

1	DEVELOPMENT AND OPTIMIZATION OF NOVEL ENCAPSULATION STRUCTURES OF
2	INTEREST IN FUNCTIONAL FOODS THROUGH ELECTROSPRAYING
3	Rocio Pérez-Masiá, Jose M. Lagaron, Amparo López-Rubio*
4	Novel Materials and Nanotechnology Group, Institute of Agrochemistry and Food
5	Technology (IATA-CSIC), Avda. Agustin Escardino 7, 46980 Paterna (Valencia), Spain
6	
7	*Corresponding author: Tel.: +34 963900022; fax: +34 963636301.
8	E-mail address: <u>amparo.lopez@iata.csic.es</u> (A. Lopez-Rubio)
9	Novel Materials and Nanotechnology Group, Institute of Agrochemistry and Food
10	Technology (IATA-CSIC), Avda. Agustin Escardino 7, 46980 Paterna (Valencia), Spain
11	Other e-mail addresses: rocio.perez@iata.csic.es (R. Pérez-Masiá)
12 13	lagaron@iata.csic.es (J.M. Lagaron)
14	
15	
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1 Abstract

2 The aim of this work was to establish strategies for the development of electrosprayed 3 encapsulation structures, of interest in food applications, based on aqueous hydrocolloid 4 dispersions. Specifically, various polysaccharides and two different proteins were evaluated for 5 capsules formation. To this aim, the hydrocolloid dispersion properties were analysed and 6 compared with the solution properties of two polymers readily spinnable in water (PVOH and 7 PEO). Increasing the hydrocolloid concentration to promote chain entanglements resulted in a 8 valid strategy only for a few matrices (related to their greater Mw). As alternative strategies to 9 improve the physical properties and, thus, the sprayability of the dispersions, addition of gums 10 and surfactants to modify their viscosity and surface tension, respectively, was evaluated. 11 Moreover, denaturation of proteins was also carried out in order to investigate the effect of 12 this treatment on the electrospraying process and on capsules formation. Results showed that 13 the incorporation of some of these molecules, as well as protein denaturation, significantly 14 changed the physical properties, allowing the development of encapsulation structures from 15 all the hydrocolloids assayed. The morphology of the structures obtained was characterized 16 and the molecular organization of some of the capsules was studied and related to the 17 electrosprayability and capsules morphology.

18 Keywords: electrospinning, electrospraying, encapsulation, hydrocolloids, bioactives

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1 1. Introduction

The encapsulation of food and nutraceutical ingredients is an emerging area of interest due to the instability of some of these compounds at ambient and digestive conditions (Ezhilarasi et al. 2013). In general, encapsulation seeks to protect these products and, thus, assure their health-promoting properties, although it can also be used to improve sensorial properties of food products containing ingredients that inherently have undesirable flavours and/or odours (Nasirullah et al. 2011).

8 Apart from the conventional microencapsulation techniques, such as spray drying or 9 coarcervation, electrohydrodynamic processes have been recently suggested to be simple and straightforward methods to generate submicron encapsulation structures for a variety of 10 bioactive molecules (Xie et al. 2008; Lopez-Rubio and Lagaron 2012; Bock et al. 2012; Pérez-11 12 Masiá et al. 2013, Bakhshi et al. 2013). These techniques use electrostatic forces to produce 13 electrically charged jets from viscoelastic polymer solutions which on drying, by the evaporation 14 of the solvent, produce ultrathin structures (Li and Xia 2004). When ultrathin continuous fibres 15 are obtained, the process is called "electrospinning". When size-reduced capsules are attained, the process is normally referred to as "electrospraying" due to the non-continuous nature of 16 the structures obtained. For food and nutraceutical applications, capsules are generally 17 18 preferred, since apart from facilitating handling and subsequent incorporation into different 19 products, they also present greater surface/volume ratio and, thus, are expected to have better release profiles than fibres (Hong et al. 2008). The morphology and composition of 20 21 micro/nanostructures attained can be modulated through controlling the process parameters, 22 mainly the operational conditions (the high voltage applied, the distance between the spinneret 23 and the collector and the feeding rate), the solution properties (the viscosity, the surface tension and the electrical conductivity), and the material of choice. Specifically, for food and 24 25 nutraceutical applications, the encapsulating material should be suitable for human 26 consumption. Moreover, although during the electrospraying process the solvent should be

completely evaporated, it may be convenient to only make use of allowed food contact solvents
 in order to avoid toxicity problems, as it has been proven that a certain amount of solvent can
 remain in the electrospun structures (Aceituno-Medina et al. 2013).

