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TITLE OF SUBMISSION: A Comparative Evaluation of Endodontic Irrigation Methods for Removal of the Smear Layer

DATE SUBMITTED: December 13th, 2016

I certify that I am the sole author of this thesis, and that any assistance I received in its preparation has been fully acknowledged and disclosed in the thesis. I have cited any sources from which I used ideas, data, or words, and labeled as quotations any directly quoted phrases or passages, as well as providing proper documentation and citations. This thesis was prepared by me, specifically for the M.S. degree and for this assignment.

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A Comparative Evaluation of Endodontic Irrigation Methods for Removal of the Smear Layer

By

Ramzi Walid Alhashimi

A thesis submitted to the College of Dental Medicine of Nova Southeastern

University in partial fulfillment of the requirements for the degree of MASTER OF

SCIENCE IN DENTISTRY

Department of Endodontics

College of Dental Medicine

Nova Southeastern University

December 2016

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Synopsis

The purpose of this in vitro study is to compare the effect of various irrigation systems on smear layer removal in curved root canals.

Root canal irrigation plays an important role in the debridement and disinfection of the root canal system. It has been well documented that the flushing component of the irrigants is as important as the tissue dissolving capability. Therefore, the efficacy of the irrigant might also be influenced by the method by which it is introduced.

Fifty-one recently extracted molar teeth with root curvatures of more than 30° were selected according to Schneider's method. The teeth were decoronated to obtain a standardized root length of 12 mm. The root tips were sealed with hot glue and embedded into a silicone mold. The canal preparations were performed by using ProTaper[™] and ProFile[™] systems up to #35,04. Sodium hypochlorite (NaOCI 6%) and ethylenediaminetetraacetic acid (EDTA 17%) were used as root canal irrigants according to Yamada protocol. To maintain irrigation consistency, a programmable syringe pump was connected to each system.

After finishing the cleaning and shaping of the curved canals, the final cleansing of the root canal space, with proper irrigation solutions, were accompanied by activation systems.

Five different treatment modalities were tested; Group 1: Traditional irrigation, Group 2: EndoActivator[™], Group 3: Passive ultrasonic irrigation (PUI),

Group 4: EndoVac[™], Group 5: Saline. The root halves (n=102) were imaged with the FEI Quanta 200 scanning electron microscope[™] (SEM). Over 7000 magnified images were reviewed and scored by three board certified Endodontists in a double-blind manner. The data was analyzed by using the Cochran-Mantel-Haenszel method, Pairwise Comparisons and Intra-class correlation coefficients. The EndoVac[™] system (an apical negative pressure irrigation system) was found to be significantly more effective (p<0.05) than the other groups in all sections observed, this would include the apical, middle and coronal sections for the elimination of the smear layer as well as the debris removal and improved tubule visibility.

The negative pressure delivery systems may provide cleaner surfaces in the canals of curved roots of at least 30 degree or more.

Acknowledgements

I am very grateful to everyone who has supported me to reach my career goal. I am also honored to have won a research prize at the 2013 AAE conference in recognition of my work.

I would like to express my sincere gratitude to my mentor Dr T. Cem Sayin, for his patience, time, motivation, and immense knowledge. He was a constant source of information, support and optimism. His guidance helped me in all the time of research and writing of this thesis. I could not have imagined having a better mentor and advisor for my master study.

Furthermore, I would like to thank Dr Kenneth Namerow for providing advice, knowledge and for giving me this great opportunity to be in his program. Also, I like to thank Dr Michael Flax for being always there for me whenever I needed him. I thank Dr Rita Steiner for her time, support and for being a true friend.

I would like to express my very profound gratitude to my mother, my father and my sister Dana for providing me with unfailing support, love, faith and continuous encouragement throughout my years of study and throughout my life. I would not be the person I am today without them.

Table of Contents

<u>Title</u>		Page
Synopsis		4
Acknowle	edgments	6
Table of (Contents	7
Abbreviat	tions	10
Glossary	of Statistical Terms	12
Products	Used	13
1.	Introduction	14
1.1	Chemo-mechanical preparation	15
1.2	Dentin	17
1.3	Smear layer	19
1.4	Biofilm	21
1.5	Irrigation solutions	24
1.5.1	Sodium Hypochlorite (NaOCl)	24
1.5.2	Ethylenediaminetetraacedic Acid (EDTA)	35
1.6	Activation methods	40
2.	Materials and methods	53
3.	Results	64
4.	Discussion	77
5.	Conclusion	92

References 93	6. Refe
ires	List of Figures
1. Treatment Groups 59	Figure 1.
2. Representative SEM micrographs taken from the coronal, middle and the	Figure 2.
apical third of the canals	
3. Sample SEM micrograph to illustrate Nova Grid Scoring System taken	Figure 3.
from one of the EndoVac specimen	
4. Scoring System	Figure 4.
5. Sample from the form that was provided to the evaluator for data	Figure 5.
collection	
5.1. Distribution of tubule visibility scores at coronal, middle and apical levels	Figure 6.1.
5.2. Distribution of smear layer scores at coronal, middle and apical levels. 67	Figure 6.2.
5.3. Distribution of remaining debris scores at coronal, middle and apical	Figure 6.3.
levels	

List of tables

Table 1.	Average scores of SEM evaluation of tubule visibility, smear layer and
	remaining debris. Scores 1-2 (clean canal wall) versus 3-4
Table 2.	Tubules Descriptive Statistic 69
Table 2.1.	Tubules Intra Class Correlation Coefficient-Rater Agreement
Table 2.2.	Tubules Pairwise Comparisons for All Sections
Table 2.3.	Tubules Pairwise Comparisons for Coronal Sections

Table 2.4.	Tubules Pairwise Comparisons for Middle Sections	71
Table 2.5.	Tubules Pairwise Comparisons for Apical Sections	71
Table 3.	Smear Layer Descriptive Statistic	72
Table 3.1.	Smear Layer Intra Class Correlation Coefficient-Rater Agreement	72
Table 3.2.	Smear Layer Pairwise Comparisons for All Sections	72
Table 3.3.	Smear Layer Pairwise Comparisons for Coronal Sections	73
Table 3.4.	Smear Layer Pairwise Comparisons for Middle Sections	73
Table 3.5.	Smear Layer Pairwise Comparisons for Apical Sections	74
Table 4.	Debris Descriptive Statistic	74
Table 4.1.	Debris Intra Class Correlation Coefficient-Rater Agreement	74
Table 4.2.	Debris Pairwise Comparisons for All Sections	75
Table 4.3.	Debris Pairwise Comparisons for Coronal Sections	75
Table 4.4.	Debris Pairwise Comparisons for Middle Sections	76
Table 4.5.	Debris Pairwise Comparisons for Apical Sections	76

Abbreviations

μm	Micrometer
NiTi	Nickel-Titanium
ISO	International Standardization Organization
SEM	Scanning Electron Microscope
mm	Millimeter
AAE	American Association of Endodontists
TEM	Transmission Electron Microscope
PRC	Polymerase Chain Reaction
NaOCl	Sodium Hypochlorite
СНХ	Chlorhexidine
EDTA	Ethylenediaminetetraacedic Acid
MTAD	Mixture of a Tetracycline, Acid, and Detergant
min	Minute
h	Hour
F	Fahrenheit
°C	Degree Centigrade
CA	Citric Acid
STP	Sodium Triphosphate
PUI	Passive Ultrasonic Irrigation
UI	Ultrasonic irrigation

- MDT Master Delivery Tip
- ICC Intra-Class correlation coefficients
- C. albicans Candida albicans
- E. faecalis Enterococcus faecalis
- PSP Programmable Syringe Pump

Glossary of Statistical Terms

P value The probability of obtaining a result equal to or "more extreme" than what was actually observed when the null hypothesis is true. The p value significant level for this thesis was p<0.05.

