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High-speed multi-beam X-ray imaging using a lens coupling detector system

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Abstract

We present a high-speed multi-beam X-ray imaging realized using a detector system and the recently developed multi-beam X-ray optics [Voegeli et al., *Optica* **7**, 514 (2020)]. The detector utilized optical relay lenses and mirrors for connecting four scintillator screens to a CMOS camera, enabling the high-speed simultaneous acquisition of multiple projection images. We successfully acquired nine projection images in 0.5 ms with a spatial resolution of 70 μm . Dynamical behaviors of a light-bulb filament and a living ladybug were captured with a temporal resolution of 0.5 ms, demonstrating the potential for high-speed and high-spatial-resolution 4D X-ray tomography.

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3 With growing interest in dynamical phenomena in various fields of fundamental and
4 industrial sciences, demand for accessing internal structures of objects with high spatial and
5 temporal resolutions has been increasing. X-ray imaging is often used to visualize internal
6 microstructures of a wide variety of objects non-destructively, which even include weakly
7 X-ray-absorbing objects by virtue of phase-contrast imaging techniques.¹⁻²⁴⁾ The high-speed
8 X-ray imaging has been developed significantly in the past two decades, largely due to the
9 availability of high-brilliance synchrotron radiation (SR) sources and X-ray free-electron
10 lasers. These X-ray sources realized the high-spatial-resolution (on the order of or better than
11 10 μm) two-dimensional (2D) imaging with a temporal resolution even better than μs .²⁵⁻³⁴⁾

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13 For the 3D imaging of non-repeatable phenomena, generally the temporal resolution
14 becomes worse since the depth-resolved visualization requires a rotation of the sample. In
15 particular, a 3D tomographic reconstruction requires a few hundred projection images, and
16 eventually the temporal resolution would be as low as subsecond.³⁵⁻³⁸⁾ A conceptually simple
17 approach to the faster data acquisition is to increase the speed of sample rotation. By using
18 this approach, 4D tomography with a temporal resolution of a few ms and a spatial resolution
19 of a few tens of μm was realized,^{21,28,29,34)} and an even higher temporal resolution can be
20 achieved by applying data processing techniques such as compressed sensing and interior
21 tomography to a smaller number of projection data.^{29,39-42)} However, such a high-speed
22 rotation is incompatible with a sample that is affected by the centrifugal force arising from
23 the rotation, e.g., living beings and fluids.

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25 X-ray multi-beam technique,⁴³⁻⁴⁵⁾ which can illuminate a sample from multiple directions
26 simultaneously, is an alternative promising approach to the high-speed 4D tomography.
27 Hoshino *et al.* developed three-beam imaging system using a direct SR beam and two Bragg-
28 reflected beams from Si single crystals, and succeeded in capturing motions of heart and
29 lungs of a living mouse with a temporal resolution of a few tens of ms.⁴³⁾ Villanueva-Perez
30 *et al.* obtained three projection images simultaneously by using a Si single crystal and
31 showed its potential extension to the nine-beam imaging.⁴⁴⁾ Recently, we have developed a
32 multi-beam X-ray optics consisting of Si single-crystalline blades which can illuminate a
33 sample from more than 30 different directions. Thirty-two projection images covering an
34 angular range of more than $\pm 70^\circ$ were obtained without moving the sample and optics, and
35 a 3D tomogram was successfully reconstructed with the help of a compressed sensing
36 algorithm.⁴⁵⁾ To realize the high-speed 4D tomography, a detector system is required that can
37 simultaneously capture the multiple projection images, distributed in such a wide angular
38 range, with high spatial and temporal resolutions.

