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### Research Article

# Regulation of Osteoblast Differentiation by Acid-Etched and/or Grit-Blasted Titanium Substrate Topography Is Enhanced by 1,25(OH)<sub>2</sub>D<sub>3</sub> in a Sex-Dependent Manner

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This study assessed contributions of micron-scale topography on clinically relevant titanium (Ti) to differentiation of osteoprogenitor cells and osteoblasts; the interaction of this effect with  $1\alpha$ ,25-dihydroxyvitamin  $D_3$  ( $1\alpha$ ,25(OH) $_2D_3$ ); and if the effects are sex-dependent. Male and female rat bone marrow cells (BMCs) were cultured on acid-etched (A,  $R_a=0.87~\mu m$ ), grit-blasted (GB,  $R_a=3.90~\mu m$ ), or grit-blasted/acid-etched (SLA,  $R_a=3.22~\mu m$ ) Ti. BMCs were sensitive to surface topography and underwent osteoblast differentiation. This was greatest on SLA; acid etching and grit blasting contributed additively. Primary osteoblasts were also sensitive to SLA, with less effect from individual structural components, demonstrated by enhanced local factor production. Sex-dependent responses of BMCs to topography varied with parameter whereas male and female osteoblasts responded similarly to surface treatment.  $1\alpha$ ,25(OH) $_2D_3$  enhanced cell responses on all surfaces similarly. Effects were sex-dependent and male cells grown on a complex microstructured surface were much more sensitive than female cells. These results indicate that effects of the complex SLA topography are greater than acid etching or grit blasting alone on multipotent BMCs and committed osteoblasts and that individual parameters are sex-specific. The effect of  $1\alpha$ ,25(OH) $_2D_3$  was sex dependent. The results also suggest that levels of  $1\alpha$ ,25(OH) $_2D_3$  in the patient may be important in osseointegration.

#### 1. Introduction

Current dental practice employs implants with a variety of surface modifications, yielding improved bone-to-implant contact and patient outcomes. Alterations in surface microtopography change the adsorption of proteins to the implant surface, which also affects cell attachment and differentiation [1–3]. Many studies, including those from our group, have shown that surface microroughness influences osteoblast response [4–6]. A series of studies assessing the role of specific surface properties using electro-micromachined, acidetched, or grit-blasted/acid-etched titanium (Ti) substrates showed that the greatest osteoblast differentiation was present

on the more topographically complex surfaces, with both micron- and submicron-scale features [7–9].

For an implant to become osseointegrated, cells that migrate to the area must attach to the surface and then differentiate into mature osteoblasts. Recently, we demonstrated that commercially available human mesenchymal stem cells are also sensitive to Ti surface microtopography and exhibit osteoblast differentiation even in the absence of media supplements typically used to promote mineralized bone nodule formation [6]. Wnt5a mediated the effects of the surface through the noncanonical Wnt signaling pathway [10]. Stangl et al. [11] showed that a human fetal osteoblast cell line responded preferentially to changes in microtopography

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of commercially pure Ti surfaces, indicating that progenitor cells in the osteoblast lineage are affected as well.

Grit blasting and acid etching are widely used in combination to modify titanium implants. Grit blasting imparts macron- and micron-scale topographic structures on implant surfaces, while acid etching creates micron-, submicron-, and nanoscale topographies. The application of these two techniques in combination creates implant surfaces with a complex topography that has been well studied in osseointegration *in vivo* [12, 13] and osteoblasts *in vitro* [14]. These studies demonstrate that the topographical features of Ti surfaces affect differentiation of osteoprogenitor cells and maturation of osteoblast lineage cells. However, less is known about the individual contributions of these substrate features to directing osteoblastic differentiation of progenitor cells or maturation of committed osteoblasts.