Pairwise comparisons Is a statistical tool to rank and compare entities in pairs to decide which of each entity is favorable or if they are alike or not.

Cochran-Mantel-Haenszel method Is a technique utilized in the analysis between two categorical variables or groups to create an estimate for the relation between an exposure or treatment and the outcome.

Intra-class correlation coefficients Is a statistical assessment for the reliability of findings to show how strongly the items in the identical groups are related to each other.

Products Used

Name	Manufacturer	City, State
Max-I-Probe needle	Dentsply	York, PA
EndoActivator	Dentsply	York, PA
EndoVac	Discus Dental	Culver, CA
Sodium Hypochlorite	Vista Dental	Racine, WI
Ethylenediaminetetraacetic acid	Elleman	New York, NY
Global Endodontic Microscope	Global Surgical Corporation	St. Louis, MO
ProTaper	Dentsply	York, PA
ProFile	Dentsply	York, PA
Programmable Syringe Pump	World Precision Instruments, Inc	Sarasota, FL

1. Introduction

1.1 Chemo-mechanical preparation:

Endodontic therapy is based on the removal of infected pulpal tissues and dentinal debris from the root canal system. The success of the endodontic treatment depends on many factors, commonly called the Endodontic triad, such as mechanical preparation, irrigation, and root canal obturation (1-4).

The Chemo-mechanical preparation is accomplished by combining the mechanical instrumentation with the antibacterial irrigation. The goals of this preparation are to reduce microorganisms from root canal system which are known to cause inflammatory reaction, to remove organic and inorganic tissues that may support microbial growth, and to reduce the risk of pushing the debris beyond the apical construction of the root canal system which may cause inflammation (5).

Infected root canal systems can harbor between $<10^2$ to $>10^8$ bacterial cells (6). These bacteria are able to penetrate into dentinal tubules up to 400 μ m (7-9). Mechanical instrumentation is a key factor in microbial load reduction in the infected root canal system (5). Byström and Sundqvist found significant reduction in the number of bacterial in infected root canal by 100 to 1,000 fold after instrumentation with stainless steel hand files and irrigation with only 10 mL of physiologic saline solution per canal (10). However, canals could not be consistently rendered bacteria-free.

Dalton et al, compared bacterial reduction after instrumentation with either 0.04 tapered Nickel-Titanium (NiTi) rotary files to bacterial reduction with stainless steel K-file step back technique using only sterile saline. No significant difference was found between the two techniques with 72% of instrumented teeth still harboring positive culture (11).

Oval canals are one of the challenges during chemo-mechanical preparation, this was confirmed by Wu et al as they showed in their study a 42% unprepared canal walls after an even circumferential hand filing, this mechanical filling was only able to remove the inner layer of dentin from 58% of the circumference of the canal wall (12).

These studies clearly showed us the importance of irrigation along with the instrumentation. There is no doubt that mechanical instrumentation is not enough to disinfect the root canal system, yet, it plays an important part in bacterial reduction in infected root canal systems.

Different mechanical instrumentation techniques were developed from using ISO standardized 0.02 tapered stainless steel hand files to the engine-driven instrumentation since the introduction of NiTi instruments in 1988 (13). As previously mentioned, Mechanical instrumentation creates a path for the disinfectant solution to reach most of the enclosed infected parts of the root canals (14) and work towards shaping the canal and facilitate the placement of a biocompatible root filling material (5).

Mechanical instrumentation by itself is limited at completely eliminating residual bacteria and necrotic debris (10). According to Bystrom et al, mechanical

instrumentation eliminates bacteria in only 20-30% of cases (10,15). Peters et al confirmed these findings by using an advance technology, micro computed tomography (micro-ct). According to their findings, they reported that mechanical instrumentation left 35% or more of the canal surfaces untouched (16).

Classically, Mizrahi et al performed a scanning electron microscope (SEM) study using different instrumentation technique on 30 teeth and they found that one half of the root canal is most often better instrumented than the other half and no instrumentation technique were able to remove all the debris (17).

The root canal system consists of lateral and accessory canals, isthmuses, fins and other anatomical complexities that add significant limitations to complete elimination of debris from root canal system (18-20). Peters et al showed high percentage of root canal walls that were untouched with the current instrumentation technique (21).

Another classical study has shown that root canals morphology is very complex and that mechanically prepared canals contains areas not accessible by endodontic instruments (22). With that said, to achieve an enhanced disinfection of the root canal system, the mechanical instrumentation should be used in conjugations with an effective antimicrobial irrigant (23).

Chemo-mechanical preparation does not effectively debride the entire root canal system. These irrigation methods are effective and helpful in cleaning root canals coronally but show limitation at the apical part. To be effective, endodontic irrigants should ideally be delivered at 1-3 mm from the working length (24,25).

1.2 Dentin:

Dentin is a complex structure composed of odontoblast, odontoblastic processes, dentin tubules, non-collagenous proteins, and mineralized collagen forming the main dentinal corps. Dentin is classified into 3 types: Primary, secondary, and tertiary. Only primary and secondary dentin forms the dentin tissue of the normal non-carious teeth. Dentin tubules enclose and protect odontoblastic processes from environmental harmful stimuli. Odontoplastic process secretes the proteic matrix formed by collagen and non-collagen proteins (26,27).

Dentin is composed of nearly 22% hydrated organic matrix by weight. It is similar in composition to bone. Dentin has mainly Type-I collagen fibrils and reinforcing phase of nanocrystalline apatite mineral that contributes to its mechanical properties (28,29). Type I collagen is secreted by odontoblast into predentin at the proximal portion of the odontoblastic process. These process located within dentin tubule and secrets the dentin proteic and nonproteic components responsible for the dentinal biomineralization process (30).

Dentinal tubules, are microscopic channels which have a diameter of 2.5 μ m close to the pulp and extend to the outer surface of cementum or enamel with a diameter of 0.9 μ m at the dentino-enamel junction (31,32). The number of dentin tubules range between 18,000-21,000 per mm² (33). Dentin consists of about 70% inorganic materials mainly hydroxyapatite, 20% organic materials mainly type I collagen and 10% water.

There are three types of dentin present; **Primary dentin:** this type of dentin usually located between enamel and pulp chamber. During odontogenesis, odontoblasts play an important role in the formation of primary dentin until the tooth becomes functional. The outer layer closest to enamel is called **mantle dentin**, this is an atubular layer with thin and curved tubules. The diameter of this layer is between 15-30 mm thick and it is less mineralized. **Predentin** is the newly secreted unmineralized dentin which is between 10-47 micrometer and it is similar to the osteoid in bone.

Secondary dentin: this type of dentin form after the completion of root formation which is usually after the establishment of contacts between antagonistic cusps and will continues throughout life. This dentin is responsible for the shrinkage in the size of pulp chamber with patient age. The S-curve patter of the tubules looks more accentuated in this dentin due to space restriction.

Tertiary dentin: this type of dentin forms as a respond to an external stimulation such as decay or abrasion. It is either a reactionary type from a preexisting odontoblast or reparative from newly differentiated odontoblast like cell. deposition of tertiary dentin can occur rapidly depending on the duration and intensity of the stimuli, which will usually result in irregular tubular configuration (32,34,35).

