



#### High-dose etoposide formulations do not saturate intestinal P-glycoprotein

Development, stability, and pharmacokinetics in Sprague-Dawley rats

Al-Ali, Ahmed A.Abdulhussein; Sandra, Louis; Versweyveld, Dries; Pijpers, Ils; Dillen, Lieve; Vermeulen, An; Snoeys, Jan; Holm, René; Nielsen, Carsten Uhd

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1	High-dose etoposide formulations do not saturate intestinal P-glycoprotein: Development,
2	stability, and pharmacokinetics in Sprague-Dawley rats
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4	Ahmed A. Abdulhussein Al-Ali <sup>a</sup> , Louis Sandra <sup>o</sup> , Dries Versweyveld <sup>c</sup> , Ils Pijpers <sup>a</sup> , Lieve Dillen <sup>a</sup> ,
5	An Vermeulen <sup>b</sup> , Jan Snoeys <sup>d</sup> , René Holm <sup>e,f</sup> , and Carsten Uhd Nielsen <sup>a*</sup>
6	
_	
7	": Department of Physics, Chemistry and Pharmacy, University of Southern Denmark, Campusvej 55,
8	DK-5230 Odense M, Denmark
9	<sup>b</sup> : Quantitative Sciences, Janssen R&D, a division of Janssen Pharmaceutica NV, Turnhoutseweg 30,
10	2340 Beerse, Belgium
11	<sup>c</sup> : Non Clinical Safety, Janssen R&D, a division of Janssen Pharmaceutica NV, Turnhoutseweg 30
11	. Ivon Chinear Safety, Janssen Red, a division of Janssen Fharmaceutea IVV, Furmioutseweg 50,
12	2340 Beerse, Belgium
13	<sup>d</sup> : Drug Metabolism and Pharmacokinetics (DMPK), Janssen R&D, a division of Janssen
14	Pharmaceutica NV, Turnhoutseweg 30, 2340 Beerse, Belgium
15	<sup>e</sup> : Drug Product Development, Janssen R&D, a division of Janssen Pharmaceutica NV,
10	Turmhoutservez 20, 2240 Beerree Balaium
16	Turnnoutseweg 50, 2540 Beerse, Bergium
17	<sup>f</sup> : Department of Science and Environment, Roskilde University, 4000 Roskilde, Denmark
18	*: Corresponding author at: Department of Physics, Chemistry and Pharmacy, University of Southern
19	Denmark, Campusvej 55, DK-5230 Odense M, Denmark. Phone: +45 6550 9427 e-mail: <u>cun@sdu.dk</u>
20	

21 Abstract: It has been suggested that oral absorption of low-permeable P-glycoprotein (P-gp) substrates can be increased through saturation of P-gp. For BCS class IV drug substances, saturating 22 P-gp is challenging due to low aqueous solubility. The present study investigated if the BCS IV drug 23 substance etoposide could be solubilized to a concentration saturating P-gp after oral administration. 24 A formulation consisting of 10% (w/v) of pluronic<sup>®</sup> F-127 and polyvinylpyrrolidone/vinyl acetate 25 (PVP/VA), and 57% (v/v) ethanol enhanced etoposide's solubility approximately 100 times (16 mg 26 mL<sup>-1</sup>) compared to its aqueous solubility. In vitro, this formulation was stable upon dilution in 27 28 simulated intestinal fluid. In male Sprague-Dawley rats, oral administration of increasing solubilized etoposide doses using the formulation matrix increased the AUC<sub> $0-\infty$ </sub> of etoposide dose-proportionally 29 but resulted in a lower absolute oral bioavailability (F) and rate of absorption as compared to control. 30 At the highest investigated dose (100 mg kg<sup>-1</sup>), AUC<sub>0- $\infty$ </sub> and C<sub>max</sub> were significantly increased by 2.9-31 and 1.4-fold, respectively, compared to control dosed at 20 mg kg<sup>-1</sup>. A single oral dose of 20 mg kg<sup>-1</sup> 32 <sup>1</sup> zosuguidar followed by 20 mg kg<sup>-1</sup> oral etoposide increased F 8.6-fold. In conclusion, a stable 33 formulation with improved etoposide solubility was developed, yet the formulation did not result in 34 35 increased oral bioavailability of etoposide.

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Keywords: P-glycoprotein, Etoposide, Zosuquidar, Population pharmacokinetics, Sprague-Dawley
 rats.

#### 43 **1. Introduction:**

P-glycoprotein (P-gp, MDR1) has been shown to limit the intestinal absorptive permeability of low-44 permeable substrates in cell cultures (Alsenz et al., 1998; Collett et al., 1999; Sparreboom et al., 1997; 45 Terao et al., 1996; Troutman and Thakker, 2003b). In vivo, in wild type (WT) rats, P-gp restricts the 46 47 oral bioavailability of several P-gp substrates such as loperamide (Zamek-Gliszczynski et al., 2012), 48 paclitaxel (Zamek-Gliszczynski et al., 2012), digoxin (Nielsen et al., 2016), and etoposide (Al-Ali et 49 al., 2018a). This is evident since the oral bioavailability is significantly increased in *mdr1a* deficient rats (Al-Ali et al., 2018a; Nielsen et al., 2016; Zamek-Gliszczynski et al., 2012). Moreover, co-50 51 administration of P-gp substrates with potent small-molecular P-gp inhibitors such as verapamil (Tsuruo et al., 1981), dexverapamil (Gramatté and Oertel, 1999), valspodar (PSC-833) (Mayer et al., 52 1997; vanAsperen et al., 1997), or zosuguidar (LY335979) (Bardelmeijer et al., 2004) increased the 53 oral bioavailability of the substrates in preclinical studies. However, using inhibitors to increase the 54 55 oral bioavailability of P-gp substrates in some cases also affects metabolism via the cytochrome 56 P450s and results in adverse effects (Breedveld et al., 2006; Palmeira et al., 2012; Varma et al., 2003; 57 Varma and Panchagnula, 2005). Other studies have shown that co-administration of pharmaceutical excipients such as nonionic surfactants may also have the potential to increase the oral bioavailability 58 of digoxin (Cornaire et al., 2004; Nielsen et al., 2016; Zhang et al., 2003), etoposide (Akhtar et al., 59 2017; Al-Ali et al., 2018a), and paclitaxel (Varma and Panchagnula, 2005) in WT rats. To overcome 60 the cellular efflux mediated by P-gp to increase intestinal absorption, it should in theory be possible 61 to saturate the transporters by achieving intestinal concentrations well above the K<sub>m</sub>-value for the 62 63 substrate-transporter binding as mentioned by e.g. Lin and Yamazaki (Lin and Yamazaki, 2003). 64 Taking into consideration the degree of passive diffusion, intestinal metabolism, and P-gp substrate binding affinity, this may be a feasible strategy for drug substances with sufficient aqueous solubility, 65 low passive diffusion, and limited metabolism. The experimental evidence for the feasibility of 66

saturating P-gp in the intestine through a pharmaceutical formulation strategy is however relatively 67 68 limited and ambiguous. Lin and Yamazaki and Chiou et al., retrospectively, interpreted the pharmacokinetic human studies of the BCS II compound talinolol made by de Mey et al., and 69 concluded that since the dose normalized AUC values after oral administration of increasing talinolol 70 71 doses increased with higher doses, this suggested saturation of P-gp efflux (Chiou et al., 2001; de Mey et al., 1995; Lin and Yamazaki, 2003). Talinolol is also a substrate of absorptive solute carriers 72 including organic anion transporting polypeptide 1A2 (OATP1A2) and OATP2B1 (Shirasaka et al., 73 74 2010) making the absorption kinetics quite complicated.

