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Effect of haemolysis on FTIR and Raman spectra of blood plasma

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Abstract

Haemolysis is a very common phenomenon and is referred as the release of intracellular components from red blood cells to the extracellular fluid. Haemolysed samples are often rejected in clinics due to the interference of haemoglobin and intracellular components in laboratory measurements. Plasma and serum based vibrational spectroscopy studies are extensively applied to generate spectral biomarkers for various diseases. However, no studies have reported the effect of haemolysis in blood based vibrational spectroscopy studies. This study was undertaken to evaluate the effect of haemolysis on infrared and Raman spectra of blood plasma. In this study, prostate cancer plasma samples (n=30) were divided into three groups (non-haemolysed, mildly haemolysed and moderately hemolysed) based on the degree of haemolysis and FTIR and Raman spectra were recorded using high throughput (HT)-FTIR and HT-Raman spectroscopy. Discrimination was observed between the infrared and Raman spectra of non-haemolysed and haemolysed plasma samples using principal component analysis. A classical least square fitting analysis showed differences in the weighing of pure components in non-haemolysed and haemolysed plasma samples. Therefore, it is worth to consider the changes in spectral features due to haemolysis when comparing the results within and between experiments.

Keywords: Haemolysis, blood plasma, FTIR spectroscopy, Raman spectroscopy, principal component analysis, classical least squares fitting analysis.

1. Introduction

Haemolysis (or hemolysis) refers to the breakdown of erythrocytes and resulting in the release of intracellular components into the extracellular fluid, i.e. the plasma or serum [1]. Haemolysis is discernible as a red colouration of the plasma or serum after centrifugation of the sample and can occur both in-vivo and in vitro. The upper reference limit for free haemoglobin in plasma is around 20 mg/L [2]. Several factors causing in-vitro haemolysis are given in Table 1 [2]. Not all haemolysed specimens can be associated with in-vitro haemolysis because more than 50 medical conditions are associated with in-vivo haemolysis [3], such as cancer [4], autoimmune disorders [5], surgery [6] etc. In-vivo haemolysis can be easily concealed by in-vitro haemolysis. In these cases, samples haemolysed because of a medical condition may be refused because haemolysis had been attributed to improper specimen phlebotomy, without considering the condition causing in-vivo haemolysis [7].

In-vivo haemolysis can be distinguished from in-vitro haemolysis by estimating the concentration of haptoglobin [8]. Haptoglobin is formed in the liver and binds to free haemoglobin released from in-vivo lysed red cells to prevent its toxic effects [9]. The haptoglobin levels are reduced in the presence of large amounts of free haemoglobin, a decrease in the concentration of serum haptoglobin is the most marked laboratory indicator of in-vivo haemolysis [9]. In severe cases of in-vivo haemolysis, haptoglobin levels may be very low or even undetectable, whereas with in-vitro haemolysis the concentration of haptoglobin is usually not affected [8]. However, several studies have examined the potential of haptoglobin have been shown depending on the cutoff concentration used. One study used a haptoglobin cutoff of less than 25 mg/dL and demonstrated 83% sensitivity and 96% specificity for intravascular haemolysis [10]. Another used a haptoglobin cutoff of less than 28 mg/dL and noted 91.8% sensitivity and 98.4% specificity for intravascular haemolysis, late to the liver cirrhosis, disseminated ovarian carcinomatosis, pulmonary sarcoidosis, and elevated oestrogen states [9].

In general, there is no gold standard test to confirm in-vivo haemolysis, and most often labs rely on other clinical factors (e.g. increased reticulocyte count and decreased haptoglobin) and correlation with other laboratory markers (e.g., complete blood count, lactate dehydrogenase and indirect bilirubin) in addition to a patient's history [2,9].

Many laboratory chemistry tests depend on the evaluation of light that passes through a sample, and therefore haemolysed blood can interfere with these tests, as the red colour of haemoglobin can interfere with the absorption of light as it passes through a haemolysed sample [12]. In spectrophotometric assays, the absorption peak of oxyhaemoglobin lies between 531 and 543 nm. This absorption peak is relatively broad so haemolysis intervenes over many wavelengths that are used for the quantification of analytes [12]. Haemolysis also interferes with laboratory tests by releasing analytes into the serum or plasma that are elevated in concentration within the red blood cells compared to serum or plasma, thereby giving false concentrations of measured analytes [13].

The application of vibrational spectroscopy (infrared and Raman spectroscopy) to generate spectral biomarkers of disease using biofluids such as plasma or serum is gaining increased focus. Infrared spectroscopy is based on the absorption of infrared radiation by the sample under study and the fact that molecules absorb specific frequencies of the incident light which are characteristic of their structure. Raman spectroscopy is based on inelastic scattering of monochromatic light, usually from a laser source. Many articles have been published reporting the use of Fourier Transform Infrared (FTIR) and Raman spectroscopy with serum and/or plasma as non-invasive diagnostics for various diseases, including cancers [14–17]. Despite haemolysis being very common in practice, no spectroscopic study has examined its effects on spectral markers and the concentration of analytes.

This study was undertaken to investigate the effect of haemolysis on Raman and FTIR spectra of plasma in prostate cancer patient plasma samples (n = 30). A combination of ultraviolet (UV)-Visible, high throughput (HT) - Raman and HT-FTIR spectroscopies were used to evaluate the spectral content of both haemolysed and non-haemolysed plasma. Significant spectral differences were observed in the infrared and Raman spectra of non-haemolysed and haemolysed plasma samples. The acquired FTIR and Raman spectra were also analysed by principal component analysis (PCA) and classical least squares (CLS) fitting analysis in the MATLAB environment.

