

1 **A novel intraoperative ultrasound probe for transsphenoidal surgery: first-in-human**
2 **study**

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30 *Activities related to the present article:*

31 The Authors declare that there is no conflict of interest.

32 *Activities not related to the present article:*

33 TV is co-founder and shareholder of Hypervision Surgical; TV is also
34 shareholder of Mauna Kea Technologies.

35 **Author Contribution:**

36

37 *Study conception and design:* IC, RD, CLH, SO, VV, TV, HJM, NLD.

38

39 *Acquisition of data:* IC, RD, HJM, NLD.

40

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46

47 All Authors have given final approval of the version to be published. All Authors agree to be
48 accountable for all aspects of the work.

49 **Abstract**

50

51 *Background:* Ultrasound has been explored as an alternative, less bulky, less time-consuming
52 and less expensive means of intraoperative imaging in pituitary surgery. However, its use has
53 been limited by the size of its probes relative to the transsphenoidal corridor. We developed a
54 novel prototype that is more slender than previously reported forward-viewing probes and, in
55 this report, we assess its feasibility and safety in an initial patient cohort.

56

57 *Method:* The probe was integrated into the transsphenoidal approach in patients with pituitary
58 adenoma, following a single-centre prospective proof of concept study design, as defined by
59 the IDEAL guidelines for assessing innovation in surgery (IDEAL stage 1 – Idea phase).

60

61 *Results:* The probe was employed in 5 cases and its ability to be used alongside the standard
62 surgical equipment was demonstrated in each case. No adverse events were encountered. The
63 average surgical time was 20 minutes longer than that of 30 contemporaneous cases operated
64 without intraoperative ultrasound.

65

66 *Conclusion:* We demonstrate the safety and feasibility of our novel ultrasound probe during
67 transsphenoidal procedures to the pituitary fossa, and, as a next step, plan to integrate the device
68 into a surgical navigation system (IDEAL Stage 2a – Development phase).

69 **Background**

70

71 Pituitary tumours are common, affecting 15-20% of the population¹ and the transsphenoidal
72 approach is the preferred corridor to access these lesions when surgery is indicated. However,
73 despite advances in microsurgical and endoscopic technique,² some pituitary tumours remain
74 difficult to cure. About a third of patients undergoing transsphenoidal surgery will have an
75 incomplete resection.³ As a consequence, different intraoperative imaging modalities have
76 been explored to address this shortcoming, including magnetic resonance imaging (MRI) and
77 computed tomography (CT).^{4, 5} Although both intraoperative MRI and CT can provide high-
78 resolution images, their bulkiness, cost and impact on the duration of surgery related to the
79 acquisition of images, can all be advanced as obstacles to their regular and widespread use, not
80 only in transsphenoidal surgeries but in neurosurgical procedures in general.

81

82 Intraoperative ultrasound presents with several advantages in this regard and so, has been
83 investigated during intracranial procedures as an alternative means of intraoperative imaging
84 for real-time intraprocedural orientation and to assess the extent of tumour resection.⁶⁻⁹ But its
85 application to transsphenoidal surgery is notably limited by the size of its probes, and by the
86 fact that later probes – having adopted a side-viewing design precisely in an attempt to reduce
87 their size – produce images that are more difficult to interpret intraoperatively.^{10, 11} To both
88 these ends, we have developed a slender, forward-viewing ultrasound device for
89 transsphenoidal access and plan to create novel software tools to integrate this device into a
90 surgical navigation system. It is hoped that this integrated system will be helpful in locating
91 residual pituitary tumour tissue as well as neurovascular structures. Building upon our pre-
92 clinical experience with the probe on phantom heads,¹² the purpose of the current study is to
93 confirm the feasibility and safety of this new intraoperative ultrasound device in an initial
94 patient cohort. As such, the work presented here is at stage 1 (Idea phase) of the “Innovation,
95 Development, Exploration, Assessment, and Long-Term Study (IDEAL) model” statements.¹³

96

97 **Method**

98

99 Ethical approval was obtained from our local ethics committee (19/LO/0882), and the trial was
100 registered on ClinicalTrials.gov (NCT03284775).

101

102 *Study design*

103 A single-centre prospective proof of concept study design was adopted, as defined by the
104 IDEAL guidelines for assessing innovation in surgery, and the relevant reporting guidelines
105 were used in the preparation of this manuscript.^{13, 14}

106

107 The study began in October 2019 and involved patients undergoing transsphenoidal surgery
108 for pituitary adenoma at the National Hospital for Neurology and Neurosurgery.