75 Since high doses of a P-gp substrate are needed to saturate the transporter, and as most P-gp substrates are poorly water-soluble substances (Wang et al., 2001), suitable pharmaceutical formulation 76 approaches are required to solubilize the substrate. SMEEDs formulations could be used, but they 77 often contain surfactants that are also P-gp inhibitors see e.g. Zhao et al. (Zhao et al., 2013). Thus, in 78 79 the present study a formulation that can maintain the substrate in a solubilized-form upon dilution in 80 the intestinal lumen without P-gp inhibiting surfactants was developed using etoposide a BCS class 81 IV P-gp substrate. Etoposide was selected since intestinal P-gp limited oral etoposide bioavailability in WT rats, whereas etoposide was completely absorbed in *mdr1a* deficient rats (Al-Ali et al., 2018a). 82 83 Moreover, data suggests that Bcrp has very little impact on the intestinal absorption of etoposide in mice (Allen et al., 2003). A formulation was designed with ethanol and surfactant to enhance the 84 solubility of etoposide. Etoposide has a low aqueous solubility of  $0.15-0.2 \text{ mg mL}^{-1}$  (Beig et al., 2015; 85 Darwish et al., 1989) and since 10% ethanol significantly enhanced etoposide stability in artificial 86 87 intestinal fluid, ethanol was used as a solubilizing co-solvent for etoposide (Joel et al., 1995). Since 88 many nonionic surfactants inhibit P-gp in vitro (Al-Ali et al., 2019; Al-Ali et al., 2018b; Batrakova et al., 1999; Batrakova et al., 2003; Gurjar et al., 2018; Li-Blatter et al., 2012; Lo, 2003; Zhao et al., 89 90 2016) and *in vivo* (Akhtar et al., 2017; Al-Ali et al., 2018a; Ma et al., 2011; Nielsen et al., 2016; Zhao 91 et al., 2013), a surfactant without P-gp inhibiting properties was chosen to evaluate the effect of increasing the dose of etoposide without a potential surfactant mediated P-gp inhibitory effect. 92 Previous in vitro studies have reported that pluronic® F-127 did not inhibit the P-gp-mediated efflux 93 of several substrates e.g. rhodamine 123 (Al-Ali et al., 2019; Batrakova et al., 2003; Wei et al., 2013), 94 95 nelfinavir (Shaik et al., 2008), digoxin (Gurjar et al., 2018), and etoposide (Al-Ali et al., 2018a), hence this surfactant was chosen. Polyvinylpyrrolidone-vinyl acetate (PVP/VA) was suggested as a 96 potential precipitation inhibitor (Kalaiselvan et al., 2006; Knopp et al., 2016; Xu and Dai, 2013) and 97 98 formulation stabilizer during storage (Knopp et al., 2016; Prudic et al., 2014), thus it was included in the formulation. 99

The aim of the present study was to prepare an oral formulation of high concentration of etoposide and to investigate the stability on storage, and upon dilution in fasted state simulated intestinal fluid (FaSSIF). Furthermore, the formulation was used to investigate if the systemic exposure of orally administered etoposide in rats could be increased through saturation of P-gp transport activity.

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#### 105 **2. Material and methods:**

#### 106 *2.1. Materials*

107 Caco-2 cells were obtained from the American Type Culture Collection (ATCC). Cell culture media 108 and Hanks balanced salt solution (HBSS) were obtained from Life Technologies (Høje-Taastrup, 109 Denmark). Etoposide (>99% purity) was purchased from Selleckchem (Munich, Germany). Sodium 110 chloride, sodium taurocholate, sodium hydroxide, potassium chloride, L- $\alpha$ -phosphatidylcholine 111 (approx. 60%), potassium phosphate monobasic (≥97%), and pluronic<sup>®</sup> F-127 suitable for cell 112 culture, 2-(N-morpholino) ethane sulfonic acid (MES), N-[2-Hydroxyethyl] piperazine N'-[2-113 ethanesulfonate] (HEPES), verapamil, digoxin, and bovine serum albumin (BSA) were from Sigma

(Brøndby, Denmark). Ethanol (99.5 %) was from VWR Chemicals (Fontenay-sous-Bois, France). 114 Polyvinylpyrrolidone-vinyl acetate (Kollidon<sup>®</sup> VA 64, referred as PVP/VA) meets Ph. Eur. standards 115 and was from BASF SE (Ludwigshafen, Germany). Transwell<sup>®</sup> inserts with polycarbonate membrane 116 (0.4 µm pore size, 1.12 cm<sup>2</sup>) were from Corning Life Sciences and purchased through Sigma Aldrich 117 (Brøndby, Denmark). Whatman<sup>®</sup> Nuclepore<sup>™</sup> Track-Etched Membranes (0.03 µm pore-size, 19 mm 118 in diameter) were purchased from Sigma Aldrich (Brøndby, Denmark). LOCTITE® 401 glue was 119 purchased from RS Components Ltd. (Corby, UK). <sup>3</sup>H-etoposide (specific activity 700 mCi mmol<sup>-1</sup>) 120 was from Moravek (CA, USA). <sup>14</sup>C-glycine (specific activity 87 mCi mmol<sup>-1</sup>) was purchased from 121 Larodan (Solna, Sweden) and <sup>14</sup>C-mannitol with a specific activity of 51.50 mCi/mmol was from 122 Sigma Aldrich (Brøndby, Denmark). Ultima Gold liquid was purchased from Perkin Elmer 123 124 (Skovlunde, Denmark). The radio-chemical purity of the isotopes was greater than 97%.

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#### 126 2.2. Cell culture and transport experiments

Caco-2 cells were cultured as previously described by Nielsen and co-workers (Nielsen et al., 2001). 127 Briefly, cells were seeded in culture flasks and passaged in Dulbecco's Modified Eagle's medium 128 (DMEM) supplemented with 10 % fetal bovine serum, penicillin/streptomycin (100 U ml<sup>-1</sup> and 100 129 µg ml<sup>-1</sup>, respectively), 1 % L-glutamine, and 1 % non-essential amino acids. Cells were seeded onto 130 tissue culture treated Transwells (1.0 cm<sup>2</sup>, 0.4  $\mu$ m pore size) at a density of 10<sup>5</sup> cells cm<sup>-2</sup>. 131 Transepithelial electrical resistance (TEER) at room temperature was measured before the 132 experiment. All TEER values of monolayers used were >400  $\Omega$  cm<sup>2</sup>. Transport experiments were 133 performed on day 24-28 after seeding. 134

Apical (A) to basolateral (B) and B to A fluxes of tritium labeled etoposide was measured in 10 mM
HEPES buffers adjusted to pH 7.4. The concentration of etoposide on the donor (cis) side was 20 –

