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1 **Distribution of technetium-99m PEG-liposomes during oligofructose-induced laminitis**
2 **development in horses**

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23 **Highlights**

- 24 • This study investigated whether polyethylene-glycol (PEG) coated liposomes accumulate in
- 25 the lamellar tissue during laminitis development
- 26 • ^{99m}Tc -PEG-liposomes were administered to normal horses and horses with oligofructose-
- 27 induced laminitis
- 28 • Scintigraphic examination and lamellar tissue collection demonstrated liposome
- 29 accumulation in the lamellar tissue of horses with oligofructose-induced laminitis.
- 30 • Liposomes may have potential for targeted lamellar drug delivery in acute laminitis

31 **Abstract**

32 Liposomes are phospholipid nanoparticles used for targeted drug delivery. This study
33 aimed to determine whether intravenous liposomes accumulate in lamellar tissue during
34 laminitis development in horses so as to assess their potential for targeted lamellar drug
35 delivery. Polyethylene-glycol (PEG) coated liposomes were prepared according to the film
36 hydration method and labelled using ^{99m}Tc -hexamethyl-propylene-amine-oxime. Six horses
37 received 10 g/kg oligofructose via nasogastric tube to induce laminitis, and four control
38 horses received water via nasogastric tube. All horses received 300 μmol ^{99m}Tc -PEG-
39 liposomes (5.5 GBq) plus 5.5 $\mu\text{mol}/\text{kg}$ PEG-liposomes by slow intravenous infusion.
40 Scintigraphic imaging was performed at 0, 6 and 12 h post-infusion. Technetium-99m
41 liposome uptake was measured in regions of interest over the hoof, fetlock and metacarpus.
42 At the study end-point horses were euthanased, tissue samples collected and tissue liposome
43 levels were calculated as the percentage of the injected dose of ^{99m}Tc -liposomes per kilogram
44 of tissue. Data were analysed non-parametrically.

45 All horses receiving oligofructose developed clinical and histological signs of
46 laminitis. Technetium-99m liposome uptake in the hoof increased with time in laminitis
47 horses ($P=0.04$), but decreased with time in control horses ($P=0.01$). Technetium-99m
48 liposome levels in lamellar tissue from laminitis horses was 3.2-fold higher than controls
49 ($P=0.02$) and were also higher in laminitis vs. control skin, muscle, jejunum, colon, and
50 kidney ($P<0.05$). Liposomes accumulated in lamellar tissue during oligofructose-induced
51 laminitis development and demonstrated potential for targeted lamellar drug delivery in acute
52 laminitis. This study provides further evidence that lamellar inflammation occurs during
53 laminitis development. Liposome accumulation also occurred in the skin, muscle, jejunum,
54 colon and kidneys, suggesting systemic inflammation in this model.

55

56 *Keywords:* Nanoparticle, Horse, Liposome, Scintigraphy, Nanotechnology

57

58 Introduction

59 Acute laminitis is a crippling disease of the horse foot with irreversible pathology so
60 prophylaxis is paramount. There are three broad aetiological categories of laminitis, namely,
61 endocrinopathic, sepsis-related and supporting limb laminitis. Similar to sepsis-related organ
62 failure in humans, sepsis-related laminitis often results in the demise of the patient after
63 successful treatment of the primary condition. Sepsis is defined as documented or suspected
64 infection, plus systemic manifestations of infection (Cawcutt and Peters, 2014).

65

66 The oligofructose model of laminitis involves administration of 10 g/kg oligofructose
67 by nasogastric tube, resulting in clinical signs of enterocolitis, presumptive disruption of the
68 gastrointestinal barrier, documented endotoxaemia and subsequent laminitis development
69 (van Eps et al., 2006; Bailey et al., 2009). A systemic inflammatory response occurs
70 mirroring that which occurs during human sepsis, including the classical symptoms of
71 pyrexia, tachycardia, tachypnoea, haemoconcentration and leucocytosis (van Eps et al., 2006;
72 Belknap, 2007; Bailey et al., 2009; Cawcutt and Peters, 2014). During the development of
73 oligofructose-induced laminitis, endothelial activation, leukocyte infiltration and an increase
74 in pro-inflammatory cytokine and cyclooxygenase (COX)-2 expression occur in the lamellae
75 in common with findings seen in organ failure associated with human sepsis (Black et al.,
76 2006; Belknap et al., 2007; Tadros et al., 2012). Therefore the oligofructose model is
77 considered to be an appropriate model for naturally-occurring sepsis-related laminitis, such
78 that occurs secondary to diseases such as colitis (Belknap et al., 2007; Belknap and Black,
79 2012; van Eps, 2012; Kullmann et al., 2014).