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3 Recently, we developed a detector system with a flexible branched optical fiber bundle,
4 which was capable of simultaneous recording of four projection images on a single CMOS
5 camera.⁴⁶⁾ The system realized a spatially flexible detection of the multiple beams, however,
6 the resulting spatial resolution was as low as 200 μm . In the present report, we show a
7 detector system which realized the multi-beam X-ray imaging with a higher spatial
8 resolution. We succeeded in the simultaneous detection of nine projection images of a sample
9 in 0.5 ms with a spatial resolution of 70 μm . Non-repeatable dynamical phenomena were
10 captured with a temporal resolution of 0.5 ms, suggesting its promising capability for the
11 high-speed 4D tomography.
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18 The layout of the multi-beam X-ray imaging is schematically illustrated in Fig. 1. The
19 layout is similar to the previous study⁴⁶⁾ except for the detector system. The experiment was
20 performed at BL28B2 in SPring-8, Japan, and a white SR beam from a bending magnet was
21 used. We used a component of the multi-beam X-ray optics⁴⁵⁾, which consists of eight
22 Si(001) single-crystalline blades aligned on a hyperbolic plane. Each of the blades diffracted
23 X-rays by the (110) lattice planes and illuminated the sample, placed at the focus of the
24 hyperbola, from a different angle. The X-ray beams passing through the sample was incident
25 on the scintillator screens [Mitsubishi Chemical Corporation, DRZ-HR ($\text{Gd}_2\text{O}_2\text{S}:\text{Tb}$,
26 thickness: 50 μm)], and the fluorescence were transferred through the relay lenses
27 (magnification of 1) and mirrors to a CMOS camera (Photron FASTCAM Mini AX50, pixel
28 size: 20 $\mu\text{m} \times 20 \mu\text{m}$). The simultaneous acquisition using a single CMOS camera in a
29 relatively small space (see the photo of Fig. 1) can solve the practical issues of cost and space
30 for realizing the multi-beam X-ray imaging.
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41 A part of the white SR beam directly impinging on the sample was also used to obtain a
42 projection image. The image was recorded with a high-spatial-resolution detector consisting
43 of a scintillator screen ($\text{Ce}:\text{Gd}_3\text{Al}_2\text{Ga}_3\text{O}_{12}$, thickness: 10 μm), a mirror, relay lenses, and a
44 CMOS camera (Photron FASTCAM Nova S12 type 1000 K, effective pixel size: 4.6 $\mu\text{m} \times$
45 4.6 μm). The transmittance of the projection image was calculated by $(I-B)/(I_0-B)$, where I
46 and I_0 are the intensities with and without the sample, respectively, and B is the readout noise
47 of a CMOS camera.
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A tungsten wire (Nilaco, diameter: 50 μm) was used as a test sample, in order to estimate
the spatial resolution of the lens-coupling detector system. The nine projection images were
successfully acquired at the same time with a frame rate of 2000 fps, as shown in Fig. 2. The
beam numbers L1–L4 and R1–R4 are defined in Fig. 1, and the projection angles are shown
in Fig. 2. The corresponding X-ray energies for the Si 220 Bragg reflection are 20.6 keV,

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3 24.9 keV, 32.2 keV, and 46.5 keV for the L1 and R1, L2 and R2, L3 and R3, and L4 and R4
4 beams, respectively. The contrast of the images obtained by the L3, L4, R3, and R4 beams
5 are lower as compared to the other images with lower X-ray energies, since the transmittance
6 increases with X-ray energy. The FWHM of the profile across the wire width, averaged for
7 the images obtained by the L1, L2, R1, and R2 beams, was $120 \pm 7 \mu\text{m}$, indicating that the
8 spatial resolution of the detector was about $70 \mu\text{m}$ which was mainly determined by the
9 thickness of the scintillator screens ($50 \mu\text{m}$) and the pixel size of the CMOS camera ($20 \mu\text{m}$).
10 The spatial resolution is much better than that of the detector system with the branched
11 optical fiber bundle, about $200 \mu\text{m}$.⁴⁶⁾ The resolution of the fiber-coupling system would be
12 largely restricted by the surface roughness of the optical fibers.

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14 To demonstrate the capability for the time-resolved imaging, we observed the moment of
15 breaking of a light-bulb filament (STANLEY MA302, 14 V/60 mA) caused by an overload
16 (100 V, 0.24 A). Fig. 3 shows the projection images (natural logarithm of the X-ray
17 transmittance) made by the white SR, L1, L2, R1, and R2 beams, captured (a) before, (b)
18 during, and (c) after the breaking. Each image was captured successively at a frame rate of
19 2000 fps. The movies for the nine projection images are provided in the Supplementary data.
20 Note that we surrounded the light bulb with a black-painted polyimide tape to reduce the
21 background light emitted from the glowing light bulb; the small dots seen in the images
22 made by the white SR beam originated from air bubbles formed in between the polyimide
23 tape and light bulb.

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25 In the beginning of the breaking, the left half of the filament was deformed as seen in Fig.
26 3(b): the bending points A and B indicated by the arrows were clearly observed. Three ms
27 later, the right half of the filament began to deform (see the Supplementary data), and
28 eventually the filament was completely broken at point C as clearly seen in Fig. 3(c). We
29 estimated the amount of displacement of point D indicated in Fig. 3(c) from its original
30 position in Fig. 3(a). By linear least-squares fitting to the change of pixel position in the
31 images obtained by the white SR, L1, R1, and R2 beams, the amount of displacement along
32 the depth direction, here defined as the direction of the L2 beam, was estimated to be -0.12
33 mm.

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35 We also show a movie of a ladybug in the other Supplementary data. A motion of its leg
36 was successfully captured by the white SR, L1, L2, R1, and R2 beams at a frame rate of
37 2000 fps, suggesting the possible capability of *in-vivo* observation of living beings.

