



# Highly magnetic iron carbide nanoparticles as effective $T_2$ contrast agents†

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This paper reports that iron carbide nanoparticles with high air-stability and strong saturation magnetization can serve as effective  $T_2$  contrast agents for magnetic resonance imaging.  $\text{Fe}_5\text{C}_2$  nanoparticles ( $\sim 20$  nm in diameter) exhibit strong contrast enhancement with an  $r_2$  value of  $283.2 \text{ mM}^{-1} \text{ s}^{-1}$ , which is about twice as high as that of spherical  $\text{Fe}_3\text{O}_4$  nanoparticles ( $\sim 140.9 \text{ mM}^{-1} \text{ s}^{-1}$ ). *In vivo* experiments demonstrate that  $\text{Fe}_5\text{C}_2$  nanoparticles are able to produce much more significant MRI contrast enhancement than conventional  $\text{Fe}_3\text{O}_4$  nanoparticles in living subjects, which holds great promise in biomedical applications.

Magnetic resonance imaging (MRI), based on the interaction of protons with the surrounding molecules of tissues that can provide excellent anatomical details, is currently one of the most powerful medical imaging techniques.<sup>1</sup> MRI contrast agents are a group of contrast media that can greatly improve the accuracy and specificity of MRI by enhancing the visibility of the target from the background.<sup>2–5</sup> For example, superparamagnetic iron oxide nanoparticles with the ability to shorten  $T_2$  relaxation times are one of the most common negative contrast agents and have been used in the clinic.<sup>6–8</sup> However, iron oxide nanoparticles with relatively low saturation magnetization exhibit moderate  $T_2$  contrast enhancement. The transverse relaxivity ( $r_2$ ) values of commercial iron oxide based contrast agents, such as ferumoxides, ferumoxtran, and ferumoxsil, are typically in the range  $50\text{--}110 \text{ mM}^{-1} \text{ s}^{-1}$  at 0.47 T.<sup>9</sup> Recently, intensive research has been devoted to synthesizing highly magnetic nanoparticles, since nanoparticles with larger saturation magnetizations can more effectively shorten  $T_2$  relaxation times, resulting in greater

MRI contrast enhancement.<sup>10–12</sup> For example, manganese or zinc-doped iron oxide nanoparticles with high magnetization and increased relaxivity have been developed.<sup>13–16</sup> However, doping nanoparticles with potentially toxic metals has always been a concern because of their harmful effects in living organisms. Iron has the highest saturation magnetization at room temperature of any element,<sup>17</sup> and has been shown to be a safe element in the body after the biodegradation of iron oxide nanoparticles,<sup>18,19</sup> suggesting that iron nanoparticles may be ideal contrast agents for high-performance MRI. Despite tremendous efforts, the development of stable iron nanoparticles remains challenging due to the fast oxidation of iron and the significant loss of magnetization upon exposure to air,<sup>20</sup> which hampers the further biomedical applications. Therefore, it is necessary to develop a suitable iron-based contrast agent that not only has a large saturation magnetization value, but also is stable in biological media for diagnostic applications.

Iron carbides have attracted considerable attention over the past several decades owing to their distinguished properties and promising applications. Recently, several studies have been focused on the synthesis of iron carbide nanostructures with controlled size and morphology.<sup>21–24</sup> Iron carbide nanoparticles exhibit excellent catalytic activity and high magnetization, and hold great promise for applications in catalysis and magnetic hyperthermia.<sup>23,24</sup> Herein, we investigate the stability of iron carbide nanoparticles with high saturation magnetization and report that  $\text{Fe}_5\text{C}_2$  nanoparticles can serve as biocompatible and effective  $T_2$  contrast agents for *in vivo* MRI.