109

110 *Participants*

111 The minimum inclusion criteria were 1) adult patients, 2) undergoing transsphenoidal surgery,
112 3) diagnosis of pituitary adenoma on pre-operative MRI, and 4) able to provide consent. The
113 patients recruited were highly selected, and we favoured patients with more normal anatomical
114 configurations and standard pathological appearances.

115

116 All patients gave their written informed consent to test our ultrasound probe after the risks,
117 benefits, and alternatives were discussed. Patients were specifically informed that this was the
118 first clinical application of this novel ultrasound probe.

119

120 Patients were recruited from October 2019 to March 2020, when the UK entered a lockdown
121 in response to the COVID-19 pandemic. All operations were performed by IC, HJM, and NLD,
122 who have a subspecialty interest in pituitary surgery, and were involved with the design and
123 preclinical assessment of the ultrasound probe. All operations took place at the National
124 Hospital for Neurology and Neurosurgery, which is a large regional neuroscience centre, that
125 carries out approximately 150-200 pituitary operations each year.

126

127 *Intervention*

128 Our quasi-forward-looking ultrasound probe is shown in Figure 1. It is a clinical-grade
129 prototype manufactured by Vermon (Vermon S.A., Tours, France) based on design
130 requirements stemming from our research team. Vermon is a company specialising in advanced
131 transducer technologies. The probe's design corresponds to a novel version of two previous
132 prototypes, which were also manufactured by Vermon and used successfully for patients
133 undergoing transsphenoidal surgery.^{12,13} Our novel transducer consists of an endoscopic-
134 shaped probe with a shaft that is slenderer than in previous versions. The tip is 200 mm long
135 and has a diameter of 7 mm. At the end of the probe, an 80-element convex array with a

136 curvature radius of 8.48 mm is located along the tip, imaging both in the forward and side
137 directions. The centre frequency is higher than previous prototypes, 18 MHz, to improve image
138 resolution. The transducer's connector is compatible with the CE-marked SonixTouch
139 ultrasound console (BK Ultrasound, UK). The ultrasound probe is cleaned before and after use
140 using standard wet wipes, and is gelled and draped in the usual fashion during surgery
141 (Molnlycke Healthcare, UK).

142

143 The surgical technique for the endoscopic transsphenoidal approach is unchanged to that used
144 without the ultrasound probe. General anaesthesia is administered, and nasal mucosal
145 decongestants applied (Moffat's solution). Patients are positioned supine, in the conversational
146 position,¹⁵ and the operative field prepared and draped in a sterile fashion. Access to the sella
147 turcica is performed through a monostril endoscopic approach. If needed, the floor and
148 anterior wall of the sella are drilled off. A cruciate incision is made to the dura mater and the
149 tumour removed using curettes and rongeurs. The ultrasound probe is applied to the sella before
150 and after the dural incision for visualisation of the tumour and surrounding neurovascular
151 structures. Haemostasis is achieved using bipolar electrocautery, Spongostan (Ethicon,
152 Johnson & Johnson) or Surgiflo (Ethicon, Johnson & Johnson). In case of an intraoperative
153 cerebrospinal fluid (CSF) leak, a fat graft is harvested from the patient's abdomen and placed
154 over the dural defect. Nasal packing is not placed in the absence of CSF leak.

155

156 *Measures of outcome*

157 The primary outcomes of the study were to demonstrate that the use of the ultrasound device
158 in pituitary surgery is both technically feasible and safe. Technical feasibility was assessed by
159 the ability of the probe to be used during transsphenoidal surgery alongside standard surgical
160 equipment. Device safety was assessed by the number, type, and severity of adverse events
161 related to use of the device, e.g. device malfunction.

162

163 The secondary outcomes were to demonstrate that the ultrasound device does not adversely
164 affect the occurrence of postoperative complications, the operating time (minutes), and the
165 length of stay (days). For this purpose, the operating times and length of stay were also
166 collected for a series of 30 consecutive patients with pituitary adenoma, operated before and
167 contemporaneously to this study, by the same surgical team and with the same surgical
168 technique, but in whom intraoperative ultrasound had not been used. Postoperative
169 complications to be recorded included death, cerebrospinal fluid leak, meningitis, vascular

170 complications, visual complications, diabetes insipidus, hypopituitarism, and cranial nerve
171 injury. Vascular complications to be recorded included carotid or other vessel injury, or
172 symptomatic haematoma. Venous bleeding from the cavernous sinus was to be considered a
173 vascular complication only if it prevented completion of the surgical procedure. Epistaxis was
174 only to be considered a vascular complication if it warranted return to the operating room.
175 Cerebrospinal fluid leaks to be recorded included all postoperative leaks requiring lumbar
176 drainage or repair. Patients with Cushing's disease receiving postoperative cortisol, or in whom
177 a hypophysectomy was carried out were also not included as surgical complications.

