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Rational Design of Amphiphilic Fluorinated Peptides: Evaluation of Self-Assembly Properties and Hydrogel Formation

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Advanced peptide-based nanomaterials composed of self-assembling peptides (SAPs) gain an emerging interest in pharmaceutical and biomedical applications. The introduction of fluorine into peptides, in fact, offers unique opportunities to tune their biophysical properties and intermolecular interactions. In particular, the degree of fluorination plays a crucial role in peptide engineering as it can be used to control the intensity of fluorine-specific interactions. Here, we designed and explored a series of amphipathic self-assembling peptides by incorporating the fluorinated amino acids (2*S*)-4-monofluoroethylglycine (**MfeGly**), (2*S*)-4,4-difluoroethylglycine (**DfeGly**) and (2*S*)-4,4,4-trifluoroethylglycine (**TfeGly**) as main components. This approach enabled studying the impact of fluorination on secondary structure formation and peptide self-assembly on a structural basis. We show that the interplay between polarity and hydrophobicity, both induced by varying degrees of side chain fluorination, affects peptide folding and leads to the generation of peptide hydrogels composed of fluorinated aliphatic amino acids. Molecular simulations revealed the formation of electrostatically driven intra-chain and inter-chain contact pairs caused by side chain fluorination. Our study provides a systematic report about the distinct features of fluorinated oligomeric peptides with potential applications as peptide-based biomaterials.

Introduction

Self-assembling peptides (SAPs) are often composed of an amphiphilic structure motif based on alternating arrangements of hydrophobic and hydrophilic residues.[1-4] More than two decades ago the first and most prominent variants **EAK16-II** H_2N-(Ala-Glu-Ala-Glu-Ala-Lys-Ala-Lys)$_2$-OH and **RADA16-II** H_2N-(Arg-Ala-Arg-Ala-Asp-Ala-Asp-Ala)$_2$-OH were discovered by Zhang *et al.*[5] These peptides served as essential motifs to study the hierarchical construction of β-sheet-based macroassemblies.[2, 5-8] Since then, SAPs have attracted paramount interest in biomedical research for their biocompatibility, biodegradability, and biofunctionality. They were utilized in the fields of tissue engineering and wound healing by functioning as growth and adhesive substrates.[9-14] Their self-assembly is driven by non-covalent interactions such as hydrogen bonding, electrostatic interactions, hydrophobic interactions, aromatic interactions (π–π stacking) and van der Waals forces.[15-18] A promising approach to produce novel functional peptide-based biomaterials consists in the systematic incorporation of fluorinated amino acids. These non-natural building blocks turned out to be a powerful tool to fine-tune biophysical and chemical properties of peptides and proteins.[19] Fluorine possesses unique properties like a strong inductive effect combined with a high electronegativity. The replacement of a single C-H bond with C-F is generally considered to be isosteric.[20, 21] To date, investigations of the effects of fluorinated amino acids on hydrophobicity[22, 23], secondary structure formation[24, 25], protein-protein interactions[26], amyloid folding kinetics[27, 28], proteolytic stability[29], chemical and biological properties of fluorinated peptide-based materials[30], and on the integration of fluorine into living organisms[31, 32] have been reported by our group. Vast majority of previous studies including our own efforts examining fluorinated amino acids in the context of peptide and protein chemistry were limited to the incorporation of one or only a few of these building blocks. Moreover, the chemical nature and biological features of polyfluorinated peptides with a large proportion of fluorinated amino acids were seldom

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studied. We are confident that the development of symmetrical peptides containing several of such building blocks could serve to effectively measure fluorine-specific interactions in self-assembly processes. The fabrication of polyfluorinated peptides obviously requires generous amounts of fluorinated amino acids.[33] Thus, we have recently reported an improved synthetic strategy to obtain the fluorinated amino acid (2*S*)-4-monofluoroethylglycine (**MfeGly**) in gram scale.[34] Moreover, Soloshonok *et al.* developed a general and practical synthetic process to obtain enantiomerically pure Fmoc-protected fluorinated amino acid through an asymmetric and Ni(II)-complex mediated stereoselective synthesis (*see* ***scheme S1*** *in the supporting information*).[35-38] In current attempts, we developed a strategy for the synthesis of a diverse range of aliphatic fluorinated amino acids with corresponding ligand complex.[39]

With this work, we aim to contribute to the future design of fluorinated peptide-based biomaterials. We designed an amphipathic motif including the well-studied non-proteogenic amino acid α-aminobutyric acid (Abu), which is reported as suitable hydrophobic building block for SAPs.[40, 41] The varying degree of fluorination was adjusted by multiple incorporation of its derivatives (2*S*)-4-monofluoroethylglycine (**MfeGly**), (2*S*)-4,4-difluoroethylglycine (**DfeGly**) and (2*S*)-4,4,4-trifluoroethylglycine (**TfeGly**). With this peptide library we assessed the impact of fluorine-specific interactions on the intrinsic hydrophobicity, secondary structure formation, self-assembling properties, the morphology of amyloid-like aggregates and the formation of peptide hydrogels. Molecular simulations of the different fluorinated peptides demonstrate that the peptide-peptide interactions are finely tuned by the ability of fluorine atoms to form electrostatic contact pairs with positively partially charged atoms on the backbone and on the side chains. This ability in turn depends critically on the number of fluorinated atoms, which explains how the fluorination degree controls peptide structure formation.

Results and discussion

Peptide design: Estimation of sequence length, hydrophobicity, and fluorine-induced polarity

Our rational design is based on a cationic *Abu-Lys* repeating unit. Both the N- and C-terminus are capped to avoid charge repulsions between distinct peptides, encouraging intermolecular interactions between the hydrophobic side chains. A π-system derived from 4-aminobenzoic acid (**[4]Abz**, **PABA**) was set on the C-terminus; this building block is a widely used fluorescent probe and enables precise control over peptide stock concentrations.[42] To determine a chain length sufficient for β-sheet formation, we characterized a series of **AbuK**-derived peptides with repeating units ranging from five to eight alternating residues and studied the ability of secondary structure formation in physiological conditions *via* CD spectroscopy (**figure 1a**). High peptide concentrations (2 wt%) were chosen to induce peptide self-assembly. As can be seen from the CD spectra, only **AbuK14** (Ac-(Abu-Lys)$_7$-**[4]Abz**-NH$_2$)

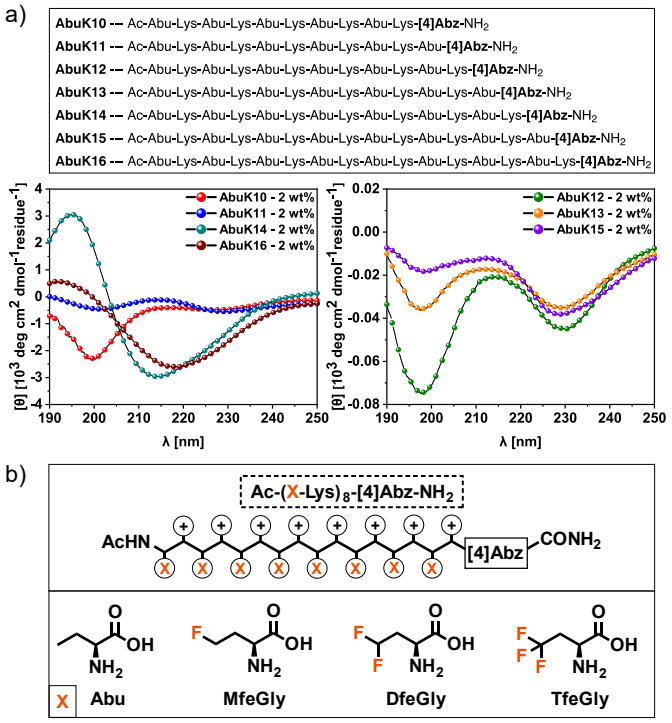

Figure 1: a) CD spectra of 2 wt% **AbuK10**-**AbuK16** in 50 mM Bis-tris propane + 150 mM NaCl, pH 7.4 recorded at 37 °C. **b)** Peptide motif (**AbuK16**, **MfeGlyK16**, **DfeGlyK16**, **TfeGlyK16**) and chemical structures of **Abu** and its derivatives **MfeGly**, **DfeGly** and **TfeGly**.

and **AbuK16** (Ac-(Abu-Lys)$_8$-**[4]Abz**-NH$_2$) formed β-sheet structures (λ_{min} = 214-220 nm), whereas the remaining variants (**AbuK10-13**, **AbuK15**) tend to form polyproline type II helices (PPII). This is proven due to the characteristic positive and negative maxima at λ_{max} = 218-228 nm and λ_{min} = 205-198 nm. The PPII helix comprises an extended left-handed helical structure and was also found for similar *Ala-Lys* derived SAPs.[43, 44] As the 16-meric peptide **AbuK16** has shown to form β-sheets, we synthesized the polyfluorinated amphipathic peptides **MfeGlyK16** (Ac-(MfeGly-Lys)$_8$-**[4]Abz**-NH$_2$), **DfeGlyK16** (Ac-(DfeGly-Lys)$_8$-**[4]Abz**-NH$_2$) and **TfeGlyK16** (Ac-(TfeGly-Lys)$_8$-**[4]Abz**-NH$_2$) by substitution of **Abu** with each fluorinated derivative according to eight repeating units (**figure 1b**).