Several reports have shown surface-dependent differences of osteoblasts in response to osteotropic hormones such as  $1\alpha,25$ -dihydroxyvitamin D<sub>3</sub>  $(1\alpha,25(OH)_2D_3)$  [15–18]. Interestingly, not only are responses to  $1\alpha,25(OH)_2D_3$  on complex microstructured surfaces greater than on smooth surfaces, but there are sex-specific differences in hormone responses as well. Our group has demonstrated that calvarial osteoblasts from male donors exhibit a more robust response to  $1\alpha,25(OH)_2D_3$  than cells from female donors, increasing important osteogenic markers as well as soluble factors that increase the angiogenic and osteogenic microenvironment [15]. Similarly, sex-specific responses to a variety of stimuli have been observed in myotubes [19], angiogenesis [20], spleen, and thymus [21, 22]. These observations suggest that osteoblast cells may also respond to surface roughness modifications in a sex-dependent manner.

The aim of the present study was to evaluate the role of topographic surface features in osteogenic differentiation of rat bone marrow stromal cells (BMCs) and in the maturation of rat calvarial osteoblasts and to assess whether the effects of specific surface treatments, either alone or in combination, are sex-dependent. In addition, we examine how treatment with  $1\alpha,25(OH)_2D_3$  modifies the responses of male and female primary cells to these surface topographies.

#### 2. Materials and Methods

2.1. Preparation and Characterization of Ti Disks. Titanium (Ti) disks were prepared from 1 mm thick sheets of grade 2 unalloyed Ti (ASTM F67 "Unalloyed Titanium for Surgical Implant Applications") with a 15 mm diameter to fit in a 24-well culture plate as previously described [16, 23, 24]. Briefly, disks were washed in acetone and processed through a 2% ammonium fluoride, 2% hydrofluoric acid, and 10% nitric acid solution at 55°C for 30 s to pretreat Ti disks. Submicronscale rough (A) surfaces were produced by treating pretreated disks with heated, concentrated acid, resulting in  $R_a$  of 870 nm. GB surfaces were produced by coarse grit blasting with 0.25–0.50 mm corundum grit at 5 bars until the surface reached a uniform gray tone pretreatment disks ( $R_a$  = 3.90  $\mu$ m). To produce disks with a mixed topography (SLA), grit-blasted disks were acid-etched ( $R_a$  = 3.22  $\mu$ m). Scanning

electron microscopic images and surface characterization have been described previously [8, 14].

2.2. Bone Marrow Cell Isolation and Response. Bone marrow cells (BMCs) were isolated from the tibias and femurs of 100-125 gram male and female Sprague-Dawley rats under Georgia Institute of Technology Institutional Animal Care and Use Committee Protocols and following appropriate guidelines. For each sex, marrow was isolated and pooled from the tibias and femurs of four animals. Marrow was flushed from the intramedullary canal of each bone into a sterile conical tube using a 5 mL syringe and 18-gauge needle. Marrow was briefly incubated with Collagenase IA (Sigma Aldrich, St. Louis, MO) to release the cells from the matrix. The cells were pelleted and plated in a flask for expansion. Cells were cultured in Mesenchymal Stem Cell Growth Media (Lonza Biosciences, Walkersville, MD). At first passage, cells were plated on tissue culture polystyrene (TCPS) or Ti surfaces (A, GB, SLA) at 5,000 cells/cm<sup>2</sup> (based on a 15 mm diameter smooth surface) and grown to confluence on TCPS, typically after 7 days. At confluence, media were changed and cells incubated for an additional 24 hours.

2.3. Rat Osteoblast Cultures. Osteoblasts were isolated from frontal and parietal (calvaria) bones of 100-125 gram male and female Sprague-Dawley rats using enzymatic isolation as described previously [25]. Briefly, rat bones cleaned of periosteum and soft tissues were cut into 1-2 mm<sup>2</sup> pieces. The bone chips were washed three times in Hank's balanced salt solution (HBSS, Invitrogen, Carlsbad, CA) containing 3% penicillin-streptomycin (Invitrogen). After washing, bone chips were digested with an enzymatic cocktail of collagenase IA and dispase (Invitrogen) in HBSS for 1 hour at 37°C. The supernatants of the first two digestions were discarded to avoid contamination by fibroblasts. The bone chips were digested three more times using the same method; at each step, the digestion media were collected and quenched with Dulbecco's modification of Eagle's medium (DMEM, cellgro, Manassas, VA) supplemented with 10% fetal bovine serum (Thermo Fisher HyClone, Waltham, MA) and 1% penicillinstreptomycin (Invitrogen). Calvaria from eight rats per sex were pooled for each experiment.