The CLS fitting analysis was employed to estimate the changes in the weighting of various analytes in non-haemolysed and haemolysed plasma samples.

2. Experimental section

2.1. Ethical approval

Ethical approval was awarded by the Technological University Dublin Research Ethics Committee for the collection of blood samples from healthy donors. The prostate cancer patients used in this study were recruited from the Cancer Trials Ireland (formerly All Ireland Cooperative Oncology Research Group, ICORG) trial 08-17 which is entitled "A Prospective Phase II Dose Escalation Study Using intensity modulated radiotherapy (IMRT) for High Risk N0 (cancer has not spread to nearby lymph nodes) M0 (or elsewhere in the body) Prostate Cancer (NCT00951535)". The patients were recruited for a translational study on vibrational spectroscopy for monitoring radiation therapy response [18]. The translational research study was approved by the St Luke's Radiation Oncology Network Research Ethics Committee and all research was performed in accordance with relevant guidelines and regulations. Informed consent was obtained from all participants. Fresh whole blood was drawn into Li-heparin tubes at St. Luke's Radiation Oncology Network, St. Luke's Hospital (SLRON SLH), in Dublin, and were coded before being transferred to the Technological University (TU) Dublin laboratory. Plasma from prostate cancer patients were used to study the effect of in-vivo haemolysis on Raman and FTIR spectra of blood plasma. The clinical characteristics of prostate cancer patients are detailed in Table 2. Plasma from male healthy donor (age, 50 years) was used to study the effect of in-vitro haemolysis on Raman spectra of blood plasma.

2.2. Plasma isolation

Plasma was isolated from these blood samples by centrifugation at 3500 g for 5 minutes at 18^oC. The samples were subsequently stored at -80^oC prior to FTIR and Raman acquisition.

2.3. Haemoglobin isolation

A volume of 1ml of whole blood sample was centrifuged at 3500 g for 5 minutes to remove plasma. The pelleted red blood cells (RBCs) was purified by washing with phosphate buffer saline (PBS) for at least three times. The residual PBS was removed by centrifugation at 3500 g for 1 minute . After purification, deionised water was added to the RBCs and sonication was performed for 30 sec to rupture the RBCs. Then, the diluted haemoglobin was further centrifuged at 3500 g for 5 minutes to remove RBC membrane. The isolated diluted hemoglobin sample was stored at -80^oC before Raman measurements.

2.4. Ultraviolet - visible spectroscopy

UV-visible spectroscopy is generally used in analytical chemistry for the quantitative determination of various analytes. UV-visible spectroscopy uses light in the visible and adjacent ranges. In this study, free haemoglobin of the plasma samples was measured spectrophotometrically (Perkin Elmer Lambda 900) with water as a blank. Thirty microliters of plasma samples were deposited on the quartz microsample cell with 0.1mm pathlength and the absorbance at 414 nm were used to determine the haemolysis in the sample. The concentration of haemoglobin in plasma was determined using the Beer-Lambert law.

2.5. FTIR spectroscopy

The sample preparation and acquisition methodology for FTIR spectra was detailed in our previous paper [18]. Briefly, plasma samples stored at -80° C were thawed at room temperature and were diluted threefold in physiological water. A volume of 4 μ L diluted plasma sample was deposited on a 384-well silicon plate (Bruker Optics GmbH, Ettlingen, Germany), and air-dried at room temperature. For each sample, 10 spots were used giving 10 instrumental replicates. The plate was then inserted into a high-throughput module (HTS-XT, Bruker Optics GmbH) attached to an FTIR spectrometer (Tensor 27, Bruker Optics GmbH). FTIR spectra were acquired in the transmission mode using the OPUS v6.5 software (Bruker Optics GmbH) in the wavenumber range from 4000 to 400 cm⁻¹, using a spectral resolution of 4 cm⁻¹ and 32 co-additions. FTIR spectra were then subjected to a quality test (OPUS v6.5) and details of this test are fully described in reference [19, 20]. Spectra that passed the quality test were pre-processed and processed in the wavenumber range from 800 to 4000 cm⁻¹.

2.6. Raman spectroscopy

Raman spectra from liquid plasma samples were recorded using an in house developed HT-Raman spectroscopy method [17]. Briefly, 20 μ l of liquid plasma samples were deposited on a cover glass bottomed 96 well plate (MatTek corporation) and Raman spectra of the plasma samples were acquired using a 785nm laser focused through a 10x objective (N.A. 0.25). Spectra were recorded using a diffraction grating ruled with 300 lines/mm giving a spectral resolution of ~2.1cm⁻¹. Spectra were recorded automatically from each well where the spectrometer was programmed using an in-house developed high throughput macro template. Each spectrum was acquired over the region from 400 –1800 cm⁻¹. Ten spectra were recorded from each sample for each patient with a 20 s x 2 integration time. Multiple wavenumber calibration spectra of 1,4-Bis (2-methylstyryl) benzene and intensity calibration spectra of National Institute of Standards and Technology (NIST) Standard Reference Material (SRM) no. 2241 were recorded along with each sample acquisition and used in spectral post-processing.

2.7. Pure molecular reference species recording

All pure molecular references species (Table 3) were purchased from Sigma Aldrich. These molecular species include proteins, lipids and other analytes which are usually found in the blood plasma. Moreover, previous other studies also reported the variations in most of these molecular species due to the effect of haemolysis [13, 21–23]. Additionally, molecular reference species of lipids and fatty acids were included to study their interference in the plasma spectra due to in-vivo haemolysis. More details of these pure molecular reference species are provided in supplementary material.