Rational design applying fluorinated amino acids in peptide scaffolds crucially depends on a reliable determination of their hydrophobic nature. Estimation of the intrinsic hydrophobicity is indispensable to discuss fluorine-specific interactions for each oligopeptide. In this work, the hydrophobic properties of peptides were determined through an RP-HPLC based assay (**figure 2a**). In general, the hydrophobicity of the peptides increases with the number of fluorine substituents of the individual amino acids. However, **MfeGlyK16** is more polar compared to **AbuK14** and **AbuK16** and in accordance to prior observed trend of fluorine-induced hydrophobicity studies on the amino acids **Abu**, **MfeGly**, **DfeGly** and **TfeGly**.[27, 45] We thus conclude the origin of the decrease in non-polar character of **MfeGlyK16** lies rather in the physicochemical properties of its side chain than in the overall fluorine content. Theoretical approaches to determining the hydrophobic nature of

a)

Peptide	Retention time ϱ [min]
AbuK14	(15.333 ± 0.0173)
MfeGlyK16	(15.285 ± 0.075)
AbuK16	(16.368 ± 0.087)
DfeGlyK16	(18.780 ± 0.044)
TfeGlyK16	(23.054 ± 0.031)

b)

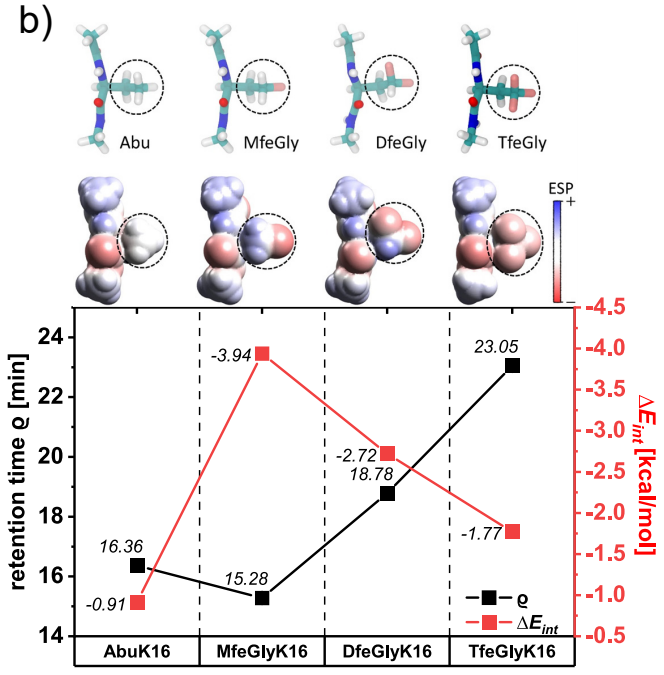

Figure 2: a) Retention times ϱ of **AbuK14**, **AbuK16**, **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** as experimental index of intrinsic hydrophobicity. An increase in ϱ corresponds to an enhanced non-polar character of respective peptide. The eluents were **(A)** H_2O + 0.1% (v/v) TFA and **(B)** ACN + 0.1% (v/v) TFA by applying a gradient of 5% → 40% **(B)** over 30 min. **b)** Geometry optimized structures of different amino acid residues marked with dashed circles with the N-terminal acetyl cap and the C-terminal N-methylamide cap obtained from quantum mechanical (MP2/6-31G*) calculations are shown in the ball-stick representation (top row). Atoms are colored according to atom types: carbon (cyan), nitrogen (blue), oxygen (red), hydrogen (white), and fluorine (pink). The corresponding space-filling models are colored according to the calculated electrostatic potential (ESP) showing the varying polarities for the different side chains. The calculated interaction energies ΔE_{int} (HF/6-31G*) of water with an **Abu**, **MfeGly**, **DfeGly** and **TfeGly** side chain are plotted against retention times ϱ of **AbuK16**, **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16**. For comparison, we also calculated the change in ΔE_{int} for water-water interactions (-5.85 kcal/mol).

fluorinated amino acids emphasized an alteration of non-polar character through side chain-based interactions in aqueous conditions triggered by fluorination.[46] To get deeper insights into the impact of fluorine-specific interactions, we used quantum mechanical (QM) calculations for the residues of **Abu**, **MfeGly**, **DfeGly** and **TfeGly**-derived motifs. The QM geometry optimized structures, their electrostatic potential (ESP) maps and water interaction energies ΔE_{int} for the different types of amino acids are shown in **figure 2b**. The ESP maps reveal different degrees of side chain polarities, the lowest for **Abu** and the highest for **MfeGly**. Interestingly, with further increase in fluorination (**DfeGly**, **TfeGly**), the polarity decreases again. To quantify the hydrophobicity of the side chains, we calculated ΔE_{int} for the different types of amino acids by many initial configurations of an amino acid–water complex for each amino acid type. ΔE_{int} is found to be the smallest for **Abu** (-0.91 kcal/mol) and the largest for **MfeGly** (-3.94 kcal/mol). Like the side chain polarity, ΔE_{int} decreases with further increase of fluorination: **DfeGly** (-2.72 kcal/mol) and **TfeGly** (-1.77 kcal/mol). It should be noted that these ΔE_{int} values are smaller than the water–water interaction energy of -5.85 kcal/mol, which implies that all these amino acids are hydrophobic. The theoretical values corroborate the experimental trends of peptide hydrophobicity, emphasizing the impact of fluorine-induced polarity changes as seen for **MfeGlyK16**.

Secondary structure formation of amphipathic peptides

All oligopeptides were studied over a wide concentration range (0.1 wt% - 1 wt%) with CD spectroscopy experiments (**figure 3**). Secondary structure formation was investigated at physiologically buffered (pH 7.4) and basic (pH 9.0) conditions. The results at pH 7.4 show for **AbuK16** and **MfeGlyK16** the typical course of absorption of a random coil motif at a concentration of 0.1 wt% (**figure 3a**). An increase in peptide concentration (≥ 0.25 wt%) generated the formation of PPII helices (**figure 3b**) as discussed for **AbuK**-derived peptides before. Interestingly, the formation of β-sheets was not observed for **MfeGlyK16** in higher concentrations of 1 wt% and 2 wt% (**figure 3d**), very different to the observations for **AbuK14** and **AbuK16** (see **figure 1a**). Increasing the degree of fluorination has shown to trigger β-sheet formation (≥ 0.25 wt%) for **DfeGlyK16**; for lower concentrations (0.1 wt%) a random coil conformation was observed (**figure 3a-3d**). A growth in fluorine-content on each individual amino acid increases the hydrophobic nature while similarly decreasing the polarity and, therefore, promoting β-sheet formation. In this manner, the most fluorinated peptide **TfeGlyK16** was found to form β-sheets at all selected concentrations (**figure 3a-3d**).

We further studied these peptides at basic conditions (pH 9.0) (**figure 3e-f**) which promote neutralization of the overall positive charge and, thus, to provoke β-sheet formation. All peptides undergo β-sheet formation at a concentration of 0.25 wt%. Both peptides **AbuK14** and **AbuK16** formed β-sheets at respective concentrations at pH 9.0, whereas significant higher concentrations are necessary in physiological conditions (2 wt%). The only exception in this regard is the variant **MfeGlyK16**, which does not form β-sheets even at higher concentrations of 1 wt% (see **figure 3f**). Comparison of **MfeGlyK16** with **AbuK14**, both possessing similar values of peptide hydrophobicity, appointed a lack in β-sheet assembly for **MfeGlyK16** caused by the side chain properties. Likewise, calculated ΔE_{int} values suggests the residue of **MfeGly** to be better accommodated in a water-exposed environment. We propose this circumstance, phenomenologically, as notable driving force maintaining **MfeGlyK16** in a PPII-like

