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1 **PySTACHIO: Python Single-molecule TrACking stoiCHiometry Intensity and simulatiOn, a flexible,**
2 **extensible, beginner-friendly and optimized program for analysis of single-molecule microscopy**
3 **data**

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11

12 **Highlights**

- 13 • We present PySTACHIO, a refined version of our spot tracking algorithm
14 • We demonstrate highly improved performance over previous MATLAB versions
15 • PySTACHIO can accurately estimate stoichiometries and 2D diffusion coefficients
16 • Performance is comparable to state-of-the-art packages on challenge data
17 • PySTACHIO has both GUI and command line interfaces and can be hosted as a web app

18

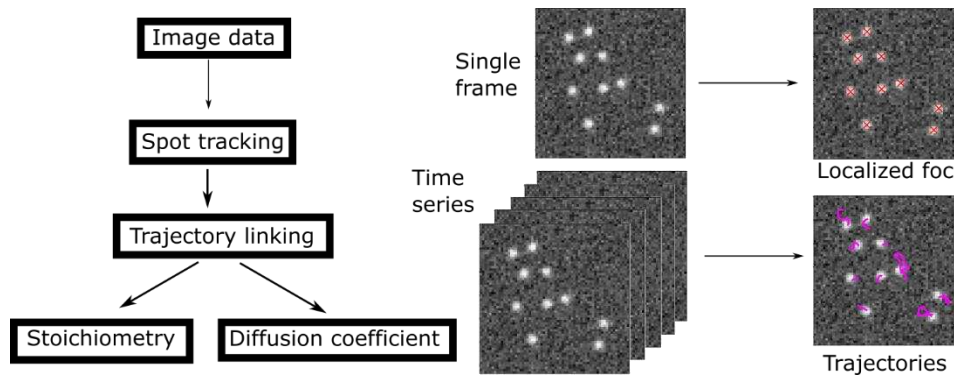
19 **Abstract**

20 As camera pixel arrays have grown larger and faster, and optical microscopy techniques ever more
21 refined, there has been an explosion in the quantity of data acquired during routine light microscopy.
22 At the single-molecule level, analysis involves multiple steps and can rapidly become
23 computationally expensive, in some cases intractable on office workstations. Complex bespoke
24 software can present high activation barriers to entry for new users. Here, we redevelop our
25 quantitative single-molecule analysis routines into an optimized and extensible Python program,
26 with GUI and command-line implementations to facilitate use on local machines and remote
27 clusters, by beginners and advanced users alike. We demonstrate that its performance is on par with
28 previous MATLAB implementations but runs an order of magnitude faster. We tested it against
29 challenge data and demonstrate its performance is comparable to state-of-the-art analysis
30 platforms. We show the code can extract fluorescence intensity values for single reporter dye
31 molecules and, using these, estimate molecular stoichiometries and cellular copy numbers of
32 fluorescently-labeled biomolecules. It can evaluate 2D diffusion coefficients for the characteristically
33 short single-particle tracking data. To facilitate benchmarking we include data simulation routines to
34 compare different analysis programs. Finally, we show that it works with 2-color data and enables
35 colocalization analysis based on overlap integration, to infer interactions between differently
36 labelled biomolecules. By making this freely available we aim to make complex light microscopy
37 single-molecule analysis more democratized.

38

39

40 Graphical abstract



41

42

43 Keywords

44 SMLM, super-resolution microscopy, molecular stoichiometry, diffusion coefficients, image analysis,
45 analysis software

46

47 1. Introduction

48 Cell biology was transformed by the advent of super-resolution microscopy, a sub-theme of which is
49 single-molecule localization microscopy (SMLM) [1]. SMLM techniques determine the spatial
50 location of single fluorophores to below the optical diffraction limit by fitting a point spread function
51 (PSF) to the experimentally acquired image data. These localizations can be used in a 'pointillist'
52 method to reconstruct a single or time series super-resolved image, as in Photo-Activated Light
53 Microscopy (PALM) [2] and Stochastic Optical Reconstruction Microscopy (STORM) [3], or single-
54 molecules or clusters can be tracked as a function of time while quantifying their intensity and
55 diffusion coefficients [4]–[7]. Particularly, analysis of intensity and step-wise photobleaching has
56 become a powerful tool to measure the stoichiometry (i.e. the number of fluorescently labelled
57 biomolecules present in any given tracked object) and copy number of molecular complexes in cells
58 [8]–[14]. Multiple algorithms and software packages have been written and made available to
59 researchers to analyze these super-resolution microscopy data either as standalone suites or as
60 plugins for popular image analysis programs such as ImageJ [15]. However, limited software tools
61 are available for stoichiometry determination and none are available, to our knowledge, exploiting
62 the speed and extensibility of Python.

63 Existing super-resolution localization software has been extensively reviewed and compared [16],
64 [17] but we discuss some of the more popular packages here. Among the most popular super-
65 resolution reconstruction package is ThunderSTORM [18], a multi-purpose tool which is capable of
66 reconstructing data from both STORM and PALM, techniques which both work to increase the
67 temporal and spatial separation of emitting fluorophores so that the point spread function (usually
68 approximated as a 2D Gaussian intensity profiles in the focal plane) can be fit to one fluorescence
69 emitter only. ThunderSTORM is a powerful and flexible toolbox which gives high sub-pixel
70 reconstruction accuracy, although for this to be the case the experiment must be optimized for and
71 performed on fixed cells, and as a result dynamic information such as that embodied within effective
72 diffusion coefficients are in general inaccessible. Similar approaches are also shared by other popular
73 algorithms such as RainSTORM [19], QuickPALM [20] and DAOSTORM [21] which again produce high
74 spatial resolution with the caveat that there is no temporal information. However, in the case of

75 DAOSTORM, multiple point spread function fits allow the reconstructible density of fluorophores to
76 rise by approximately sevenfold, while QuickPALM also includes utilities for 3D reconstruction and
77 drift correction, processes that would generally be included in a larger multi-package workflow.
78 Some routines have also been developed based not on classical algorithms but on machine learning
79 in the case of 3B (standing for “Bayesian analysis of bleaching and blinking”) [22], which hold the
80 promise of more efficient analysis of large time-series data but which require careful interpretation
81 of the results as well as considered choice of models and priors in the case of Bayesian statistics.

