vascular amputation.

Generally, the results of our meta-analysis are in agreement with the study of Waters et al,⁶ as both studies indicate the highest ECw for persons with a vascular transfemoral amputation and the lowest ECw for nonvascular transtibial amputations. Although the

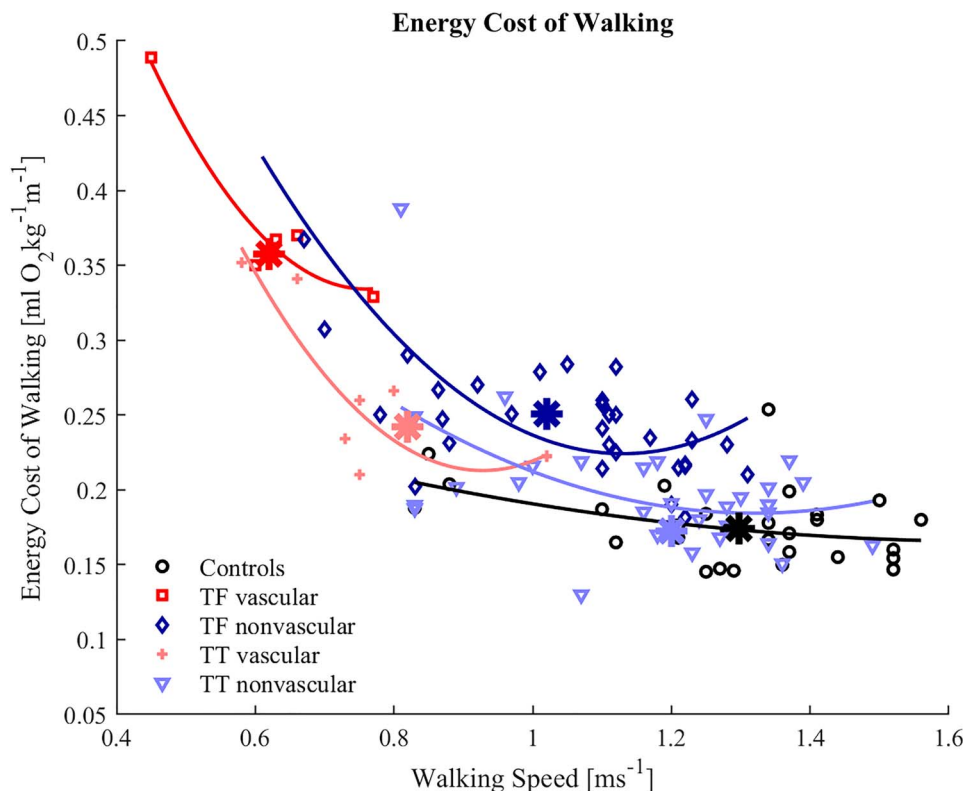


Figure 3. The effect of walking speed on ECw. The average ECw and walking speed derived from analysis 1 is indicated with an asterisk (*) for each subgroup. CO, controls; TT, transtibial; TF, transfemoral. The values of the coefficients a, b, and c represent the description of the second-order polynomial function for each subgroup. CO: $a = 0.06$, $b = -0.19$, $c = 0.32$, $R^2 = 0.17$; TF vascular: $a = 1.58$, $b = -2.40$, $c = 1.24$, $R^2 = 0.93$; TF nonvascular: $a = 0.73$, $b = -1.66$, $c = 1.16$, $R^2 = 0.60$; TT vascular: $a = 1.23$, $b = -2.28$, $c = 1.27$, $R^2 = 0.75$; TT nonvascular: $a = 0.27$, $b = -0.72$, $c = 0.66$, $R^2 = 0.27$. ECw, energy cost of walking.