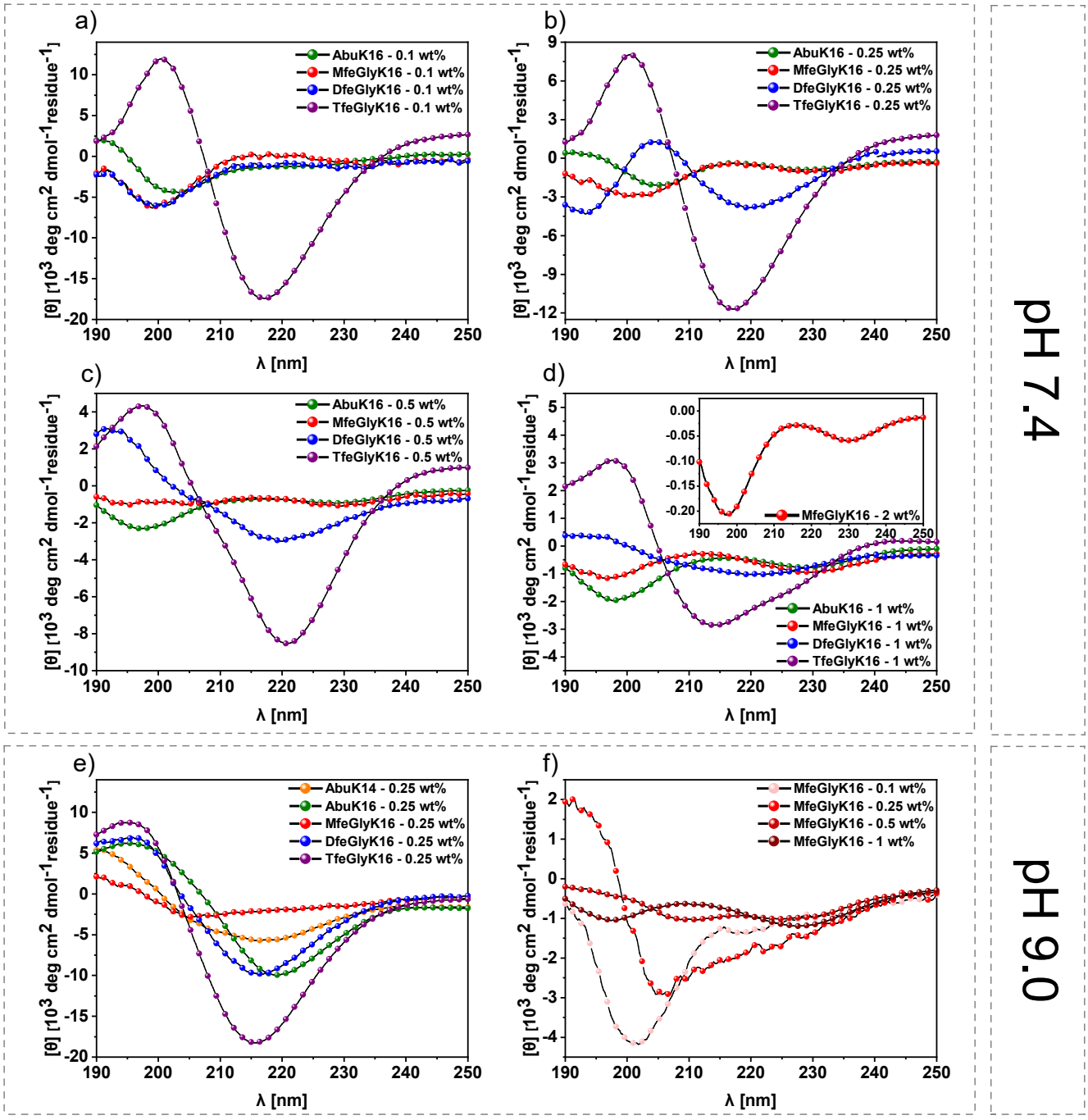

Figure 3: CD spectra of amphipathic oligopeptides **AbuK16 (green)**, **MfeGlyK16 (red), DfeGlyK16 (blue)** and **TfeGlyK16 (violet)** at **a)** 0.1 wt%, **b)** 0.25 wt%, **c)** 0.5 wt% & **d)** 1 wt% (also 2wt% for **MfeGlyK16**) concentration in 50 mM Bis-tris propane + 150 mM NaCl, pH 7.4 recorded at 37 °C. CD spectra of **e)** 0.25 wt% amphipathic oligopeptides **AbuK14**, **AbuK16, MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** and **f)** 0.1 - 1 wt% **MfeGlyK16** in 50 mM Bis-tris propane + 150 mM NaCl, pH 9.0 recorded at 37 °C.

conformation. Beside the polar effects of each fluorinated side chain, their intrinsic secondary structure propensities are crucial factors to understand fluorine-driven peptide folding. As reported by Gerling *et al.* the **MfeGly** side chain possesses the highest helical propensity among its fluorinated derivatives **DfeGly** and **TfeGly**.[27] In correlation to given CD data, we suggest a synergetic effect of intrinsic folding propensity and fluorine-induced polarity by multiple incorporation of **MfeGly** causing the folding pattern of **MfeGlyK16**. For this purpose, we executed MD simulations to further elucidate this experimental finding. The herein obtained theoretical results are discussed subsequently in the context of this paper.

Peptide self-assembly and characterization of fluorinated peptide-based hydrogels

Earlier reports indicated the nanocomposites of amphipathic peptides to possess similar properties as the cross-β-sheet structure of amyloid fibrils.[47, 48] In order to study structural features of these peptides we used thioflavin T (ThT) fluorescence spectroscopy (**Figure 4a**). This dye shows a strong fluorescence upon binding to amyloid-like morphologies caused by rotational immobilization, leading to an increase in fluorescence emission with a maximum at 485 nm. All samples were analyzed after 24 h of incubation time. We additionally studied all solutions by cryo-EM to determine the morphology of the formed aggregates (**Figure 4b-e**). For **AbuK16** and **MfeGlyK16** we did not observe any increase in fluorescence intensity (range: 0.01 wt% - 1 wt%). As discussed above, CD spectroscopy at given concentrations confirms our finding that these peptides do not form β-sheets but PPII helices. In contrast, **DfeGlyK16** showed a 9.5-fold enhanced fluorescence emission (1 wt%) compared to the control sample (ThT-dye in buffer without peptide, FL_{485m} = 1.0), indicating the formation of amyloid-like aggregates. A small increase in FL intensity was observed for **DfeGlyK16** at a minimal concentration of 0.25 wt%, which was also the lowest concentration revealing β-sheet structures in respective CD spectra. **TfeGlyK16** samples showed a dramatic enhancement of the fluorescence intensity of up to 180-fold at 1 wt%. Furthermore, the presence of amyloid-like fibrils was confirmed by congo red (CR) staining experiments *(see supporting information, **figure S97**)*. Our results indicate a correlation between the degree of fluorination and the ability to form amyloid-like structures. Cryo-EM studies were performed with those solutions for which a secondary structure pattern or amyloid-like behavior was detected by ThT staining. **DfeGlyK16** (0.25 wt%) (**Figure 4d**) and **TfeGlyK16** (0.1 wt%) (**Figure 4e**) both formed amyloid-like structures. As expected, through CD and ThT staining experiments, **AbuK16** (0.25 wt%) and **MfeGlyK16** (0.25 wt%) did not form any fibrillary structures *(see supporting information, **figure S98-S102**)*. At elevated concentrations of 2 wt%, however, we detected β-sheet formation for **AbuK14** and **AbuK16** by CD measurements (see prior data in **figure 1a**). Cryo-EM of these **AbuK**-derived sequences at 2 wt% concentration provided narrow ribbons composed of single strands in a highly regular line pattern (**figure 4b-c**). A similar morphology from assembled fibrils based on a *de novo* designed coiled coil-based amyloidogenic peptide was studied in prior work.[49] CD data of **MfeGlyK16** at analog concentrations provide a PPII-like structural pattern and no similar β-sheet assemblies were found in this case. We also applied small-angle X-ray scattering (SAXS) experiments on supposedly amyloid-like fibrils containing solutions of the peptides **AbuK16**, **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** over a

