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To the Graduate Council:

I am submitting herewith a thesis written by Robbie Alhakeem entitled "Determination of the bremsstrahlung spectra of a clinical linear accelerator using a Simpson iteration technique." I have examined the final electronic copy of this thesis for form and content and recommend that it be accepted in partial fulfillment of the requirements for the degree of Master of Science, with a major in Nuclear Engineering.

Laurence Miller, Major Professor

We have read this thesis and recommend its acceptance:

Accepted for the Council: Carolyn R. Hodges

Vice Provost and Dean of the Graduate School

(Original signatures are on file with official student records.)

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Laurence I Miller

Dr. Laurence Miller, Major Professor

We have read this thesis and Recommend its acceptance:

trian Oliver

Accepted for the Council:

Vice Provost and Dean of Graduate Studies

Determination of the Bremsstrahlung Spectra of a Clinical Linear Accelerator using a Simpson Iteration Technique

A Thesis Presented for the Master of Science Degree at The University of Tennessee, Knoxville

> Robbie Alhakeem December 2002



Abstract

X-ray spectral reconstruction from x-ray transmission data was investigated using graphite as an attenuating material which has a monotonic declining mass attenuation coefficient for energies up to 30 MeV, and by employing the numerical method for unfolding spectra. No experimental investigation of energies above 10 MeV using this technique has been performed prior to this research. Previous works utilizing this method have used material such as lead and aluminum which exhibit an increase in attenuation coefficients in the 8 to 10 MeV range and beyond. This increased attenuation leads the Simpson technique to produce a number of non-unique fractional fluencies representing dual energies. Photon energy spectra for 6 MV and 18 MV beams produced by Varian 6100 and Varian 2100C linear accelerators were determined to validate the consistency of the measured data and the modeling method. The resulting Simpson unfolded spectra were compared to the published 6 MV Mohan spectrum and an interpolated 18MV spectrum. Both spectra are Monte Carlo based and used in the ADAC Laboratories three dimensional Pinnacle treatment planning system (3DPRTP). Modal energies for the Simpson technique were determined and compared to the modal energies for the Mohan spectrum and the interpolated 18 MV spectrum. Our method's modal energies for the 6MV beams were similar to the Mohan 6MV spectrum. The modal energies for this work are 0.73 MeV for 2100-6 MV beam and 0.84 MeV

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for the 6100. For the 2100-18 MV beam, the modal energy for the determined Simpson spectrum was approximately 4.2 MeV. The Pinnacle (ADAC 3DPRTP) interpolated 18 MV spectral model yield a modal energy of 1.0 MeV. All of the above spectra were also compared to a Huang modified Jones-fit Laplace transform generated energy fluence spectra. The Laplace technique produced modal energies of 1 MeV for the 2100-6 MV beam and .7 MeV for the 6100 photon beams. The 2100-18 MV modal energy for the Laplace technique was 2.5 MeV. The relatively large differences in the modal energies for the 18 MV spectra lead the author to compare the results with a fourth spectral model generated by Francois and Catala through a technique of direct resolution of a matrix system of transmission data. The Francois – Catala technique yields a number of modal energies for 15MV to 20 MV beam spectra ranging from 2.76 to 3.58 MeV. These modal energies agree with the Simpson model as opposed to the interpolated 18 MV model. The HVL data also suggests that the modal energy of the beam is substantially larger than 1 MeV. The disagreement of all the above models leads the author to conclude that further work and unification of methodology is needed to verify true photon energy spectra.

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Chapter 1

Introduction

1.1 Rationale for Determining the Energy Spectrum

Chemical and biologic changes in tissue exposed to ionizing radiation depend more on the energy absorbed than on the amount of ionization the radiation produces in air. Dose from ionizing radiation is defined as the amount of energy absorbed from the imparted energy per unit mass to a small volume of the irradiated medium. The modern radiotherapy linear accelerator (Linac) produces several monochromatic electron beams and photon beams. This allows for a range of dose distributions to match the goals of treatment planning. Photon beams in a Linac are produced via bremsstrahlung interactions of the monochromatic electrons with a tungsten target in the treatment head. These interactions produce a spectrum of photon energies ranging from zero up to the energy of the incident electron beam, and the shape of the energy spectrum directly affects dose deposition in a medium. The spectral distribution of photons for each Linac is unique for a specific configuration. The measured photon energy spectrum is dependent on the target, flattening filter, ionization chamber, and bending magnet. Because of slight variations in manufacturer tolerance, the x-ray spectrum from two accelerators of the same design operating at the same monochromatic electron energy may be different.

1.2 Problems and Methods of Determining Clinical Photon Spectra

A reliable method of determining the energy spectrum is desirable especially for three-dimensional (3-D) treatment planning. Direct measurement of the high energy photon beam spectrum using scintillation detectors such as NaI (Tl) or Ge (Li) is difficult due to the high dose rates produced, and the detector low collection efficiency due to the large range in energy of the photons produced. However, measurements have been attempted, using both direct and indirect techniques. One method places a scatterer at an angle with the primary axis and perpendicular to NaI (Tl) detector (Levy et al 1975, Brownridge et al 1984, Landry and Anderson 1991). Monte Carlo calculations have been used also to theoretically determine the energy spectra (Mohan et al 1985, Kan et al 1987, Chaney et al 1994). Monte Carlo techniques are considered the gold standard for simulating the production of the bremsstrahlung spectrum, and the interaction of the photon beam with the beam shaping components in the accelerator head. Computer Programs such as the EGS4, BEAM, and ITS (ETRAN) simulate electromagnetic cascades in various geometries. They have the ability to realistically model radiation transport of photons and electrons in a variety of elements, compounds or mixtures. However, the results of these programs are highly dependent on the level of detailed description of the accelerator head design. A common approach is to separate the model into a series of individual component modules (CMs), each of which operates independently of the other component modules and occupies a slab at right angles with the beam axis. The computer computational times are typically in the range of several hours, today, as compared to 600 hours on a VAX 11/780 (D.W.O Rogers et al 1994).

The time constraint and the specific knowledge of geometrical and material makeup of the head design makes this method rather complicated for routine clinical applications.

Determination of the photon spectrum from measured beam parameters has been studied by several investigators. One approach (Bloch and Mcdonough 1997) is to fit calculated data represented as a percent of the point of maximum dose (PDD) from a monoenergetic beam to a measured PDD from a clinical beam. This data is combined with an electron disequilibrium factor in the buildup region to produce a meaningful spectrum. Measured attenuation data has been used to model the photon spectrum from the keV range to the MeV range. Figure 1 illustrates the mass attenuation coefficient of various elements versus energy. Note that for photon energies from the keV up to the low MeV range the photoelectric effect is dominant. The steep decline in attenuation coefficient versus energy for most materials is beneficial in producing a unique signature for an energy spectrum. In the Compton region, common attenuating material such as lead and aluminum experience an increase in the mass attenuation coefficient starting at the 8 to 10 MeV regions and above. Other attenuating material such as water and carbon exhibit a monoenergetic decline of mass attenuation coefficient to well over the 25 MeV range. The rate of decline with energy plays an important role in the ability to use the material for spectral analysis.

Laplace transforms have been used to unfold photon spectra in the photoelectric and Compton regions (Huang et al 1980, Archer et al, 1982). In this method, the x-ray attenuation curve is fitted to an analytical function containing several parameters. If the model is appropriately chosen, its inverse Laplace transform will generate a unique solution of the original spectrum. This method was applied by Silberstein (Huang et al



Figure 1. Mass Attenuation Coefficient versus Photon Energy for various elements. (Johns and Cunningham. "The Physics of Radiology", 3rd edition 1969)

investigated in this work and others. Figure 2 displays a based on Jones method spectrum and a based on Huang method spectrum 1980) and later improved by Jones (Huang et al 1980), Huang et al (Huang et al 1980) for а 4MV-photon beam. The pair production spectra were not

1.3 Work Objectives

quadrature is developed. This method had been evaluated (Huang et al 1982, Pirametti et In this work an iteration technique that uses the Simpson numerical integration



Figure 2. Relative fractional photon fluence F(E) in percent per MeV as a function of photon energy E for a Varian Clinac-4 determined by Huang et al second order polynomial Laplace model(solid curve) vs. a Jones model(dashed curve). (Huang, Kase, and Bjangard: Spectral characterization 1982.)

al 1989), but no experimental investigation of energies above 10 MeV has been performed to date. This is due to the use of material such as lead and aluminum with a limited useful attenuating range vs. energy. The limitation is due to the fact that the attenuation coefficient of both these materials begin to increase above 10MeV, and this produces a non-unique representation of the beam energies as discussed in the Methods and Materials section. The attenuation material chosen for this work is graphite since it does not suffer from such a limitation and energy spectra for a Varian 6100 and 2100C beams were developed from a Simpson spectral unfolding algorithm. The Varian 2100C is a dual energy photon unit with a 6 MV photon beam (2100-6 MV) and an 18 MV photon beam (2100-18 MV). The spectra obtained were compared to spectra used in a Pinnacle three dimensional treatment planning (P3DRTP)system currently used at the Thompson Cancer Survival Center (TCSC). The P3DRTP system is a product of ADAC. ADAC is a manufacturer of Radiation Therapy and Nuclear Medicine equipment located in Milpitas, California. The P3DRTP spectrum is initially assumed to represent a particular machine and then refined by each radiotherapy department through comparing computed and measured open field depth dose curves and by adjusting the spectrum until the shape of the two curves matches. All of the above spectra were also compared to the Huang Laplace transform generated spectrum described in the previous section.