178

179 A short written assessment of the probe usage was performed by the surgeon carrying out the
180 procedure after each operation.

181

182 **Results**

183

184 *Baseline data*

185 Eleven patients were approached to participate in this study and all eleven were recruited, but
186 only five participated (2 female, 3 male; age range: 42–73 years), due to the study's
187 discontinuation in the general response to the COVID-19 pandemic. Diagnosis was
188 gonadotroph pituitary macroadenoma in three cases, acromegaly in one case (somatotroph
189 pituitary microadenoma), and a haemorrhagic cystic residual of a previously resected
190 gonadotroph macroadenoma in the remaining case.

191

192 *Intervention and outcomes*

193 Primary outcomes

194 The probe's ability to be used alongside the standard surgical equipment for transsphenoidal
195 procedures (Figure 2A) was demonstrated in all cases. Once the sella turcica is entered, we
196 usually fix the endoscope, using its holder, in the supero-external angle of the sphenoid opening
197 for the greater part of the procedure, allowing bimanual handling of instruments in and around
198 the pituitary fossa. Our ultrasound probe could be handled in the same way as another
199 instrument, under endoscopic vision and without entering into conflict with the endoscope in
200 all five cases (Figure 2B).

201

202 No adverse events related to the device were encountered.

203

204 Secondary outcomes

205 Following discharge, one patient represented with a delayed CSF leak in the context of an acute
206 abdominal obstruction and subsequently developed meningitis. None of the patients had new
207 pituitary hormonal deficits postoperatively, aside one patient who remained on hydrocortisone
208 replacement therapy on follow-up.

209

210 Operating time ranged from 68 to 110 minutes (mean: 93 min) and length of stay was 4 days
211 in one case, 5 days in two cases, 6 days in one case and 18 days in the case with acute abdominal
212 obstruction (median: 5 days). This represents a 20 min difference when compared to the
213 average operating time of thirty contemporaneous, consecutive cases of pituitary adenoma
214 resection performed by our team without intraoperative ultrasound (range: 45–168 min, mean:
215 73 min). The length of stay for this same group, on the other hand, was comparable (range: 2
216 – 20 days, median: 4 days).

217

218 Three written assessments positively underlined that tumour and vessels were readily
219 identifiable, and in two cases that an adenoma residual was evident. In one of these cases,
220 ultrasound allowed to identify a residual that would not have otherwise been noticed.
221 Additional remarks were that ultrasound clarity was best before opening the dura mater, that
222 flowable haemostatic matrix obscured the view and that the Doppler overlay was useful for a
223 better distinction of the structures dorsal to the tumour. One assessment observed that the probe
224 would be best used alongside neuronavigation, in view of the difficulty to convincingly identify
225 the anatomy on ultrasound in that particular case.

226

227 **Discussion**

228

229 *Principal findings*

230 The present study shows that the use of our novel ultrasound device, specifically developed for
231 the transnasal corridor to the pituitary gland, is both technically feasible and safe.

232

233 We did not encounter any adverse effects in this preliminary cohort. The use of the ultrasound
234 probe did not significantly disrupt the surgical workflow and the additional average surgical
235 time compared favourably with scanning times reported for other intraoperative imaging
236 modalities.¹⁶⁻¹⁸ We did however experience some difficulty with flattening the superfluous
237 folds of the probe's protective sterile sheath, actually intended for bulkier probes and so adding

238 unwanted volume to our prototype (Figure 2B). This led to the aggregation of air bubbles near
239 the tip of the probe, causing the formation of reflection artifacts in the image (Figure 4C). We
240 rapidly learned to make use of a sterile elastic band to maintain the sheath taut around the
241 probe's tip (Figure 2A). Nevertheless, a dedicated slimmer sheath or a transducer design
242 compatible with standard sterilisation processes would be a preferable solution for future use.
243 Finally, the probe did not enter into conflict with the endoscope, which was positioned
244 superolaterally in the ipsilateral nostril, and so could be introduced under direct endoscopic
245 vision (Figure 2B).