1.3 Smear layer:

A surface film of debris retained on dentin and other surfaces after instrumentation with either engine driven or hand endodontic files; consists of dentin particles, remnants of vital or necrotic pulp tissue, bacterial components and retained irrigant (36). Smear layer is not observed on un-instrumented surfaces and it is usually occluding the dentinal tubules orifices (37).

Lester and Boyde in 1963 described the smear layer as "organic matter trapped within translocated inorganic dentin" (38). Eick et al performed a Scanning Electron Microscope Study (SEM) study to examine the cut tooth surfaces, the results showed non homogenous debris particles with a size range between 0.5-0.15 μ m (39). Another study showed a similar thin layer of debris that was 2 to 5 micrometers in thickness (40). McComb and Smith were the first to mention this layer in instrumented root canals. They concluded that the smear layer consists of dentin particles, remnants of vital or necrotic pulp tissue and bacterial remnant (organic and inorganic component) (41).

Smear layer has two main components, the **organic component** which is formed by vital or necrotic tissue, bacteria, blood cells, dentin collagen fibers and odontoblastic processes and **inorganic component** which is formed by hard tissue particles of the tooth composed of hydroxyapatite that were loosened during the instrumentation process (42).

In a SEM study to examine the morphological characteristics of the smear layer in teeth that were instrumented with K-type files and irrigated with 5.25%

solution of NaOCI, two confluent components were recognized: the smear layer on the canal wall surface which was about 1 to 2 μ m in thickness and the smeared material in the dentinal tubules which was packed into some of the tubules for a distance up to 40 μ m. This smeared layer has not been found on the uninstrumented walls and these findings strongly suggest that this layer results directly from instruments used to prepare the root canal walls. This layer appears to be friable and only loosely adherent (42).

The smear layer might harbor microorganisms, infect dentinal tubules, impede penetration or diffusion of antibacterial irrigants and medications into the dentinal tubules (43-48), as well as compromise the seal between the filling materials and dentinal wall (38,42,49-54). The smear layer also increases the micro leakage after canal obturation and interferes with the apical seal (55). In a study to examine the effect of the smear layer on the penetration depth of three different sealers (AH Plus, Apexit, and a Grossman Type-Roth 811) into the dentinal tubules. The smear layer prevented all the sealers from penetrating dentinal tubules & adversely affected the coronal and apical sealing ability of sealers (56). Another research study also confirmed the importance of removal of the smear layer and to establish a patent dental tubule for minimizing the time required to achieve the disinfecting effect of intracanal medications (7).

On the other hand, there are few studies that supported the concept of not removing the smear layer (57-59). During restorative procedures, the formation of the smear layer on dentin will form a protective diffusion barrier preventing the bacteria from entering the dentinal tubules. The permeability of the dentin will

increase by the removal of the smear layer with the acid etch (57). It has been well documented that the removal of the smear layer also facilitates the passive penetration of bacteria into the dentinal tubules (58). Furthermore, Love et al investigated in a study the penetration of Streptococcus gordonii into smeared and non-smeared dentin. This study has shown that smear layer is an effective barrier on the dentinal tubules as the non-smeared sample showed total bacterial penetration (59).

1.4 Biofilm:

Biofilm is the colonization and organization of microorganism at a surface and solution interface (36). It possesses the ability to self-organize (autopoiesis), withstand environmental perturbations (homeostasis), must be more effective in association than in isolation (synergy), and respond to environmental changes as a unit rather than a single individuals (community) (60,61). Biofilm major components are: Bacterial cells, solid surface, and a fluid medium. Bacteria has the ability to form biofilm on any surface that has nutrient containing fluid (62,63). Floating bacteria (planktonic microorganisms) which are in suspended form and are commonly seen within or outside the biofilm, are prerequisite for a biofilm formation (64). Approximately, 85% of the biofilm matrix material consist of protein, polysaccharides, nucleic acids, and salt. The other 15% is made up of microbial cells (65). Bacteria in biofilm are protected from host defenses and antimicrobial agents by a special mechanism that is dissimilar than the "classic" genetic mechanism (gene mutation or genetic exchange). This mechanism is determined by some peculiarity of biofilm growth (66,67).

The different biofilm associated resistance mechanism can be summarized by: restricted penetration, antimicrobial destroying enzymes and gene transfer, quorum sensing, altered growth rate, Stress response to hostile environmental conditions leading to an overexpression of antimicrobial agent destroying enzymes and Intracellular biofilm (66-72).

Endodontic bacterial biofilms are classified as (73):

- Intracanal biofilms
- Extraradicular biofilms
- Periapical biofilms
- Biomaterial-centered infections

Intracanal biofilm: These are microbial biofilm formed on the root canal dentin of infected tooth. First identification of this type biofilm was reported by Nair under transmission electron microscopy (TEM) (74). The majority of these organism were loose collections of cocci, rods, filaments and spirochetes apart from these bacterial condensations were seen as palisade structure similar to dental plague on tooth surface (75). A SEM study by Sen et al showed that the bacteria formed dense colonies on the canal walls and in inter/intra tubular dentin as well. They also reported fungi forming dense but separate colonies on the canal walls (76).

Extraradicular biofilm: These are root surface biofilms formed adjacent to the root apex of endodontically infected teeth (77). Tronstad et al have shown in a research study on refractory endodontic cases, a smooth and structureless biofilm with a variety of bacterial forms (cocci, rods with presence of some fibrillary form) at the tip of the roots next to the apical foramen (78). Others, also reported a multilayered bacteria embedded in a heavy extracellular matrix in teeth with chronic apical periodontitis (79).

Ricucci et al reported two cases of unhealing fistula after conventional root canal treatment. In one of the cases the fistula did not heal even after an apical surgery. Histology of the apical biopsy revealed a calculus-like material on the external surface of the root apex after post treatment periapical periodontitis. They related the cause for the failure to the biofilm formation on these root surfaces. (80).

Using polymerase chain reaction (PCR)-based 16s RNA gene assay, Conrads showed F. nucleatum, Po. Gingivalis and Tannerella forsythensis to be associated with extraradicular biofilm (81).

Periapical biofilm: It is an isolated biofilm seen in the periapical region of endodontically infected teeth. This type of biofilm may or may not be dependent on the root canal infection (73). The bacteria in this biofilm have the ability to resist host defense and cause periapical lesions (82).

Actinomyces species and Propionibacterium propionicum have been seen in asymptomatic periapical lesions refractory to endodontic treatment (83). Sulphur granules have seen in these species which appear as ray fungus microscopically. (84).

Foreign body centered biofilm: It is usually found when bacteria adhere to both an artificial biomaterial surface and from biofilm structures which is also known as biomaterial-centered infection (85). It is a major complication associated with prosthesis and in implant supported prosthesis. Takemura et al showed that gram positive facultative anaerobes have the ability to colonize and produce extracellular polymeric matrix surrounding the gutta-percha points, while serum plays a crucial role in biofilm formation (86).

1.5 Irrigation solutions:

1.5.1 Sodium Hypochlorite (NaOCl):

Sodium Hypochlorite has a long history in medicine and dentistry. During World War I, chemist Henry Drysdale Dakin and surgeon Alexis Carrel utilized the buffered 0.5% NaOCI solution as antiseptic substance in the treatment of infected wounds (87).

Austin et al showed in their study that the chlorine concentration in Dakin's hypochlorite solution dropped quickly when the solution contacts necrotic tissues compared to the normal tissues. This fall in chlorine concentration will be

completed when the necrotic tissues particles are completely dissolved. Hypochlorite solution has an excellent cleansing ability on necrotic tissues. It also shows a much more irritating effect on the rabbit skin than Chloramine-T solution or the alkaline control solution (88).