82 Away from STORM/PALM-type static reconstruction, many codes have been developed to find
83 individual foci in noisy live-cell microscopy data. In general, classical algorithms in the same class as
84 PySTACHIO and ADEMScode operate through identification of local intensity maxima, though some
85 include pre-filtering steps such as Gaussian filtering [23]–[27], Laplacian of Gaussian [25], [26], [28],
86 wavelet products [29], [30], or deconvolution [31]. In general, a functional form is then fit to
87 detected peaks (commonly Gaussian but occasionally Lorentzian[32]), though in some cases
88 localization itself is done using adaptive thresholding methods [27]. PySTACHIO and ADEMScode
89 both use Gaussian filtering, peak detection, intensity threshold masking, and finally iterative
90 Gaussian fitting, meaning spot detection in PySTACHIO is comparable to state-of-the-art methods.

91 Having found spots in individual image stack frames, the challenge is then to compile these into
92 individual focus trajectories. Here, PySTACHIO and ADEMScode use the most conservative approach,
93 which is to link spots between frames based on distance thresholding, as some other algorithms do
94 [30], though some also include thresholding on the shape of the fitted Gaussian function to
95 determine whether two foci are the same particle. However, more exotic algorithms are also in use
96 today, such as multiple hypothesis tracking [33], probabilistic data association [34], and nearest-
97 neighbor assignment [24]. Many of these also make use of so-called ‘dropped frame’ tolerance [17]
98 – that is to say, if a spot exists in a position (x,y) in frame n , is not detected in frame $n+1$, but is
99 localized near to (x,y) in frame $n+2$ the trajectory is accepted and the ‘dropped’ localization is filled
100 in *a posteriori*. While this has been shown to work well in some systems, we use the conservative
101 strict-linking method in PySTACHIO to avoid the risk of mis-linking in the highly crowded and
102 diffusive live cell environment.

103 After tracking, many packages are available for post-processing either trajectories or spot
104 intensities. Spot diffusion can be analyzed to extract physically relevant properties such as the
105 diffusion coefficient, or to elucidate modes of motion – i.e. tethered, semi-tethered or free diffusion,
106 for example by trajectory postprocessing with Single-Molecule Analysis by Unsupervised Gibbs
107 sampling (SMAUG) [35] which uses a machine learning approach to undercover the diffusion states
108 underlying the determined fluorophore trajectories. Similarly, Bayesian approaches may be used to
109 identify single fluorophore bleaching steps to estimate stoichiometries [36]. However, these are
110 generally used after the tracking and trajectory determination has taken place and are more
111 accurately classified as post-processing packages.

112 In Python, some single-molecule tracking codes have been developed, trackpy is based on the
113 commonly used Crocker and Greir algorithm [24] and recently TRAIT2D [37] has also been
114 developed. However, these packages are not capable of molecular stoichiometry analysis. In this
115 paper, we present PySTACHIO, a standalone single-molecule image analysis framework written in
116 Python 3.8 and based on our original MATLAB (MathWorks) framework [38], that had been
117 developed and improved from a range of earlier core algorithms implemented both in MATLAB [39]
118 and LabVIEW [40], [41] (NI), but used a MATLAB version and libraries that gave improvements in
119 computational speed through parallelization of key For Loop structures [8]. Given single-molecule

120 photobleach image series, PySTACHIO tracks molecule positions detected in the focal plane of the
121 fluorescence microscope as a function of time and calculates their stoichiometry and diffusion
122 coefficients. It fits a kernel density function to the measured background-corrected intensities and
123 produces an estimate of the fluorescence intensity denoted as I_{single} , that corresponds to the
124 characteristic brightness of a single fluorophore molecule integrated over all pixels in the central
125 circular region of the PSF minus any contributions due to local background such as camera noise,
126 sample autofluorescence and of fluorophores that are not in the focal plane but still contribute
127 fluorescence detected by the camera detector. This I_{single} estimate can be used alongside
128 interpolation and model fits of the fluorophore photobleaching probability to give the initial
129 fluorescence intensity to estimate the stoichiometries of detected fluorescence foci and estimate
130 the total copy numbers of fluorescence emitter inside individual whole cells. It includes an easy to
131 use GUI which is configured to be installable as a web hosted app (at the time of writing we have a
132 demonstration instance available for public use) as well as a command-line tool which may be used
133 to run PySTACHIO on batches of data on remote clusters. PySTACHIO is written to be both modular
134 and extensible and we hope that this skeleton application will be further developed by us and others
135 in the future.

136 2. Methods

137 The underlying principles of PySTACHIO are the same as those in our previous code [38]. In brief, the
138 algorithm works by generating candidate fluorescent foci from the raw image using an optional
139 Gaussian blur followed by a top-hat transformation to detect the background. The image is then
140 binarized, with the threshold automatically determined from the peak of the pixel intensity
141 histogram. A series of morphological opening and closing is used to determine candidate pixels
142 associated with individual fluorescent foci. The center coordinates are then optimized through
143 iterative Gaussian masking which when converged, reports the central position to sub-pixel accuracy
144 with a precision related to the number of photons received from the fluorophore and the pixel size
145 (a general rule of thumb for 5 ms exposure and a standard green fluorescent protein this lateral
146 spatial precision is ~ 40 nm). Candidate foci are then assessed for signal-to-noise ratio (SNR) by
147 comparing the integrated intensity within a 5 pixel radius of the candidate center coordinate with
148 the standard deviation of the pixel intensities inside a larger 17x17 pixel square centered on the
149 fluorescent focus center, excluding those within the center circle. Those that fall below the threshold
150 (typically 0.4, whose value is informed by *in vitro* calibration data using surface immobilized
151 fluorophores [10] combined with edge-preserving filters applied to the time-resolved data that allow
152 single-molecule bleach steps to be detected directly [42]) are then removed from the candidate foci
153 list, while the remaining accepted foci are then corrected for local background by subtraction of the
154 mean of the intensities of the local background pixels within the 17x17 pixel square but excluding
155 the 5 pixel radius circle.

156 Foci detected in successive frames are then linked into particle trajectories if the distance between
157 them falls between a user-settable parameter, by default 5 pixels based around the typical width of
158 the PSF, specifically approximately the full width at half maximum of a single GFP molecule PSF in
159 our single-molecule microscope [43]. The linked foci are built up into a trajectory which is written to
160 a file alongside key information at that frame – namely intensity, foci widths, and SNR values. These
161 are trivially read in for post-processing or visualization either with PySTACHIO or with a range of
162 bespoke software. If two trajectories collide, both are terminated at that frame at the coincident
163 locus since this results in the lowest likelihood for incorrect linking of nearby fluorescent foci, but
164 trivial user-modification of this criterion can enable linking-decision criteria based on physical
165 parameters such as foci intensity to generate much longer trajectories if required [44].

