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1 Effect of portable non-invasive ventilation on thoracoabdominal

2 volumes in recovery from intermittent exercise in patients with COPD

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- 14 **Running Head:** Effect of portable NIV during recovery from exercise in COPD
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19 Abstract

20 Background: We previously showed that use of portable non-invasive ventilation 21 (pNIV) during recovery periods within intermittent exercise improved breathlessness and exercise tolerance in COPD patients compared to pursed-lip breathing (PLB). 22 23 However, in a minority of patients recovery from dynamic hyperinflation (DH) was 24 better with PLB, based on inspiratory capacity. We further explored this using 25 Optoelectronic Plethysmography to assess total and compartmental 26 thoracoabdominal volumes.

Methods: Fourteen COPD patients (mean±SD) (FEV1: 55±22% predicted) underwent,
in a balanced order sequence, two intermittent exercise protocols on the cycle
ergometer consisting of five repeated 2-min exercise bouts at 80% peak capacity,
separated by 2-min recovery periods, with application of pNIV or PLB in the first
minute of recovery.

32 **Results:** Our findings identified 7 patients showing recovery in DH with pNIV (DH 33 responders) while 7 showed similar or better recovery in DH with PLB. When pNIV 34 was applied, DH responders compared to DH non-responders exhibited greater tidal 35 volume (by 0.8±0.3 L, p=0.015), inspiratory flow rate (by 0.6±0.5 L/sec, p=0.049), prolonged expiratory time (by 0.6±0.5 sec, p=0.006) and duty cycle (by 0.7±0.6 sec, 36 p=0.007). DH responders showed a reduction in end-expiratory thoracoabdominal 37 38 DH (by 265±633 ml) predominantly driven by reduction in the abdominal 39 compartment (by 210±494 ml); this effectively offset end-inspiratory rib-cage DH. Compared to DH non-responders, DH responders had significantly greater BMI by 40 41 8.4 \pm 3.2 kg/m², p=0.022 and tended towards less severe resting hyperinflation by 42 0.3±0.3 L.

43 **Conclusion:** COPD patients who mitigate end-expiratory rib-cage DH by expiratory 44 abdominal muscle recruitment benefit from pNIV application.

45 46

47 Keywords: Exercise, NIV, COPD, Opto-Electronic Plethysmography, Dynamic
 48 Hyperinflation

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60 New and Noteworthy

61 Compared to the pursed-lip breathing technique, acute application of portable non-62 invasive ventilation during recovery from intermittent exercise improved end-63 expiratory thoracoabdominal dynamic hyperinflation (DH) in 50% of COPD patients (DH responders). DH responders, compared to DH non-responders, exhibited a 64 reduction in end-expiratory thoracoabdominal DH predominantly driven by the 65 abdominal compartment that effectively offset end-expiratory rib cage DH. The 66 67 essential difference between DH responders and DH non-responders was, therefore, 68 in the behaviour of the abdomen.

69 Introduction

70 Expiratory flow limitation (EFL) is an important pathophysiological hallmark in 71 Chronic Obstructive Pulmonary Disease (COPD), limiting exercise tolerance 72 secondary to increased dynamic hyperinflation (DH) (13, 38). DH is manifested by increased end-expiratory lung volume that reduces inspiratory reserve volume (IRV). 73 74 This forces COPD patients to breathe close to their total lung capacity (TLC), 75 increasing both work of breathing and breathlessness (38). Additionally, DH may 76 cause adverse central hemodynamic effects by reducing venous return, thus 77 impairing the normal increase in stroke volume and cardiac output during exercise 78 (1, 50). Non-invasive ventilation (NIV) is one of the ergogenic approaches that has 79 been implemented to reduce DH and breathlessness, thus improving exercise 80 tolerance in COPD (3).

A limited number of studies have assessed the effect of NIV on the magnitude of DH during exercise by measuring inspiratory capacity (IC) (38) in patients with COPD with conflicting evidence. Accordingly, application of NIV during exercise has shown to either increase DH (43), or decrease DH (39), albeit the change in IC in the latter study (39) still indicated significant DH above resting values (38). IC manoeuvres are, however, effort dependent and therefore the estimate of DH may be inaccurate, especially during intense exercise.

88 Application of a portable NIV (pNIV) device (VitaBreath, Philips Respironics Morrisville, PA, USA) was recently shown to increase intermittent exercise tolerance 89 90 and improve breathlessness in comparison to the pursed lip breathing (PLB) 91 technique in 16/24 COPD patients when applied in the first minute of recovery periods during successive bouts of intermittent exercise (10, 48). VitaBreath is a 92 portable, handheld, battery-powered, pNIV device that provides an expiratory 93 94 positive airway pressure (EPAP) of 8 cmH₂O and inspiratory positive airway pressure (IPAP) of 18 cmH₂O (17). The VitaBreath device is no longer commercially available, 95 but similar devices may come to market. Nevertheless, the aforementioned studies 96 97 (10, 48) provided proof of concept on how NIV can be applied intermittently during recovery from exercise in patients with COPD, and how to identify patients most 98 99 likely to respond to NIV. Furthermore, considering that use of pNIV in activities of daily living improves anxiety around breathlessness, as well as perceived time of 100 recovery from it (48), ventilatory support during recovery from exercise is potentially 101 102 of value to the COPD patient.

We previously showed that whilst the majority of COPD patients experienced a greater reduction in DH with pNIV compared to PLB (DH responders) based on measurement of IC, in 8/24 of patients the improvement in DH was greater with PLB than pNIV (DH non-responders); it may be that the fixed IPAP and EPAP were suboptimal, at least for DH non-responders (10, 48). Interestingly, DH non108 responders tended to have greater resting airway obstruction and baseline lung 109 hyperinflation, whilst during exercise they exhibited greater restrictions to tidal 110 volume expansion compared to DH responders. Tidal volume expansion during 111 exercise depends on the degree of exercise-induced EFL (12, 18, 33) and the ability 112 to decrease end-expiratory thoracoabdominal volume by recruitment of expiratory abdominal muscles (12, 27, 49). Accordingly, it was suggested that DH responders 113 114 would represent those patients exhibiting greater capacity to increase tidal volume 115 by recruiting expiratory abdominal muscles (11). However, in our earlier studies (10, 116 48) we did not assess the degree of expiratory abdominal muscle recruitment. 117 Furthermore, DH was assessed one minute following pNIV and PLB application by 118 performing inspiratory IC manoeuvres (36). Thus, the acute effect of pNIV 119 application on DH was not investigated.

120 Optoelectronic Plethysmography (OEP) allows breath-by-breath assessment of end-121 inspiratory and end-expiratory total and compartmental (rib cage and abdominal) 122 thoracoabdominal volumes without the necessity to perform IC manoeuvres (2). The 123 purpose of the present study was to assess total and compartmental 124 thoracoabdominal volumes during acute application of pNIV during recovery from 125 exercise. We hoped to better understand why the rate of recovery from DH is slower 126 with pNIV compared to PLB in DH non-responders compared to DH responders (10, 127 48).

128 Earlier work has shown that application of continuous positive airway pressure 129 (CPAP: 7.5-10 cm H_2O) during exercise is associated with inflation of the rib cage 130 compartment with concomitant deflation of the abdominal compartment, secondary to expiratory abdominal muscle recruitment, in the majority of COPD patients (43). 131 132 Accordingly, it was reasoned that during acute application of pNIV in recovery from 133 intermittent exercise, DH responders would exhibit greater recruitment of expiratory 134 abdominal muscles alongside greater expiratory flow rates when compared to DH 135 non-responders.

137 Methods

138 Study design

139 This was a crossover study investigating the acute effect of pNIV compared to the 140 PLB technique on thoracoabdominal volumes in recovery from intermittent exercise. 141 Central hemodynamic responses, local respiratory muscle oxygen availability and 142 respiratory muscle electromyography activity were also assessed. Patients 143 underwent two sub-maximal intermittent exercise tests sustained at 80% of peak 144 work rate (WRpeak) on a cycle ergometer using both pNIV and the PLB technique during recovery from exercise in a balanced order on the same day. The 145 146 investigations were carried out following the rules of the Declaration of Helsinki of 147 1975 (51), revised in 2013. NHS Research Ethics Committee approval (Ref: 19/NE/0091) and Clinical Trials registration (NCT03848819) were obtained. All 148 149 participants provided written informed consent.

