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## A multi-beam X-ray imaging detector using a branched optical fiber bundle

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We developed a multi-beam X-ray imaging detector, consisting of four scintillator screens connected by a branched optical fiber bundle with a CMOS camera. By using the detector and a multi-beam imaging optics with silicon single crystalline blades designed for a white synchrotron radiation source, we successfully demonstrated multi-beam X-ray imaging with an exposure time of 1 ms. The long and flexible optical fiber bundle used for the detector enables us to realize high-speed multi-beam X-ray imaging with high flexibility at a low cost.

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X-ray imaging is a powerful tool for two- and three-dimensional visualization of inner structures in samples that are opaque to visible light. A two-dimensional projection image is easily obtained with a simple experimental setup consisting of an X-ray source and an X-ray imaging detector. Synchrotron radiation (SR) sources and X-ray free-electron laser (XFEL) have enabled us to realize even lower than  $\mu\text{s}$  temporal resolutions<sup>1–10</sup> with the help of X-ray phase-contrast imaging techniques such as the propagation-based imaging (PBI)<sup>11–13</sup> or grating-based imaging (GBI) techniques.<sup>4,5,14–34</sup> However, inner structures in the depth direction cannot be differentiated from the projection image. On the other hand, X-ray tomography allows us to visualize three-dimensional structures in a sample, but it typically requires hundreds of projection images, which are obtained by the rotation of the sample or of both the X-ray source and detector. Recently, X-ray tomography for rotating samples with

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a measurement time of a few ms and a spatial resolution of a few tens of  $\mu\text{m}$  was successfully realized by using a white SR source.<sup>4,5,10,31)</sup> However, high-speed rotation of a sample with a few tens of thousands rpm hinders to precisely control the environment around the sample. In addition, the high-speed rotation cannot be applied to liquids and living animals because of the centrifugal force arising from the rotation.

Recently, a few X-ray multi-beam techniques have been proposed for SR sources and/or x-ray free-electron laser,<sup>35–37)</sup> which can differentiate inner structures in the depth direction, and real-time multi-beam X-ray imaging with a temporal resolution less than 10 ms could be realized if the images projected by the multi-beams are simultaneously obtained. In this paper, we report on a multi-beam X-ray imaging detector, consisting of four scintillator screens connected by a branched optical fiber bundle with a CMOS camera. Using the detector, we successfully obtained five projection images with a temporal resolution of 1 ms.

Photos of the branched optical fiber bundle used for the multi-beam X-ray detector are shown in Fig. 1. Each optical fiber constituting the bundle has a diameter of  $50\ \mu\text{m}$  and a length of 2 m (SOG-70S  $50\ \mu\text{m}$ , SUMITA OPTICAL GLASS, Inc.), and can be flexibly bent. The bundle has four branches, each of which has three segments with a size of  $5\ \text{mm} \times 7.5\ \text{mm}$  (totally,  $5\ \text{mm} \times 22.5\ \text{mm}$ ) and transmits images from one side to the other, as shown in the right figure of Fig. 1. The multi-beam X-ray detector was constructed by the branched optical fiber bundle, scintillator screens, relay lenses, and a CMOS camera for visible light (see Fig. 2). On the top of each branch of the bundle, the surface of a scintillator screen was fixed with optical oil sandwiched between them, and the other side was coupled with the relay lenses to the CMOS camera.

The experimental setup for multi-beam X-ray imaging using the detector is shown in Fig. 2. The experiment was performed at BL28B2 in SPring-8, Japan, where a white SR beam from a bending magnet is available. We employed a multi-beam X-ray optics consisting of four Si(001) single-crystalline blades with different angles to the impinging white SR beam,<sup>37)</sup> each of which reflects X-rays satisfying the Bragg condition. We used the Laue-case reflections from the (110) crystal planes, which were designed to cross on the sample. The four reflected X-ray beams passed through a sample, and projected its images on scintillator screens (Mitsubishi Chemical Corporation, DRZ-HR ( $\text{Gd}_2\text{O}_2\text{S}:\text{Tb}$ ,  $50\ \mu\text{m}$ )). The projected images on the screens were transmitted by the optical fiber bundle to its other side, and captured by a CMOS camera (Photron FASTCAM Mini AX50) with a pixel size of  $20\ \mu\text{m} \times 20\ \mu\text{m}$  through relay lenses with a magnification of 1. The white SR beam was also directly used for obtaining a projection image, which was captured by a high-spatial-resolution X-ray image detector

(the inset of Fig. 2) with an effective pixel size of  $4.6 \mu\text{m}$  consisting of a scintillator screen ( $\text{Gd}_2\text{O}_2\text{S: Tb}$ ,  $10 \mu\text{m}$ ), a mirror, relay lenses, and a CMOS camera (Photron FASTCAM Mini AX100).