current meta-analysis shows that people with an amputation have higher ECw compared to people without an amputation, these differences were smaller than those reported by Waters et al.⁶ Waters et al⁶ reported the highest ECw values among all included studies for each single subgroup of people with an amputation. Where Waters et al⁶ reported an increase between 25% and 120%, we found an average increase between 12% and 102%. This overestimation could be a result from the relatively small population studied by Waters et al,⁶ which might not have been fully representative for the general population of people with a lower-limb amputation. In addition, improved rehabilitation and/or prosthetic technology in recent years may have contributed to these different estimates. Worthy of note, however, no clear trend between year of publication and differences in energy cost can be observed among the included studies (Figure 2). Albeit that we only included studies at self-selected comfortable walking speed, while the advantages of some modern prostheses have been shown to be more apparent at slow or high walking speeds.⁴⁰

Our results show that self-selected walking speed partly accounts for the higher ECw in people with a lower-limb amputation. The relation between walking speed and ECw can be modeled as a U-shaped function.^{41,42} For healthy individuals without an amputation, costs are minimal around $1.2 \text{ m}\cdot\text{s}^{-1}$ but rise rapidly at lower and faster walking speeds. Figure 3 provides additional insight into the effect of walking speed on ECw by visualizing the position of the curves of all subgroups relative to each other. The coefficients of

these curves do not have a physiological meaning, but only serve to describe the relationship between self-selected walking speed and ECw for each of the subgroups. It is expected that the speed-ECw curves of people with a lower-limb amputation are shifted upward as a consequence of reduced gait economy.²⁵ Figure 3 demonstrates that irrespective of such an upward shift, a substantial part of the difference in ECw at self-selected walking speed is because of the fact that people with a lower-limb amputation, and especially those with a vascular cause of amputation, walk at slow speeds on the steeply ascending side of the speed-ECw curve. Hence, differences in ECw at self-selected walking speed between groups could partly be explained by their lower self-selected walking speeds, next to the upward shift of the speed-ECw curve. Note that an accurate analysis of the speed-ECw curves could not be performed in this study because data of subgroups were not available over comparable and full ranges of the walking speed spectrum. Therefore, we cannot draw definitive conclusions on the potential upward shift or shift in most economic speed for these subgroups.

Previous studies have shown that for people with a lower-limb amputation, especially those with vascular cause of amputation and transfemoral amputation, preferred walking speed is generally slower than their most economic speed.^{25,26} People might reduce speed because of balance problems and associated fear of falling,⁴³ but it has been shown that the reduction in walking speed might also be related to energetic limitations. People with a lower-limb amputation generally have a reduced aerobic capacity, especially

people with a vascular cause of amputation.⁴⁴ The combination of reduced capacity and high demand increases the relative aerobic load at a given walking speed, which is known to affect quality of life in people with a lower-limb amputation.⁸ Reducing self-selected walking speed may therefore be necessary to maintain aerobic load within sustainable limits, that is, at an acceptable percentage of maximal aerobic capacity.^{6,26} Yet this comes at the expense of walking economy. Consequently, next to level and cause of amputation, self-selected walking speed (and underlying factors such as physical fitness and fear of falling) needs to be taken into account as an important predictor of the ECw of individuals with lower-limb amputation.

Our current review complements recent work by van Schaik et al.,⁴⁵ who performed a systematic review and meta-analysis of the metabolic requirement of daily activities, including walking, in people with lower-limb amputation. In contrast to our analysis, this earlier study used energy consumption per unit of time ($\text{mL}\cdot\text{O}_2\cdot\text{kg}^{-1}\cdot\text{min}^{-1}$) as outcome of interest. In agreement with our results, they found a significant effect of level of amputation on energy requirement of walking, but no effect of cause of amputation was found. This was attributed to the low number of studies reporting on people with vascular cause of amputation. Van Schaik et al.⁴⁵ showed that walking at slower speeds resulted in lower energy consumption per unit of time—which is in line with the idea that people with a lower-limb amputation probably walk slower to reduce the relative aerobic load of walking. However, when energy consumption is expressed per unit of time, it is ignored that such a decrease in walking speed reduces walking economy (i.e. energy cost per unit distance). Our current review thus provides further important insights into the effects of reduced preferred walking speed on energy cost of people with different levels and causes of amputation. In addition, we also show how slower self-selected walking speed in persons with an amputation is related to an increase in energy cost, both as function of level and cause of amputation, which was not available in the study by van Schaik et al.⁴⁵