To confirm osteoblastic phenotype of isolated rat calvarial cells, we also examined cell responses to 24-hour treatment with the osteotropic hormone  $1\alpha,25(\mathrm{OH})_2\mathrm{D}_3$  (Enzo Life Sciences, Plymouth Meeting, PA) after confluence on TCPS. Both male and female rat cells exhibited dose-dependent decreases in cell number and increased alkaline phosphatase specific activity and osteocalcin levels in response to treatment with  $10^{-10}$  M,  $10^{-9}$  M, and  $10^{-8}$  M  $1\alpha,25(\mathrm{OH})_2\mathrm{D}_3$  (data not shown).

Validated rat osteoblasts were plated on TCPS or Ti surfaces at a density of 10,000 cells per cm<sup>2</sup>. Media were exchanged at 24 hours and then every 48 hours until the cells reached confluence on TCPS. At confluence, the cells were treated with vehicle (0.001% ethanol) or  $10^{-8}\,\mathrm{M}$   $1\alpha,25(\mathrm{OH})_2\mathrm{D}_3$  for 24 hours and harvested as described below.

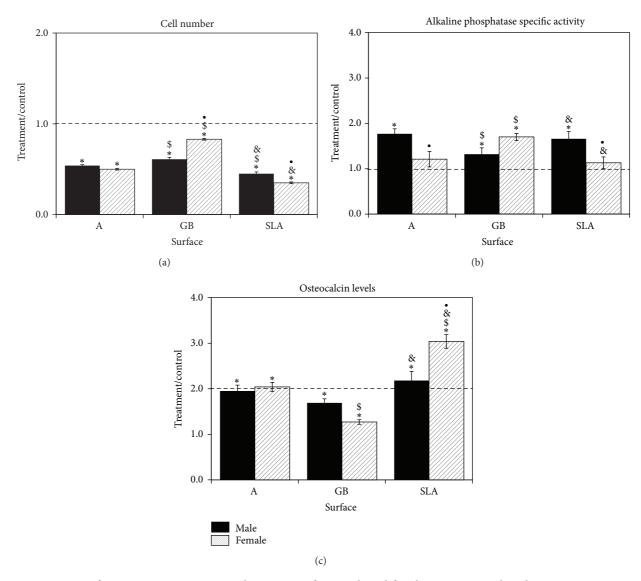


FIGURE 1: Response of rat BMCs to microstructured titanium surfaces. Male and female BMCs were cultured on TCPS, A, GB, or SLA surfaces and grown to confluence. Cell number (a), alkaline phosphatase specific activity (b), and osteocalcin levels (c) were measured. Data are displayed as treatment/control of cells on Ti surfaces to cells on TCPS.  $^*P < 0.05$  versus TCPS;  $^*P < 0.05$  versus A surface;  $^*P < 0.05$  versus GB;  $^*P < 0.05$ , female versus male.