520 µM. Samples (20 µl) were taken from the donor solution at t=0 and 210 min and 150 µl samples 137 138 were taken from the receiver solution and replaced with fresh buffer (t=30, 60, 90, 120, 150, 180, and 210 min). The transport of <sup>3</sup>H-etoposide was also measured in the presence of 100 µM of digoxin and 139 50 µM verapamil on both donor and receiver side, respectively. Samples were transferred to 140 141 scintillation vials, where 2 ml of scintillation fluid was added and the radioactivity was counted in a liquid scintillation analyzer. Fluxes were constant after 60 min. The steady state flux values were thus 142 obtained as the means of the flux values between 90-210 min. After the experiment, the integrity of 143 the Caco-2 cell monolayers was evaluated by <sup>14</sup>C-mannitol transport studies. Samples were taken 144 from the donor chamber (10 µl) at 20, 40, and 60 min, and from the receiver chamber at 0, 20, 40, 145 and 60 min. The permeability (P<sub>app</sub>) of mannitol was unaffected by etoposide, digoxin and verapamil 146 and had a  $P_{app}$  value of 1.4  $10^{-06} \pm 4.2 \ 10^{-07} \text{ cm s}^{-1}$ . The transport across the filter without Caco-2 cells 147 was investigated in order to assess whether the filter was a barrier to diffusion of etoposide. The 148 permeability across the filter was calculated using non-steady state kinetics and had a value of 3.1 10<sup>-</sup> 149  $^{04} \pm 4.2 \ 10^{-05} \ \text{cm s}^{-1}$ . 150

The P-gp dependent flux (J<sub>P-gp</sub>) was calculated similarly to described by Troutman and Thakker 151 152 (Troutman and Thakker, 2003a), where the total flux of etoposide was subtracted with the flux of etoposide in the presence of 100 µM of digoxin and 50 µM verapamil to yield the concentration 153 dependent effect of P-gp on etoposide transport. Here we used Caco-2 cells from ATCC, and 154 proteomics data suggest that BCRP expression is very low in the substrain compared to Caco-2 cells 155 156 obtained from The European Collection of Authenticated Cell Cultures (ECACC) or/and Deutsche Sammlung von Mikroorganismen und Zellkulturen (DSMZ), as reviewed in Al-Ali et al., 2019 (Al-157 Ali et al., 2019). In Caco-2 cells from DSMZ it has been shown that 25 µM zosuquidar abolish 158 polarized etoposide transport completely (Nielsen et al., 2020), while it has also been shown that 159

verapamil completely abolishes polarized etoposide in Caco-2 cells (Mo et al., 2011). Therefore, it
seems likely that in Caco-2 cells from ATCC BCRP has a minor impact on etoposide transport.
The resulting etoposide flux in the B-A direction was then fitted to the following equation:

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$$J_{P-gp} = \frac{J_{P-gp,\max*C_d}}{K_{m,app}+C_d}$$
(1)

where,  $J_{P-gp}$  is the P-gp mediated flux,  $J_{P-gp,max}$  is the maximal flux,  $K_{m,app}$  is the apparent Michaelis constant and  $C_d$  is the donor concentration.

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#### 168 *2.3. Animals*

In vivo pharmacokinetic studies were performed in WT male Sprague-Dawley rats, which were from 169 Charles River Laboratories (Sulzfeld, Germany). The study protocol was approved by the local ethical 170 171 committee in accordance with EC Directive 2010/63/EU and Belgian Law/1991 for Protection of Vertebrate Animals used for Experimental and other Scientific Purposes. The rats were received one 172 week prior to the in vivo experiments, acclimatized and maintained on standard feed conditions with 173 free access to water. The animals were fasted for 16 h before the pharmacokinetic studies. During the 174 experiments, the rats had free access to water, but not food. At the day of the experiment, the weight 175 176 of the animals was 242-275 g.

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#### 178 2.4. Preparation of etoposide-containing formulations

Different formulations of etoposide were prepared using the nonionic surfactant pluronic<sup>®</sup> F-127, the copolymer PVP/VA, ethanol, and ultra-purified water (Table 1). Pluronic<sup>®</sup> F-127 was first dissolved in 57% (v/v) ethanol solution at room temperature. Etoposide was then added to the surfactant-

containing solution and placed in a water bath at 40° C for 15-30 min, before the solution was mixed 182 using a magnetic stirrer for 15-30 min. The solution was visually inspected for undissolved particles. 183 PVP/VA powder was subsequently added, and the mixture placed in a water bath at 37°C for 15-30 184 min, before being mixed using a magnetic stirrer for 15-30 min. The solution was again visually 185 186 investigated for undissolved particles. Finally, provided that the etoposide-containing formulation was clear, the formulation was transferred to a glass container, protected from light, and kept at room 187 temperature overnight (approx. 15 h). If no sign of precipitation appeared after 15 h, the formulation 188 was further investigated for precipitation upon dilution with FaSSIF, see details below. 189

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2.5. Monitoring of etoposide containing-formulations diluted with fasted state simulated intestinal fluid

193 Monitoring that etoposide does not precipitate in the different formulations when diluted with FaSSIF was investigated as previously described by Al-Ali et al. (Al-Ali et al., 2018a). Briefly, FaSSIF was 194 prepared according to Galia et al., composed of 0.39 g potassium phosphate monobasic, 0.77 g 195 potassium chloride, 3 mM sodium taurocholate, 0.75 mM L-a-phosphatidylcholine, and ultra-purified 196 water added to 100 mL (Galia et al., 1998). The pH was then adjusted to  $6.50 \pm 0.05$  with sodium 197 hydroxide before the osmolality was adjusted to  $270 \pm 10$  mOsm kg<sup>-1</sup> using sodium chloride (Galia 198 et al., 1998). The different formulations of etoposide were then added to FaSSIF in a ratio of 1:2 199 (formulation:FaSSIF) to simulate the likely intestinal dilution in the rats (McConnell et al., 2008) and 200 monitored for two hours by measuring the absorbance at 400 nm and 25°C every 10 min using a UV-201 spectrophotometer (Genesys 10-S from Thermo Fisher Scientific (WI, USA)). Before each 202 measurement, solutions were mixed for 10 seconds using pipetting. 203

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#### 205 2.6. Dialysis studies investigating etoposide release from different formulations

Dialysis studies were designed and optimized as previously described by Al-Ali et al., (Al-Ali et al., 206 207 2018a), with minor modifications. In brief, the dialysis setup allows the diffusion of free-fraction of etoposide (unbound to micelles) and retains etoposide-bound to micelles, which should be not 208 209 diffused across a 0.03 µm pore-size polycarbonate membrane during the course of the experiment (2 h). Polycarbonate membranes (0.03 µm pore size, 19 mm in diameter) were attached to Transwell 210 holders (1.12 cm<sup>2</sup>) by LOCTITE® 401 glue and left to dry at room temperature overnight (Al-Ali et 211 212 al., 2018a). The Transwell inserts, with attached polycarbonate membranes, were then hydrated overnight in ultra-purified water. On the day of the experiment, Transwell inserts with polycarbonate 213 membranes were first pre-incubated with HBSS supplemented with 10 mM HEPES and adjusted to 214 pH 7.40  $\pm$  0.05 (HBSS<sup>+</sup>) on a shaking plate at 220 rpm at 37° C for 10 min. Donor solutions of <sup>3</sup>H-215 etoposide and <sup>14</sup>C-glycine were prepared in HBSS<sup>+</sup> (Control), or in different formulation-matrices 216 containing 10% (w/v) PVP/VA, 57% (v/v) ethanol, and pluronic<sup>®</sup> F-127 at 1.5, 3 or 10%, referred to 217 as Matrix-PF127 1.5%, Matrix-PF127 3%, or Matrix-PF127 10%, respectively, or mixed with a 218 formulation with the highest concentration of etoposide. This formulation contained 15-16 mg mL<sup>-1</sup> 219 etoposide, 10% (w/v) of pluronic<sup>®</sup> F-127 and PVP/VA, and 57% (v/v) ethanol. The solution 220 containing radioactive compounds was then added to FaSSIF at a 1:2 ratio to achieve final 221 concentrations of <sup>3</sup>H-etoposide and <sup>14</sup>C-glycine at 0.25 µCi mL<sup>-1</sup>, 0.36 µM and 0.25 µCi mL<sup>-1</sup>, 2.87 222 223  $\mu$ M, respectively, before these isotopes-containing solutions (500  $\mu$ L) were added to the upper side of the polycarbonate membrane. Experiments started when receiver-release media (1650 µL) was 224 225 loaded in the lower side of the polycarbonate membrane. Receiver-release media consisted of HBSS buffer supplemented with 10 mM HEPES and adjusted to pH  $6.50 \pm 0.05$  for all conditions except 226 for the formulation containing the highest concentration of etoposide where the medium was the 227 matrix of this formulation (i.e. 10% of pluronic® F-127 and PVP/VA, and 57% ethanol without 228