80

81 Distal limb cryotherapy prevents sepsis-related laminitis (Van Eps and Pollitt, 2004;
82 van Eps et al., 2014; Kullmann et al., 2014), but it is labour-intensive and practically
83 challenging. Potential therapeutic targets involved in the pathophysiology of sepsis-related
84 laminitis have been identified and include inflammation (Belknap et al., 2007; Leise et al.,
85 2011, 2012; Visser and Pollitt, 2011; Tadros et al., 2012), proteolytic enzyme activation
86 (Pollitt et al., 1998; Visser and Pollitt, 2012; Wang et al., 2012) and wntless-related
87 integration site (Wnt)-pathway dysregulation (Wang et al., 2013). Pharmaceuticals directed to
88 address these targets are available and include non-steroidal anti-inflammatory drugs,
89 corticosteroids, signal transducer and activator of transcription (STAT) 3 inhibitors (Leise et
90 al., 2012), protease inhibitors (Pollitt et al., 1998; De Savi et al., 2011) and Wnt-pathway
91 agonists (Wang et al., 2013). Evaluation of these substances for laminitis prophylaxis has
92 been hindered by their unsuitability for systemic delivery due to cost, rapid clearance, low
93 bioavailability, inability to achieve therapeutic tissue concentrations, unwanted systemic side
94 effects and/or degradation in the circulation (Levin et al., 2006; Nourian et al., 2010).

95

96 Recent work has investigated methods of regional lamellar delivery (Nourian et al.,
97 2010; Underwood et al., 2015; C. Underwood et al, unpublished data). Despite initial
98 promising results (Nourian et al., 2010), intraosseous infusion of the distal phalanx does not
99 consistently yield therapeutic lamellar drug concentrations (C. Underwood et al., unpublished
100 data). Regional limb perfusion requires frequent dosing (of each limb separately) to maintain
101 therapeutic concentrations (Underwood et al., 2015), so the technique is not suitable for
102 widespread clinical application. A means of lamellar drug delivery that provides sustained,
103 therapeutic lamellar drug concentrations and has potential for clinical application is required.

104

105 Nanoparticles are ordered structures used for targeted drug delivery. They improve
106 the therapeutic index and safety profile of the substances they carry (Cordeiro et al., 2000;
107 Metselaar et al., 2003; Hofheinz et al., 2005; Rose et al., 2005). Nanoparticles also provide a
108 means of sustained delivery over a period of days or even weeks (Sahoo and Labhasetwar,
109 2003; Bakker-Woudenberg et al., 2005; Fahmy et al., 2005). As a consequence, nanoparticle
110 formulations may require a reduced dose compared to free drug, thus reducing the cost of
111 expensive pharmaceuticals (Underwood and van Eps, 2012).

112

113 Liposomes are phospholipid nanoparticles that form highly flexible delivery systems
114 with the ability to carry both hydrophilic and hydrophobic pharmaceuticals. Their safety and
115 biodistribution has been established in normal horses (Underwood et al., 2012). Small
116 polyethylene-glycol (PEG) coated liposomes are most suitable for targeted drug delivery after
117 intravenous (IV) administration. Following injection, a relatively small number of PEG-
118 liposomes are endocytosed by macrophages. Those evading endocytosis remain in circulation
119 for prolonged periods of time (Arulsudar et al., 2004). Together with their small size, these
120 long-circulating characteristics confer the ability to extravasate at sites of increased vascular
121 permeability and facilitate accumulation in the tissue around those sites (Laverman et al.,
122 2001). This has been termed the enhanced permeability and retention (EPR) effect and is the
123 underlying principle behind many passively targeted nanoparticle drug delivery systems.