Chapter 2

Theory

2.1 The Bragg-Gray Cavity Theory

The Bragg-Gray cavity theory may be used to calculate the dose directly from ion chamber measurements in a medium. According to the Bragg-Gray theory (Kahn,1994), ionization produced in a gas filled cavity through inelastic collisions of entering primary (produced by photons) and secondary electrons (produced by primary and subsequent generations of electrons), is directly proportional to the energy absorbed in the surrounding medium. The following assumptions are made: the electrons undergoing these collisions are stopped in the chamber, and the chamber must be small enough not to cause a disruption in the distribution of electrons that would exist in the medium without the cavity. Equation 1 describes the conversion of ionization in the gas filled $\frac{\overline{S}}{\rho}$ absorbed

dose in the medium by application of the Bragg-Gray principle (Kahn, 1994).

$$D_{med} = J_g * \frac{\overline{W}}{e} * \left(\frac{\overline{S}}{\rho}\right)_g^{medium}$$
(1)

 $D_{med} = \text{the absorbed dose in the medium (in the absence of the cavity)} = \text{the ionization charge of one sign produced per unit mass of the cavity gas}$ $<math>\left(\frac{\overline{S}}{\rho}\right)_{g}^{nedium} = \text{a weighted mean ratio of the mass stopping power of the medium}$

to that_of the cavity gas for the electrons crossing the cavity.

 $\frac{\overline{W}}{e}$ = 33.97 J/C. Average energy required per unit charge of ionization produced in air.

The product of $J_g * \frac{W}{e}$ is the energy absorbed per unit mass of the cavity gas. The stopping power is defined as the energy loss by electrons per unit path length in a material (Kahn, 1994). The first assumption in the Bragg-Gray theory is inconsistent with the second when using a practical chamber since the chamber has to be large enough to exceed the range of the secondary electrons so that they would not deposit some of their energy in the medium, and small enough not to perturb the distribution of electrons that would exist when the chamber is not present. Hence, Equation 1 is further modified to include the Spencer – Attix theory (Kahn, 1994), or restriction.

2.2 The Spencer-Attix Theory

In this theory (Kahn, 1994) the secondary electrons are divided into two groups that are separated by a cutoff energy Δ that corresponds to the energy of an electron that can just cross the cavity (10 – 20 keV). Below that energy, an electron is considered "Slow" and is assumed to deposit all its energy at the point of its original generation. Hence, the stopping power is redefined as the restricted mass collision power with Δ as the cutoff energy. Equation 2 is based on the Spencer-Attix theory (Kahn, 1994)

$$D_{med} = J_{g} * \frac{\overline{W}}{e} * \left(\frac{\overline{L}}{\rho}\right)_{g}^{medium}$$
(2)

 $\left(\frac{\overline{L}}{\rho}\right)_{g}^{\text{medium}}$ = Restricted mean mass collision stopping power, averaged over the electron slowing down spectrum in the wall material.

Practical ionization chambers perturb the photon and electron fluence in various ways. Therefore Equation 2 is further modified to Equation 3 to account for these effects:

$$D_{med} = M * N_{gas} * \left(\frac{\overline{L}}{\rho}\right)_{g}^{medium} * P_{ion} * P_{repl} * P_{wall} \qquad (3)$$

- M = Charge collected
- N_{gas} = Dose to the gas per unit charge or electrometer reading.
- P_{ion} = Factor that corrects for ionization recombination losses that occur at the time of beam calibration. It is the inverse of the collection efficiency and has a value of unity or above.
- P_{repl} = Replacement correction which depends upon the type and energy of the radiation, it is the ratio of photon energy fluence at the center of the cavity when the cavity is filled with medium to that when the cavity is filled with air.
- P_{wall} = Correction factor that accounts for the difference between the composition of the chamber wall and the phantom as it pertains to photon beam interactions in the users beam.

2.3 Improvement of Dosimetric Accuracy:

Most dosimetry protocols for verification of dose in comparison to Linac output

(TG21 1984, IPSM 1990, IAEA 1987) utilize a tissue phantom ratio (TPR) at depths of

10cm and 20 cm to estimate the restricted mass collision stopping power (TG21 1984).

Figure 3 illustrates the TPR method of measurement where ionization chamber readings

are taken at two depths while the distance between the source and the ionization chamber

remains constant.



Figure 3. Tissue Phantom Ratio (TPR) method of measurement where ionization chamber readings are taken at two depths while the distance between the source and the ionization chamber remains constant.

The ratio is then correlated with the solid water curve to find the nominal accelerating potential (NAP) and the stopping power, as in Figure 4. (Solid water is a material of equivalent electron density to water. Electron density is the predominant factor in the photon interaction with matter.) The Nominal Accelerating Potential is an agreed upon representation of the average photon beam obtained from a TPR (10 cm depth, and 20 cm depth) versus restricted mass collision stopping power .



Figure 4. Ratio of mean restricted stopping power for several phantom materials to air as function of the ionization ratio and the nominal accelerating potential. (Taken from TG21, 1984)

In Figure 4 the restricted mass collision stopping power corresponds to a general representation of photon spectra where all beams of the same Nominal accelerating energy are considered equal. Of course this is not the case, since the monochromatic energy of the electrons leaving the exit window of the accelerator structure defines the manufacturer-designated energy of the photon beam, which is transformed into a polyenergetic spectrum. Therefore, dosimetric accuracy would be enhanced if the restricted mass collision stopping power were calculated as a weighted sum of the values of monoenergetic beams (Andreo and Nahum 1985).

Chapter 3

Methods and Materials

3.1 The Simpson Iteration Technique

The basic transmission function for the photon beam is $T(x) = \frac{I(x)}{I(0)}$ where I (x)

describes the intensity or signal of the beam after an absorber of thickness x. I (0) is the intensity of the beam without an absorber. Equation 4 describes the transmission function of a polyenergetic beam

$$T(x) = \int_{0}^{E_{max}} e^{\mu(E)x} F(E) dE$$
(4)

Where μ (E) denotes the linear attenuation coefficient at energy E and F (E) is the photon spectrum. According to Huang et al and Pirametti et al, the above equation can be linearly approximated using the Simpson rule to obtain the following:

$$T(x_i) = \frac{\Delta E}{3} * (F_1 e^{-\mu_1 x_i} + 4F_2 e^{-\mu_2 x_i} + 2F_3 e^{-\mu_3 x_i} + 4F_4 e^{-\mu_4 x_i} + \dots + 2F_{(n-2)} e^{-\mu_{(n-2)} x_i} + 4F_{(n-1)} e^{-\mu_{(n-1)} x_i} + F_n e^{-\mu_n x_i})$$
(5)

In Equation 5, n is the total number of energy groups; and is specified to be odd since the Simpson rule requires an odd number of intervals. $\Delta E = \frac{(E_n - E_1)}{(n-1)}$ is the final maximum

energy minus the initial energy divided by the number of intervals represented by n-1.

 $F(j) = F_1, F_2, F_3, F_4 \dots F_n$ are the fractional values of the spectrum in each energy range, and $\mu(j)$ are the attenuation coefficients for photons of energies Ej. Equation 5 may be written as

$$T(x_{i}) = \frac{\Delta E}{3} \sum_{j=1}^{n} A_{ij} F_{j}$$
 (6)

Here
$$A_{ij} = \alpha e^{-\mu_j x_i}$$
 and $\alpha = \begin{cases} 1 & \text{for } j = 1 \text{ and } n \\ 4 & \text{for } j = 2, 4, (n-1) \\ 2 & \text{for } j = 3, 5, (n-2) \end{cases}$ (7)

One method for solving this equation is a nonlinear least square iteration method (NLSIM). The NLSIM approach assumes a starting spectrum G_{J}^{k} , where k denotes the consecutive number of iterations. Thus k = 0 refers to the initial assumed set of fractions F_{j} which make up G_{J}^{k} .

Based on the expected physical shape of a photon spectrum, F_1 through F_n are assumed to rise from F_1 towards a maximum fractional photon fluence and then decrease towards F_n . This maximum fractional photon fluence designates the modal or the most frequently occurring energy in the beam. The transmission factor (C_i^k) is calculated using Equation 5 and compared to T (x_i) using the statistic Chi square (χ^2) (Huang et al 1984).

$$\chi^{2} = \sum_{i=1}^{n} \left(\frac{C_{i}^{k} - T(x_{i})}{\gamma_{i}T(x_{i})} \right)^{2}$$
(8)

where $\gamma_i T(x_i)$ is the estimated uncertainty and it is equal to one fractional standard deviation of the measured transmission value T (x_i).

$$\gamma_{i} = \begin{cases} 0.0015 & \text{for} \quad T \ge .05 \\ 0.0050 & \text{for} \quad T < .05 \end{cases}$$

In our own modified Simpson iteration the following procedure is employed:

- 1. Select a number of equal energy intervals for carbon associated with their respective attenuation coefficients.
- 2. Begin with an initial spectrum designated as spectrum G_0 which translates to an initial set of fractional photon fluencies. (F₁, F₂, F₃, ..., Fn) corresponding to the chosen energies.
- 3. Calculate $F_1 = F_1 \left(\frac{T(x_i)}{C_i^k} \right)$ where T (x_i) is a transmission factor for a chosen length and C_i^k is the Simpson iteration calculated transmission factor.
- 4. Replace G_0 with G_1 which is comprised of (F1', F1, F2, F3... Fn).
- 5. Calculate the transmission factor C_i^k .
- 6. Calculate $\chi^2 = \sum_{i=1}^n \left(\frac{C_i^k T(x_i)}{\gamma_i T(x_i)} \right)^2$.
- 7. If $\chi^2' > \text{or} = \text{to } \chi^2$ undo step 3 and go to step 9.
- 8. If $\chi^2' < \chi^2$, set $\chi^2 = \chi^2$ then go to step 9.
- 9. Set j = j + 1 Repeat 2 through 8 unless if j is > n where n is the total number of fractional photon fluencies. The above part of the iteration is repeated until X^2 is minimized.