4 Electrospraying from aqueous solutions, apart from not generating toxicity problems, has the 5 advantage of being beneficial from an environmental point of view. However, the use of water 6 further complicates electrospraying due to the ionization of water molecules at high voltages in an air environment, which may cause corona discharge. Besides, aqueous solutions present 7 8 high surface tension values which hinder the formation of stable jets during the process. 9 Nevertheless, it is possible to obtain micro- and nanocapsules through electrospraying from aqueous solutions using some biopolymers such as polyvinyl alcohol (PVOH) or polyethylene 10 11 oxide (PEO). These biopolymers have been already used for capsules formation through 12 electrohydrodynamic processes, mainly for pharmaceutical and medical applications (Sridhar et 13 al. 2011; Zamani et al. 2013). However, for the incorporation of the micro/nanocapsules within 14 food matrices, the use of food hydrocolloids as encapsulating matrices is highly preferred, not 15 only for achieving a better integration of the capsules in the foodstuffs, but also to improve 16 assimilation of the capsules from the consumers. The use of food hydrocolloids further 17 complicates the electrospraying process, since these materials are usually low molecular weight 18 polymers which do not generate sufficient viscosity and that generally have strong inter- and 19 intramolecular forces, which need to be somehow counteracted to promote capsule formation 20 (Nagarajan et al. 2007; Stijnman et al. 2011).

In this work, a thorough study about the electrospraying of different food hydrocolloids from aqueous solutions has been carried out. Specifically, various polysaccharides, such as dextran, maltodextrin, a resistant starch, pullulan and fructooligosaccharides (FOS), and two proteins (a whey protein concentrate from milk and a soy protein isolate) were evaluated as matrix materials. To this aim, different hydrocolloid aqueous solutions were prepared, characterized and compared with the physical properties of aqueous solutions made from spinnable polymers

in water (specifically, PVOH and PEO). Specifically, the viscosity, surface tension and electrical 1 conductivity of the solutions were evaluated. Afterwards, the physical properties of the 2 3 solutions were optimized for the electrospraying process through the incorporation of different 4 substances. Particularly, the influence of gums on the solution viscosity and the effect of 5 surfactant addition on the surface tension values were studied when capsules could not be 6 attained from the neat hydrocolloidal solutions. Moreover, denaturation of the proteins was also carried out in order to understand how this change in molecular conformation affected 7 8 capsules formation. The morphology of the structures attained was analysed through scanning 9 electron microscopy (SEM) and the molecular organization of the capsules was studied through attenuated total reflectance infrared spectroscopy (ATR-FTIR). 10

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12 2. Materials and methods

13 2.1. Materials

14 PVOH was kindly donated by Plásticos Hidrosolubles (Spain). The commercial resistant starch 15 was Fibersol[®] (www.fibersol.com) commercial grade, manufactured by ADM/Matsutani (lowa, USA). The fructooligosaccharides (FOS) used were Fibruline Instant (FI) and Fibrulose F97, which 16 were kindly donated by InnovaFood S.L (Spain). Whey protein concentrate (WPC) was kindly 17 18 donated by ARLA (ARLA Food Ingredients, Viby, Denmark). Under the commercial name Lacprodan® DI-8090, the composition per 100 g of product consisted of ~80 g of protein, ~9 g of 19 20 lactose, and ~8 g of lipids, the rest being water and minerals like sodium and potassium. Soy 21 protein isolate (SPI) was donated by The Solae Company (Switzerland). Guar gum was 22 purchased at Capers Community Markets (Canada). PEO, dextran, maltodextrin (DE 16.5-19.5), pullulan, Xanthan gum, Span-20 and folic acid were supplied by Sigma-Aldrich (Spain) and they 23 24 were used as received, without further purification.

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1 2.2. Preparation of the hydrocolloid dispersions

The biopolymers (PVOH and PEO) and the SPI dispersions were prepared by dissolving 5, 10 or (w/v) of the polymers in distilled water. When higher concentrations of these materials were used, very dense dispersions were obtained, which were difficult to characterize. The rest of the food hydrocolloid dispersions (dextran, resistant starch, FOS, maltodextrin, pullulan and WPC) were prepared by dissolving 10, 20 or 40% (w/v) of the hydrocolloids in distilled water. (w/w) of gums and/or 5% (w/w) of surfactant respect to the polymer weight were added when needed.

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10 2.3. Characterization of the dispersions

The apparent viscosity (ηa) of the polymeric dispersions at 100 s⁻¹ was determined using a rotational viscosity meter Visco Basic Plus L from Fungilab S.A. (San Feliu de Llobregat, Spain) using the Low Viscosity Adapter (LCP) spindle. The surface tension of the dispersions was measured using the Wilhemy plate method in an EasyDyne K20 tensiometer (Krüss GmbH, Hamburg, Germany). The conductivity of the dispersions was measured using a conductivity meter XS Con6 (Labbox, Barcelona, Spain). All measurements were made in triplicate at 25°C.

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18 2.4. Electrospraying process

The electrospraying apparatus, equipped with a variable high-voltage 0-30 kV power supply, 19 20 was a Fluidnatek[®] basic setup assembled and supplied by Biolnicia S.L. (Valencia, Spain). Details 21 about the basic electrospraying setup can be found elsewhere (Torres-Giner et al. 22 2010). Dispersions were introduced in a 5 mL plastic syringe and were electrosprayed under a 23 steady flow-rate using a stainless-steel needle with internal diameter 0.9 mm. The needle was 24 connected through a PTFE wire to the syringe. The syringe was lying on a digitally controlled 25 syringe pump while the needle was in horizontal towards a stainless-steel plate attached to a 26 copper grid used as collector. The experiment was carried out at ambient conditions (20ºC and

40% RH). The conditions for obtaining the capsules were modified depending on the polymer
used. Basically, the flow rate was set from 0.1 to 0.15 mL/h. Specifically, the flow rate was set at
0.1 mL/h for FOS dispersions and 0.15 mL/h for the rest of the hydrocolloid dispersions. The
voltage varied from 9 to 16 kV and the distance between the tip and the collector varied from 9
to 20 cm.