150 Participants

Inclusion criteria were stable COPD, aged 40 years or older with a smoking history of at least 10 pack years, and who exhibited substantial exercise-induced DH at the limit of incremental cycle exercise tolerance (i.e.: change in inspiratory capacity from baseline >0.15 L or >4.5% of predicted resting IC) (38). Exclusion criteria included COPD exacerbation within 6 weeks prior to exercise testing, unstable comorbidities and inability to exercise.

157 Baseline Assessment – Visit 1

Prior to exercise testing, participants attended North Tyneside General Hospital for baseline assessment. This included spirometry, body plethysmography lung volume measurements, diffusion capacity, resting electrocardiography (ECG) evaluation, medical history and examination. Following medical assessment, patients performed a ramp incremental exercise test with increments of 5-10 watts every minute to the limit of tolerance on a cycle ergometer (Ergoselect 200, Ergoline GmbH, Bitz, Germany) (48) to establish presence of DH (38, 48) and WRpeak.

165 Intermittent Exercise Protocol – Visit 2

Patients underwent two intermittent exercise protocols on the cycle ergometer (Ergoselect 200, Ergoline GmbH, Bitz, Germany). The exercise protocol consisted of five repeated 2-min exercise bouts at 80% of predefined WRpeak, separated by 2min recovery periods, to allow application of pNIV or the PLB technique. During the first minute of each recovery period, patients breathed through the pNIV device or adopted the PLB technique. During the second minute of each recovery period patients breathed normally. Before each exercise test patients underwent threeminutes of baseline measurements (quiet breathing-QB) followed by a three-minutewarm-up period with no cycling load.

After the termination of the 5th exercise bout patients underwent 5 minutes of 175 measurements during recovery. Patients performed IC manoeuvres to allow 176 177 calculation of thoracoabdominal volumes at total lung capacity (TLC) during QB, the 178 second minute of each exercise bout and each recovery period as previously 179 described (40). Total and compartmental thoracoabdominal volumes were recorded 180 by OEP during QB, exercise and recovery periods. Circulatory responses and local 181 respiratory muscle oxygenation were measured non-invasively using impedance 182 cardiography technology and near-infrared spectroscopy, respectively throughout 183 QB, exercise and recovery periods. Electromyography (EMG) activity of respiratory 184 muscles (intercostal, scalene and rectus abdominis) was recorded during the first 185 minute of each recovery period using surface electromyography electrodes. 186 Peripheral oxygen saturation (SpO₂%) was continuously monitored by a pulse 187 oximeter (Onyx Vantage 9590, Nonin Medical Inc, USA). Finally, following each 188 exercise bout dysphoea and leg discomfort were recorded on the modified 1-10 Borg 189 scale (6).

190 *pNIV and pursed lip breathing*

During the first minute of each recovery period in one of the exercise tests, pNIV was applied via the VitaBreath device. The VitaBreath is a portable, handheld, batterypowered, non-invasive ventilation device (pNIV) intended to reduce activity-related shortness of breath (17). It delivers fixed high inspiratory (18 cm H₂O) and expiratory (8 cm H₂O) pressures, but it can only be used during recovery periods interspersing bouts of physical activity.

Patients practiced using the VitaBreath device and the correct adoption of the PLB technique with guidance from a respiratory nurse during the first visit. During the second visit a respiratory physician was present to ensure that patients were able to follow the instructions provided by the researchers and perform the pNIV and PLB techniques correctly.

202 Thoracoabdominal volumes

During both intermittent exercise tests, thoracoabdominal wall kinematics were assessed by the OEP system (BTS, Milano, Italy) during QB, the second minute of each exercise bout and throughout the recovery periods as follows: the movement of 89 retro-reflective markers placed over the anterior, lateral and posterior chest wall was recorded. Each marker was tracked by eight video cameras (Smart System BTS, Milan, Italy), four in front of the subject and four behind. Subjects used grasp handles positioned at the mid sternum level to lift their arms away from the rib cage so that lateral markers could be visualised. Dedicated software reconstructed the three-dimensional coordinates of the markers in real time by stereophotogrammetry and calculated total and compartmental thoracoabdominal volume and volume variations using Gauss's theorem. The chest wall was modelled as being composed of two compartments—the rib cage and the abdominal compartments. Total thoracoabdominal volume is the sum of these two compartmental volumes (49).

216 Circulatory responses

217 During both intermittent exercise tests, participants were connected to a portable 218 device using impedance cardiography technology (Physio Flow, Enduro, PF-07, 219 Manatec Biomedical, Folschviller, France). The validity of cardiac output recordings 220 using Physio Flow, in comparison to the dye dilution method and the direct Fick method, has been confirmed in both healthy subjects and those with 221 222 cardiorespiratory disease (9, 26, 46). Cardiac output (CO), heart rate and stroke 223 volume were recorded continuously as previously detailed (34). Six electrodes were 224 placed on patients, two on the left carotid artery (Z1 and Z2), two in the breast area 225 (EKG1 and EKG2) and two in the chest area [Z3 and Z4-EKG3 (neutral)] (34).

226 Local respiratory muscle oxygen availability

Local respiratory muscle oxygen availability of the intercostal muscles (7th intercostal 227 228 space) and rectus abdominis was assessed throughout QB, exercise and recovery 229 periods by a NIRO 200 spectro-photometer (Hamamatsu Photonics KK, Hamamatsu, 230 Japan). The NIRO 200 uses Spatially Resolved Spectroscopy method to detect 231 changes in Tissue Oxygenation Index (TOI), Oxygenated haemoglobin (HbO₂), and 232 Deoxygenated haemoglobin (HHb) and its validity has been previously established 233 (29). Two sets of NIRS optodes were placed, one on the skin over the 7th left 234 intercostal space at the midaxillary line and the other over the left rectus abdominis. 235 The optode separation distance was 4 cm, corresponding to a penetration depth of 236 approximately 2 cm. The left intercostal and rectus abdominis were used in order to 237 avoid potential blood flow contributions from the liver (25). NIRS values were zeroed 238 at the start point of each exercise protocol. NIRS data were sampled at 6 Hz and 239 exported in document file format and averaged for offline analysis at 60 s intervals.

240

241 **Respiratory muscle electromyography**

EMG was used to assess respiratory muscle activation during application of pNIV or PLB. Prior to placement of electrodes, the skin was cleaned. Surface electrodes (Delsys Trigno, Delsys, Boston, MA, USA) were placed as previously been described (8) on the surface over the right seventh intercostal space, 2 cm lateral to the umbilicus, over the muscle mass of rectus abdominis and over the scalene muscle. EMG data were recorded during quiet breathing and at the first minute of each recovery period when pNIV or PLB were applied for 30 seconds. Finally, EMG data were recorded at 2000Hz and were filtered at 25–500 Hz during each trial (Spike 2, Cambridge Electronic Design, Cambridge, UK) (8). All EMG was processed using custom written scripts in Matlab (The Mathworks, Inc. Natick, MA, USA). Data are presented as fractional change in electromyographic activity from baseline values.

253 Statistical analysis

254 Estimation of sample size within each breathing modality (i.e. pNIV and PLB) was 255 based on the results of our previous study (48). Using the minimum clinically 256 important difference in DH assessed by inspiratory capacity manoeuvres defined as 257 4.5% of predicted resting IC (mean: 120 ml within our previous cohort) and observed 258 SD: 110 ml (48), an alpha significance level of 0.05 (2-sided) and 80% power, a 259 minimum total sample size of 13 patients was required. Fourteen patients were 260 recruited in order to achieve balance in the order that the pNIV and PLB trials were 261 performed. Seven patients had previously participated in a study undertaken by our 262 group (48). Data are presented as mean \pm standard deviation (SD) unless otherwise 263 stated. DH responders were identified as patients showing a reduction in end-264 expiratory thoracoabdominal volume with pNIV at least 120 ml greater than that 265 seen with PLB at the first minute of recovery, whereas DH non-responders were 266 those failing to show this degree of response with pNIV compared to PLB (10). The 267 120 ml dichotomous value was based on our earlier study (10) indicating that 268 patients showing an reduction in DH \geq 120 ml (40) when using pNIV compared to the 269 PLB technique were identified as DH responders. Patients showing a decrease in DH 270 < 120 ml, or an increase, in DH using pNIV compared to PLB were defined as DH non-271 responders. Independent sample t-tests were employed to compare baseline 272 characteristics between DH responders and DH non-responders. Two-way repeated 273 measures ANOVA followed by least significant difference (LSD) post-hoc analysis was 274 employed to assess differences in total and compartmental thoracoabdominal 275 volumes, breathing pattern, circulatory responses and local respiratory muscle 276 oxygenation between both the pNIV device and PLB exercise tests, and between DH 277 responders and DH-non responders. Activation of respiratory muscle EMG activity is 278 presented as percentage of change from baseline (QB) and was analysed using 279 paired sample t-tests. Data present mean values for thoracoabdominal and 280 compartmental volumes, circulatory responses, local respiratory muscle oxygen availability, and respiratory muscle EMG activity for: QB, the 5 exercise bouts, the 1st 281 282 and 2nd minutes of all 5 recovery periods as well as the 3rd, 4th and 5th minute of 283 recovery following the final exercise bout. The level of significance for all analyses 284 was set at p < 0.05.