NaOCI has many desirable features, its antimicrobial characteristics (89,90-93), its excellent ability to dissolve organic tissues (94-98) and its capability to denature endotoxins (99). Besides that, NaOCI solution is inexpensive, has a decent shelf life and it is easily available (100).

NaOCI display a dynamic balance as seen by the reaction:

 $NaOCI + H2O \leftrightarrow NaOH + HOCI \leftrightarrow Na^{+} + OH^{-} + H^{+} + OCI^{-}$

NaOCI dissolve organic and fat components, it reduces the surface tension of the solution by degrading fatty acids and transforming them into fatty acids salts (soap) and glycerol (alcohol) (101). It also neutralizes amino acids forming water and salt (neutralization reaction). There is a reduction of pH with the exit of hydroxyl ions (101).

NaOCI contains hypochlorous acid. When this substance comes in contact with organic tissues, it acts as a solvent and release chlorine, which combines with the protein amino group to form chloramines (chloramination reaction) which interfere with the cell metabolism. Hypochlorous acid and hypochlorite ions cause amino acid degradation and hydrolysis (101). Chlorine (a strong oxidant) causes an irreversible oxidation of essential bacterial enzymes (cysteine) which produces an antimicrobial effect by inhibiting these enzymes (101-103).

Thus, the saponification, the neutralization of the amino acid, and chloramination reactions that occurs in the presence of microorganism and organic tissues produce the antimicrobial effect and cause tissue dissolution (101). Sodium hypochlorite is a strong base (pH > 11), the high pH value makes NaOCI a strong antimicrobial agent and similar to the mechanism of action of calcium hydroxide (104).

The effect of antimicrobial agents on biofilm results in different outcomes. Enumeration of the different effects on bacterial biofilms reveals that the possible outcomes are: complete dissolution of cells, bacterial cell disruption and separation from the biofilm (105).

Free floating bacteria presenting in an aqueous environment, so called planktonic microorganism, are prerequisite for biofilm formation (64). Microbial communities in biofilms are difficult to eradicate and resistant to the anti-microbial agents. Reports show this resistant could be 2-1,000 fold more than the corresponding planktonic form (106).

An in vitro evaluation of 2.25% NaOCI, 0.2% Chlorhexidine (CHX), 10% iodine, 5ppm colloidal silver and phosphate buffered saline (PBS) as control against biofilms of Prevotella intermedia, Peptostreptococcus micros, Streptococcus intermedius, Fusobacterium nucleatum and Enterococcus faecalis. The incubation period with these agents were 15 min to 1h, the results showed that NaOCI was the most effective agent followed by iodine and none of the agents were effective against F. nucleatum after 15 min (107).

According to Cvek et al and Bystrom & Sundqvist, NaOCI at 0.5% or 5% concentration has similar clinical efficiency in mechanical debridement of the root canal (108,109). Other studies also showed a 0.5%-1% concentration with neutral pH has an optimal antimicrobial effectiveness with minimal tissue irritating effect (110,111).

Microorganism communities in biofilm could be 1000-1500 times more resistant to antimicrobial agents (112). The biofilm community provides protection and resistant to these bacterial colonies against disinfecting agents.

In a different in vitro study, the effectiveness of 1%,3% and 6% NaOCI, 2% CHX and BioPure MTAD were tested on apical dentin biofilms. The intracanal contents were collected from patients diagnosed with chronic apical periodontitis. The results indicated that 6% NaOCI was the only irrigant capable of both rendering bacteria nonviable and physically removing the biofilm (113).

The effect of different concentrations of NaOCI on the growth and susceptibility of mono and dual-species biofilms of Fusobacterium nucleatum or Peptostreptococcus micros in vitro at 24 h or 96 h were compared by Ozok et al Their results showed that even though a 24 h dual-species biofilms had similar viable counts to those of mono-species biofilms, they still showed more resistance to NaOCI. Dual-species biofilms were more resistant and had more viable counts than monospecies biofilms at 96h. The resistance to NaOCI increased as the age of biofilms increased. Biofilms mixed species of F. nucleatum and P. micros showed a time-dependent synergy in growth and resistance to NaOCI (114).

The antimicrobial efficacy of 5.25% NaOCI, BioPure MTAD and Tetraclean (Ogna Laboratori Farmaceutici, Milano, Italy) against E. faecalis biofilms generated on cellulose nitrate membrane filters were compared by Giardino et al Only 5.25% NaOCI was effective in removing the biofilm on the surface of the membrane (115). A different study compared the effectiveness of 6% NaOCI, 1% NaOCI, smear clear [™], 2% CHX and BioPure[™] MTAD[™]. The results showed significant difference between 1% and 6% NaOCI and the other agents. 1% and 6% NaOCI were found to be more efficient against E. faecalis biofilm (91).

Sodium hypochlorite fragments long peptide chains and chlorinates protein terminal groups (116). Marending et al. showed that NaOCI caused a concentration-dependent reduction of elastic modulus and flexural strength in human root dentin which affected the mechanical properties of dentin. Also, the reduction of carbon and nitrogen was related to the hypochlorite concentration. NaOCI also altered intertubular dentine permeable to basic fuchsindye, although no effect of hypochlorite on inorganic dentin components under Scanning Electron Microscope. They also reported under SEM 3D reconstructions of exposed dentin surface a severely altered peripheral dentin matrix when exposed to 5% NaOCI (117). Sim et al. showed a reduction in the dentin flexural strength and elastic modulus when exposed to 5.25% NaOCI compared to saline solution (118).

Another study tested the effect of irrigating with 2.5% and 6% NaOCI for 5,10 or 20 min on root dentin microhardness. There was a significant difference in groups irrigated for 10 or 20 min and because of this effect, they recommended to limit the irrigation time to a period less than 10 min so not to weaken the tooth.

They also found that at a depth of 500 μ m from lumen, 6% NaOCI has more effect on dentin microhardness than 2.5%, therefore, it is recommended not to use higher concentrations of NaOCI to preserve the physical properties of dentin (119).

Mountouris et al used both reflectance FTIR microspectroscopy and tapping mode atomic force microscopy to evaluate the deproteination potential of 5% aqueous NaOCI solution on the molecular composition and morphology of smear layer. The results showed that NaOCI reduced organic matrix (amid I, II, III peaks) but did not affect carbonates and phosphates. (120).

Another study treated the radicular segments from human teeth with 5% NaOCI for 2 min, control group was treated with distilled water. The specimens were processed for indirect immunofluorescence by using antitype I collagen and antichondroitin sulfate antibodies. The exposure to 5% NaOCI produced a drastic loss of immunoreactivity in the dentin surface with alteration in dentin collagen and glycosaminoglycans. It also showed the protective role of hydroxyapatite on organic matrix stability (121).

Saleh et al showed that irrigating the canal with 3% H₂O₂ / 5% NaOCI and 17% EDTA solutions significantly reduced the microhardness of root canal dentin. According to da Cunha et al. 10 min deproteination with 5% NaOCI reduced the push-out bond strength between dentin surfaces and fiber posts cemented (122). Sodium hypochlorite degenerate dentin by dissolution of dentinal collagen. The residual NaOCI may interfere with polymerization of the bonding resin due to oxygen generation. (123). A different study tested the effect of 10% NaOCI on the shear bond strength of different adhesive systems. The increase in the NaOCI

application time resulted in a progressive decrease in shear bond strengths for both dentin adhesives with the integrity of the collagen fibrils left exposed upon acid-etching which play a major role in the adhesive system (124).