No values of F(E) were allowed to be less or equal to zero (Huang et al 1994) in order to obtain a meaningful spectrum with all the factors in Equation 5 larger than zero.

The initial spectrum designated as spectrum G₀ is set to increase towards the modal energy and then decrease. The modal energy or the most frequently occurring energy was designated as the average effective energy which corresponds to a half value layer (HVL) of the transmission data. The HVL is the attenuator thickness in the path of the beam where the signal detected at the collecting chamber is half the original signal. The effective energy is the energy of photons in a monoenergetic beam that is attenuated at the same rate as the heterogeneous photon beam in question. Since the attenuation coefficient curve for a given material is characterized by the slope or linear attenuation coefficient (μ), the effective energy is determined by finding the energy of the monoenergetic photons which have the same (μ) as the given beam. In a heterogeneous beam the 2nd HVL is greater than the first and so on. This is due to the filtering out of the lower energy photons thus resulting in a hardened beam with higher average energy of photons. Each consecutive HVL corresponds to a larger effective energy. In this work we define the modal energy as the average of the effective energies for the 1st, 2nd, and 3rd HVL's.

3.2 The Huang modified Jones Fit Laplace Transform for Resolving Energy Spectra

In this method, an x-ray attenuation data are fitted to an analytical function containing several parameters. If the model is appropriately chosen, its inverse Laplace transform will generate a unique solution that resembles the original spectrum. The modified Jones method developed by Huang et al fits the experimental transmission data T(x) data to the exponential function in Equation 9.

$$T(x) = e^{(-ax+bx^2)}$$
⁽⁹⁾

a and b are positive, the inverse Laplace transform of Equation 9 yields Equation 10, a function assumed to fit the spectrum (P.H. Huang et al 1983)

$$f(\mu) = \left(\frac{1}{2\sqrt{\pi b}}\right) e^{\left[\frac{-(\mu-a)^2}{4b}\right]}$$
(10)

where:

 $f(\mu)$ = Fraction of the total signal produced by photons with attenuation coefficient μ per interval μ in the un-attenuated beam.

 $f(\mu)$ is related to F(E) which is the fraction of signal produced by photons of energy E in the range dE through Equation 11

$$F(E) = -f(\mu)\frac{d\mu}{dE}$$
(11)

3.3 The Pinnacle 3DPRTP Energy Spectrum Model

The Pinnacle 3 DPRTP system contains a number of initial spectra models, which are fine tuned through comparison with the appropriate PDD data .The PDD data can be measured in a Source to Surface Distance geometry (SSD) with the source being 100 cm from the surface of a water phantom (Khan , F.M. 1994). The dose is determined using an ionization chamber that is connected to an electrometer. The maximum dose occurs at the depth of maximum buildup. The equations for determining the electron contamination in relation to depth, off axis distance, and field size effect are displayed in Figure 5.



Figure 5. Electron contamination in relation to depth off axis distance and the field size effect.

The spectrum is adjusted until the shape of the two curves matches well. Figure 6 is the Profile Statistics window where the matching of the PDD's is performed. The spectrum in Figure 7 is a Mohan 6MeV photon spectrum (Mohan, R. and C. Chui. 1985) obtained through a Monte Carlo modeling and used as an initial spectrum in Pinnacle. It is first adjusted for the $10x10 \text{ cm}^2$ field size until there is a reasonably good match and then repeated for all the other field sizes. A fine tuning sequence automatically adjusts the relative photons per energy to achieve the final spectrum.



Figure 6. ADAC Laboratories Pinnacle screen for measured versus calculated PDD's. The measured PDD's are adjusted as a direct result of fine tuning the spectrum.



Figure 7. The Pinnacle Photon model editor is used to fine tune a published spectrum to represent the measured PDD data for a linear accelerator. The above spectrum is a Mohan Monte Carlo model (Mohan & Chui, 1985)

3.4 Choice Of Attenuation Material

This technique requires material with an attenuation coefficient that monotonically decreases with the increase in energy over the desired range. The LSIM diverges above energies of 4 MeV for lead and 11 MeV for aluminum since the attenuation coefficient of these materials, μ (E), levels off and begins to increase. This results in most unfolding algorithms yielding a non-unique solution. Our unfolding technique relies on attenuation coefficients as unique value for all energies. For example in the case of an 18 MeV photon beam being attenuated through a medium, both lead and aluminum have attenuation coefficients μ (E) which correspond to two different

E₅. energies as seen in Figure 8, where μ (E) would correspond to two energy values E₃ and

monotonically from 0 to 30 MeV. Table 1 and Figure 9 display the mass attenuation range since its linear attenuation coefficient has been experimentally verified to decrease Carbon is more suitable than lead and aluminum for the 12 MeV and above photon beam



of interest. monotonically declining attenuation coefficient with increasing energy in the range the non uniqueness of a solution produced by a material which does not posses a Figure 8. A plot of linear mass attenuation coefficient versus energy demonstrating

Table 1.	Mass atte	nuation co	efficient (μ/ρ) vs. Energy	for Carbon	$(\rho = 2.2)$	gm/cm [°]
Taken fi	rom The Pl	hysics of R	adiation ther	apy, Faiz M	Kahn)		

Energy	μ/ρ	Energy	μ/ρ	Energy	μ/ρ
MeV	(cm ² /g)	MeV	(cm ² /g)	MeV	(cm ² /g)
0.01	2.1600	3.20	0.0346	6.40	0.0241
0.10	0.1490	3.40	0.0341	6.50	0.0240
0.20	0.1220	3.50	0.0336	6.60	0.0238
0.30	0.1060	3.60	0.0331	6.70	0.0237
0.40	0.0953	3.70	0.0325	6.80	0.0236
0.50	0.0870	3.80	0.0320	6.90	0.0234
0.60	0.0805	3.90	0.0315	7.00	0.0232
0.70	0.0756	4.00	0.0305	7.10	0.0230
0.80	0.0707	4.10	0.0302	7.20	0.0228
0.90	0.0671	4.20	0.0298	7.30	0.0227
1.00	0.0635	4.30	0.0295	7.50	0.0224
1.10	0.0611	4.40	0.0291	7.80	0.0221
1.20	0.0588	4.50	0.0288	7.90	0.0219
1.30	0.0564	4.60	0.0285	8.00	0.0216
1.40	0.0541	4.70	0.0281	10.00	0.0196
1.60	0.0502	4.80	0.0278	11.00	0.0193
1.70	0.0487	4.90	0.0274	12.00	0.0191
1.80	0.0473	5.00	0.0271	13.00	0.0188
1.90	0.0458	5.10	0.0269	14.00	0.0186
2.00	0.0443	5.20	0.0266	15.00	0.0170
2.10	0.0434	5.30	0.0264	16.00	0.0169
2.20	0.0426	5.40	0.0261	17.00	0.0168
2.30	0.0417	5.60	0.0257	18.00	0.0166
2.40	0.0408	5.70	0.0254	19.00	0.0165
2.50	0.0400	5.80	0.0252	20.00	0.0158
2.60	0.0391	5.90	0.0249	21.00	0.0157
2.70	0.0382	6.00	0.0247	21.00	0.0156
2.80	0.0373	6.10	0.0245	22.00	0.0155
2.90	0.0365	6.20	0.0244	24.00	0.0153
3.00	0.0356	6.30	0.0243	25.00	0.0151
3.10	0.0351	6.30	0.0243	27.00	0.0149



Figure 9. Mass Attenuation Coefficient for Carbon versus Energy. (Khan, F. M. 1994. "The Physics of Radiation Therapy")

Chapter 4

Setup and Data Acquisition

4.1 Setup

A Varian 6100 single 6 MV photon energy Linac and a Varian 2100C dual photon energy Linac with 6 and 18 MV photon beams were used. Figures 10, 11, 12, and 13 illustrate the setup. The attenuator was comprised of a number of 3x3 cm² graphite slabs 0.8 cm, 2.54 cm, 5.08 cm, 10.16 cm, 20.32 cm, and 40.64 cm in length, placed along the beam centerline at 100-cm SSD. Different combinations of the slabs were used to achieve a wider range of attenuating lengths. Buildup caps were placed on the ionization chambers. The purpose of the buildup cap is to achieve electronic equilibrium in open-air measurements so as to satisfy the Bragg-Gray principle. For the Varian 6100, the ionization chamber with a 6 MV build up cap was placed at distances of 123.5 cm and 184.5 cm from the 100 cm SSD. This was done to observe the effect of scatter due to distance between the attenuator material and the detector. The consistency of the measurements in producing comparable transmission ratios for different slab thickness was observed at both distances. The chamber was placed at 184.5 cm for both the 2100-6 MV and the 2100-18 MV using 6 MV and 18 MV buildup caps, respectively. Secondary blocks were positioned next to the graphite slab to further discriminate against scatter as seen in Figures 10 and 11. The chamber was also surrounded with blocks to further



Figure 10. Experimental setup


Figure 11. 6100Varian setup with the graphite attenuator placed at 100cm SSD with the NEL farmer detector on the opposite side.