Limitations

One main limitation of the current review is the heterogeneity of the included studies in terms of group size, participant characteristics (e.g. age and time since amputation), and study characteristics (e.g. walking speed and duration, treadmill vs overground walking). Our risk-of-bias assessment highlights the importance of standardizing measurement protocols and measuring and reporting possible confounding factors. This heterogeneity—which has also been discussed by others^{7,45,46}—could explain the considerable range of estimates for increased ECw at preferred walking speed between studies. Moreover, this heterogeneity may influence the accuracy of our estimates, when factors such as group size, participants, and study characteristics were not distributed equally over the different subgroups. Although there were not enough studies available to statistically investigate the effect of such factors, inspection of the included studies did not point to clear systematic differences in these factors between subgroups. Our second limitation is related to converting all outcomes into the same unit. The applied equations included some assumptions about resting metabolism and RER. In Equation (1), RER was

assumed to be equal to 1; this value might be slightly too high to achieve during walking for people with an amputation. However, Equation (1) was applied to only 3 studies in *analysis 1* and 6 studies in *analysis 2*. Moreover, effect of lower bound RER values would not exceed 5% in ECw and would not have affected our overall conclusions. A final limitation pertains to the fact that this systematic review was not prospectively registered with PROSPERO, which would in hindsight have been preferred.

Further research

The current meta-analysis provides quantitative estimates of ECw in people with a lower-limb amputation with different causality and at different levels. However, the reliability of these results may be affected by the heterogeneity of the studies that were combined. Therefore, future research should clearly report and standardize factors such as walking speed, walking surface, and duration of the walking trial. Moreover, the risk-of-bias assessment shows the importance of matching possibly confounding factors such as age and physical fitness when comparing different groups of persons with and without amputations, and of providing detailed information regarding data analysis (i.e. walking at steady state and calculation of ECw). Related to this, there is a clear need for studies that investigate the interaction of level and cause of amputation and walking speed within a single study. This is essential to better understand the effects of these factors on the ECw after amputation. Furthermore, future research should especially focus on the ECw and walking speed of people with an amputation because of vascular reasons because data for this specific patient group are scarce while the incidence of dysvascular amputation is the highest of all causes in Western countries. This group is also known to have limited exercise capacity, which compounds the negative effects of high aerobic demand of walking for regaining walking ability.^{26,44}

Conclusion

This systematic review provided updated quantitative estimates of ECw of people with a lower-limb amputation at their preferred walking speed, stratified for level and cause of amputation. Based on our meta-analysis, differences in ECw of +12% and +41% were found for people with nonvascular transtibial and transfemoral amputations compared to people without an amputation, respectively, and more pronounced differences in ECw were found for people with vascular transtibial (+36%) and transfemoral amputations (+102%). Moreover, our data suggest that a slow preferred walking speed may be a key factor for the observed increase in ECw in people with a lower-limb amputation. The estimates provided in this review study can be used as reference values in clinical practice, to improve patient expectations, guide clinical decision making, and benchmark prosthetic developments.

Author contribution

The authors disclosed the following roles as contributors to this article: S.E. performed the data collection, analysis, and writing of the article. H.H. conceived the general idea of this article and contributed to

writing and proofing of the manuscript. E.K. performed RevMan data analysis and contributed to writing and proofing the manuscript.

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Supplemental material

There is no supplemental material in this article.