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7 2.5. Scanning electron microscopy (SEM)

8 SEM was conducted on a Hitachi microscope (Hitachi S-4100) at an accelerating voltage of 10 9 KV and a working distance of 12-16 mm. The capsules were sputtered with a gold-palladium 10 mixture under vacuum before their morphology was examined using SEM. Capsule diameters 11 were measured by means of the Adobe Photoshop CS3 extended software from the SEM 12 micrographs in their original magnification.

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14 2.6. Attenuated total reflectance infrared spectroscopy (ATR-FTIR)

ATR-FTIR spectra were collected at 25°C in a FTIR Tensor 37 equipment (Bruker, Germany). The spectra were collected in the different materials by averaging 20 scans at 4 cm⁻¹ resolution. The experiments were repeated twice to verify that the spectra were consistent between individual samples.

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20 2.7. Statistical analysis

Statistical analysis of data was performed through analysis of variance (ANOVA) using
Statgraphics Centurion XV (Manugistics Corp., Rockville, MD). Homogeneous sample groups
were obtained by using LSD test (95% significant level).

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3. Results and Discussion

2 3.1. Characterization and comparison between PVOH and PEO vs. food hydrocolloids dispersion

3 properties and evaluation of their electrosprayability

4 The success of the electrohydrodynamic process strongly depends on the dispersion properties. 5 Thus, the physical properties of the PVOH and PEO polymers and food hydrocolloidal 6 dispersions were analysed and related to their electrospinnability/electrosprayability. The 7 morphology of the structures obtained was also investigated. Table 1 shows the viscosity, the surface tension, the electrical conductivity and the electrospinnability of the different 8 9 dispersions prepared. This table also shows the capsule's morphology and the capsule's average 10 size in the cases where it was possible to electrospun/electrospray the dispersions. Generally, it 11 was observed that the solutions containing the high molecular weight polymers (PVOH and PEO) had higher viscosities and lower surface tension values than the hydrocolloid-based 12 13 dispersions and both conditions favoured the electrospinning process. These physical properties 14 made that either capsules or fibres were attained from the different polymer solutions assayed. 15 Regarding the aqueous hydrocolloidal dispersions, it was seen that only a few of them had the 16 capacity of forming encapsulation structures through electrospraying. Specifically, only the 17 hydrocolloids which presented a higher molecular weight and, thus, led to a significant viscosity 18 increase when increasing the hydrocolloid concentration in the dispersion, were able to form capsules. These results can be explained on the basis of dispersion properties in relation with 19 20 the electrospinning/electrospraying process. On one hand, it is well-known that 21 electrospinning/electrospraying is only achieved when the dispersion viscosity is high enough to 22 produce the necessary polymer entanglements to form the fibres/capsules. On the other hand, 23 the surface tension is also a crucial parameter for the process, since high surface tension values 24 could overcome the electrostatic forces generated by the high voltage applied and the electrical 25 conductivity of the dispersion and, thus, hinder the Taylor cone formation and the subsequent 26 electrospinning/electrospraying process (Bock et al. 2012; Fong et al. 1999). Regarding the

electrical conductivity, it was seen that this parameter did not considerably affect the process
and, for similar viscosity and surface tension values, electrosprayability was not modified at
different conductivity values. Nevertheless, it is worth noting that, if electrical conductivity is
too high, there is too much charge carried by the electrospraying jet, fact that can destabilize
the jet and complicate the process (Bock et al. 2012; Ding et al. 2005).

6 Regarding the capsules morphology it was seen that for PVOH and PEO at low polymer 7 concentrations, beads were formed, while increasing the polymer concentration and, thus, the 8 viscosity, fibres were obtained. This can be explained by an increase in the polymer chain 9 entanglements when the viscosity was higher, which led to the formation of fibres. It is important to note that the chain entanglements also depend on the molecular weight of the 10 11 polymers and, as a result, for similar viscosity values, different morphologies can be attained 12 depending on the polymer used (Bock et al. 2012). Concerning the size of the structures 13 developed, it was observed that a greater size distribution was obtained for the hydrocolloid-14 based capsules. This fact was probably due to the more unfavourable physical properties of 15 these dispersions, which destabilized the electrospraying jet and led to more heterogeneous 16 structures.

Therefore, from Table 1 it was concluded that in order to carry out a stable electrospraying 17 18 process, it was necessary to modify the viscosity and the surface tension of the food 19 hydrocolloid dispersions. Specifically, higher viscosities and lower surface tension values should 20 be attained. Nevertheless, an exception was observed for the SPI dispersion. In this case, it was 21 seen that although its physical properties seemed to be appropriate for capsule development 22 through electrospraying, unstable jetting occurred and encapsulation structures could not be developed from the SPI dispersions. This fact could be related to the globular structure of the 23 soy protein, with strong inter- and intramolecular forces which impeded chain entanglements 24 25 between adjacent molecules needed for capsules formation (Vega-Lugo and Lim 2008). 26 Therefore, protein thermal denaturation could improve the electrospraying process of SPI

dispersions since unfolding the protein chains could favour the formation of polymer
 entanglements.