Approximately 1–2 mg of each lyophilised analyte or 10 μ L of liquid analyte was deposited on a calcium fluoride slide and Raman spectra were recorded with a 785 nm laser excitation. The laser was focused through a 10× objective (N.A. 0.25) using a diffraction grating ruled with a grating of 300 lines per mm. Five spectra per sample were recorded for the acquisition time of 10 seconds and 2 accumulations. FTIR spectra of all analytes were recorded using Attenuated total reflectance (ATR)-FTIR (Perkin Elmer). Approximately 1 mg of lyophilised analyte or 5 μ L of liquid analyte (allowed to dry at room temperature) was placed on the ATR crystal (Diamond / Zinc Selenide with refractive index 2.4) and FTIR spectra were acquired in the transmission mode using the

spectrum software and using the following conditions: wavenumber range from 4000 to 700 cm⁻¹, spectral resolution of 4 cm⁻¹, and each spectrum was averaged over 8 scans.

2.8. Data analysis

All spectral processing procedures were carried out using MATLAB (R2017a; Mathworks Inc., Natick, MA), along with in-house developed algorithms and procedures available within the PLS Toolbox (v 8.0.2, Eigenvector Research Inc., Wenatchee, MA).

2.8.1. Pre-processing

Pre-processing of FTIR spectra includes baseline correction, calculation of second derivative spectra and vector normalisation. Baseline correction was performed using the rubberband baseline subtraction [24]. Second derivative spectra were calculated using Savitsky-Golay algorithm [25] and a window length of 9 points. All spectra were standardized using vector normalization before analysis.

The acquired Raman spectra were wavenumber calibrated relative to an in-house standard of 1,4-Bis (2-methylstyryl) benzene using in-house developed calibration procedures [26] and the instrument response correction was performed using the spectrum of NIST Standard Reference Material (SRM) no. 2241, according to the method described [27]. Briefly, SRM 2241 emits a broadband luminescence spectrum when illuminated with 785 nm Raman excitation laser. The shape of this luminescence spectrum is represented by a polynomial expression that relates the relative spectral intensity to the Raman shift. This polynomial along with a standard luminescence spectrum can be employed to determine the spectral intensity-response correction, which is unique to each Raman system. The derived instrument intensity response correction can be used to obtain Raman spectra that are corrected for instrument dependent artifacts [27]. The wavenumber and instrument response correction were performed using a Savitzky-Golay filter. The background and baseline correction were performed using Extended Multiplicative Scattering Correction (EMSC). Then, spectra were standardized using vector normalization. An example of intensity corrected, and pre-processed liquid plasma spectrum is shown in Figure 1.

2.8.2. Multivariate analysis

Pre-processed FTIR and Raman spectra were further processed with PCA and CLS fitting analysis.

2.8.2.1. PCA

PCA was performed with the similar approach as described earlier [18]. In brief, PCA is a commonly used method for multivariate data compression and visualization. It describes data variance by identifying a new set of orthogonal features, called principal components (PCs).

2.8.2.2. CLS fitting analysis

In this study, classical least squares (CLS) fitting analysis was performed on the second derivative FTIR spectra and vector normalised Raman spectra to estimate the relative fraction (a proxy for concentration) of reference spectra (of pure components) within a sample spectrum. The use of CLS fitting analysis to determine the relative concentrations of cellular components have been reported previously [28,29]. The pure components used in this study are given in Table 2. CLS is an exploratory method that assumes that any complex spectrum is the linear sum of contributions from spectra of pure components that contribute to the spectrum as described in the following equation [30]:

$$S = a_1C_1 + a_2C_2 + \dots + E$$

Where S represents a sample spectrum, a1 and a2 are component spectra and C1 and C2 are the weights or concentrations assigned to each component spectrum. In the case of a Raman or FTIR spectrum, not all contributing pure components are known. Therefore, an error or residual, E, in the fitting estimation will be observed that will equate to the difference between the sample spectrum and the sum of the component spectra:

$$E_j = S_j - (a_{1j}C_1 + a_{2j}C_2 + a_{3j}C_3)$$

Where E_j is the error associated with the intensity of the j-th wavenumber. Applying CLS minimizes the error in fitting the sample spectrum, *S*. The minimum error occurs when the differential of the sum of squared errors is equal to zero.

$$\frac{(d(\sum jE_j^2)}{dC_1} = \frac{d\sum_j(S_j - (a_{1j}C_1 + a_{2j}C_2 + a_{3j}C_3)^2)}{dC_1} = 0$$

Differentiating with respect to each of the component will give the above equation and using the method of simultaneous equations the weighting components can be calculated. Alternatively

using matrix methods and the matrix of weighting coefficients can be solved for using the following equation.

$$[C] = [A] [a]^T [aa^T]^{-1}$$

where *a* is a component of sample spectra.

3. Results and discussion

3.1. Haemoglobin spectra

Three different types of plasma samples were observed in our plasma biobank (Figure 2). The normal plasma sample is clear and pale yellow in colour (Figure 2C). The haemolysed plasma sample is pale red in colour (Figure 2A) and the lipemic plasma sample is white in colour (Figure 2B). Lipemia is a turbidity of the sample caused by aggregation of lipoprotein particles ³¹.