Dentine bond strength and marginal adaptation of direct composite decrease significantly after NaOCI application by (-25%) and (-30%) respectively (125). Another study showed that after 24 months, the retention rates for Prime & Bond 2.1 system with and without 10% NaOCI pre-treatment were 80% and 63% respectively. No significant differences were found at any time between groups for retention or marginal staining (126).

Different study used SEM and CLSM-visualization of the dentin-composite interface and for bond strength measurements. The results showed that the removal of the collagen layer with 10% NaOCI can enhance or decrease bond strength depending on the bonding agent used (127).

The microtensile bond strength of four adhesive systems to root dentin with or without 5% NaOCI was tested in another study. Statistically significant differences were found among the NaOCI treated and non-treated groups. The 5% NaOCI reduced the bond strengths to dentin in almost all resin cements by 18% (128). In addition to that, Morris et al reported that 15-20 min of 5% NaOCI treatment reduced bond strength of C&B Metabond to root canal dentin by 67% (129). Same effect was also reported by Erdemir et al (130). On the other hand, Correr et al, showed that dentin surface treated with 10% NaOCI did not affect the resin-dentin bonding strength in primary teeth (131).

Potent anti-oxidants agents such as ascorbic acid or sodium ascorbate have been shown to completely reverse the reduction in bond strength. (132,133).

Preheating NaOCI solutions appears to improve its necrotic pulp tissue dissolution capacity and efficacy. A rise in temperature by 25°C increased NaOCI efficacy by a factor of 100. The 1% NaOCI solution at 45°C dissolve pulp tissues as effectively as the 5.25% solution at 20°C (134). Cunningham et al reported that 2.6% NaOCI solution at a temperature of 37° C. was equally effective as collagen dissolving agent when compared to 5.2% NaOCI at either 21°C. or 37°C. They also showed that warming of NaOCI solution to 37°C produced a 4% and 9.5% reduction in the chlorine availability for the 2.5% and 5% solutions respectively after 24h (135). Another study tested the 2.6% and 5.25% concentration of NaOCI against rat connective tissue specimens. The results showed that regardless of the concentration, NaOCI heated to 140F was more effective than the same solution at 73.2F. Furthermore. 5.25% concentration was more effective than those at 2.6% at either temperature (136).

The dilution of NaOCI significantly reduces its necrotic tissue dissolution ability. Same study also reported that 5.25% NaOCI was the most effective antibacterial concentration and dilution of this concentration to 0.5% and 1% rendered NaOCI ineffective as necrotic tissue solvents (137). McComb and Smith evaluated the debridement property of 6% NaOCI and 1%. They concluded that during chemomechanical preparation, the 1% concentration was not as effective as the 6% in producing clean canals (37).

When NaOCI is added to the water, it undergoes the following reaction:

NaOCI + $H_2O \rightarrow NaOH + HOCI$ (hypochlorous acid) (1)

In aqueous solution, hypochlorous acid partially dissociates into the anion hypochlorite (OCI⁻):

HOCI $\leftarrow \rightarrow$ H⁺ + OCI ⁻ (2)

The available chlorine is the sum of the HOCI⁺ and OCI⁻ concentration in the solution (138).

In equation #2, hypochlorous acid dissociation depends on pH, as HOCI is consumed through its germicidal function, the clinical equilibrium between HOCI and OCI⁻ is maintained (108). According to Baker et al, at pH 10, all chlorine is in the OCI⁻ form, at 4.5 pH, where all chlorine is in the form of HOCI, the reverse occurs. With higher pH, the disinfecting properties decrease (139).

Bloomfield and Miles confirmed that hypochlorite at lower pH has greater antimicrobial activity (138). The availability of chlorine is dependent on the pH of the solution. Above pH of 7.6, the main form is hypochlorite and below this value is hypochlorous acid (140).

Another in-vitro study evaluated the effectiveness of different NaOCI concentration (1%, 2.5% and 5.25%) against E. faecalis. No significant difference between the three concentrations was found as all of these concentrations showed large zone of inhibition against E. faecalis. The study suggested that the use of large amount of irrigant compensated for the effect of concentration (141).

The antimicrobial efficacy of NaOCI is mainly due to its ability to oxidize and hydrolyse cell protein and to some extent, osmotically draw fluids out of cells due to its hypertonicity (142). At high concentration, NaOCI is very toxic and tends to induce tissue irritation on contact (110). In addition to that, NaOCI is a very alkaline solution with a pH of approximately 11-12. This makes the solution very hypertonic (~2800 mOsmol/kg) (142). When NaOCI contacts tissue protein, nitrogen, formaldehyde and acetaldehyde are formed within a short time and the peptide link are broken resulting in dissolution of proteins (110).

Sudden onset of pain is a landmark of tissue damage and may happen immediately or be delayed for couple of minutes or even hours (143). Involvement of the maxillary sinus will cause an acute sinusitis (144). bruising and ecchymosis of the surrounding mucosa and possibly the facial skin can also result due to bleeding into the interstitial tissues which may also include the formation of a hematoma (145,146).

Basically, NaOCI is cytotoxic to all cells except heavily keratinized epithelia. Pashley et al showed in their study that dilution as low as 1:1000 caused complete hemolysis of RBC's in vitro. Undiluted and 1:10 dilutions produced moderate to severe irritation to rabbit eyes which healed after 24 to 48 h. intradermal injections of undiluted 1:1, 1:2, and 1:4 dilutions of NaOCI produced skin ulceration (142).

A study was conducted to investigate different concentrations of NaOCI for antibacterial activity and tissue toxicity at 5,10,15, and 30 min. Concentration of NaOCI were 0.25%, 0.025% and 0.0125%. The results showed that a bactericidal effect were observed for concentrations as low as 0.025%. Tissue toxicity was

observed at concentration of 0.25%. Therefore, the 0.025% concentration preserves bactericidal properties and eliminates the harmful effect on wound healing (147). A different study by Becker et al. reported extreme pain, hematoma and ecchymosis with profuse hemorrhage when 5.25% NaOCI was forced beyond the apex of maxillary cuspid. Applying wet compresses to the face helped in reducing the burning sensation and relieved the pain. The patient was given antibiotics and analgesic and the tooth left open for drainage. There was an increase in the swelling during the next few days but the pain had subsided. Patient face had returned to normal after one month (148).

It is recommended that the clinician should look both clinically and radiographically for immature apices, resorption, apical perforation or any other conditions that result in irrigant extrusion beyond root canal to the surrounding tissues. Irrigation should be performed slowly and under gentle movement of the needle to prevent the binding of the needle into the canal wall (149). It was also recommended to keep a reservoir from the irrigant solution in the coronal chamber and to carry it into the canal during filling preparation to minimize the risk of extruding the irrigant beyond the root apex (110,150).

1.5.2 EDTA:

Ethylenediaminetetraacetic acid (EDTA) is a chelating agent with chemical formula $(HO_2CCH_2)_2NCH_2CH_2N(CH_2CO_2H)_2$.

This compound was first introduced by Ferdinand Munz in 1935 as an alternative to citric acid to use with dye solutions in the textile industry. He prepared it from ethylene diamine and chloroacetic acid (93).

Nygaard-Ostby in 1957 were the first to introduce EDTA to dentistry as an aid for the preparation of narrow and calcified root canals. EDTA is a polyprotic acid whose sodium salts are noncolloidal organic agents that can form nonionic chelates with metallic ions (94,95). It is usually used in a concentration between 10% and 17%, and to increase its chelating effectiveness, its pH was modified from 4 to a value between 7 and 8 (94-96).