286 Results

Overall, patients had moderately severe airway obstruction and significant lung hyperinflation at rest (Table 1). Peak exercise capacity was severely impaired; patients exhibited exercise-induced DH and low peak oxygen consumption at the limit of tolerance (Table 1). DH responders had significantly greater BMI and inspiratory flow rate at rest (Table 1).

292 Thoracoabdominal volumes for all patients

293 Across all 14 patients, total end-expiratory and end-inspiratory thoracoabdominal and compartmental volumes were not significantly different during exercise 294 295 between PLB and pNIV trials (Figure 1). Compared to QB, end-expiratory 296 thoracoabdominal volume increased by an average of 266±152 ml during exercise 297 indicating presence of DH (38). Thoracoabdominal IRV at the end of exercise was on 298 average 645±439 ml (Figure 1a). Compared to QB at the end of exercise we found an 299 average increase of 326±291 ml (p=0.001) in thoracoabdominal volume at TLC 300 (Figure 1a).

301 With acute pNIV application in the first minute of recovery total end-inspiratory 302 thoracoabdominal volume was greater compared to PLB application (by: 230±207 303 ml; p=0.047) (Figure 1a), secondary to greater end-inspiratory rib cage volume (by: 304 266±196; p=0.005) (Figure 1b). Total end-expiratory thoracoabdominal volumes 305 were not different (p=0.673) between acute PLB and pNIV applications in the first 306 minute of recovery (Figure 1a). During pNIV application there was a greater increase 307 in end-expiratory rib cage volume (by 198±185 ml p=0.047 value) (Figure 1b) 308 compared to PLB, which was partially compensated by the lower end-expiratory 309 abdominal volume (by 141±124 ml p=0.022) (Figure 1c). IRV (relative to TLC at the 310 end of exercise) was on average 257±227 (p=0.038) ml lower with acute pNIV 311 application compared to PLB, indicating ventilatory constraints (36). At the 5th 312 minute of recovery following the last exercise bout, neither end-inspiratory nor end-313 expiratory total thoracoabdominal volumes returned to levels recorded during QB 314 (Figure 1a).

315 Thoracoabdominal volumes during exercise

During exercise total end-expiratory thoracoabdominal volumes were not different (p>0.05) between pNIV and PLB trials for DH responders and DH non-responders, (Figure 2). DH responders and DH non-responders exhibited an increase in endexpiratory thoracoabdominal volume (by: 281±135 ml and by: 248±161 ml, respectively) compared to QB, indicating exercise-induced DH (38) (Figure 2a & 2d). However, DH responders significantly decreased (p<0.05) end-expiratory abdominal volume during exercise compared to QB in both trials (Figure 2c), whereas DH nonresponders maintained end-expiratory abdominal volume unchanged from QB in both trials (p>0.05) (Figure 2f). Exercise IRV was not different (p=0.391) between DH responders (644±513 ml) and DH non-responders (528±353 ml) (Figure 2a & 2d). During exercise DH responders exhibited greater inspiratory and expiratory flow rates compared to DH non-responders (Figure 3 a & 3b).

328 **DH responders in recovery from exercise**

329 Our analysis identified 7 patients as DH responders and 7 patients as DH nonresponders (Table 1). In DH responders, during acute application of pNIV compared 330 331 to PLB, total end-expiratory thoracoabdominal volume was lower by 209±422 ml (38) 332 (Figure 2a), secondary to significantly lower end-expiratory abdominal volume with 333 pNIV compared to PLB (by: 219±197 ml; p=0.026) (Figure 2c), thereby indicating 334 greater expiratory abdominal muscle recruitment. In DH responders during acute 335 application of pNIV compared to PLB, numerical differences did not reach statistical significance for total end-inspiratory thoracoabdominal volume (by 224±465 ml; 336 p=0.250) (Figure 2a) consequently to differences in end-inspiratory rib cage volume 337 (by 186±368 ml; p=0.230) (Figure 2b). IRV with pNIV tended to be lower (p=0.078) 338 compared to PLB (by 302±421 ml) (Figure 2a and Table 2). At the 5th minute of 339 340 recovery following the last exercise bout, neither end-inspiratory nor end-expiratory 341 total thoracoabdominal volumes returned to levels recorded during QB (Figure 2a).

342 DH non-responders in recovery from exercise

343 In DH non-responders, during acute application of pNIV compared to PLB, total end-344 expiratory thoracoabdominal volume was greater (p=0.001) by 356±153 ml (Figure 345 2d) secondary to greater end-expiratory rib cage volume with pNIV compared to PLB 346 (by: 416±86; p=0.001) (Figure 2e) and unchanged end-expiratory abdominal volume 347 (Figure 2f). During acute application of pNIV total end-inspiratory thoracoabdominal 348 volume was greater compared to PLB (by: 238 ± 218 ml; p=0.047) (Figure 2d), 349 secondary to greater end-inspiratory rib cage volume (by: 346±199 ml; p=0.004) 350 (Figure 2e). There was no significant difference in IRV between pNIV and PLB application (p=0.252) (Figure 2d and Table 2). At the 5th minute of recovery following 351 352 the last exercise bout, neither end-inspiratory nor end-expiratory total 353 thoracoabdominal volumes returned to levels recorded during QB (Figure 2d).

354 Differences between DH responders and non-responders in recovery from exercise

Considering pNIV application alone, DH responders compared to DH non-responders
 exhibited a reduction in end-expiratory thoracoabdominal DH (by 265±633 ml)
 predominantly driven by reduction in the abdominal compartment (210±494 ml),
 thereby effectively offsetting end-inspiratory rib cage DH.

360 **Breathing pattern in DH responders and DH non-responders**

361 DH responders: During acute pNIV application compared to PLB, DH responders had 362 greater minute ventilation (by: 6.5±6.4 L/min; p= 0.009), secondary to greater tidal volume (by: 0.5±0.4 L; p=0.002) without any differences in breathing frequency, 363 inspiratory and expiratory time, or duty cycle (Table 2). During acute pNIV 364 365 application compared to PLB, DH responders exhibited greater inspiratory flow rate 366 (by: 0.4±0.3 L/sec; p=0.001) and greater expiratory flow rate (by: 0.2±0.2 L/sec; p=0.048) (Figures 3a & 3b, Table 2). There were no differences either in average 367 values for breathlessness (p=0.745) or in leg discomfort (p=0.880) between pNIV and 368 369 PLB application in DH responders (Table 2).

370 DH non-responders: Compared to PLB, with acute pNIV application DH nonresponders increased their minute ventilation (by: 5.7±4.5 L/min; p=0.018) by 371 372 adopting a more tachypnoeic breathing pattern (compared to DH responders) as 373 breathing frequency was greater with pNIV compared to PLB (by: 7±6 breaths/min; 374 p=0.002) (Table 2). The tachypnoeic breathing pattern resulted in lower inspiratory 375 time (by: 0.3 ± 0.2 sec; p=0.019), lower expiratory time (by: 0.8 ± 0.6 sec; p=0.001) and 376 lower total duty cycle (by: 1.1±0.8 sec; p=0.001) with pNIV application compared to 377 PLB (Table 2). Moreover, with pNIV application compared to PLB there was a trend 378 for greater inspiratory flow rate (by 0.2±0.2 L/sec p=0.064), whilst expiratory flow 379 rate was significantly greater (by: 0.2±0.2 L/sec; p=0.011) (Figures 3a & 3b, Table 2). 380 Following acute application of pNIV compared to PLB breathlessness was lower in DH non-responders (by: 1.1±0.9; p=0.001), whilst leg discomfort was unaffected 381 382 (p=0.203) (Table 2).