Figure 3 shows a representative UV-Visible absorption spectrum of haemoglobin recorded from the haemolysed prostate cancer plasma sample. The absorption bands at 414 cm⁻¹, 546 cm⁻¹ and 571 cm⁻¹ indicates the presence of oxyhaemoglobin. Figure 4 shows the FTIR absorption spectrum recorded from the haemoglobin standard (Sigma Aldrich). As haemoglobin is a protein, the FTIR absorption spectrum contains amide I band (between 1600 and 1700 cm⁻¹), amide II band (between 1510 and 1580 cm⁻¹), amide III band (between 1300 and 1400 cm⁻¹), amide A band (between 3300 and 3500 cm⁻¹). Figure 5A, 5B and 5C shows the Raman spectra recorded from the lyophilised haemoglobin standard, diluted haemoglobin standard and the haemoglobin isolated from blood respectively. The Raman spectra acquired from the lyophilised haemoglobin standard gave a fluorescence signal because of the bright red colour of haemoglobin. However, the fluorescence signal was not observed in Raman spectra from diluted and isolated haemoglobin. This might be due to the reduction of red colour of haemoglobin by diluting with deionised water. The Raman spectrum from diluted haemoglobin and isolated haemoglobin contains protein related bands at 750 cm⁻¹, 1002 cm⁻¹, 1035 cm⁻¹, 1125-1150 cm⁻¹, 1210 cm⁻¹ (phenylalanine), 1170 cm⁻¹ (tyrosine), 1035 cm⁻¹, 1230 cm⁻¹ -1300 cm⁻¹ (Amide III), 1480 cm⁻¹ - 1580 cm⁻¹ (Amide III), and 1600 -1660 cm⁻¹ (phenylalanine, tyrosine, Amide I). These bands are more prominent in diluted haemoglobin compared to isolated haemoglobin from RBC.

3.2. Plasma categorization based on haemolysis

Specimens were categorized according to the haemoglobin concentration into three groups:

- Group 1 (0 0.1g/L), non-haemolysed (n=12);
- Group 2 (0.20 0.50 g/L), mildly haemolysed (n=10);
- Group 3 (0.50 0.93 g/L), moderately haemolysed (n=8).

The results were analysed to determine if non-haemolysed, mildly haemolysed and moderately haemolysed samples had a significant impact on the analyte concentrations estimated by CLS fitting analysis. The median free haemoglobin concentrations for groups 1, 2 and 3 were measured as 0.02, 0.44 and 0.71 g/L respectively. At free haemoglobin concentration of 0.2 g/L, haemolysis was visible by the light red colour of the plasma. The haemolysed plasma samples appeared to be more turbid compared to non-haemolysed plasma samples. The increase in turbidity in haemolysed samples may be due to hyperlipidemia. It has been reported that hyperlipidemia is associated with increased haemolysis [32]. It is postulated that enhanced lipid concentration changes the lipid content of the erythrocyte membrane, resulting in increased erythrocyte fragility and subsequent leakage of cellular content into the plasma [32].

3.3. Comparison of spectral features of non-haemolysed and haemolysed plasma samples

Figure 6 shows the mean FTIR spectra of non-haemolysed and haemolysed plasma obtained from the prostate cancer patients. To explain the differences between each group, difference spectra were computed by subtracting the spectra of haemolysed plasma samples from the spectra of non-haemolysed plasma samples. The first panel in Figure 7 shows the difference FTIR spectra obtained from moderately haemolysed and mildly haemolysed plasma samples. The second panel shows the difference FTIR spectra obtained from mildly haemolysed and non-haemolysed plasma samples and the third panel shows the difference FTIR spectra obtained from moderately haemolysed plasma samples.

Major differences were observed in the region around 1550 cm⁻¹ (Amide II) [20], 1660 cm⁻¹ (Amide I) [20], 1740-1760 cm⁻¹ (stretching vibrations of (C=O) of fatty acids, triglycerides, and

cholesterol esters) [33], 2800-2950 cm⁻¹ (stretching vibrations of (CH₂/CH₃) of lipids fatty acids, triglycerides and proteins) [33], 3300 cm⁻¹ (Amide A) [20] and 3400-3600 cm⁻¹ (OH stretch) [34] between non-haemolysed and haemolysed plasma groups. The increase in fatty acids (1740-1760 cm⁻¹), lipids (2800-2960 cm⁻¹) and OH stretch (3400-3600 cm⁻¹) and the decrease in glycogen, nucleic acids (1000-1100 cm⁻¹) [33,35], amide II (1550 cm⁻¹), amide I (1660 cm⁻¹) and amide A (3300 cm⁻¹) were observed with an increase in haemolysis. The decrease in amide II, amide I and amide A suggests the decrease in protein content with an increase in haemolysis and the increase in fatty acids, lipids and OH stretch suggest the increase in lipids with an increase in haemolysis. The increase in haemolysis [32]. As mentioned earlier, the haemolysed plasma samples may indicate in-vivo haemolysis [32]. As mentioned earlier, the haemolysed plasma specimens appeared to be more turbid compared to non-haemolysed plasma samples due to hyperlipidemia. The increase in lipid concentration with an increase in haemolysis has also been reported previously [32].