The transmission electron microscopy (TEM) image shows that the as-synthesized  $\text{Fe}_5\text{C}_2$  nanoparticles were  $\sim 20$  nm in diameter with spherical and rod-shaped structures (Fig. 1a). The high-resolution TEM (HRTEM) image reveals that the lattice spacing in the core was 0.205 nm, corresponding to the (510) plane of  $\text{Fe}_5\text{C}_2$ , while the shell was amorphous (Fig. 1b). The X-ray powder diffraction (XRD) pattern confirms that the crystal structure of iron carbide nanoparticles is consistent with that of  $\text{Fe}_5\text{C}_2$  (JCPDS no. 36-1248). We further employed X-ray photoelectron spectroscopy (XPS) to investigate the surface

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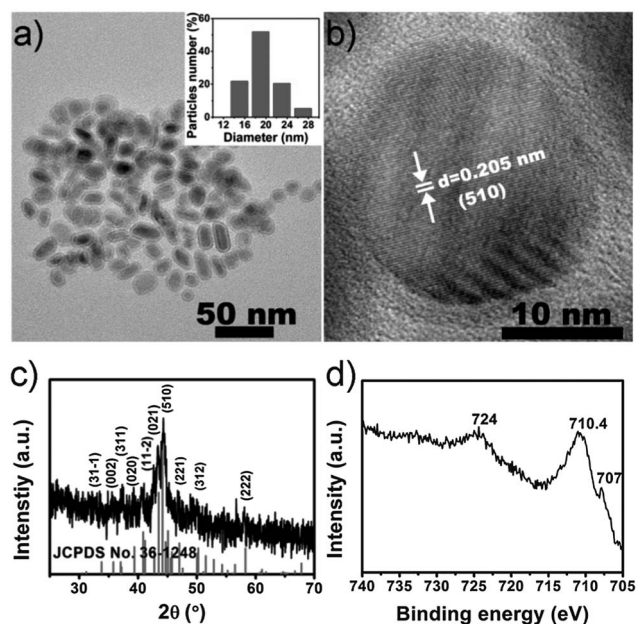


Fig. 1 (a) TEM image and size distribution histogram (inset), (b) HRTEM image, (c) XRD pattern, and (d) Fe 2p XPS spectrum of  $\text{Fe}_5\text{C}_2$  nanoparticles.

nature of  $\text{Fe}_5\text{C}_2$  nanoparticles (Fig. 1d). The peak at  $\sim 707$  eV in the Fe 2p XPS spectrum can be ascribed to the Fe–C bond,<sup>23</sup> indicating the successful synthesis of iron carbide nanoparticles. Two peaks at  $\sim 710.4$  eV and  $\sim 724$  eV can be assigned to iron(III) oxide,<sup>25</sup> together with the peak at  $\sim 284$  eV in the C 1s spectrum (Fig. S1†), indicating the coexistence of the iron oxide and the carbon amorphous shell.<sup>23</sup>

We then investigated the magnetic properties of  $\text{Fe}_5\text{C}_2$  nanoparticles using a superconducting quantum interference device (SQUID) magnetometer. The hysteresis loop shows that the as-synthesized  $\text{Fe}_5\text{C}_2$  nanoparticles exhibit a soft ferro/ferrimagnetic behavior with a saturation magnetization value of  $\sim 120$  emu  $\text{g}^{-1}$  at 300 K (Fig. 2a). This saturation magnetization value is very close to that of the iron carbides reported previously,<sup>22,26</sup> and is much higher than that of iron oxide nanoparticles with similar size (typically range from 40–70 emu  $\text{g}^{-1}$ ).<sup>27–29</sup> Remarkably, the  $\text{Fe}_5\text{C}_2$  nanoparticles also display a high stability against oxidation. The  $\text{Fe}_5\text{C}_2$  nanoparticles show little magnetization change even after two month air exposure (Fig. 2b). The highly crystalline structure and the presence of carbon atoms may prevent the oxidation of  $\text{Fe}_5\text{C}_2$  nanoparticles. For comparison, we synthesized the amorphous Fe (denoted as amor-Fe) nanoparticles<sup>20</sup> with  $\sim 14$  nm in diameter and studied the stability in air. The saturation magnetization of the freshly prepared  $\sim 10$  nm Fe nanoparticles has been reported up to 198 emu  $\text{g}^{-1}$ .<sup>24</sup> In our experiment, the saturation magnetization of the as-synthesized  $\sim 14$  nm amor-Fe nanoparticles dropped to  $\sim 100$  emu  $\text{g}^{-1}$  only after 1 day air exposure, and was further decreased to  $\sim 26$  emu  $\text{g}^{-1}$  after 30 days. Obviously, the  $\text{Fe}_5\text{C}_2$  nanoparticles are much more stable than amor-Fe nanoparticles in air, suggesting that  $\text{Fe}_5\text{C}_2$  nanoparticles with great feature of excellent oxidation resistance are suitable for further potential applications.