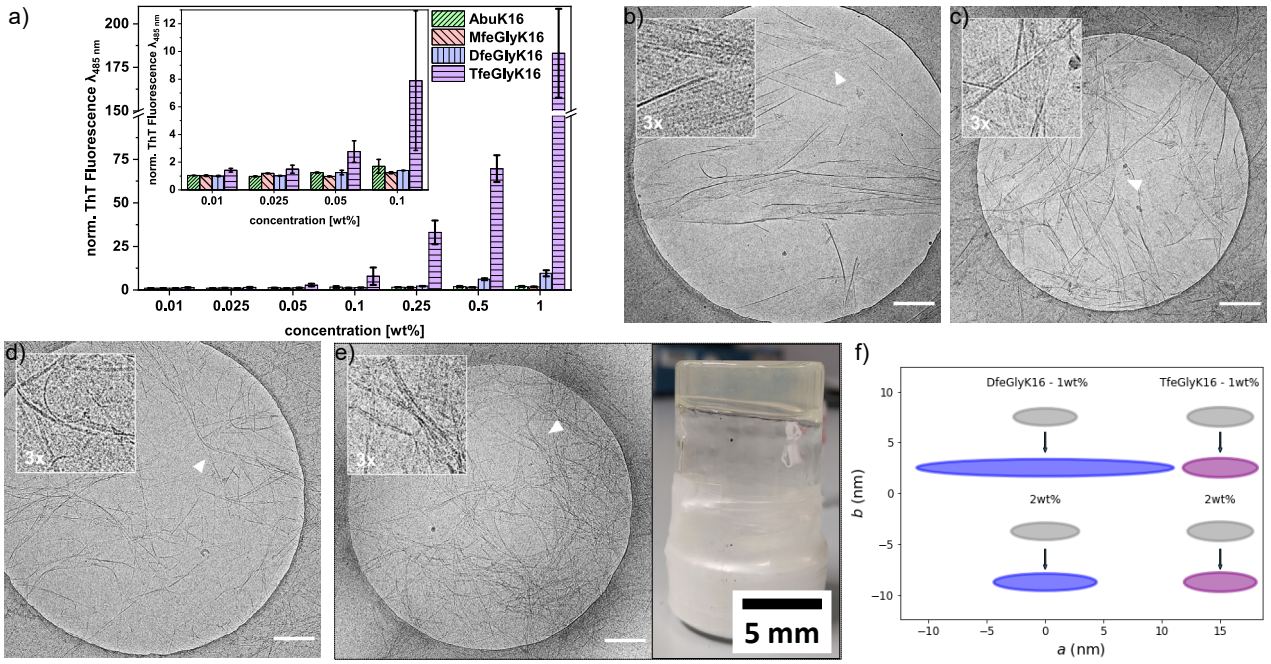

Figure 4: a) Thioflavin T assays of **AbuK16 (green), MfeGlyK16 (red), DfeGlyK16 (blue)** and **TfeGlyK16 (violet)** incubated for 24 h at 37 °C in 50 mM Bis-tris propane + 150 mM NaCl containing 20 µM ThT dye, pH 7.4. Fluorescence emission was measured at 485 nm and normalized to a negative control (solely buffer) with a FL intensity of 1.0. Cryo-EM micrographs of **b) AbuK14** (2 wt%, diluted to 0.2 wt%), **c) AbuK16** (2 wt%, diluted to 0.2 wt%), **d) DfeGlyK16** (0.25 wt%) and **e) TfeGlyK16** (0.1 wt%) + image of a **TfeGlyK16**-based hydrogel at pH 7.4 (0.5 wt%). All samples were dissolved in 50 mM Bis-tris propane + 150 mM NaCl, pH 7.4. Insets display magnified areas of the micrographs indicated by white arrow heads. The scale bar denotes 200 nm for each micrograph. **f)** Fibril cross sections corresponding to the SAXS model curves for samples of **DfeGlyK16** and **TfeGlyK16** at concentrations of 1 wt% and 2 wt% obtained through SAXS experiments. The cross-sections are of elliptical shape defined by major and minor semi-axis *a* and *b*, respectively. Plotted are the cross-sections derived from SAXS measurement frames *n* = 1 (after 120 seconds (grey ellipses)) and 50 (after 3000 seconds (colored ellipses)). Fibril growth is illustrated by arrows.

wide range of concentration (*see supporting information for detailed SAXS interpretation*). SAXS data from peptides **DfeGlyK16** and **TfeGlyK16** (both 1 wt% and 2 wt%) scale approximately with q^{-1} (**TfeGlyK16**) and q^{-2} (**DfeGlyK16**) at low *q*-values (*see **figure S111** and **figure S112** in the supporting information*). Such scaling behavior indicates a nearly circular cross-section for the fibrils of **TfeGlyK16** (interpreted as *circular cylinder)* and a flat cross-section for **DfeGlyK16** (interpreted as *extended parallelepiped*).[28, 50] Data evaluation with both theoretical models in terms of time-resolved experiments [with measurement frames of n = 1 (recorded ca. 120 s after sample preparation) and n = 50 (recorded 3000 s after sample preparation)] revealed an increase of the major semi axis from *a* = 2.7 nm to 11.0 nm for **DfeGlyK16** (1 wt%) and from 2.9 nm to 4.4 nm (2 wt%). In contrast, the short semi-axis of the cross section is constant at *b* = 0.85 nm. For **TfeGlyK16** an increase of the *a*-axis from 2.8 nm to 3.2 nm and from 2.8 nm to 3.1 nm at 1 wt% and 2 wt%, respectively, was determined. Here, the short semi-axis of the cross section is constant at *b* = 0.95 nm. An overview on the differences of cross-sections found for both polyfluorinated systems between data frame n = 1 and n = 50 is given in **figure 4f**.

After having characterized the mesoscopic structure of the different systems, we then turned to study their macroscopic viscoelastic properties. Here, we performed strain-controlled oscillatory shear rheology measurements with the aim of evaluating the influence of fluorination on the mechanical properties of these gel matrices at pH 7.4 and pH 9.0. Amplitude γ (maximum deformation) sweeps at 1 Hz oscillation frequency were performed before the frequency-dependent measurements to ensure that the value γ of the deformation always was chosen such that the experimental conditions remained always in the linear viscoelastic (LVE) regime. As a result, the amplitude γ for the oscillatory measurements was fixed at a value of 0.1%. The frequency sweeps were conducted in an angular frequency range of 0.314 to 314 rad/s to determine the storage and loss moduli G' and G'' (**figure 5**). First, we investigated the peptides **AbuK16**, **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** at physiological conditions of pH 7.4 (**Figure 5a-b**). As the non-fluorinated **AbuK16** (0.5 wt%) formed only a low viscous solution at physiological conditions, we established a further reference sample comprising a *Leu-Lys* repeating unit (**LeuK16**, Ac-(Leu-Lys)$_8$-**[4]Abz**-NH_2) to distinguish between the impact of hydrophobicity and fluorine substituents. The *Leu-Lys* unit was utilized before by Schneider and co-workers for the development of peptide-based hydrogels.[51] Through our RP-HPLC assay, we found **LeuK16** (ϱ = 28.84 ± 0.025 min) to possess greater hydrophobicity than **TfeGlyK16** (*see supporting information, **figure S96***). In addition, for **TfeGlyK16** measurements were done also at lower concentrations of 0.25 and 0.1 wt%. They are given in **figure 5b** and show a very strong reduction of the viscoelastic properties upon dilution, the elastic properties being reduced by a factor of around 80. Finally, for all 0.5 wt% samples we also studied their rheological behavior at pH 9.0 to see how the change of pH affects the viscoelastic properties of the systems. Looking at **figure 5c** one observes that especially the elastic properties described by G' are now much closer than at pH 7.4. For all samples at pH 7.4 and pH 9.0, G' is at about one order of magnitude larger than G'', indicating that these are gel-like

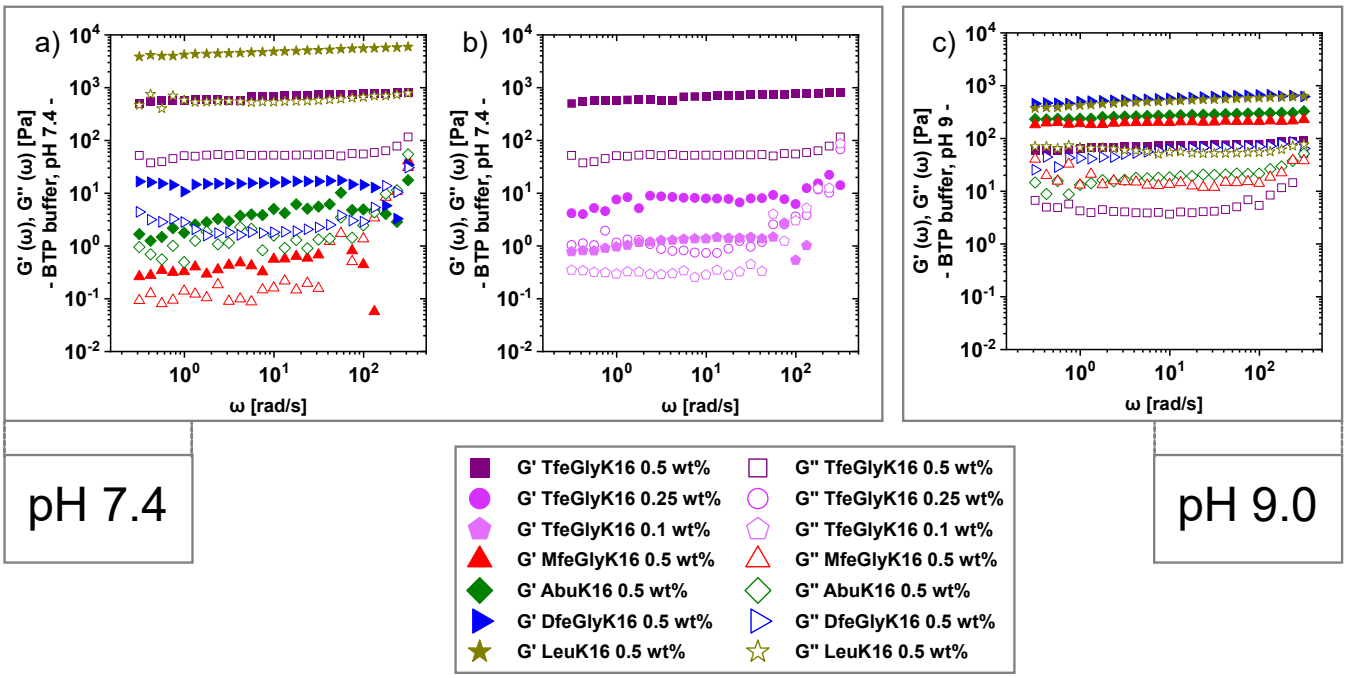

Figure 5: Storage modulus G' and loss modulus G'' as measured in frequency sweeps (ɣ= 0.1%) at T = 37°C for: **a)** the peptides **AbuK16**, **MfeGlyK16**, **DfeGlyK16**, **TfeGlyK16** and **LeuK16** (all 0.5 wt%) at pH 7.4; **b)** the peptide **TfeGlyK16** at concentrations of 0.5 wt%, 0.25 wt%, and 0.1 wt% at pH 7.4; c) the peptides **AbuK16**, **MfeGlyK16**, **DfeGlyK16**, **TfeGlyK16** and **LeuK16** (all 0.5 wt%) at pH 9.0. All samples were prepared with in 50 mM Bis-tris propane + 150 mM NaCl.