Figure 8 shows the mean Raman spectra of non-haemolysed and haemolysed plasma obtained from the prostate cancer patients. The first panel in Figure 9 shows the difference Raman spectra obtained from moderately haemolysed and mildly haemolysed plasma samples. The second panel shows the difference Raman spectra obtained from mildly haemolysed and non-haemolysed plasma samples and the third panel shows the difference Raman spectra obtained from moderately haemolysed and non-haemolysed plasma samples and non-haemolysed plasma samples. Major intensity related differences were observed in the region around 877 cm⁻¹, 881 cm⁻¹, 1006 cm⁻¹, 1085 cm⁻¹, 1210 cm⁻¹, 1270 cm⁻¹, 1302 cm⁻¹, 1345 cm⁻¹, 1450 cm⁻¹, 1528 cm⁻¹, and 1660 cm⁻¹. The bands corresponding to phenylalanine (1006 cm⁻¹ and 1210 cm⁻¹) [36] increased with increase in haemolysed plasma compared to haemolysed plasma. The CH₂ deformation (1340 cm⁻¹) [37] bands were decreased with increase in haemolysis. The bands corresponding to cholesterol (881cm⁻¹ and 1450 cm⁻¹) [38] and triglycerides (877 cm⁻¹, 1270 cm⁻¹ and 1450 cm⁻¹) [38] were increased with increase in haemolysis. This increase in lipid profile with an increase in haemolysis was also observed in the FTIR spectral analysis.

3.4. Multivariate analysis

3.4.1. PCA

PCA was performed on second derivative of the mean FTIR spectra by patient, using the wavenumber range of 4000-800 cm⁻¹. PCA was carried out with 10 PCs and the first 2 PCs accounted for \sim 91% of the total percentage variance. The first two PCs were used to visualize the classification between the groups. The scatter plot revealed three well differentiated clusters between the analysed groups (Figure 10A).

The PCA analysis showed clear discrimination between the FTIR spectra of non, mildly and moderately haemolysed plasma samples. PC1 showed the discrimination between the FTIR spectra of non and mild haemolysed plasma samples and moderate haemolysed plasma samples. PC1 shows positive band associated with proteins (1657 cm⁻¹) in the moderately haemolysed plasma group and negative bands associated with glycogen, nucleic acids (1040 cm⁻¹, 1063 cm⁻¹, 1090 cm⁻¹ ¹ and 1120 cm⁻¹), lipids, triglycerides and fatty acids (1744 cm⁻¹, 2853 cm⁻¹, 2926 cm⁻¹ and 2963 cm⁻¹) in the non and mildly haemolysed plasma groups. PC2 showed the discrimination between the FTIR spectra of non-haemolysed and mild haemolysed plasma samples. PC2 shows positive bands at 1040 cm⁻¹, 1120 cm⁻¹ and 1640 cm⁻¹ in the mildly haemolysed plasma group and negative bands at 1744 cm⁻¹, 2853 cm⁻¹, 2926 cm⁻¹ and 2963 cm⁻¹ in the non-haemolysed plasma group. The positive bands in PC2 are assigned to glycogen, RNA and protein and negative bands are assigned to lipids, triglycerides and fatty acids. The PCA analysis showed the main discriminating features between non-haemolysed and haemolysed plasma samples are related to glycogen, nucleic acids, proteins, fatty acids, triglycerides and lipids. The FTIR difference spectrum analysis also showed similar discriminating spectral features between the non-haemolysed, mild and moderate haemolysed plasma samples.

Figure 11 shows the results of PCA analysis performed on the vector normalised Raman spectra of non-haemolysed and haemolysed plasma groups. The first two PCs accounted for ~58% of the total percentage variance and the scatter plot revealed overlapped clusters between the analysed groups. Only PC1 showed the discrimination between the Raman spectra of non and mild haemolysed plasma samples and moderate haemolysed plasma samples. PC1 has positive bands at 1003 cm⁻¹, 1080 cm⁻¹, 1155 cm⁻¹, 1430 cm⁻¹ and 1650 cm⁻¹ in the non and mildly haemolysed

plasma groups and negative bands at 1007 cm⁻¹, 1210 cm⁻¹, 1260 cm⁻¹, 1346 cm⁻¹ 1460 cm⁻¹ and 1660 cm⁻¹ in the moderately haemolysed plasma group. The positive bands assigned to proteins, amino acids, carotenoids and lipids, and negative bands related to amino acids, proteins and lipids. The PCA showed proteins and lipids are the major discriminating features between the Raman spectra of plasma from non and mildly haemolysed versus moderately haemolysed patient groups. Similar discriminating features were also observed in the difference spectrum analysis of Raman spectra from non-haemolysed and haemolysed plasma groups.

3.4.2. CLS fitting analysis

CLS fitting analysis was performed to examine the alterations in the weighting of analytes in Raman and FTIR spectra with variable haemolysis. Significance testing was performed on the identified plasma analytes using two-tailed students t-tests with the significance level of $p \leq 0.05$, 0.01 and 0.001. Figure 12 shows the results of CLS fitting analysis performed on the nonhaemolysed and haemolysed plasma second derivative FTIR spectra. In particular a differentiation in the weighting of albumin, phosphatidyl-ethanolamine (p-ethanolamine), uric acid, ceramide, thymidine, ubiquitin, triglyceride, Interleukin-6 and Interleukin-8 were observed between the FTIR spectra of non-haemolysed and haemolysed plasma samples. An increase in the weighting of albumin, ceramide, uric acid and ubiquitin was observed with an increase in haemolysis. Conversely a decreased weighting of thymidine and interleukin-6 was observed with increase in haemolysis. Similarly, a decreased weighting of triglyceride was observed in the haemolysed samples compared to non-haemolysed plasma samples. The increase in ceramide and pethanolamine suggests an increase in lipid concentration with increase in haemolysis. An increased concentration of albumin [13] and ubiquitin [39] with an increase in haemolysis has also been reported previously.