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INSERT TABLE 1 ABOUT HERE

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6 3.2. Improvement of aqueous hydrocolloidal dispersions for electrospraying

From Table 1 it can be seen that most of the aqueous hydrocolloidal dispersions were not 7 8 suitable for electrospraying and, thus, it was not possible to develop encapsulation structures 9 from them at the various concentrations assayed. In contrast, the different PVOH and PEO 10 solutions and some hydrocolloid-based dispersions obtained from the higher molecular weight 11 materials (dextran, pullulan and WPC) were spinnable giving raise to either capsules or fibres 12 depending on the solution properties. As it was commented before, the main reasons of the 13 sprayability differences were the low viscosity together with too high surface tension values 14 that presented most of the hydrocolloid dispersions. Various strategies were established in 15 order to improve these physical properties and, thus, be able to electrospray the hydrocolloidbased dispersions which could not form capsules with the previous conditions assayed. For 16 increasing the viscosity, different methodologies were followed depending on the hydrocolloid 17 18 type. For the polysaccharide dispersions (resistant starch, maltodextrin, F97 and FI) some 19 thickening agents were added. Specifically, 1% (w/w) with respect to the polymer of guar gum 20 (GG) and xanthan gum (XG) were incorporated in the dispersions. Concerning the SPI dispersion 21 greater viscosity values were sought by the denaturation of the protein through a thermal 22 treatment. Denaturation leads to protein unfolding and exposure of the functional groups 23 which could improve intermolecular interactions, both between the different protein chains 24 and with the solvent, resulting in increased viscosity. For the reduction of the surface tension, a 25 5% (w/w) with respect to the polymer weight of surfactant was incorporated in both, the 26 polysaccharide and the protein dispersions. Specifically, a non-ionic surfactant (Span-20) was

added, since it has been previously reported that electrically charged surfactants give rise to 1 more instability in the electrospraying jet, thus, hampering capsule development (Pérez-Masiá 2 3 et al. 2014). Moreover, both strategies were carried out together in order to ascertain if 4 electrosprayability and capsule morphology were significantly affected when viscosity and 5 surface tension were simultaneously modified. Specifically, Span-20 and guar gum were added 6 to reduce surface tension and increase their viscosity, respectively. In the case of the SPI dispersion, the combined effect of the thermal denaturation and surfactant addition was also 7 8 studied. The different strategies were investigated using the aqueous dispersions with 20% 9 (w/v) of hydrocolloids, except for SPI, where 10% (w/v) dispersions were used. Table 2 compiles the physical properties, electrosprayability, morphology and average size of the capsules 10 11 obtained from the hydrocolloid dispersions containing the different additives. From this table, it can be observed that the incorporation of the different substances effectively modified their 12 13 viscosity, surface tension and conductivity, allowing stable electrospraying from almost all the 14 hydrocolloid dispersions studied. The specific effects derived from the incorporation of the 15 different additives on physical properties and capsule morphology are further described and discussed below. 16

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20 3.2.1. Addition of gums

From Table 2 it can be observed that, as expected, the incorporation of gums to the polysaccharide dispersions significantly increased their viscosity. However, it was seen that xanthan gum led to a considerably greater increase than guar gum, due to the ability of xanthan molecules, in dispersion, to form a highly ordered network of entangled, stiff molecules through its charged trisaccharide side-chains (Norton et al. 1984). Furthermore, xanthan gum also led to greater surface tension and to a significant increase in the electrical conductivity values when

1 compared to guar gum, thus destabilizing the electrospraying jet. This fact explained the continuous dripping during electrospraying in all the dispersions containing xanthan gum. 2 Another interesting observation was that, upon addition of the gums, a continuous film was 3 4 formed together with the capsules in most of the materials assayed. This was probably because 5 of the ability of gums to retain water, causing an incomplete drying of the electrospraying jet 6 and leading to the collapse of the humid structures in the collector which formed a continuous hydrocolloid film. This effect could not be avoided even modifying the processing parameters, 7 8 such as lowering the feeding rate, increasing the tip to collector distance or increasing the 9 hydrocolloid concentration so as to facilitate the elimination of the solvent. It is also important to note that FOS also presented a greater ability to retain water than other hydrocolloids. Thus, 10 FOS capsules were obtained by increasing the tip-to-collector distance with respect to the other 11 12 hydrocolloids in order to avoid water drops on the collector. From the average capsules sizes 13 obtained it was seen that addition of xanthan gum led to the formation of smaller structures, 14 probably because of the higher electrical conductivity of the dispersions. Figure 1 shows the 15 polysaccharide capsules obtained with gums. From this figure it is clearly observed that addition 16 of xanthan gum led to the formation of smaller capsules. It was also seen that a continuous film was formed in most of the materials. 17