383 Differences in breathing pattern between DH responders and DH non-responders

When pNIV was applied, DH responders compared to DH non-responders exhibited greater tidal volume (by 0.8±0.5 L, p=0.015), inspiratory flow rate (by 0.6±0.5 L/sec, p=0.049), prolonged expiratory time (by 0.6±0.5 sec, p=0.006) and duty cycle (by 0.7±0.6 sec, p=0.007) whilst breathing frequency was lower (p=0.019) (Table 2).

With pNIV application numerical differences for expiratory flow rate in DH responders compared to DH non-responders (by 0.2±0.5 L/min) did not reach statistical significance (p=0.389). IRV relative to end-exercise TLC during acute pNIV application was not different between DH responders and DH non-responders (p=0.968) (Figures 2a and 2d).

393 Central haemodynamic responses

394 CO was unaffected by acute pNIV application compared to PLB in both DH 395 responders and DH non-responders (Figure 4c & 4f). However, in DH responders, 396 throughout recovery from exercise, pNIV application resulted in significantly greater CO compared to PLB (p=0.024) (Figure 4c) and did not return towards baseline at the 5th minute of recovery. In DH non-responders there were no differences in the pattern of response in any of the central haemodynamic variables between pNIV and PLB application in recovery from exercise (Figure 4 d-f), whereas CO returned towards baseline at the 5th minute of recovery.

402 EMG muscle activity

Surface muscle EMG revealed two different patterns of respiratory muscle activation 403 404 during recovery from exercise. DH responders exhibited greater inspiratory and 405 expiratory EMG muscle activity (delta of percentages from baseline between 406 conditions) with pNIV application compared to PLB as this was reflected by the 407 greater activation of intercostal (by: 20±16%; p=0.043), scalene (by: 50±33%; 408 p=0.013) and rectus abdominis (by: 67±57%; p=0.014) muscles (Table 3). In contrast, 409 DH non-responders using pNIV compared to PLB exhibited reduced inspiratory 410 (intercostal and scalene) EMG muscle activity, and increased expiratory (abdominal) 411 EMG muscle activity. This was reflected by lower EMG activity of intercostal (by: 32±22%; p=0.009) and scalene (by: 32±30%; p=0.047) muscles and greater EMG 412 413 activity of rectus abdominis muscle (by: 33±31%; p=0.049) (Table 3). Accordingly, 414 greater EMG activity of the inspiratory muscles during pNIV compared to PLB was 415 evident in DH responders compared to DH non-responders for intercostal (p=0.004) 416 and scalene (p=0.007) muscles. There was no difference in the pattern of rectus 417 abdominis EMG muscle activity between DH responders and DH non-responders 418 with pNIV compared to PLB applications (p=0.538); both DH responders and DH non-419 responders increased EMG abdominal muscle activity with pNIV compared to PLB 420 (Table 3). However, DH responders exhibited a two fold greater increase in EMG 421 abdominal muscle activity with pNIV compared to PLB in comparison to DH non-422 responders (Table 3).

423 **Respiratory muscle oxygen availability**

424 In DH responders, when pNIV was applied compared to PLB, deoxygenated 425 haemoglobin was greater in intercostal muscles (by: $2.3\pm2.1 \mu$ mol/L; p=0.048) and 426 rectus abdominis muscle (by: $1.8\pm1.7 \mu mol/L$; p=0.047). In DH non-responders, pNIV 427 application compared to PLB caused greater levels of deoxygenated haemoglobin in 428 intercostal (by: 2.1 \pm 1.5 µmol/L; p=0.040) and rectus abdominis (by: 4.6 \pm 4.0 µmol/L; 429 p=0.045) muscles. There were no differences in the pattern and magnitude of 430 response of deoxygenated haemoglobin of intercostal and abdominal muscles 431 between DH responders DH non-responders.

432 Discussion

433 Main findings

434 In line with our earlier studies (10, 48) we have identified two different patterns of 435 DH response to acute application of pNIV compared to PLB in recovery from exercise 436 in COPD: DH responders showing a greater improvement in DH using pNIV compared 437 to PLB of at least 120 ml and DH non-responders failing to show this degree of 438 response with pNIV compared to PLB. When pNIV was applied in recovery from 439 exercise, DH responders compared to DH non-responders exhibited greater tidal 440 volume, inspiratory and expiratory flow rates, prolonged expiratory time and duty 441 cycle, and experienced lower end-expiratory DH secondary to greater expiratory 442 abdominal muscle recruitment. DH responders had significantly greater BMI and 443 resting inspiratory flow rate, and less severe resting hyperinflation compared to DH 444 non-responders.

445 Study novelties

446 To the best of our knowledge this is the first study to assess total and 447 compartmental thoracoabdominal volumes acutely during application of a NIV 448 method in recovery from exercise in patients with COPD. Use of optoelectronic 449 plethysmography allowed patients to breathe normally and carry out ventilatory measurements without the need of a valve and mouthpiece. In contrast to our 450 451 previous studies (10, 48), the present study used optoelectronic plethysmography to 452 assess the magnitude of dynamic hyperinflation in recovery from exercise when 453 using pNIV or PLB without requirement of inspiratory capacity manoeuvres that are 454 effort dependent (1, 2). Finally, use of optoelectronic plethysmography allowed us to 455 evaluate the breathing pattern throughout the application of pNIV and PLB including 456 breath-by-breath recordings of expiratory and inspiratory time and flow rates, total 457 duty cycle, tidal volume, breathing frequency, and minute ventilation.

458 Differences in baseline characteristics between DH responders and non-responders

459 One significant difference between DH responders and DH non-responders was 460 elevated BMI presented in the group of DH responders. A recent study (10) argued 461 that a possible mechanism that allowed DH responders compared to DH non-462 responders to benefit from pNIV was the increased BMI (10). It has previously been 463 reported that the respiratory muscles of COPD with high BMI might have a 464 mechanical advantage in comparison to patients with normal BMI (35). This has been 465 attributed to the increased inspiratory capacity (i.e. lower resting hyperinflation) in 466 patients with high BMI, which was evident in the DH responders in the present 467 study. Moreover, patients with high BMI might have an advantage when using pNIV, 468 which applies a high expiratory positive airway pressure (8 cmH₂O) in comparison to 469 other NIV devices (7, 19, 22, 44, 45, 47). It is known that intrinsic positive end470 expiratory pressure (PEEPi) needs to be closely matched with extrinsic positive end-471 expiratory pressure (PEEPe) (31). If PEEPe is significantly lower than PEEPi there will 472 be no improvement in operational lung volumes (14, 32). In contrast, if PEEPe is 473 much greater than PEEPi, dynamic hyperinflation will worsen and result in adverse 474 central haemodynamic responses (16, 28). Patients with higher BMI exhibit greater 475 PEEPi (35), thus NIV devices with higher expiratory positive airway pressure (PEEPe), such as the VitaBreath device in the present study (8 cm H_2O), might be better suited 476 477 to patients with high BMI (10). Future devices may be able to tailor the expiratory 478 pressure to overcome expiratory flow limitation in individual patients.

479 **DH responders**

Application of pNIV compared to PLB was associated with increased end-inspiratory rib cage and total thoracoabdominal volumes in DH responders. This finding is explained by the high fixed IPAP (18 cmH₂O) provided by the VitaBreath device, but is in line with other NIV methods showing an inflation of the rib cage compartment with NIV application (43). However, application of pNIV compared to PLB lessened end-expiratory abdominal and total thoracoabdominal volumes in DH responders.

