NEURO



Intensity standardization of MRI prior to radiomic feature extraction for artificial intelligence research in glioma—a systematic review

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Received: 14 January 2022 / Revised: 11 March 2022 / Accepted: 10 April 2022 \odot The Author(s) 2022

Abstract

Objectives Radiomics is a promising avenue in non-invasive characterisation of diffuse glioma. Clinical translation is hampered by lack of reproducibility across centres and difficulty in standardising image intensity in MRI datasets. The study aim was to perform a systematic review of different methods of MRI intensity standardisation prior to radiomic feature extraction.

Methods MEDLINE, EMBASE, and SCOPUS were searched for articles meeting the following eligibility criteria: MRI radiomic studies where one method of intensity normalisation was compared with another or no normalisation, and original research concerning patients diagnosed with diffuse gliomas. Using PRISMA criteria, data were extracted from short-listed studies including number of patients, MRI sequences, validation status, radiomics software, method of segmentation, and intensity standardisation. QUADAS-2 was used for quality appraisal.

Results After duplicate removal, 741 results were returned from database and reference searches and, from these, 12 papers were eligible. Due to a lack of common pre-processing and different analyses, a narrative synthesis was sought. Three different intensity standardisation techniques have been studied: histogram matching (5/12), limiting or rescaling signal intensity (8/12), and deep learning (1/12)—only two papers compared different methods. From these studies, histogram matching produced the more reliable features compared to other methods of altering MRI signal intensity.

Conclusion Multiple methods of intensity standardisation have been described in the literature without clear consensus. Further research that directly compares different methods of intensity standardisation on glioma MRI datasets is required.

Key Points

- Intensity standardisation is a key pre-processing step in the development of robust radiomic signatures to evaluate diffuse glioma.
- A minority of studies compared the impact of two or more methods.
- Further research is required to directly compare multiple methods of MRI intensity standardisation on glioma datasets.

Keywords Magnetic resonance imaging · Glioma · Reproducibility of results

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Abbreviations

BraTs	Brain tumour image segmentation benchmark
CycleGAN	Cycle-consistent adversarial network
FLAIR	Fluid-attenuated inversion recovery
GBM	Glioblastoma
GLCM	Grey-level co-occurrence matrices
HSASR	Histogram specification with automated
	selection of reference frames
HS-GS	Histogram specification-grid search
ICC	Intraclass correlation coefficient
IDH1	Isocitrate dehydrogenase 1
MGMT	- O6-methylguanine-DNA methyltransferase
mpMRI	Multiparametric MRI
OS	Overall survival
PRISMA	Preferred Reporting Items for Systematic
	Reviews and Meta-Analysis
QUADAS-2	Quality Assessment of Diagnostic Accuracy
	Studies 2
ROI	Region of interest
SPM12	Statistical Parametric Mapping 12
T1Gd	T1-weighted gadolinium enhanced
T1W	T1-weighted
T2W	T2-weighted
TCIA	The Cancer Imaging Archive
VOI	Volume of interest

Introduction

Adult-type diffuse gliomas are a varied group of highly invasive and heterogenous brain tumours (Fig. 1), with an annual US incidence of 5–6/100,000 and glioblastoma (GBM, the most aggressive glioma) accounting for nearly 50% [1]. Despite maximal safe resection of enhancing tumour, and adjuvant therapy with concomitant temozolomide chemotherapy and 60 Grey in 30 fractions of radiotherapy, followed by 6 cycles of temozolomide ('Stupp protocol'), median overall survival of patients with GBM remains poor at 12–15 months [2, 3].

Multiparametric MRI (mpMRI), with its excellent soft tissue contrast, is frequently used to characterise these tumours [4]. Growing interest in using artificial intelligence (AI) to augment information provided by MRI includes, but is not limited to, non-invasive prediction of cytogenetic alterations, distinguishing treatment effects from pseudoprogression, and distinguishing infiltrative non-enhancing tumour from oedema [5].

Radiomics is a quantitative analytic method of extracting mineable data from medical imaging, and machine learning is typically used to correlate radiomic features and patientspecific data relating to prognosis and/or outcome [6]. Quantitative assessment of the whole tumour volume and surrounding tissues is attractive in the study of a heterogenous disease, which is hampering current treatment strategies [5]. Many radiomic studies evaluating types of diffuse glioma aim to predict prognosis [7], non-invasively diagnose genetic and molecular changes [8] (which play a key role in diagnosis, prognosis, and management), and distinguish between treatment effects and tumour progression [9].