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INSERT FIGURE 1 ABOUT HERE

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21 3.2.2. SPI denaturation

As commented above, the strategy to increase the viscosity of the SPI dispersion was to apply a thermal treatment to induce denaturation, to both unfold the protein chains and expose their functional groups to facilitate entanglements. However, from Table 2, it can be observed that denaturation led to a significant viscosity decrease of the SPI dispersion. This fact could be related to the protein extraction process carried out by the suppliers. According to Vega-Lugo

and Lim (2008), as-received SPI used in this work was highly hydrolysed during the extraction 1 process, which may have contributed to poor intermolecular interactions and thus, to its lower 2 viscosity after the thermal treatment. Nevertheless, denaturation of SPI improved the 3 4 electrospraying of this hydrocolloid, probably because of the destruction of the globular 5 structure of the native protein, which led to greater chain entanglements. Figure 2 shows the 6 SEM image of the SPI capsules obtained after denaturation. It was seen that multiple particles and very small capsules were obtained, probably because of the lower viscosity and the higher 7 8 conductivity values of SPI. For high electrical conductivity values, the columbic repulsion forces 9 are greater and compete with the viscoelastic forces of the dispersion, disentangling more easily the polymer network which is being formed during electrospraying. Therefore, increasing 10 conductivity makes it easier for the dispersion to be broken up into smaller droplets, giving rise 11 12 to different morphologies (Bock et al. 2012).

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16 3.2.3. Addition of surfactant

From Table 2 it can be observed that the incorporation of Span-20 effectively significantly 17 18 dropped the surface tension of all the dispersions assayed. It was seen that for all the 19 hydrocolloids, similar surface tension values were attained when adding the surfactant, 20 regardless the presence or absence of gum. This fact was due to the surfactant concentration 21 added. It is well-known that surfactants absorb at solution surfaces, thereby lowering the 22 surface tension of the medium in which they are dissolved. Furthermore, above a critical 23 concentration, the so-called critical micelle concentration (CMC), the surface tension of the solutions reaches an equilibrium value. The CMC of Span-20 and its respective equilibrium 24 surface tension values in various solutions were previously studied (Pérez-Masiá et al. 2014) 25 26 and it was seen to be 0.1 mM. In this work, Span-20 was added above its CMC, so the plateau

surface tension was reached in all the dispersions assayed. Figure 3 shows the SEM images of 1 the capsules obtained from the hydrocolloid/surfactant dispersions. It was seen that addition of 2 Span-20 to the resistant starch dispersion led to the formation of very homogenous capsules. In 3 4 the case of FOS, capsules aggregation and a partial collapse of the structures were observed 5 when Span-20 was added. This fact could be due to the greater ability of water retention of 6 FOS, which hindered the electrospraying jet drying. In fact, tip-to-collector distance had to be increased in this case with respect to the other hydrocolloids, as it was commented before. 7 8 Therefore, although the collected material was apparently dried, humid structures could be 9 reaching the collector and causing the capsules collapse. Very small capsules with multiple morphologies were attained from maltodextrin and SPI due to the higher electrical conductivity 10 of these dispersions. It is worth noting that addition of Span-20 enabled the electrospraying of 11 12 SPI, even when it was not subjected to thermal treatment. This was probably because of an 13 interaction between the surfactant and the protein. From Table 2 it was seen that the 14 incorporation of Span-20 produced a significant viscosity change on the SPI dispersion, which 15 suggested an interaction between both components. This interaction probably favoured chain 16 entanglements during the electrospraying process and led to the capsules formation.

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20 3.2.4. Effect of combined addition of gums, surfactant and/or denaturation

From Table 2 it can be seen that, when the strategies to improve dispersion properties for electrospraying were carried out together, their viscosity and surface tension values were brought to suitable values for capsule formation using this electrohydrodynamic process. Figure 4 shows the SEM images of the capsules obtained combining the strategies to increase the viscosity and reduce the surface tension of the hydrocolloid dispersions. It was observed that, the presence of the gum in the case of the polysaccharide dispersions, hindered solvent evaporation and, thus, a continuous film was also generated during the electrospraying process.
This fact was mainly seen in FOS, since in this case, both the gum and the surfactant may be
contributing to the water retention. In the case of SPI, when the surfactant was incorporated to
the denatured protein dispersion, small, wrinkled and aggregated particles were obtained
probably because of its high electrical conductivity.

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9 3.3. Molecular organization of the capsules

10 ATR-FTIR experiments were carried out in order to figure out the effect of the addition of gums 11 and surfactants and the effect of denaturation on the molecular organization of the hydrocolloid matrices and, thus, to better understand the capsules morphologies attained. 12 13 Figure 5 shows the ATR-FTIR spectra of some of the hydrocolloids assayed. Initially, resistant 14 starch and FOS-FI capsules were analysed as an example of the polysaccharide capsules 15 behaviour when incorporating the gums and the surfactant. Moreover, SPI capsules were also studied to better understand the influence of the thermal treatment and of the surfactant 16 incorporation on these capsules. Figures 5A and 5B show the ATR-FTIR spectra of resistant 17 starch and FI capsules, respectively, from 1200 to 700 cm⁻¹. This region includes the most 18 19 characteristic vibrational bands of the carbohydrates. From these figures it was observed that all the electrosprayed structures presented narrower and better defined bands than the pure 20 21 components, which indicated that the formation of capsules led to a greater molecular order 22 when comparing to the bulk materials. Specifically, for the resistant starch, this area shows the C-O stretching and C-OH bending vibrations at around 1148, 1072 and 1010 cm⁻¹. Further bands 23 were also found at around 924, 850 and 766 cm⁻¹ which were attributed to skeletal vibrations of 24 the pyranose ring, specifically to C-H stretching vibration and the $\alpha(1-6)$ and $\alpha(1-4)$ glycosidic 25 26 bonds (Smrčková et al. 2013; Siddiqui et al. 2014). Concerning the spectra of the FI capsules,