etoposide) in order to prevent etoposide precipitation when accumulated in the receiver chamber.
Experiments were performed at 37° C and shaking mode 220 rpm. Donor samples were collected at
0, 60 and 120 min, while receiver samples were collected at 15, 30, 60, 90, and 120 min. Receiverrelease medium was replaced at each sampling occasion in order to preserve the sink condition.
Finally, Ultima Gold scintillation fluid (2 mL) was added to every sample, vortexed for one minute
and counted for 10 min on a scintillation counter (TriCarb 4910TR) from Perkin Elmer, USA.

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#### 236 2.7. Pharmacokinetic study in wild-type male Sprague-Dawley rats

The rats were randomly assigned to receive different doses of etoposide in ethanol solution or in a 237 formulation matrix consisting of 10% (w/v) pluronic® F-127 and PVP/VA, 57% (v/v) ethanol, and 238 ultra-purified water. For intravenous administration, the rats received etoposide solution (2.86 mg 239 mL<sup>-1</sup> in 57% v/v ethanol) at a dose of 5 mg kg<sup>-1</sup> etoposide. Administration volume was adjusted to 2 240 mL with water before dosing the rats. For oral administration by oral gavage, the control group 241 received an etoposide solution (2.86 mg mL<sup>-1</sup> in 57% v/v ethanol) at a dose of 20 mg kg<sup>-1</sup> etoposide 242 and a dosing volume of 7 mL kg<sup>-1</sup>. In the positive control group, the rats received a zosuquidar 243 solution (2 mg mL<sup>-1</sup>) at a dose of 20 mg kg<sup>-1</sup> and dosing volume of 10 mL kg<sup>-1</sup>, 30 min before the 244 administration of etoposide doses which were administered in a similar fashion to the control group. 245 For oral administration of increasing doses of etoposide, an increasing concentration of etoposide was 246 solubilized in the formulation matrix i.e. 2.86, 7.15 and 14.3 mg mL<sup>-1</sup>. These etoposide-containing 247 formulations were administered at doses of 20, 50, and 100 mg kg<sup>-1</sup>, respectively, in a dosing volume 248 of 7 mL kg<sup>-1</sup>. Each dosing group consisted of 5-6 male Sprague-Dawley rats. After oral or intravenous 249 administration of etoposide, blood samples were collected at 0.25, 0.5, 0.75, 1, 2, 3, 4, and 6 h, as 250 251 well as at 5 min (0.0833 h) post intravenous administration of etoposide. The samples were obtained at each sampling point by puncturing the lateral tail vein using a 23G needle and approximately 35  $\mu$ L of blood were collected using a capillary tube from VITREX Medical A/S (Herlev, Denmark). The capillaries with samples were then sealed with VITREX Sigillum Wax. Plasma samples were harvested immediately from these capillaries after centrifugation at 1900xg for 10 min at 4° C and transferred to a 10  $\mu$ L end-to-end capillary (VITREX) followed by storage at -20° C until further bioanalysis. At 6 h, the last samples were collected, and the animals were euthanized.

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#### 259 2.8. Quantification of etoposide in pharmacokinetic studies

Quantification of etoposide in plasma samples was performed on an API 4000™ LC/MSMS System 260 from AB SCIEX (Ontario, Canada). Briefly, plasma samples were precipitated with acetonitrile after 261 262 wash-out from the end-to-end capillaries. Chromatographic separation was carried out using an Acquity UPLC BEH C18 column (1.7 µm, 2.1 mm × 50 mm). Gradient elution was performed at 50 263 °C with 0.01M ammonium acetate (mobile phase A) and acetonitrile (mobile phase B). Starting 264 conditions were 5 % B for 0.25 minutes, then a linear gradient to 95% B was applied over 1.25 265 minutes, followed by an isocratic hold at 95% B for 0.5 min before re-equilibration at 5% B. Total 266 267 run time was 2.5 min and a flow rate of 0.6 mL/min was applied.

The LC-MS/MS was operated in positive ion mode using the TurboIonSprayTM-interface (electrospray ionization), and was optimized for the quantification of etoposide, applying multiple reaction monitoring (m/z 587.2  $\rightarrow$  m/z 381).

Incurred samples were quantified against calibration curves prepared in blank rat plasma. Independent
quality control samples were included to evaluate accuracy (between 80 and 120% of the nominal

value) of the analytical run. The concentrations were correlated linearly, with a  $1/x^2$  weighing, with the MS response between 1.00 and 10000 ng mL<sup>-1</sup>.

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#### 276 2.9. Population Pharmacokinetic analysis

Population pharmacokinetic analysis was performed using Monolix 2018R2 (Lixoft SAS, Antony, France) based on a two-compartment population pharmacokinetic model with linear first order elimination and an oral depot compartment with subsequent first order absorption. Population pharmacokinetic parameter estimates were generated using the stochastic approximation expectationmaximization (SAEM) algorithm. Modeling was performed using the clearance parameterization assuming a lognormal distribution of individual parameters. The individual parameter estimates for the *i*th subject were modeled according to equation 2.

284 
$$\theta_i = \theta_{\text{pop}} \cdot e^{\eta_{\theta,i}}$$
 (2)

where  $\theta_i$  is the individual parameter estimate for the *i*th subject,  $\theta_{pop}$  is the typical population 285 parameter estimate and  $\eta_{\theta,i}$  is assumed to be the random individual deviation for the *i*th subject for a 286 particular population parameter  $\theta$ . The clearance parametrization included the volume of the central 287 288 compartment  $(V_1)$ , the elimination clearance (CL), the volume of the peripheral compartment  $(V_2)$ , and the inter-compartmental flow between the central and the peripheral compartment (Q<sub>2</sub>). Oral 289 administration was modeled using a dosing compartment and subsequent first order absorption. The 290 final model included covariate effects, which partly explained differences observed between animals 291 assigned to the different formulation groups. Forward inclusion of covariates was judged based on 292 the decrease in objective function value expressed as -2 log likelihood (-2LL) and Akaike's 293 294 information criterion (AIC). Covariate selection was guided by physiological plausibility and statistical significance (P < 0.05). Covariate effects of the final population model included the presence of zosuquidar on F and the presence of experimental matrix (referred as formulation Gmatrix) on F and  $k_a$ . The final model estimated inter-individual variability for F,  $k_a$ , V<sub>1</sub> and CL. Residual error was accounted for by a combined (additive and proportional) error model (Equation 3).