166 Single-molecule foci intensities, I_{single} , are estimated by taking the background-corrected intensities
167 as calculated above for all foci, or optionally for all foci in the final half of the data acquisition in
168 which most of the sample has been photobleached. The intensities are then binned into a histogram,
169 and a kernel density function estimate (KDE) [12] fitted using the `gaussian_kde` routine from `scipy`
170 with a kernel width set to 0.7 (set on the basis of typical estimates to size of I_{single} compared to the
171 background noise [45]). The peak of this fit is then found, and this is taken to be the I_{single} value.
172 Though we do not explicitly calculate or propagate errors on I_{single} values (or other estimated
173 values) an error bar may be estimated by taking the full width at half maximum value of the peak in
174 the KDE plot which corresponds to I_{single} . Note however that this approach relies on having good
175 single-molecule data as an input to the routine – the data should for example be fairly low density,
176 either monomeric fluorophores or photobleaching over the course of the acquisition. Once I_{single} is
177 found, it can be set as a parameter for future analysis runs rather than calculating it each time. Using
178 the I_{single} value, the molecular stoichiometry is found for each fluorescent focus by dividing its total
179 integrated intensity by the I_{single} value to give the value for the number of fluorophores present in
180 that focus. For trajectories which begin in the first four frames of the acquisition, we fit a straight
181 line to the first three intensity values of the trajectory and extrapolate back to the initial intensity,
182 which is used to generate a stoichiometry value corrected for photobleaching. A linear fit is used as a
183 compromise approximation to the expected exponential photobleach probability function, since it
184 approximates the initial points of an exponential decay for higher stoichiometry foci to acceptable
185 accuracy, but also fits the flat linear section of a step-wise photobleach of a lower stoichiometry
186 fluorescent focus during which potentially no photobleaching may have occurred [46]. Other
187 methods for stoichiometry determination involve counting the number of steps directly [47]. This
188 works well for low copy number proteins in high SNR environments where single steps are easily
189 resolved but is less general, although has been automated using methods such as Hidden Markov
190 modelling [48].

191 Diffusion coefficients are generated from the detected trajectories by plotting the mean squared
192 displacement as a function of time for each diffusing particle. The initial section of the mean squared
193 displacement (MSD) vs. time interval relation for each tracked focus (by default, the first four time
194 intervals values) is then fit with a straight line, and its gradient and intercept extracted. By default,
195 the fitting algorithm constrains the intercept to be the known localization precision (this is a
196 limitation of the current implementation – other work as demonstrated that in the presence of
197 camera blur and other errors this assumption may be faulty [49]). The diffusion coefficient is then
198 given as the gradient divided by four for 2D diffusion in the lateral focal plane of the microscope.
199 Typically, trajectories of five frames or fewer are disregarded from the diffusion analysis, but this
200 parameter may be modified by the user to account for longer or shorter duration trajectories
201 depending on their specific imaging conditions.

202 Simulated diffusing and photobleaching fluorescent foci are created with an initially pseudo-random
203 position. If the diffusion coefficient is non-zero, the fluorophore is assigned a pseudo-random
204 displacement drawn from a distribution designed to give the input diffusion coefficient as time $t \rightarrow \infty$.
205 The foci photobleach after a pseudo-random time, the scale of which is set by a user-set bleach time
206 parameter. If the maximum stoichiometry is above 1 molecule, each initial fluorescent focus is given
207 a pseudo-random number of fluorophores and hence has intensity $n \cdot I_{\text{single}}$. After each frame, each
208 fluorophore has a probability of photobleaching and those that do have their brightness removed
209 from the simulation while the others remain. This static probability of photobleaching on each frame
210 mimics the step-wise photobleaching behavior of clusters of fluorophores and can be used for I_{single}
211 analysis (see Figure 2). Note that here that unlike state-of-the-art fluorescence simulation packages
212 (e.g. FluoSim [50]) we do not seek to model exact fluorophore photophysics so parameters such as

213 fluorescence lifetime, photoblinking, and emission distributions are neglected. Instead, in
214 PySTACHIO the desired number of fluorophores are seeded in an “on” (or emitting) state, and
215 stochastically photobleach with a user-settable probability per frame which leads to an overall
216 exponential decay of emitters. After photobleaching, fluorophores do not return to the on state.
217 Fluorophores photobleach with a uniform probability of photobleaching at any point within a frame
218 exposure. To simulate this, we generate a uniform random number between 0 and 1 and give the
219 following frame that fraction of I_{single} in addition to the $n \cdot I_{\text{single}}$ that it receives due to the
220 emitters in the on state. During diffusion simulations, fluorophore movement occurs as a step at the
221 end of each frame and the fluorophores are assumed to be static throughout the frame integration
222 time – an assumption which significantly improves computational efficiency, but which could be
223 improved in later version of the codebase. Similarly, we do not model fluorophores diffusing in and
224 out of the plane of focus which would require not only 3D diffusion but also a 3D points spread
225 function, increasing computational complexity considerably.

226 A graphical user interface (GUI) which runs locally in a browser window was written using plotly
227 Dash and is capable of selecting files, running analysis, changing parameters, and showing results
228 and simulated data on separate tabs. On the command line, we make use of Python 3’s
229 multiprocessing module to parallelize the tracking portion of the code using multiple CPU cores in a
230 way analogous to OpenMP. PySTACHIO is not GPU-accelerated at this time.

231 The overall workflow of PySTACHIO is given in flowchart form in Figure 1a.

232

233 3. Results

234 3.1 PySTACHIO performs well at identifying foci in simulated data

235 Figure 1b shows simulated image data with crosses overlaid at the detected positions of simulated
236 fluorophores, where the simulation parameters were taken to be consistent with experimentally
237 observed values (l_{single}=10,000 bg_{_mean}=500 bg_{_std}=120 num_{_spots}=10 frame_{_size}=(128,128)
238 diffusion_{_coeff}=1.0 pixel_{_size}=0.120 [these are the default simulation parameters for both the
239 installable PySTACHIO and the web-hosted instance]). By measuring detected positions and
240 comparing to the known simulated ground truth, we can plot the root mean squared error (Figure
241 1c). We note that that these errors are sub-pixel in scale with the modal error being around 0.2
242 pixels, a distance in our simulation of approximately 20 nm, comparable to previous experimental
243 findings [51]. In Figure 1b, we see that in this case out of ten spots with optimal parameter choices
244 (snr_{_filter_{_cutoff}}=0.4 bw_{_threshold_{_tolerance}}=0.8 num_{_frames}=2 subarray_{_halfwidth}=8
245 inner_{_mask_{_radius}}=3 max_{_displacement}=7 filter_{_image}=Gaussian min_{_traj_{_len}}=2) all ten are
246 detected, which is consistent with (though slightly superior to) previous detection accuracies with
247 this method [38] – however, this is highly dependent on well-optimized parameter choices.