Figure 5B shows the C-O-C stretching vibration at ~1110 cm⁻¹, the C-OH stretching vibration at 1 ~1018 and 990 cm^{-1} , and the C-H stretching vibration at ~930 cm^{-1} (Tewari and Malik 2007). 2 3 Another remarkable observation was that the OH stretching band which appeared at around 4 3300 cm⁻¹ arose at lower wavenumber in FI structures than in the resistant starch ones (data 5 not shown). Moreover, this band was also moved towards lower wavenumbers when xanthan 6 gum was added (data not shown). The lower wavenumber indicated the presence of more bonded OH groups, probably because of greater water retention of these structures (those with 7 8 FOS and with xanthan gum) as it was commented before (D'Souza et al. 2008).

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12 Finally, the molecular organization of the SPI capsules was also studied, to better understand the electrosprayability differences and the capsules morphology in this case. Figure 5C shows 13 the ATR-FTIR spectra of the protein materials from 1800 to 1100 cm⁻¹, where the most 14 15 characteristic protein bands are found. Specifically, the amide I and amide II bands arose at around 1630 and 1530 cm⁻¹ respectively. It was observed that denaturation led to a band 16 broadening and a shift towards higher wavenumbers of both amide bands. The broadening 17 18 could be related to a greater molecular disorder due to the protein unfolding. Regarding the 19 amide bands shift, it could be due to a protein structure variation. Specifically, the amide I shift 20 was attributed to a secondary structure variation, since during thermal treatment the hydrogen 21 bonds stabilizing the native structure of the proteins are disrupted, causing loss of the α -helix 22 and β -sheets structures and creating new β -sheets arrangements (Eissa et al. 2006). The amide 23 II band variations were related to in plane N-H and C-N vibrations (Kong and Yu 2007). Nevertheless, these changes may have favoured the protein entanglements during 24 25 electrospraying and, thus, enable capsules formation.

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3 4. Conclusions

4 From this study it has been demonstrated that the addition of gums and surfactants effectively 5 modified the aqueous hydrocolloid dispersions properties allowing capsule formation through electrospraying. Results showed that, generally, addition of surfactants, and especially non-6 7 ionic surfactants, was the most interesting strategy for improving the sprayability of these 8 materials, since gums retained too much solvent and protein denaturation led to aggregated 9 and wrinkled particles. These results are very interesting for food-related applications, since 10 addition of gums and surfactants allowed structure formation through electrospraying avoiding 11 the use of organic solvents, which are not allowed in the food industry. Moreover, the use food 12 hydrocolloids as matrix materials also favour the application of these capsules in foodstuffs. 13 Particularly, these capsules could be used to protect different bioactive ingredients, such as 14 vitamins, antioxidants, enzymes or probiotics, which are extremely sensitive to ambient and 15 food processing conditions. Nevertheless, it is worth noting that matrix materials are water 16 dispersible and, thus, their protective ability should be evaluated when incorporated to 17 aqueous food products.

