

# Diffusion measures and Connectometry in the Human Hippocampal-Subfields Using Super-Resolution HYDI.

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## Synopsis

The aging process is known to cause morphological and structural alterations in the human brain. Using a sub-millimeter super-resolution hybrid diffusion imaging (HYDI), we studied the effects of aging on the structural connectivity between the hippocampal subfields as well as between the hippocampus and the cerebral cortex.

## Introduction

The recent advancements in high-resolution anatomical magnetic resonance imaging (MRI) such as T1-weighted (T1W) or T2-weighted (T2W) imaging have enabled the feasibility of submillimeter in-plane resolution of the hippocampus, which has allowed the automatic segmentation of the hippocampal subfields<sup>1,2</sup>. Using anatomical MRI, most of the previous studies focused on the volumetric changes in the hippocampal subfields<sup>3,4</sup>. However, changes in specific hippocampal fiber pathways within the brain's structural networks have not been closely investigated, largely due to the limited spatial resolution in diffusion MRI (dMRI). With an adequate spatial resolution, dMRI could provide microstructural measurements and the associated tractography for the in-vivo human hippocampal subfields. In this study, we used super-resolution hybrid diffusion imaging (HYDI) to study the effects of aging on diffusion metrics in the hippocampal subfields and on structural connectivity between the subfields.

## Methods

**Patients:** Twelve healthy participants were recruited from the Indiana Alzheimer Disease Center and communities. There were five participants with an age larger than 65 years old (73 +/- 9.9 years) and the remaining seven participants with an age less than 35 years old (28.6 +/- 4.2 years). Each group had two male participants. **Imaging:** MRI scans were performed on the participants in a Siemens MAGNETOM Prisma 3.0 T scanner. High-resolution T1W images were acquired with an MPRAGE sequence at 0.8 x 0.8 x 0.8 mm<sup>3</sup> resolution, TR=2400 ms, TE=2.22 ms, TI=1000 ms, flip-angle=8°, 256 mm field-of-view, 208 slices, and GRAPPA acceleration iPAT= 2. A high-resolution Turbo-Spin-Echo T2W images were acquired with a high in-plane resolution of 0.4 x 0.4 mm in an oblique plane perpendicular to the main axis of the hippocampus, a slice thickness of 2 mm, TR=8310 ms, TE=50 ms, flip-angle=122°, 175 mm field-of-view, 32 slices, and GRAPPA acceleration iPAT=2. HYDI<sup>5,6</sup> was performed with a single-shot spin-echo EPI sequence, a multiband factor of 3, TE=74.2 ms, and TR=4164 ms, 220 mm field of view, 114 slices, isotropic resolution of 1.25mm, and 10:51 (min: sec) acquisition time. The diffusion scheme included four shells of b-values 500, 800, 1600, 2600 s/mm<sup>2</sup>, a total of 134 diffusion-directions, and 8 non-diffusion weighted volumes. Two sets of data were acquired with reversed phase-encode blips. **Preprocessing:** All the DW-images were denoised from Rician noise using overcomplete local-Principal-Component-Analysis as proposed in<sup>7</sup>. FSL-*topup* and FSL-*eddy*<sup>8</sup>, part of the FSL package version 6.0.0 (FMRIB, Oxford, UK), were used to correct motion, susceptibility, and eddy current distortions. To achieve super-resolution, a collaborative-patch-based-method<sup>9</sup> was then used to bring the 1.25 mm<sup>3</sup> resolution HYDI data to a submillimeter resolution of 0.625 mm<sup>3</sup>. This submillimeter diffusion data was then used to compute diffusion tensor imaging (DTI) metrics and neurite density and orientation dispersion imaging (NODDI) metrics<sup>10</sup>. **Post-processing:** Figure 1 shows the workflow of the postprocessing. The high-resolution T1W and T2W images were used for segmenting the hippocampal subfields with the Automatic Segmentation of Hippocampal Subfields (ASHS) method<sup>2</sup>. The hippocampal subfields were transformed from the T2W image space to the super-resolution diffusion space using ANTs<sup>11</sup>. In parallel, the HYDI multi-shell data was processed for tractography with generalized q-sampling imaging (GQI) approach<sup>12</sup> and the hippocampal subfields as seed regions-of-interest (ROIs). Connectivity matrices (i.e., connectomes) were computed between the subfields and between the hippocampus and the cerebral cortices as in normalized streamline counts. **Connectometry statistical analysis:** To study the effect of aging on the hippocampus-cortex streamline connections, a group-wise connectometry analysis was used<sup>13,14</sup>. In this analysis, the diffusion data were reconstructed in the MNI space using q-space diffeomorphic reconstruction<sup>15</sup> to obtain the spin distribution function<sup>12</sup>. The output resolution of the resampling to the MNI space is 1mm-isotropic. The quantitative anisotropy (QA)<sup>12</sup> was extracted as the local connectome fingerprint<sup>14</sup> and used in the connectometry analysis. The analysis used the MNI-space hippocampal regions<sup>16</sup> as ROIs.