systems, for which the elastic properties dominate.[17] Both moduli increase somewhat with increasing frequency, thereby showing power law behavior, but with a rather small exponent. The plateau storage modulus G_0, is of particular interest for gel-like systems. According to classical rubber elasticity theory[52], G_0 can be related to the crosslinking density ν of the gel. The crosslinking density can in turn be used to estimate an average mesh size ξ in the system, given as:

$$\nu = G_0/kT = \xi^{-3}$$

where k is the Boltzmann constant and T is the temperature. The respective G_0 values for the peptide gels were determined by taking the average of the storage modulus G' data for **$\omega \leq 10^2$ rad/s**. These values and calculated mesh sizes are summarized in **table 1**.

At pH 7.4 and 0.5 wt% concentration, **MfeGlyK16** (0.53 Pa) shows the lowest G_0 value when comparing to **AbuK16** (4.81 Pa) and its higher fluorinated variants **DfeGlyK16** (15.3 Pa) and **TfeGlyK16** (670 Pa); the reference **LeuK16** possessed by far the highest value of G_0, owing largely to a higher degree of hydrophobicity of the side chain compared to **TfeGly**.[45] Consequently, these experimental data show a consistent analogy to the hydrophobicity trend depicted through our RP-HPLC assay and underline a direct coherence between rheological stiffness and non-polar properties of each amino acid residue (**MfeGly < Abu < DfeGly < TfeGly < Leu**). Thus, successive addition of fluorine atoms strengthens this hydrogel scaffold at physiological conditions.

An interesting behavior is observed upon increasing the pH from 7.4 to 9.0, which lowers the peptide overall charge originating from the Lys residues (**figure 5c**). Now, G_0 increases tremendously for **MfeGlyK16** (209 Pa), **AbuK16** (264 Pa) and **DfeGlyK16** (554 Pa) but drops by almost one order of magnitude for **TfeGlyK16** (70 Pa) and **LeuK16** (564 Pa), thereby bringing all the values closer together. This corresponds to an increase of G_0 by a factor of 394 (**MfeGlyK16**), 55 (**AbuK16**) and 36 (**DfeGlyK16**), but also a reduction of G_0 by a factor of 9.6 (**TfeGlyK16**) and 8.6 (**LeuK16**). The greatest change in viscoelastic stability is observed for the peptide with the lowest hydrophobicity (**MfeGlyK16**) within this work and becomes weaker with increasing non-polar properties (**AbuK16**, **DfeGlyK16**). This surprising loss in G_0 of **TfeGlyK16**-derived hydrogels was confirmed by further measurements at both pH values with independently prepared samples *(see supporting information, **figure S104-106**)*. As an explanation, we suggest a major leverage of side chain-neutralization on the viscoelastic stability of these supramolecular matrices depending rather on peptide hydrophobicity than on fluorine-specific interactions. An almost equal loss in G_0 value in context of pH change found for **LeuK16** in correlation to **TfeGlyK16** serves as further confirmation of this experimental finding. Hence, the divergence in rheological properties between **DfeGlyK16** and **TfeGlyK16**-based hydrogels is, in particular, an interesting phenomenon as it seems to be triggered by only a single H-F substitution of each amino acid residue.

Table 1: Results for the plateau modulus G_0 and corresponding mesh sizes ξ.

Name	c (wt%)	pH	G_0 (Pa)	ξ (nm)
LeuK16	0.5	7.4	4869 ± 124	9.83 ± 0.08
		9	564.4 ± 7.2	20.17 ± 0.09
TfeGlyK16	0.5	7.4	670 ± 19	19.05 ± 0.18
		9	70.24 ± 1.4	40.4 ± 0.3
	0.25	7.4	8.63 ± 0.79	81.3 ± 2.5
	0.1	7.4	1.09 ± 0.12	161.9 ± 5.7
DfeGlyK16	0.5	7.4	15.30 ± 1.04	67.14 ± 1.5
		9	554 ± 15	20.29 ± 0.18
AbuK16	0.5	7.4	4.81 ± 0.22	98.72 ± 1.54
		9	264.1 ± 5.1	25.98 ± 0.17
MfeGlyK16	0.5	7.4	0.53 ± 0.02	205.37 ± 2.53
		9	208.8 ± 0.83	28.10 ± 0.04

MD simulations of amphipathic peptides

Finally, we have performed MD simulations of **AbuK16**, **MfeGlyK16**, **DfeGlyK16**, and **TfeGlyK16** in explicit solvent at two different pH values: pH 7 (where for simplicity we assume all Lys residues to be charged) and pH 11 (where we assume all Lys residues to be charge neutral). The aim was to understand how fluorine-specific interactions may modify inter-peptide interactions and thereby control the formation of higher-ordered structures as observed in the above-discussed experiments. Interestingly, we find intra-strand contact pair formations between the fluorine atom of each **MfeGly** residue (**MfeGlyK16**) and backbone hydrogen atoms located on the peptide's amide bonds (**figure 6a**). Such contact pairs are absent in the cases of **DfeGlyK16** and **TfeGlyK16**, whose side chains are randomly oriented as found for **AbuK16 (figure 6a)**. The intra-strand contact pair formation observed for **MfeGlyK16** can be rationalized by the strongly polar **MfeGly** side chain as described before. The free energy profiles of inter-strand interaction as a function of the inter-strand separation for the different peptide types at pH 7 are shown in **figure 6b**, which reveal two distinct minima for each peptide type but **MfeGlyK16**, for which there is only one minimum. The shallow minimum at a larger inter-peptide separation observed for **AbuK16**, **DfeGlyK16**, and **TfeGlyK16** is due to the partially hydrophobic, *non-standard* (synonymous for **Abu**, **MfeGly**, **DfeGly** and **TfeGly**) amino acid (AA) side chain-side chain interaction, whereas the global minimum at a smaller inter-peptide separation is due to the *non-standard* AA side chain–Lys side chain and *non-standard* AA side chain–backbone interactions (see snapshots in **figure 6c**). In contrast, the minimum free-energy structure of **MfeGlyK16** is due to the polar, *non-standard* AA side chain–backbone and *non-standard* AA side chain–side chain interactions, and the charged Lys residues protrude out to minimize the electrostatic repulsion. Although negative and comparable free energy values for all cases imply that every peptide type can form strongly bounded dimers, the possibility of peptide fibril formation depends on whether two such dimers can in turn form favorable contacts with each other. As depicted in **figure 6d** for **AbuK16**,

DfeGlyK16, and **TfeGlyK16**, two dimers placed parallel to each other can form favorable contacts between the *non-standard* AA and Lys side chains (which are found to be important for the stability of a dimer as well). In contrast, two **MfeGlyK16** dimers placed parallel to each other face charged end groups of the Lys residue (-NH_3^+), and thus repel each other. Therefore, higher-