248 We have also applied PySTACHIO to previously generated challenge data [17] using the SNR=4
249 diffusing data set which was noted to be the threshold for most packages to reliably super-resolve
250 spots. Run on single frames with optimal parameter choices (snr_{_filter_{_cutoff}}=0.6 num_{_frames}=100
251 pixel_{_size}=0.067 bw_{_threshold_{_tolerance}}=0.5 subarray_{_halfwidth}=8 struct_{_disk_{_radius}}=10
252 inner_{_mask_{_radius}}=3 max_{_displacement}=7 filter_{_image}=Gaussian min_{_traj_{_len}}=3), we find that 83-
253 100% of spots are identified, with an average detection rate 92%. Here, we used a radius cutoff of 2
254 pixels to discriminate between false and true positives. False positives range between 0 and 4 per
255 frame with an average 1.3 false positive spots per frame (note that each simulated frame here has
256 ca. 50 spots so this represents a low percentage error). Per frame, we find between 0 and 12 false
257 negatives with an average of 5.5 false negatives per frame. This is consistent with PySTACHIO and
258 ADEMScode performance on other trial data – we find that in general false negatives outnumber
259 false positives as spots are discarded which are too close together and cannot be found if they are
260 too close to the frame edge, as the bounding box would then extend beyond the frame itself. With
261 these detection and error rates, we report a frame-by-frame Jaccard similarity index 0.8-1.0, mean
262 0.91. Compared to the ground truth data, we find a root mean square localization error of 0.47
263 pixels, which at this simulated pixel size corresponds to approximately 30 nm.

264 However, PySTACHIO's more common operation mode is trajectory linking, and with this enabled we
265 also discard any spots which are not part of a trajectory with a length greater than a user-specified
266 cutoff (usually three frames). This leads to higher error rates but fewer false positives. Running
267 PySTACHIO with trajectory linking reflects this. Here, we find an average true positive rate of 81.9
268 (range 66.1% to 92.5%), average false negatives per frame increase to an average of 14.1 false
269 negatives per frame (range 6-22), and false positives reduce to an average of 0.5 false positives per
270 frame (range 0-4), leading to an average Jaccard similarity index of 0.81 (range 0.65-0.93). We note
271 here that we do not correct for putative 'dropped frames' as do other software platforms [17] – we
272 insist on strict linking where each spot must be detected and localized within the cutoff radius for
273 each frame step. In the highly diffusive subcellular environment this strict linking increases
274 confidence in individual tracks though does so at the cost of removing some trajectories from later
275 analysis.

276 We also used the challenge data to accurately measure the performance of our code compared to
277 that of our previous version ADEMScode. We found that with the same parameter set, PySTACHIO

278 tracked all 100 frames in *ca.* 60 s while it took ADEMStCode around 560 s for the same tracking
279 operation – a speedup in the new version of approximately 10x.

280 *3.2 Simulating step-wise photobleaching*

281 By giving each simulated fluorescent focus a notional number of fluorophores, we can simulate
282 clusters of proteins. In the simulation parameters, we specify a probability of each fluorophore
283 photobleaching between simulated frames. To simulate the next frame therefore we iterate through
284 each fluorophore and generate a uniform pseudo-random number to determine if the fluorophore
285 has photobleached (trivial modifications also allow users to define different probability distributions
286 depending on the photophysics of the dye under study and the imaging environment). Repeating
287 this for many frames gives an image where initially bright foci decay in a stochastic step-wise
288 manner with an underlying exponential probability, as seen in Figure 2b. We have also implemented
289 the Chung-Kennedy step-preserving filter [12] here which is shown as an inset to Figure 2b.

290 *3.3 Single fluorophore brightness determination, and measuring stoichiometry*

291 Tracking the intensity of all the foci across all frames we can form a histogram and approximate this
292 with a Gaussian kernel density function with a specified bandwidth. By taking the peak of this KDE
293 we approximate the underlying I_{single} value, i.e., the integrated intensity of a single molecule
294 (Figure 2a). Dividing the initial brightness of the focus, we can find the number of fluorophores that
295 compose it, the so-called stoichiometry. We estimate the $t=0$ intensity of the focus by fitting the
296 intensities of the focus in the second, third, and fourth frames with a straight line and extrapolating
297 this back to the first frame to approximately correct for photobleaching. This extrapolated
298 brightness is then divided by the I_{single} value to give the stoichiometry. Testing this on simulated
299 data gives excellent agreement with the input ground truth values (Figure 2c). It is easy to modify
300 the form of the interpolation function as required, for example to use an exponential interpolation,
301 however, a straight line we found to be a pragmatic compromise to both approximate a short
302 section of an exponential photobleaching response function but also provide reasonable
303 interpolation in instances where no photobleaching of track foci had actually occurred for which
304 exponential interpolation would be unphysical.

305 *3.4 Generating trajectories for simulated diffusing fluorophores*

306 By comparing localized foci between frames and applying a distance threshold, we work out which
307 pairs of foci are likely to be the same molecule. These have their positions linked between frames to
308 form a trajectory. Comparing the input ground truth to the measured trajectory (Figure 3a) shows an
309 excellent level of correspondence, with the same distribution of absolute errors as in Figure 1c.

310 *3.5 Determining diffusion coefficients in simulated data*

311 To determine the diffusion coefficient for each tracked fluorescent focus, we begin by plotting the
312 MSD against time interval, τ (Figure 3b). According to Brownian motion, these plots should be a
313 straight line whose gradient is four times the diffusion coefficient. We therefore fit a straight line
314 and extract the gradient to estimate the diffusion coefficient. In order to avoid biases due to
315 unusually long trajectories, by default we take only the first four MSD plot points, and we weight the
316 linear fit to these towards the lower τ values containing more points. In our previous MATLAB
317 implementation this was also constrained such that the intercept of the fit passed through the
318 known localization precision. The default setting in PySTACHIO performs an unconstrained fit to
319 cover instances where users have not measured the localization precision; however, we found that
320 the average diffusion coefficient estimate is still within errors of the ground truth. As we see in

321 Figure 3c the straight-line fits give a distribution of values centered around the simulated ground
322 truth. Running and tracking ten simulations at each simulated diffusion coefficient, we build up
323 statistics as in Figure 3d. Although the spreads are relatively high, the ground truth line hits each
324 interquartile range which for single-molecule data is an acceptable level of accuracy. We note
325 however that in general our estimations skew marginally lower than the ground truth values. We
326 hypothesize this to be due to the step-length distributions in each simulation. As diffusion coefficient
327 increases, the chance of a fluorophore moving a step length greater than our distance cutoff for a
328 fluorophore to be linked between successive frames goes up. Because of this, trajectories may be
329 split into two parts, each of which necessarily contains the lower-apparent-diffusion parts of the
330 trajectory. Although this is a weakness, it is common to all distance-cutoff methods and underlines
331 the need for thoughtful selection of parameters based on fluorophore density and the physical
332 properties of the system under investigation. We also note that this small bias is in all case
333 significantly less than the standard deviation.