## Results

Figure 2 shows the diffusion metrics of each of the hippocampal subfields, including the Cornu-Ammonis subfields (CA1-3), dentate gyrus (DG), entorhinal cortex (ERC) and subiculum (SUB). The older participants had significantly lower DTI fractional anisotropy in the CA1, DG and CA3 (i.e., Welch two-sample t-test p-value < 0.05, without multiple-comparison correction). While not significant, a trend of lower NODDI intracellular volume fraction (ICVF) was observed in older participants. Figure 3a shows the connectivity matrices computed using the number of streamlines normalized by the volume of the subfields involved in each connection. Connectivity matrices were computed in the left and right hippocampal subfields in the older and younger groups; Figure 3b shows the non-zero connectivity vectors from the left and right hippocampi to cortical regions for both age groups. Figures 3,4 show a significantly weaker connection in the older participants, especially in the left hippocampus. The connectometry analysis depicted by Figure 5, shows that the QA was negatively correlated with the subjects' age in each of the MNI-hippocampal ROIs with a false discovery rate (FDR) that ranged between 0.0075 and 0.01.

## Discussion and Conclusion

Our study suggests that age decreases the structural organization inside the hippocampal subfields as well as along the fiber tracks between the hippocampal subfields and the cerebral cortices with decreased FA and QA. This method holds promise for providing information regarding

hippocampal integrity in Alzheimer's disease.

## Acknowledgements

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## Figures

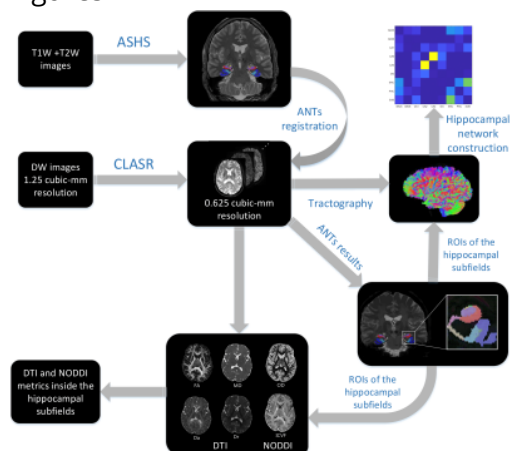


Figure 1. A framework of the analysis used in the hippocampal subfield network construction as well as computing the DTI and NODDI metrics



Figure 4. (a) A connectivity network of the left hippocampus showing significant differences (p-value <0.05 denoted by '\*') between the older and younger groups in the CA1-DG, DG-CA3, DG-CA2, and CA2-CA3 ROIs. It also shows a significant difference (p-value <0.01 denoted by '\*\*') in the CA1-SUB connection. (b) A connectivity network of the right hippocampal showing a significant difference (p-value <0.05 denoted by '\*') between the older and younger groups only in the CA1-SUB connection.

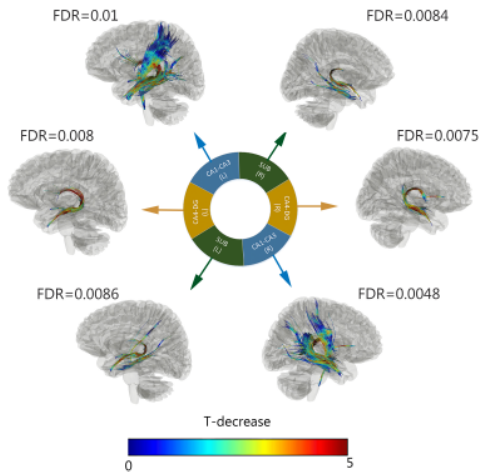


Figure 5. Connectometry analysis showing that the quantitative anisotropy (QA) was negatively correlated with the subjects' age in each of the MNI-hippocampal ROIs with an FDR that ranges between (0.0075 and 0.01). These tracks included corpus callosum, left and right corticospinal tracts, left and right corticothalamic pathway, left and right cingulum, left and right fornix, left and right optic nerves, left and right inferior longitudinal fasciculus, left and right trochlear. The tracks are color-coded with T statistics related to a negative correlation with QA.