It is well known that COPD patients develop varying degrees of expiratory flow 486 487 limitation. This leads to DH at different ventilatory levels during exercise, but which 488 greatly differ among patients with COPD (21, 49). Indeed, Vogiatzis and colleagues 489 identified two different DH patterns during exercise and in recovery from exercise, 490 namely early and late DH (49). COPD patients who developed late DH during exercise 491 were those who compensated end-expiratory rib cage DH by expiratory abdominal 492 muscle recruitment (49). When using pNIV, DH responders in the present study exhibited a similar pattern to that previously described for late DH (49); they were 493 494 able to compensate end-expiratory rib cage DH by recruiting their expiratory 495 abdominal muscles. Furthermore, during exercise and during acute pNIV application, 496 DH responders exhibited greater expiratory flow rates compared to PLB thereby indicating lower degrees of expiratory flow limitation. Presumably, when using pNIV 497 498 compared to PLB, expiratory abdominal muscle recruitment in conjunction with 499 greater expiratory flow rate and marginally prolonged expiratory time was effective 500 in reducing end-expiratory DH in recovery from exercise (27). Greater expiratory abdominal muscle recruitment with pNIV compared to PLB was in turn corroborated 501 by greater rectus abdominis muscle EMG activity alongside increased rectus 502 503 abdominis deoxygenated haemoglobin; this suggests greater oxygen extraction due 504 to increased muscle activation.

505 DH responders were less flow limited during exercise and during acute pNIV 506 application compared to DH non-responders, inferred by the greater inspiratory and 507 expiratory flow rates (Figure 3), allowing them to increase tidal volume more than 508 DH non-responders. Thoracoabdominal tidal volume during acute application of 509 pNIV was nearly two-fold greater in DH responders than DH non-responders (Table 510 2). DH responders were able to expand their tidal volume firstly by increasing their 511 end-inspiratory thoracoabdominal volume, and secondly by decreasing their end-512 expiratory thoracoabdominal volume during acute application of pNIV. This increase 513 in tidal volume was the result of greater thoracoabdominal volume at total lung 514 capacity, allowing a larger increase in end-inspiratory volume up to the point of 515 reaching critical mechanical constraints (Figure 2 a) (38). Greater end-inspiratory 516 thoracoabdominal volume was also associated with greater intercostal and scalene 517 EMG muscle activity and inspiratory flow rates. The increased tidal volume during 518 acute pNIV application was the result of increased abdominal muscle recruitment, 519 which was greater in DH responders compared to DH non-responders (Figure 2c & 520 2f). This finding is further supported by the EMG data on rectus abdominis showing a 521 two-fold increase in EMG activity with pNIV compared to PLB in DH responders 522 versus DH non-responders. Thus, greater expiratory abdominal power output (the 523 product of their velocity of shortening and the force they develop) in DH responders 524 was expressed more as expiratory flow and less as pressure secondary to lower 525 dynamic airway compression (27). This is most likely the reason why we did not find 526 impaired central hemodynamic responses with pNIV compared to PLB in DH 527 responders. However, greater EMG rectus abdominis muscle activity with pNIV 528 compared to PLB application may account for the lack of difference in dyspnoea 529 levels despite lower DH, given that increased expiratory muscle activity during 530 positive-pressure breathing has been postulated to increase breathlessness (42). 531 Moreover, in DH-responders there was no meaningful difference in dyspnoea 532 between pNIV and PLB. This might be attributed to IRV with pNIV been lower 533 compared to PLB as a result of significantly greater tidal volume expansion with pNIV 534 application (Table 2) (40). Furthermore inspiratory muscle (intercostal and scalene) 535 activity was significantly greater with pNIV compared to the PLB technique (Table 3). 536 Increased inspiratory muscle effort has been shown to be associated with a rise in 537 perceived inspiratory difficulty reflecting increased dissociation between the 538 increased central neural drive and the blunted mechanical response of the 539 respiratory system (23, 37).

540

541 **DH non-responders**

Application of pNIV compared to PLB was associated with increased end-inspiratory and end-expiratory rib cage volumes. However, the increase in end-expiratory rib cage volume was not compensated by a reduction in end-expiratory abdominal volume as reported above for DH responders. This led to an increase in total endexpiratory thoracoabdominal volume and thus DH, which limited tidal volume expansion. In line with our earlier studies (10, 48) tidal volume expansion was restricted with pNIV compared to PLB application; patients adopted a more tachypnoeic-breathing pattern that reduced inspiratory and expiratory time as well as duty cycle. However, both inspiratory and expiratory flow rates were greater with pNIV compared to PLB secondary to the high fixed airway pressures delivered pNIV.

During pNIV compared to PLB, DH non-responders exhibited greater rectus 552 553 abdominis EMG activity (and deoxygenated haemoglobin) which, despite the 554 increase in expiratory flow rate, was not successful in mitigating end-expiratory 555 thoracoabdominal DH. This is most likely occurred because in DH non-responders 556 PEEPe did not closely match PEEPi (14), confirming earlier concerns that the fixed IPAP and EPAP were probably suboptimal, at least for DH non-responders (10, 48). 557 558 DH non-responders may have benefited if the expiratory pressure was automatically 559 tailored to the individual to overcome expiratory flow limitation, whilst avoiding 560 excessive pressures.

561 Furthermore, inspiratory EMG muscle activity was lower with pNIV compared to PLB as the high inspiratory positive airway pressure (18 cmH_2O) was effective in 562 overcoming inspiratory flow limitation, thereby necessitating less effort from the 563 564 inspiratory muscles. Reduced work of breathing with inspiratory positive airway 565 pressure is possibly associated with lower dyspnoea (20). Interestingly, in DH non-566 responders, dyspnoea was significantly lower in the pNIV trial compared to PLB. This 567 is attributed to the finding that inspiratory muscle (intercostal and scalene) activity 568 was significantly greater with PLB compared to the pNIV (Table 3), thereby inducing 569 a greater rise in perceived inspiratory difficulty (23, 37).

570 Thoracoabdominal volumes during exercise and in recovery

571 In the present study, thoracoabdominal volume at total lung capacity increased from 572 baseline during exercise by an average of 326 ml. This finding is in agreement with a 573 previous study in which COPD patients progressively increased thoracoabdominal 574 volumes at total lung capacity by approximately 200 ml, during a ramp incremental 575 exercise protocol (49). However, despite the fact that patients in the present study 576 performed intermittent submaximal exercise, we report greater increase in 577 thoracoabdominal volumes at total lung capacity compared to that study (49). This 578 might be attributed to the application of pNIV during the recovery periods between 579 exercise bouts, which increased end-inspiratory thoracoabdominal volume in both 580 DH responders and DH non-responders. Importantly, in both DH responders and DH 581 non-responders end-expiratory thoracoabdominal volume did not recover towards 582 quiet breathing by five minutes into recovery. This is in keeping with the studies (41, 583 49) that found that dynamic hyperinflation 3-5 minutes into recovery from symptom 584 limited exercise was greater than at baseline. The present study extends these 585 findings by showing that in both DH responders and DH non-responders, rib cage 586 hyperinflation during exercise and recovery should have enhanced the threshold loading of the muscles of the rib cage compartment so that recovery ofhyperinflation would take longer to return to baseline (41).

589 Haemodynamic responses

590 Previous studies have reported that application of NIV in patients with COPD at rest 591 reduces cardiac output (4, 11). Our short application time of pNIV (1-min) in both DH 592 responders and DH non responders may have prevented adverse circulatory effects; 593 this is in contrast to the existing literature where NIV application exceeded 5 minutes 594 and resulted in adverse circulatory responses (4, 5, 11, 24).

595 Study limitations

596 Some outcomes were clinically, but not statistically, significant. This may simply 597 reflect the limited sample size and a definitive outcome may have been achieved in a 598 larger population. The present study was powered to identify differences in the rate 599 of DH between pNIV and PLB. Moreover, we did not measure PEEPi and work of 600 breathing. Measurement of PEEPi could have helped us compare the differences 601 between PEEPe provided by pNIV and the actual PEEPi of DH responders and DH 602 non-responders; this in turn could have potentially further supported the 603 interpretation of our findings. Assessment of the work of breathing would have 604 allowed us compare our findings with the study by Petrof and colleagues (43) who 605 employed CPAP during exercise and further corroborate their findings as we 606 measured respiratory electromyography muscle activity. Although we only recorded 607 the EMG activation of the respiratory muscles during the recovery periods, it is 608 possible that signal could be contaminated by abdominal muscle activation for the 609 purposes of core stabilization whilst sitting on the cycle ergometer. The validity of 610 both surface EMG and NIRS recordings has been previously established (15, 29, 30). 611 Although we ensured that the quality of our measurements was sufficient to include 612 in our analysis, high adipose tissue on the abdomen is possible to have affected the 613 quality of the EMG and NIRS signals.