334 *3.6 PySTACHIO computational efficiency*

335 Figure 4 shows the computational scaling of PySTACHIO with common variables. In Figure 4a, the
336 scaling of PySTACHIO shows the expected quadratic scaling with frame size, though with an artefact
337 for low frame sizes. These simulations were performed with a fixed number of simulated foci and as
338 such, as the frame size increases the effective focus density is reduced. This is correlated with a
339 decrease in overall runtime despite the larger frame. We hypothesize that in some circumstances
340 Gaussian masking can take significantly longer to converge in the case that there are two or more
341 fluorophores in close proximity that lead to heightened or irregular local backgrounds, leading to
342 overall profiling of the Gaussian masking to get a higher standard deviation of runtime as shown in
343 Supplementary Figure 1. Between the 64x64 and 128x128 pixel simulations therefore the higher
344 overhead of the larger frame is outweighed by the cost savings of fluorophores which are more
345 spatially separated.

346 In Figure 4b we see the scaling due to number of foci (though with a large enough frame size that
347 the fluorophores remain spatially separated), while in Figure 4c the scaling due to number of frames.
348 In each case the scaling is linear, which is the expected behavior given the $O(N)$ scaling
349 considerations in each case.

350 *3.7 GUI and terminal modes*

351 As well as being run in the terminal, plotly.dash was used to create a browser-based dashboard.
352 Here, users can select files for tracking and post-processing and change key parameters to observe
353 their effect on results. Users can also choose to simulate data within the GUI application and is
354 therefore most suited to smaller datasets, new users, or exploratory/preliminary analysis.

355 By contrast, the terminal application supports batch processing and runs in headless mode with
356 results written to files including graph generation for usual usage modes, such as stoichiometry
357 calculation, diffusion coefficient calculation, and so on. Usage on the command line is in the
358 following format: `PySTACHIO.py tasks file_root keyword_args` where `tasks` is one or more from `track`
359 `simulate` `postprocess` `view` where the arguments must be separated by commas but without spaces;
360 `file_root` is the path and root name of the file to be tracked (if in simulation mode, this is used for
361 output files) and should be specified without the `.tif` extension. This root is used also for all the
362 output files and plots. `keyword_args` allow the user to specify individual parameters to override
363 defaults, e.g. `snr=0.5`. The command line implementation can therefore be trivially used to script
364 convergence tests across a range of parameters, producing graphs for each condition.

365 3.8 *Visible copy number analysis*

366 If the user supplies a binary cell mask in .tif format where pixels of value 0 represent background,
367 value 1 pixels belong to cell 1, PysTACHIO will find the integrated and background-corrected
368 intensity for each cell in the first bright frame and report an approximate copy number for that
369 segmented binary large object (BLOB), valuable for users who wish to know how many fluorescently
370 labelled biomolecules are, for example, present in any given single biological cell. Under tests (see
371 Figure 5a) we simulated 100 fluorophores pseudo-randomly distributed in a 3D rod-like bacterial cell
372 typical of many light microscopy investigations, focused at the midplane of the cell. We performed
373 this ten times with varying noise. The mean total copy number was 99 ± 0.2 (S.E.M.), once corrected
374 for the presence of any of out-focal-plane fluorescence [51].

375 3.9 *Linking foci in dual-color experiments*

376 For two-color experiments, often employed to enable whether different biomolecules in a cell
377 interact with each other, the color channels are analyzed separately initially as for single color
378 microscopy. The tracked foci data for each position are used to generate the distances between each
379 set of fluorophores between frames in each channel. Foci pairs with a distance higher than a user-
380 settable cut-off (default five pixels) are discarded. The rest have an overlap integral calculated using
381 their fitted Gaussian widths, and if this integral is above a threshold the pairs are taken to be
382 colocalized [39]. In experimental data, such putative colocalization can then be indicative of binding
383 between tagged molecules, at least to within the experimental localization precision of typically a
384 few tens of nanometers.

385 Tests on simulated data (Figure 5b) show that the algorithm works well in high SNR regimes, with all
386 located foci correctly linked. However, the simulated data has various simplifications not present in
387 real data. First, simulated two color data has perfect registration between channels, while for real
388 data channels can be misaligned or contain chromatic and other aberrations necessitating linear or
389 affine transformation between channels and tracked foci data. Depending on the microscope this
390 may introduce a significant source of error. In simulated data, the foci are high SNR and have the
391 same SNR across colors which is generally not true for real life data and again introduces error.
392 Careful interpretation of output data is therefore necessary.

393 3.10 *Comparison to live cell data*

394 We compared PySTACHIO to previously describe single-molecule localization data obtained from a
395 study of a fluorescently labeled transcription factor, Mig1, inside live budding yeast cells [1] and
396 analyzed trajectories for foci stoichiometries. Our results (Figure 5 panels c and c) show good
397 agreement with previously described results. A fitted Gaussian kernel density estimation shows a
398 peak at 4.4 which as half width at half maximum 4.5, a range which is within error of published
399 results for a cluster size of associated Mig1 molecules [4], [46].

400 **4 Discussion**

401 Our single-molecule analysis software has been translated into Python and is now between 10 and
402 20x faster than the MATLAB implementation. It also has a user-friendly interface alongside a simple-
403 to-script command line interface for power users. Our results work well on simulated data and are
404 comparable to previous analyses of experimental data.

405 PySTACHIO is capable not only of tracking particles and track analysis but also simulation and
406 molecular stoichiometry calculation for even high (10s-100s) stoichiometries. It is written entirely in
407 Python 3.8 and free packages for Python and is written in a modular and extensible way to facilitate

408 customization for a wide array of image analysis projects. PySTACHIO is released under the MIT
409 license allowing anyone to download and modify our code at any time. We hope therefore that our
410 program will be accessible for new users and democratize image analysis as well as forming a basis
411 for advanced users to interrogate their data in depth. Particularly, there is enormous potential to
412 integrate PySTACHIO into recent Python microscope control software [52], [53].