2.4. Biochemical and Immunoassays. Cell number was determined in all cultures 24 hours after cells on TCPS reached confluence. Cells were released from the surfaces using two sequential 10 m incubations in 0.25% trypsin at 37°C, to ensure that any remaining cells were removed from rough Ti surfaces, and counted using an automatic cell counter (ZI Particle Counter, Beckman Coulter, Fullerton, CA). Osteoblast differentiation and maturation were evaluated using alkaline phosphatase specific activity as an early marker and osteocalcin secretion as a later marker [26]. Cellular alkaline phosphatase specific activity (orthophosphoric monoester phosphohydrolase, alkaline; E.C. 3.1.3.1) of the cell lysates was assayed by measuring the release of p-nitrophenol from p-nitrophenylphosphate at pH 10.2 and results were normalized to total protein content of the cell lysates (Pierce BCA Protein

Assay, Thermo Fisher, Rockford, IL). Levels of osteocalcin in the conditioned media were measured by immunoassay (Osteocalcin EIA, Biomedical Technologies, Stoughton, MA).

The conditioned media were also assayed for growth factors and cytokines. Active TGF- $\beta$ 1 was measured prior to acidification of the conditioned media, using an enzymelinked immunosorbent assay (R&D Systems, Minneapolis, MN). Total TGF- $\beta$ 1 was measured after acidifying the media and latent TGF- $\beta$ 1 was defined as total TGF- $\beta$ 1 minus active TGF- $\beta$ 1. Osteoprotegerin (OPG) was measured using an ELISA kit (DuoSet, R&D Systems, Minneapolis, MN). Vascular endothelial growth factor (VEGF) was measured in the conditioned media of BMCs using an ELISA kit (R&D Systems). Immunoassays were normalized to total cell number.

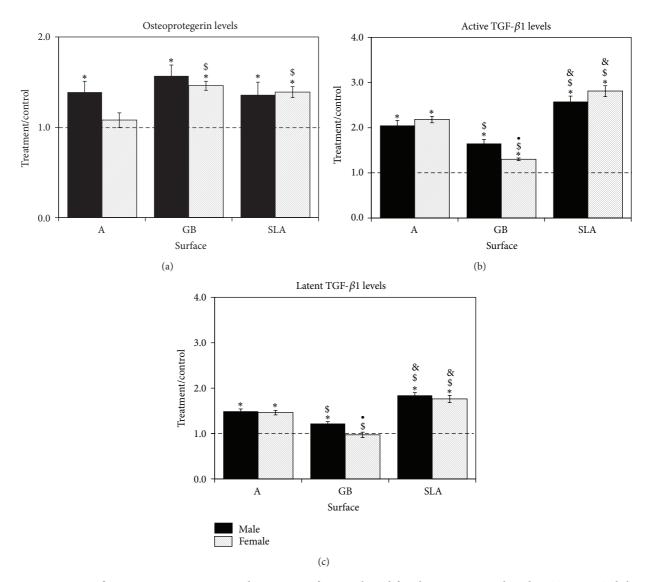


FIGURE 2: Response of rat BMCs to microstructured titanium surfaces. Male and female BMCs were cultured on TCPS or Ti disks and grown to confluence. OPG (a), active TGF- $\beta$ 1 (b), and latent TGF- $\beta$ 1 (c) were measured in the conditioned media. Data are displayed as treatment/control of cells on Ti surfaces to cells on TCPS. \*P < 0.05 versus TCPS; \*P < 0.05 versus A surface; \*P < 0.05 versus GB; \*P < 0.05, female versus male.

2.5. Statistical Analysis. Data presented are treatment/control ratios from one of two experiments, both with comparable results. Responses on TCPS serve as controls. For each experiment, each variable was tested in six independent cultures. Data were first analyzed by ANOVA; when statistical differences were detected, a post hoc analysis of Bonferroni's modification of Student's *t*-test was used. *P* values <0.05 were considered to be significant.

#### 3. Results

BMCs had lower cell number when cultured on Ti substrates in comparison to TCPS (Figure 1(a)). This effect was significantly lower on SLA compared to GB and A and significantly lower on A than GB. Female cells had higher cell number on GB and lower cell number on SLA than male cells.