246

247 Operator feedback collected following surgery conveyed that vessels and tumour contours
248 were readily identified on ultrasound (Figures 3 & 4); that clarity was felt to be best before
249 opening the dura mater; and that the use of flowable haemostatic matrix obscured the
250 ultrasound views. Although our project is not yet at a phase to assess our probe's intraoperative
251 impact on surgical decision-making, anecdotally it did allow to identify an adenoma residual
252 in one patient that would otherwise have been missed.

253

254 *Relation to other studies*

255 Our prototype is less bulky than another recent forward-viewing probe, which was found to be
256 too large to safely enter the sphenoid sinus in 2 patients of the 24 included in that report.¹¹ The
257 same group reported six years earlier on their experience with a slenderer prototype, where the
258 transducer was side-viewing, but where the ultrasound images were also less intuitive as a
259 consequence.¹⁰ Side-viewing designs have since become commercially available. Indeed, the
260 development of thin ultrasound probes, dedicated to the transsphenoidal approach, has been
261 based on a necessary trade-off between image quality (which is dependent on the number of
262 ultrasound elements, greater in the side-viewing prototype) and image intuitiveness (best in the
263 forward-viewing probe). Moreover, a side-viewing probe needs to be inserted *into* the sella
264 turcica to be able to scan the sellar structures, thereby limiting its use to larger tumours, where
265 an initial cavity has to first be made for the probe's tip to be introduced.^{10, 11, 19} In contrast, a
266 forward-viewing probe does not have to enter the sella to scan it.

267

268 It is with these surgically relevant considerations that we decided to centre further development
269 around a forward-viewing prototype, and to work on optimising image quality for the purpose
270 of transsphenoidal surgery while at the same time keeping the probe's diameter in proportion
271 with the surgical corridor. Accordingly, our prototype has a diameter of 7 mm, in contrast to

272 the 12 x 8 mm rectangular tip of the previously reported forward-viewing probe discussed
273 above.¹¹ The transducer's array also has a higher central frequency, 18 MHz, as compared with
274 the transsellar and intrasellar probes, which exhibit a central frequency of 10.3 MHz and 12
275 MHz, respectively. The number of piezoelectric elements was raised to 80 and the pitch size
276 reduced to 100 μm to mitigate the appearance of grating lobes artifacts, as suggested by
277 Solheim et al.¹⁰ The miniaturisation of the linear convex array allowed us to place it in the
278 forward-looking direction and provide more familiar imaging planes.

279

280 The high frequency of our transducer provides high-resolution images but also affects the
281 imaging depth due to the generation of pulses of shorter wavelength, which are more attenuated
282 in tissue. However, we did not require an imaging depth greater than 4 cm during surgery, and
283 the effect of attenuation on the image quality was negligible. Furthermore, the probe's
284 resolution was assessed in a previous experiment¹² and consisted in imaging a 25 μm tungsten
285 fibre at different depths in a water bath. The average resolution of our transducer across depth
286 (from 0.5 cm to 2.5 cm with intervals of 0.5 cm) was measured to 0.26 mm (± 0.02) in the axial
287 plane and 1.3 mm (± 0.3) in the lateral plane.

288

289 *Strength and limitations*

290 The strength of this report is its continuity with previous pre-clinical work, ensuring that the
291 surgical team, who had also been involved in the prototype's design, already had a good
292 working knowledge of the system for the purpose of the IDEAL stage 1 assessment intended
293 in this study.

294

295 Although an IDEAL stage 1 study is intended as a proof of concept and is therefore usually
296 limited to a small number of patients, our cohort was in fact smaller than we had initially
297 planned due to the study having been suspended in the wake of the COVID-19 pandemic. This
298 point can be advanced as a limitation to the descriptive nature of this report.

299

300 **Conclusion**

301

302 Our study demonstrates the safety and feasibility of our ultrasound probe during
303 transsphenoidal approaches to the pituitary fossa. An IDEAL stage 2a (Development phase) is
304 now planned to integrate this device into a surgical navigation system, as a means of further
305 enhancing the intraoperative understanding of the surgical field.