Figure 12. NEL 0.6 cm³ farmer chamber detector placed at 184.5 cm from the SSD position. The surrounding Cerrobend blocks are used to minimize scatter contribution to detector readings.



Figure 13. A view alongside the Graphite in the direction of the detector.

reduce the scatter due to scattered radiation (Figure 12). Since the slab is relatively narrow, special care was given to insure the beam is properly aligned through the central axis. A 1x1-cm²-field size at 100 cm SSD producing 1 cGy / MU (MU = monitor unit) beam was centered at the front end of the slab.

4.2 Method of Data Collection and Analysis

Measurements were all taken along the central axis only using a Keithly 616 electrometer and NEL farmer chamber. Open-air measurements were taken as the un-attenuated signal I(0). Subsequent measurements I (x) was taken with different slab thickness where x denotes an attenuator thickness in cm. The average modal attenuation coefficient was determined by plotting transmission T(x) vs. graphite 28 thickness in cm to determine 1^{st} , 2^{nd} , and 3^{rd} HVL's and by averaging the corresponding effective energies. A visual basic program was developed, using the Simpson rule technique outlined in section 3.1 to unfold the spectrum. This program uses attenuation coefficients vs. energy for graphite and combines it with the transmission versus attenuating length data to produce a meaningful energy spectrum. A model that uses 79 energies to define 79 values for the spectrum, associated with F₁ through F₇₉ was chosen. The odd number of energies was picked to satisfy the requirement of the Simpson equation, the number of nodes was picked to give a resolution of more than one fractional photon fluence (F_i) per MeV. The modal energy was predetermined according to the methods described above. The initial values of F₁ through F₇₉ were set to rise towards the energy associated with the modal energy and then decline towards the final energy. Output for the program consists of:

- 1. The Spectrum of the beam.
- 2. The value of the 1st, 2nd and 3rd HVL and the corresponding effective energies along with the average modal energy.
- 3. The value of χ^2 and the spectrum (F₁ through F₇₉).

The unfolded spectra were compared to spectra used in the ADAC Laboratories 3DPRTP system currently used at the Thompson Cancer Survival Center (TCSC). All of the above spectra were also compared to modified Jones fit Laplace transform generated spectra

Chapter 5

Results and Discussion

5.1 Scatter Considerations

The transmission ratio data $\frac{I(x)}{I(0)}$ listed in Table 2 is for a chamber setup at 125.3

cm and 184.5 cm from the attenuator are almost identical for the two sets of 6 MV measurements. Thus, we can conclude that the detector was placed at a distance sufficiently large from the source for its response to be affected with scattered radiation. The setup shown in Figures 10, 11 and 12 was utilized to discriminate against scatter of the beam and leakage which is defined as all radiation originating in the gantry head of the Linac except the useful beam (NCRP REPORT No.49, 1994, Structural Shielding Design And Evaluation For Medical Use of X Rays And Gamma Rays Of Energies Up to

Table 2. Relative electrometer readings for a Varian 6100 6 MV and a Varian 21006 MV photon beam attenuated through graphite taken at distances of 125.3 cm and184.5 cm between the source and the detector.

Graphite Slab Thickness (cm)	6100 6MV I(x)/I(0) Measurement At x=125.3cm	2100 6MV I(x)/I(0) Measurement at x = 184.5cm
2.54	0.8020	0.8027
5.08	0.6586	0.6570
17.78	0.2440	0.2429
38.10	0.0576	0.0572

10 MeV). Leakage measurements were taken behind the beam exit window and at 90 degrees off the beam's central axes at a distance of 1 m from the source. Leakage was well below 0.1% of the useful beam measured along the beam axes at 1 m SSD. Electrometer readings of the primary beam were taken with and without the Cerrobend blocks shown in Figures 11, 12, and 13. These readings were not affected by the removal of the blocks. Nevertheless, the blocks were kept to obtain maximum protection against scatter.

The open-air measurements along with the subsequent attenuation thickness electrometer readings are displayed in Table 3.and Table 4. The two tables contain the corresponding transmission data T (x) for a separation of 184.5 cm between the chamber and the source.

Attenuation thickness(cm)	2100-6MV electrometer readings	6100-6MV electrometer readings	2100-18MV electrometer readings
0.00	2.271	2.036	3.220
0.80	2.043	1.818	3.017
2.54	1.823	1.651	2.780
5.08	1.492	1.417	2.553
7.62	1.206	1.142	2.246
10.16	0.999	0.978	2.010
12.70	0.813	0.816	1.796
17.78	0.552	0.562	1.443
20.32	0.463	0.489	1.298
22.86	0.381	0.412	1.165
25.40	0.320	0.352	1.048
38.10	0.130	0.156	0.677
40.64	0.113	0.137	0.623
43.18	0.094	0.119	0.562
78.74	0.009	0.015	0.147

Table 3. Electrometer readings (nC) for the Varian 6100 6 MV beam and the 2100CD for 6 and 18MV beams.

Table 4. Transmission data $T(x) = \frac{I(x)}{I(0)}$ calculated using the electrometer readings

Attenuation thickness (cm)	T(X),2100-6 MV T(0) = 2.271 nC	T(X) 6100 T(0) = 2.036 nC	T(X)2100-18 MV T(0) = 3.220 nC		
0.80 0.900		0.893	0.937		
2.54	0.803	0.811	0.864		
5.08	0.657	0.696	0.793		
7.62	0.531	0.561	0.700		
10.16	0.440	0.480	0.624		
12.70	12.70 0.358		0.558		
17.78	0.243	0.276	0.448		
20.32	20.32 0.204		0.403		
22.86 0.168		0.202	0.362		
25.40	0.141	0.173	0.326		
38.10	0.057	0.077	0.210		
40.64	0.050	0.067	0.193		
43.18	0.042	0.058	0.175		
78.74	0.004	0.008	0.046		

in Table 3

5.2 Modal Energy Results

The average modal attenuation coefficient was determined by plotting transmission T(x) vs. graphite thickness in cm, then finding the 1st, 2nd, and 3rd HVL's which correspond to effective energies as described in the Methods and Materials chapter. The average modal attenuation coefficients for the three beams and their corresponding energies are displayed in Table 5. Figure 14 is a plot of the transmission T(x) vs. Graphite thickness in cm.

Table 5. Experimentally determined average modal energies for the 6100 Varian and 2100 6 MV and 2100 18 MV photon beams.

Beam	Average Modal Attenuation Coefficient cm ² /g	Corresponding Modal Energy (MeV)		
6100	0.062	0.835		
2100 6 MV	0.075	0.734		
2100-18 MV	0.030	4.177		



Figure 14. Transmission vs. thickness for a Graphite attenuator.



Figure 15. Simpson generated photon energy spectrum for a Varian 2100 6 MV beam. Modal Energy = 0.734 MeV.



Figure 16. Simpson generated energy spectrum for a Varian 6100 6MV beam. Modal Energy = 0.835 MeV

Table 6. Ending minimized Chi square modal energy values for the Simpson generated 6 MV photon spectra.

Beam	χ ²	Modal Energy (MeV))		
6100	54744	0.835		
2100 6 MV	28539	0.759		



Figure 17. Simpson generated photon energy spectra of the 2100-6 MV and 6100-6 MV beams.

5.3 Resulting Spectral Model for 6 MV Beams

The resulting Simpson generated photon spectra for the 6 MV beams are shown in Figure 15, Figure 16, and Table 6.

Figure 17 is a comparative display of the two spectra. The generated spectra of this work were compared to a Mohan spectrum model used in the ADAC 3DPRTP system for the Varian 6100 and the 2100 6MV beams.

Figure 18 shows the Mohan beam spectrum model. All of the above spectra were also compared to their respective Huang modified Jones Laplace transform models. The Laplace models were generated as described in section 3.2. Figures 19 and 20 are the fitted data to equation 9. Table 7 includes the corresponding values for a and b which are used in equations 10 and 11 to generate the Laplace spectra.

Figures 21 and 22 display the Simpson generated spectra for the Varian-6100 and Varian-2100 6 MV beams vs. the Pinnacle spectrum and the Laplace spectra. Table 8 is a comparison of the modal energies for the Simpson models vs. the Pinnacle generated spectra and the modified Jones Laplace spectra. The Huang modified Jones method yielded a modal energy of 1.0 MeV for the 2100-6 MV beam and 0.7 MeV for the 6100-6 MeV beam.

5.4 Resulting Spectral Model for the 18MV Beam

The Simpson modeling technique is capable of generating energy spectral distribution for the 18 MV photon beam. The generated spectral model of this work is compared to the spectral model used in the Pinnacle 3DPRTP.



Figure 18. Pinnacle photon energy spectrum based on a Mohan Monte Carlo model.