Alkaline phosphatase specific activity was sensitive to surface topography in a sex-specific manner (Figure 1(b)). Activity was increased in male cells on A and SLA in comparison to TCPS. However, in female BMC cultures, activity was increased only on in cells on GB. Both male and female BMCs exhibited increased osteocalcin in their conditioned media on all surfaces (SLA > A > GB) (Figure 1(c)). This effect was comparable in male and female cultures on GB surfaces, but cells isolated from female rats produced more osteocalcin on SLA than males.

OPG was increased in male cells by 30–50% on all surfaces (Figure 2(a)). Female BMCs showed a comparable increase in OPG on GB and SLA surfaces over levels on TCPS when compared to males. However, female cells cultured on A surfaces did not exhibit increased OPG in comparison to TCPS. Male BMCs produced more active (Figure 2(b)) and

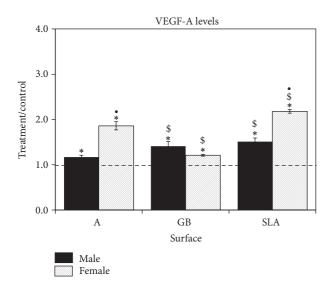


FIGURE 3: Response of rat BMCs to microstructured titanium surfaces. Male and female BMCs were cultured on TCPS or Ti disks and grown to confluence. VEGF was measured in the conditioned media. Data are displayed as treatment/control of cells on Ti surfaces to cells on TCPS. \*P < 0.05 versus TCPS; \*P < 0.05 versus A surface; \*P < 0.05 versus GB; \*P < 0.05, female versus male.

latent (Figure 2(c)) TGF- $\beta$ 1 on all Ti substrates (SLA > A > GB) in comparison to TCPS. Female cells produced similar levels of active TGF- $\beta$ 1 on A and SLA in comparison to male cells; however, they secreted less active and latent TGF- $\beta$ 1 on GB than male cells.

VEGF was also produced in a surface-dependent, sexspecific manner by BMC cells (Figure 3). Male cells produced more VEGF on GB and SLA than on TCPS. In contrast, female cells produced more VEGF on A and SLA than on GB. Female cells produced more VEGF-A on acid-etched A and SLA surfaces than male cells.

Osteoblasts had reduced cell numbers when cultured on Ti surfaces when compared to TCPS (Figure 4(a)). This was less pronounced in cultures grown on GB surfaces compared to A and SLA surfaces and was most pronounced on SLA. 1α,25(OH)<sub>2</sub>D<sub>3</sub> enhanced the decreased cell number of cells grown on SLA surface. In male cells on all surfaces decreased cell number but only affected female cells on SLA. Alkaline phosphatase specific activity was greater in osteoblast cultures grown on Ti substrates in comparison to TCPS (Figure 4(b)).  $1\alpha,25(OH)_2D_3$  increased activity on all surfaces examined. Alkaline phosphatase specific activity was significantly stimulated in osteoblasts from male rats in comparison to female cells. Levels of osteocalcin in the conditioned media were higher in osteoblast cultures on all Ti surfaces compared to TCPS (Figure 4(c)).  $1\alpha,25(OH)_2D_3$ increased osteocalcin in male and female osteoblast cultures, but the stimulatory effect was significant and more than three times greater in the male cells compared to female cells. Moreover, the stimulatory effects of  $1\alpha,25(OH)_2D_3$  were less robust on GB than on A or SLA in the male cells.

OPG was also increased in osteoblast cultures on Ti surfaces in comparison to TCPS (SLA > A > GB) (Figure 5(a)).

