Deep Brain Stimulation: Awake and Asleep Options

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"Good stereotactic surgery for movement disorders can be performed with or without the microelectrode, and poor surgical results can occur both with and without the microelectrode." – Dr. Roy Bakay¹



Figure 1

Early methods of localizing deep brain structures. **A.** Anteroposterior and **B.** lateral views of a pneumoencephalogram obtained by filling the ventricles with air; and **C.** Anteroposterior and **D.** lateral views of a ventriculogram obtained by injecting the ventricles with contrast medium.

A BRIEF HISTORY OF DBS AND NEUROIMAGING

Stereotactic neurosurgery is founded on the ability to accurately localize and safely access targets within the brain in a minimally-invasive manner. The stereotactic method was first described in 1908 by Sir Victor Horsley and Robert Clarke at University College London, where they developed an apparatus for animal experimentation that allowed them to establish a threedimensional Cartesian coordinate system for targeting. At that time, however, x-rays were the only available form of imaging the human body and as such, localizing intracranial targets relied on a combination of knowledge from anatomical atlases and the visualization of a few intracranial landmarks such as the pineal gland or the foramen of Monroe. These landmarks could be visualized by filling the ventricles with air (pneumoencephalogram) or a contrast medium (ventriculogram) [Figure 1]. In 1947, Ernst Spiegel and Henry Wycis created the first human stereotactic frame that allowed for lesioning of deep brain nuclei for the treatment of psychiatric disease.²

With imaging limited to x-rays alone, a need arose for another means of confirming the appropriate location where a lesion would be made or an electrode would be implanted. Nicholas Wetzel and Ray S. Snider have been accredited with performing the first microelectrode recording (MER) in humans in 1958 during a pallidotomy.³ Over time, particularly with the popularization of thalamotomy for the treatment of Parkinson's disease and with a growing appreciation of characteristic recordings of specific nuclei, MER became commonplace in stereotactic neurosurgery.

Over the following decades, deep brain stimulation (DBS) gained favor over ablation due to a lower side effect profile and to the ability to reverse the effects of the former. As with early deep brain lesioning, deep electrical stimulation of brain structures was originally introduced as a therapeutic option to treat behavioral disorders or chronic pain.² Natalia Petrovna Bekthereva was the first to implant electrodes into subcortical structures for chronic stimulation for hyperkinetic disorders, but the idea to use chronic stimulation as a therapeutic method did not emerge until Alim-Louis Benabid's report in 1987 on stimulation of the Vim nucleus for treating a patient with tremor.²

It is also in this decade that the field of neuroimaging was completely changed by the introduction of magnetic resonance imaging (MRI). Improvements in imaging began a decade earlier, however, when the first clinical computed tomography (CT) scan was performed in 1971 [Figure 2].⁴ While better than x-rays, CT scans were still limited in their ability to represent soft tissue. This limitation would be addressed by MRI, which also emerged in the 1970s; and the first MR images of a human brain were generated in 1978 [Figure 3a].⁵ Nevertheless, images generated on clinical MR scanners were still not capable of accurately representing targets such as the subthalamic nucleus (STN) or the globus pallidus pars interna (GPi). As such, DBS targeting continued to rely on previously established locations from accepted atlases, such as that of Schaltenbrand and Wahren. In order to account for anatomical variation between patients, MERs and awake testing were necessary to ensure proper positioning of DBS electrodes.

With sufficient safety and efficacy data, the Food and Drug Administration (FDA) approved DBS as a treatment for essential tremor in 1997 and for Parkinson's disease in 2002.⁶ Now, more than 135,000 patients worldwide have received DBS therapy.⁷ While the majority of centers continue to perform the surgery awake and with MER, there has been a trend towards performing the surgery under general anesthesia and without MER. Improvements in technology and a deeper understanding of MRI physics has allowed for clearer and more accurate representations of intracranial anatomy [Figure 3b-d]. We are now able to consistently visualize the borders of deep brain nuclei on MR images acquired on clinical scanners, which in turn facilitates surgical planning and allows for an image-guided, image-verified approach to DBS implantation [Figure 4]. Overall, it is the advances in both surgical technologies and neuroimaging techniques that have allowed for the maturation of stereotactic neurosurgery over the past several years. Here, we will outline both the "awake" and "asleep" versions of the surgical procedure; and provide an overview of the pros and cons of each approach.

DBS VERIFIED BY MICROELECTRODE RECORDINGS AND MACROSTIMULATION

The most common method of implanting DBS electrodes in the United States involves microelectrode recordings (MERs) and macrostimulation in an awake patient. As

mentioned above, this technique allows the surgeon to confirm the target for electrode placement with neurophysiologic recordings and immediate clinical response.