124

125 Increased vascular permeability occurs at sites of inflammation that occurs during
126 laminitis development (Belknap et al., 2007; Visser, 2009; Faleiros et al., 2011; Tadros et al.,
127 2012). Therefore, liposomes may accumulate in lamellar tissue during laminitis development
128 and provide a means of targeted lamellar drug delivery. The objectives of this study were (1)

129 to establish whether liposomes accumulate in the lamellar tissue during laminitis
130 development in the oligofructose (OF) model of laminitis (a sepsis model), and (2) to
131 establish the biodistribution of liposomes during sepsis in the OF model.

132

133 **Materials and methods**

134 The project was approved by the University of Queensland Animal Ethics Committee
135 (approval number: SVS/117/11) that monitors compliance with the Animal Welfare Act
136 (2001) and The Code of Practice for the care and use of animals for scientific purposes
137 (current edition).

138

139 *Animals and laminitis induction*

140 Ten mature Standardbred geldings (aged 4-11 years, 395-583 kg bodyweight), with
141 no lameness and no gross nor radiographic abnormalities of the feet were enrolled in the
142 study. The horses were housed and fed in stables for 4 weeks prior to the experiment as
143 previously described (van Eps and Pollitt, 2006).

144

145 During the experiment the horses were housed in climate-controlled, lead lined stalls
146 and had ad libitum access to hay and water. Six horses (laminitis group) received alimentary
147 overload with OF (bolus dose of 10 g/kg OF via nasogastric tube, up to a maximum dose of
148 4.2 kg) to induce laminitis as previously described (van Eps and Pollitt, 2006). Four control
149 horses (control group) received equivalent volumes of plain water by nasogastric tube. The
150 horses were monitored every 2 h throughout the study and heart rates, respiratory rates and
151 temperatures were recorded every 6 h. Upon onset of Obel grade 2 lameness, defined as

152 lameness detectable at the walk (Obel, 1948), a single dose of phenylbutazone
153 (Phenylarthrite, Ausrichter) was administered IV at 8 mg/kg.

154

155 *Liposome preparation*

156 Dipalmitoyl phosphatidylcholine (DPPC) and PEG-(2000)-distearoyl
157 phosphatidylethanolamine (PEG-(2000)-DSPE) were obtained from Lipoid, cholesterol and
158 glutathione (GS-H) were obtained from Sigma. All chemicals were of reagent grade. A
159 chloroform/methanol mixture (10:1 volumetric ratio) containing DPPC, PEG-(2000)-DSPE
160 and cholesterol was prepared at a molar ratio of 1.85:0.15:1. A lipid film was formed by
161 rotary evaporation followed by nitrogen flushing to remove residual organic solvent. The
162 lipid film was dispersed at 50 °C in 100 mmol/L GS-H in 4-(2-hydroxyethyl)piperazine-1-
163 ethanesulfonic acid (HEPES) buffer (10 mmol/L HEPES, 135 mmol/L NaCl, pH 7.5) at a
164 total lipid concentration of 100 mmol/L. Empty liposomes were dispersed in HEPES buffer
165 only.

166

167 The liposomes were sequentially sized by extrusion using a high pressure extruder
168 (Lipex) with polycarbonate filters of 200, 100, 80 and 50 nm pore size (Whatman
169 International). Untrapped GS-H was removed by dialysis against HEPES buffer using
170 Slide-A-Lyzer dialysis cassettes with a molecular cut-off of 10 kDa (Pierce). Finally, the
171 liposomes were passed through a 0.2 mm sterile disc filter. The mean particle size was
172 determined by dynamic light-scattering with an ALV CGS-3 system (Malvern instruments).
173 The liposomes had a mean size of 85 nm with a polydispersity index of 0.139. Phospholipid
174 content was determined with a phosphate assay (Fiske, 1925; Rouser et al., 1970). The final
175 liposome preparations contained an average of 33.3 mg total lipid/mL.

176

177 *Radiolabelling of liposomes*

178 Preformed G-SH-PEG-liposomes were labelled by transporting ^{99m}Tc as a lipophilic
179 ^{99m}Tc -hexamethylpropylene-amine-oxime (HMPAO) complex through the lipid bilayer as
180 described previously (Underwood et al., 2012). The ^{99m}Tc -HMPAO was irreversibly trapped
181 in the internal aqueous phase due to reduction by the encapsulated G-SH (Oyen et al., 1996).
182 For each dose, 8.5 GBq of ^{99m}Tc was incubated with 1 mg HMPAO (Ceretek, GE
183 Healthcare). A dose calibrator (Atom Lab 400, Biodex) was used to measure the activity of
184 liposomal and non-bound ^{99m}Tc -HMPAO to enable calculation of labelling efficiency.