This was even more evident in female osteoblast cultures.  $1\alpha,25(OH)_2D_3$  increased OPG by more than 100% in osteoblasts on all surfaces (A, SLA > GB) with no difference between male and female. The response of female osteoblasts was less robust on A and SLA but was comparable to the male cells on GB. Active TGF- $\beta$ 1 was increased in male and female osteoblasts on all surfaces in comparison to control (SLA < A < GB) (Figure 5(b)). Treatment with  $1\alpha,25(OH)_2D_3$  caused significant increases in TGF- $\beta$ 1 in male and female cells on all surfaces (GB < A < SLA). In the untreated osteoblasts, there was no difference between male and female cells in TGF- $\beta$ 1 levels. However, treatment with  $1\alpha,25(OH)_2D_3$  caused a statistically greater increase in male cells than in female cells on A and GB surfaces; however, there was no difference on SLA substrates. Latent TGF- $\beta$ 1 was increased in male osteoblasts on all surfaces in comparison to control and in female osteoblasts grown on A and SLA surfaces; female osteoblasts on GB surfaces were not significantly different from control (Figure 5(c)). Treatment with  $1\alpha,25(OH)_2D_3$ increased latent TGF- $\beta$ 1 in male and female cells on all surfaces following a similar pattern (GB < A < SLA). Male cells had significantly higher levels of latent TGF-\(\beta\)1 than females on all surfaces after treatment with  $1\alpha,25(OH)_2D_3$ ; untreated female osteoblasts had lower levels of TGF- $\beta$ 1 on GB surfaces than male cells.

#### 4. Discussion

This study examined the effects of different clinically relevant surfaces on osteoprogenitor differentiation and osteoblast maturation. BMCs grown on Ti surfaces that were acidetched, grit-blasted, or grit-blasted and acid-etched exhibited a similar reduction in cell number and enhancement of alkaline phosphatase activity and OPG levels. However, the SLA surface, which is the combination of acid etching and grit blasting, significantly enhanced in an additive manner the production of osteocalcin, active and latent TGF- $\beta$ 1, and VEGF in comparison to the other surfaces. These results using primary rat BMCs were similar to the effects of SLA on human mesenchymal stem cells obtained from Lonza that were described previously [6]. The results also demonstrated that the effect of the surface was sex-dependent for some but not all parameters. The clinical importance of this observation in females needs to be examined.

Osteoblast cultures grown on the same Ti surfaces showed similar results with respect to proliferation and maturation as BMCs: reduced proliferation and enhanced production of osteocalcin, OPG, and active and latent TGF- $\beta$ 1. The effects of surface topography were enhanced on SLA, as has been noted previously for the human osteoblast-like MG63 cell line [5, 16, 27]. Both male and female osteoblasts respond similarly to the different surfaces, with the exception of increased levels of OPG in cultures of female cells grown on SLA. These results may indicate that both sexes can osseointegrate well with the appropriate surface and that SLA has a better ability to enhance osteoblastic differentiation and maturation in comparison to either processing method alone.

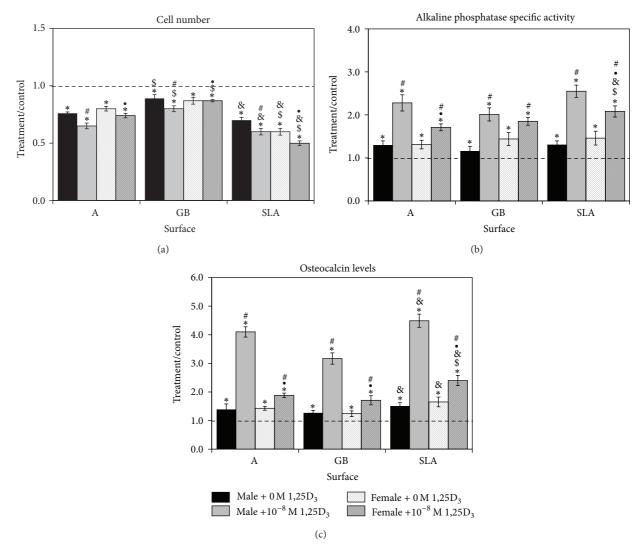


FIGURE 4: Effect of Ti surface topography with or without  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub> on osteoblast differentiation of rat calvarial osteoblasts. Male and female calvarial osteoblasts were cultured on TCPS or Ti disks. At confluence, cells were treated for 24 hours with  $10^{-8}$  M  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub>. Cell number (a), alkaline phosphatase specific activity (b), and osteocalcin levels (c) were measured. Data are displayed as treatment/control of cells on Ti surfaces to cells on TCPS. \*P < 0.05 versus TCPS; \*P < 0.05 versus A surface; \*P < 0.05 versus GB; \*P < 0.05, female versus male; \*P < 0.05 versus 0 M  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub>.

