

18 **ABSTRACT**

19 Reference point indentation (RPI) has emerged as a novel tool to measure material-level
20 biomechanical properties *in vivo*. Human studies have been able to differentiate fracture versus
21 non-fracture patients while a dog study has shown the technique can differentiate drug
22 treatment effects. The goal of this study was to extend this technology to the *in vivo*
23 measurement of rats, one of the most common animal models used to study bone, with
24 assessment of intra- and inter-animal variability. Seventy-two skeletally mature male Sprague-
25 Dawley rats were subjected to *in vivo* RPI on the region between the tibial diaphysis and
26 proximal metaphysis. RPI data were assessed using a custom MATLAB program to determine
27 several outcome parameters, including first cycle indentation distance (ID-1st), indentation
28 distance increase (IDI), total indentation distance (TID), first cycle unloading slope (US-1st), and
29 first cycle energy dissipation (ED-1st). Intra-animal variability ranged from 13-21% with US-1st
30 and Tot Ed 1st-L being the least variable properties and IDI the most highly variable. Inter-
31 animal variability ranged from 16% (US-1st) to 25% (ED-1st and IDI). Based on these data, group
32 size estimates would need to range from 9-18/group to achieve sufficient power for detecting a
33 25% difference in a two-group experiment. Repeat tests on the contralateral limb of a small
34 cohort of animals (n=17) showed non-significant differences over 28 days ranging from -6% to -
35 18%. These results provide important data on RPI variability (intra- and inter-animal) in rats that
36 can be used to properly power future experiments using this technique.

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39 INTRODUCTION

40 Assessment of biomechanical properties has long been confined to pre-clinical studies and,
41 more specifically, ex-vivo mechanical tests. Recent technology, termed reference point
42 indentation (RPI), has made it possible to assess biomechanical properties *in vivo* (Hansma et
43 al., 2008). *In vivo* studies have shown that RPI can differentiate between patients who have
44 fractured versus non-fracture patients (Diez-Perez et al., 2010) as well as patients who have
45 been treated with bisphosphonates versus those who were treatment naïve (Güerri-Fernández
46 et al., 2012). *In vivo* testing of dogs has shown RPI can differentiate raloxifene treatment from
47 controls after six months of clinically relevant dosing (Aref et al., 2013). In addition, a related
48 device (Osteoprobe) that operates using slightly different technology revealed significant
49 differences in the material properties of patients with diabetes versus healthy controls (Farr et
50 al., 2014). Collectively, these data show promise for RPI technology to allow minimally invasive
51 measures of material-level biomechanical properties.

52 Rodents represent the most commonly used animal model to study bone and are often
53 the model first used to evaluate novel interventions (Kalu, 1991; Thompson et al., 1995).
54 Although several studies have assessed biomechanical properties of rodent bone *ex vivo*, there
55 have been no reports of *in vivo* assessment of rodents. The goal of this study was to determine
56 the intra- and inter-animal variability, as well as the variability over time (in order to understand
57 potential variability that might occur in control animals in future intervention studies), for *in vivo*
58 measures with RPI in skeletally mature rats. These data will be essential to understand the
59 practicality of the technique for use in rats as well as to provide variability data to help design
60 adequately powered experiments.

61 METHODS

62 *Experimental design*

63 Seventy-two skeletally mature male (6 month old) Sprague Dawley rats were purchased
64 (Harlan) and acclimatized for one week prior to reference point indentation (RPI) testing. A
65 subset of animals (n=17) underwent a second RPI test session 28 days after the first test.
66 These repeat test sessions were performed on the contralateral limb to avoid any local tissue
67 damage caused by the first test session. Following each testing session, animals were returned
68 to their cages. These animals were part of a larger experiment that is outside the scope of this
69 current report. All procedures were approved by the Indiana University School of Medicine
70 Animal Care and Use Committee prior to the start of the study.