Figure 13 shows the results of CLS fitting analysis performed on the Raman spectra from nonhaemolysed and haemolysed plasma. Significant differences were observed in the weighting of uric acid, albumin, insulin, p-ethanolamine, creatinine, interleukin-6, RNA, urea and thymidine. A decreased weighting for uric acid and urea was observed with increase in haemolysis. A decreased concentration of uric acid with increase in haemolysis has also been reported previously [21] and may arise from a premature decomposition of haemoglobin [21]. Conversely an increased weighting of RNA and Interleukin-6 was observed with increase in haemolysis. Kirschner *et al.* reported an increase in the micro RNA levels in haemolysed plasma specimens [23]. The weighting of insulin within Raman spectra was decreased in mildly haemolysed samples and increased in moderately haemolysed plasma samples. The weighting of albumin and creatinine was decreased in moderately haemolysed samples compared to non and mildly haemolysed plasma samples.

Variations in the weighting of albumin, uric acid, p-ethanolamine, interleukin-6 and thymidine were observed in both FTIR and Raman spectra of non-haemolysed and haemolysed plasma samples. Increased weighting of p-ethanolamine was observed in both FTIR and Raman spectral analysis. The FTIR spectral analysis showed an increased weighting of albumin with an increase in haemolysis but a slightly decreased level of albumin was observed in the Raman spectra of the moderately haemolysed plasma samples. A decreased weighting of uric acid, thymidine and interleukin-6 was observed in the FTIR spectral analysis with an increase in haemolysis. Conversely, an increased weighting of uric acid, thymidine and interleukin-6 levels were observed in the Raman spectral analysis. The differences in the CLS fitting analysis results of FTIR and Raman spectra may be due to the employment of different pre-processing and sample preparation methods. Second derivative FTIR spectra were used in this analysis, second derivative spectra allow more distinct identification of small and adjacent lying absorption peaks which are not clearly visible in the original spectrum. The FTIR spectra were recorded from diluted and dried plasma samples and Raman spectra were recorded from liquid plasma samples. Differences in the sample preparation methods might also affect the identification of plasma analytes. However, further studies would be required to confirm the variation in plasma analytes due to the different sample preparation methods.

4. Interpatient variability

The above studies were carried out on plasma samples obtained from various prostate cancer patients. To avoid any interpatient variability, plasma from a healthy control subject was spiked with increasing concentrations of diluted haemoglobin (extracted from whole blood), 0.44 g/L (mildly haemolysed), 0.93 g/L (moderately-haemolysed) and 1.31g/L (grossly-haemolysed). Figure 14 shows the mean spectra of non-haemolysed and in-vitro haemolysed plasma samples. Intensity related differences were observed across the spectra in the analysed plasma groups. A decrease in the bands around 1007 cm⁻¹, 1450 cm⁻¹ and 1660 cm⁻¹ were observed with an increase

in in-vitro haemolysis. These spectral features were increased with an increase in haemolysis in the Raman spectra of plasma from prostate cancer patients and could originate in in-vivo haemolysis or interpatient variability. Figure 15 shows the PCA scatter plot for non-haemolysed and in-vitro spiked-haemolysed plasma samples. The first two PC's accounted for $\sim 25\%$ of the total percentage variance and the scatter plot revealed overlapped clusters between the analysed groups. This suggests that there are no significant discriminating spectral features between the non-haemolysed and in-vitro haemolysed plasma specimens.

The CLS fitting analysis performed on the in-vitro haemolysed plasma samples showed differences in the weighting of uric acid, albumin, insulin, p-ethanolamine, Interleukin-6, RNA, urea and thymidine (Figure 16). A decrease in insulin concentration was observed with an increase in haemolysis. This might be attributable to the previously observed release of proteolytic enzymes during hemolysis that destroys small peptides such as insulin, gastrin etc [22]. However, this trend was not observed in prostate cancer plasma samples. The increased concentration of urea in haemolysed samples was reported previously [40] and this effect might be due to the cellular release of urea into plasma during haemolysis [40]. However, in this study, the concentration of urea was increased gradually from non-haemolysed through mildly haemolysed up to moderately haemolysed samples and then decreased in grossly haemolysed plasma samples. Conversely, a decreased weighting of urea was observed in prostate cancer plasma samples with an increase in haemolysis. The decreased levels of uric acid [13], creatinine [13], insulin [22] and increased levels of urea [40], micro RNA [23] and interleukins [41] were reported with an increase in haemolysis. Similar trends were observed in this study up to moderately haemolysed samples but a deviation in this trend was observed in grossly haemolysed samples. This might be due to dilution or to interference from the bright red colour of haemoglobin as more haemoglobin was added to the plasma to produce the grossly haemolysed plasma sample. This results in dilution and alteration of analytes present in the plasma sample. Previous studies have also reported variations in severely haemolysed plasma samples due to dilution [13, 40].

The weighting of uric acid, Interleukin-6 and RNA were consistent in both in-vitro haemolysed and prostate cancer plasma samples and the weighting of urea, insulin, p-ethanolamine, thymidine and creatine were inconsistent between the in-vitro and prostate cancer plasma samples. Consistent weighting of pure components in in-vitro haemolysed samples and prostate cancer haemolysed plasma samples suggests the interference of haemoglobin colour and intercellular components of RBC in the weighing of plasma analytes. Inconsistent weighting of pure components in in-vitro haemolysed and prostate cancer haemolysed plasma samples might be due to in-vivo haemolysis or due to the development of cancer.