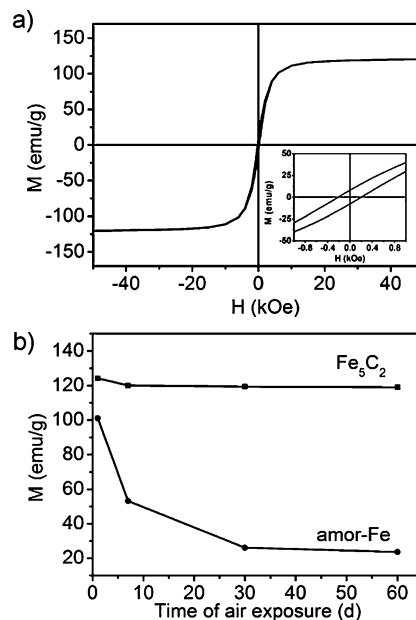


Fig. 2 (a) Magnetic hysteresis loop of the  $\text{Fe}_5\text{C}_2$  nanoparticles recorded at 300 K (inset: magnification of the low-field region). (b) Stability analysis of  $\text{Fe}_5\text{C}_2$  nanoparticles and amor-Fe nanoparticles in air.

To make the as-synthesized  $\text{Fe}_5\text{C}_2$  nanoparticles water-dispersible for biomedical applications, we simply modified the particle surface with sodium tartrate *via* a ligand exchange method. The obtained aqueous solution containing  $\text{Fe}_5\text{C}_2$  nanoparticles is highly stable over at least three months without any precipitate (Fig. S2†), suggesting that tartrate-coated  $\text{Fe}_5\text{C}_2$  nanoparticles are suitable for *in vitro* and *in vivo* studies. The morphology of nanoparticles shows no obvious change as observed in TEM images (Fig. S2†). The dynamic light scattering (DLS) analysis indicates that the tartrate-coated  $\text{Fe}_5\text{C}_2$  nanoparticles are very stable without aggregation in aqueous solution (Fig. S3†). We then evaluated the cytotoxicity of the water-dispersible  $\text{Fe}_5\text{C}_2$  nanoparticles using the tetrazolium-based colorimetric assay (MTT assay). The result shows that more than 85% of cells were viable even at the highest concentration (100  $\mu\text{g Fe mL}^{-1}$ ,  $\sim 1.8$  mM, measured by inductively coupled plasma atomic emission spectroscopy, ICP-AES), indicating the good biocompatibility of tartrate-coated  $\text{Fe}_5\text{C}_2$  nanoparticles (Fig. 3).

We next investigated the ability of  $\text{Fe}_5\text{C}_2$  nanoparticles for MRI contrast enhancement. We used  $\text{Fe}_3\text{O}_4$  nanoparticles ( $\sim 20$  nm in diameter) and amor-Fe nanoparticles ( $\sim 14$  nm in diameter) as two control samples (Fig. S4†). All tartrate-coated solution samples have been stored in the air for one month. We first prepared samples of these three types of nanoparticles with different Fe concentrations (determined by ICP-AES) and collected the  $T_2$ -weighted phantom images at a 0.5 T MRI system. For a given Fe concentration,  $\text{Fe}_5\text{C}_2$  nanoparticles exhibit the strongest negative contrast effect (darken signal) among three types of nanoparticles, suggesting the capability of  $\text{Fe}_5\text{C}_2$  nanoparticles as high-performance  $T_2$  MRI contrast agents (Fig. 4a). We further measured the transverse relaxivity ( $r_2$ ) at 0.5 T according to the linear relationship of transverse