185

186 *Liposome administration and monitoring procedures.*

187 All horses received 300 μmol (phospholipid) ^{99m}Tc -PEG-liposomes and 5.5 μmol
188 phospholipid/kg bodyweight unlabelled PEG-liposomes in 1 L 0.9% NaCl via IV catheter
189 into the left jugular vein. Unlabelled liposomes were administered to increase the total
190 phospholipid dose to a level above that at which rapid clearance is seen (Laverman et al.,
191 2000). In the laminitis group two horses received liposomes immediately after OF
192 administration (LAM-0), two received liposomes 12 h after OF administration (LAM-12) and
193 two received liposomes 18 h after liposome administration (LAM-18). The liposomes were
194 infused slowly to avoid complement mediated hypersensitivity reactions (Szebeni, 2005).
195 Heart rate, respiratory rate and rectal temperature were monitored every 10 min for 60 min
196 from the start of the infusion.

197

198 *Imaging studies*

199 Scintigraphic examinations were performed in all horses at 1, 6 and 12 h after the start
200 of the liposome infusion (p.i.) using a large field-of-view scintillation camera with a high
201 resolution collimator (Technicare Omega 500 gamma camera, GE Healthcare) in a climate
202 controlled lead-lined room. Scans were also performed at 18 and 24 h p.i. in the LAM-0
203 group. Post-acquisition nuclear medicine software was used for image display and analysis
204 (NuQuest v3.0 imaging software, MedX).

205

206 Three-minute static images of the dorsal and lateral aspects of both forefeet were
207 acquired at each time point with the hooves positioned a set distance from the camera. Images
208 were stored in a 256×256 matrix and were analysed retrospectively by a blinded observer
209 (CU) with all measurements performed in triplicate.

210

211 The count density was established in regions of interest (ROI) over the hoof, fetlock,
212 and metacarpus in each image. The count density per second (CD/s) was calculated, and
213 corrected for both the decay and the total initial dose in each horse. The ratio of the count
214 densities in the hoof and metacarpus (hoof:metacarpus) and the fetlock and metacarpus
215 (fetlock:metacarpus) in each horse were calculated. Hoof wall surface temperature (HWST)
216 was recorded before each examination using a hand-held infra-red scanner (Exergen).

217

218 *Liposome biodistribution*

219 Blood samples were collected directly from the right jugular vein immediately
220 following liposome infusion and at 6 and 12 h p.i. Blood radioactivity was measured on a

221 shielded well scintillation gamma counter (Ludlum Instruments) and corrected for volume
222 and decay. The half-life of ^{99m}Tc -liposomes was roughly estimated by non-compartmental
223 analysis using a log-linear model on PKSolver (China Pharmaceutical University).

224

225 At the end of the study (immediately following the 12 h scintigraphic examination in
226 the LAM-12 and LAM-18 groups and the 24 h scintigraphic examination in the LAM-0
227 group) the horses were examined for lameness at the walk. Lameness was scored according
228 to the Obel grading system (Obel, 1948). The horses were euthanased with pentobarbital
229 sodium (20 mg/kg IV). Samples of lung, liver, spleen, kidney, jejunum, colon, forelimb
230 lamellar tissue, muscle, skin and adipose tissue were dissected immediately following
231 euthanasia. Samples were weighed and the activity of the sample (equivalent to the amount of
232 ^{99m}Tc -liposomes present in the sample (Phillips et al., 1992) was measured using a shielded
233 well scintillation gamma counter (Ludlum instruments). To correct for physical decay, an
234 aliquot of the original injected dose was counted simultaneously. The results were expressed
235 as percentage injected dose/kg of tissue (% ID/kg).

236

237 *Histological evaluation*

238 Dorsal lamellar sections from the forelimbs were fixed using 10% neutral buffered
239 formalin, processed by routine paraffin embedding, sectioned at 4 μm and stained with
240 haematoxylin and eosin and periodic acid–Schiff for light microscopy as previously
241 described (Pollitt, 1996). Histological analysis was performed by a blinded observer (AVE).
242 The severity of laminitis pathology was scored for each section using a system based on the
243 0-3 scale previously described by Pollitt (Pollitt, 1996).