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Matrix (9	6)	Viscosity (cP)	Surface Tension (mN/m)	Electrical Conductivity (µS)	Sprayability	Morphology	Average capsule's size (μm)
	5	9.1 ± 0.7^{a}	40.6 ± 0.6^{a}	181.3 ± 4.1^{a}	YES	Capsules + thin fibers	0.7 ± 0.2 ^a *
PVOH (M _w ~ 100000)	10	28.2 ± 2.3^{b}	42.1 ± 0.1^{b}	300.0 ± 7.0^{b}	YES	Fibers	0.1 ± 0.1^{b}
(w,	20	884.9 ± 14.1 ^c	43.7 ± 0.4^{c}	391.7 ± 2.1 ^c	YES	Fibers	0.2 ± 0.1^{b}
	5	58.1 ± 1.4^{a}	55.9 ± 1.5^{a}	144.6 ± 1.3^{a}	YES	Capsules + thin fibers	$0.5 \pm 0.1^{a*}$
PEO (M _w ~ 200000)	10	374.1 ± 7.8 ^b	53.5 ± 0.2^{b}	144.4 ± 4.1^{a}	YES	Capsules + thin fibers	0.5 ± 0.1^{a} *
	20	18738.0 ± 106.2 ^c	50.1 ± 1.8^{c}	159.2 ± 2.0^{b}	YES	Fibers	0.3 ± 0.1^{b}
	10	10.9 ± 0.5^{a}	57.3 ± 0.1^{a}	50.4 ± 2.3^{a}	NO		
Dextran (M ~ 70000)	20	28.8 ± 0.1^{b}	54.2 ± 0.3^{b}	28.9 ± 0.8^{b}	NO		
(40	94.2 ± 2.9 ^c	$59.3 \pm 0.3^{\circ}$	23.5 ± 0.5 ^c	YES	Capsules	0.9 ± 0.5^{a}
Resistant	10	4.4 ± 0.5^{a}	59.2 ± 0.4^{a}	28.8 ± 2.2 ^a	NO		
Starch (M., ~ 1700-	20	5.5 ± 0.5^{a}	57.1 ± 1.6^{b}	18.0 ± 1.1^{b}	NO		
2700)	40	9.1 ± 0.9^{b}	57.9 ± 0.8 ^{ab}	18.9 ± 0.6^{b}	NO		
	10	4.8 ± 0.5^{a}	52.0 ± 0.7^{a}	503.0 ± 1.4^{a}	NO		
$(M_{\rm w} \sim 1300)$	20	5.2 ± 0.2^{a}	52.7 ± 0.1^{a}	677.5 ± 0.7 ^b	NO		
(40	5.3 ± 0.5^{a}	51.6 ± 0.4^{a}	896.7 ± 1.2^{c}	NO		
	10	18.9 ± 0.1^{a}	58.7 ± 0.1^{a}	19. 7 ± 0.5 ^a	NO		
Pullulan (M _w ~ 100000)	20	133.3 ± 0.7 ^b	53.2 ± 0.2^{b}	17.3 ± 0.4^{b}	YES	Capsules + thin fibers	1.0 ± 0.7 ^a *
	40	1690.6 ± 9.1 [°]	$58.5 \pm 1.4^{\circ}$	16.8 ± 0.1^{b}	YES	Fibers	0.1 ± 0.1^{b}
FOS-F97	10	4.8 ± 0.2^{a}	61.6 ± 0.8^{a}	51.1 ± 1.5 ^a	NO		
(M _w ~ 330-	20	5.2 ± 0.6^{a}	63.6 ± 0.9^{b}	49.9 ± 0.7^{a}	NO		

1 Table 1. Solution properties and electrosprayability of the different matrice

6500)	40	7.2 ± 1.2^{b}	64.3 ± 0.1^{b}	44.7 ± 0.1^{b}	NO		
FOS-FI	10	5.4 ± 0.4^{a}	59.9 ± 0.4^{a}	72.0 ± 3.6^{a}	NO		
(M _w ~ 330-	20	5.6 ± 0.3^{a}	58.6 ± 1.0^{b}	69.1 ± 1.6^{a}	NO		
8100)	40	8.29 ± 0.5^{b}	58.1 ±0.2 ^b	79.9 ± 3.1^{b}	NO		
WPC	10	5.4 ± 0.3^{a}	46.7 ± 1.0^{a}	1643.0 ± 25.5 ^a	NO		
$(M_w \sim 20000-$	20	10.8 ± 0.5^{b}	46.5 ± 0.7^{a}	2280.0 ± 10.1 ^b	YES	Multiple particles	
70000)	40	49.0 ± 1.3^{c}	41.9 ± 0.2^{b}	2753.3 ± 20.8 ^c	YES	Capsules	1.0 ± 0.6^{a}
SPI	5	10.6 ± 0.4^{a}	44.4 ± 0.6^{a}	1689.7 ± 11.0^{a}	NO		
$(M_w \sim 30000-$	10	70.5 ± 3.4^{b}	44.4 ± 0.5^{a}	2723.3 ± 23.1 ^b	NO		
350000)	20				NO		

Table 2. Solution properties, electrosprayability and morphology of the different hydrocolloidal solutions with different additives: guar gum (GG), xanthan
 gum (XG) and Span-20.