Furthermore, it is surprising that DH responders showed no difference in breathlessness between pNIV and PLB application. This finding might be due to the fixed duration of exercise as in our earlier study DH responders exercised for longer compared to DH non-responders consequently to lower breathlessness at isotime (10). Interestingly this earlier study from our group showed that in DH responders, use of pNIV during daily activities over a 12-week period made them less anxious about becoming breathlessness compared to DH non-responders (10).

Finally, in contrast to the existing literature using other NIV methods (39, 43) inspiratory and expiratory positive airway pressures were fixed and could not be adjusted for each patient in the present study. Accordingly, DH non-responders may 624 have responded well to different settings tailored to their physiological needs. 625 Individualized pressure titration using a NIV module with adjustable settings may 626 have provided more useful insight by clarifying whether an optimal pressure setting 627 exists that offers equivalent or superior relief compared to PLB. This technology 628 already exists, has been incorporated in standard home ventilators and could be 629 implemented in future pNIV devices. This warranties further studies to test this 630 possibility. We did not assess the reproducibility of physiological measures during the pNIV and PLB trials to avoid exposure of patients to additional exercise testing. 631

632 Clinical implications

633 The delayed recovery of dynamic hyperinflation following cessation of intermittent 634 exercise has important clinical implications when designing rehabilitative exercise training regimes for patients with severe COPD, particularly if NIV is to be applied 635 636 only during recovery from exercise. It is apparent from our results that whilst acute 637 pNIV application was effective only in a specific subgroup of patients, clinical 638 characteristics such as baseline hyperinflation can help predict response. 639 Furthermore, COPD patients whose breathing control resembles that of a healthy 640 individual in recruiting expiratory muscles during exercise (1, 50) are more likely to 641 benefit from NIV; they may mitigate rib cage dynamic hyperinflation by expiratory 642 abdominal muscle recruitment. Nevertheless, DH non-responders were less 643 breathless and had greater expiratory flow with pNIV, therefore pNIV was not 644 without some benefit even to this subgroup of patients. During recovery from 645 exercise the improvement in DH lasted only transiently (1-min, during pNIV 646 application) in DH responders. If implementing the use of NIV in the pulmonary 647 rehabilitation setting NIV should perhaps be applied for longer to facilitate complete 648 recovery of DH before moving to a new exercise task. However, considering the 649 variation in response we have reported, it is important that clinicians assess the 650 response to pNIV on an individual basis in order to verify whether using a portable NIV device during rehabilitation or at home makes the patient feeling better or 651 652 worse. An earlier study from our group showed that in DH responders, use of pNIV 653 during daily activities over a 12-week period made them less anxious about 654 becoming breathlessness compared to DH non-responders (10).

655

656 *Conclusions*

657 COPD patients most likely to benefit from NIV in their recovery from exercise are 658 those who are able, during exercise and in recovery from exercise, to mitigate end-659 expiratory rib cage dynamic hyperinflation by expiratory abdominal muscle 660 recruitment alongside increased expiratory flow rates.

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663

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668

669 Disclosure

670 The authors declare that they have no competing interests.

671 References

672 1. Aliverti A. Mechanics of Breathing- New Insights from New Technologies. 2014. 673 2. Aliverti A, and Pedotti A. Opto-electronic Plethysmography. In: Mechanics of 674 Breathing, edited by Aliverti A, Brusasco V, Macklem PT, and Pedotti A. Milano: Springer 675 Milan, 2002, p. 47-59. 676 3. Ambrosino N, and Cigni P. Non invasive ventilation as an additional tool for exercise 677 training. Multidisciplinary respiratory medicine 10: 14, 2015. 678 4. Ambrosino N, Nava S, Torbicki A, Riccardi G, Fracchia C, Opasich C, and Rampulla C. 679 Haemodynamic effects of pressure support and PEEP ventilation by nasal route in patients 680 with stable chronic obstructive pulmonary disease. Thorax 48: 523-528, 1993. 681 5. Baratz DM, Westbrook PR, Shah PK, and Mohsenifar Z. Effect of nasal continuous 682 positive airway pressure on cardiac output and oxygen delivery in patients with congestive 683 heart failure. Chest 102: 1397-1401, 1992. Borg GA. Psychophysical bases of perceived exertion. Med Sci Sports Exerc 14: 377-684 6. 685 381, 1982. 686 7. Borghi-Silva A, Mendes RG, Toledo AC, Malosá Sampaio LM, da Silva TP, 687 Kunikushita LN, Dutra de Souza HC, Salvini TF, and Costa D. Adjuncts to physical training of 688 patients with severe COPD: oxygen or noninvasive ventilation? Respiratory care 55: 885-894, 689 2010. 690 8. Cardoso DM, Fregonezi GA, Jost RT, Gass R, Alberton CL, Albuquerque IM, Paiva 691 DN, and Barreto SS. Acute effects of Expiratory Positive Airway Pressure (EPAP) on different 692 levels in ventilation and electrical activity of sternocleidomastoid and parasternal muscles in 693 Chronic Obstructive Pulmonary Disease (COPD) patients: a randomized controlled trial. 694 Brazilian journal of physical therapy 20: 525-534, 2016. 695 Charloux A, Lonsdorfer-Wolf E, Richard R, Lampert E, Oswald-Mammosser M, 9. 696 Mettauer B, Geny B, and Lonsdorfer J. A new impedance cardiograph device for the non-697 invasive evaluation of cardiac output at rest and during exercise: comparison with the 698 "direct" Fick method. Eur J Appl Physiol 82: 313-320, 2000. 699 Chynkiamis N, Armstrong M, Hume E, Alexiou C, Snow L, Lane ND, Hartley T, 10. 700 Bourke SC, and Vogiatzis I. Effect of portable non-invasive ventilation on exercise tolerance 701 in COPD: One size does not fit all. Respiratory physiology & neurobiology 277: 103436, 2020. 702 Diaz O, Iglesia R, Ferrer M, Zavala E, Santos C, Wagner PD, Roca J, and Rodriguez-11. 703 Roisin R. Effects of noninvasive ventilation on pulmonary gas exchange and hemodynamics 704 during acute hypercapnic exacerbations of chronic obstructive pulmonary disease. American 705 journal of respiratory and critical care medicine 156: 1840-1845, 1997. 706 12. Diaz O, Villafranca C, Ghezzo H, Borzone G, Leiva A, Milic-Emil J, and Lisboa C. Role 707 of inspiratory capacity on exercise tolerance in COPD patients with and without tidal 708 expiratory flow limitation at rest. Eur Respir J 16: 269-275, 2000. 709 13. Eltayara L, Becklake MR, Volta CA, and Milic-Emili J. Relationship between chronic 710 dyspnea and expiratory flow limitation in patients with chronic obstructive pulmonary 711 disease. American journal of respiratory and critical care medicine 154: 1726-1734, 1996. 712 Gay PC, Rodarte JR, and Hubmayr RD. The effects of positive expiratory pressure on 14. 713 isovolume flow and dynamic hyperinflation in patients receiving mechanical ventilation. The 714 American review of respiratory disease 139: 621-626, 1989. 715 Gilleard WL, and Brown JM. An electromyographic validation of an abdominal 15. 716 muscle test. Archives of physical medicine and rehabilitation 75: 1002-1007, 1994. 717 Grubler MR, Wigger O, Berger D, and Blochlinger S. Basic concepts of heart-lung 16. 718 interactions during mechanical ventilation. Swiss medical weekly 147: w14491, 2017. 719 Hardy W, and Jasko J. Evaluation of a Portable Positive Pressure Device to Relieve 17. 720 Dyspnea During Exercise in COPD Patients. 2015.