244

245 *Data analyses*

246 Data were analysed using a statistical software package (GraphPad Prism 6). The data
247 were tested for normality using D'Agostino-Pearson omnibus normality tests. Data
248 distributions were either non-Gaussian, or group numbers were too small to presume a
249 normal distribution, hence non-parametric tests were used. Non-paired data were compared
250 by Mann *U* Whitney tests. Comparisons of repeated measured were analysed using Friedman
251 analyses with Dunn's post-tests. For the analysis of scintigraphic data only data from the final
252 12 h of the LAM-0 group were used. Significance was set at $P \leq 0.05$. Unless otherwise stated,
253 data are expressed as median [interquartile range].

254

255 **Results**

256 All horses that received OF (the laminitis group) developed fever, diarrhoea and
257 lameness (Obel grade 2-3). Median histological scores were significantly greater in the
258 laminitis group (1.5[1-2]) compared to the control group (0[0-0.38], $P=0.01$).

259

260 Radiolabelling efficiency was 82[63-90]% and the median activity of the ^{99m}Tc -
261 liposomes immediately prior to infusion was 5.5[4.5-6.6] GBq. There was no difference in
262 the median radioactivity of the ^{99m}Tc -liposomes administered to laminitis versus control
263 horses (5.0[4.2-6.8] GBq vs. 6.1[4.8-6.4] GBq, respectively). Each horse received the full
264 liposome dose and the median infusion time was 38[35-49] min. No adverse reactions were
265 detected and there were no significant changes in heart rate, respiratory rate or temperature
266 during the infusion (data not shown).

267

268 Based on the radioactivity in sequential blood samples (corrected for decay), the
269 ^{99m}Tc -liposomes exhibited slow elimination from the circulation with a median half-life of
270 22.9[8.4-32.4] h. Due to the limited number of time-points, these half-lives are only a rough
271 estimate. There was no difference in the median half-life between the laminitis and control
272 groups. There was a decrease in the blood radioactivity (corrected for decay) with time in the
273 laminitis group ($P<0.001$; Fig. 1). At 12 h p.i. the blood radioactivities in laminitis horses
274 were lower than those in control horses ($P=0.01$; Fig. 1).

275

276 The scintigraphic images demonstrated subjective diffuse increased ^{99m}Tc -liposome
277 uptake in the hoof and distal limb of laminitis horses compared to controls; evident at 6 h,
278 and more marked at 12 h p.i. (Fig. 2). In the laminitis group the CD/s increased with time in
279 the dorsal hoof and fetlock ROIs ($P<0.01$; Figs. 3A and B). Conversely in control horses the
280 CD/s in the dorsal hoof, fetlock and metacarpal ROIs decreased with time, and the CD/s in
281 the lateral hoof ROI also decreased with time p.i ($P<0.05$; Figs. 3 A-C). The CD/s in the
282 lateral hoof ROIs were higher in laminitis horses compared to controls at 6 and 12 hours p.i.
283 ($P=0.02$; Fig. 3D). The lateral hoof:metacarpal and fetlock:metacarpal CD/s ratios were
284 higher in laminitis horses compared to controls at 12 h (1.9[1.8-2.0] vs. 1.5[1.4-1.6] and
285 1.5[1.4-1.8] vs. 1.1[1.0-1.1], respectively, $P=0.03$). There was no change in HWST with
286 time, and there was no difference in HWST between laminitis and control horses at any time-
287 point.

288

289 The ^{99m}Tc -liposomal levels in lamellar tissue of laminitis horses were higher than
290 those in controls (0.21[0.14-0.3] %ID/kg vs. 0.065[0.06-0.11] %ID/kg, respectively;
291 $P=0.019$; Fig. 4). Lamellar ^{99m}Tc -liposome levels were highest when the liposomes were
292 administered at 18 h p.i; with a 4.8 fold increase compared to control horses (Fig. 5), however
293 the numbers were too small for statistical analyses. There were increased ^{99m}Tc -liposome
294 levels in the skin, muscle, jejunum, colon and kidney of laminitis horses compared to controls
295 ($P<0.05$; Fig. 4). There was a trend towards increased ^{99m}Tc -liposome levels in the liver of
296 laminitis horses compared to controls, and towards decreased ^{99m}Tc -liposome levels in the
297 blood of laminitis horses compared to controls ($P=0.06$; Fig. 4).