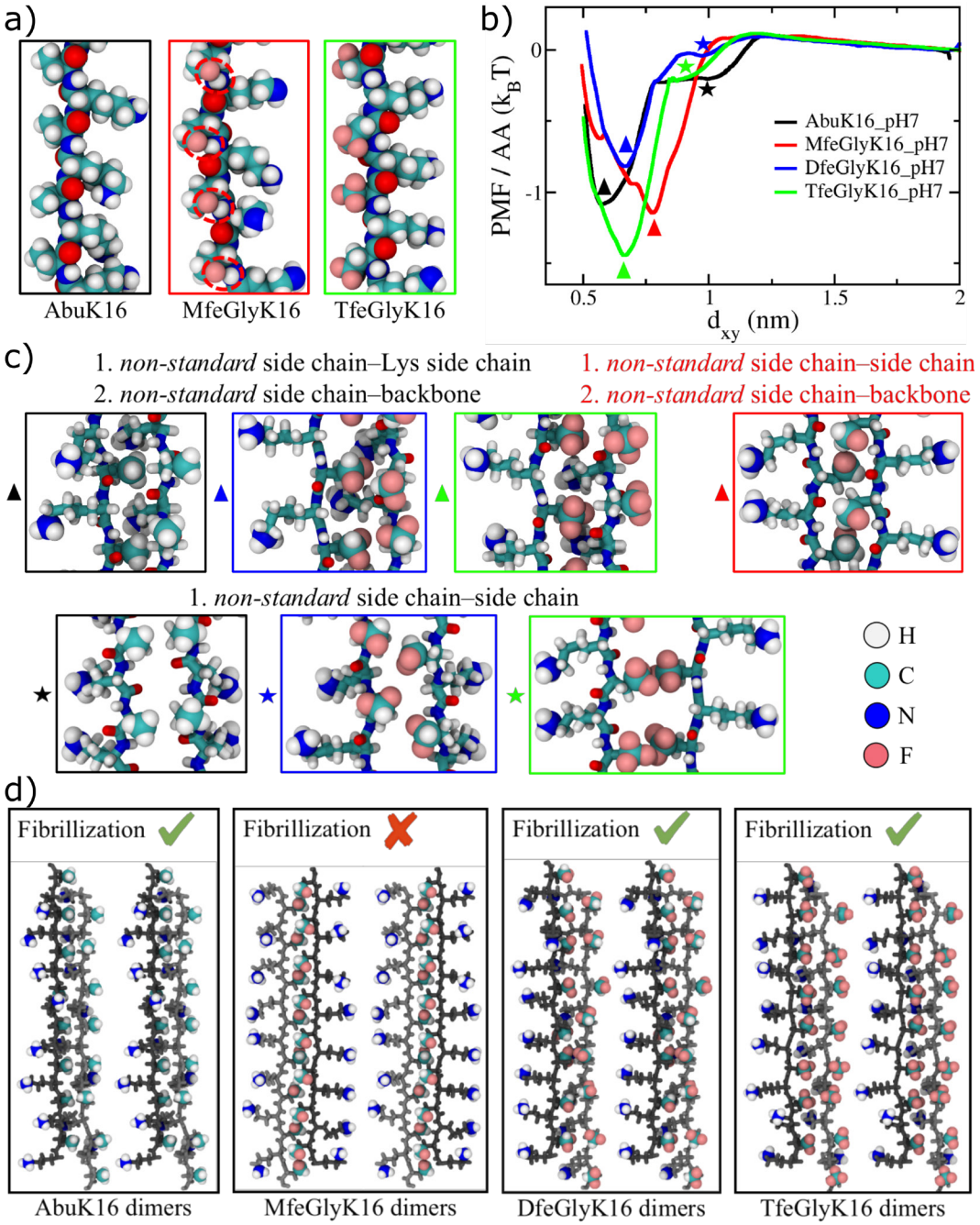

Figure 6: MD simulations results for amphipathic peptides; water is included in the simulations, but not shown for clarity **a)** Snapshots for representative parts of periodic **AbuK16**, **MfeGlyK16**, and **TfeGlyK16** single strands (taken from umbrella sampling simulations when two strands are far apart) are shown in the space-filling representation and atoms are colored as: H (white), C (cyan), N (blue), O (red), F (pink). Fluorine atoms from **MfeGly** residues and the amide-backbone derived hydrogen atoms form strong intra-strand contact pairs which are marked by red, dashed ellipses. Such contact pairs are not observed for **Abu** and **TfeGly**. **b)** The potential of mean force (PMF) per amino acid (AA) as a function of inter-strand separation d_{xy} at pH 7 (charged Lys), depicting the free energy profile of interaction between two peptide strands for side chains with different degree of fluorinations. The global minimum for each peptide type is marked by a triangle, whereas a secondary shallow minimum at a farther distance (when present) is marked by a star symbol. **c)** Structures corresponding to free energy minima for each peptide type are shown in ball-stick representation; the terminal group of each side chain is highlighted in the space-filling representation. Atom colors are the same as in **a)** and colors of enclosing boxes are the same as colors of the PMF profiles in **b)**. Dominant binding modes are given at the top of each snapshot. **d)** Schematic depicting the possibility of fibrillization of the dimer complex for the different peptide types. One strand of a dimer complex (shown in the ball-stick representation) is colored as light-gray, whereas the other strand is colored as dark-gray. The end groups of sidechains Lys (-NH_3^+), **Abu** (-CH_3), **MfeGly** (-CFH_2), **DfeGly** (-CF_2H), and **TfeGly** (-CF_3) are highlighted in space-filling representation.

order structure formation or fibrillization at pH 7 is predicted to be possible for **AbuK16**, **DfeGlyK16**, and **TfeGlyK16**, but not for **MfeGlyK16**, explaining our experimental findings at physiological conditions. The free energy profiles at pH 11, shown in ***figure S109*** *(supporting information),* reveal only one free-energy minimum for each peptide type, the depth of which is more than that of the corresponding peptide type at pH 7. The increased interaction strength is due to the reduced electrostatic repulsion between the two strands, as Lys residues are charge neutral at pH 11. For **MfeGlyK16**, the intra-strand contact pair formation *(see supporting information, chapter 12)* expose its opposite side backbone atoms that can form H-bonds with the backbone atoms of another **MfeGlyK16** strand, resulting in a very compact **MfeGlyK16** dimer with enhanced side chain-side chain interactions *(see snapshots in **figure S109** within the supporting information*). These strong cooperative interactions lead to a 2-3 times deeper free energy minimum for **MfeGlyK16** than other peptide types, for which the inter-peptide interactions are dominated by weak backbone-side chain and side chain–side chain contacts. Like at pH 7, for **AbuK16**, **DfeGlyK16**, and **TfeGlyK16**, two dimers placed parallel to each other can form the same favorable contacts as found in the stability of a single dimer, and hence the dimer structure can be periodically extended from either side by adding more dimers to produce large-scale peptide fibrils. For **MfeGlyK16**, the dimer structure is the most stable among the different peptide types and the inter-dimer interaction strength is expected to be lower due to the only possible side chain–side chain interaction as backbone atoms in a dimer complex are shielded by **MfeGly** side chains given by intra-strand contact pair formation. Hence, higher-order structures are expected to be less stable for **MfeGlyK16** and would provide an explanation for its structural properties.

Conclusions

In this work, we systematically designed and characterized a library of oligopeptides with fluorinated amino acids in large proportion. The peptides **AbuK16**, **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** served as models to evaluate the impact of fluorine-specific interactions in context of secondary structure formation, peptide self-assembly and hydrogel formation. The fluorination degree of the aliphatic side chain plays a crucial role for the intrinsic hydrophobic properties. This led not only to different secondary structures such as PPII helices or β-sheets, but also to fluorine-driven self-assembly into ordered nanostructures. On the other hand, we found for **MfeGlyK16** at physiological conditions an obliteration of β-sheet assembly, explained by MD simulations that find strong dimer formation preventing peptide fibrillization. Rheological characterization revealed a correlation between the hydrophobic nature of each fluorinated amino acid and an enhanced viscoelastic stability of resulting hydrogel matrices as shown for **MfeGlyK16**, **DfeGlyK16** and **TfeGlyK16** in physiological conditions, but also a loss in mechanical stiffness for the latter variant at pH 9.0. This study firstly established and studied a library of distinctive aliphatic and polyfluorinated SAPs for which fluorine-specific interactions were evinced by significant alterations of intra- and intermolecular interactions. The underlined design principle, the unique properties of the peptides and resulting hydrogel matrices will contribute to the future development of *de novo* designed fluorinated biomaterials.

Experimental section

General methods

^{1}H-, ^{13}C- and ^{19}F-NMR spectra (see supplementary information) were recorded at room temperature using a JEOL ECX 400 (JEOL, Tokyo, Japan), a JEOL ECP 500 (JEOL, Tokyo, Japan) or a Bruker AVANCE III 700 (700 MHz, BRUKER, Billerica, MA, USA). Chemical shifts δ are reported in ppm with the solvent resonance (MeOH-d_4) as the internal standard. HRMS were determined on an Agilent 6220 ESI-TOF MS instrument (Agilent Technologies, Santa Clara, CA, USA). For analysis, the MassHunter Workstation Software VersionB.02.00 (Agilent Technologies, Santa Clara, CA, USA) was used. IR Spectra were recorded on an ALPHA II FT-IR spectrometer (Bruker, USA). All NMR and IR spectra were evaluated by using Mnova/Mestrenova (Mestrelab Research, Ca, USA). Elemental analysis was proceeded by use of an VARIO EL elemental analyzer (Elementar Analysensysteme GmbH, Langenselbold, Germany). All essential data for compound characterization is placed within the SI. All chemicals were purchased from commercial sources (Merck, Sigma-Aldrich, VWR, Fluorochem) and used without further purification. The Fmoc-protected fluorinated amino acid **TfeGly** was synthesised according to literature (see supporting information, chapter *"Gram scale synthesis and characterization of fluorinated amino acid Fmoc-TfeGly-OH"*). **MfeGly** and **DfeGly** were synthesised by Suvrat Chowdhary and Thomas Hohmann.