71 *Reference point indentation (RPI)*

72 Material-level mechanical properties of the anterior surface of the tibial cortex were assessed *in*
73 *vivo* using RPI (Biodent Hfc, Active Life Scientific, Santa Barbara, CA). This site was chosen as
74 it has been utilized previously in human and dog *in vivo* studies, and its limited soft tissue
75 coverage facilitates easy access to the bone surface. The cortical thickness in this region is
76 around 4 mm thick. Rats were placed under general anesthesia using inhalation isoflurane, and
77 a local anesthetic was injected just beneath the skin in the region of testing. Skin overlying the
78 region was pierced with a sterile BP1 probe contained within the measurement head unit (MHU)
79 attached to a modified holder apparatus (**Figure 1**). The MHU was lowered vertically, normal to
80 the surface of the bone, until the probe assembly rested on the bone surface. As opposed to
81 previous *in vivo* work in humans and dogs, we did not scrape the periosteum prior to testing due
82 to challenges working in the small target area. Following positioning of the reference probe, a
83 reference force of ~13 Newtons was applied to stabilize the MHU, and the measurement
84 protocol was initiated. Measurements began with a series of four preconditioning cycles (1N
85 force at 5 Hz) followed by a series of 10 testing cycles (10 N at 2 Hz). This force was chosen to
86 match *in vivo* levels used previously in humans and dogs. To achieve our goal of three usable
87 tests for each animal, between three and seven measurements, within a few mm of each other,

88 were collected. For the multiple tests on each animal an average was taken for a given
89 parameter and that data-point was used to compare that parameter across animals. All animals
90 were conscious and mobile ~10 minutes post-testing. There was no sign of post-test pain or
91 discomfort as assessed by visual inspection of animals during normal cage activity.

92 Raw data output from the RPI analysis software (version 2.0) were imported into a
93 customized MATLAB code (Mathworks) (Aref et al., 2013). Primary variables of interest from the
94 MATLAB program include first cycle indentation distance (ID-1st), which represents the depth
95 the probe penetrated on the initial cycle; first cycle energy dissipation (ED-1st), which represents
96 the energy dissipated in the first cycle; first cycle unloading slope (US-1st) which represents
97 material stiffness (damage modulus) for the first cycle; indentation distance increase (IDI), which
98 represents the penetration depth between the first and 10th cycle; total indentation distance
99 (TID),) which represents the distance from the bone surface to the depth of penetration after the
100 10th cycle; and total energy dissipation (Tot ED) which represents the total energy dissipation
101 summed over all 10 cycles (**Figure 1**). Our previous work has shown that parameters analyzed
102 by the MATLAB software that were also generated by the manufacturer software yielded
103 correlation coefficients of >0.96 (Aref). The advantage of the MATLAB program over the
104 manufacturer software is that additional data, specifically cycle-by-cycle and energy data are
105 generated.

106 *Data Analyses*

107 Intra-animal variability was assessed by calculating the coefficient of variation (CV) for all tests
108 within an animal. Inter-animal variation was assessed by calculating CVs for each outcome
109 parameter across all animals. Paired t-test analyses were used to compare baseline and 28
110 day data.

111 **RESULTS**

112 A total of 319 tests were conducted in the 72 animals. Of these, 49 tests were deemed
113 unsuccessful during testing based on the operators noting various problems with the tests.
114 These included the test having a negative IDI (probe final position is above original reference
115 position), decreasing displacement in first few cycles (resulting in a negative loading slope), or
116 the measurement unit shifting during test. Upon removal of these unsuccessful tests, 71
117 animals had between 2 and 5 measures, and these were used for subsequent analyses (one
118 animal was removed because it had only one acceptable measure).

119 Intra-animal variation of RPI parameters ranged from between 13.3 and 20.6% (**Table 1,**
120 **Figure 2A**). The least variable parameters within animals were US 1st and Tot ED 1st-L, each
121 with a coefficient of variation of 13%. The most variable parameter within animals was IDI a CV
122 of 20.6%. Inter-animal variation ranged from 16-25% (**Table 2, Figure 2B**). The least variable
123 parameter among animals was US-1st (CV = 16%), while both ED-1st and IDI had the largest
124 CVs of 25%.

125 One month following the initial RPI tests, a subset of animals (n=17) underwent a
126 second RPI test on the contralateral limb. In this smaller dataset, intra-animal variation ranged
127 from 45-74% with TID and ID-1st being the least variable parameters and US-1st the most
128 variable. The inter-animal variability in this data set ranged from 13-23% with the least variable
129 parameter being US-1st and the most variable being TID and ID-1st (data not shown).