References

- Fard B, Dijkstra PU, Stewart RE, et al. Incidence rates of dysvascular lower extremity amputation changes in Northern Netherlands: a comparison of three cohorts of 1991-1992, 2003-2004 and 2012-2013. *PLoS One* 2018; 13: e0204623.
- Rommers, G. M., Vos, L. D. W., Groothoff, J. W., Schuiling, C. H., & Eisma, W. H. (1997). Epidemiology of lower limb amputees in the north of The Netherlands: aetiology, discharge destination and prosthetic use. *Prosthetics and Orthotics International*, 21(2), 92-99.
- Davies B and Datta D. Mobility outcome following unilateral lower limb amputation. *Prosthet Orthot Int* 2003; 27: 186-190.
- MacKenzie EJ, Bosse MJ, Castillo RC, et al. Functional outcomes following trauma-related lower-extremity amputation. *JBJS* 2004; 86: 1636-1645.
- Sansam K, Neumann V, O'Connor R, et al. Predicting walking ability following lower limb amputation: a systematic review of the literature. *J Rehabil Med* 2009; 41: 593-603.
- Waters R, Perry J, Antonelli D, et al. Energy cost of walking of amputees: the influence of level of amputation. *J Bone Joint Surg Am* 1976; 58: 42-46.
- Van Velzen J, van Bennekom CA, Polomski W, et al. Physical capacity and walking ability after lower limb amputation: a systematic review. *Clin Rehabil* 2006; 20: 999-1016.
- Franceschini M, Rampello A, Agosti M, et al. Walking performance: correlation between energy cost of walking and walking participation. New statistical approach concerning outcome measurement. *PLoS One* 2013; 8: e56669.
- Houdijk H, Pollmann E, Groenewold M, et al. The energy cost for the step-to-step transition in amputee walking. *Gait Posture* 2009; 30: 35-40.
- Kuo AD and Donelan JM. Dynamic principles of gait and their clinical implications. *Phys Ther* 2010; 90: 157-174.
- Meinders M, Gitter A and Czerniecki JM. The role of ankle plantar flexor muscle work during walking. *Scand J Rehabil Med* 1998; 30: 39-46.
- Lamoth CJ, Ainsworth E, Polomski W, et al. Variability and stability analysis of walking of transfemoral amputees. *Med Eng Phys* 2010; 32: 1009-1014.
- Kendell C, Lemaire E, Dudek N, et al. Indicators of dynamic stability in transtibial prosthesis users. *Gait Posture* 2010; 31: 375-379.
- Viton JM, Mouchnino L, Mille M, et al. Equilibrium and movement control strategies in trans-tibial amputees. *Prosthet Orthot Int* 2000; 24: 108-116.
- Hak L, van Dieën JH, van der Wurff P, et al. Walking in an unstable environment: strategies used by transtibial amputees to prevent falling during gait. *Arch Phys Med Rehabil* 2013; 94: 2186-2193.
- Houdijk H. Effects of balance support on energy cost of walking in people with lower limb amputation. *Arch Phys Med Rehabil* 2020; 102: 1340-1346.e3.
- Waters RL and Mulroy S. The energy expenditure of normal and pathologic gait. *Gait Posture* 1999; 9: 207-231.
- Esposito ER, Rodriguez KM, Rábago CA, et al. Does unilateral transtibial amputation lead to greater metabolic demand during walking. *J Rehabil Res Dev* 2014; 51: 1287-1296.
- Russell Esposito E, Rábago CA and Wilken J. The influence of traumatic transfemoral amputation on metabolic cost across walking speeds. *Prosthet Orthot Int* 2018; 42: 214-222.
- Gailey R, Wenger M, Raya M, et al. Energy expenditure of trans-tibial amputees during ambulation at self-selected pace. *Prosthet Orthot Int* 1994; 18: 84-91.
- Mengelkoch L, Kahle J and Highsmith M. Energy costs & performance of transtibial amputees & non-amputees during walking & running. *Int J Sports Med* 2014; 35: 1223-1228.
- Delussu AS, Paradisi F, Brunelli S, et al. Comparison between SACH foot and a new multiaxial prosthetic foot during walking in hypomobile transtibial amputees: physiological responses and functional assessment. *Eur J Phys Rehabil Med* 2016; 52: 304-309.
- Paysant J, Beyaert C, Datié AM, et al. Influence of terrain on metabolic and temporal gait characteristics of unilateral transtibial amputees. *J Rehabil Res Dev* 2006; 43: 153-160.