Synthesis and purification of peptides

All peptides were synthesized with a microwave-equipped Liberty Blue™ peptide synthesizer (CEM, Matthews, NC, USA). A Rink Amide ProTide™ resin (CEM, Matthews, NC, USA) was utilized and the synthesis was performed either in 0.05 mmol or 0.1 mmol scale using Oxyma/DIC as activating reagents (0.05 mmol scale: 0.5 M Oxyma in DMF and 0.25 M DIC in DMF / 0.1 mmol scale: 1 M Oxyma in DMF and 0.5 M DIC in DMF). Coupling of native Fmoc-protected amino acids occurred in DMF using 5 eq. of substance (For fluorinated amino acids only 1.5 eq. were used) with 5 eq. of activating reagents and double couplings of 4 min coupling time (For fluorinated amino acid: mono coupling of 10 min) at 90°C. For deprotection of the N-terminus, a 10% piperazine (w/v) solution in EtOH / NMP (1:9) with 0.1 M HOBt was used. Acetylation was done manually in three batches using acetic anhydride (10% v/v) and DIPEA (10% v/v) in DMF (6 mL). All peptides were cleaved from the resin by treatment with TFA /TIPS/H_2O (90/5/5) for three hours using sonication at room temperature. Then the resins were washed with TFA and DCM,

and excess of solvents were removed by evaporation. Peptides were dried by lyophilization before purification with preparative reversed phase HPLC. Purification of synthesized peptides was performed on a Knauer low-pressure HPLC system (Knauer GmbH, Berlin, Germany) sold by VWR (Darmstadt, Germany), comprising a LaPrep Sigma preparative pump (LP1200), a ternary low-pressure gradient, a dynamic mixing chamber, a 6-port-3-channel injection valve with an automated preperative 10 mL sample loop, a LaPrep Sigma standard 1-channel-UV-detector (LP3101), a flow cell with 0.5mm thickness and a 16-port LaPrep Sigma fractionation valve (LP2016). A Kinetex RPC18 endcapped (5 µM, 100 Å, 250 x 21.2 mm, Phenomenex®, USA) HPLC-column was used. A Security GuardTM PREP Cartridge Holder Kit (21.20 mm, ID, Phenomenex®, USA) served as pre-column. As eluents water and ACN, both containing 0.1% (v/v) TFA were applied. HPLC runs were performed with a flow rate of 15.0 mL/min, UV-detection occurred at 220 nm for respective peptides. Data analysis occurred with an EZChrom Elite-Software (Version 3.3.2 SP2, Agilent). After separation, the purity of the collected fractions was determined by analytical HPLC. Analytical HPLC was carried out on a Chromaster 600 bar DAD-System with CSM software or a Hitachi Primaide™ UV-HPLC system (both from VWR/Hitachi, Darmstadt, Germany). A Kinetex® RP-C18 (5 µM, 100 Å, 250 x 4.6 mm, Phenomenex®, USA) column and a SecurityGuard™ Cartridge Kit equipped with a C18 cartridge (4 x 3.0mm, Phenomenex®, USA)) as pre-column was used. Otherwise, a Luna® RP-C8 (5 µm, 100 Å, 150 x 3 mm, Phenomenex®, USA) column was used. As eluents water and ACN, both containing 0.1% (v/v) TFA were applied. A flow rate of 1 mL/min was used and UV-detection occurred at 220 nm or 280 nm for respective peptides. Data analysis was done with EZ Chrom ELITE software (version 3.3.2, Agilent). The resulting pure peptides (>95%) were obtained after lyophilization of the collected fractions. All essential data for the quantification of purified peptides (HPLC data, HRMS spectra) can be found in the supporting information (***figure S37-S91***, ***table S1-S22***).

Lyophilization

To lyophilize the synthesized peptides a laboratory freeze dryer ALPHA 1-2 LD (Christ Gefriertrocknungsanlagen GmbH, Osterode am Harz, Germany) was used.

Sample preparation - Exchange of TFA adduct

All purified peptides were inevitably obtained as corresponding TFA adducts during resin cleavage and subsequent RP-HPLC purification using eluents containing 0.1% TFA. Peptide samples (about 13 mg each) were dissolved in 800 µL MilliQ-H_2O and transferred on a VariPure IPE exchange column (100 mg, 3 mL) (Agilent Technologies, Santa Clara, CA, USA). These columns were previously washed and pre-conditioned with MeOH (3 * 3 mL) and MilliQ-H_2O (3 * 3 mL). The resin was additionally washed with MilliQ-H_2O (500 µL) and the collected peptide fractions were combined. Afterwards, desired samples were lyophilized to obtain the peptide with bicarbonates as counter-ions.

Preparation of peptide stock solutions and self-assembly

Peptide stock solutions were prepared by dissolving lyophilized peptide powder (10-15 mg) in 1,1,1,3,3,3-hexafluoropropan-2-ol [HFIP] (2 mL) and treatment for 15 min in an ultrasound-bath to dissolve preformed aggregates. An aliquot of 10 µL was evaporated and the dried peptide film dissolved in a 6M guanidine hydrochloride (GndHCl) solution (pH 7.4), resulting into a dilution factor (DL) of 100. These samples were measured *via* UV detection at 280 nm by use of an Eppendorf BioPhotometer plus with semi-micro–VIS Cuvettes (PMMA) 10x100 (Eppendorf, Hamburg, Germany). All UV spectra were baseline corrected with a reference spectrum of a sample containing solely buffer solution. The UV absorbance given through the fluorophore ***p*-aminobenzoic acid (PABA)** at the C-terminus of the peptides at 280 nm was evaluated in triplicates. By use of a calibration curve derived from ***p*-aminohippuric acid (PAH)** *(see supporting information, **figure S92**)*, the concentration of each stock solution was calculated. If not otherwise stated, all peptide samples were treated following this protocol before each measurement: An aliquot from the HFIP peptide stock solution was taken and evaporated. The dried peptide was then dissolved in respective buffer and vortexed (1 min), sonicated (5min) and finally ultracentrifuged (1 min) at room temperature.

RP-HPLC assay for estimation of hydrophobicity

The protocol for the RP-HPLC assay was previously established by our group.[27, 28] Peptide samples were dissolved in 250 µL of a mixture of 5% (v/v) ACN in 95% (v/v) Milli-Q-water containing 0.1% TFA and filtered over a syringe filter with 0.2 µm pore size. The overall concentration of each sample was 0.2 mM. The retention times of all samples were determined on a C18 column (Capcell C18, 5 µm) using a LaChrom-ELITE-HPLC-System (VWR International) with UV detection at 280 nm. A linear gradient from 5 to 40% ACN + 0.1% TFA in 30 min was applied at room temperature and all experiments were performed in triplicates.

QM calculations

All QM calculations were performed using Gaussian 16.1.[53] **Abu**, **MfeGly**, **DfeGly**, and **TfeGly**-derived motifs, as shown in Figure 2b, were taken for QM calculations. Geometry optimizations of these structures were done at the MP2/6-31G* level of theory. Water interaction energies were obtained from the HF/6-31G* single point calculations of the geometry optimized structures. Electrostatic potential maps for the geometry optimized structures were rendered using the Avogadro software.[54] Dihedral energy scans were performed at the MP2/6-31G* level of theory. Force field parameters and partial atomic charges for the amino acid Abu and its fluorinated variants (MfeGly, DfeGly, and TfeGly) were initially obtained from CHARMM36m[55] and

CGenFF[56] parameters, using the CGenFF program.[57, 58] As there were large penalties for dihedral angle angles associated with side chain rotations (Cα–Cβ–Cγ–F and Cα–Cβ–Cγ–H) and partial atomic charges, new parameters were derived from QM energy scans and water interaction energies, respectively using the FFParam package.[59] Optimized partial atomic charges and dihedral parameters for the different amino acids are given in the supporting information (chapter 12).