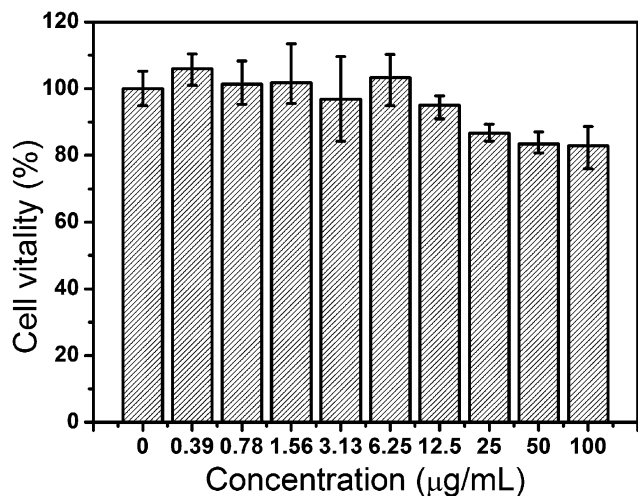


Fig. 3 Cell viability of HeLa cells after being incubated with  $\text{Fe}_5\text{C}_2$  nanoparticles with different Fe concentrations at 37 °C for 24 h.

relaxation rates ( $R_2$ , i.e.,  $1/T_2$ ) versus Fe concentrations (Fig. 4b). The  $r_2$  value of  $\text{Fe}_5\text{C}_2$  nanoparticles is  $\sim 283.2 \text{ mM}^{-1} \text{ S}^{-1}$ , which is about twice as high as that of  $\text{Fe}_3\text{O}_4$  nanoparticles ( $\sim 140.9 \text{ mM}^{-1} \text{ S}^{-1}$ ) and also much higher than those of commercial  $T_2$  contrast