$$\log(Y_{ij}) = \log(c_{\text{pred},ij}) + (a + b \cdot \log(c_{\text{pred},ij}))\epsilon_{ij}$$
(3)

where the *j*th observation of the *i*th subject deviates from the *j*th prediction of the *i*th subject,  $c_{pred,ij}$ , by an additive term, a, and a proportional term, b.  $\epsilon_{ij}$  was assumed to be the random variable for the *j*th concentration of the *i*th individual, sampled from a distribution with zero as a mean and a variance of  $\sigma^2$ . Individual Bayesian estimates were used to calculate mean AUC<sub>0-∞</sub> per study cohort. Individual AUC<sub>0-∞</sub> values (AUC<sub>0-∞,i</sub>) were calculated as shown in equation 4.

$$306 \quad AUC_{0-\infty,i} = \frac{F_i \cdot D}{CL_i}$$
(4)

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The results of *in vitro* studies were obtained from at least three experiments and presented as mean values  $\pm$  SEM. Caco-2 cell experiments were conducted in three independent cell passages and values are presented as mean values  $\pm$  SEM. The results of the *in vivo* pharmacokinetic studies were obtained from 5 or 6 rats per study cohort and data are presented as mean values  $\pm$  SEM. Statistical analysis was performed using GraphPad Prism 7.01 from GraphPad Software, LLC (San Diego, CA, USA). One-way ANOVA test followed by Tukey's multiple comparisons test were selected for multiple comparisons. P value < 0.05 was considered statistically significantly different from control. 316 Moreover, dose-proportionality has been assessed by plotting  $AUC_{0-\infty}$  as a function of oral etoposide 317 doses and linear regression analysis was performed.

318

#### 319 **3. Results**

#### 320 *3.1. Transepithelial flux of etoposide across Caco-2 cells*

Etoposide transport across Caco-2 monolayers was investigated, and in the following Figure 1, the 321 A-B and B-A flux dependent on P-gp is shown. The A-B flux dependent on P-gp shows a gradual 322 323 increase as a function of concentration and at higher concentrations the flux is relatively linear as a function of concentration in the apical donor solution (Fig. 1A). In the B-A direction, the flux of 324 etoposide across Caco-2 cells monolayers can be described by Michaelis-Menten like kinetics where 325 326 the flux becomes saturated with increasing concentration in the basolateral medium. The resulting kinetical parameters were estimated at  $257 \pm 32 \mu$ M,  $199 \pm 17 \text{ pmol cm}^{-2} \text{ min}^{-1}$ , and  $1.7 \pm 0.2$  for 327  $K_{m,app}$ ,  $J_{P-gp, max}$ , and the Hill coefficient, respectively. 328

329

#### 330 *3.2. Etoposide did not precipitate in formulations containing high percentages of ethanol*

Different formulations of etoposide were prepared using 44% or 57% (v/v) ethanol, 2-10% (w/v) 331 pluronic® F-127, and 0-15% (w/v) PVP/VA (Table 1). Etoposide in formulations containing 44% 332 (v/v) ethanol either contained low concentration of etoposide such as 9 mg mL<sup>-1</sup> (Formulation A), 333 which was not sufficient to perform our study or precipitated after overnight incubation such as 334 Formulation B (Fig. 2). Etoposide formulations (C-G) showed no signs of etoposide precipitation 335 after overnight incubation; e.g. Formulation G as shown in Figure 2. Etoposide solubility in these 336 formulations containing 57% (v/v) ethanol was higher than in formulation A and B. Formulation D 337 showed that 6% (w/v) of the surfactant was required to dissolve 15 mg mL<sup>-1</sup> etoposide in PVP/VA-338

free formulation. Formulations A, C, and E-G were designed to contain 5-15% (w/v) PVP/VA as a potential precipitation inhibitor. Formulation G consisting of 10% (w/v) of pluronic<sup>®</sup> F-127 and PVP/VA, 57% ethanol, and water could solubilize an amount of etoposide corresponding to a 100fold increase compared to the aqueous solubility. Further studies were conducted to investigate whether etoposide precipitates after the addition of different formulations to FaSSIF.

344

345 3.3. Etoposide did not precipitate from Formulation G after dilution in fasted state simulated
346 intestinal fluid

Formulations C-E showed a fast etoposide precipitation (less than 30 min) after dilution in FaSSIF. 347 Formulation F started to precipitate after approx. one hour and reached similar levels of absorbance 348 349 values as C-E at 90 min. Therefore, formulations C-F were only prepared and investigated once. Formulation G showed no sign of etoposide precipitation for 120 min (Fig. 3). After 120 min, 350 etoposide started to precipitate indicating that the matrix of formulation G was able to maintain 351 etoposide in a solubilized form in FaSSIF for two hours (Fig. 3), which is the period that likely covers 352 the absorption phase of etoposide in rats. Equal amounts of pluronic® F-127 and PVP/VA at 10% 353 354 (w/v) were required to maintain etoposide in a solubilized form when diluted with FaSSIF. Among the investigated formulations, formulation G was stable in FaSSIF and the next step was to investigate 355 if the formulation G would retain etoposide. 356

357

358 3.4. Etoposide release was similar from different surfactant-containing solutions and matrix of
 359 formulation G

As shown in Figure 4, simultaneous etoposide and glycine release from different pluronic<sup>®</sup> F-127containing solutions and formulation G to receiver-release media increased time dependently. The release of etoposide and glycine from different pluronic<sup>®</sup> F-127-containing formulations and from formulation G was similar to the release in the control buffer i.e. without surfactant. Moreover, there was no statistically significant difference between the slopes of the time-dependent release of etoposide or glycine compared to control. The presence of non-radiolabeled etoposide in formulation G did not affect the release of radiolabeled etoposide during the course of the experiment.

367

# 368 3.5. Etoposide population pharmacokinetics in WT male Sprague-Dawley rats after intravenous 369 and oral administration

370 Pharmacokinetic data available included 321 concentration-time points collected from 35 male WT Sprague-Dawley rats. The PK profile af intravenous administration of etoposide is shown in figure 5, 371 illustrating a fast distribution phase followed by a slower elimination phase. Data points at 4 h post 372 intravenous administration of etoposide are not shown in Figure 5 as the plasma concentration values 373 374 were below the limit of quantification (LOQ) at this time point, and only three plasma-concentrations 375 had values above LOQ at 6 h. Etoposide pharmacokinetic profiles after oral administration of etoposide-containing solutions were best described by a two-compartment structural model with 376 linear elimination and first-order absorption (Fig. 6). Subsequently, a covariate model was developed 377 378 to account for the inter-individual variability arising from the experimental design. The introduction of zosuquidar dose as a covariate on the oral bioavailability F, and matrix-G presence as a covariate 379 on F as well as on the absorption rate constant (k<sub>a</sub>) significantly improved the model fit. After 380 covariate inclusion, the unexplained inter-individual variability for F and ka, calculated as the square 381 root of the exponential variance of  $\eta$  minus 1, decreased from 153% for F and 59.7% for k<sub>a</sub> to 15.9% 382

and 53.5%, respectively, from the base structural model to the final covariate model ( $\Delta 138\%$  for F 383 and  $\Delta 6.15\%$  for k<sub>a</sub>). Estimated population pharmacokinetic parameters, precision of the parameter 384 estimates and objective function values of both the base structural model and the final covariate model 385 386 are presented in Table 2. Empirical Bayesian estimates were used to calculate AUC<sub>0-∞</sub> and dose normalized AUC<sub>0- $\infty$ </sub>. AUC<sub>0- $\infty$ </sub>, dose normalized AUC<sub>0- $\infty$ </sub>, t<sub>1/2</sub>, t<sub>max</sub> and C<sub>max</sub> are presented in Table 3. 387 Rats pretreated with zosuquidar showed the largest etoposide exposure (AUC<sub>0- $\infty$ </sub> of 4511 ng h mL<sup>-1</sup> 388 kg). Dose-proportional etoposide exposure was observed for the 20, 50, and 100 mg kg<sup>-1</sup> dosing 389 cohorts receiving etoposide prepared in the matrix of formulation G (i.e. 10% of pluronic<sup>®</sup> F-127 and 390 PVP/VA, 57% ethanol, and water), and R square was equal to 0.99 when the AUC was plotted as a 391 function of dose (supplementary figure S1). However, the F, ka, AUC<sub>0-∞</sub>, and C<sub>max</sub> were significantly 392 lower when the rats were dosed with etoposide 20 mg kg<sup>-1</sup> dissolved in the matrix of formulation G 393 compared to the control group. Etoposide oral bioavailability significantly increased when the rats 394 were pretreated with zosuquidar. The oral pharmacokinetic profile showed that the oral absorption of 395 etoposide was slower in matrix-based formulations as was also apparent from the decreased ka values. 396