306 **References**

307

- 308 1. Ezzat S, Asa SL, Couldwell WT, et al. The prevalence of pituitary adenomas: a
309 systematic review. *Cancer*. Aug 1 2004;101(3):613-9. doi:10.1002/cncr.20412
- 310 2. Marcus HJ, Hughes-Hallett A, Kwasnicki RM, Darzi A, Yang GZ, Nandi D.
311 Technological innovation in neurosurgery: a quantitative study. *J Neurosurg*. Jul
312 2015;123(1):174-81. doi:10.3171/2014.12.JNS141422
- 313 3. Dallapiazza RF, Grober Y, Starke RM, Laws ER, Jr., Jane JA, Jr. Long-term results of
314 endonasal endoscopic transsphenoidal resection of nonfunctioning pituitary macroadenomas.
315 *Neurosurgery*. Jan 2015;76(1):42-52; discussion 52-3. doi:10.1227/NEU.0000000000000563
- 316 4. Chittiboina P. iMRI During Transsphenoidal Surgery. *Neurosurg Clin N Am*. Oct
317 2017;28(4):499-512. doi:10.1016/j.nec.2017.05.005
- 318 5. Sylvester PT, Chicoine MR. Intraoperative Imaging for Pituitary Surgery. In: Laws E,
319 Jr., Cohen-Gadol A, Schwartz T, Sheehan J, eds. *Transsphenoidal Surgery*. Springer; 2017.
- 320 6. Mair R, Heald J, Poeata I, Ivanov M. A practical grading system of ultrasonographic
321 visibility for intracerebral lesions. *Acta Neurochir (Wien)*. Dec 2013;155(12):2293-8.
322 doi:10.1007/s00701-013-1868-9
- 323 7. Sweeney JF, Smith H, Taplin A, Perloff E, Adamo MA. Efficacy of intraoperative
324 ultrasonography in neurosurgical tumor resection. *J Neurosurg Pediatr*. May 2018;21(5):504-
325 510. doi:10.3171/2017.11.PEDS17473
- 326 8. Marcus HJ, Vercauteren T, Ourselin S, Dorward NL. Intraoperative Ultrasound in
327 Patients Undergoing Transsphenoidal Surgery for Pituitary Adenoma: Systematic Review
328 [corrected]. *World Neurosurg*. Oct 2017;106:680-685. doi:10.1016/j.wneu.2017.07.054
- 329 9. Sastry R, Bi WL, Pieper S, et al. Applications of Ultrasound in the Resection of Brain
330 Tumors. *J Neuroimaging*. Jan 2017;27(1):5-15. doi:10.1111/jon.12382
- 331 10. Solheim O, Selbekk T, Lovstakken L, et al. Intrasellar ultrasound in transsphenoidal
332 surgery: a novel technique. *Neurosurgery*. Jan 2010;66(1):173-85; discussion 185-6.
333 doi:10.1227/01.NEU.0000360571.11582.4F
- 334 11. Solheim O, Johansen TF, Cappelen J, Unsgard G, Selbekk T. Transsellar Ultrasound in
335 Pituitary Surgery With a Designated Probe: Early Experiences. *Oper Neurosurg (Hagerstown)*.
336 Jun 1 2016;12(2):128-134. doi:10.1227/NEU.0000000000001108
- 337 12. Mihecin S, Marcus H, Delaunay R, et al. Preclinical assessment of a novel intraoperative
338 ultrasound probe for transsphenoidal surgery, In: CARS 2018 - Computer Assisted Radiology
339 and Surgery Proceedings of the 32nd International Congress and Exhibition, Berlin, Germany,

340 June 20-23 2018. *Int J Comput Assist Radiol Surg* 2018;13(Suppl 1):57-59.
341 doi:10.1007/s11548-018-1766-y

342 13. McCulloch P, Altman DG, Campbell WB, et al. No surgical innovation without
343 evaluation: the IDEAL recommendations. *Lancet*. Sep 26 2009;374(9695):1105-12.
344 doi:10.1016/S0140-6736(09)61116-8

345 14. Bilbro NA, Hirst A, Paez A, et al. The IDEAL Reporting Guidelines: A Delphi
346 Consensus Statement Stage Specific Recommendations for Reporting the Evaluation of
347 Surgical Innovation. *Ann Surg*. Jan 1 2021;273(1):82-85.
348 doi:10.1097/SLA.0000000000004180

349 15. Ekanayake J, Baudracco I, Quereshi A, Vercauteren T, Dorward NL. The
350 conversational position in endoscopic pituitary surgery. *Br J Neurosurg*. Feb 2018;32(1):44-
351 46. doi:10.1080/02688697.2017.1406058

352 16. Ramm-Pettersen J, Berg-Johnsen J, Hol PK, et al. Intra-operative MRI facilitates
353 tumour resection during trans-sphenoidal surgery for pituitary adenomas. *Acta Neurochir*
354 (*Wien*). Jul 2011;153(7):1367-73. doi:10.1007/s00701-011-1004-7