For a demonstration of the multi-beam X-ray imaging, a USB flash memory was used as a sample. Figure 3 (a) shows a photo of the irradiated side of the sample. Figure 3 (b) shows a projection image (natural logarithm of the X-ray transmittance) of the sample with a large field of view, preliminarily obtained using a laboratory X-ray generator (RIGAKU Ultrax18 with a tungsten target, tube voltage 50 kV, tube current 10 mA, effective source size  $0.1 \text{ mm}$  (horizontal)  $\times$   $0.2 \text{ mm}$  (vertical)). The field of view corresponds to the area in the square shown in Fig. 3 (a). An X-ray imaging detector with an effective pixel size of  $5.5 \mu\text{m} \times 5.5 \mu\text{m}$  (Hamamatsu Photonics C14120-20P) based on a scintillator screen ( $50 \mu\text{m}$ -thick  $\text{Lu}_3\text{Al}_5\text{O}_{12}: \text{Ce}$ ), a fiber optic plate, and a CMOS camera was used with an exposure time of 1 s. Figures 3 (c1)-(c4) are the projection images corresponding to the area of the dotted square in Fig. 3 (b) obtained by the multi-beam imaging setup shown in Fig. 2. The four images were simultaneously obtained with an exposure time of 1 ms. Here, Figs. 3 (c1)-(c4) corresponds to beam 1, 2, 3, and 4 in Fig. 2, and the projection angles for the beams were  $11.5^\circ$ ,  $7.96^\circ$ ,  $-7.96^\circ$ , and  $-14.9^\circ$ , corresponding to 32.1 keV, 46.5 keV, 46.5 keV, and 24.9 keV for the 220 Bragg reflection, respectively. It can be seen that the positions of electrode B and hole C shift relative to component A. This shift in the positions reflects the difference in the depths of A, B, and C. The spatial resolution of the images was  $200 \mu\text{m}$ , which should be mainly determined by the thickness of the scintillator screen ( $50 \mu\text{m}$ ), the diameter of the optical fiber ( $50 \mu\text{m}$ ), and a finite distance between the scintillator screen and the surface of the optical fiber bundle. Figure 3 (d) is the projection image corresponding to the area of the dashed square in Fig. 3 (c2) obtained by using the white SR beam and the high-spatial-resolution X-ray imaging detector. The image was obtained with an exposure time of 0.1 ms and the spatial resolution of the image was  $10 \mu\text{m}$ , although its field of view is smaller than those obtained by the multi-beam detector. Thus, we demonstrated that the setup simultaneously provides four projection images with an exposure time of 1 ms and a high-spatial resolution projection image with an exposure time of 0.1 ms.

From the shift of electrode B and hole C relative to component A, we can estimate the depth of B and C relative to A. From linear least-squares fittings to the shifts obtained from the four images of Fig. 3 (c1)-(c4), the depths of B and C were estimated to be  $-1.20 \text{ mm}$  and  $-0.63 \text{ mm}$ , respectively, where the positive direction of depth was taken in the direction of the impinging X-ray beam from upstream to downstream.

**Fig. 1.** Photos of optical fiber bundle used for multi-beam X-ray detector (left) and transmitted image on one side (right).

**Fig. 2.** Schematic illustration of experimental setup for multi-beam X-ray imaging using white synchrotron radiation (SR) beam at BL28B2 in SPring-8, Japan (top view). Inset: side view of high-spatial-resolution X-ray imaging detector for white SR beam.