At our institution, the trajectory to the desired target is first planned on a T2 weighted or proton density (PD) MRI as well as on volumetric (1cm³ voxel) T1 weighted gadolinium-enhanced MRI. In order to optimize MERs and the reliability of intraoperative testing, the patient's



Figure 2

The first clinical computed tomography (CT) scan performed in 1971 at Atkinson Morley's Hospital, in London, England.



Figure 3

The evolution of magnetic resonance imaging (MRI) **A**. The first clinical MRI was performed in 1978 in England. Since then, imaging has improved significantly with increasing magnet strength from **B**. 3T imaging first performed in 1984, **C**. 7T imaging first performed in 1999, and **D**. 9.4T imaging first performed in 2007.

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Figure 4

Magnetic resonance images (MRI) can now be optimized to clearly visualize deep brain structures for targeting in deep brain stimulation (DBS). **A**. A T2 sequence MRI is used to visualize the subthalamic nucleus (STN) **B**. highlighted in red; and **C**. A proton density (PD) sequence MRI is used to visualize the globus pallidus (GP) **D**. highlighted in red

are in the OFF-state during the time of surgery. The first stage of the procedure starts with placement of a stereotactic (Leksell) frame under local anesthesia. After a reference CT is acquired with the frame on the patient, this image is merged with the MRI containing the stereotactic plan. This step allows for the calculation of the stereotactic Leksell frame coordinates, which defines the planned room, the patient is positioned in a semirecumbent position with the head fixed to the operating room table. Under monitored anesthetic care, incisions are made in the scalp and 14mm burr holes are drilled in the skull. Once the dura and pia have been sharply opened, the microelectrode drive is assembled on the Leksell frame. It is at this time that the patient is awakened and MERs are

performed to confirm the desired target based on characteristic neuronal firing patterns [Figure 5]. If MERs do not confirm appropriate placement, a new tract is made to help optimize electrode position. The location of this tract is typically offset by 2mm from the original tract and depends on the MERs and the neurosurgeon's knowledge of the surrounding anatomy. Only after MERs have been optimized and the most suitable location has been mapped is the electrode implanted. Across multiple centers, the average number of MER tracts has been reported to be 2.3 for each implanted electrode.^{8,9} After the DBS electrode has been placed into the desired deep brain target, it is subjected to intraoperative test stimulation in order to confirm therapeutic efficacy and ensure that there are no associated side effects. If a second electrode is to be implanted, this process is repeated. With both electrodes in their final location, the ends of the wires are capped and tunneled under the skin to a point behind the patient's ear. In a review of the literature, the mean operating room time for a unilateral DBS implantation was reported to be 223.83 minutes: and 279.79 minutes for simultaneous bilateral implantation.¹⁰

The second stage of the procedure consists of connecting the intracranial electrode wires to an implantable pulse generator. This portion of the procedure is always performed under general anesthesia, and may be performed either on the same day as the first stage, or in a delayed fashion as an outpatient procedure.

DBS VERIFIED BY INTRAOPERATIVE IMAGING

Over the past several years, a growing number of centers have started to offer DBS surgery under general anesthesia – or "asleep" DBS. The main premise of this approach is that MRI technology is now capable of clearly identifying the anatomy of the deep brain target; and that intraoperative imaging can be used to verify the location of the DBS lead in this target. As such, both MRI¹¹⁻¹³ and CT¹⁴⁻¹⁷ have been used to accomplish the necessary task of image verification in "asleep" DBS. Although intraoperative MRI allows for direct visualization of the electrode



Figure 5

Dr. Ashwini D. Sharan inserts the DBS electrode into its final position after verifying its optimal position with microelectrode recordings. Macrostimulation will then be used to test for therapeutic effect and rule out side effects from stimulation.



Figure 6

Dr. Chengyuan Wu performs an "asleep" DBS surgery in which the final electrode position is confirmed with intraoperative imaging.

without the need for image fusion, the use of intraoperative CT has been found to be safe and accurate as well.¹⁸

At our institution, the trajectory to the desired target is once again planned

on a T2 weighted or proton density (PD) MRI as well as on volumetric (1cm³ voxel) T1 weighted gadoliniumenhanced MRI. The first stage of the procedure similarly starts with