Figure 19. Huang modified Jones fit of the 6100 transmission data T(x) to the exponential function in Equation 9, $T(x) = e^{(-\alpha x + bx^2)}$.



Figure 20. Huang modified Jones fit of the 2100 6 MV experimental data T(x) to the exponential function in Equation 9, $T(x) = e^{(-ax+bx^2)}$

Table 7. Fitted values of parameters a and b of equation 9, $T(x) = e^{(-ax+bx^2)}$ to the experimental attenuation data T(x) of the photon beams.

Beam	А	b
2100 6 MV	0.065	0.0003
6100	0.075	0.0004



Figure 21. A comparison of the Simpson generated spectrum Versus the Pinnacle spectrum, and the modified Jones spectrum for the Varian 6100 beam.



Figure 22. A comparison of the Simpson generated spectrum Versus the Pinnacle spectrum, and the Laplace modified Jones spectrum for the 2100-6X beam.

able	8.	A	comparison	of	the	modal	energies	for	the	Simpson	models	vs.	the
Pinnao	cle	gen	erated spect	ra a	ind t	he modi	ified Jone	s La	plac	e spectra.			

Beam	Modal Energy MeV
Pinnacle – Mohan Monte Carlo 6MV	0.800
Simpson 2100 6 MV	0.759
Laplace 2100-6 MV	1.000
Simpson 6100	0.835
Laplace 6100	0.700

.Figures 23 and 24 displays the Simpson generated spectra for the 2100-18 MV beam vs. the Pinnacle spectrum and the Laplace spectrum Table 10 includes the corresponding values for a and b which are used in Equations 10 and 11 which were used to generate the Laplace spectra. The Laplace models were generated as described in section 3.2, figure 25 shows these data fit to Equation 9.

The Pinnacle spectral model yielded a modal Energy of 1.50 MeV, where as the Simpson model experimentally defined modal energy was 4.17 MeV, and Huang modified Jones method yielded a modal energy of 2.50 MeV. The relatively large differences in the modal energies for the 18 MV spectra lead the author to compare the results with a fourth spectral model generated by Francois and Catala through a technique of direct resolution of a matrix system of transmission data (A. Catal et al 1993). The Francois – Catala technique yields a number of modal energies for 15MV to 20 MV beam spectra ranging from 2.76 to 3.58 MeV. These modal energies agree better with the Simpson model than the interpolated 18 MV model. The collected HVL data also suggests that the modal energy of the beam is substantially larger than 1.5 MeV which is the modal energy of the interpolated ADAC 18 MV spectrum.



Figure 23. Energy Spectrum generated using the Simpson technique for the 2100-18 MV beam.



Figure 24. A comparison of the Simpson generated spectrum versus the Pinnacle spectrum and the Laplace transform for the 2100-18 MV beam.

 Table 9. Modal Energy and fractional photon fluence of the modal energy for the

 Pinnacle, Simpson, and Laplace spectrum modeling techniques

Spectrum Type For the 2100-18 MV beam	Modal Energy MeV
Pinnacle 2100-18 MV	1.50
Laplace 2100-18 MV	2.50
Simpson 2100-18 MV	4.17

Table 10. Fitted values of parameters a and b of equation $9, T(x) = e^{(-\alpha x + bx^2)}$ to the experimental attenuation data T(x) of the photon beams.

Beam	A	b	
2100-18 MV	0.04	0.000045	



Figure 25. Huang modified Jones fit of the 2100-18 MV experimental data T(x) to the exponential function in equation 9, $T(x) = e^{(-ax+bx^2)}$.

Chapter 6

Conclusions and Future Work

6.1 Conclusion

In conclusion, the photon spectrum of a high-energy Linac can be measured through the use of a monoenergetically declining attenuation coefficient attenuator. Carbon is a good choice for such material. The attenuation data can be converted to a spectral distribution using spectral unfolding techniques. The resulting Simpson unfolded spectra's were compared to the published 6 MV Mohan spectrum and an interpolated 18MV spectrum. Both spectra's are Monte Carlo based and used in the ADAC Laboratories three dimensional Pinnacle treatment planning system. Modal energies for the Simpson technique were determined and compared to the modal energies for the Mohan spectrum and the interpolated 18 MV spectrum. Our methods modal energies for the 6MV beams were similar to the Mohan 6MV spectrum. All of the above spectra's were also compared to a Huang modified Jones-fit Laplace transform generated energy fluence spectra. The relatively large differences in the modal energies for the 18 MV spectra lead the author to compare the results with a fourth spectral model generated by Francois and Catala through a technique of direct resolution of a matrix system of transmission data. The Francois – Catala technique yields a number of modal energies which agree with the Simpson model as opposed to the interpolated 18 MV model. The HVL data also suggests that the modal energy is closer to the Simpson and Francois – Catala modal energies. The disagreement of all the above models leads the author to

conclude that further work and unification of methodology is needed to verify true photon energy spectra.

6.2 Future Work

In future work we plan to investigate resolving the photon energy spectrum via Monte Carlo calculations. We also hope to resolve the discrepancies that exist in current spectral models and thus, create a proposal for future spectral modeling criteria. References

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Appendices

5

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Appendix A

A Visual Basic Program for the Simpson Iteration Technique



Dim f(500) As Single, T(500) As Single, Aij(200, 200) As Double, Ef As Double Dim Ei As Double, j As Integer, nu(300) As Single, CCOUNT(5000, 5000) As Single Dim EnergyInterval As Integer, I As Integer, e(200) As Single, Alpha As Integer Dim c(200) As Double, X(500) As Single, Xi2 As Single, K As Integer, ci(300) As Single

Dim L As Integer, R As Integer, CHI2 As Single, m As Integer, n As Single, cprime(300), chii(300)

Dim LU As Integer, adjust As Integer, gam As Single, en As Integer, energy As Integer, evenodd As Integer, XI(300, 300) As Single, XIPRIME(300, 300) As Single Dim TestXi(500, 500) As Double

Private Sub Command1_Click() Sum = 0 List2.Clear . List3.Clear List4.Clear List5.Clear List6.Clear chi2square = 0chilsquare = 0For I = 1 To endn X(I) = 0#T(I) = 0#Next I test = 1E+16'NUMBER OF SIMPSON NODES endn = 79'Establish initial and final energies If List1 = "2100-18X" Then Ef = 18# $E_i = 0.01$ End If If List1 = "2100-6X" Or List1 = "6100" Then Ef = 6# $E_i = 0#$ End If ***** '1st energy coefficient represents LOWEST energy component ' establish energies and corresponding attenuation coefficients

'nu is energy attenuation coefficient e is the energy For eS = 1 To endn Step 1 e(eS) = (Ef / endn) * eS $nu(eS) = 0.0603 * (e(eS) ^ -0.438)$

Next eS

' divide the transmission data with a maximum of 79cm graphite into 'endn equal interval e.g 1st cut = largest X(I) ' Plot T(I) vs X(I)

If List1 = "2100-18X" Then For I = 1 To endn

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X(I) = (79 / endn) * I
T(I) = 0.9115 * Exp(-(0.0384 * X(I)))
List4.AddItem T(I)
' Determine nodal energy
'Tnoatten = I(0)
If T(I) \ge (Tnoatten / 2) - 0.015 And T(I) \le (Tnoatten / 2) + 0.015 Then
nodalt = T(I)
nodalx = X(I)
nodalnu = -Log(nodalt) / (2.265 * nodalx)
nodalE = e(nodalx)
End If
If T(I) \ge (Tnoatten / 4) - 0.015 And T(I) \le (Tnoatten / 4) + 0.015 Then
second nodalt = T(I)
second_nodalx = X(I) - nodalx
second_nodalnu = -Log(second_nodalt) / (2.265 * second_nodalx)
second nodalE = e(second nodalx)
End If
If T(I) \ge (\text{Tnoatten} / 8) - 0.015 \text{ And } T(I) \le (\text{Tnoatten} / 8) + 0.015 \text{ Then}
Third_nodalt = T(I)
Third Nodalx = X(I) - (second nodalx) - nodalx
Third_Nodalnu = -Log(Third_nodalt) / (2.265 * Third_Nodalx)
Third_NodalE = e(Third_Nodalx)
End If
Avarage_Nodal_E = (nodalE + second_nodalE + Third_NodalE) / 3
Avarage NodalX = (nodalx + second nodalx + Third Nodalx) / 3
Average_Nodalnu = (nodalnu + second_nodalnu + Third_Nodalnu) / 3
Next I
End If
If List1 = "2100-6X" Then
For I = 1 To endn
X(I) = (79 / endn) * I
T(I) = 0.9332 * Exp(-0.0713 * X(I))
List4.AddItem T(I)
'Tnoatten = I(0)
If T(I) \ge (\text{Tnoatten } / 2) - 0.015 \text{ And } T(I) \le (\text{Tnoatten } / 2) + 0.015 \text{ Then}
nodalt = T(I)
nodalx = X(I)
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nodalnu = -Log(nodalt) / (2.265 * nodalx)
nodalE = e(nodalx)
End If
If T(I) \ge (Tnoatten / 4) - 0.015 And T(I) \le (Tnoatten / 4) + 0.015 Then
second_nodalt = T(I)
second_nodalx = X(I) - nodalx
second_nodalnu = -Log(second_nodalt) / (2.265 * second_nodalx)
second_nodalE = e(second_nodalx)
End If
If T(I) \ge (Tnoatten / 8) - 0.015 And T(I) \le (Tnoatten / 8) + 0.015 Then
Third nodalt = T(I)
Third Nodalx = X(I) - (second nodalx) - nodalx
Third_Nodalnu = -Log(Third_nodalt) / (2.265 * Third_Nodalx)
Third NodalE = e(Third Nodalx)
End If
Avarage Nodal E = (nodalE + second nodalE + Third NodalE) / 3
Avarage_NodalX = (nodalx + second_nodalx + Third_Nodalx) / 3
Average_Nodalnu = (nodalnu + second_nodalnu + Third_Nodalnu) / 3
Next I
End If
If List 1 = "6100" Then
For I = 1 To endn
X(I) = (79 / endn) * I
T(I) = 0.9274 * Exp(-0.063 * X(I))
List4.AddItem T(I)
'Tnoatten = I(0)
If T(I) \ge (Tnoatten / 2) - 0.015 And T(I) \le (Tnoatten / 2) + 0.015 Then
nodalt = T(I)
nodalx = X(I)
nodalnu = -Log(nodalt) / (2.265 * nodalx)
nodalE = e(nodalx)
End If
If T(I) \ge (Tnoatten / 4) - 0.015 And T(I) \le (Tnoatten / 4) + 0.015 Then
second_nodalt = T(I)
second nodalx = X(I) - nodalx
second_nodalnu = -Log(second_nodalt) / (2.265 * second_nodalx)
second_nodalE = e(second_nodalx)
End If
If T(I) \ge (Tnoatten / 8) - 0.015 And T(I) \le (Tnoatten / 8) + 0.015 Then
Third_nodalt = T(I)
Third_Nodalx = X(I) - (second_nodalx) - nodalx
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```
Third_Nodalnu = -Log(Third_nodalt) / (2.265 * Third_Nodalx)