**Fig. 3.** (a) Photo of irradiated (upstream) side of sample (USB flash memory). (b)-(d) Projection images (natural logarithm of X-ray transmittance) of sample. (b) Preliminarily obtained projection image of sample by using laboratory X-ray source with field of view shown in (a) (gray scale:  $-4.5-0.3$ ). (c1)-(c4) Projection images obtained by multi-beam X-ray imaging detector for beam 1, 2, 3, and 4 in Fig. 2 (gray scale:  $-2.7-0.3$ ). (d) Projection image obtained by directly using white synchrotron beam (gray scale:  $-4.5-0.3$ )

One of the advantages of the multi-beam X-ray imaging detector is its flexibility. The scintillator screens on the top of the branched optical fiber bundle can be flexibly allocated for various multi-beam X-ray imaging experiments including those for laboratory X-ray sources.<sup>38-41)</sup> They can be located even inside a sample. In addition, the system can be realized at a lower cost than that required for several CMOS cameras. For these reasons, the multi-beam X-ray imaging detector reported in this paper should provide a promising approach for multi-beam X-ray imaging with a high speed and/or a high throughput.

In summary, we developed a four-beam X-ray imaging detector, consisting of four scintillator screens connected by a branched optical fiber bundle with a CMOS camera. By using the detector and a multi-beam imaging optics with silicon single crystalline blades designed for a white SR source, we successfully demonstrated five-beam X-ray imaging with an exposure time of 1 ms. The long and flexible optical fiber bundle used for the detector enables us to realize high-speed multi-beam X-ray imaging with high flexibility at a low cost.

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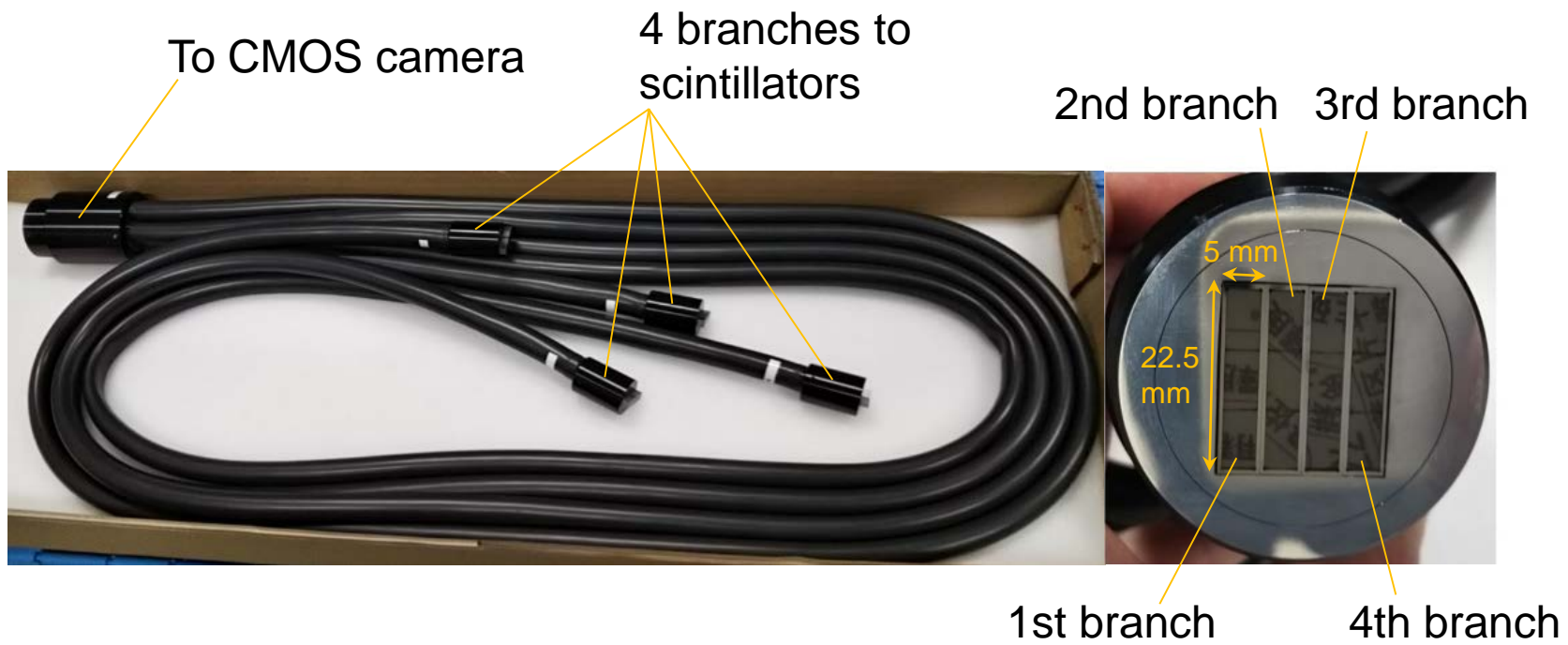


Fig. 1 W. Yashiro et al.