397

#### 398 **4. Discussion**

In the present study, a stable formulation containing high concentration of etoposide and ethanol (57%) was developed using a surfactant without P-gp inhibiting properties. After oral administration of etoposide in this formulation, no increased bioavailability related to P-gp saturation could be shown, illustrating the practical difficulties in saturating P-gp mediated transport of low soluble drug substances for increasing the oral absorption through a formulation approach.

To investigated if the transport of etoposide was saturable, we used the approach described by Troutman and Thakker (Troutman and Thakker, 2003a), in which the net flux due to P-gp mediated

transport is estimated by subtracting the flux under P-gp inhibited conditions. We found that the B-A 406 transport was saturable with kinetical parameters similar to the ones described by Troutman and 407 Thakker in Caco-2 cells, for  $K_{m,app}$  257 vs. 461  $\mu M,$  and for  $J_{max}$  199 vs. 354 pmol cm^{-2} min^{-1} 408 (Troutman and Thakker, 2003a). Makhey et al. found a similar K<sub>m</sub> value of 113 µM in Caco-2 cells 409 410 and 94-119 µM in stripped rat intestinal tissue (Makhey et al., 1998). Troutman and Thakker estimated a higher K<sub>m</sub> value of 1360 µM for the A-B transport direction (Troutman and Thakker, 411 412 2003a), however this value was outside the concentration range that could be investigated in our setup. Even though the B-A transport appears saturable and while it is more difficult to be assessed from 413 the A-B transport, studies in wild-type and knock-out rats clearly show that the apically located P-gp 414 is highly attenuating the oral etoposide absorption (Al-Ali et al., 2018a). Considering the above 415 416 mentioned K<sub>m</sub> values, generally of approximately 100-500 µM, an intestinal concentration of 10 times these values would likely be required to fully saturate P-gp mediated transport by etoposide itself, 417 corresponding to approximately 5000 µM for the worst case scenario. A solubility higher than that 418 could be achieved with formulation G (16 mg mL<sup>-1</sup> (27183 µM)) containing 10% of pluronic<sup>®</sup> F-127 419 and 10% PVP/VA. 16 mg ml<sup>-1</sup> is approximately 100-fold higher than the aqueous solubility of 420 etoposide (Beig et al., 2015; Darwish et al., 1989). Pluronic® F-127 forms micelles that have the 421 capacity to solubilize lipophilic drug substances e.g. meso-tetraphenyl porphine (mTPP) (Sezgin et 422 al., 2007), rofecoxib (Ahuja et al., 2007), ibuprofen (Wan et al., 2010), paclitaxel, and lapatinib 423 (Kelishady et al., 2015). The reported critical micelle concentration (CMC) values of pluronic<sup>®</sup> F-424 425 127 were 1, 0.1, and 0.025% (w/v) at 25, 30, and 35°C (Alexandridis and Hatton, 1995), respectively. Etoposide in micelles could be retained from permeation and hence the oral absorption could be 426 427 decreased, which has been reported with 25% polysorbate 20 (Al-Ali et al., 2018a). However, the presence of different concentrations of pluronic<sup>®</sup> F-127 did not affect the *in vitro* release of etoposide 428 and glycine compared to the release from a surfactant-free formulation. Similarly, 1% (w/v) pluronic<sup>®</sup> 429

F-127, which is above the CMC value, did not affect the release of the lipophilic drug rofecoxib
(Ahuja et al., 2007) (Log P 2.56) (Chemicalize, 2018).

432 Previous pharmacokinetic studies in rats have shown that t<sub>max</sub> of etoposide exposure was between 0.25-1.75 h (Al-Ali et al., 2018a; Li et al., 2009; Zhao et al., 2013), therefore the formulation should 433 434 maintain etoposide in its solubilized form for two hours when diluted in FaSSIF. This period was considered sufficient for further in vivo studies. In formulation G, solubilized etoposide did not 435 precipitate for two hours when diluted with FaSSIF. Thus, pluronic<sup>®</sup> F-127 probably had two 436 functions: i) enhanced the solubility of etoposide, and ii) decreased the precipitation rate of etoposide 437 438 as it was also suggested by (Li et al., 2012; Xu and Dai, 2013), thereby stabilizing the formulation in FaSSIF. Importantly, it seems that a balance between pluronic<sup>®</sup> F-127 and PVP/VA concentrations 439 (i.e. 10% of each) in the formulation was needed to achieve these formulation characteristics. Thus, 440 if an intestinal dilution of 3-10 is expected after oral administration of a 16 mg mL<sup>-1</sup> etoposide 441 formulation, and initial estimated intestinal concentration of 2718 - 9061 µM could be obtained, 442 443 which could be able to saturate P-gp assuming that etoposide remains in solution.

In rats receiving 100 mg kg<sup>-1</sup> of etoposide in formulation G, a higher  $AUC_{0-\infty}$  was obtained compared to rats receiving 20 mg kg<sup>-1</sup> etoposide in a 57% ethanol solution. Even though the systemic exposure of etoposide increased with higher doses, the absolute bioavailability decreased, and this does not seem to involve P-gp saturation by etoposide as the absolute bioavailability should then increase. However, zosuquidar enhanced the oral absorption and bioavailability of etoposide. Yet, in the presence of 20 mg kg<sup>-1</sup> zosuquidar, only 34.5% of the etoposide dose reached the systemic circulation, thus zosuquidar itself most likely did not cause full inhibition of intestinal P-gp.