130 Changes between baseline and one month measures were calculated to determine
131 variability over time in untreated animals. All six parameters were, on average, lower at the
132 second measurement relative to the first, with decreases ranging from -6% to -18% (**Table 3**).
133 For each parameter, there was a wide range of responses with some animals increasing, some
134 decreasing, and others unchanged (**Figure 3**). There was no significant difference in any
135 parameter between baseline and day 28.

136 **DISCUSSION**

137 There is significant experimental value in assessing outcome variables *in vivo* yet from the
138 perspective of biomechanical properties this presents unique challenges. Serum/urine
139 biomarkers have long been used to track bone remodeling parameters over time, and recent
140 advances in imaging have allowed for high resolution *in vivo* longitudinal measures of bone
141 density and structure (Bouxsein and Delmas, 2008). These measures allow individual variability
142 to be accounted for in statistical analyses, allowing for the utilization of fewer subjects/animals
143 compared to traditional cross-sectional designs. The development of reference point
144 indentation (RPI) technology has made it possible now to assess material-level biomechanical
145 properties of bone *in vivo* (Aref et al., 2013; Diez-Perez et al., 2010). Although studies have
146 used RPI in rodent bone *ex vivo* (Gallant et al., 2013), no data exists on its *in vivo* application in
147 this animal model.

148 Inter-individual variability of *in vivo* measures on human patients has been reported to be
149 between 15% and 24% for IDI and 10-17% for Total ID (Diez-Perez et al., 2010; Güerri-
150 Fernández et al., 2012). Inter-individual variability of *in vivo* measurements in dogs ranged from
151 5% (US-1st) to 27% (ID-1st and Energy-1st) (Aref et al., 2013). Our current work in rats falls
152 within these same ranges. Because of the larger data set (n=71) and use of inbred rats, inter-
153 individual variability should be lower than previous studies in dogs and humans. One potential
154 explanation for this is size differences. The test is being conducted over a larger percentage of
155 the total bone length in rats compared to dogs and humans and thus may be incorporating more
156 of the natural variability in properties that exist along the length of the bone. The small size also
157 presents challenges to orienting the test set-up that are not of concern in larger test subjects.
158 Alternatively, the lack of periosteum scraping in the rats may increase the variation. Due to the
159 small target region we opted not to scrape periosteum as has been done in dogs and humans. It

160 is also possible that the inherent properties of the microstructure in rat bone are simply more
161 variable than they are in dogs or humans.

162 In an attempt to put the inter-animal variations into context, we calculated CVs for an
163 archived set of untreated rat femoral whole bone three-point bending tests from our laboratory
164 (**Table 4**). These values range from 7-30% for common parameters such as ultimate load,
165 stiffness, and energy to failure, suggesting that RPI tests produce data that fall near the upper
166 range of variability produced by traditional *ex vivo* mechanical tests. Despite its variability,
167 though, RPI is currently the only technique that provides *in vivo* measurements of skeletal
168 material properties in rodents. This is valuable as it would allow for the reduction of animal
169 numbers and, if the effect sizes are sufficient, the detection of changes in mechanical properties
170 over time. For example, in an experimental design of two groups, the number of animals
171 needed to detect, with 80% power, a 25% difference in outcomes based on the inter-animal
172 variation the study would need between 9-18 animals per group at any single time point of
173 measure (**Table 2**).

174 The presented data should be considered within the context of some limitations. As this
175 was the first attempt to extend this *in vivo* technology to rats, refinement in this technique could
176 lower the variation in future studies. Despite our previous experience with *in vivo* testing (Aref
177 et al., 2013), the smaller length scale of the rat, relative to the dog, was challenging. The
178 development of hardware to help standardize position of test locations along the length of the
179 tibia may help reduce intra-individual variability. We also conducted repeated measures on the
180 contralateral limb without knowledge of side-to-side variability in RPI properties. Therefore, we
181 are unable to determine whether decreases in the values of RPI parameters between time
182 points is a product of time (and/or growth) or a product of variability between limbs. Our
183 rationale for not performing repeat tests on the same limb was based on the assumption there
184 would be residual damage (or healing in response to damage) at the 28-day time point. Hence,

185 we aimed to avoid any influence of such damage on the second measure. Whether or not such
186 damage persists remains unknown and should be the focus of future work as testing of the
187 same limb is likely to reduce variability. Previous work on *ex vivo* specimens has shown that
188 lower load values (5N versus 10N) yielded lower viability (Setters and Jasiuk, 2014) thus it's
189 possible that using lower loads *in vivo* would have benefit.