721 18. Hyatt RE. Expiratory flow limitation. Journal of applied physiology: respiratory, 722 environmental and exercise physiology 55: 1-7, 1983. 723 Johnson JE, Gavin DJ, and Adams-Dramiga S. Effects of training with heliox and 19. 724 noninvasive positive pressure ventilation on exercise ability in patients with severe COPD. 725 Chest 122: 464-472, 2002. 726 Kallet RH, and Diaz JV. The physiologic effects of noninvasive ventilation. Respir 20. 727 Care 54: 102-115, 2009. 728 21. Koulouris NG, Dimopoulou I, Valta P, Finkelstein R, Cosio MG, and Milic-Emili J. 729 Detection of expiratory flow limitation during exercise in COPD patients. Journal of Applied 730 Physiology 82: 723-731, 1997. 731 Labeix P, Berger M, Court Fortune I, Feasson L, Verges S, and Costes F. Quadriceps 22. 732 Endurance Increases Following Cycling Exercise With Non-Invasive Ventilation In Moderate-733 To-Severe COPD Patients. A Non-Randomized Controlled Study. Int J Chron Obstruct Pulmon 734 Dis 14: 2461-2468, 2019. 735 23. Laveneziana P, Webb KA, Wadell K, Neder JA, and O'Donnell DE. Does expiratory 736 muscle activity influence dynamic hyperinflation and exertional dyspnea in COPD? Respir 737 Physiol Neurobiol 199: 24-33, 2014. 738 24. Leech JA, and Ascah KJ. Hemodynamic effects of nasal CPAP examined by Doppler 739 echocardiography. Chest 99: 323-326, 1991. 740 25. Louvaris Z, Habazettl H, Wagner H, Zakynthinos S, Wagner P, and Vogiatzis I. Nearinfrared spectroscopy using indocyanine green dye for minimally invasive measurement of 741 742 respiratory and leg muscle blood flow in patients with COPD. Journal of applied physiology 743 (Bethesda, Md : 1985) 125: 947-959, 2018. 744 26. Louvaris Z, Spetsioti S, Andrianopoulos V, Chynkiamis N, Habazettl H, Wagner H, 745 Zakynthinos S, Wagner PD, and Vogiatzis I. Cardiac output measurement during exercise in 746 COPD: A comparison of dye dilution and impedance cardiography. Clin Respir J 13: 222-231, 747 2019. 27. 748 Macklem PT. Exercise in COPD: damned if you do and damned if you don't. Thorax 749 60: 887-888, 2005. 750 Mahmood SS, and Pinsky MR. Heart-lung interactions during mechanical 28. 751 ventilation: the basics. Annals of translational medicine 6: 349, 2018. 752 29. Mancini DM, Bolinger L, Li H, Kendrick K, Chance B, and Wilson JR. Validation of 753 near-infrared spectroscopy in humans. J Appl Physiol (1985) 77: 2740-2747, 1994. 754 30. Marshall P, and Murphy B. The validity and reliability of surface EMG to assess the 755 neuromuscular response of the abdominal muscles to rapid limb movement. Journal of 756 electromyography and kinesiology : official journal of the International Society of 757 Electrophysiological Kinesiology 13: 477-489, 2003. 758 Milesi I, Porta R, Barbano L, Cacciatore S, Vitacca M, and Dellacà RL. Automatic 31. 759 tailoring of the lowest PEEP to abolish tidal expiratory flow limitation in seated and supine 760 COPD patients. Respir Med 155: 13-18, 2019. 761 32. Milesi I, Porta R, Cacciatore S, Vitacca M, Dellacà R, and Barbano L. Effects of 762 automatic tailoring of Positive End Expiratory Pressure (PEEP) by Forced Oscillation 763 Technique (FOT) during nocturnal Non-Invasive Ventilation (NIV) in Chronic Obstructive 764 Pulmonary Disease (COPD). European Respiratory Journal 50: PA2179, 2017. 765 33. **Milic-Emili J.** Inspiratory capacity and exercise tolerance in chronic obstructive 766 pulmonary disease. Canadian respiratory journal 7: 282-285, 2000. 767 34. Nasis I, Kortianou E, Vasilopoulou M, Spetsioti S, Louvaris Z, Kaltsakas G, Davos CH, Zakynthinos S, Koulouris NG, and Vogiatzis I. Hemodynamic effects of high intensity interval 768 769 training in COPD patients exhibiting exercise-induced dynamic hyperinflation. Respiratory 770 physiology & neurobiology 217: 8-16, 2015.

771 35. O'Donnell DE, Ciavaglia CE, and Neder JA. When obesity and chronic obstructive 772 pulmonary disease collide. Physiological and clinical consequences. Ann Am Thorac Soc 11: 773 635-644, 2014. 774 36. O'Donnell DE, D'Arsigny C, and Webb KA. Effects of hyperoxia on ventilatory 775 limitation during exercise in advanced chronic obstructive pulmonary disease. American 776 journal of respiratory and critical care medicine 163: 892-898, 2001. 777 O'Donnell DE, Hamilton AL, and Webb KA. Sensory-mechanical relationships during 37. 778 high-intensity, constant-work-rate exercise in COPD. Journal of applied physiology 779 (Bethesda, Md : 1985) 101: 1025-1035, 2006. 780 O'Donnell DE, Revill SM, and Webb KA. Dynamic hyperinflation and exercise 38. 781 intolerance in chronic obstructive pulmonary disease. American journal of respiratory and 782 critical care medicine 164: 770-777, 2001. 783 O'Donnell DE, Sanii R, Giesbrecht G, and Younes M. Effect of continuous positive 39. 784 airway pressure on respiratory sensation in patients with chronic obstructive pulmonary disease during submaximal exercise. The American review of respiratory disease 138: 1185-785 786 1191, 1988. 787 40. O'Donnell DE, and Webb KA. Exertional breathlessness in patients with chronic 788 airflow limitation. The role of lung hyperinflation. The American review of respiratory disease 789 148: 1351-1357, 1993. 790 41. O'Donnell D, Johnson B, Richter K, Kesten S, and Hamilton A. Inspiratory capacity 791 and dyspnoea during recovery from symptom-limited exercise in COPD patients treated with 792 tiotropium. Eur Respir J 24: 214s, 2004. 793 Paton J, Swaminathan S, Sargent C, and Keens T. Expiratory muscle endurance and 42. 794 the oxygen cost of expiration in normal adults. In: CLINICAL RESEARCHSLACK INC 6900 795 GROVE RD, THOROFARE, NJ 08086, 1989, p. A214-A214. 796 Petrof BJ, Calderini E, and Gottfried SB. Effect of CPAP on respiratory effort and 43. 797 dyspnea during exercise in severe COPD. Journal of applied physiology (Bethesda, Md : 1985) 798 69: 179-188, 1990. 799 44. Renston JP, DiMarco AF, and Supinski GS. Respiratory muscle rest using nasal BiPAP 800 ventilation in patients with stable severe COPD. Chest 105: 1053-1060, 1994. 801 45. Reuveny R, Ben-Dov I, Gaides M, and Reichert N. Ventilatory support during 802 training improves training benefit in severe chronic airway obstruction. Isr Med Assoc J 7: 803 151-155, 2005. 804 Tan KH, Lai FO, and Hwang NC. Measurement of cardiac output using Physio Flow 46. 805 with different positions of electrode placement. Singapore Med J 47: 967-970, 2006. 806 47. Toledo A, Borghi-Silva A, Sampaio LM, Ribeiro KP, Baldissera V, and Costa D. The 807 impact of noninvasive ventilation during the physical training in patients with moderate-to-808 severe chronic obstructive pulmonary disease (COPD). Clinics (Sao Paulo) 62: 113-120, 2007. 809 48. Vogiatzis I, Chynkiamis N, Armstrong M, Lane ND, Hartley T, Gray WK, and Bourke 810 SC. Intermittent Use of Portable NIV Increases Exercise Tolerance in COPD: A Randomised, 811 Cross-Over Trial. J Clin Med 8: 94, 2019. 812 49. Vogiatzis I, Georgiadou O, Golemati S, Aliverti A, Kosmas E, Kastanakis E, Geladas 813 N, Koutsoukou A, Nanas S, Zakynthinos S, and Roussos C. Patterns of dynamic 814 hyperinflation during exercise and recovery in patients with severe chronic obstructive 815 pulmonary disease. *Thorax* 60: 723-729, 2005. 816 Vogiatzis I, and Zakynthinos S. Factors limiting exercise tolerance in chronic lung 50. 817 diseases. Compr Physiol 2: 1779-1817, 2012. 818 WorldMedicalAssociation. Declaration of Helsinki World Medical Associaton. 51.