5. Conclusions

Haemolysis, in-vitro or in-vivo, can affect the concentration of analytes present in the blood plasma and serum. Haemolysis can interfere in the quantification of several analytes in three different ways. The first one is the interference of the red coloration of haemoglobin with the absorption of light as it passes through a sample. The second interference is by releasing analytes into the serum or plasma that are in high concentration within the red blood cells and the third interference is by increasing lipid and fatty acid concentration in in-vivo haemolysis. Many studies have reported the interference of haemoglobin in various biochemical assays, including UV-visible spectroscopy. This study aimed to investigate the changes in the IR and Raman spectra of nonhaemolysed and haemolysed plasma samples. The mean spectra showed more changes in the FTIR spectral features of non-haemolysed and haemolysed patient plasma groups compared to the Raman spectral features. The increased haemolysis with an increase in the lipid content suggests an in-vivo haemolysis in the prostate cancer plasma samples. The PCA analysis performed on FTIR spectra showed a good separation of the plasma groups compared to the PCA performed on Raman spectra. This suggest that FTIR spectroscopy is a preferred method for the analysis of haemolysed samples. Finally, the CLS fitting analysis suggested significant alterations in the weighing of analytes in FTIR and Raman spectra of non-haemolysed and haemolysed patient plasma groups. The Raman spectroscopy study on in-vitro haemolysed samples showed minor changes in the spectral features of non-haemolysed and haemolysed plasma specimens and CLS fitting analysis showed similar changes in the weighting of some pure components as observed in the Raman spectra of plasma from prostate cancer patients.

This study suggests that the FTIR spectra show more significant changes in the spectral features and in the weighting of pure components due to haemolysis compared to the Raman spectra. However, further FTIR studies should be performed on in-vitro haemolysed samples to confirm these results. Both in-vitro and in-vivo haemolysis is a common phenomenon and rejecting these samples could limit the diagnostic performance of Raman and FTIR spectroscopy. However, when including haemolysed samples in clinical spectroscopy studies, it is important to consider any changes in FTIR and Raman spectral features due to haemolysis when comparing results within and between experiments. Differences in the spectral features due to haemolysis will be observed within the patient group but most likely, these differences will be minor when compared between patient groups, for example control and cancer cases. However, further studies are needed to confirm this.

This is the first study to report the effect of haemolysis on infrared and Raman spectra of blood plasma. This study was performed on a limited sample set and validation of these results on a larger cohort will be necessary to confirm the effect of in-vitro and in-vivo haemolysis on FTIR and Raman spectra of blood plasma. Future work should also involve biological assays showing proteins, lipids, circulating nucleic acids and other analyte levels to corroborate the findings of the CLS fitting analysis.

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Tables

 Table 1: Factors causing in vitro haemolysis [2].

During specimen collection	After Specimen collection		
Strong aspiration while puncturing superficial	Vigorous shaking of collected sample		
veins			
Aspiration with large needles causes higher	Centrifugation of sample before completion of		
haemolysis because of an increase in the flow-	coagulation		
rate, flow speed and turbulence.			
Partial blockage of a venous or arterial catheter	Centrifugation of partially coagulated samples		
causes strong aspiration of the sample collected	from patients on anticoagulants		
with a syringe.			
Specimen collection and subsequent splitting	Positive or negative pressure in sample		
into multiple tubes with a syringe.	collection tube		
	Dilution of blood with hypotonic solutions		
	Freeze thawing of whole blood		
	Storage or transportation of collected specimen		
	over several days at ambient temperatures		

	Non-haemolysed	Mildly-haemolysed	Moderately-haemolysed
Number of subjects	12	10	08
Sex	М	М	М
Age (Years)			
Mean	70.4	67.1	74.1
Median	69.5	67	74
Range	58 - 79	58 - 76	70 - 79
PSA (ng/ml)			
Mean	14.38	17.9	13.7
Median	10.95	7.57	9.8
Range	1.55 - 40.04	4 - 62	6.8 - 26.5
T stage			
T2	04 (33.3%)	03 (30%)	01 (12.5%)
Т3	08 (66.6%)	07 (70%)	07 (87.5%)
Gleason score	<u> </u>	X /	
7	04 (33.3%)	04 (40%)	04 (50%)
8	06 (50%)	04 (40%)	02 (25%)
9	02 (16.6%)	02 (20%)	02 (25%)

Table 2: Clinical characteristics of prostate cancer patients used in the study.

Category	Pure components	
Protein and related compounds	Apolipoprotein E4, Albumin, Haemoglobin Interleukin-6, Interleukin-8 and Ubiquitin	
	Arachidonic acid, Cholesterol, Ceramide	
Lipids and Fatty acids	Linolenic acid, Linoleic acid,	
	Oleic acid, Triglyceride, polyunsaturated fatty acid (PUFA),	
	Sphingomyelin,	
	phosphatidylcholine, phosphatidylethanolamine,	
	phosphatidylserine, prostaglandin E1,	
	phosphatidylinositol	
Nucleic acids and related compounds	DNA, RNA, Thymidine	
Metabolism and others	Glucose, Glycogen, Creatinine, Uric acid, Urea, Insulin and β-carotene	

 Table 3: Pure molecular reference species used in haemolysis study

Figures



Figure 1: Mean and standard deviation of instrument response corrected and pre-processed liquid plasma Raman spectrum.



Figure 2: Three different types of liquid plasma samples in plasma biobank.



Figure 3: UV-VIS absorption spectrum of oxyhaemoglobin



Figure 4: Mean and standard deviation of FTIR absorption spectrum of haemoglobin.



Figure 5: Mean and standard deviation Raman spectrum of (A) haemoglobin standard (B) diluted haemoglobin standard and (C) haemoglobin isolated from blood.