One of the main inorganic components of the dentin is the calcium ion present in hydroxyapatite crystals. Any irrigant that will alter the calcium ion will affect the chemical composition of the dentin which in turn affect the permeability, microhardness and solubility of the dentin (151-153).

EDTA has a self-limiting property. This explain why its chelating action stopped once it reached equilibrium with calcium ions (97). Like other chelators, EDTA prompts the uptake of positive ions and will react with calcium ions in the hydroxyl apatite crystals, this reaction will change the microstructure of the dentin and soften it by changing the calcium-phosphorus ratio. These changes in the Ca-P ratio will affect the permeability and the hardness of the dentin and reduce the
torsional stress on the engine driven or rotary files that have been used for instrumentation (154).

The antibacterial property of EDTA is relatively limited (155), and its cleaning ability is mainly due to its ability to work as a chelator and detach the biofilm that adhere to the canal walls (94). Yoshida el al conducted a study on infected teeth and showed when 15% EDTA was used as a root canal irrigant with ultrasonic agitation, no bacteria could recover from 93 out of 129 root (156).

The biocompatibility of EDTA was also tested by Nygaard-Ostby, by evaluating the effect of forcing 15% EDTA into the periapical tissues of vital and necrotic teeth for up to 14 months, no tissue damage was detected. In addition to that, no pulpal necrosis was detected when EDTA was placed for up to 28 days after pulpotomy therapy (97).

The ability of EDTA to demineralize the dentin is due to its reaction with calcium ions in the hydroxyapatite crystals and forms soluble calcium chelates (97). EDTA also has the ability to decalcify dentin to a depth of 20-30 μ m in five min (98). According to Calt et al, EDTA has the ability to remove the inorganic components of smear layer in less than 1 minute if its solution is able to reach to the surface of the root canal wall. Goldman et al. found that the smeared layer is mainly calcific in nature, and only chelating agents such as EDTA or citric acid can remove this layer (99). NaOCI by itself cannot remove the smear layer (37,44,157,158).

A SEM study was conducted to assess the final flush with different root canal irrigating solutions and showed that the combined use of 10 ml from 17%

EDTA solution buffered to pH 7.7 followed by 10 ml of 5.25% NaOCI solution was the most effective method in removing both superficial debris and smear layer components, and with this approach, the gold standard in the irrigation protocol was demonstrated (44).

Another study found that irrigating the canals walls with 17% EDTA and 6% NaOCI for 1 min is more effective in removing the smear layer than the 15 or 30 seconds groups (159). In addition to that, the use of an activation method (automated-dynamic activation with RinsEndo or the sonic-activation group with Endo-activator) with 17% EDTA and 3% NaOCI, were significantly better in removing the smear layer in the apical third than other groups (160).

Many studies were conducted to test the effect of EDTA and other chelating agents on the micohardness of the dentin (161-164). Cruz-Filho et al compared the effect of (15% EDTA, 10% citric acid, 5% malic acid, 10% sodium citrate, apple vinegar) on dentin lumen. EDTA and citric acid groups showed a sharp decrease in dentin microhardness compared to other group without a significant difference between each other (161).

Sayin et al conducted another study to evaluate the effect of single and combined use of EDTA with other agents on the micro-hardness of the dentin. Their results showed that the single and combined use of EDTA with 2.5% NaOCI significantly decreased the micro-hardness of the dentin. There is also a significant decrease only for EDTA and EDTA + NaOCI in the coronal region and for EDTAC and EDTAC + NaOCI in the apical and middle regions of the root canal (162). On the other hand, no significant difference was found between 17% EDTA and 7%

maleic acid in the reduction of microhardness but maleic acid significantly increased the surface roughness more than EDTA (163).

The effect of increasing the time of application of 17% EDTA, 17% EDTAC and 10% citric acid was also tested. No significant differences between initial microhardness after 1 min of application, however, EDTA produced a significantly greater reduction in microhardness after 3 min. EDTA and EDTAC showed no significant difference after 5 min while citric acid group showed less reduction (164).

Different studies have shown the antagonistic interactions occurring when NaOCI was used together with chelators. This interaction will cause a loss in the free available chlorine for NaOCI which consequently reduces the tissue dissolution ability of the NaOCI and its antimicrobial activities to a lesser extent (165,166).

A study by Baumgartner et al was conducted to measure the amount of chlorine gas that was evolved when 5.25% NAOCL was mixed with other irrigants. The study related the release of chlorine gas to the reduction of the PH values in the NaOCI solution. This chlorine gas was evolved significantly more when NaOCI was mixed with 50% citric acid than with 17% EDTA (167).

Both EDTA and citric acid strongly reduce the available chlorine in NaOCI solution which will result in a reduction in the effectiveness of the NaOCI and rendering the solution ineffective. (95,167). Zehnder et al tested the interaction of 17% EDTA with pH 8, 10% citric acid (CA), and other alternative chelators: 9% sodium triphosphate (STP), 15% amino tris methylenephosphonic acid (ATMA)

and 7% 1- hydroxyethylidene-1, 1-bisphosphonate (HEBP) with NaOCI. STP solution did not interact with NaOCI and showed 100% of free available chlorine, HEBP solution showed some reduction in the available chlorine, was dose dependent and continued over time. EDTA and ATMA groups caused an almost complete loss of chlorine and this effect was even more clear with CA group which showed a zero chlorine content in less than one min (168).

It has been shown in multiple studies that NaOCI does not really affect the chelating ability of the EDTA. Others, report a decrease in the tissue dissolving ability and the antimicrobial property of NaOCI when mixed with different chelators. (95,96,168).

1.6 Activation methods:

The root canal system has a very complex and irregular anatomy that mechanically instrumented canals harbor areas not attainable by currently utilized endodontic instruments (22).

According to Wu et al., in the apical areas of the oval canals, only 40% of the canal walls can be touched by the rotary instruments as both the balanced force (removed only 38.6% from inner layer of dentin) and circumferential filling (removed 57.7%) left large portions of the canal walls un-instrumented (12). Many studies showed that the canal fins, cul-de-sacs and isthmi all left untouched after instrumentation with nickel-titanium instruments, they also showed that these instruments work mainly on the central body of the canal (21,20,169,170).

Irrigation is an important part in root canal debridement however, there is no ideal irrigant which will combine all the ideal characteristics, even when its altered by changing the pH value (171,172), increasing the temperature (134,173,178), or increasing the wetting ability by adding a surfactant (174,175). Throughout the history of endodontics, many efforts have been made to develop more effective irrigant delivery and agitation systems and to improve root canal cleaning. These systems mainly divided into two broad categories: manual and machine assisted agitation devices (175).

Manual agitation technique (passive irrigation) involves the use of needles of different gauges and different designs (some are designs to dispense the irrigant through the most distal end, others have closed-ended tip that deliver the irrigant

laterally or side-vented channels.), to deliver the irrigant inside the canal. This can be done either passively or with agitation by moving the needle up and down (176). To reduce the chance of apical extrusion of the irrigant, the needle should remain loose inside the canal. The use of this technique will allow an easy control for the volume of the irrigant and the depth of the needle within the canal (175,177).

One of the critical factors that affect the efficiency of the manual irrigation is the depth of the needle. Grossman showed the importance of the adequate enlargement of the root canal to improve the irrigation efficiency. it was also reported that the irrigation with size 28G safety-ended needle will be less effective when the canal is enlarged to a size less than 40 at the apex (1,179,180).