Third_NodalE = e(Third_Nodalx)

End If

Avarage_Nodal_E = (nodalE + second_nodalE + Third_NodalE) / 3

Avarage_NodalX = (nodalx + second_nodalx + Third_Nodalx) / 3

Average_Nodalnu = (nodalnu + second_nodalnu + Third_Nodalnu) / 3

Next I

End If
```

```
******
```

```
chisquare = 3000000000#
K = Avarage_NodalX
TestXi(10, 0.1) = 0\#
'Do While chisquare >= 300000
For mm = K - 1 To K + 1 Step 0.1
For nn = 0.4 To 0.008 Step -0.01
chi2square = 0#
For m = 1 To end Step 1
If List 1 = "2100-18X" Then
n = mm
f(n) = nn
ri = 0.18
End If
If List1 = "2100-6X" Then
n = mm
f(n) = nn
ri = 0.33
End If
If List1 = "6100" Then
n = mm
f(n) = nn
r_{i} = 0.32
End If
If m = n Then
f(m) = f(n)
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End If

If m < n Then

sintheta = f(n) / n

f(m) = (m) * sintheta

End If

If m > n Then

sintheta = f(n) / (endn - n)

f(m) = (endn - m) * sintheta

End If

If m = 1 Or m = endn Then

f(m) = 0.001

End If
```

Next m

'GoTo 800

Sum = 0 chisquare = 0#

test = 1000000000 For I = 1 To endn Step 1

'Begin iteration by establishing curve fits for T(I)

End If

```
'f(j): Fraction of photons of a certain energy represented in beam
'Establish Simpson equation
Sum = 0#
evenodd = 1
For j = 1 To endn Step 1
  DELTAE = (Ef - Ei) / (endn - 1)
       If j = 1 Then
       Alpha = 1
       End If
       If (j = 2 * (evenodd)) Then
       Alpha = 4
       Else
       If (j = 2 * (evenodd) + 1) Then
       evenodd = evenodd + 1
       Alpha = 2
       End If
       End If
       If j = endn Then
       Alpha = 1
       End If
Aij(I, j) = Alpha * Exp(-nu(j) * X(I) * 2.265)
```

'Sums all individual Simpson values Sum = Sum + Aij(I, j) * f(j)

Next j

' calculate C(I)

'Calculate Xi^2 pertinent to this value of I and sum to get Xi^2 for all I

'TRIANGULAR ITERATION

' PREPARE CHISQUARE FOR F1 THROUGH FN ITERATION ' This loop subtracts each individual simpson value and multiplies it by 'T(i)/C(i) then returns it to the equation ci(I) = (DELTAE / 3) * Sum 'For 11 = 1 To ENDN Step 1 'Sum = Sum - Aij(I, 11) * f(11) 'f(11) = f(11) * (T(I) / ci(I)) 'Sum = Sum + Aij(I, 11) * f(11) 'Next 11

' calculate adjusted C(i) ' Calculate adjusted Xi^2 pertinent to this value of I and sum to get Xi^2 for all I

ci(I) = (DELTAE / 3) * Sum

chilsquare = chilsquare + (Abs(ci(I) - T(I)) 2 / (gam * T(I)) 2)

' calculate adjusted C(i) ' Calculate adjusted Xi^2 pertinent to this value of I and sum to get Xi^2 for all I

'NODE by NODE iteration F1 through FN

List6.AddItem chilsquare

For L = 1 To endn Step 1 $XI(L, I) = (Abs(ci(I) - T(I))^2 / (gam * T(I))^2)$ Sum = Sum - Aij(I, L) * f(L) f(L) = f(L) * (T(I) / ci(I))Sum = Sum + Aij(I, L) * f(L)

cprime(I) = (DELTAE / 3) * Sum $XIPRIME(L, I) = (Abs(cprime(I) - T(I)) ^ 2 / (gam * T(I)) ^ 2)$

```
If XIPRIME(L, I) < XI(L, I) Then
chi2square = Abs(chi1square - XI(L, I))
XI(L, I) = XIPRIME(L, I)
ci(I) = cprime(I)
chi2square = chi2square + XI(L, I)
Else
chi2square = Abs(chi1square - XI(L, I))
```

```
Sum = Sum - Aij(I, L) * f(L)

f(L) = f(L) * (ci(I) / T(I))

Sum = Sum + Aij(I, L) * f(L)

ci(I) = (DELTAE / 3) * Sum

XI(L, I) = (Abs(ci(I) - T(I)) ^ 2 / (gam * T(I)) ^ 2)

chi2square = chi2square + XI(L, I)

End If
```

Next L List5.AddItem e(I)

Next I

chi2square = 0

TestXi(mm, nn) = chilsquare If List1 = "2100-18X" Then If TestXi(mm, nn) < 29700 Then ri = nn GoTo 800 End If End If

If List1 = "6100" Then If TestXi(mm, nn) < 55700 Then ri = nn GoTo 800 End If

End If

If List1 = "2100-6X" Then If TestXi(mm, nn) < 30300 Then ri = nn GoTo 800 End If

End If chilsquare = 0# Next nn Next mm

```
800 txti2 = e(second_nodalx)
txtj2 = second_nodalx
Txti3 = e(Third_Nodalx)
Txtj3 = Third_Nodalx
Text1 = 0.0603 * (Avarage_Nodal_E ^ -0.438)
txti = nodalE
txtj = nodalx
txti4 = Avarage_Nodal_E
txtj4 = Avarage_Nodal_E
txtj4 = Avarage_NodalX
For 11 = 1 To endn
List3.AddItem ci(11)
Next 11
```