- Starholm IM, Mirtaheri P, Kapetanovic N, et al. Energy expenditure of transfemoral amputees during floor and treadmill walking with different speeds. *Prosthet Orthot Int* 2016; 40: 336-342.
- Genin JJ, Bastien GJ, Franck B, et al. Effect of speed on the energy cost of walking in unilateral traumatic lower limb amputees. *Eur J Appl Physiol* 2008; 103: 655.
- Wezenberg D, van der Woude LH, Faber WX, et al. Relation between aerobic capacity and walking ability in older adults with a lower-limb amputation. *Arch Phys Med Rehabil* 2013; 94: 1714-1720.
- Traballesi M, Porcacchia P, Aversa T, et al. Energy cost of walking measurements in subjects with lower limb amputations: a comparison study between floor and treadmill test. *Gait Posture* 2008; 27: 70-75.
- Wells G, Shea B, O'Connell D, et al. *Newcastle-Ottawa Quality Assessment Scale Cohort Studies*. University of Ottawa. Ottawa 2014.
- Garby L and Astrup A. The relationship between the respiratory quotient and the energy equivalent of oxygen during simultaneous glucose and lipid oxidation and lipogenesis. *Acta Physiol Scand* 1987; 129: 443-444.
- Higgins JPT, Thomas J, Chandler J, Cumpston M, Li T, Page MJ, Welch VA (editors). *Cochrane Handbook for Systematic Reviews of Interventions*. 2nd Edition. Chichester (UK): John Wiley & Sons, 2019.
- Eckard CS, Pruziner AL, Sanchez AD, et al. Metabolic and body composition changes in first year following traumatic amputation. *J Rehabil Res Dev* 2015; 52.
- Ganguli S, Datta S, Chatterjee B, et al. Metabolic cost of walking at different speeds with patellar tendon-bearing prosthesis. *J Appl Physiol* 1974; 36: 440-443.
- Jaegers SM, Vos LD, Rispen P, et al. The relationship between comfortable and most metabolically efficient walking speed in persons with unilateral above-knee amputation. *Arch Phys Med Rehabil* 1993; 74: 521-525.
- Kark L, Vickers D, McIntosh A, et al. Use of gait summary measures with lower limb amputees. *Gait Posture* 2012; 35: 238-243.
- Ladlow P, Nightingale TE, McGuigan MP, et al. Impact of anatomical placement of an accelerometer on prediction of physical activity energy expenditure in lower-limb amputees. *PLoS One* 2017; 12: e0185731.
- Herr HM and Grabowski AM. Bionic ankle-foot prosthesis normalizes walking gait for persons with leg amputation. *Proc Biol Sci* 2012; 279: 457-464.
- Pinzur MS, Gold J, Schwartz D, et al. Energy demands for walking in dysvascular amputees as related to the level of amputation. *Orthopedics* 1992; 15: 1033-1037.
- Garcia MMdN, Lima JRPd, Costa Junior JD, et al. Energy expenditure and cardiovascular response to traumatic lower limb amputees' gait. *Fisioterapia em Movimento* 2015; 28: 259-268.
- Schnall BL, Wolf EJ, Bell JC, et al. Metabolic analysis of male service-members with transtibial amputations carrying military loads. *J Rehabil Res Dev* 2012; 49.
- Highsmith MJ, Kahle JT, Bongiorni DR, et al. Safety, energy efficiency, and cost efficacy of the C-Leg for transfemoral amputees: a review of the literature. *Prosthet Orthot Int* 2010; 34: 362-377.
- Molen NH, Rozendal RH and Boon W. Graphic representation of the relationship between oxygen consumption and characteristics of normal gait of the human male. *Proc K Ned Akad Wet C* 1972; 75: 305-314.
- Zarrugh M, Todd F and Ralston H. Optimization of energy expenditure during level walking. *Eur J Appl Physiol Occup Physiol* 1974; 33: 293-306.
- Miller WC, Speechley M and Deathe AB. Balance confidence among people with lower-limb amputations. *Phys Ther* 2002; 82: 856-865.
- Wezenberg D, de Haan A, Faber WX, et al. Peak oxygen consumption in older adults with a lower limb amputation. *Arch Phys Med Rehabil* 2012; 93: 1924-1929.
- van Schaik L, Geertzen JH, Dijkstra PU, et al. Metabolic costs of activities of daily living in persons with a lower limb amputation: a systematic review and meta-analysis. *PLoS One* 2019; 14: e0213256.
- Kahle JT, Highsmith MJ, Schaepper H, et al. Predicting walking ability following lower limb amputation: an updated systematic literature review. *Technol Innovat* 2016; 18: 125.