Establishment of a healthy vasculature is critical for implant osseointegration [28]. Both male and female cells increased levels of VEGF in response to Ti surfaces, indicating the cells have begun to signal for new vasculature in response to the surface. However, while male BMCs showed a greater increase in VEGF on GB and SLA surfaces, female BMCs increased VEGF production in response to the submicron-scale topographic features induced by acid etching. Similar studies using human alveolar osteoblasts have shown that VEGF production is increased in cells grown on A and SLA surfaces [29], and previous studies from our group showed that VEGF levels also increased in human mesenchymal stem cells and MG63 cells in response to surface topography [6, 30]. Additionally, in vitro studies have shown that androgen induced a sex-dependent effect on angiogenesis in a Matrigel assay [20].

Previously we demonstrated that fetal rat calvarial osteoblasts are more sensitive to treatment with  $1\alpha,25(OH)_2D_3$  when cultured on Ti substrates [31]. In the present study, we sought to decouple the topographic features that enhanced osteoblast response to  $1\alpha,25(OH)_2D_3$  using adult rat osteoblasts. The rat osteoblasts cultured on Ti respond to  $1\alpha,25(OH)_2D_3$  with decreased cell number and increased alkaline phosphatase specific activity and osteocalcin production in comparison to cells cultured on TCPS. In contrast, this differential response to the vitamin D metabolite may be due to an increased maturation state of the cells grown on Ti substrates at the time of treatment, as has been demonstrated in other studies [31–33].

The effects of  $1\alpha,25(OH)_2D_3$  on the rat osteoblasts were sex-dependent. Treatment with  $1\alpha,25(OH)_2D_3$  increased OPG protein levels in both male and female osteoblasts,

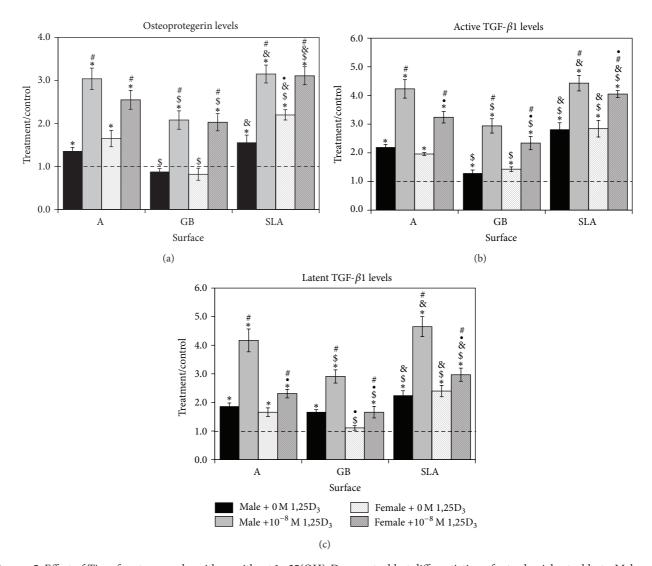


FIGURE 5: Effect of Ti surface topography with or without  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub> on osteoblast differentiation of rat calvarial osteoblasts. Male and female calvarial osteoblasts were cultured on TCPS or Ti disks. At confluence, cells were treated for 24 hours with  $10^{-8}$  M  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub>. OPG (a), active TGF- $\beta$ 1 (b), and latent TGF- $\beta$ 1 (c) were measured in the conditioned media. Data are displayed as treatment/control of cells on Ti surfaces to cells on TCPS. \*P < 0.05 versus TCPS; \*P < 0.05 versus A surface; \*P < 0.05 versus GB; \*P < 0.05, female versus male; \*P < 0.05 versus 0 M  $1\alpha$ ,25(OH)<sub>2</sub>D<sub>3</sub>.