413

414 **Code availability** The PySTACHIO source is available to download from GitHub at
415 <https://github.com/ejh516/pystachio-smt>. A static version of the code used for this publication is
416 available via Zenodo [54]. PySTACHIO will soon be available as an installable package on PyPI as
417 `pystachio-smt`. A web-hosted instance is available at the time of writing for public use which
418 contains the key utilities of the code as described to enable users to explore its functionality prior to
419 downloading locally and adapting to their own specific needs. Details of how to access this web
420 version are available in the GitHub.

421

422 **CRedit author statement**

423 **JS:** Conceptualization, Data curation, Formal analysis, Investigation, Methodology, Software,
424 Validation, Visualization, Writing - original draft, Writing - review & editing. **EH:** Data
425 curation, Formal analysis, Investigation, Methodology, Software, Validation, Visualization,
426 Writing - original draft, Writing - review & editing. **AW:** Methodology, Supervision,
427 Validation, Writing - original draft, Writing - review & editing. **ML:** Conceptualization,
428 Funding acquisition, Project administration, Resources, Supervision, Writing - original draft,
429 Writing - review & editing.

430

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434 project.

435

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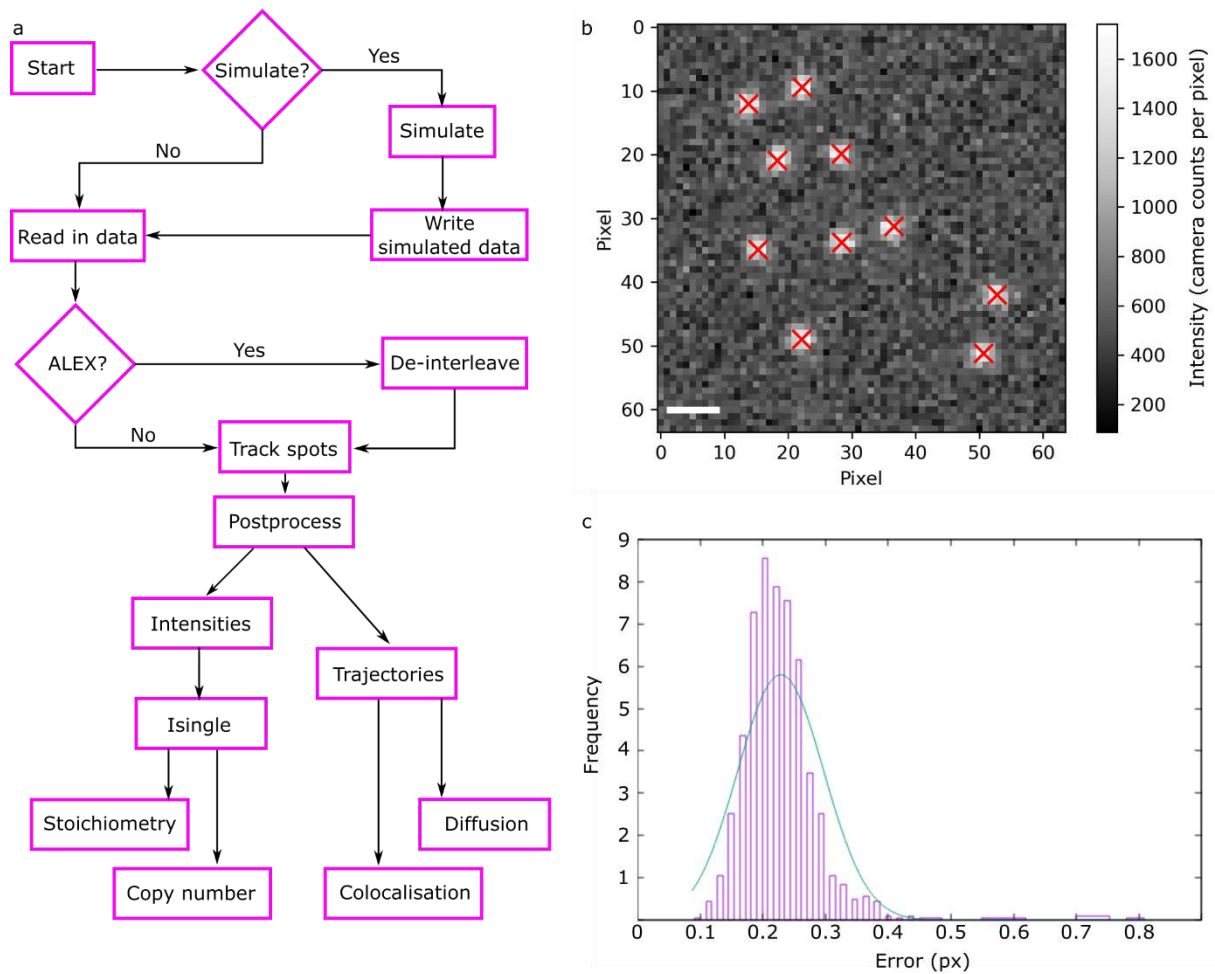
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605 **Figures and captions**

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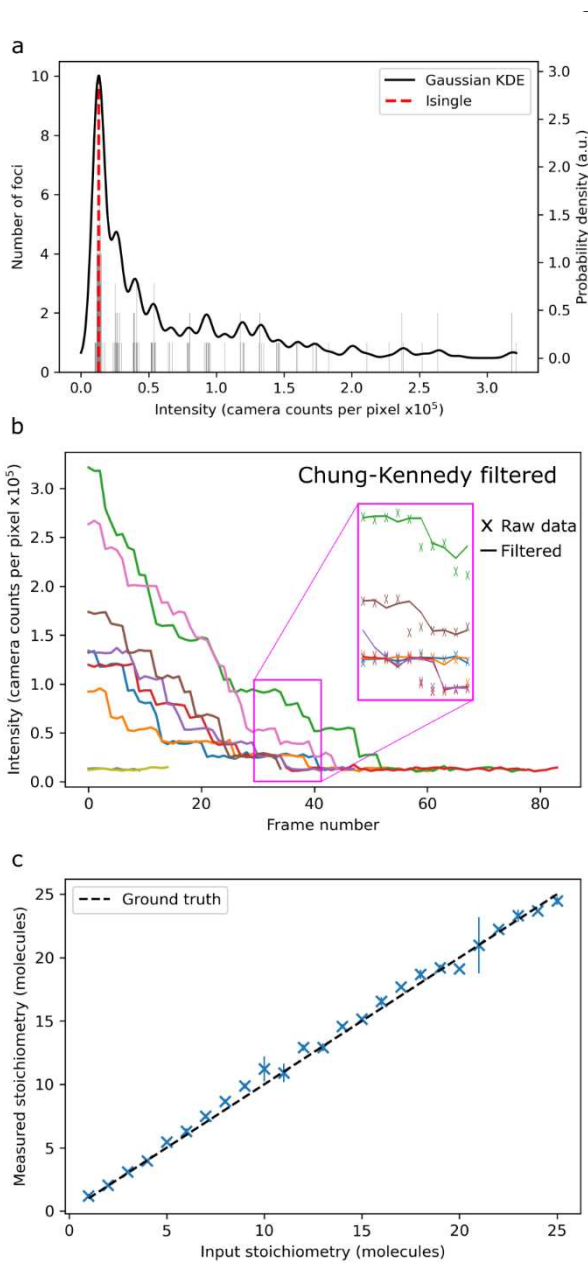