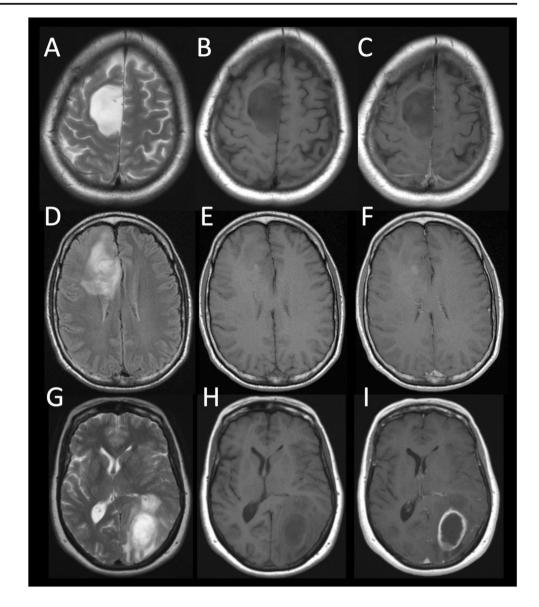
Despite its promise, radiomics has largely been limited to small retrospective proof-of-principle studies, without sufficient evidence to support translation into radiological practice [10]. MRI-based radiomics is limited by the non-biological, scanner-dependent variation in image signal intensity [11–14]. MR intensity does not map easily to a physical tissue property, in contrast to CT, and shows variation between timepoints, vendors, magnetic field strengths, and acquisition settings [15–18]. Radiomic features are highly sensitive to the values of the signal intensities in the image, and nonbiological alteration must be removed. Therefore, MRI signal intensity must be standardised, i.e. the range and distribution of voxel intensity must be similar across patients, prior to radiomic analysis to ensure that the results are reproducible [11]. Despite this, there is a lack of consensus as to the optimal method when characterising diffuse glioma. Although not a specific diagnosis, diffuse glioma is a useful grouping, as they often share the same radiomics pipeline and are a commonly studied group of related tumours [13, 16]. We aim to perform a systematic review of the literature examining the efficacy of different MRI intensity standardisation procedures prior to the extraction of radiomic features in the setting of adult-type diffuse glioma.

Materials and methods

Search strategy and selection criteria

This systematic review was undertaken according to the 'Preferred Reporting Items for Systematic Reviews and Meta-Analysis' (PRISMA) statement. A search of MEDLINE, EMBASE, and SCOPUS databases was performed on 5 October 2021 using the following concepts, linked by the "AND" operator, including synonymous terms that were linked with the "OR" operator: (1) MRI, (2) radiomics, (3) intensity standardisation, and (4) glioma. No limit was placed on the date, language, location, or type of study. Exclusion criteria were the following: non-human based, not regarding adult-type diffuse gliomas, non-original research, non-MR radiomics, no mention of intensity standardisation, or no assessment of the effect of intensity standardisation (compared to another method or to no standardisation). After removing duplicates, articles were screened based on titles and abstract, and subsequently the full text. References in the included articles were manually reviewed. Full search strategy, methodology, and PRISMA checklist are available in the supplementary files.

Fig. 1 MR imaging in three different examples of adult-type diffuse gliomas



Quality assessment

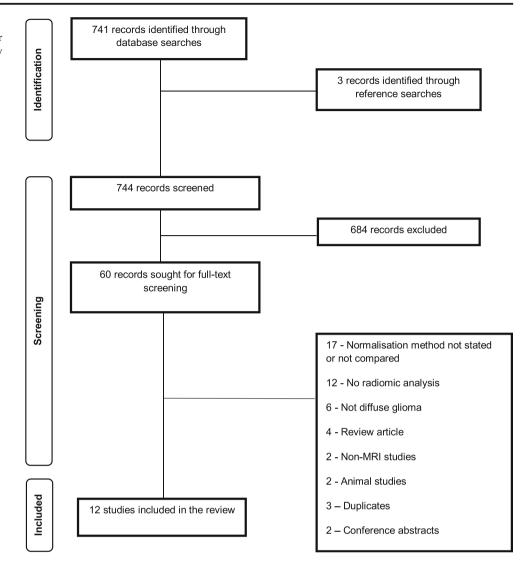
Quality Assessment of Diagnostic Accuracy Studies 2 (QUADAS-2) was used to assess the risk of bias [19]. QUADAS-2 was used because the objective was to evaluate performance of any given intensity standardisation method, when compared to either no standardisation or another method. QUADAS-2 assesses four domains: (1) patient selection—description of how patients were recruited such as inclusion and exclusion criteria; (2) index test—how the index test was conducted and interpreted; (3) reference standard—how the reference test was conducted and interpreted; and (4) flow and timing—patients that did not have the index or reference test or were excluded from final analysis. Each domain was assessed for risk of bias and the first three domains were also assessed for applicability and categorised as either low risk, high risk, or unclear. The index