47. Carse B, Scott H, Brady L, et al. A characterisation of established unilateral transfemoral amputee gait using 3D kinematics, kinetics and oxygen consumption measures. *Gait Posture* 2020; 75: 98–104.
48. Chin T, Sawamura S, Shiba R, et al. Effect of an Intelligent Prosthesis (IP) on the walking ability of young transfemoral amputees: comparison of IP users with able-bodied people. *Am J Phys Med Rehabil* 2003; 82: 447–451.
49. Gailey R, Nash MS, Atchley T, et al. The effects of prosthesis mass on metabolic cost of ambulation in non-vascular trans-tibial amputees. *Prosthet Orthot Int* 1997; 21: 9–16.
50. Gailey R, Lawrence D, Burditt C, et al. The CAT-CAM socket and quadrilateral socket: a comparison of energy cost during ambulation. *Prosthet Orthot Int* 1993; 17: 95–100.
51. Ganguli S, Bose KS and Datta SR. Performance of BK amputees using PTB prostheses. *Acta Orthop Scand* 1975; 46: 123–134.
52. Gardinier ES, Kelly BM, Wensman J, et al. A controlled clinical trial of a clinically-tuned powered ankle prosthesis in people with transtibial amputation. *Clin Rehabil* 2018; 32: 319–329.
53. Gitter A, Czerniecki J and Weaver K. A reassessment of center-of-mass dynamics as a determinate of the metabolic inefficiency of above-knee amputee ambulation. *Am J Phys Med Rehabil* 1995; 74: 332–338.
54. Gjovaag T, Starholm IM, Mirtaheeri P, et al. Assessment of aerobic capacity and walking economy of unilateral transfemoral amputees. *Prosthet Orthot Int* 2014; 38: 140–147.
55. Gjovaag T, Mirtaheeri P and Starholm IM. Carbohydrate and fat oxidation in persons with lower limb amputation during walking with different speeds. *Prosthet Orthot Int* 2018; 42: 304–310.
56. Hsu M-J, Nielsen DH, Yack J, et al. Physiological comparisons of physically active persons with transtibial amputation using static and dynamic prostheses versus persons with nonpathological gait during multiple-speed walking. *JPO J Prosthetics Orthot* 2000; 12: 60–67.
57. Hunter D, Cole ES, Murray JM, et al. Energy expenditure of below-knee amputees during harness-supported treadmill ambulation. *J Orthop Sports Phys Ther* 1995; 21: 268–276.
58. Ijmker T, Houdijk H, Lamoth CJ, et al. Energy cost of balance control during walking decreases with external stabilizer stiffness independent of walking speed. *J Biomech* 2013; 46: 2109–2114.
59. Jarvis HL, Bennett AN, Twiste M, et al. Temporal spatial and metabolic measures of walking in highly functional individuals with lower limb amputations. *Arch Phys Med Rehabil* 2017; 98: 1389–1399.
60. Mengelkoch LJ, Kahle JT and Highsmith MJ. Energy costs and performance of transfemoral amputees and non-amputees during walking and running: a pilot study. *Prosthet Orthot Int* 2017; 41: 484–491.
61. Esposito ER, Choi HS, Darter BJ, et al. Can real-time visual feedback during gait retraining reduce metabolic demand for individuals with transtibial amputation? *PloS One* 2017; 12: e0171786.
62. Russell Esposito E, Aldridge Whitehead JM and Wilken JM. Step-to-step transition work during level and inclined walking using passive and powered ankle-foot prostheses. *Prosthet Orthot Int* 2016; 40: 311–319.