819 https://www.wma.net/what-we-do/medical-ethics/declaration-of-helsinki/. [14 Jan, 2019].

Figures legends

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Figure 1. Effect of the application of portable non-invasive ventilation (pNIV) (closed symbols) compared to pursed lip breathing (PLB) (open symbols) on: a) total thoracoabdominal volume, b) rib cage volume and c) abdominal volume in all patients. Circles: end-expiratory volume, triangles: end-inspiratory volume, rhombuses: total thoracoabdominal volume. Grey area highlights acute application of pNIV or PLB. Data are presented as mean ± SEM. QB: quiet breathing, REC: recovery. * p < 0.05 pNIV vs PLB.

829

830 Figure 2. Effect of the application of portable non-invasive ventilation (pNIV) (closed 831 symbols) compared to pursed lip breathing (PLB) (open symbols) in DH responders (left 832 panel) and DH non-responders (right panel) on: a & d) total thoracoabdominal volume, b & 833 e) rib cage volume and c & f) abdominal volume. Circles: end-expiratory volume, triangles: 834 end-inspiratory volume, rhombuses: total thoracoabdominal volume. Grey area highlights 835 acute application of pNIV or PLB. Data are presented as mean ± SEM. QB: quiet breathing, 836 REC: recovery. * p<0.05 pNIV vs PLB, † p<0.05 QB vs exercise in end-expiratory volume, §; 837 minimum clinical importance difference between pNIV and PLB.

838

Figure 3. Effect of the application of portable non-invasive ventilation (pNIV) (closed symbols) compared to pursed lip breathing (PLB) (open symbols) in DH responders (circles) and DH non-responders (triangles) on: a) inspiratory flow rate and b) expiratory flow rate.
Data are presented as mean ± SEM. QB: quiet breathing, REC: recovery.* p<0.05 pNIV vs
PLB, ‡ p<0.05 between responders versus non-responders with pNIV.

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Figure 4. Effect of the application of portable non-invasive ventilation (pNIV) (closed symbols) compared to pursed lip breathing (PLB) (open symbols) in DH responders (left panel) and DH non-responders (right panel) on: a & d) stroke volume, b & e) heart rate and c & f) cardiac output. Data are presented as mean ± SEM. QB: quiet breathing, REC: recovery.
* p < 0.05 pNIV vs PLB.



Figure 1



Figure 3





Figure 4







	All patients	DH Responders	DH Non-responders	D
	(n=14)	(n=7)	(n=7)	P
Age (years)	68.4±8.4	67.7±6.1	69.1±10.7	0.764
BMI (kg/m²)	28.6±7.2	32.8±6.7	24.4±5.0	0.022
FEV ₁ (L)	1.34±0.69	1.53±0.81	1.14±0.53	0.301
FEV ₁ (% predicted)	55±22	56±23	54±21	0.861
FVC (L)	2.91±1.07	3.28±1.00	2.53±1.08	0.204
FVC (% predicted)	95±26	93±22	96±31	0.876
FEV ₁ /FVC	45±13	45±14	45±12	0.984
TLC (% predicted)	126±36	134±41	117±30	0.432
FRC (% predicted)	151±56	167±62	135±50	0.355
RV (% predicted)	173±81	191±93	155±71	0.465
IC (% predicted)	63±18	68±20	58±16	0.319
IC/TLC (%)	35±10	34±8	37±13	0.581
RV/TLC (%)	53±14	53±14	53±15	0.984
DLco (% predicted)	50±19	50±24	49±15	0.930
Inspiratory flow rate (L/sec)	0.5±0.2	0.6±0.2	0.4±0.1	0.042
Expiratory flow rate (L/sec)	0.3±0.1	0.3±0.2	0.3±0.1	0.266
WRpeak (Watts)	56±27	63±31	49±21	0.097
WRpeak (% predicted)	54±30	52±39	56±22	0.778
VO₂peak (% predicted)	71±19	72±19	69±20	0.758
ΔIC peak (ml)	-575±246	-621±173	-529±309	0.501

Table 1 Patient Demographic data

BMI, body mass index; FEV₁, forced expiratory volume in the first second; FVC, forced vital capacity; TLC, total lung capacity; FRC, functional residual capacity; RV, residual volume; IC, inspiratory capacity; DLco, transfer factor of the lung for carbon monoxide; WRpeak, peak work rate; VO₂peak, peak oxygen uptake; Δ IC, change from baseline in inspiratory capacity; values presented as mean ± SD for all baseline characteristics.

	Responders			Non-Responders		
	pNIV	PLB	р	pNIV	PLB	р
V _T (L)	1.9±0.7	1.4±0.5	0.002	1.1±0.3*	1.2±0.4	0.369
bf (breaths/min)	21±3	22±5	0.478	27±5*	20±4	0.002
V _E (L/min)	39.0±16.6	32.5±12.4	0.009	29.1±7.6	23.4±9.2	0.018
Ti (sec)	1.1±0.2	1.2±0.3	0.454	1.0±0.2	1.3±0.3	0.019
Te (sec)	1.9±0.4	1.8±0.3	0.765	1.3±0.3*	2.1±0.6	0.001
Ttot (sec)	3.0±0.4	3.0±0.5	0.828	2.3±0.4*	3.4±0.8	0.001
Inspiratory flow rate (L/sec)	1.8±0.6	1.4±0.5	0.001	1.2±0.4*	1.0±0.4	0.064
Expiratory flow rate (L/sec)	1.1±0.5	0.9±0.4	0.048	0.9±0.2	0.7±0.3	0.011
IRV (ml)	200±446	502±477	0.078	240±549	444±246	0.252
Dyspnoea (Borg)	3.1±1.3	3.0±1.3	0.745	2.5±0.7	3.6±1.1	0.001
Leg Discomfort (Borg)	3.8±1.7	3.9±2.0	0.880	3.5±0.9	4.0±1.5	0.203

pNIV: portable non-invasive ventilation, PLB: pursed lip breathing, V_T: tidal volume, bf: breathing frequency, V_E: minute ventilation, Ti: inspiratory time; Te: expiratory time; Ttot: duty cycle time, IRV: inspiratory reserve volume *; p<0.05 responders versus non-responders with pNIV application. Data presented as mean \pm SD

Table 2. Breathing pattern and symptoms during acute application of pNIV and PLB

Table 3.	Electromyographic activity of respiratory muscles during a	cute application of
pNIV or	PLB	

	Responders			Non-Responders			
	pNIV	PLB	р	pNIV	PLB	р	
Intercostal (% baseline)	111±26	91±28	0.043	103±33	135±70	0.009	
Scalene (% baseline)	192±81	142±38	0.013	143±43	175±79	0.047	
Rectus abdominis (% baseline)	175±126	108±25	0.014	179±140	146±59	0.049	

pNIV; portable non-invasive ventilation, PLB pursed lip breathing. Data presented as mean ± SD of the fractional change in electromyographic activity from baseline values

Table 4.	Respiratory	muscle	oxygen	availability

	R	esponders		Non-Responders			
	pNIV	PLB	р	pNIV	PLB	р	
ΔHbO₂ intercostal (µmol/L)	-2.0±4.2	-3.4±3.0	0.120	-1.7±1.6	-2.4±2.1	0.449	
ΔHbO₂ abdominal (µmol/L)	0.8±1.0	-0.2±1.5	0.421	0.8±6.2	-3.3±3.9	0.378	
ΔHHb intercostal (µmol/L)	3.5±3.0	1.2±1.4	0.048	5.3±3.7	3.2±4.7	0.040	
ΔHHb abdominal (µmol/L)	4.6±1.7	2.8±3.8	0.047	3.5±3.3	-1.1±1.8	0.045	
ΔTOI intercostal (%)	-3.0±1.9	-4.0±2.2	0.597	-3.4±1.1	-2.6±1.9	0.505	
ΔTOI abdominal (%)	-4.1±3.2	-3.0±2.7	0.070	-5.8±2.6	-1.6±2.7	0.031	

pNIV; portable non-invasive ventilation, PLB; pursed lip breathing, Δ HbO₂: change in oxygenated haemoglobin from baseline, Δ HHb: change in deoxygenated haemoglobin from baseline, Δ TOI: change in tissue oxygen index from baseline. Data are presented as mean ± SD