test was taken to be the intensity standardisation method under investigation, and the reference test was either no standardisation or an alternative method used as a comparator. Two reviewers (F.M., K.F.) independently reviewed each study and any disagreement resolved by consensus.

Results

Search results

After duplicate removal, 741 results were returned from database searches (Fig. 2). Following title and abstract screening, full-text screening was undertaken for 60 articles. Twelve articles meeting the inclusion criteria were included in the review. Two studies by Florez et al [20, 21] were included separately as one used only radiomic features from a fluidFig. 2 PRISMA flowchart illustrating the study selection for the systematic review of intensity normalisation in diffuse glioma radiomic studies



attenuated inversion recovery (FLAIR) sequence [21] and the other used a radiomics extracted from a combination of MRI sequences [20], and this may have an impact upon the results of any intensity standardisation process.

Quality assessment

Risk of bias was assessed for each of the four domains and applicability assessed for the first three domains outlined above. Apart from risk of bias in the patient selection domain and applicability concern for the index test, all other domains were low risk for all studies (Table 1). Ten studies were deemed to have unclear risk due to lack of information on how patients were selected. It was unclear whether institutional patients were selected consecutively or randomly or, if publicly available datasets were used, it was unclear whether any inclusion/exclusion criteria were used to select patients.

For applicability concerns of the index test, two studies [26, 27] were deemed high risk because it was not possible

to isolate the effects of standardisation from other pre-processing. Two studies [24, 30] were low risk in all domains. Two studies by Florez et al [20, 21] also included patients with meningioma, but were not thought to be at risk of bias or an applicability concern as the results for the GBM patients were presented separately.

Characteristics of included studies

Significant heterogeneity in the pre-processing steps and in analysis methodology (Table 2) precluded a meta-analysis and a narrative synthesis is presented.

All studies were retrospective, although two studies [24, 30] utilised prospectively acquired data. Eight included multicentre data, and for one [27], it was unclear whether data comprised single or multicentre data. Five studies used a publicly available multicentre dataset from The Cancer Imaging Archive (TCIA) [29], or competition data from the brain tumour image segmentation benchmark (BraTs) [31] in addition

Study	Risk of bias				Applicability con	cerns	
	Patient selection	Index test	Reference standard	Flow and timing	Patient selection	Index test	Reference standard
Chen et al 2019 [22]	Unclear	Low	Low	Low	Low	Low	Low
Zhao et al 2020 [23]	Unclear	Low	Low	Low	Low	Low	Low
Reuze et al 2018 [24]	Unclear	Low	Low	Low	Low	High	Low
Um et al 2019 [25]	Unclear	Low	Low	Low	Low	Low	Low
Upadhaya et al 2016 [26]	Unclear	Low	Low	Low	Low	High	Low
Florez et al 2018 [21]	Unclear	Low	Low	Low	Low	Low	Low
Florez et al 2018 [27]	Unclear	Low	Low	Low	Low	Low	Low
Hu et al 2021 [28]	Unclear	Low	Low	Low	Low	Low	Low
Hoebel et al 2021 [24]	Low	Low	Low	Low	Low	Low	Low
Vils et al 2021 [29]	Low	Low	Low	Low	Low	Low	Low
Carré et al 2020 [13]	Unclear	Low	Low	Low	Low	Low	Low
Orlhac et al 2020 [14]	Unclear	Low	Low	Low	Low	Low	Low

 Table 1
 Summary of the risk of bias and applicability concerns for the 12 studies

to institutional data. One study [27] used only publicly available data.