298

299 Discussion

300 This study demonstrates that liposomes accumulate in the lamellar tissue during the
301 development of sepsis-related laminitis using the OF experimental model. This conclusion is
302 supported by both the scintigraphic imaging studies and the tissue biodistribution data.
303 Previous studies have reported evidence of lamellar inflammation during laminitis
304 development (Black et al., 2006; Belknap et al., 2007; Leise et al., 2011; Visser and Pollitt,
305 2011; Tadros et al., 2012). The accumulation of liposomes in lamellar tissue provides further
306 evidence that lamellar inflammation and increased vascular permeability occurs during
307 laminitis development in the OF model.

308

309 The primary objective of this study was to evaluate whether liposomes accumulate in
310 (and have potential for) targeted lamellar drug delivery. The increased lamellar liposome
311 levels in laminitis horses at 12 h p.i indicates that liposomal drug delivery systems have

312 potential to yield sustained lamellar drug concentrations. Recent studies performed in our
313 laboratory investigated lamellar marimastat concentrations after IV administration of 0.23
314 mg/kg bodyweight (104 mg/450 kg horse) (Underwood et al., 2015). If the same dose was
315 administered in liposomes at 18 h post-OF, based on the lamellar liposome levels in the
316 LAM18 group (0.31% ID/kg), the lamellar marimastat concentration would be 332 ng/g
317 tissue at 12 h post injection.

318

319 Although these calculations are merely speculative, this exceeds both the
320 concentrations achieved 12 h after RLP and the concentration necessary for inhibition of 90%
321 of lamellar MMP-2 and MMP-9 (Underwood et al., 2015; C. Underwood et al., unpublished
322 data). Additionally, as reported in previous studies investigating liposome accumulation in
323 inflammation, liposomes would probably continue to accumulate in the following 12h
324 resulting in further increases in lamellar drug concentrations (Oyen et al., 1996; Boerman et
325 al., 1997; Erdogan et al., 2000).

326

327 There were no adverse reactions to liposome administration, and no changes in heart
328 rate, respiratory rate or temperature; adding to the evidence from previous studies
329 (Underwood et al., 2012; Burton, 2013) that slow IV liposome administration is safe in
330 horses. Therefore, based on this preliminary study liposomes appear to have potential for
331 lamellar drug delivery.

332

333 The subjective increase in lamellar liposome levels between LAM-0, LAM-12 and
334 LAM-18 groups, respectively, suggests there is a temporal increase in lamellar inflammation

335 post-OF administration, consistent with previous reports (Visser, 2009). Liposomes were
336 administered immediately following, then at 12 h and 18 h after OF administration to achieve
337 high circulating liposome levels coinciding with the onset of lamellar inflammation (Visser,
338 2009). The highest uptake was achieved when liposomes were administered at 18 h post-OF.
339 By 18 h the horses were exhibiting Obel grade 1-2 lameness, which may be too late for
340 delivery of laminitis prophylactics. However, prophylactic digital cryotherapy is effective
341 when initiated at Obel grade 2 lameness (18.5 h post-OF administration; van Eps et al.,
342 2014), so it is possible that a pharmaceutical means of laminitis prophylaxis would still be
343 effective at this stage. Further work is needed to evaluate the optimal time-point for
344 administration of liposomal-formulations of drugs for laminitis prophylaxis.

345

346 The 3.2 fold increase in the liposome levels in the lamellar tissue of laminitis horses
347 compared to controls is somewhat lower than that the 24-fold increase reported in infected
348 muscle in an equine focal infection model (Underwood, 2011). This initially seems somewhat
349 discouraging; however, there are three key points to consider: firstly, liposome accumulation
350 depends on the intensity of the inflammatory response (Oyen et al., 1996); focal infection
351 models involve established inflammation, whereas in the present study liposomes were
352 administered before or during the early stages of inflammation. Secondly, the biodistribution
353 data in the focal infection study was obtained at 24 h p.i. whereas most of the data in this
354 study were collected at 12 h p.i. (LAM-12 and LAM-18). Liposomes accumulate gradually
355 with time (Boerman et al., 1997; Oyen et al., 1996). In a mouse focal infection model the
356 abscess:control muscle ratio increased from 2.2 at 6 h p.i., to 11.7 at 24 h p.i. (Erdogan et al.,
357 2000); therefore, it is probable if sampled at a later time-point there would be greater lamellar
358 accumulation of liposomes. Thirdly, as lamellar inflammation and laminitis pathology are
359 focused at the dermoepidermal interface (Pollitt, 1996; Faleiros et al., 2011), greater liposome

360 accumulation may be present at this target site than in the lamellar tissue as a whole
361 (Metselaar et al., 2003).