Matrix (%)	Additive (%)	Viscosity (cP)	Surface Tension (mN/m)	Electrical Conductivity (μS)	Sprayability	Morphology	Average capsule's size (μm)
		5.5 ± 0.5 ^a	57.1 ± 1.6 ^a	18.0 ± 1.1^{a}	NO		
	GG (1%)	11.6 ± 0.3 ^b	55.3 ± 0.6^{b}	24.3 ± 0.2^{b}	YES	Capsules + Films	0.8 ± 0.6^{a}
Resistant Starch	XG (1%)	177.7 ± 0.6 ^c	$58.5 \pm 0.3^{\circ}$	147.5 ± 1.0 ^c	YES	Capsules + Films	0.4 ± 0.3^{b}
(20%)	Span-20 (5%) GG (1%)/Span-20	5.6 ± 0.3^{a}	25.6 ± 0.1^{d}	25.3 ± 0.5^{bd}	YES	Capsules	0.5 ± 0.4^{b}
	(5%)	11.4 ± 0.3 ^b	25.9 ± 0.1^{d}	26.7 ± 1.7 ^d	YES	Beads + Films	0.7 ± 0.3^{a}
		5.2 ± 0.2^{a}	52.7 ± 0.1^{a}	677.5 ± 0.7 ^a	NO		
	GG (1%)	11.2 ± 0.2^{b}	50.0 ± 0.5^{b}	697.0 ± 4.6 ^b	YES	Capsules + Films	0.7 ± 0.6^{a}
Maltodextrin	XG (1%)	$58.6 \pm 0.8^{\circ}$	50.1 ± 2.1^{b}	822.0 ± 12.2 ^c	YES	Capsules + Films	0.3 ± 0.2^{b}
(20%)	Span-20 (5%)	5.8 ± 0.1^{a}	$25.1 \pm 0.6^{\circ}$	681.0 ± 7.1 ^ª	YES	Capsules	0.1 ± 0.1^{c}
	GG (1%)+ Span-20 (5%)	11.6 ± 0.3 ^b	25.4 ± 0.2 ^c	694.3 ± 5.3 ^b	YES	Capsules + Films	0.6 ± 0.5^{a}
		5.2 ± 0.6^{a}	63.6 ± 0.9^{a}	49.9 ± 0.7 ^a	NO		
	GG (1%)	16.9 ± 0.8 ^b	39.1 ± 0.8^{b}	47.9 ± 0.6^{a}	YES	Capsules + Films	0.6 ± 0.8^{a}
FOS-F97 (20%)	XG (1%)	192.0 ± 5.2 ^c	$48.4 \pm 0.2^{\circ}$	168.4 ± 2.2 ^b	YES	Capsules + Films	0.3 ± 0.5^{b}
100107 (2070)	Span-20 (5%)	5.3 ± 0.3^{a}	26.0 ± 0.6^{d}	$55.1 \pm 0.4^{\circ}$	YES	Capsules (Aggregates)	0.6 ± 0.3^{a}
	GG (1%)+ Span-20 (5%)	16.5 ± 1.1 ^b	25.8 ± 0.2^{d}	71.1 ± 1.8 ^d	YES	Capsules + Films	1.7 ± 1.2 ^c
		5.6 ± 0.3^{a}	58.6 ± 1.0 ^ª	69.1 ± 1.6^{a}	NO		
	GG (1%)	18.1 ± 1.3 ^b	49.9 ± 1.7 ^b	80.5 ± 3.5 ^b	YES	Capsules	0.6 ± 0.8^{a}
FOS-FI (20%)	XG (1%)	542.6 ± 10.5 ^c	58.1 ± 2.0^{a}	227.7 ± 2.5 ^c	YES	Capsules + Films	0.1 ± 0.1^{b}
	Span-20 (5%)	5.5 ± 0.2^{a}	26.0 ± 0.2^{c}	62.9 ± 0.2^{d}	YES	Capsules (Aggregates)	0.5 ± 0.3^{a}
	GG (1%)+ Span-20	45.4 ± 2.8^{d}	25.5 ± 0.1 ^c	80.0 ± 1.5^{b}	YES	Capsules + Films	$0.3 \pm 0.3^{\circ}$

	(5%)						
		70.5 ± 3.4^{a}	44.4 ± 0.5^{a}	2723.3 ± 23.1 ^ª	NO		
	Denaturation	26.6 ± 4.1^{b}	42.6 ± 0.7^{b}	2810.0 ± 40.0^{b}	YES	Capsules/Particles	0.2 ± 0.1^{a}
SPI (10%)	Span-20 (5%)	$59.0 \pm 0.8^{\circ}$	$32.3 \pm 0.3^{\circ}$	2643.3 ± 15.3 ^c	YES	Capsules/Particles	0.3 ± 0.2^{b}
	Denat + Span-20 (5%)	56.3 ± 2.0 ^c	32.0 ± 0.3 ^c	2493.3 ± 35.1 ^d	YES	Capsules/Particles	0.2 ± 0.1^{c}

FIGURE CAPTIONS

Figure 1. SEM images of capsules with 1% (w/w) of gum obtained from 20% (w/v)
hydrocolloidal dispersions: (A) Resistant Starch/GG; (B) Maltodextrin/GG; (C) FOS-F97/GG; (D)
FOS-FI/GG; (E) Resistant Starch/XG; (F) Maltodextrin/XG; (G) FOS-F97/XG; and (H) FOS-FI/XG.
Scale marks correspond to 5 μm.

Figure 2. SEM image of capsules obtained from 10% (w/v) SPI solutions after denaturation.

Figure 3. SEM images capsules with 5% (w/w) of Span-20 obtained from different
hydrocolloidal dispersions: (A) 20% (w/v) Resistant starch; (B) 20% (w/v) Maltodextrin; (C) 20%
(w/v) FOS-F97; (D) 20% (w/v) FOS-FI; and (E) 10% (w/v) SPI. Scale marks correspond to 5 μm
(images A, C and D) and 2 μm (images B and E).

Figure 4. SEM images of capsules with 1% (w/w) of guar gum (GG) and 5% (w/w) of Span-20
obtained from the different hydrocolloidal dispersions: (A) Resistant Starch/GG/Span-20; (B)
Maltodextrin/GG/Span-20, (C) FOS-F97/GG/Span-20 and (D) FOS-FI/GG/Span-20; and (E)
denatured SPI/Span20. Scale marks correspond to 5 μm.

Figure 5. ATR-FTIR spectra of electrosprayed capsules obtained from different hydrocolloidal
dispersions: (A) resistant starch; (B) FOS-FI; and (C) SPI.



FIGURE 1.







FIGURE 3.