B.



Figure 6: Mean FTIR spectra of non-haemolysed, mildly haemolysed and moderately haemolysed plasma samples.



Figure 7: Difference FTIR spectra of non-haemolysed and haemolysed plasma groups. Difference spectra were computed by subtracting the mean FTIR spectra of haemolysed plasma from the mean FTIR spectra of non-haemolysed spectra.



Figure 8: Mean Raman spectra of non-haemolysed, mildly-haemolysed and moderately-haemolysed plasma samples.



Figure 9: Difference Raman spectra of non-haemolysed and haemolysed plasma groups. Difference spectra were computed by subtracting the mean Raman spectra of haemolysed plasma from the mean Raman spectra of non-haemolysed spectra.



Figure 10: PCA for FTIR spectra of non-haemolysed, mildly-haemolysed and moderatelyhaemolysed plasma samples. (A) Score plots are shown for patients at non-haemolysed plasma (blue), mildly-hemolysed plasma (red), and moderately-hemolysed plasma (yellow (B) PC-1 and PC-2 loading plots for regions 800 - 1800 cm⁻¹ and 2800 - 3100 cm⁻¹. Covariance ellipse (95% confidence) are shown for each class.







Figure 11: PCA for Raman spectra of non-haemolysed, mildly-haemolysed and moderatelyhaemolysed plasma samples. (A) Score plots are shown for patients at non-haemolysed plasma (blue), mildly-hemolysed plasma (red), and moderately-hemolysed plasma (yellow (B) PC-1 and PC-2 loading plots for regions 600 – 1800 cm⁻¹. Covariance ellipse (95% confidence) are shown for each class.

A.



Figure 12: Relative concentrations of pure molecular reference species from least squares fit of FTIR spectra of non-haemolysed and haemolysed prostate cancer plasma samples. Error bars represent the standard error. Significance shown by (*, **, and ***) indicates the significance of $p \le 0.05$, $p \le 0.01$ and $p \le 0.001$ respectively.



Figure 13: Relative concentrations of pure molecular reference species from least squares fit of Raman spectra of non-haemolysed and haemolysed prostate cancer plasma samples. Error bars represent the standard error. Significance shown by (*, **, and ***) indicates the significance of $p \le 0.05$, $p \le 0.01$ and $p \le 0.001$ respectively.



Figure 14: Mean Raman spectra of non-haemolysed and in vitro haemolysed plasma samples.



Figure 15: PCA scatter plot for Raman spectra of non-haemolysed and in vitro haemolysed plasma samples. Covariance ellipse (95% confidence) are shown for each class.



Figure 16: Relative concentrations of pure molecular reference species from least squares fit of Raman spectra of non-haemolysed and in vitro haemolysed plasma samples. Error bars represent the standard error. Significance shown by (*, **, and ***) indicates the significance of $p \le 0.05$, $p \le 0.01$ and $p \le 0.001$ respectively.

Supplementary material

 Table S1: Details of pure molecular reference species used in this study.

SN	Component name	Company	Product number	State		
Protein and related species						
1	Albumin	Sigma Aldrich	A7030	Powder		
2	Haemoglobin	Sigma Aldrich	H7379	Powder		
3	Interleukin-6	Sigma Aldrich	I13965	Powder		
4	Interleukin-8	Sigma Aldrich	I-1645	Powder		
5	Ubiquitin	Sigma Aldrich	U6253	Powder		
6	Apolipoprotein E4	Sigma Aldrich	A3234	Powder		
Nucleic acids and nucleobases						
7	RNA	Sigma Aldrich	R6750	Powder		
8	DNA	Sigma Aldrich	D-1626	Powder		
9	Thymidine	Sigma Aldrich	T1895	Powder		
Lipids, fatty acids and related species						
10	Ceramide	Sigma Aldrich	22244	Powder		
11	Cholesterol	Sigma Aldrich	C3045	Powder		
12	Linoleic acid	Sigma Aldrich	L1376	Liquid		
13	Linolenic acid	Sigma Aldrich	L2376	Liquid		
14	Oleic acid	Sigma Aldrich	O1008	Liquid		
15	L-a-Phosphatidylcholine	Sigma Aldrich	L4129	Powder		
16	L-a-Phosphatidylserine	Avanti	8703363C	Liquid		
17	L-α-Phosphatidylinositol	Sigma Aldrich	P-6636	Powder		
18	L-α-Phosphatidylethanolamine	Sigma Aldrich	P-7693	Powder		
19	Prostaglandin E1	Sigma Aldrich	P5515	Liquid		
20	PUFA	SUPELCO	47015-U	Liquid		
21	Sphingomyelin	Sigma Aldrich	S0756	Powder		
22	Triglyceride mixture	Sigma Aldrich	17811-1AMP	Powder		
23	Arachidonic acid	Sigma Aldrich	10931	Liquid		

Other metabolites						
24	β-Carotene	Sigma Aldrich	C4582	Powder		
25	Urea	Sigma Aldrich	U4884	Powder		
26	Uric acid	Sigma Aldrich	U2625	Powder		
27	Creatinine	Sigma Aldrich	C4255	Powder		
28	Glucose	Sigma Aldrich	G8270	Powder		
29	Glycogen	Sigma Aldrich	G0885	Powder		
30	Insulin	Sigma Aldrich	12643	Powder		





Figure S1: Raman spectrum of pure molecular reference species.











Figure S2: FTIR spectrum of pure molecular reference species.











Wavenumber (cm⁻¹)