451 Surprisingly, the absolute oral bioavailability of etoposide was low compared to our previous study 452 (Al-Ali et al., 2018a). Al-Ali and coworkers reported that the oral bioavailability of etoposide was 27

 $\pm$  5% (Al-Ali et al., 2018a). Zhao and co-workers reported an oral bioavailability of etoposide of 25 453  $\pm$  7% in WT male Sprague-Dawley rats dosed with 12 mg kg<sup>-1</sup> etoposide suspended (1.5 mg mL<sup>-1</sup>) in 454 0.5% sodium carboxymethyl cellulose (Zhao et al., 2013). Li and co-workers reported an oral 455 bioavailability of  $7.5 \pm 1.8\%$  in WT male Sprague-Dawley rats after oral administration of a 6 mg kg<sup>-</sup> 456 <sup>1</sup> etoposide solution prepared as an injectable formulation (specific composition not specified) (Li et 457 al., 2009). In the present study, it was not clear why the oral bioavailability of etoposide was low in 458 459 the control group, however, besides the known variabilities observed between animal studies (Festing and Altman, 2002), one could speculate that the 57% of ethanol could be the cause, since etoposide 460 could precipitate in the intestinal lumen. In the previous study by Al-Ali et al, the oral bioavailability 461 of etoposide (27%) was obtained after administration of 20 mg kg<sup>-1</sup> in 40% ethanol (2 mg ml<sup>-1</sup>) 462 administered with a dosing volume of 10 mL kg<sup>-1</sup> (Al-Ali et al., 2018a). In the present study an 463 etoposide solution (2.86 mg mL<sup>-1</sup>) in 57% (v/v) ethanol at a dose of 20 mg kg<sup>-1</sup> etoposide and a dosing 464 volume of 7 mL kg<sup>-1</sup> was used, thus approximately similar absolute amounts of ethanol were 465 administered in the two studies, but the concentration of etoposide and the amount of water differ, 466 with concentration of etoposide in the previous study being lower and water amount higher. This 467 468 could affect the susceptibility of etoposide precipitation in the solution used here to be higher. Ethanol is rapidly absorbed in rats with a t<sub>max</sub> less than 60 min and 50% disappearance of ethanol from the 469 stomach after 60 min (Siegers et al., 1972). If etoposide has indeed precipitated, this could explain 470 471 the low bioavailability. Population analysis indicated that formulation G decreased both the oral 472 bioavailability and the absorption rate while a clear increase in oral bioavailability was quantified in the presence of zosuquidar administration. Introduction of these covariate effects on the respective 473 474 parameters of the population pharmacokinetic model significantly decreased the objective function values (OFVs) and improved the model fit upon inspection of diagnostic plots (see Table 2). It has 475 been described earlier that 25% (v/v) polysorbate 20 decreased etoposide oral absorption, when 476

similar doses of 20 mg kg<sup>-1</sup> of etoposide were co-administered in rats (Al-Ali et al., 2018a). In the study reported by Al-Ali et al., dialysis experiments showed that polysorbate 20 at 25% (v/v) abolished etoposide release across polycarbonate membranes (Al-Ali et al., 2018a). In contrast, the present study showed that etoposide release from the matrix across polycarbonate membrane was not affected by the presence of different components in the formulation such as pluronic<sup>®</sup> F-127. *In vivo*, this points to an effect of the high ethanol concentration rather than incomplete release from colloidal structures present in the intestinal lumen.

484

#### 485 **5.** Conclusion

In conclusion, an oral formulation of high-concentration of etoposide, which maintained etoposide in 486 487 a solubilized form under short-term storage conditions and when diluted with simulated intestinal fluid was developed. Administration of increasing etoposide doses using this formulation-matrix 488 enhanced the plasma exposure of etoposide dose-proportionally. However, the applied doses were 489 not able to saturate P-gp, and the absolute absorption fraction decreased as a function of increasing 490 dose. To saturate intestinal P-gp by etoposide in rats, oral formulations maintaining high 491 492 concentrations of etoposide in solution are needed, yet the present study is a starting point for developing formulation approaches using other drug candidates aimed at increasing the oral 493 absorption of P-gp substrates and illustrates the difficulties in developing formulations aimed at 494 495 saturating intestinal P-gp transport.

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503

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506

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512

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514

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#### 673 Figures Legends:

## **Figure 1. Transepithelial P-gp dependent flux of etoposide across Caco-2 cell monolayers.** The steady-state P-gp dependent flux (pmol cm<sup>-2</sup> min<sup>-1</sup>) of etoposide across Caco-2 cells grown on permeable support for 24-28 days was studied as a function of etoposide concentration ( $C_d$ , $\mu M$ ) in the donor solution. The A-B transport (**A**) and B-A (**B**) transport was measured in 3 cell passages. In

B, the line is obtained by fitting experimental points to Eq. 1 described in Materials and Methods.
Values are given as mean ± SEM.

680

Figure 2. Pictures of etoposide formulations after 15 hours of storage at room temperature.
Formulation B contained 12 mg mL<sup>-1</sup> etoposide, 10% (w/v) of pluronic<sup>®</sup> F-127 in 44% (v/v) ethanol.
Formulation G contained 16 mg mL<sup>-1</sup> etoposide, 10% (w/v) of pluronic<sup>®</sup> F-127, and 10% (w/v) of
PVP/VA in 57% (v/v) ethanol.

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Figure 3. Absorbance measurments at 400 nm of etoposide formulations added to fasted state simulated intestinal fluid (FaSSIF) in a ratio of (Formulation:FaSSIF, 1:2) as a function of time. Etoposide formulations were composed as shown in Table 1. The measurments were performed at room temperature. For formulation G, n=4 and as mean  $\pm$  SEM, for other formulations n=1.

690

Figure 4. Time dependent release of etoposide and glycine from different formulations across 691 **0.03 µm polycarbonate membrane.** Donor solutions of <sup>3</sup>H-etoposide and <sup>14</sup>C-glycine were prepared 692 in Hanks Balanced Salt Solution (HBSS) buffer supplemented with 10 mM HEPES and adjusted to 693 pH 7.40  $\pm$  0.05 (Control), or in different formulation-matrix containing 10% (w/v) PVP/VA, 57% 694 (v/v) ethanol, and pluronic<sup>®</sup> F-127 (PF127) at 1.5, 3, or 10% (w/v), referred as Matrix-PF127 1.5%, 695 Matrix-PF127 3%, or Matrix-PF127 10%, respectively, or mixed with formulation G which contained 696 15-16 mg mL<sup>-1</sup> etoposide, 10% (w/v) of PF127 and PVP/VA, and 57% (v/v) ethanol. Receiver-release 697 media were HBSS buffer supplemented with 10 mM HEPES and adjusted to pH  $6.50 \pm 0.05$  for all 698 conditions, except in formulation G condition where the receiver-release media was the matrix of 699

700	formulation G (i.e. 10% (w/v) of PF127 and PVP/VA, and 57% ethanol, and q.s. water but without
701	etoposide). Experiments were performed at 37 °C and shaking mode 220 rpm. Data are expressed in
702	mean $\pm$ SEM from 3-4 independent membranes and as one membrane per experiment.

703

704

Figure 5. Plasma concentration time profile of etoposide after intravenous administration of 5
 mg kg<sup>-1</sup> etoposide to wild-type male Sprague-Dawley rats. Each data point is shown as mean ±
 SEM from 3-6 rats.

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709 Figure 6. Plasma concentration time profiles of etoposide after oral administration of different doses of etoposide in wild-type male Sprague-Dawley rats. A) Etoposide was administered orally 710 at a dose of 20 mg kg<sup>-1</sup> in 57% (v/v) ethanol solution (Control), or at increasing doses of etoposide 711 dissolved in matrix at 20, 50, and 100 mg kg<sup>-1</sup> etoposide. The matrix was consisted of 10 % (w/v) 712 pluronic<sup>®</sup> F-127 and PVP/VA, and 57% (v/v) ethanol, and q.s. water. At the highest oral dose, the 713 714 formulation is referred as formulation G. B) Etoposide was administered orally as control after the rats were received an oral dose 20 mg kg<sup>-1</sup> of zosuquidar. Each data point is shown as mean  $\pm$  SEM 715 716 from 5-6 rats. The solid lines are only connecting the data points.

717

#### 718 Supplementary Figure S1. AUC after oral administration as a function of dose.

Each data point is shown as mean  $\pm$  SEM from 5-6 rats.