190 In conclusion, we present data on the *in vivo* variability of reference point indentation
191 testing in skeletally mature rats. These data will provide a foundation for designing future
192 studies using this technology by providing the intra-, inter-, and repeated measure variability in
193 measures.

194

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199 **Conflict of Interest statement**

200 The authors have no conflict of interest related to this work.

201 **Table 1.** Intra-animal variation of RPI in skeletally mature male rats

	1st Cycle Indentation Distance (ID 1 st)	1st Cycle Energy Dissipated (ED 1st)	1st Cycle Unloading Slope (US 1st)	Indentation Distance Increase (IDI 1st-L)	Total Indentation Distance (TID 1st-L)	Total Energy Dissipated (Tot ED 1st-L)
Mean CV within animal, %	17.4	14.1	13.3	20.6	16.9	13.4
Standard deviation, %	10.4	10.8	13.0	14.9	10.2	9.3

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203 **Table 2.** Inter-animal variation of RPI in skeletally mature male rats

	1st Cycle Indentation Distance (ID 1st) - μm	1st Cycle Energy Dissipated (ED 1st) - μJ	1st Cycle Unloading Slope (US 1st) - $\text{N}/\mu\text{m}$	Indentation Distance Increase (IDI 1st-L) - μm	Total Indentation Distance (TID 1st-L) - μm	Total Energy Dissipated (Tot ED 1st-L) - μJ
Mean	116	342	0.42	10.68	121	885
Standard deviation	25	86	0.07	2.71	25	206
Coefficient of Variation (CV), %	21	25	16	25	21	23
Animals needed in each of two groups to detect a 25% treatment effect	13	17	9	18	12	15

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206 **Table 3.** Percent difference of RPI parameters between baseline and 28-day test sessions.

	1st Cycle Indentation Distance (ID 1st)	1st Cycle Energy Dissipated (ED 1st)	1st Cycle Unloading Slope (US 1st)	Indentation Distance Increase (IDI 1st-L)	Total Indentation Distance (TID 1st-L)	Total Energy Dissipated (Tot ED 1st-L)
MEAN, %	-6	-9	-13	-13	-7	-18
SD	36	30	29	42	35	34

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209 **Table 4.** Inter-animal variability of traditional mechanical properties assessed by 3 point

210 bending.

	Ultimate Force (N)	Displacement to Yield (mm)	Postyield Displacement (mm)	Total Displacement (mm)	Stiffness (N/mm)	Work to Yield (mJ)	Postyield Work (mJ)	Total Work (mJ)
Mean	230	447	305	752	510	41	64	105
Standard deviation	21	61	91	52	47	9	17	13
Coefficient of Variation (CV), %	9	14	30	7	9	22	27	13

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215 **Figure Legends.**

216 **Figure 1.** *In vivo* testing set up and outcome parameters for RPI in skeletally mature rats. (A)

217 The animals lower limb was flexed at the knee joint and placed on an elevated support
218 so that the proximal tibial plateau was perpendicular to the testing probe. The foot was
219 secured in place at the ankle and then a series of 10 cyclic indents were initiated where
220 the test probe penetrates to a force of 10 N and then retracts. (B) Following the first
221 cycle of the cyclic test, key outcomes of 1st cycle indentation distance (1st cycle ID), 1st
222 cycle unloading slope (1st cycle US) and 1st cycle energy dissipation (1st cycle ED) can
223 be calculated. Additional parameters are obtained after the 10th cycle, including total
224 indentation distance (Total ID), indentation distance increase (IDI) and energy
225 dissipation (Total ED).

226 **Figure 2.** RPI variability within animal and among animals. (A) Intra-animal variation,
227 presented as the mean and standard deviation of the coefficient of variation (%) within a
228 given animal. (B) Inter-animal variation, presented as the CV (%) for each variable
229 across all animals.