The aims of the studies can be divided into two groups:

- 1. To assess the impact of intensity standardisation on the robustness and repeatability of radiomic features, and/or
- 2. To assess the impact of intensity standardisation on a predictive radiomics model.

Nine studies assessed the impact of intensity standardisation on a predictive model. Five studies assessed the impact of standardisation on feature robustness (two studies included both aims). Three groups, Hoebel et al [30], Carré et al [13], and Orlhac et al [14] used a 'scan-rescan' method to test radiomic feature robustness, which involved scanning the same patient after a short interval at different field strengths [13, 14] or on the same machine [30]. Two other studies, Um et al [32] and Reuze et al [26] assessed differences in the feature distribution between paired scanners or the ability of a classifier to distinguish patients scanned internally vs externally [32].

The three main approaches to intensity standardisation can be categorised as histogram matching, deep-learning, or limiting or rescaling the signal intensities. Most of the included studies evaluated one method; however, Carré et al [13] and Hoebel et al [30] used two or more. Further detail on the approaches is discussed in the upcoming sections.

Histogram matching

Histogram matching involves transforming the signal intensities of an image to produce a match between the histogram of the reference and transformed image [25, 33]. The reference histogram is calculated from mean intensities of training images, at pre-specified intensity landmarks [33].

Um et al [32] assessed radiomic feature robustness after the following pre-processing steps: 8-bit rescaling, bias field correction, histogram matching, and isotropic resampling. A Random Forest classifier was used to predict whether images were from internal or external datasets and classification accuracy was measured using the Matthews correlation coefficient. A value of 1 means perfect prediction and 0 no better than chance, and therefore no scanner dependency. The value > 0.2 was taken to mean that images could still retain scanner dependence. Multiple classes of features were extracted. For edge features, different filters (Sobel, Laplacian of Gaussian, Gabor, wavelet) were applied and first-order features extracted. Haralick features were calculated from the grey-level cooccurrence matrices (GLCM). For baseline images, the Matthews correlation coefficients were 0.36, 0.22, and 0.39 (measured from the provided bar chart) for Haralick and the Sobel and Laplacian of Gaussian features, respectively. Histogram matching significantly decreased these to 0.191, 0.170, and 0.140 respectively (p < 0.01).

Zhao et al [34] used histogram specification-grid search (HS-GS), and Chen et al [23] used histogram specification with automated selection of reference frames (HSASR), which automatically select the training histogram. Zhao et al compared the predictive ability of standardised compared to unstandardised images for glioma grading demonstrating an area under the curve (AUC) of 0.956, 27% higher than that without standardisation. Using HSASR, Chen et al achieved 0.9934 AUC for grading (AUC 0.8512 without). These were the highest achieved for glioma grading, although a direct comparison to other methods of intensity standardisation would have been helpful in interpreting the results.