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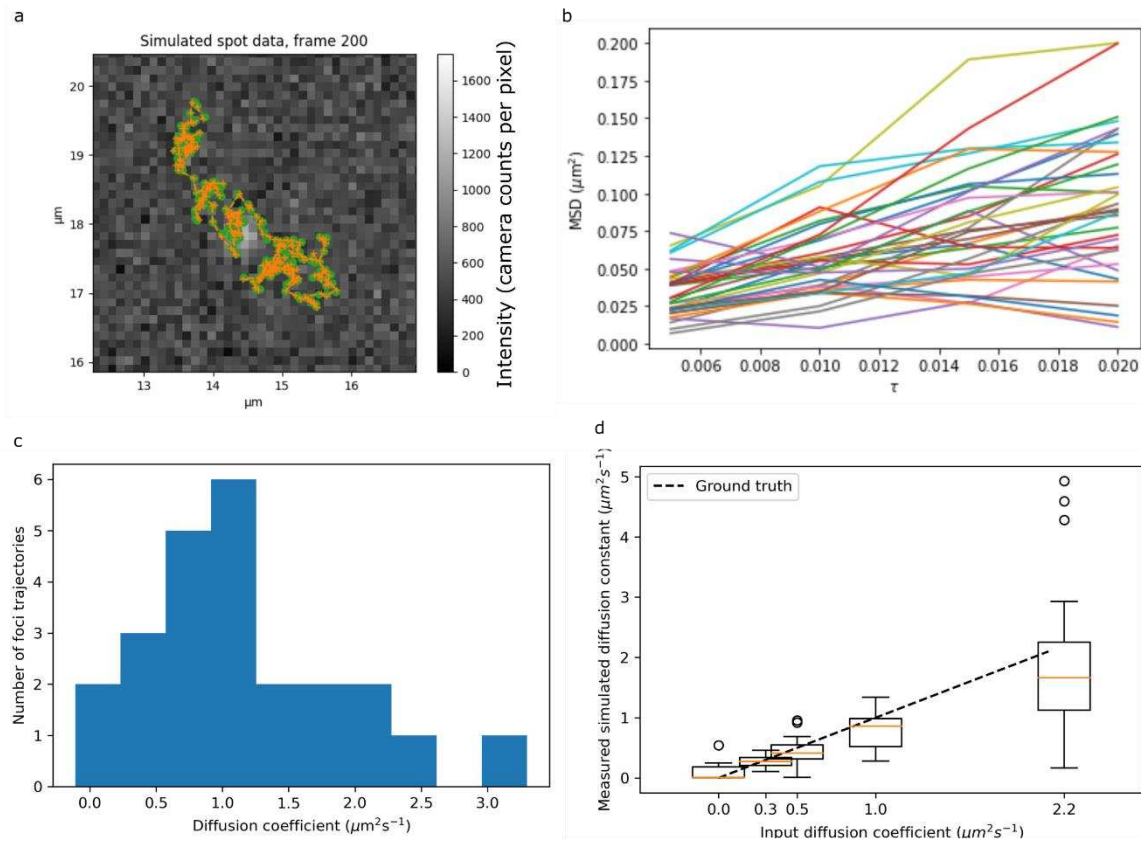
608 **Figure 1:** a) Flowchart of the PySTACHIO workflow; b) simulated data with identified foci indicated
609 with red crosses. Here, the foci were simulated with Isingle 14,000, pixels were 120x120nm in size,
610 and the background had mean and standard deviation 500 and 120 counts respectively. c) Error on
611 simulated foci in pixel units. Bar: 1 μ m.

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L4 **Figure 2:** Simulated step-wise
L5 photobleaching of immobile multi-
L6 fluorophore foci. a) The KDE fit of
L7 measured intensities gives an accurate
L8 estimation of I_{single} (input $I_{\text{single}} \sim 14,000$
L9 counts); b) intensity plots of the tracked
L10 foci show characteristic photobleaching
L11 steps. Inset: Chung-Kennedy [42] filtered
L12 intensity traces show clear steps; c) the
L13 rounded stoichiometry reproduces the
input stoichiometry within error across
the stoichiometry range 1-25 molecules.



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629 **Figure 3:** a) Simulated fluorophore trajectory with the tracked trajectory overlaid; b) mean squared
 630 displacement (MSD) plots for diffusing fluorophores; c) histogram of measured diffusion coefficients;
 631 d) box plot showing the distribution of measured diffusion coefficients for given input diffusion
 632 coefficients. Here the orange central line is the mean, with the box itself representing interquartile
 633 range (IQR). The whiskers represent the IQR \pm one standard deviation, and circles show datapoints
 634 outside this range. In all cases, the ground truth line (dashed in black) passes through the
 635 interquartile range of the measured diffusion coefficients. The upper simulated limit for diffusion
 636 coefficient is set by theoretical considerations of the maximum detectable diffusion coefficient
 637 based on the criterion of a maximum of a five pixel separation between foci in subsequent image
 638 frames to be considered part of the same focus trajectory assuming rapid Slimfield millisecond
 639 single-molecule microscopy [55].