63. Askew GN, McFarlane LA, Minetti AE, et al. Energy cost of ambulation in trans-tibial amputees using a dynamic-response foot with hydraulic versus rigid “ankle”: insights from body centre of mass dynamics. *J NeuroEng Rehabil* 2019; 16: 39.
64. Barth DG, Schumacher L and Thomas SS. Gait analysis and energy cost of below-knee amputees wearing six different prosthetic feet. *JPO J Prosthetics Orthot* 1992; 4: 63–75.
65. Bell JC, Wolf EJ, Schnall BL, et al. Transfemoral amputations: is there an effect of residual limb length and orientation on energy expenditure? *Clin Orthop Relat Res* 2014; 472: 3055–3061.
66. Bellmann M, Schmalz T and Blumentritt S. Comparative biomechanical analysis of current microprocessor-controlled prosthetic knee joints. *Arch Phys Med Rehabil* 2010; 91: 644–652.
67. Buckley JG, Jones SF and Birch KM. Oxygen consumption during ambulation: comparison of using a prosthesis fitted with and without a tele-torsion device. *Arch Phys Med Rehabil* 2002; 83: 576–581.
68. Buckley JG, Spence WD and Solomonidis SE. Energy cost of walking: comparison of “intelligent prosthesis” with conventional mechanism. *Arch Phys Med Rehabil* 1997; 78: 330–333.
69. Cao W, Zhao W, Yu H, et al. Maximum swing flexion or gait symmetry: a comparative evaluation of control targets on metabolic energy expenditure of amputee using intelligent prosthetic knee. *BioMed Res Int* 2018; 2018: 2898546.
70. Casillas J-M, Dulieu V, Cohen M, et al. Bioenergetic comparison of a new energy-storing foot and SACH foot in traumatic below-knee vascular amputations. *Arch Phys Med Rehabil* 1995; 76: 39–44.
71. Darter BJ and Wilken JM. Gait training with virtual reality-based real-time feedback: improving gait performance following transfemoral amputation. *Phys Ther* 2011; 91: 1385–1394.
72. Darter BJ and Wilken JM. Energetic consequences of using a prosthesis with adaptive ankle motion during slope walking in persons with a trans-tibial amputation. *Prosthet Orthot Int* 2014; 38: 5–11.
73. Detrembleur C, Vanmarsenille JM, De Cuyper F, et al. Relationship between energy cost, gait speed, vertical displacement of centre of body mass and efficiency of pendulum-like mechanism in unilateral amputee gait. *Gait Posture* 2005; 21: 333–340.
74. Göktepe AS, Cakir B, Yilmaz B, et al. Energy expenditure of walking with prostheses: comparison of three amputation levels. *Prosthet Orthot Int* 2010; 34: 31–36.
75. Grabowski AM, Rifkin J and Kram R. K3 Promoter™ prosthetic foot reduces the metabolic cost of walking for unilateral transtibial amputees. *JPO J Prosthetics Orthot* 2010; 22: 113–120.
76. Graham LE, Datta D, Heller B, et al. A comparative study of oxygen consumption for conventional and energy-storing prosthetic feet in transfemoral amputees. *Clin Rehabil* 2008; 22: 896–901.
77. Hsu M-J, Nielsen DH, Lin-Chan S-J, et al. The effects of prosthetic foot design on physiologic measurements, self-selected walking velocity, and physical activity in people with transtibial amputation. *Arch Phys Med Rehabil* 2006; 87: 123–129.
78. Kirker S, Keymer S, Talbot J, et al. An assessment of the intelligent knee prosthesis. *Clin Rehabil* 1996; 10: 267–273.