Table 2	Summary of key features from the included studies $(n = 1$	om the included	1 studies $(n = 12)$	2)					
Study	Aims	Patients (train:test seta)	MRI sequences examined	Normalisation method	Pre-processing	Segmentation method	Radiomics software	Results	Conclusion
Chen et al 2019 [22]	To improve prediction of glioma grade using radiomics and the HSASR method of normalisation	521 (416:105)	TIGd	HSASR method	Skull stripping and resampling	Manual	Pyradiomics	Highest AUC was 0.9934 for glioma grading with processing compared to 0.8512 without. The AUC after processing generally increased by	Multicentre data processed by this method have good adaptability, which improves grading results and has value for clinical prediction
Zhao et al 2020 [23]	To examine the impact standardising MRI images with the HS-GS method has on using radiomics to predict glio- ma grades	693 (554:139)	TIGd	HS-GS method	Skull stripping and resampling	Manual	Pyradiomics	The AUC of the predicted classification after HG-GS processing is 0.956 which is 26.96% higher than not perform- ing a standardisation method	The results show that by adding HS-GS method to standard pre-processing, the diagnostic perfor- mance of using radiomics for glioma grading improves with respect to AUC, ACC, sensitivity, and specifici-
Reuze et al 2018 [24]	To assess the effect of intensity rescaling on radiomic analysis of multicentre cohorts and the impact on the robustness of radiomic features	190 (n/a)	TIGd	Intensity rescaling	Spatial resampling and discretisation of grey levels	Manual	LIFEx freeware	Out of the 31 textural features that were extracted, only 11 were deemed to be robust after the harmonisation method	Overall, the efficiency of the harmonisation method differed between devices, therefore it was not deemed to be a sufficient method to correct the differences
Um et al 2019 [25]	To determine the utility of a 161 (111:47) FLAIR, T1W, set of pre-processing and T1Gd methods on improving MRI radiomic feature robustness across multi-institutional datasets	161 (111:47)		Histogram standardisation	Co-registration	Semi-automatic	Computational Environment for Radiotherapy Research (CERR)	From all of the pre-processing methods, histogram standardisation had a superior perfor- mance at reducing covar- iate shift, as Haralick, Soebel, and Laplacian of Gaussian features re- turned a significant de- crease of Matthews cor- relation coefficient to 0.191, 0.170, and 0.140	From all the pre-processing methods, histogram standardisation contrib- utes the most an tentib- vestigated measures such as feature dependence on scanner variability and covariate shift
Upadhaya et al 2016 [26]	To identify the impact of adding several pre-processing steps on the accuracy of the prog- nostic model which identifies patients above	58 (58:58b)	TIW, T2W, TIGd, and FLAIR	Dynamics intensity limitation	Bias field correction, skull stripping, co-registration, spatial resampling, and intensity quantisation	Automatic	Not identified	respectively ($p < 0.01$) The additional pre-processing steps im- proved the prognostic model from sensitivity and specificity of 79% and 86% respectively to a	The addition of investigated pre-processing methods highlights how various acquisition methods from different MR scan- ners can influence the

Table 2	(continued)								
Study	Aims	Patients (train:test seta)	MRI sequences examined	Normalisation method	Pre-processing	Segmentation method	Radiomics software	Results	Conclusion
Florez et al 2018 [21]	and below a median sur- vival of 12 months To assess the ability of radiomic feature, to differentiate gross tumour volume (GTV) from oedema and differ- entiate vasogenic from tumour cell infiltration	17 (17;n/a)	T1W, T1Gd, T2W, FLAIR and apparent diffusion coefficient (ADC)	1%-99% normalisation	Segmentation	Semi-automatic MatLab version 2016a	MatLab version 2016a	sensitivity and specificity of 93% Out of all of the sequences examined, T1Gd with 1–99% normalisation was the model best at classifying tumours with an AUC > 0.97	accuracy of prognostic models From the several hundred of radiomic feature extracted, only a small subset showed excellent ability to classify turnour tissue
Florez et al 2018 [27]	To assess the ability of radiomic features to distinguish oedema and infiltrative turnour based on FLAIR sequence	20 (20;n/a)	FLAIR	1–99% nomalisation	Segmentation	Semi-automatic MatLab version 2016a	MatLab version 2016a	Performance using single best discriminator reduced with addition of normalisation (AUC 0.87 vs 0.84) in patients with CRM	Small subset of texture features shows the ability to discriminate oedema from tumour
Hu et al 2021 [28]	To evaluate the impact MIL normalisation has on segmentation and feature extraction which allows the prediction of pathological grading and <i>IDHI</i> status	800 (533:267)	T1W, T1Gd, and FLAIR for all of the datasets (and T2W for the BraTs dataset, n = 285)	CycleGAN	Modality normalisation, layer spacing normalisation	Automatic	Not identified	MIL normalisation improved the AUC of pathological grading and IDH1 status prediction by 32% and $25%$ ($p < 0.001$) respectively. The accuracy of the pathological grading and IDH1 mutation prediction rose from 0.69 and 0.70 to 0.89 and 0.91 respectively after MIL	MIL normalisation can produce high-quality standardised data which is imperative for radiomic analysis
Hoebel et al 2021 [24]	To assess the impact of intensity normalisation methods (z-score normalisation and histogram matching) and intensity quantisation methods has on the re- peatability and reproduc- ibility of features extract- ed from a scan-rescan glioblastoma cohort.	48 (n/a)	TIGd and FLAIR	z-Score normalisation and histogram matching	Segmentation, registration, bias field correction, and whole-brain extraction	Manual	Pyradiomics	normasiation For intensity features, both methods improved the repeatability on FLAIR images when compared to non-normalised base- line ($p = 0.003$ for z-score and $p = 0.002$ for histo- gram matching). This differs for T1Gd as both methods did not signifi- cantly effect the intraclass correlation coefficient of intensity features be-	Both normalisation methods showed better repeatability for FLAIR images than T1Gd images, which may be a consequence of variations in contrast administration and timing of image acquisition after contrast administration
Vils et al 2021	To evaluate the association between radiomic	118 (69:49)	T1Gd	Linear intensity interpolation		Manual	Z-Rad	tween scan and rescan Regarding radiomic models capable of predicting	The proposed model may be a non-invasive