although this effect was greater in males. This confirms previous results in our laboratory demonstrating upregulation of OPG mRNA expression and protein levels after treatment with  $1\alpha,25(OH)_2D_3$  in human osteoblast and MG63 cells cultured on SLA surfaces [15, 34]. Interestingly, treatment of male osteoblasts with  $1\alpha,25(OH)_2D_3$  increased latent TGF- $\beta$ 1 more than active TGF- $\beta$ 1; in female osteoblasts, the greatest response was in active TGF- $\beta$ 1. Previous studies indicate that active TGF- $\beta$ 1 increases in response to  $1\alpha,25(OH)_2D_3$ treatment, possibly due to activation of latent TGF- $\beta$ 1 [35, 36]. However, the dimorphism in the response suggests that in female osteoblasts  $1\alpha,25(OH)_2D_3$  shifts TGF- $\beta1$  levels towards the active form to inhibit bone remodeling [37], while in male cells there is more latent TGF- $\beta$ 1 to allow cells to progress towards terminal osteoblast differentiation [32].

 $1\alpha,25(OH)_2D_3$  enhanced osteoblast maturation and inhibited osteoblast proliferation on all surfaces. When calculated as fold increase, this effect was similar on all surfaces examined. These results indicate that each of these surfaces affects the osteoblast phenotype and makes cells more sensitive to the hormone effect.

The effect of  $1\alpha,25(OH)_2D_3$  on osteoblast cells grown on rough surfaces was sex-dependent since the enhancement of all the parameters examined was significantly higher in male cells in comparison to female cells. These results are in agreement with other studies that have found that femoral neck osteoblasts from males have larger increases in osteocalcin secretion in response to  $1\alpha,25(OH)_2D_3$  than female cells [38]. Clinically, vitamin D deficiency has been correlated with decreased bone mineral density in male, but not female, patients [39]. These results may indicate that

males are more sensitive to vitamin D levels and suggest that if we would like to achieve maximum osseointegration clinically, especially in compromised cases, we could examine the patient's vitamin D levels and supplement as needed if levels are outside the normal range.

The results of the present study indicate that BMCs, the first cells to recognize the surface in vivo, are sensitive to surface topography and can undergo osteogenic differentiation in response to surface cues. The effect was mainly in response to the complex SLA topography and the surface treatments (acid etching and grit blasting) contribute additively to this effect. BMC response to the topographies in this study exhibited sex dependence in some parameters, indicating that they are differentially regulated by both substrate structural elements and cell sex. Primary osteoblasts were also sensitive mainly to the complex SLA topography, with less effect of the individual structural components. Osteoblast response to topography was not sex-dependent to the extent seen in the BMCs. Treatment with  $1\alpha,25(OH)_2D_3$  enhanced osteoblast response to the surfaces examined, with a similar fold increase on all surfaces. The response of osteoblasts to  $1\alpha,25(OH)_2D_3$  is sex-dependent and male cells grown on a complex microstructure surface are much more sensitive  $1\alpha,25(OH)_2D_3$  treatment.

#### 5. Conclusions

These results demonstrate that both surface roughness and systemic hormones can affect bone formation at the implant site. While males and females have similar responses to surface roughness, they differ in production of local factors regulating bone resorption and in the magnitude of the response  $1\alpha,25(OH)_2D_3$ . These factors are important as future modifications are made to tailor implants to sex-specific differences to improve osseointegration and long-term implant life.

#### **Disclosure**

The funding sources had no role in study design, data collection, data analysis/interpretation, or paper publication.

#### **Disclaimer**

The content of this paper is solely the responsibility of the authors and does not necessarily represent the official views of the National Institutes of Health (NIH).

#### **Conflict of Interests**

The authors declare that there is no conflict of interests regarding the publication of this paper.

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