230 **Figure 3.** Percent difference of *in vivo* RPI measures taken 28 days apart, on contralateral
231 limbs, in untreated skeletally mature male rats. Box plots represent the median, 10th,
232 25th, 75th and 90th percentiles, as well as those individual data points outside this range.

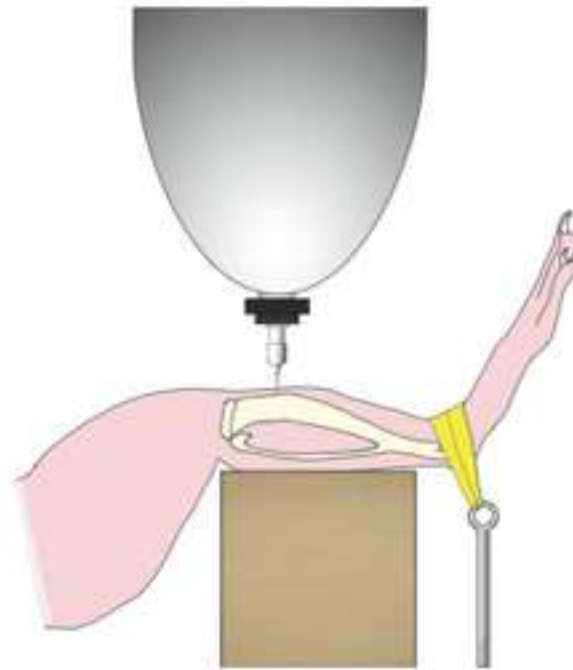
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Figure 1



First cycle

10th cycle

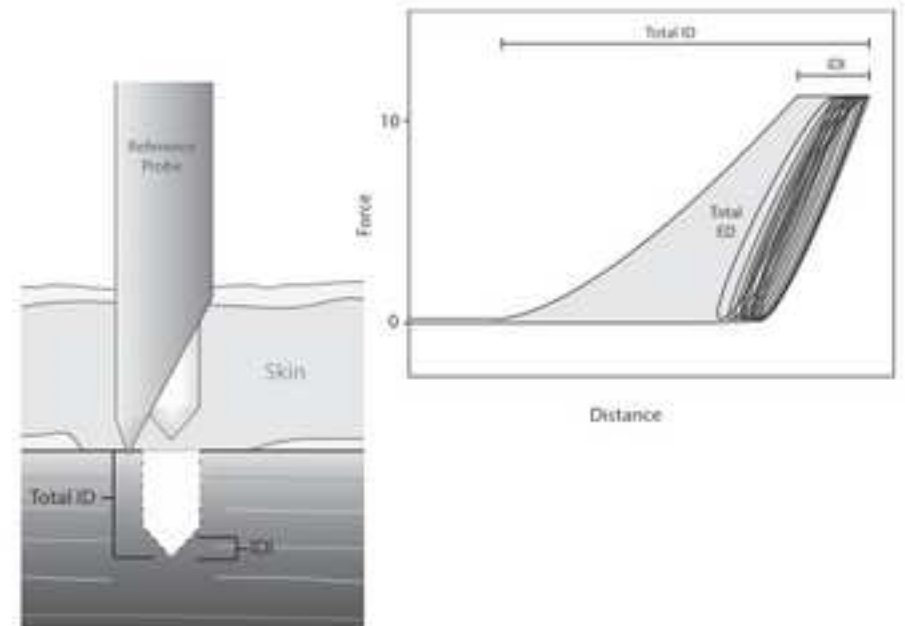
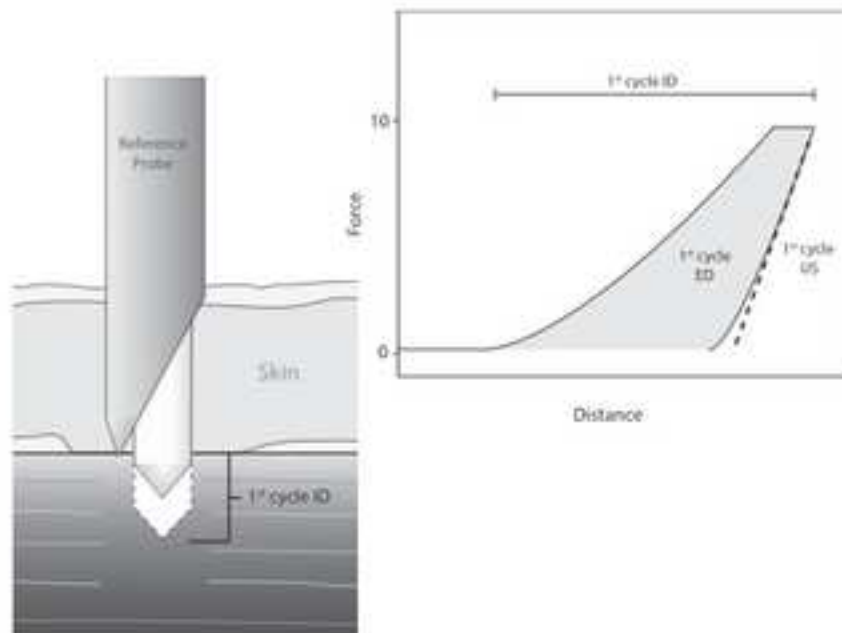