Table 2	Table 2 (continued)								
Study	Aims	Patients (train:test seta)	MRI sequences examined	Normalisation method	Pre-processing	Segmentation method	Radiomics software	Results	Conclusion
[29]	features, clinical outcome, and molecular characteristic such as MGMT status				Segmentation and manual extraction of brain tissue			MGMT status, images where the features were extracted from turnoural volumes of interest and normalised with linear interpolation were the only images validated in an independent cohort with an AUC of 0.670 (0.55% CTI 0.5341–0.8056)	approach to predict pa- tient response to chemo- therapy
Carré et al 2020 [13]	To assess the impact of three intensity normalisation methods coupled with grey level discretisation on the task of tumour grade classification in two independent cohorts	263 (195:48) TIGd and FLAIR	TIGd and FLAIR	Nyul, WhiteStripe, and Z score normalisation method	Bias field correction, Manual spatially resampled, skull-stripping, co-registration and segmentation	Manual	Pyradiomics		A combination of <i>z</i> -score normalisation and absolute discretisation produces the best results for models based on first and second order features
Orlhac et al 2020 [14]	To assess the impact of intensity normalisation and post-extraction re- alignment (ComBat) on the statistical distribution of radiomics from diffuse gliomas	8	TIGd and FLAIR	Hybrid WhiteStripe (and ComBat)	Co-registration, bias field correction, spatial resampling	Manual	LIFEx freeware		Intensity standardisation results in similar intensity values in images, but significant scanner-dependent changes require further correction with ComBat
<i>HSASR</i> hi ^a Train/tes	HSASR histogram specification with automatic selection of reference, $HS-GS$ histogram specification grid search ^a Train/test numbers are only stated for any predictive model developed in the study; 'n/a' stated if no model was developed	itomatic selecti any predictive	ion of referenc model develo	e, <i>HS-GS</i> histogran ped in the study; 'n	a specification grid ser /a' stated if no model	arch was developed			

^b Model developed using leave one out cross-validation, according to stated references in the study

Deep learning

Hu et al [22] describe 'MIL' pre-processing and intensity normalisation that corrects: modality incompleteness (M), uneven intensity distribution (I), and inconsistent layer spacing (L) in mpMRI datasets of T1-weighted (T1W), T1Gd, T2-weighted (T2W), and FLAIR sequences. Modality incompleteness is the absence of MRI sequences (referred to as 'modalities'), for example T1Gd. Intensity unevenness is MRI signal intensity variation, and inconsistent layer spacing refers to variation in slice thickness. Effect of MIL normalisation on accuracy of radiomics model for glioma grading, for isocitrate dehydrogenase 1 (IDH1) prediction (a key genetic marker of adult-type diffuse glioma that has prognostic and diagnostic qualities), and on tumour segmentation was assessed. A cycle-consistent adversarial network (CycleGAN) standardised signal intensities, and a deep learning network synthesised any missing MRI sequences using an encoder (a modified U-net) and separate decoder [22]. Slice thickness was standardised using interpolation software, Statistical Parametric Mapping 12 (SPM12). AUC 0.693 (95% CI 0.613-0.772) was reported for unprocessed images, which increased following synthesis of missing sequences (AUC 0.838, 0.772-0.904), intensity standardisation (0.704, 0.626-0.783), and layer space normalisation (0.716, 0.639-0.793). Combining the three steps produced the best performing model (0.89, 0.838-0.941), highlighting the additive effects of the pre-processing pipeline.