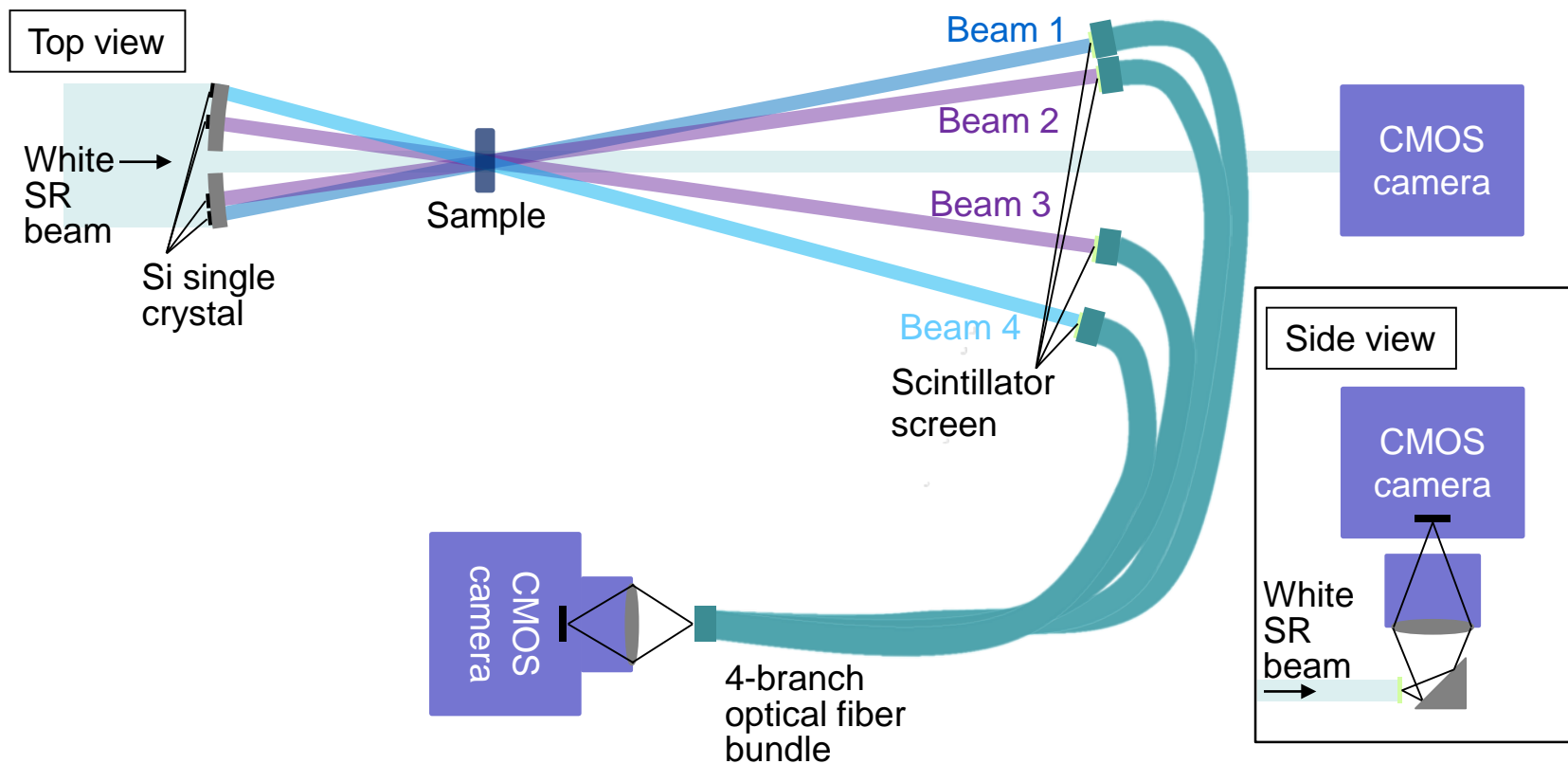


Fig. 2 W. Yashiro et al.