355 17. Zaidi HA, De Los Reyes K, Barkhoudarian G, et al. The utility of high-resolution
356 intraoperative MRI in endoscopic transsphenoidal surgery for pituitary macroadenomas: early
357 experience in the Advanced Multimodality Image Guided Operating suite. *Neurosurg Focus*.
358 Mar 2016;40(3):E18. doi:10.3171/2016.1.FOCUS15515

359 18. Mori R, Joki T, Matsuwaki Y, Karagiozov K, Murayama Y, Abe T. Initial experience
360 of real-time intraoperative C-arm computed-tomography-guided navigation surgery for
361 pituitary tumors. *World Neurosurg*. Feb 2013;79(2):319-26. doi:10.1016/j.wneu.2012.10.011

362 19. Alshareef M, Lowe S, Park Y, Frankel B. Utility of intraoperative ultrasonography for
363 resection of pituitary adenomas: a comparative retrospective study. *Acta Neurochir (Wien)*. Jan
364 5 2021;doi:10.1007/s00701-020-04674-2

365

366 **Figures**

367

368 **Figure 1.** Photograph showing the novel forward-viewing ultrasound probe. **(A)** 200 mm. **(B)**
369 15 mm. **(C)** 85 mm. The probe tip's diameter (the distance between the **two blue arrows**) is 7
370 mm. **(D)** The probe's distal 16 mm contain an 80-element convex array. The radius of the
371 transducer's curvature (**indicated by black arrowhead**) is 8.48 mm.

372

373 **Figure 2.** **(A)** Photograph of the surgical field showing the ultrasound probe in use alongside
374 the endoscope. **(B)** Top view: Transsphenoidal endoscopic view through left nostril showing
375 the opening made in an enlarged sella turcica. The pituitary tumour has been partially resected.
376 Middle view: The sphenoid sinus is filled with water to reduce acoustic impedance. Lower
377 view: The ultrasound probe's tip is inserted through the sellar opening under endoscopic vision.

378

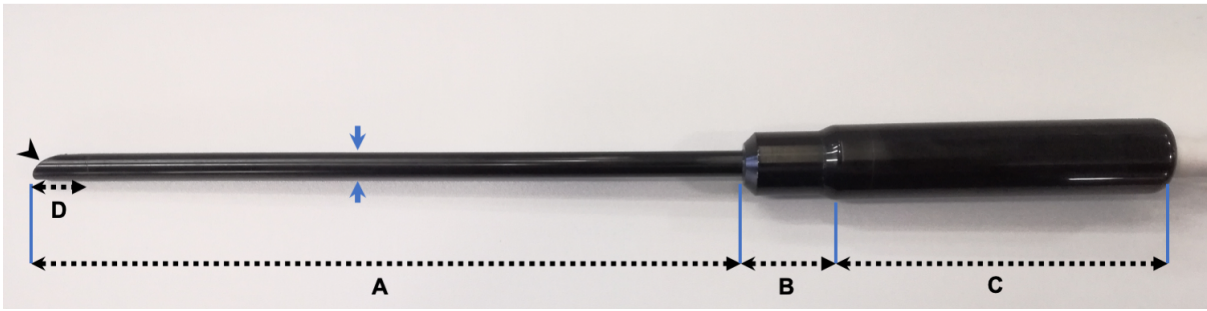
379 **Figure 3.** **(A)** T2-weighted coronal magnetic resonance imaging slice of a patient with a
380 pituitary macroadenoma with suprasellar expansion causing displacement of the optic chiasm.
381 The inset in the top right corner of panel A is a T1-weighted sagittal slice in the same patient
382 indicated the level of the coronal slice (thin blue line). The white rectangular frame centred on
383 the tumour's apex, seen protruding through the diaphragm sellae, provides the approximative
384 bearings of panel B, whilst the oblique frame centred on the cavernous segment of the right
385 internal carotid artery provides the bearings for panel C. **(B)** Intraoperative ultrasonographic
386 caption showing the suprasellar portion of the tumour, protruding through the diaphragm sellae.
387 The diaphragm sellae is indicated on either side of the tumour by arrowheads. The
388 hypoechogenic space dorsal to the tumour represents the posterior aspect of the suprasellar
389 cistern, just posterior to the optic chiasm and the pituitary stalk. This ultrasound caption is
390 therefore an oblique slice that represents structures slightly posterior to those shown in panel
391 A, i.e. it shows the tumour apex as it begins its posterior descent (see inset in panel A). **(C)**
392 Intraoperative ultrasonographic caption of the right infrasellar portion of the tumour. The right
393 diaphragm sellae is indicated by the white arrowhead. The asterisk indicates the cavernous
394 segment of the right internal carotid artery. Note the heterogenous "mottled" tumour
395 echogenicity visible in panels B and C, and corresponding to the intratumoural regions of T2
396 hyperintensities seen in panel A.