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39 In summary, we performed a high-speed multi-beam X-ray imaging by using a detector
40 system and the multi-beam X-ray optics.⁴⁵⁾ We utilized optical relay lenses and mirrors for
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3 connecting four scintillator screens to a CMOS camera, and successfully obtained nine
4 projection images of a sample at once with an exposure time of 0.5 ms, without moving the
5 sample, X-ray source, and detector. The spatial resolution estimated from a tungsten wire
6 (50 μm diameter) test sample was 70 μm , which is better than that of the previously reported
7 optical fiber-coupling detector, 200 μm .⁴⁶⁾ The moment of breaking of a light-bulb filament
8 and a motion of a ladybug were successfully captured with a temporal resolution of 0.5 ms,
9 demonstrating the capability for the high-speed and high-spatial-resolution multi-beam X-
10 ray imaging. The detector system can be potentially extended to capture all the ~ 30 beams,
11 distributed in an angular range of about $\pm 70^\circ$, to realize the high-speed 4D tomography.
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20 **Acknowledgments**

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22 performed in SPring-8, Japan (Proposal No. 2019B1074). The holder of the multi-beam X-
23 ray optics was fabricated in the machine shop of IMRAM, Tohoku University.
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Template for APEX (Jan. 2014)

Figure Captions

Fig. 1. Schematic illustration of the experimental layout of the multi-beam X-ray imaging using the lens-coupling detector system. Inset at the bottom: photo of the detector system.

Fig. 2. Projection images (X-ray transmittance) of the tungsten wire, simultaneously recorded by the multi-beam X-ray imaging detector with an exposure time of 0.5 ms [gray scale: 0–1.2]. The projection angles are shown in the parentheses.

Fig. 3. Projection images (natural logarithm of X-ray transmittance) of the light bulb, simultaneously recorded by the multi-beam X-ray imaging detector at a frame rate of 2000 fps [gray scale: -1.5–0.2 for the white SR beam and -2.5–0.2 for the other beams]. (a) The images recorded before the filament was broken (corresponding to the images at 4 ms of the supplementary movie). (b) and (c) The images recorded 2 ms and 7 ms later from (a), respectively.

Template for APEX (Jan. 2014)