79. Lin-Chan S-J, Nielsen DH, Yack HJ, et al. The effects of added prosthetic mass on physiologic responses and stride frequency during multiple speeds of walking in persons with transtibial amputation. *Arch Phys Med Rehabil* 2003; 84: 1865–1871.
80. Macfarlane PA, Nielsen DH, Shurr DG, et al. Transfemoral amputee physiological requirements: comparisons between SACH foot walking and Flex-Foot walking. *JPO J Prosthetics Orthot* 1997; 9: 138–143.
81. McDonald CL, Kramer PA, Morgan SJ, et al. Energy expenditure in people with transtibial amputation walking with crossover and energy storing prosthetic feet: a randomized within-subject study. *Gait Posture* 2018; 62: 349–354.
82. Orendurff MS, Segal AD, Klute GK, et al. Gait efficiency using the C-Leg. *J Rehabil Res Dev* 2006; 43: 239.
83. Rosenblatt NJ, Ehrhardt T, Fergus R, et al. Effects of vacuum-assisted socket suspension on energetic costs of walking, functional mobility, and prosthesis-related quality of life. *JPO J Prosthetics Orthot* 2017; 29: 65–72.
84. Schmalz T, Blumentritt S and Jarasch R. Energy expenditure and biomechanical characteristics of lower limb amputee gait: the influence of prosthetic alignment and different prosthetic components. *Gait Posture* 2002; 16: 255–263.
85. Seymour R, Engbretson B, Kott K, et al. Comparison between the C-leg® microprocessor-controlled prosthetic knee and non-microprocessor control prosthetic knees: A preliminary study of energy expenditure, obstacle course performance, and quality of life survey. *Prosthet Orthot Int* 2007; 31: 51–61.
86. Smith JD and Martin PE. Effects of prosthetic mass distribution on metabolic costs and walking symmetry. *J Appl Biomech* 2013; 29: 317–328.
87. Starholm I-M, Gjovaag T and Mengshoel AM. Energy expenditure of transfemoral amputees walking on a horizontal and tilted treadmill simulating different outdoor walking conditions. *Prosthet Orthot Int* 2010; 34: 184–194.
88. Tekin L, Safaz Y, Göktepe AS, et al. Comparison of quality of life and functionality in patients with traumatic unilateral below knee amputation and salvage surgery. *Prosthet Orthot Int* 2009; 33: 17–24.
89. Torburn L, Powers CM, Gutierrez R, et al. Energy expenditure during ambulation in dysvascular and traumatic below-knee amputees: a comparison of five prosthetic feet. *J Rehabil Res Dev* 1995; 32: 111.
90. Trallesi M, Delussu AS, Averna T, et al. Energy cost of walking in transfemoral amputees: comparison between Marlo Anatomical Socket and Ischial Containment Socket. *Gait Posture* 2011; 34: 270–274.
91. Hsu MJ, Nielsen DH, Yack HJ, et al. Physiological measurements of walking and running in people with transtibial amputations with 3 different prostheses. *J Orthop Sports Phys Ther* 1999; 29: 526–533.
92. Macfarlane R and Jeffcoate W. Factors contributing to the presentation of diabetic foot ulcers. *Diabet Med* 1997; 14: 867–870.
93. Rosenblatt NJ, Bauer A and Grabiner MD. Relating minimum toe clearance to prospective, self-reported, trip-related stumbles in the community. *Prosthet Orthot Int* 2017; 41: 387–392.
94. Ijmker T, Noten S, Lamoth C, et al. Can external lateral stabilization reduce the energy cost of walking in persons with a lower limb amputation? *Gait Posture* 2014; 40: 616–621.