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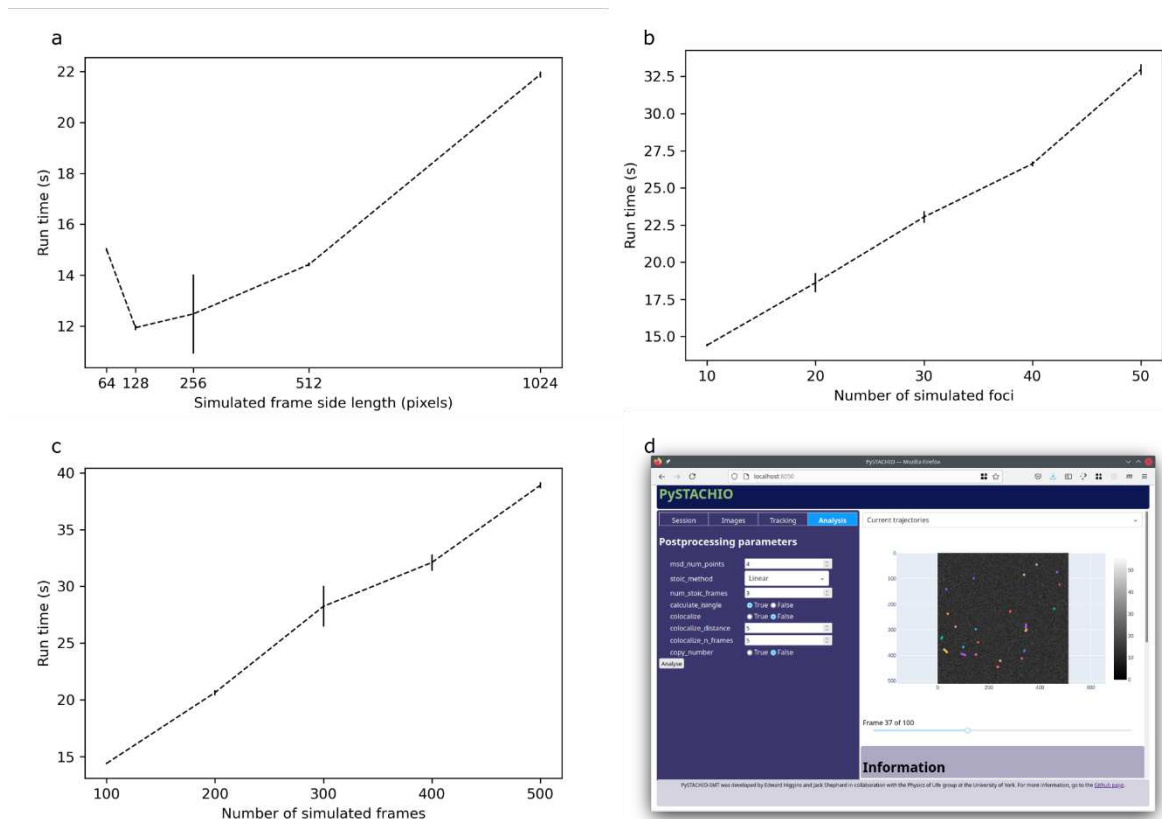
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648 **Figure 4:** Scaling of runtime for PySTACHIO with a) frame size, b) kinetic series length, and c) number
 649 of foci to track; d) a screenshot from the GUI mode showing parameter selection and tracked
 650 trajectories. In panels a-c the error bars represent standard deviation. For each data point, the
 651 tracking software was run five times. In panels b) and c) frame size was 256x256 pixels. In panels a)
 652 and c) the number of simulated foci was 10. In panels a) and b) 100 frames were simulated.

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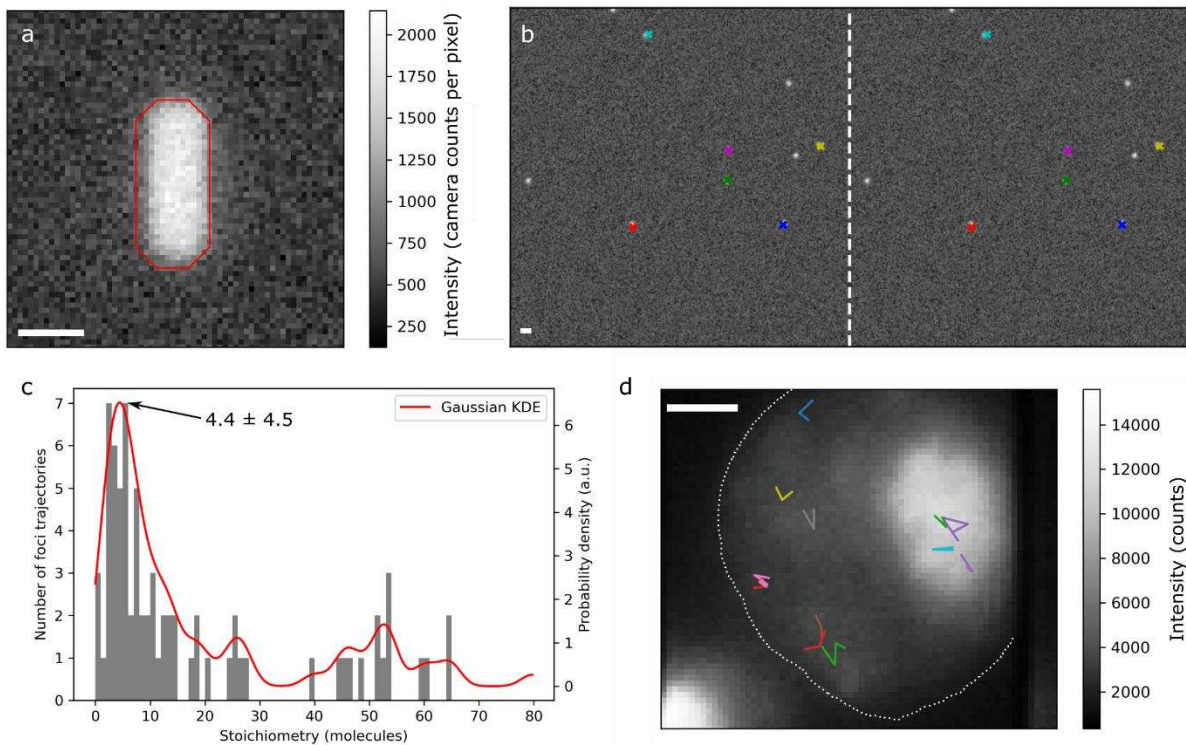
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667 **Figure 5:** a) Simulated rod-like cell with red outline indicated specified mask used for copy number
 668 analysis; b) colocalized foci in a 2-colour experiment (simulated ALEX data here presented de-
 669 interleaved for clarity). Colocalized foci are indicated by the same color in both channels. The border
 670 between the left hand and right hand channel is indicated by a vertical dashed white line; c)
 671 stoichiometries taken from live-cell data in good agreement with previously published values, with
 672 peak stoichiometry 4.4 ± 4.5 molecules; d) trajectories determined from the live-cell data overlaid on
 673 the mean of the five first bright fluorescence frames of the acquisition. The approximate cell outline
 674 is shown with a white dotted line. All scale bars: 1 μm .