Equilibrium MD simulations

To study interpeptide interactions, two periodic polypeptide chains, each with the long-axis oriented along the *z*-direction, with an interaxial distance d_{xy} of 2.5 nm, arranged antiparallel (ap) to each other were considered. Each system was solvated in a rectangular box of size 5×5×5.832 nm^3. If needed, enough counterions (Cl^- ions) were added to charge neutralize the whole system. The simulation box is shown in ***figure S108*** *(supporting information)*. CHARMM-compatible TIP3P water[60,61] and ion parameters[62] were used. The solvated system was subjected to energy minimization using the steepest descent algorithm, for removing any bad contacts. The simulation for each case was performed for 500 ns in the $Np_{xy}L_zT$ ensemble, with L_z per amino acid = 3.6 Å, at T = 300 K and p_{xy} = 1 bar with *periodic boundary condition* in *xyz* directions, using GROMACS 2020.1 package.[63] The stochastic velocity rescaling thermostat[64] with a time constant of $\boldsymbol{\tau_T}$ = 0.1 ps was used to control the temperature, while for the pressure control a semi-isotropic Parrinello-Rahman barostat[65] was used with a time constant of $\boldsymbol{\tau_p}$ = 1 ps and a compressibility of $\kappa = 4.5\times10^{-5}$ bar^{-1}. LINCS algorithm[66] was used to convert the bonds with H-atoms to constraints, allowing a timestep of Δt = 2 fs. Electrostatics interactions were computed using the particle mesh Ewald (PME) method[67] with a real-space cut-off distance of 1.2 nm, while van der Waals (VDW) interactions were modelled using Lennard-Jones potentials with a cut-off distance of 1.2 nm where the resulting forces smoothly switch to zero between 1 nm to 1.2 nm.

Umbrella sampling simulations

To calculate the free energy landscape or the potential of mean force (PMF) between two periodic polypeptide chains, the final configuration obtained from the equilibrium MD simulation was first pulled in either direction to generate initial conformations for two polypeptide chains at different interaxial separations. Total 40–50 umbrella windows, with an inter-window spacing of 0.35 Å, were simulated in the $Np_{xy}L_zT$ for 30 ns each. During these simulations, an additional umbrella potential with a spring constant of 10000 kJ·mol^{-1}·nm^{-2} was used to restrain the interaxial separation to a given distance. Every 100 fs data was collected, and the last 20 ns simulation data for each window was used to obtain the PMF using the weighted histogram analysis method (WHAM).[68,69] The *g_wham* module[70] of GROMACS was used for performing the WHAM analysis and calculating error bars using the bootstrap method.

CD Spectroscopy

Circular dichroism experiments were performed using a Jasco J-810 spectropolarimeter fitted with a recirculating chiller (D-76227, Karlsruhe). Data were recorded using 0.1 mm Quartz Suprasil® cuvettes (Hellma) equipped with a stopper. Spectra were recorded at 37 °C from 190 to 250 nm at 0.2 nm intervals, 1 nm bandwidth, 4 s response time and a scan speed of 100 nm min^{-1}. Baselines were recorded and were subtracted from the data. Each reported CD value represents the average of minimum three measurements. Further CD spectra can be found in the supporting information (***figure S93-S95***)

Congo red (CR) assay for fibril detection

Aliquots of peptide HFIP-stock solutions (0.5 wt%) were dried and then redissolved in 50 mM Bis-tris propane + 150 mM NaCl with addition of 50 µM congo red (overall pH 7.4). Negative controls were prepared by dissolving corresponding samples in buffer without dye. After dissolution, the standard self-assembly protocol was applied, and all samples were incubated overnight at 37 °C. UV spectra (300-700 nm) were recorded for all samples using a Varian Cary 50 UV-VIS Spectrophotometer (Agilent, USA) and 0.5 mm Quartz Suprasil® cuvettes (Hellma). Experimental data can be found in the supporting information (***figure S97***).

Thioflavin T (ThT) fluorescence assay for fibril setection

A suitable protocol for this assay was recently published by our group.[28] Aliquots of peptide HFIP-stock solutions were dried and then redissolved in 50 mM Bis-tris propane + 150 mM NaCl with addition of 20 µM Thioflavin T (overall pH 7.4). The buffer containing ThT was previously filtered over a nylon syringe filter with 0.2 µm pore size. After dissolution, the sample was sonicated for 30 s, transferred on a BRAND® microplate (size: 96 wells, color: black; Sigma-Aldrich), sealed to prevent evaporation and placed in an Infinite® M Nano$^+$ plate reader (Tecan Deutschland GmbH, Crailsheim, Germany). ThT fluorescence (λ_{ex}=420 nm, λ_{em} =485 nm, Z-position: 15173 nm [manual], gain: 80 [manual], lag time: 0 µs, integration time: 20 µs) was measured after 24 h incubation at 37 °C. The fluorescence intensity at 485 nm was normalized with respect to the negative control sorely containing buffer (set as FL_{int} 1.0).

Cryogenic electron microscopy (cryo-EM)

Perforated carbon film-covered microscopical 200 mesh grids (R1/4 batch of Quantifoil, MicroTools GmbH, Jena, Germany) were cleaned with chloroform and hydrophilized by 60 s glow discharging at 10 µA in a EMSCOPE SC500 before 4 µl aliquots of the peptide solution were applied to the grids. The samples were vitrified by automatic blotting and plunge freezing with a FEI Vitrobot Mark IV (Thermo Fisher Scientific Inc., Waltham, Massachusetts, USA) using liquid ethane as cryogen. The vitrified specimens were transferred to the autoloader of a FEI TALOS ARCTICA electron microscope

(Thermo Fisher Scientific Inc., Waltham, Massachusetts, USA). This microscope is equipped with a high-brightness field-emission gun (XFEG) operated at an acceleration voltage of 200 kV. Micrographs were acquired on a FEI Falcon 3 direct electron detector (Thermo Fisher Scientific Inc., Waltham, Massachusetts, USA) using the 70 µm objective aperture at a nominal magnification of 28,000, corresponding to a calibrated pixel size of 3.75 Å/pixel, respectively.

Small-angle-X-ray scattering (SAXS)

SAXS measurement were performed in a flow-through capillary with a Kratky-type instrument (SAXSess from Anton Paar, Austria) at 37±1°C. The SAXSess has a low sample-to-detector distance of 0.309 m, which is appropriate for investigations of liquid samples with low scattering intensities. The measured intensity was converted to absolute scale according to Orthaber et al.[71]. The scattering vector q is defined in terms of the scattering angle θ and the wavelength λ of the radiation (λ = 0.154 nm): thus, $q = 4\pi n/\lambda \sin\theta$. Deconvolution (slit length desmearing) of the SAXS curves was performed with the SAXS-Quant software. Samples analyzed with SAXS were used as prepared, i.e. samples were mixed with buffer solution, vortexed for 20 s and filled in the capillary. Curve fitting was conducted with *SASfit*.[72]

Rheological characterization of amphipathic peptide hydrogels

Before each measurement, peptide samples of **AbuK16**, **MfeGlyK16**, **DfeGlyK16**, **TfeGlyK16** and **LeuK16** were dissolved in 50 mM Bis-tris propane + 150 mM NaCl (either pH 7.4 or pH 9.0), treated as mentioned above and incubated at 37 °C for 24 h. All rheological measurements were performed on an Anton Paar MCR 502 WESP temperature-controlled rheometer in strain-imposed mode at physiological temperature (37 °C). For all measurements, a parallel plate geometry with chromium oxide coating was used, with a diameter of 50 mm for the upper rotating plate. The gap size between the plates was set to 175 µm. The sample and geometry were surrounded by a solvent trap to reduce effects of solvent evaporation. Further experimental data can be found in the supporting information (***figure S97***).

Author Contributions

B.K. and S.C. conceived the overall project. B.K. provided guidance on data analysis, interpretation, and manuscript preparation. S.C. designed and developed concepts and experiments, synthesized, and purified all peptides, performed CD, UV and FL experiments, established and proceeded a RP-HPLC-based hydrophobicity plot for peptides, prepared samples for further experiments and wrote the manuscript. R.F.S. performed rheology experiments and wrote the manuscript. A.K.S performed simulations. A.K.S. and R.R.N. analyzed and interpreted data and wrote the manuscript. T.t.D. assisted S.C. in synthesis and purification of peptides and circular dichroism experiments. K.B.-J. and A.F.T. performed SAXS experiments and SAXS data analysis. T.H. provided fluorinated amino acids. B.S. performed cryoEM experiments, analyzed, and interpreted data. R.R.N and M.G. provided expertise and feedback.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

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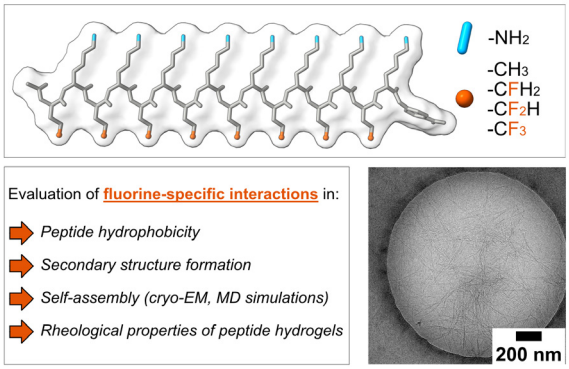
Table of Content (TOC)



Content: In this study, the tremendous impact of fluorine-specific interactions on peptide folding and self-assembly was systematically studied. Therefore, the fluorinated aliphatic amino acids **MfeGly**, **DfeGly** and **TfeGly** were incorporated in large proportion into an amphipathic peptide motif.

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