Figure 2

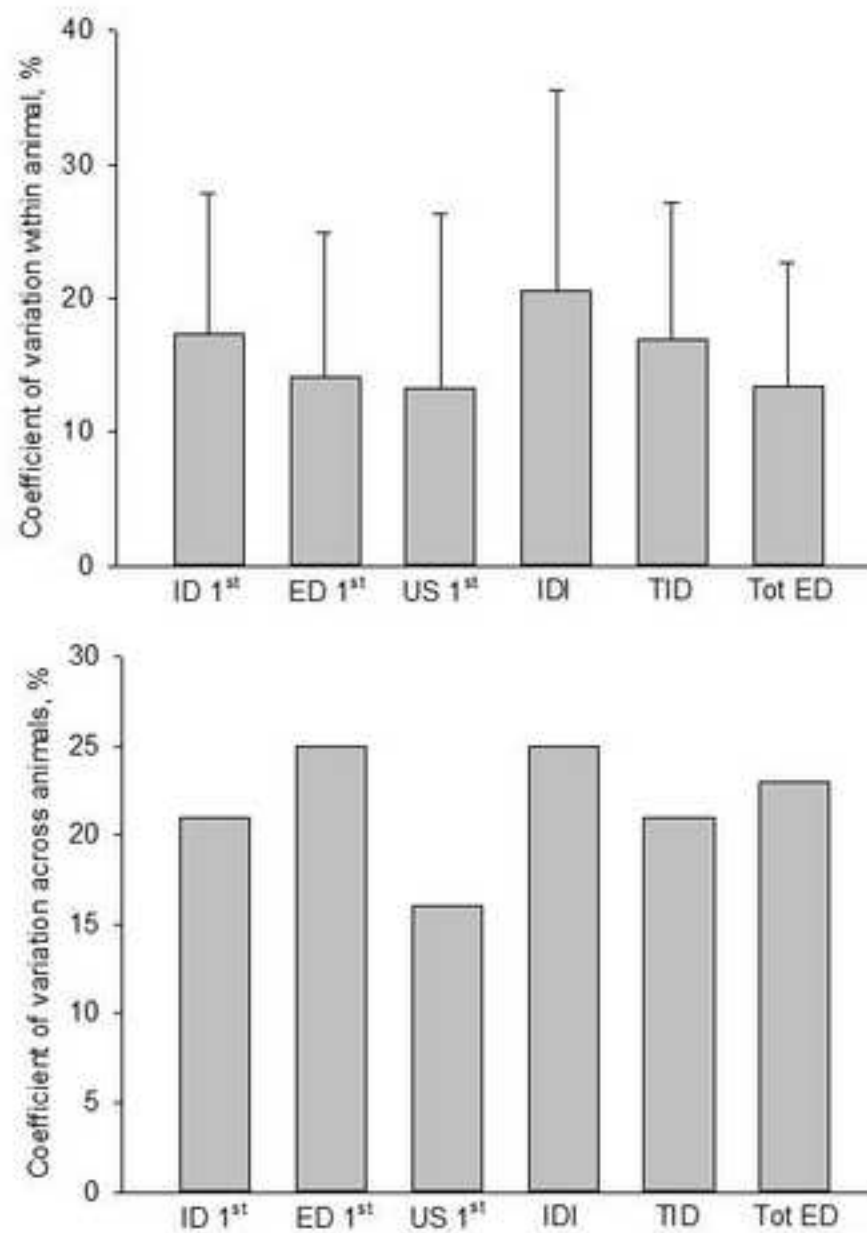
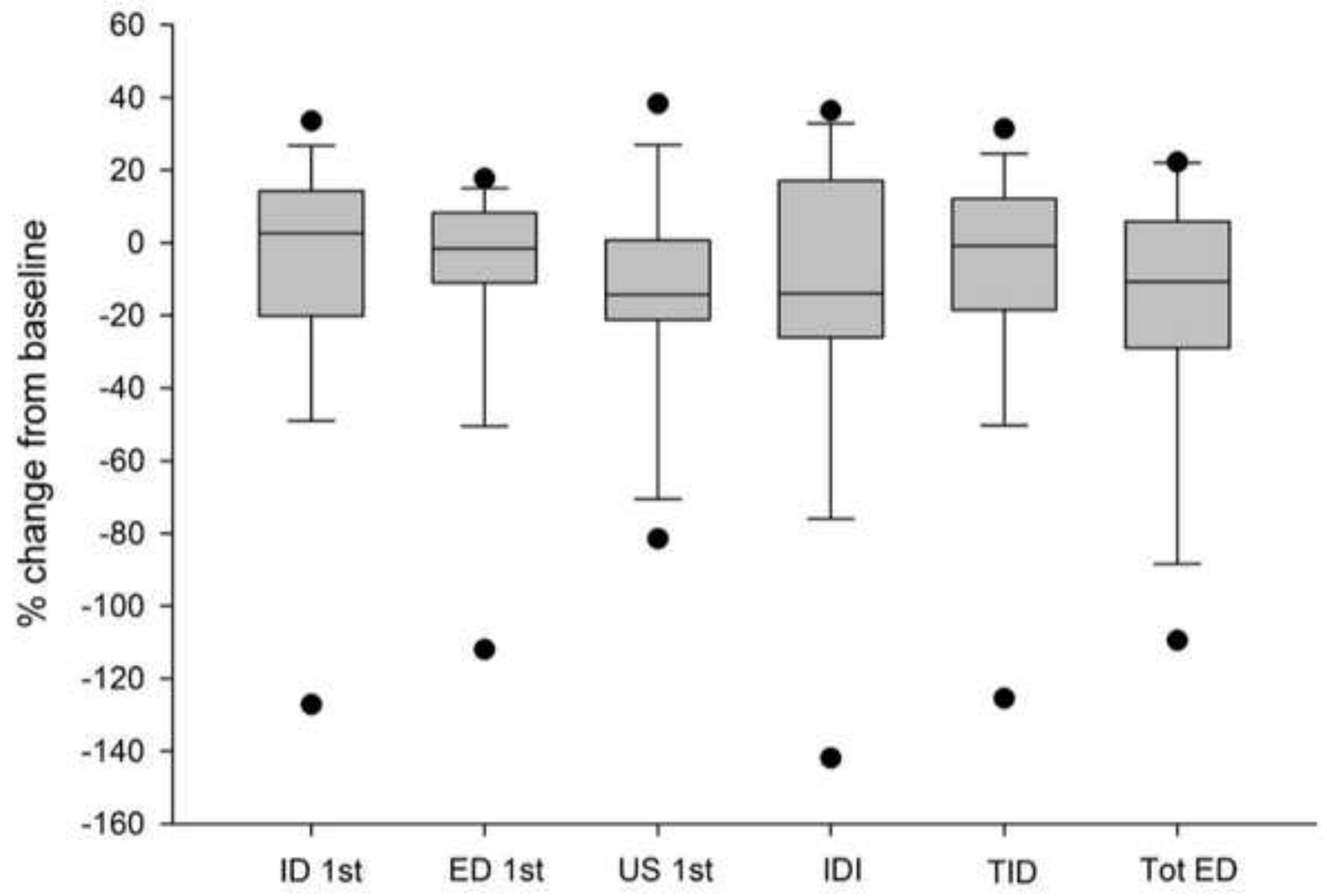


Figure 3



Conflict of Interest statement

The authors have no conflict of interest related to the work described in this manuscript.