The efficacy of the apical irrigation is directly proportional to the depth of the insertion of the needle (181). In order to allow the irrigant to reflux and move the debris coronally, the needle should fit loose in the canal. smaller gauged needle is recommended to establish deeper and more effective placement (182).

On the other hand, manual dynamic irrigation can be done by gently moving up and down a well-fitting gutta percha master cone in short 2-3 mm strokes. It has an effective hydrodynamic effect and improve the exchange of the irrigant (183-185).

McGill et al did a study to compare the efficacy of (static, manual-dynamic and automated-dynamic "RinsEndo"). The results showed that the automateddynamic technique was significantly better (16%) than static irrigation but significantly showed lower value (5%) than manual-dynamic irrigation. When the

needle was placed closer to working length, the effectiveness of the irrigation increased by 7% (186).

Many factors could have affected the positive results of manual-dynamic irrigation: a- the push-pull action of a good-fitting gutta-percha cone in the canal may produce higher intra-canal pressure alteration similar to what a drain plunger does during the pushing action, resulting to a more efficient delivery of the irrigant to the untouched canal walls; b- the frequency of push-pull action of the gutta-percha point (33 Hz - 100 strokes per 30 seconds) is more than the frequency (1.6 Hz) of positive-negative hydrodynamic pressure produced by RinsEndo, possibly creating more turbulence inside the canal; and c- the push-pull action of the gutta-percha cone probably works by physically folding and dislodging the fluid under "viscously-dominated flow" (187) in the canal, which may allow a more efficient mixing of new unreacted solution with the spent, reacted molecules of the active NaOCl irrigant (186).

Ruddle demonstrated a machine-assisted type of agitation system by using a rotary handpiece-attached microbrush to remove debris from instrumented root canals. The microbrush rotates at 300rpm, causing the bristles to deform into the irregularities of the preparation, this action will displace the debris outside the canal. this device has not been commercially available since the patent was approved in 2001 (175,188). CanalBrush (Coltene Whaledent, Langenau, Germany) has recently made it commercially available. This highly flexible endodontic microbrush can be used manually with rotary action. However, when attached to a contra-angle handpiece running at 600 rpm, it becomes more

efficacious (175). Weise et al. reported an effective method of removing the debris from simulated canal extension and irregularities by using a flexible and small CanalBrush (189).

Tronstad et al in 1985, were the first to introduce the sonic instrument for endodontics use by using an air-driven sonic vibratory handpiece to which specially designed K-type files are attached. When activated, the instruments will vibrate in a whirling motion, and will graze the root canal wall when moved up and down (190).

Sonic instruments use a lower frequency (1000-6000 Hz) compared to ultrasonic instruments (25000 Hz) and produces smaller shear stresses (191). The vibration pattern of ultrasonic files is different from that of sonic instruments. Sonic files have a single node near the attachment of the file and one antinode at the tip of the instrument whereas ultrasonic activated files have numerous nodes and antinodes across the length of the instrument (192,193). In addition to that, the amplitude or the back and forth tip movement is significantly higher and greater with sonic energy (175).

Sonic endodontic instrument produces a large elliptical oscillation when operated in air, when the sonic file was loaded, the elliptical motion was eliminated leaving a pure longitudinal file oscillation. This oscillatory pattern of the sonic file may offer a useful mode of mechanically assisted root canal debridement as it is largely unaffected by loading and retains a large displacement amplitude (185). According to Sabins et al, passive sonic or ultrasonic irrigation for 30 sec resulted in significantly cleaner canals than hand filing alone. They also showed that

ultrasonically irrigated groups had significantly less debris at both 0-3 mm and 3-6 mm levels than the sonically irrigated group (194).

The EndoActivator system (Dentsply-Sirona, USA) is a sonically driven canal irrigation system with sonic vibration (up to 10,000 cpm). This batteryoperated system comprised of a sonic handpiece and variously sized polymer tips (195). Due to the smooth structure and the flexible composition of these tips, their cutting efficiency into the dentin is very limited. A possible disadvantage to these tips is that they are radiolucent which will be difficult to identify if part of the tip separates inside the canal. This can possibly be improved by adding some radiopacifier to these polymer tips (195).

The use of EndoActivator facilitates the removal of the debris from lateral canals, remove the smear layer when used with demineralizing agents like EDTA and dislodge clumps of simulated biofilm within the curved canals of molar teeth (184,196).

A cloud of debris can be seen within a fluid-filled pulp chamber when the tip of the EndoActivator is activated. The main function of the EndoActivator is to produce vigorous intracanal fluid agitation through acoustic streaming and cavitation (195). According to Guerisolo et al., this hydrodynamic activation improves the penetration, circulation and flow of irrigant into the more inaccessible regions of the root canal system (197).

According to Van der Sluis et al., EndoActivator is an effective system to remove Ca(OH)₂ from experimental grooves within a prepared canal (198).

Furthermore, this system can also be used to deliver MTA (Dentsply-Sirona) into immature teeth with blunderbuss canals, or into perforation defects (195).

The use of ultrasonic was first introduced into dentistry by Catuna for cavity preparations using an abrasive slurry (322). Zinner reported the use of an ultrasonic instrument to remove plaque and calculus deposits from the tooth surfaces.

In 1957, Richman was the first to introduce the concept of ultrasonic instrumentation to endodontics. Martin et al. introduced the use of ultrasonically activated K-type files to remove dentin in the preparation of root canals before obturation (199,200) and in 1980, ultrasonic unit was commercially available for endodontic application (201).

The term "**endosonic**" was introduced by Martin and Cunningham as an ultrasonic synergistic system which combine both instrumentation and canal disinfection (202).

Mechanical agitation or fluid flow is more important in the ability of NaOCI to dissolve tissue than the initial percentage of available chlorine (203). The introduction of ultrasonic vibration is directly associated with the cleaning effectiveness of the irrigant to the canal space (175).

Cesar de Gregorio et al showed that ultrasonic and sonic activation resulted in a more efficient irrigation to the lateral canals at 4.5 and 2 mm from working length and the addition of EDTA did not improve the penetration of the irrigants into the lateral canals (204).

It was demonstrated that passive ultrasonic irrigation with a nickel-titanium tip has superior necrotic tissue-dissolving ability over sonic irrgant activation while preserving the simulated canal anatomy (205).

Ultrasound is a sound energy with a frequency above the range of human hearing, which is 20 kHz (206). Low frequency ultrasonic handpieces (1-8 kHz) were developed to produce lower shear stresses which cause less alteration to the tooth surface (207-210).

Two main methods for production of ultrasonic wave were identified: the first is **magnetostriction** which converts the electromagnetic energy into mechanical energy. This method has elliptical movement and oscillate in figure-eight pattern which generate heat, thus, adequate cooling is necessary.

The second method is based on the piezoelectric principle, in which a crystal is used that changes dimension when an electrical charge is applied. The deformation of this crystal is converted into mechanical oscillation without producing heat (206,211-213). The tip of piezoelectric unit moves in a linear back and forth, piston-like motion which is ideal for Endodontics use. According to Lea et al, the position of nodes and antinodes of the endosonic file activated by a 30 kHz piezon generator was along the file length and does not increase linearly with increasing generator power. This is helpful in surgical Endodontics and when troughing to look for hidden canals or when removing separated instruments or posts (214,215).

Two types of ultrasonic irrigation have been described in the literature. The first one is incorporation of simultaneous ultrasonic instrumentation and irrigation (UI). The second type is the passive ultrasonic irrigation (PUI) (198).