720

Table 1: Composition of oral formulations of etoposide. (nd : not determined,  $\checkmark$ : Yes,  $\div$  : no). <sup>a</sup>: (Li et al., 2012; Xu and Dai, 2013)

	Formulations						Function			
Composition	A	В	С	D	Е	F	G			
Etoposide (mg mL <sup>-1</sup> )	9	12	12	15	15	15	16	API, P-gp substrate		
Pluronic <sup>®</sup> F-127 (% w/v)	4.7	10	6	6	2	6	10	Surfactant, precipitation inhibitor <sup>a</sup>		
PVP/VA (% w/v)	5	-	15	-	5	10	10	Precipitation inhibitor		
Ethanol (% v/v)	44	44	57	57	57	57	57	Co-solvent/solvent		
Ultra-purified water	qs	qs	qs	qs	qs	qs	Qs	Solvent		
Stable under storage for 15 h	$\checkmark$	÷	$\checkmark$	$\checkmark$	$\checkmark$	$\checkmark$	$\checkmark$			
Stable for 2 h after dilution with FaSSIF	nd	nd	÷	÷	÷	÷	$\checkmark$			

Table 2: Population pharmacokinetic parameter estimates of the base structural model and the final covariate model. Precision of the parameter estimates is reported as relative standard error (RSE%). F = oral bioavailability, k<sub>a</sub> = absorption rate, V1 = volume of the central compartment, V2 = volume of the peripheral compartment, CL = elimination clearance, Q2 = intercompartmental clearance,  $\beta_{F,FORM}$  = categorical covariate effect of formulation G presence on F,  $\beta_{F,ZOSU}$  = categorical covariate effect of zosuquidar presence on F,  $\beta_{K_a,FORM}$  = categorical covariate effect of formulation G presence on k<sub>a</sub>, a = additive error model term, b = proportional error model term, OFV = objective function value, -2LL = minus 2 times log likelihood, AIC = Akaike information criterion.

	Base structural model	Final covariate model						
Fixed effects [RSE%]								
F (%)	6.76 [24.2]	3.92 [16.7]						
k <sub>a</sub> (h <sup>-1</sup> )	2.69 [13.1]	4.54 [20.2]						
V1 (L kg <sup>-1</sup> )	3.63 [18]	2.91 [18.7]						
V2 (L kg <sup>-1</sup> )	3.18 [12.2]	3.78 [17.9]						
CL (L h <sup>-1</sup> kg <sup>-1</sup> )	1.61 [4.62]	1.55 [10.1]						
Q2 (L h <sup>-1</sup> kg <sup>-1</sup> )	6.56 [13.6]	6.98 [18.6]						
$\beta_{F,FORM}$	-	-0.51 [37.9]						
$\beta_{F,ZOSU}$	-	2.17 [7.04]						
$\beta_{k_a,FORM}$	-	-0.713 [34.8]						
Random effects (SD) [RSE%]								
F	1.1 [13.4]	0.158 [28.1]						
ka	0.552 [20.6]	0.502 [23.2]						
V1	0.924 [13]	0.678 [15]						
CL	0.122 [35.6]	0.118 [38.8]						
Error model [RSE%]								
a	0.01 [14.1]	0.0115 [14.5]						
b	0.132 [9.34]	0.135 [10.9]						
OFV								
-2LL	-665.17	-734.78						
AIC	-641.17	-704.78						

Table 3: Estimated pharmacokinetic parameters after intravenous and oral administration of different doses of etoposide in wildtype male Sprague-Dawley rats. Matrix solution consisted of 10 % (w/v) pluronic<sup>®</sup> F-127, 10% (w/v) PVP/VA, 57% (v/v) ethanol, and q.s. water. Individual Bayesian (post hoc) estimates were used to calculate mean AUC<sub>0-∞</sub>. Data are expressed as mean ± SEM except for t<sub>max</sub> that is expressed as the median [Q1; Q3] (25% and 75% percentile). No random effects were estimated for Q and V<sub>2</sub>. Fixed effects were estimated as Q = 6.98 mL h<sup>-1</sup> kg<sup>-1</sup>, V<sub>2</sub> = 3778 mL kg<sup>-1</sup>. Statistical significance was tested by one-way ANOVA followed by Tukey's multiple comparisons test. When all the groups, except the group of rats pre-dosed with zosuquidar and the group of rats receiving i.v. administration, were included in the comparison, (\*) referred to P < 0.05 compared to control. When all the groups, except the group of rats receiving i.v. administration, were included in the comparison, (<sup>†</sup>) referred to P < 0.05 compared to control.

	Study cohorts								
Etoposide dose	20 mg kg <sup>-1</sup>	20 mg kg <sup>-1</sup>	50 mg kg <sup>-1</sup>	100 mg kg <sup>-1</sup>	20 mg kg <sup>-1</sup>	5 mg kg <sup>-1</sup>			
Condition	Control				Zosuquidar				
Etoposide solution	57% EtOH	Matrix	Matrix	Matrix	57% EtOH	57% EtOH			
Cohort Size	6	5	6	6	6	6			
Administration route	p.o.	p.o.	p.o.	p.o.	p.o.	i.v.			
F (%)	$4.0\pm0.13$	$2.4\pm0.02*$	$2.4\pm0.07*$	$2.2\pm0.09*$	$34.5\pm0.18^\dagger$	$100 \pm 0$			
ka (h <sup>-1</sup> )	$6.40\pm0.94$	$2.29\pm0.41^{*\dagger}$	$2.36\pm0.35^{*\dagger}$	$2.32\pm0.32^{*\dagger}$	$3.43\pm0.41^{\dagger}$	-			

CL (mL h <sup>-1</sup> kg <sup>-1</sup> )	$1547\pm28$	$1533\pm 6.9$	$1503\pm24$	$1587\pm39$	$1550\pm43$	$1636\pm85$
V1 (mL kg <sup>-1</sup> )	$3830\pm574$	$4263 \pm 193$	$4143\pm315$	$4953\pm 640$	$2996 \pm 436$	$809\pm50$
$AUC_{0-\infty}$ (ng h mL <sup>-1</sup> )	$518.8\pm25$	$307.2 \pm 3.5^{*}$	$816.5\pm38^*$	$1525\pm86^*$	$4511\pm384^\dagger$	$3096 \pm 155$
$AUC_{0-\infty}/D$ (h mL <sup>-1</sup> kg)	$25.9 \pm 1.3$	$15.4\pm0.2$	$16.3\pm0.8$	$14.2\pm0.9$	$225.5\pm19.2$	$619.2\pm31.0$
t½ (h)	$1.73\pm0.27$	$1.93 \pm 0.08$	$1.91\pm0.14$	$2.18\pm0.31$	$1.36\pm0.23$	$0.35\pm0.02$
t <sub>max</sub> (h)	0.375 [0.25-0.5]	0.625 [0.44-0.75]	0.75 [0.25-1.06]	0.75 [0.5-1.25]	0.5 [0.5-0.81]	-
C <sub>max</sub> (ng mL <sup>-1</sup> )	$191 \pm 19$	$63 \pm 4*$	$169 \pm 17$	$266 \pm 38*$	$1542\pm190^\dagger$	-







- -O- FaSSIF
- ← Formulation C + FaSSIF
- --- Formulation D + FaSSIF
- → Formulation E + FaSSIF
- -D- Matrix-G without etoposide + FASSIF
- **D** Formulation G + FaSSIF







- 20 mg kg<sup>-1</sup> (Control)
- **D** 20 mg kg<sup>-1</sup> in matrix
- **▼** 50 mg kg<sup>-1</sup> in matrix
- ▲ 100 mg kg<sup>-1</sup> in matrix (Formulation G)