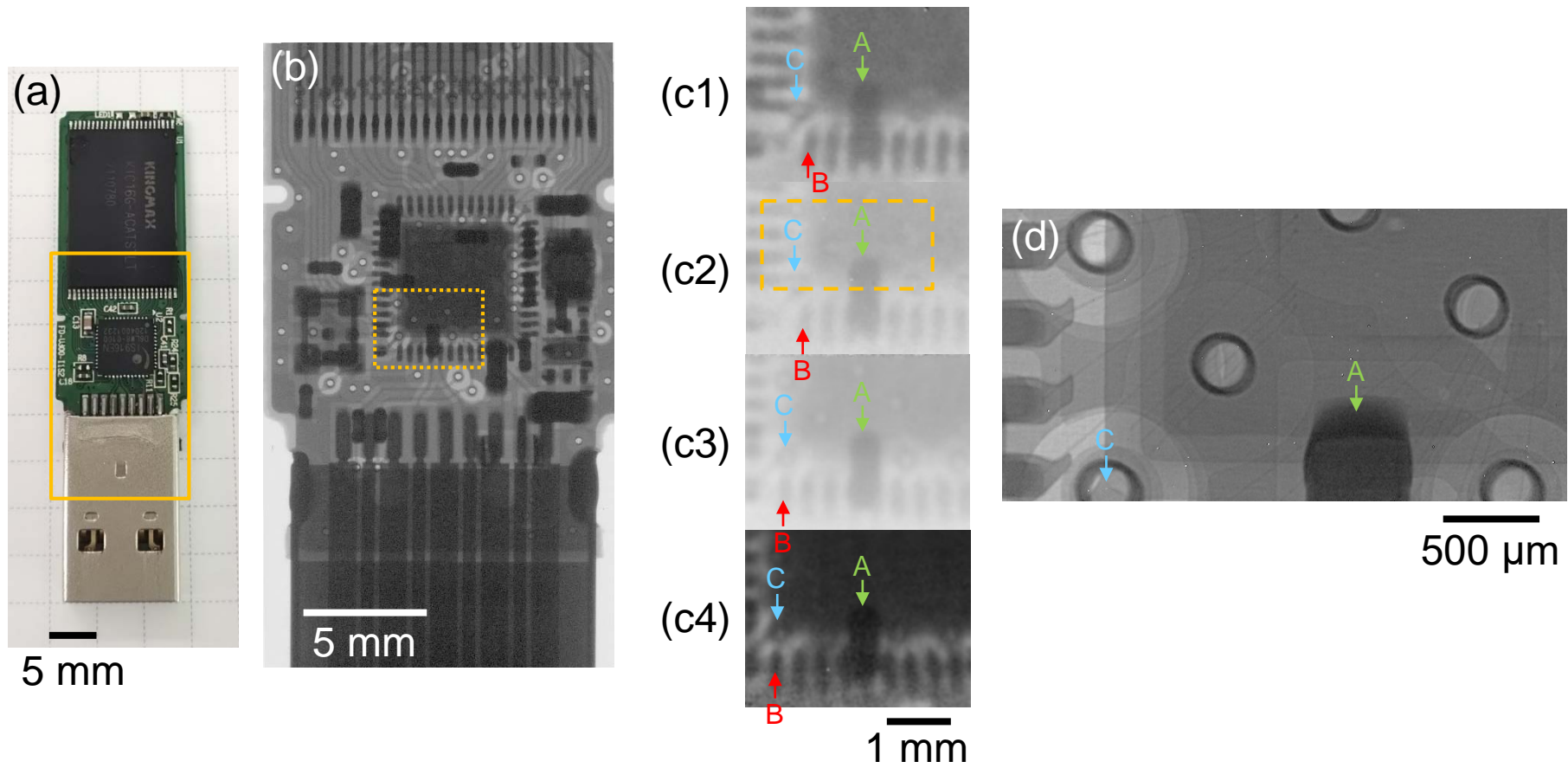


Fig. 3 W. Yashiro et al.