```
'MSChart1.chartType = VtChChartType2dArea
FNORM = 0#
For s1 = 2 To endn
If f(s1) >= f(s1 - 1) Then
Max = f(s1)
End If
Next s1
```

For 11 = 1 To endn List2.AddItem (fi(11) / Max) * ri Next 11

txtfinal = chilsquare

For s = 1 To endn Step 1 MSChart1.Row = s MSChartl.RowLabel = e(s)MSChartl.Column = 1MSChart l.Data = (f(s) / Max) * riNext s For L = 1 To end Step 1 MSChart2.Row = LMSChart2.RowLabel = e(L)MSChart2.Column = 1 MSChart2.Data = T(L)Next L For L = 1 To end Step 1 MSChart3.Row = LMSChart3.RowLabel = e(L)MSChart3.Column = 1MSChart3.Data = nu(L)Next L For 11 = 1 To end Step 1 MSChart4.Row = 11 MSChart4.RowLabel = X(11)MSChart4.Column = 1MSChart4.Data = T(11)Next 11 'Dim Msg ' Declare variable. 'On Error GoTo ErrorHandler 'Set up error handler. PrintForm 'Print form. 'Exit Sub 'ErrorHandler: ' Msg = "The form can't be printed." 'MsgBox Msg ' Display message. 'Resume Next

End Sub
Appendix B

Pinnacle 3-DPRTP Printouts

Pinnacle ³				ADAC Laborato Milpitas, CA 950	ries US	(408) 321 - 9100
Patient Name: tmp			Date/Time:	Mon Apr 11	4:07:42 20	02
Patient ID:			Comment:			(10.1)
Plan Name:			Institution:			
Trial Name:			Physician/P	hysicist: /		
Revision: R03.P03.D04	4		Planner:			
Machine: 2100C						
Version: 2001-08-14 10:	48:53					
Energy: 6 MV						
Field Size: All Field Sizes						
Too I down 171.						
Incident Fluence						
Incident fluence increase/cm	0.00843402					
Incident Iluence cone radius (Cm)	4.8004					
X (perpendicular to gantry axis) (cr	ny.0259373					
Y (parallel to gantry axis) (cm)	0.0360937			En en en Ca		
Gaussian height (cm)	0.07/069			Energy Sp	ectrum	
Gaussian width (cm)	0.93361			(Energy in Me	V)	
Jaw Banshinssion	0.00393201			Energy MeV	Rel Photon	S
Modifiers				0.10	0.00-	4
				0.20	0.004	4
Modifier scatter factor	0.249999			0.30	0.12	0
Electron Contomination	~			0.40	0.12	0
Electron Containmation				0.50	0.31-	4
On/Off	On			0.60	0.43	D
Max Depth [MAXD] (cm)	3			0.80	0.44	5
EC Surface Dose [ECD, 10x10] (D/	FID 461904			1.00	0.434	1
Depth Coefficient [K] (1/cm)	3.70675			1.25	0.41	3
Off-axis Coefficient [OAC] (1/rad^	2) 0			1.50	0.39	-
DF	0.101538			2.00	0.21	5
	116060.0	1.1		3.00	0.121	
C2 (D/Flu) = 0	1.3205			5.00	0.035	
	1.3203			5.00	0.032	
C3 (1/cm)	0.980383			8.00	0.000)
Spectral Factors						
Off-axis softening factor	12			5		
Modeling Geometry						
Fluence grid resolution (cm)	0.40					
Phantom Size - Lateral (cm)	50.00					
Oberten Sine Death (and)	50.00					10 A

Plan Authorization: _

NOT FOR CLINICAL USE

Pinnacle v6.0i Pg 1 of 1 · PHM

Pinnacle ³	RTP System 6.0i ADAC Laboratories Milpitas, CA 95035	(800) 232 - 2123 (408) 321 - 9100
Patient Name: tmp Da	te/Time: Mon Apr 1 14:07:58	2002
Patient ID: Co	mment:	192
Plan Name: Ins	stitution:	
Trial Name: Ph	vsician/Physicist: /	
Revision: R03 P03 D04 Pla	inner:	
Machine: 2100C		
Version: 2001-08-14 10:48:53		
Energy: ISMV		
Field Sizes All Field Sizes		
Field Size: All Field Sizes		
Incident Fluence		
Incident fluence increase/cm 0.00816823		
Incident fluence cone radius (cm) 24.1393		
X (perpendicular to gantry axis) (cm0.0256252		
Y (narallel to gantry axis) (cm) 0.0365621		
Gaussian height (cm) 0.0652337	Fnergy Spectrum	
Gaussian width (cm) 0.719951		
law transmission 0.00505577	(Energy in MeV)	
	Energy MeV Rel Ph	otons
Modifiers	0.10	0.023
Modifier scatter factor 0.5	0.20	0.023
	0.30	0.031
Electron Contamination	0.40	0.031
	0.50	0.069
On/Ott On	0.60 (0.090
Max Depth [MAXD] (cm) 6	0.80	0.148
EC Sufface Dose [ECD /0x10] (D/F101207532	1.00 (1.109
Depth Coefficient [K] (1/cm) 0.084/03	1.25	1.1/3
	200	181
0.00799	3.00	129
CI (D/El) 0.00077778	4.00	104
C2 (D/Flu) 0.000233378	5.00	070
(1/cm) = 0.000021	6.00-	055
	8.00	.044
Spectral Factors	10.00	.023
	15.00	.008
JII-axis soliciting factor 12	20.00 0	.002
Modeling Geometry	30.00 0	.000
Fluence grid resolution (cm) 0.40		
Phantom Size - Lateral (cm) 50.00		

Plan Authorization: _

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Pinnacle v6.0i Pg 1 of 1 - PHM

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Machine: 2100C Version: (uncommissioned) Energy: 18MV Geometry: SSD = 100 cm Field: 10 X 10

Depth Dose



Dose

Pinnacle ³		RTP System 6.0i	ADAC Laboratories	Milpitas, CA 95035	(800) 232 - 2123	t
Patient Name: tmp	Date/Time: Mon Apr 1 14:07:01 2002		Revision: R03.P03.	D04	Page:	lof
Patient ID:	Comment:		Planner:		Scaling:	Fill
Plan Name:	Physician/Physicist: /		Institution:		NOT FOR	CLINI



Appendix C

Huang modified Jones Laplace Transform Data and Printouts

MV	F(E)	Fnew(E)
0.0	0	0
0.1	3.53139E-07	9 02465E-07
0.2	0 004099139	0 01 7677536
0.3	0.119537716	0.770850695
0.4	0.487893168	4 055979349
0.5	0.859727412	9 126337143
0.6	0 914284831	12.87462313
0.7	1 000804449	14.09296061
0.8	0 696045335	13 34086892
0.9	0.609449929	11 68112364
1.0	0 32344 1599	9.456555218
1.1	0 269878951	7.890528648
1.2	0 217724915	6 365686075
1.3	0 169829537	4 965355097
1.4	0.128080879	3.744737552
1.5	0 058569439	2730602211
1.0	0.047226675	2 201/84 163
1.7	0 03/5/92/9	1 /5200690/
1.0	0.029907755	1.3/5/56/38
2.0	0.010270163	0.815342000
2.0	0.008725413	0.692016510
22	0.007372692	0 584729019
23	0.006201207	0.491819855
24	0.005192042	0411782653
2.5	0.004327245	0 343195289
2.6	0.003590013	0 284725154
2.7	0 002964775	0.235137348
2.8	0.002437243	0.193298575
2.9	0 001 994422	0 158178316
3.0	0 000952352	0 126847651
3.1	0.000842673	0.1 1400875
3.2	0.000744453	0 100720172
3.3	0 000656648	0 088840567
3.4	0 000578288	0.078238908
3.5	0.000508478	0 068794042
3.6	0 000446392	0 060394233
3.7	0 000391271	0 05293668
3.8	0 000342417	0 046327037
3.9	0.000299192	0 040478922
4.0	0 000174008	0 035313434
4.1	0.000158732	0 032213231
4.2	0.000144695	0 029364654
4.3	0.000131808	0 026/49258
4.4	0.000119964	0.02434977
4.6	0.021655.05	0.022130027
4.0	9.921000-00	0.0182003432
4.8	A 18126E.06	0.016601171
4.9	7 42137F.06	0.015061022
5.0	4.748735-05	0.013652503
5.1	4 4289E-05	0 012733094
5.2	4 12918E-05	0 011871385
5.3	3.8484E-05	0.011064136
5.4	3.58546E-05	0 010308187
5.5	3.33932E-05	0 00 9600541
5.6	3.10899E-05	0 008938359
5.7	2 89355E-05	0.00831895
5.8	2.69209E-05	0 007739768
5.9	2.50379E-05	0 007 1984
6.0	1.5034E-05	0.006692567
6.1	1.43403E-05	0.006383752
6.2	1 36766E-05	0 006088301
6.3	1 30417E-05	0 005805681
6.4	1.24345E-05	0 005535375
6.5	1.18539E-05	0 005276888
6.6	1.12987E-05	0 005029739
6.7	1.07679E-05	0.00479347
5.8	1 02606E-05	0 004567635
5.9	9 77 58E-06	0 004351808
7.0	0.001390871	0 004145576



MV	F(E)	Fnew(E)
0.01	0	0
0.10	3 33589E-12	7.11658E-12
0.20	9.21546E-06	3.31756E-05
0.30	0.003438546	0.018510301
0.40	0.05786604	0.401576375
0.50	0.260996505	2.312830566
0.60	0.52587579	6.181723572
0.70	0.880850611	10.35448882
0.80	0.893127205	14.29003528
0.90	1.000229765	16.00367624
1.00	0 661443648	16.14370937
1.10	0.628543186	15.34071504
1.20	0.571038469	13.93721008
1.30	0.496002175	12.10581579
1.40	0.411898079	10.05310566
1.50	0.205084877	7.981681694
1.60	0.173435374	6.749917265
1.70	0.14410136	5.608269142
1.80	0.119221443	4.578103401
1.90	0.09277943	3.660339153
2.00	0.043699345	2.89319799
2.10	0.037675412	2.494372092