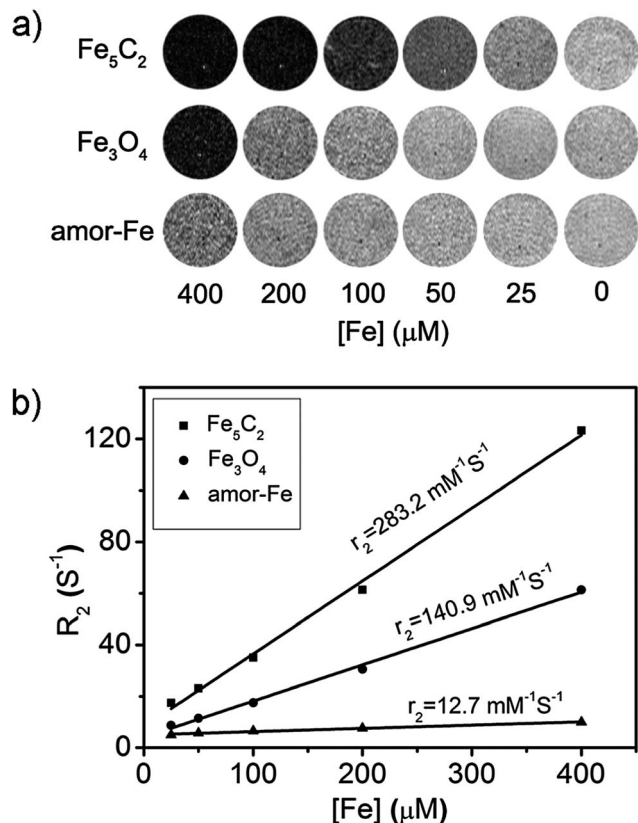


Fig. 4 (a)  $T_2$ -weighted phantom images of  $\text{Fe}_5\text{C}_2$  nanoparticles,  $\text{Fe}_3\text{O}_4$  nanoparticles, and amor-Fe nanoparticles in aqueous solution (containing 1% agar) with different Fe concentrations, respectively. (b) The linear fitting of relaxation rates ( $R_2$ ) versus Fe concentrations for  $\text{Fe}_5\text{C}_2$  nanoparticles,  $\text{Fe}_3\text{O}_4$  nanoparticles, and amor-Fe nanoparticles, respectively. The relaxivity values ( $r_2$ ) were obtained from the slopes.

agents (e.g., ferumoxides),<sup>9</sup> confirming that  $\text{Fe}_5\text{C}_2$  nanoparticles have much stronger  $T_2$  contrast enhancement than  $\text{Fe}_3\text{O}_4$  nanoparticles. On the basis of the quantum mechanical outer sphere theory, the  $T_2$  relaxivity is highly dependent on the saturation magnetization of the nanoparticles.<sup>12,30,31</sup>  $\text{Fe}_5\text{C}_2$  nanoparticles with high saturation magnetization can afford effective magnetic relaxations to the water protons around the nanoparticles and therefore results in the enhanced relaxivity.<sup>32,33</sup> The  $r_2$  value of amor-Fe nanoparticles is only  $12.7 \text{ mM}^{-1} \text{ S}^{-1}$ , which is extremely lower than those of  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles. The significant loss of magnetization results in the poor performance of amor-Fe nanoparticles in MRI contrast enhancement. Moreover, the further oxidation and instability of amor-Fe nanoparticles make them unsuitable for biomedical applications. Thus, we only used  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles as samples in subsequent *in vivo* MRI experiments.

Iron oxide nanoparticles have been extensively developed for the diagnosis of liver diseases because they are highly taken up by the hepatic Kupffer cells.<sup>34–36</sup> Thus, we focused on the liver as the targeting region for evaluating the *in vivo* MRI effects of  $\text{Fe}_5\text{C}_2$  nanoparticles. The  $r_2$  values of the  $\text{Fe}_5\text{C}_2$  and  $\text{Fe}_3\text{O}_4$  nanoparticles are 428.5 and  $232.2 \text{ mM}^{-1} \text{ S}^{-1}$  at 7 T, respectively (Fig. S5†). Meanwhile, the  $r_2$  value of  $\text{Fe}_5\text{C}_2$  nanoparticles is approximately two times larger than that of  $\text{Fe}_3\text{O}_4$  nanoparticles, which is consistent with the results obtained at 0.5 T. We intravenously injected  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles into the BALB/c mice (dosage of 2.0 mg Fe per kg, Fe concentration determined by ICP-AES) and obtained  $T_2$ -weighted images at different time points after injection on a 7 T Varian MRI scanner.  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles may have comparable biodistribution (e.g., similar liver uptake of nanoparticles) because of their similar size and surface chemistry.<sup>37,38</sup> Both coronal and transverse images show that the liver regions exhibited a noticeably darker signal after the injection of  $\text{Fe}_3\text{O}_4$  and  $\text{Fe}_5\text{C}_2$  nanoparticles (Fig. 5a and S6†). In comparison with  $\text{Fe}_3\text{O}_4$  nanoparticles,  $\text{Fe}_5\text{C}_2$  nanoparticles produced significantly darker signal in liver regions probably due to their higher  $r_2$  value. To quantify the contrast enhancement, we calculated the signal-to-noise ratio (SNR) by finely analyzing regions of interest (ROIs) of the transverse images and defined the contrast enhancement as the decrease of SNR,  $\Delta \text{SNR} = (|\text{SNR}_{\text{post}} - \text{SNR}_{\text{pre}}|) / \text{SNR}_{\text{pre}}$ . The measured  $\Delta \text{SNR}$  values of the  $\text{Fe}_5\text{C}_2$  nanoparticle group are  $54.1 \pm 7.3\%$ ,  $68.8 \pm 5.4\%$ ,  $85.0 \pm 3.8\%$ ,  $58.8 \pm 7.7\%$  at 0.5, 1 h, 2 h, 4 h after the injection, respectively, which is much higher than those of the  $\text{Fe}_3\text{O}_4$  nanoparticle group ( $26.8 \pm 3.4\%$ ,  $43.7 \pm 3.2\%$ ,  $47.1 \pm 1.7\%$ , and  $27.9 \pm 3.0\%$ , respectively), further demonstrating the excellent contrast ability of  $\text{Fe}_5\text{C}_2$  nanoparticles in MRI of small living subjects (Fig. 5b). It is worth noting that the  $\Delta \text{SNR}$  values have been falling at 4 h, and further decrease to  $28.2 \pm 5.4\%$  and  $15.3 \pm 2.2\%$  24 h after the injection of  $\text{Fe}_5\text{C}_2$  and  $\text{Fe}_3\text{O}_4$  nanoparticles, respectively. It is necessary to conduct MRI scanning within 2–4 h after administration of  $\text{Fe}_5\text{C}_2$  nanoparticles, which also meets the basic requirements of clinical diagnosis.