Limiting or rescaling signal intensity

Reuze et al rescaled the signal intensity between 0 and 32767 per patient and concurrently resampled to $0.5 \times 0.5 \times 0.5 \text{ mm}^3$ and assessed the impact on feature robustness on images from 11 MRI scanners [26]. From 31 textural features, 11 were found to be robust among differing magnetic field strength post-normalisation (p > 0.05 on Wilcoxon paired test). Results from intensity standardisation alone were not presented.

Upadhaya et al assessed the effect of pre-processing steps on the accuracy of a overall survival (OS) prediction model [27]. Baseline pre-processing steps included bias field correction, skull stripping, and registration, with additional spatial resampling, intensity quantisation, and normalisation. Intensity normalisation ignored any values outside of the range: (m-s, m+s). m and s are the mean and standard deviation of the intensity values within the VOI. If the model utilised additional sequences and pre-processing steps, sensitivity improved from 79 to 93% and specificity from 86 to 93%. The effect of intensity standardisation alone was not presented.

Florez et al evaluated intensity standardisation on differentiation of tumour volume and oedema in 17 and 20 GBM patients [20, 21]. A 1-99% normalisation, where the 1^{st} and 99th centiles of the intensity histogram are included [28], was compared to no normalisation. Normalised T1Gd sequences produced the best model with an AUC > 0.97 (0.85 without normalisation) [20]. The performance of normalised T2W images decreased—AUC of 0.85 (normalised) compared to AUC 0.91 (without). In a separate study, utilising only FLAIR, normalisation reduced AUC for discriminating tumour and oedema (AUC without 0.87, AUC with normalisation 0.84) [21].

Vils et al assessed the impact of linear intensity interpolation in 118 patients with recurrent GBM [24]. Linear intensity interpolation uses two regions of interests (ROIs) within normal contralateral white matter and the vitreous body:

intensity_{normalized}

$$= intensity_{original} \frac{500}{intensity_{white matter} - intensity_{eye}} + 800 - \frac{500 intensity_{white matter}}{intensity_{white matter} - intensity_{eye}}$$

A radiomic model for prediction of O6-methylguanine-DNA methyltransferase (MGMT) promoter methylation (molecular marker for treatment response and prognostication) following normalisation achieved an AUC of 0.673 (95% CI 0.4837–0.8618) on the validation set. Without interpolation, the model achieved an AUC of 0.660 but could not be validated.

Orlhac et al assessed the impact of hybrid WhiteStripe normalisation on the distribution of features from normal white matter and tumours in 18 patients with diffuse glioma that had been scanned and rescanned at different field strengths [14]. WhiteStripe subtracts the mean and divides by the standard deviation of normal white matter intensity [35]. WhiteStripe reduced the number of significantly different features in normal white matter (88 to 69%) and tumour (98 to 60%), highlighting considerable remaining scanner dependency.

Comparison of techniques

Carré et al [13] and Hoebel et al [30] both used histogrammatching and Z-score. Z-score normalisation subtracts the mean signal intensity from each voxel and divides by the standard deviation of the ROI [13]. Carré et al also used WhiteStripe.

Hoebel et al assessed the repeatability, using the intraclass correlation coefficient (ICC), of radiomic features extracted from a set of scan-rescan T1Gd and FLAIR images of 48 patients diagnosed with GBM [30]. *Z*-score and histogram matching improved repeatability of intensity features on FLAIR but not T1Gd. Histogram matching improved repeatability of texture features on FLAIR (p = 0.003), whereas *Z*- score did not and neither technique improved the repeatability of texture features on T1Gd.

Carré et al [13] assessed the impact of intensity normalisation on feature robustness and the prediction of glioma grading. Using a scan-rescan dataset of 20 patients with low-grade glioma, histogram matching was found to produce the highest number of robust first-order features on both T1Gd and FLAIR images (ICC and CCC > 0.80, 16 and 8 features out of 18 respectively). Regarding glioma grading using T1Gd images, and only robust features from the first scan-rescan experiment, the average balanced accuracy increased from 0.73 to 0.81, 0.79, and 0.81 for histogram, WhiteStripe, and *Z*-score respectively.

Discussion

To be clinically useful, radiomics needs to be validated [36], with unique challenges when evaluating radiomic predictive models [37]. For MRI radiomics, a key challenge to assessing repeatability and reproducibility is to remove the scanner-dependent signal intensity changes [11]. This review confirms that intensity standardisation improves radiomic feature repeatability and improves most predictive models, and therefore that the clinical radiologist needs to be aware of this crucial step in any radiomics studies or applications. Variation in methodology precluded the direct comparison of results across studies and this review has highlighted potential areas of improvement, which may improve translation of radiomic models into the clinical setting (Table 3).