397

398 **Figure 4.** **(A)** T2-weighted coronal magnetic resonance imaging slice of a patient with a
399 pituitary macroadenoma with suprasellar expansion causing compression of the optic chiasm.

400 The inset in the top right corner of panel A is a T1-weighted sagittal slice in the same patient
401 indicated the level of the coronal slice (thin blue line). The white rectangular frame centred on
402 the cavernous segment of the left internal carotid artery provides the approximative bearings
403 of panel B, whilst the left frame centred on the tumour's apex provides the bearings for panel
404 C. **(B)** Intraoperative ultrasonographic caption of the left lateral aspect of the tumour and of
405 the cavernous segment of the left internal carotid artery (asterisks). **(C)** Intraoperative
406 ultrasonographic caption showing the suprasellar portion of the tumour. The A1 segment of
407 the left anterior cerebral artery has been sliced longitudinally. Its dorsal wall is the faint
408 hyperechogenic line shown by the full white arrowhead. The contralateral A1 has been sliced
409 transversally and slightly obliquely, and can be made out faintly as an ovoid circle (hollow
410 arrowhead). The tumour is mostly of a homogenous appearance both on panels B and C. Panel
411 C is also illustrative of reverberation artifact, due to the presence of air between a segment of
412 the convex ultrasound array and the medium.
413