In summary, we successfully synthesized  $\text{Fe}_5\text{C}_2$  nanoparticles and investigated their ability to serve as high-performance  $T_2$

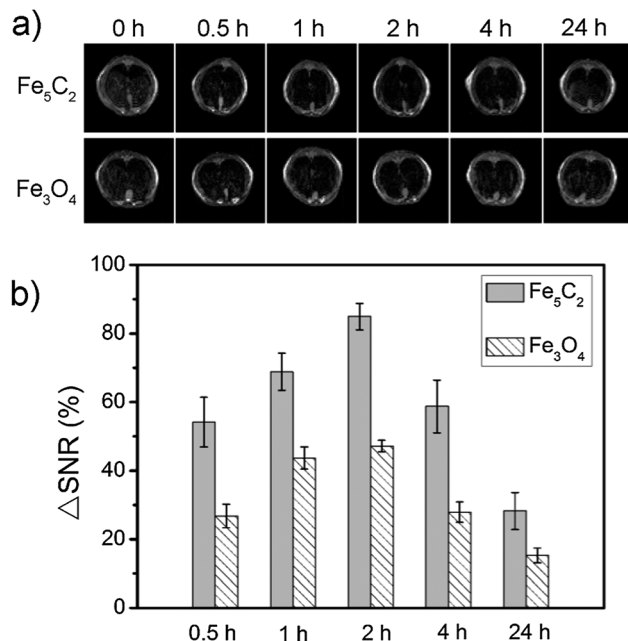


Fig. 5 (a)  $T_2$ -weighted *in vivo* MRI images of mice (transverse plane) collected at different time points after intravenous injection of  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles (with a dose of 2.0 mg Fe per kg of mouse body weight), respectively. (b) The decrease of signal-to-noise ratio ( $\Delta\text{SNR}$ ) at different time points after intravenous injection of  $\text{Fe}_5\text{C}_2$  nanoparticles and  $\text{Fe}_3\text{O}_4$  nanoparticles ( $n = 3$ ), respectively.

contrast agents. The as-synthesized 20 nm  $\text{Fe}_5\text{C}_2$  nanoparticles have a high saturation magnetization ( $\sim 120 \text{ emu g}^{-1}$ ) and remarkable oxidation resistance. Both *in vitro* and *in vivo* studies demonstrated that the  $\text{Fe}_5\text{C}_2$  nanoparticles were able to effectively shorten  $T_2$  relaxation times (with an  $r_2$  value of  $283.2 \text{ mM}^{-1} \text{ s}^{-1}$  at 0.5 T) and produce significant MRI contrast enhancement. We believe that such highly magnetic and stable iron carbide nanoparticles hold great promise in serving as novel and effective MRI contrast agents for liver imaging.

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