In two studies [26, 27], the effects of intensity standardisation were difficult to differentiate from other preprocessing, and the authors could have reported separately the impact of different pre-processing steps on feature robustness or model performance. Hu et al presented all possible combinations of pre-processing steps, with separate AUC results, so the impact of each step was identifiable. Only two studies [13, 30] compared more than one intensity technique. Given the number of methods and lack of consensus, more studies that directly compare techniques are required. This is important when interpreting the results of histogram specification studies [23, 34]. The AUC for grading was the highest reported; however, it is unclear how this relates to other techniques. A recent analysis [16] compared multiple intensity standardisation techniques and post-feature extraction correction with ComBat, a statistical normalisation for batch-effect correction in genomics that has been applied to radiomics [11, 14]. Intensity standardisation was insufficient to remove scanner dependency, but ComBat could remove scannerdependent information from extracted features [16], similar to the findings of Orlhac et al [14].

Three studies used scan-rescan data, providing the opportunity to assess radiomic feature reproducibility on images from the same patient acquired within a short time delay (i.e. days between studies). Although a tumour may change microscopically within several days, these radiomic studies assume that if the imaging appearance remains the same then the radiomic features ought to as well [13, 14, 30]. Test-retest data, along with phantom studies [16], and comparison of radiomic features extracted from normal structures provide a useful paradigm to test standardisation techniques. Open access to such data in a public repository should help further validate different intensity standardisation approaches.

Limitations to this review include not being able to retrieve full-text articles for two conference abstracts. Based on the abstracts, it is unlikely they would have been included. Their potential omission will have had a limited impact as a narrative synthesis would still have been required. QUADAS-2 is not specifically designed for assessing the efficacy of MRI intensity standardisation techniques, but we considered this a viable method given the absence of a more specific alternative. The scope of this review was to assess MRI intensity standardisation in the context of diffuse glioma and there will have been the inevitable omission of studies of other organs, brain pathologies, and healthy volunteers.

Limitation	Opportunity
1. Assessing the effect of multiple preprocessing steps simultaneously	Effects of preprocessing steps presented independently of others so their effect on the result can be determined
2. Investigating the effect of only one intensity standardisation technique	Impact of more than one standardisation method on a predictive model or feature robustness should be evaluated
3. Lack of scan-rescan data used to test the repeat- ability of radiomic features	Increased availability of datasets that have rescanned a patient with a diffuse glioma within a short time interval (i.e. days) in public databases
4. Single-centre studies used to assess standardisation techniques	Use of multi-centre datasets in assessing the efficacy of standardisation techniques and repeat- ability of radiomic features

Conclusion

No clear consensus has emerged as to which approach is the most reliable standardisation approach. In order to translate radiomics to the clinic, studies should assess the effects of intensity standardisation on their results and the impact of any intensity standardisation step should be clearly reported. Collation and sharing of scan-rescan datasets would facilitate production of radiomic models in diffuse glioma and greatly improve the development of clinically translatable models.

Supplementary Information The online version contains supplementary material available at https://doi.org/10.1007/s00330-022-08807-2.

Acknowledgements The authors would like to acknowledge Cancer Research UK funding for the Leeds Radiotherapy Research Centre of Excellence (RadNet; C19942/A28832).

Funding KF is a 4ward North Clinical PhD fellow funded by Wellcome award 203914/Z/16/Z. Salary for AFS & SC is supported by the Leeds Hospitals Charity and Leeds RadNET, and salary for MGN and AC is supported by RadNET. Salary for JOC is supported by Cancer Research UK Advanced Clinician Scientist Fellowship (C19221/A22746).

Declarations

Guarantor The scientific guarantor of this publication is SC.

Conflict of interest The authors of this manuscript declare no relationships with any companies, whose products or services may be related to the subject matter of the article.

Statistics and biometry No complex statistical methods were necessary for this paper.

Informed consent Written informed consent was not required for this study because it is a systematic review of published literature.

Ethical approval Institutional Review Board approval was not required because it is a systematic review of published literature.

Methodology

- retrospective
- observational
- performed at one institution

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