414 **Figure 1**

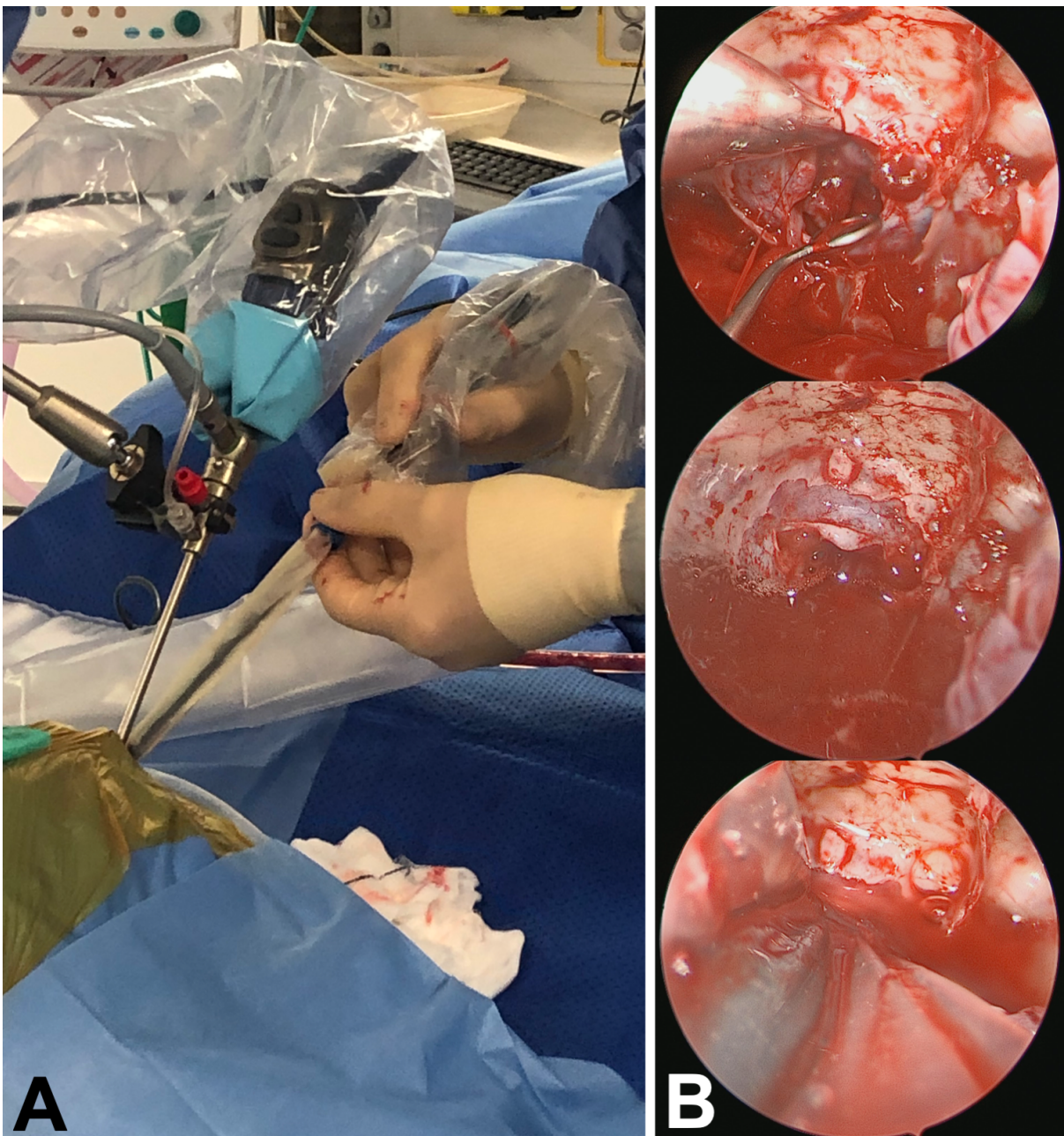


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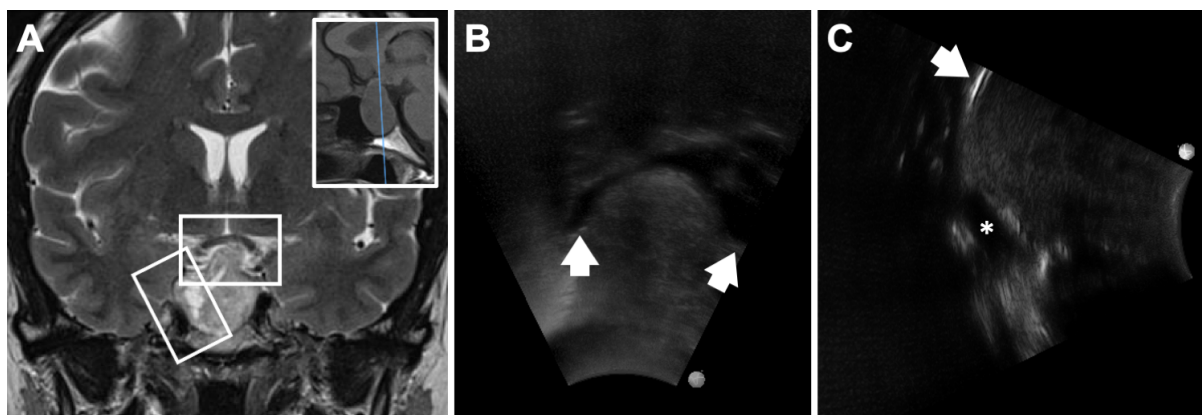
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418 **Figure 2**



419

420 **Figure 3**

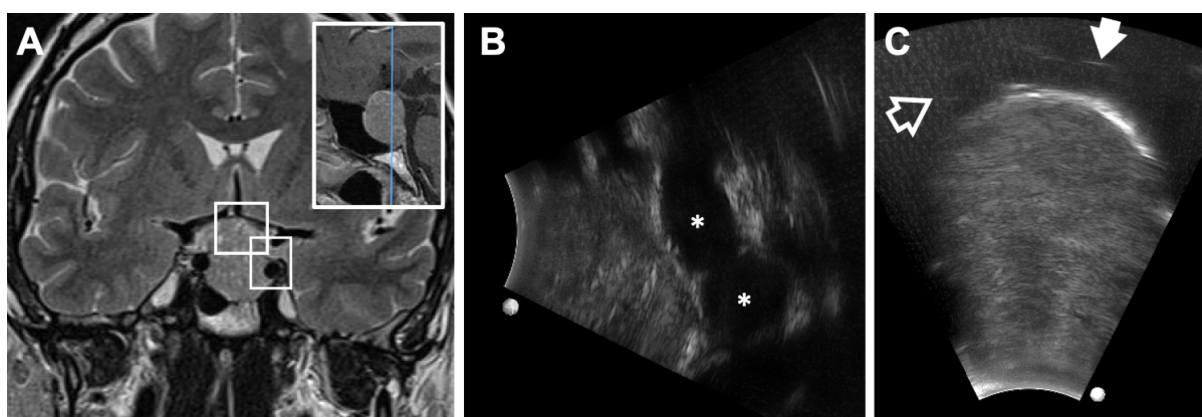


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422

423

424 **Figure 4**



425