2.20	0.032284156	2.13743378
2.30	0.027495981	1.820423545
2.40	0.02327541	1 540992641
2.50	0.019582755	1.296513464
2.60	0.016375652	1.084181128
2.70	0.013610428	0 901104173
2.80	0.011243286	0.744383099
2.90	0.009231305	0.611176086
3.00	0.004416032	0.498751881
3.10	0.003906841	0.441469118
3.20	0.00345265	0.389946387
3.30	0.003043308	0.343714823
3.40	0.002676875	0.302329421
3.50	0.002349628	0.265369711
3.60	0.002058064	0.232440115
3.70	0.001798901	0.203170009
3.80	0.001569078	0.177213542
3.90	0.001365/48	0.15424923
4.00	0.00079085	0.1339/9358
4.10	0.000719114	0 121828449
4.20	0.000592912	0 10044632
4.30	0.000537625	0.09107995
4.40	0.000487038	0.082509992
4.60	0.0004408	0.074676737
4.70	0.00039858	0.067524151
4.80	0.000360068	0.060999735
4.90	0.000324974	0.055054369
5.00	0.000206842	0.049642157
5.10	0.000192164	0.0461194
5.20	0.000178445	0.042826725
5.30	0.000165628	0.039750655
5.40	0.00015366	0.036878388
5.50	0.000142491	0.034197769
5.60	0.0001 32072	0.031697268
5.70	0.000122358	0.029365953
5.80	0.000113306	0.0:27193466
5.90	0.000104875	0.025170002
6.00	6.26627E-05	0.023286281
6.10	5.95777E-05	0.022139848
6.20	5.66336E-05	0.021045777
6.30	5.38245E-05	0.020001895
6.40	5.11449E-05	0.019006105
6.50	4.85892E-05	0.018056391
6.60	4.61524E-05	0.01715081
6.70	4.38292E-05	0.016287488
6.80	4.16149E-05	0.015464627
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12.7	操作员会	0.417326	
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Energ MV	F(E)	Fnew(E)	
0.01	0	0	
0.10	5.613E-138	7.21 E-03	Ē.
0.20	5.544E-78	9.00E-03	1
0.30	1 667E-50	1.00E-02	
0.40	1 854E-35	1.07E-02	8 -
0.50	1.195E-25	1.12E-02	8
0.60	3.948E-19	1.16E-02	
0.70	8.931E-15	1.19E-02	1
0.80	4.081E-11	1.21E-02	
0.90	1 098E-08	1.23E-02	
1.00	9.648E-07	1.25E-C2	
1.10	1 639E-05	1.26E-02	
1.20	2.065E-04	1.27E-02	
1.30	1.927E-03	1.28E-02	
1.40	1.333E-02	1.29E-02	
1.50	4.288E-02	1.30E-02	
1.60	1.026E-01	1.31 E-02	
1.70	2.182E-01	1.31 E-02	
1.80	4.180E-01	1.32E-02	
1.90	6.010E-01	1.32E-02	
2.00	6.083E-01	1.33E-02	
2.10	7.289E-01	1 33E-02	
2.20	8.385E-01	1.34E-02	
2.30	9.262E-01	1.34E-02	
2.40	9.822E-01	1.34E-02	
2.50	1.000E+00	1.34E-02	
2.60	9.776E-01	1.35E-02	
2.70	9.176E-01	1.35E-02	
2.80	8.269E-01	1.35E-02	
2.90	7.154E-01	1.36E-02	
3.00	3.484E-01	1.36E-02	
3.10	3.066E-01	1.36E-02	
3.20	2.661E-01	1.36E-02	
3.40	2.278E-01	1.36E-02	
3.50	1.922E-01	1.36E-02	(*)
3.60	1.600E-01	1.37E-02	
3.70	1.31 3E-01	1.37E-02	
3.80	3.180E-02	1.37E-02	
4.00	3.452E-02	1.37E-02	
4.10	2.893E-02	1.37E-02	
4.20	2.409E-02	1.37E-02	
4.30	1.994E-02	1.37E-02	
4.40	1.640E-02	1.38E-02	
4.50	1.340E-02	1.38E-02	
4.60	1.089E-02	1.38E-02	
4.70	8.788E-03	1.38E-02	
4.80	7.050E-03	1.38E-02	
4.90	5.621E-03	1 38E-02	
5.00	3.144E-03	1.38E-02	
5.10	2.658E-03	1.38E-02	
5.20	2.240E-03	1.38E-02	
5.30	1.881E-03	1.38E-02	
5.40	1.576E-03	1.38E-02	
5.50	1.316E-03	1.38E-02	
5.60	1.095E-03	1.38E-02	
5.70	9.085E-04	1.38E-02	
5.80	7.515E-04	1.38E-02	
5.90	6.197E-04	1.38E-02	
6.00	3.290E-04	1.39E-02	
6.10	2.605E-04	1.39E-02	
6.20	2.319E-04	1.39E-02	
6.30	2.062E-04	1.39E-02	
6.40	1.831E-04	1.39E-02	
6.50	1.625E-04	1.396-02	
6.60	1 440E-04	1.39E-02	
6.70	1.275E-04	1.39E-02	
6.80	3.383E-04	1.39E-02	
7.00	8.616E-05	1.39E-02	
7.10	7.482E-05	1.39E-02	
7.20	6.489E-05	1.39E-02	
7.30	5 621E-05	1.39E-02	
7.40	4.862E-05	1.39E-02	
7.50	4.201 E-05	1.39E-02	
7.60	3.624E-05	1.39E-02	
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8.80	5.697E-06	1.39E-02	\times	2.085
8.90	5.137E-06	1.39E-02		2.07E
9.00	4.629E-06	1.39E-02		2.06E
9.10	4.170E-06	1.39E-02		2.05E
9.20	3.753E-06	1.39E-02		2.04E
9.30	3.377E-06	1.39E-02		2.03E
9.40	3.037E-06	1.39E-02		2.02E
9.50	2.729E-06	1.39E-02		2.01E
9.60	2 452E-05	1.39E-02		2.00E
9.70	2 2015-06	1 39E-02		1 99E
0.00	1.0765.06	1 305.02		1 085
9.00	1.3735-00	1.395.02		1.975
9.90	1.7/12-06	1.392-02		19/2
10.00	8.256E-07	1.39E-02		1.905
10.10	7 797E-07	1.39E-02		1.95E
10.20	7.363E-07	1.39E-02		1.95E
10.30	6.952E-07	1.39E-02		194E
10.40	6.564E-07	1.39E-02		1.94E
10.50	6.196E-07	1.40E-02		1.93E
10.60	5847E-07	1.40E-02		1.93E
10.70	5.518E-07	1.40E-02		1.92E
10.80	5 206E-07	1 40E-02		1.925
10.00	49115.07	1.40E-02		1015
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11.00	4.633E-07	1.40E-02		1.910
11.10	4.369E-07	1,40E-02		1.908
11.20	4.120E-07	1.40E-02		1.90E
11.30	3.884E-07	1.40E-02		1.89E
11.40	3.662E-07	1.40E-02		1 89E
11.50	3.452E-07	1.40E-02		1.88E
11.60	3.253E-07	1.40E-02	- A1	1.88E
11.70	3.065E-07	1.40E-02		1.87E
11.80	2.888E-07	1.40E-02		1.87E
11.90	2 720E-07	1.40E-02		1.86E
12.00	2 562E-07	140E-02		1.86E
12.00	2 41 25.07	1405-02		1.855
12.10	2 3735 07	1.405.02		1.855
12.20	2.2/20-07	1.405.02		1.000
12.30	2.139E-07	1.402-02		1.840
12.40	2.014E-07	1.40E-02		1.846
12.50	1.895E-07	1.40E-02		1.83E
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12.60 12.70 12.80 13.00 13.10 13.20 13.30 13.40 13.50 13.60 13.70 13.80 13.80 13.80 13.90 14.00 14.00	1.679E-07 1.579E-07 1.397E-07 1.397E-07 1.313E-07 1.313E-07 1.335E-07 1.61E-07 1.025E-07 9.638E-08 9.054E-08 8.505E-08 7.503E-08 7.503E-08 7.503E-08 7.503E-08	1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02 1.40E-02		1.82E 1.81E 1.81E 1.80E 1.79E 1.78E 1.77E 1.77E 1.76E 1.76E 1.75E 1.75E
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12.60 12.70 12.80 12.90 13.00 13.20 13.30 13.40 13.50 13.60 13.70 13.80 13.90 14.10 14.20	1.678E-07 1.579E-07 1.397E-07 1.397E-07 1.313E-07 1.235E-07 1.235E-07 1.235E-07 1.025E-07 9.636E-08 9.054E-08 8.503E-08 7.503E-08 7.503E-08 6.614E-08 6.614E-08 6.614E-08 6.20E-08	1.40E-02 1.40E-		1.82E 1.81E 1.81E 1.80E 1.79E 1.78E 1.77E 1.77E 1.76E 1.75E 1.75E 1.74E 1.74E
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12.60 12.70 12.80 13.00 13.10 13.20 13.30 13.40 13.50 13.60 13.70 13.60 13.70 13.90 14.00 14.10 14.20 14.30 14.40 14.50 14.60	1.679E-07 1.579E-07 1.397E-07 1.397E-07 1.313E-07 1.313E-07 1.313E-07 1.161E-07 1.029E-07 9.536E-08 9.054E-08 8.505E-08 7.989E-08 6.614E-08 6.209E-08 5.828E-08	1.40E-02 1.40E-		1.82E 1.81E 1.81E 1.80E 1.79E 1.79E 1.78E 1.77E 1.77E 1.76E 1.75E 1.75E 1.75E 1.75E 1.74E 1.73E 1.73E 1.73E 1.73E 1.72E 1.73E
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Vita

Robbie Alhakeem was born in Essex, England on March 21, 1968. He attended schools in England, Lebanon, and France. He graduated high school in. August of 1987, he entered the University of Tennessee to pursue a degree in Nuclear Engineering. In May of 1993 he received a Bachelor of Science in that discipline. After traveling for two years, he enrolled part time in the Masters program to pursue an advanced degree in Nuclear Engineering with a concentration in Medical Physics. In 1996 he was accepted as a resident at the Thompson Cancer Survival Center in Knoxville, Tennessee where he received a formal rigorous training in clinical Medical Physics. His Masters degree was received in December of 1999.

He is presently working as a consultant at RadPhys LLC Providing a variety of services in the areas of cancer patient care, 3-D treatment planning, radiation safety, and ongoing medical physics research.