placement of a stereotactic (Leksell) frame under local anesthesia. After a reference CT is acquired with the frame on the patient, this image is merged with the MRI containing the stereotactic plan. Again, this step allows for the calculation of the stereotactic Leksell frame coordinates or robotic (Renishaw Neuromate) arm position, which defines the planned trajectory in real space. In the operating room, the patient is placed under general anesthesia and positioned in a supine position with the head fixed to the operating room table or to the stereotactic robot. The intraoperative CT (Medtronic O-Arm) is also brought into position around the surgical field. Incisions are made in the scalp and 2mm twist drill holes are drilled into the skull [Figure 6]. After the dura has been opened sharply and with cauterization, a radiofrequency probe is passed down the planned trajectory in order to measure impedances, which helps to confirm a target in gray matter. The electrode is implanted at this location and secured in place to the skull. The same process is repeated for the second electrode before an intraoperative CT scan is acquired. Before closing the incisions, this intraoperative image is merged back to the original plans and the accuracy of electrode placement is critically assessed. Only if the electrode is within the intended deep brain nucleus and within 2mm of its intended trajectory is it considered to be in an appropriate position. This verification step is critical and systematic analysis of targeting errors permits development of strategies to improve surgical accuracy and precision during subsequent procedures.¹⁹

With both electrodes in their final location, the wires are tunneled under the skin to a point behind the patient's ear. The second stage of the procedure consists of connecting the intracranial electrode wires to an implantable pulse generator, which is usually performed on the same day.

EQUIVALENCE BETWEEN TECHNIQUES

Clinical Outcomes

In a large multicenter study performed in the UK and published in 2010, 366

patients with Parkinson's disease across 13 centers were randomized to surgery and best medical therapy or to best medical therapy alone. They found that there was a significant improvement in quality of life ratings, specifically with mobility, activities of daily living, and bodily discomfort in patients that received surgical intervention in addition to medical therapy.²⁰ Specifically, patients who underwent MER-guided DBS for Parkinson's disease have demonstrated a 26-33% improvement in UPDRS-III motor scores after 6 months.^{12,21,22} Furthermore, these effects are long lasting with substantial benefits for symptoms such as tremor, rigidity, and motor complications; whereas other symptoms of akinesia, axial signs, and cognition often continue to deteriorate as part of the natural progression of the disease.23-25

The outcomes in patients undergoing "asleep" DBS has certainly been comparable, with patients experiencing a 40-66% improvement in UPDRS-III motor scores after 6 months.15,26,27 Similarly, 41 patients who underwent "asleep" STN DBS continued to demonstrate significant reduction of motor fluctuations, dyskinesias, and demands in dopaminergic medications at 5 years after implantation; however axial symptoms and bradykinesia continued to worsen as part of disease progression.²⁸ A direct comparison between the two approaches was performed by Saleh et al, who performed a retrospective review in which they compared 14 patients who underwent DBS placement under general anesthesia to 23 patients who underwent DBS placement while awake with MER. After 6 months of therapy, both groups showed statistically similar reductions in levodopa equivalent dosages.29

Associated Costs

A 2011 review of literature to date suggested that MER doubled, or even tripled, the cost of DBS implantation compared to surgery performed without MER.¹⁰ Given its retrospective nature, however, this study compared costs across multiple centers and was limited to the reported costs associated with the surgery itself. More recently, a single center study from Oregon Health and Science University reported no significant difference in cost between "awake" (\$40,052 \pm \$6,604)

and "asleep" ($33,850 \pm 4,830$) DBS when they compared 53 "awake" to 158 "asleep" procedures performed over a 5 year span at their institution.³⁰ While they reported a lower variation in procedural costs, it is important to note that this study also include all costs incurred both 30 days before and after surgery.

BENEFITS OF "AWAKE" DBS

Use of MER in an awake patient for DBS implantation certainly has a tried and true track record. It can be performed reliably even when the borders of intended deep brain target cannot be directly visualized. While clinical MR scanners are generally capable of imaging many of these targets, expertise in both MR physics and the surgical technique of DBS are necessary to establish protocols for the necessary image sequences. Furthermore, not all clinical targets are yet visible on clinical MR scanners-the borders of the ventral intermediate nucleus (Vim) of the thalamus still cannot be clearly distinguished. In such scenarios, the use of MERs increases the accuracy of DBS electrode placement.^{31,32} Even when the borders of the target, such as the subthalamic nucleus (STN) or globus pallidus pars interna (GPi), can be clearly seen, some have pointed out that the subregion of the sensorimotor region of this nucleus cannot be visualized and discerned from the cognitive and limbic regions of the nucleus.33

Another major benefit of "awake" DBS is the ability to perform intraoperative stimulation testing. The ability to immediately confirm the therapeutic efficacy of stimulation as well as ensure the absence of no side effects can certainly be reassuring not only for the neurosurgeon, but also for the patient undergoing the procedure. Finally, by having the procedure performed awake, the risks of undergoing general anesthesia are completely eliminated. It is for these reasons that many centers continue to perform DBS in this manner.