362

363 Acute laminitis shares many characteristics with sepsis-related organ failure and
364 systemic inflammatory response syndrome (SIRS) in humans (Belknap and Black, 2012;
365 Tadros et al., 2012; Cawcutt and Peters, 2014). The accumulation in skin, muscle, jejunum
366 colon and kidney, plus the trend towards increased hepatic liposome levels is supportive of a
367 systemic inflammatory response resulting in inflammation and increased vascular
368 permeability in these organs. To the authors' knowledge this is the first study to investigate
369 liposomal biodistribution in an animal sepsis model.

370

371 The accumulation of liposomes in multiple organs in our study indicates that
372 liposomes may have potential for targeted drug delivery to prevent sepsis related organ
373 failure in other species. It is, however, interesting that there was a more profound increase in
374 liposome accumulation (compared with controls) in the lamellar tissue compared with all the
375 other studied tissues. This indicates that the inflammatory response and increase in vascular
376 permeability in lamellar tissue are unique.

377

378 Increased interleukin (IL)-1 β , IL-6 IL-8, IL-10 and tumour necrosis factor (TNF)- α
379 gene expression has been reported previously in liver and lung of horses with OF-induced
380 laminitis (Tadros et al., 2012). Interestingly, in the present study, there was no evidence of
381 liposome accumulation in the lung. Normal horses demonstrate high pulmonary liposome
382 uptake (Underwood et al., 2012), most probably due to endocytosis of liposomes by the

383 increased numbers of pulmonary intravascular macrophages (PIMs) present in the horse
384 (Longworth et al., 1994). During sepsis, PIMs are activated and endocytose
385 lipopolysaccharide and bacteria (Tsokos, 2003; Parbhakar et al., 2005). Therefore, it is
386 probable that during the development of OF-induced laminitis PIMs have already been
387 activated and are unavailable to endocytose liposomes. This reduction in liposomal
388 endocytosis may counter-balance the liposomes extravasating into the pulmonary
389 parenchyma due to inflammation-associated increases in vascular permeability.

390

391 Interestingly, the median lung uptake in the LAM-18 group appeared lower than that
392 in the LAM-0 group (1.2[0.95-1.45] % ID/kg vs. 1.87 [1.59-2.15] % ID/kg, respectively),
393 potentially indicative of reduced liposomal endocytosis uptake at 18 h due to saturation of
394 PIMs in the systemic inflammatory response prior to liposome administration. However, the
395 numbers were too small for statistical analyses so further studies are necessary to evaluate
396 this hypothesis.

397

398 Limitations of our study include the small numbers of horses, particularly the low
399 numbers in each of the LAM groups, and the limited study duration of only 12 h p.i. Further
400 investigations of liposomal delivery systems for sustained lamellar drug delivery are
401 warranted. These should focus on determining free and liposome-encapsulated drug
402 concentrations at multiple time-points over a prolonged period (>24 h). When considering the
403 scintigraphic data, it is important to note that the radiopharmaceutical uptake in the hoof ROI
404 includes all sources of radioactivity within the hoof, including blood in the vascular system,
405 along with a mild shielding effect of the hoof wall. Changes in perfusion occur during
406 laminitis development and may have affected scintigraphic data (Van Eps and Pollitt, 2004).