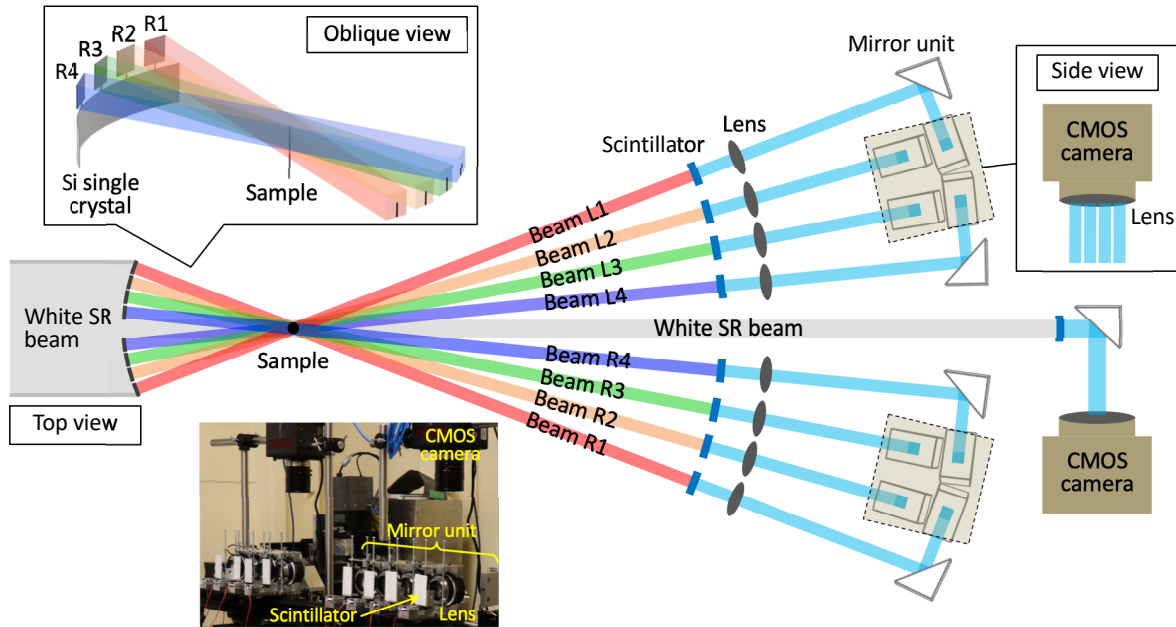


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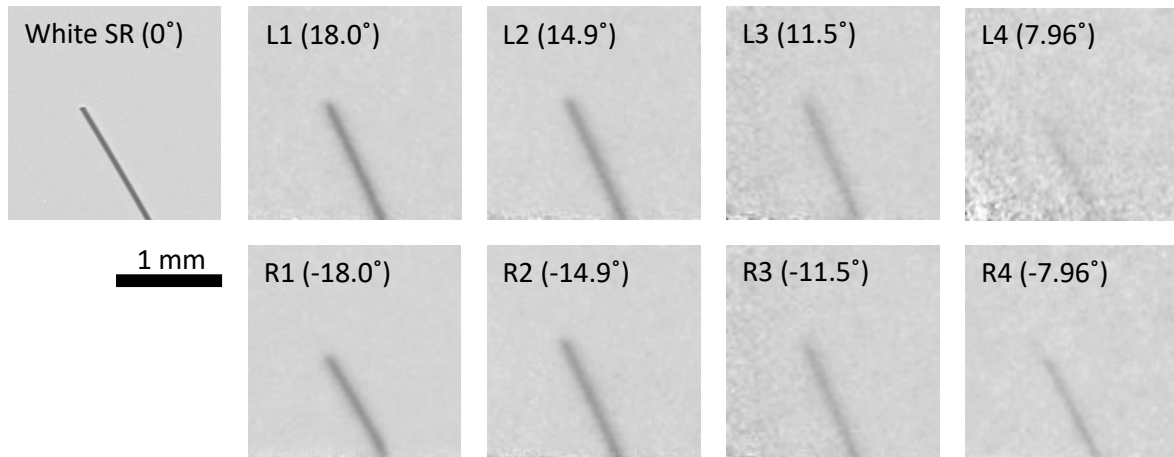


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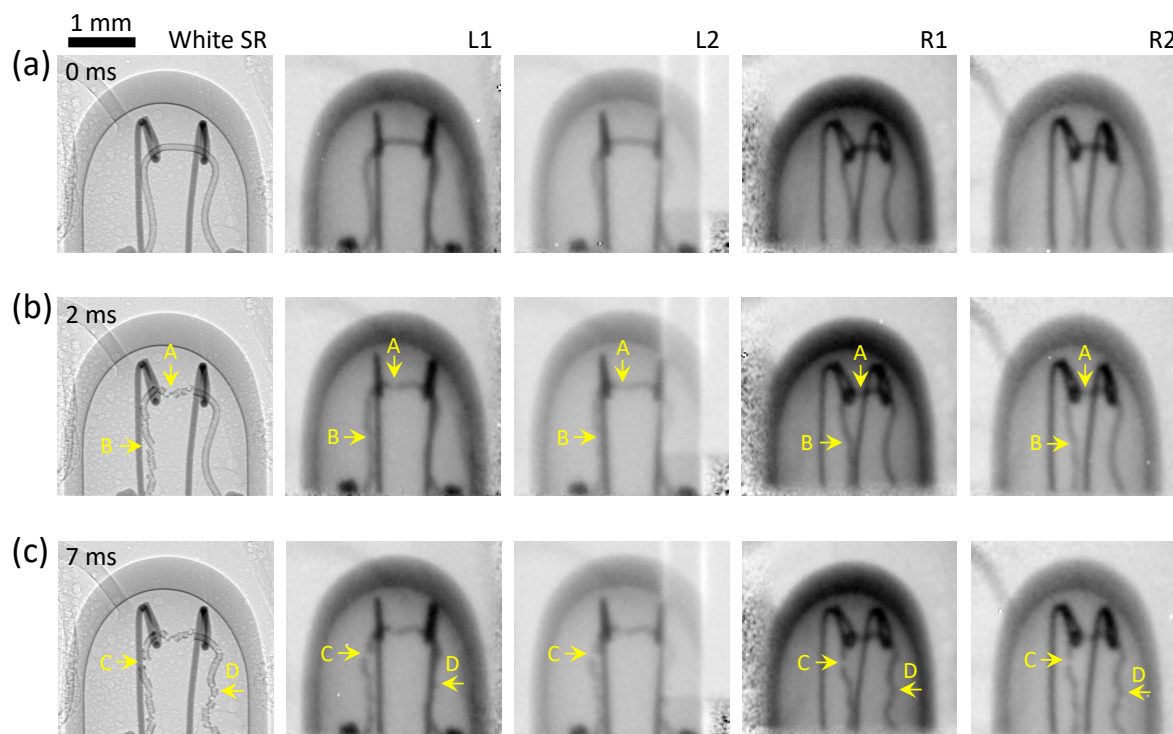


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