BENEFITS OF "ASLEEP" DBS

Increased Patient Comfort

While intraoperative testing provides immediate feedback, the time requirement of both MERs and stimulation testing for which the patient must be awake can be challenging for patients, who can fatigue, lose concentration, and in doing so, potentially reduce the reliability of this intraoperative testing.³⁴ In contrast, "asleep" DBS is associated with increased patient comfort, reduced anxiety, less back pain, and fewer anesthetic concerns about respiratory difficulties.^{19,35,36} In addition, since no intraoperative neurophysiologic or clinical testing is being performed there is no need to force the patient to an OFF-state; and the lack of complete levodopa reduces tremor severity, painful "off" dystonia or rigidity, "off" anxiety, and confusion for the patient.19,27,35,36 The result of all of these factors is more rapid mobilization after surgery and a overall shorter recovery period. Lastly, although more difficult to interpret than in awake patients, MERs can even be performed during "asleep" surgery and has been reported by a few institutions.^{34–36}

Shorter Operating Time

In eliminating the need for intraoperative recording and testing, "asleep" DBS also tends to offer shorter surgical times. As greater comfort and experience is gained with this technique, operative times have improved.²⁹ In a retrospective analysis, surgical time was reduced by an average of 175 minutes if a single electrode was implanted without MER.¹⁰ Such a reduction of the duration which a patient must remain on an operating room table has been suggested to decrease the risk of venous thrombosis and pulmonary embolism.³⁴ In addition, shorter surgical times may be related to patient comfort factors mentioned in the previous section.

Increased Accuracy

If MR imaging is not, or cannot be, optimized for a particular deep brain target, the surgeon must rely on ventricular landmarks, prior knowledge based on established atlases, and MER to identify the appropriate location for electrode implantation. Such indirect imaging methods have led to the initial track being used in 70% of cases and an average of 2.3 tracts per implanted electrode.^{8,9,37} In comparison, a single brain penetration is sufficient in 87-95% of patients undergoing MRI-guided and MRI-verified DBS; with only one additional track was required in the remainder.^{37,38}

During DBS surgery under general anesthesia, it has been theorized that the positive-pressure ventilation increases intracranial pressure, which to some extent reduces brain shift. In addition with meticulous entry planning on a gyrus and shorter surgical times are felt to reduce egress of cerebrospinal fluid and pneumocephalus, which further reduces stereotactic inaccuracy from brain shift.³⁹ In our practice, we feel that we further reduce these deleterious factors by keeping the patient supine and by drilling only a 2mm twist drill hole.

In published series of "asleep" DBS to date, the mean deviation of the implanted electrode when compared to the intended trajectory is only 1.2mm.14,15,40 While advocates of MER may argue that this low deviation supports precision and not necessarily accuracy, current experience has also shown that the site of best MER activity does not necessarily correlate with best clinical response during intraoperative testing or long-term outcome.41,42 Furthermore, in the setting of improved perioperative imaging, there exists no evidence that MER help prevent suboptimal electrode placement.^{10,43-46} In fact, cases of mistaking the recordings of the red nucleus for STN highlight the false sense of security that MER can provide.47

Reduced Risk of Intracranial Hemorrhage

One of the main arguments for DBS to be performed without MER is that there is an increased risk of intracranial hemorrhage with increased brain penetrations.31,48 In a 2011 meta-analysis of 109 studies comprising 6,237 patients and 9,890 trajectories to deep nuclei, the estimated per-trajectory intracerebral hemorrhage (ICH) rate was 1.57% with an estimated mortality rate per trajectory was of 0.14%. The use of MER and multiple trajectories to deep nuclei were both positive predictors of increased ICH risk.^{49,50} As illustrated above, the image-guided image-verified electrode implantation is associated with fewer brain penetrations, which contributes to reducing the associated risk of ICH. When evaluated separately, the overall incidence of ICH in functional neurosurgery has been reported to be 5.0%, with asymptomatic hemorrhage in 1.9% of patients, symptomatic hemorrhage in 2.1% and hemorrhage resulting in permanent deficit or death in 1.1%. In comparison, in 214 patients undergoing

image-guided DBS without MER, Zrinzo et al reported a total incidence of ICH of was 0.9%, with asymptomatic in 0.5% of patients, symptomatic hemorrhage in 0.5%, and hemorrhage resulting in permanent deficit in 0.0% of patients.⁵⁰ Overall this equates to a four to five fold increase in hemorrhage risk in awake surgery performed with MER.

CONCLUSION

Despite the significant differences between these two techniques outlined above, their clinical outcomes and procedural costs to date have been largely the same. While the benefits of neurophysiologic and clinical confirmation advocate for "awake" DBS, the advantages of greater patient comfort, decreased operating time, increased accuracy, and reduced hemorrhagic complications support "asleep" DBS. As such, it is important to discuss these factors with patients considering DBS surgery. Each approach has its own advantages and disadvantages that must be weighed with patient-specific factors, concerns, and preferences.

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