407 Although, artefactual alterations in the scintigraphic data due to changes in perfusion cannot
408 be definitively ruled out, the lack of significant changes in HWST (an indicator of digital
409 vascular perfusion), and the reduction in blood activity with time suggest the increase in CD/s
410 in the hoof ROIs of laminitis horses was attributable to liposome accumulation rather than
411 increased perfusion. The tissue biodistribution data more accurately represent liposome levels
412 in specific tissues. However, these could still have been altered by residual blood in the tissue
413 and changes in lamellar perfusion. Perfusion of the disarticulated limbs with saline may have
414 further helped to remove any residual blood from the lamellar tissue. This was attempted in
415 one forelimb of the initial two horses, however, it was not practical and did not appear to alter
416 the % ID/kg lamellar tissue (0.09 [0.08-0.1]% in the perfused limbs vs. 0.07 [0.07-0.08] % in
417 the non-perfused limbs). Therefore, it was considered unlikely that changes in perfusion had
418 a significant effect on lamellar biodistribution data; further investigation would be needed to
419 definitively rule this out.

420

421 **Conclusions**

422 IV liposome administration to horses with OF-induced laminitis resulted in liposome
423 accumulation in the lamellar tissue. The degree of liposome accumulation indicates that
424 liposomes have potential for targeted drug delivery to lamellar tissue. With further
425 experimental validation liposomal drug delivery systems could be the first clinically
426 applicable method for delivering sustained therapeutic concentrations of pharmaceuticals
427 with lamellar targets, including drugs with potential for laminitis prophylaxis, analgesics and
428 anti-inflammatories. Liposomes also accumulate in other tissues undergoing inflammation
429 and may therefore be of value as a drug delivery system in sepsis related organ failure in
430 other species.

431

432 **Conflict of interest statement**

433 None of the authors of this paper has a financial or personal relationship with other
434 people or organisations that could inappropriately influence or bias the content of the paper.

435

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442

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591 **Figure legends**

592

593 Fig. 1. Decay corrected radioactivity in sequential blood samples following ^{99m}Tc -liposome
594 infusion in laminitis (grey circles) and control (black squares) horses. At 12 h post injection
595 (p.i.) the blood radioactivity in the laminitis group was lower than that in the control group
596 (*; $P=0.01$), and lower than the activity immediately p.i. in the laminitis group (\wedge ; $P=0.001$).
597 Data are expressed as medians \pm interquartile range.

598

599 Fig. 2. Dorsal scintigraphic images from one of the control horses (A-C) and one of the
600 laminitis horses (D-F) in the study. Images A and D were obtained at 1 h post injection (p.i.),
601 B and E at 6 h p.i. and C&F at 12 h p.i. Images are corrected for acquisition time, decay and
602 initial dose.

603

604 Fig. 3. Variations in the median count density/s (CD/s) (\pm inter-quartile range), in
605 scintigraphic regions of interest (ROIs), in laminitis (grey circles) and control (black squares)
606 horses over time. All data are corrected for decay and initial dose. There was an increase in
607 the CD/s in dorsal hoof (A) and dorsal fetlock (B) ROIs of laminitis horses over time (*;
608 $P<0.01$) and a decrease in the CD/s in the dorsal hoof (A) and fetlock (B) and metacarpal (C)
609 ROIs of control horses over time (*; $P<0.01$).). The CD/s in the lateral hoof ROI (D) of
610 control horses decreased with time, (*; $P<0.05$) and was lower than that in laminitis horses at
611 6 and 12 h post injection (\wedge ; $P=0.02$). Data are expressed as medians \pm interquartile range.

612

613 Fig. 4. The median liposome levels (expressed as percentage injected dose per kilogram [%
614 ID/kg]) in various tissues in laminitis vs. control horses (LAM-0 [triangles], LAM-12
615 [circles], LAM-18 [diamonds] and control groups [black squares]). The % ID/kg was higher
616 in lamellae (A), skin (B), muscle (C), jejunum (D), colon (E) and kidney (F) of laminitis
617 horses ($P<0.05$). There were trends towards an increased % ID/kg in the liver (G) and a
618 decreased % ID/kg in the blood (H) of laminitis horses ($P=0.06$).

619

620 Fig. 5. Lamellar liposome levels appeared to increase when liposomes were administered at
621 later time-points post-oligofructose administration (LAM-0: horses that received liposomes at
622 the time of oligofructose administration; LAM-12: horses that received liposomes 12 h after
623 oligofructose administration; LAM-18: horses that received liposomes 18 h after OF
624 administration; CON: control horses that did not receive oligofructose). The bars are labelled
625 with the lamellar liposome levels in that group compared to controls. Data are expressed as
626 medians \pm interquartile range.

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