Due to the difficulty of controlling the cut of dentin and the possibility of making aberrant conformation and alteration to the canal shape, the first type has less popularity in dental practice. Therefore, literatures supported the use of ultrasound for passive irrigation (216-219).

Weller et al. in 1980, was the first to use the term Passive Ultrasonic Irrigation (PUI) to describe a passive irrigation approach where there was no instrumentation, or contact of the canal walls with an Endodontic file or instrument "noncutting" action (175,219).

Passive Ultrasonic Irrigation depends on the transmission of acoustic energy by means of ultrasonic waves from an oscillating file or smooth wire to an irrigant in the root canal. This action can produce acoustic streaming and cavitation of the irrigant (191,209,220).

During PUI, two flushing methods might be used, a continuous flush of irrigant from the ultrasonic handpiece or an intermittent flush by using syring delivery which allow more control on the amount of irrigant flowing through the apical area of the canal (175,177).

Many studies have shown the effectiveness of PUI in removing remnants of pulp tissue and canal debris (221-224), with the ability to significantly reduce the amount of planktonic bacteria (225-227) and its superiority over syringe irrigation (226). Moorer & Wesselink showed the significant increase in tissue dissolving

ability of organic material by NaOCI when NaOCI is agitated by ultrasonic (203). Other studies also explained the enhancement in this effect due to the increase in NaOCI temperature by ultrasound effect (173,228,229).

Acoustic streaming is the rapid movement of fluid in a circular or vortex-like motion around a vibrating file. Acoustic microstreaming is the acoustic streaming inside the root canal during ultrasonic irrigation which usually occurs during PUI (207,209,211,230).

The tip of the file represents the maximum displacement amplitude, a reduction in this amplitude will occurs when the file touches the canal walls at an antinode compared with when it touches at a node (198,230). When the file is unable to vibrate freely, acoustic microstreaming will become less intense, however, it will not stop completely (198,209,230).

Pre-shaping the file in a curve canal will cause more powerful acoustic streaming (198,217,220). Studies have shown that the thinner the file, the higher the frequency, streaming velocity and the displacement amplitude of the file. This will also result in a stronger acoustic microstreaming (198). The shear flow produced by the acoustic microstreaming produces shear stresses along the canal wall, which can remove debris and bacteria from the canal (198,209). Jensen et al. recommended the use of a vibrating file with small size under high power setting to reduce the chances of the file to contact the canal walls (231).

Cavitation in a fluid can be described as the impulsive formation of cavities in a liquid through tensile forces induced by high speed flows or flow gradients.

This action will cause the bubbles to expand and then rapidly collapse producing a focus of energy (198).

Acoustic cavitation can be defined as the formation of new bubbles or the expansion, contraction and/or distortion of pre-existing bubbles, so called (nuclei) in a liquid, the process being coupled to acoustic energy (198,233).

According to Roy et al. two types of cavitation can occur during PUI: transient and stable. Transient cavitation occurs when the vapor bubbles undergo highly energetic pulsations and when the file can vibrate freely or slightly touches the canal wall. This type of cavitation was more visible at the end and along the length of the file. Also in their study, they reported that a smooth file with sharp edges and a square cross-section produced significantly more transient cavitation than a regular K-file (198,230).

Stable cavitation is a linear pulsation of gas-filled bodies in a low amplitude ultrasound field. When the file comes in contact with the canal wall, stable cavitation was affected less than transient cavitation and was seen at the midpoint of the file (198,230).

Air entrapment by an advancing liquid front in closed-end microchannel is a well-recognized physical phenomenon and has been referred to as vapor lock effect in the Endodontic literatures (234-236). The contact angle of the liquid and the depth and size of the channel will determine the ability of the liquid to penetrate through these closed-end channels. In Endodontics, root canal irrigation is usually performed within time frame of minutes, air entrapment in the apical area of the

root canal might prevent the irrigant from adequately contact and disinfect this area (175, 237, 238, 235).

Senia et al. showed that NaOCI did not reach any closer that 3 mm from working length even after enlarging the apical part of the root to a size 30. This can be related to the fact that NaOCI will quickly forms micro gas bubbles at the apical end of the root canal after reacting with the organic tissues inside the root. these gas bubbles coalesce into apical vapor lock with subsequent instrumentation (175,236).

This vapor lock will prevent any irrigants from reaching into the apical area. Acoustic microstreaming and cavitation can only occur in a liquid phase, therefore once the ultrasonically activated tip leaves the irrigant and goes inside the apical vapor lock, acoustic microstreaming/cavitation becomes impossible (175,239). Boutsioukis et al. suggested a brief insertion of the needle to working length whilst irrigating at a flow rate of 0.083 mL s⁻¹ and delivering irrigant at 0.260 MI s⁻¹ without moving the needle were capable of removing an established apical vapor lock (240).

Other studies suggested the use of a hand-activated well-fitting root filling material (eg, a size 40, 0.06 taper gutta-percha point) to working length after instrumentation with the corresponding rotary instrument. This simple method will help in eliminating the vapor lock at the space previously occupied by air and will be replaced by root filling material that will carry with it a film of irrigant to working length of the canal (175,241).

Vera et al suggested to maintain the apical patency of the root canal with a size #10 ISO file to improve the apical penetration of the irrigant and overcome the vapor lock effect, this approach can be achieved after preparing the canal with an apical diameter of greater than #30 0.06 file. The results of this approach did not significantly improve the apical penetration of the irigant (242,243).

The EndoVac system (Discus Dental, Culver City, CA, USA) is a new irrigation system based on a negative pressure approach. This system consists of master delivery tip, macro-cannula and micro-cannula (239).

The master delivery tip is responsible to deliver and evacuate the irrigant. This tip is connected to a syringe of irrigant and the evacuation hood is connected via tubing to the high speed suction of the dental unit. The macro-cannula is used to suction irrigant from the chamber toward the coronal and middle sections of the root canal. the macro-cannula or micro-cannula is connected by tubing to the highspeed suction of the dental chair (239).

The macro-cannula is responsible for the initial flushing of the coronal part of the canal. The tip of the macro-cannula has a size of 0.55 mm and 0.02 taper (239).

During irrigation, irrigant will be delivered to the pulp chamber with the master delivery tip, this tip will also suction the access irrigant to prevent over flow. The cannula inside the canal will pull the irrigant from the pulp chamber down the canal by negative pressure, then the irrigant will be suctioned into the cannula and out through the suction hose. The negative pressure mechanism will enable the

irrigant to reach to the apical potion of the canal (working length) and to avoid the apical vapor lock (239,244).

Nielsen et al. compared the efficacy of EndoVac system with that of needle irrigation using NaOCI and EDTA at 1 and 3 mm from working length. No significant differences were noticed at the apical 3 mm of root canal, but EndoVac system was significantly better and resulted in less remaining debris at 1mm level from apex. They also showed that during same time, the volume of the irrigant delivered by EndoVac system was significantly higher than the volume delivered by conventional syringe irrigation with the advantage of reducing the risk of irrigant extrusion to the periapex area (245,246).

One of the disadvantages of EndoVac is the clogging of the micro-cannula holes with debris which may affect the efficacy of the system. This can be overcome by replacing the cannula or using positive pressure rinse to open the blocked holes (247).

Our research was designed to observe the different irrigation protocols, that are available today in Endodontics, to compare the results of smear layer removal, the amount of remaining debris and visibility of the dentinal tubules. Our hypothesis is that there should be no significant difference.

2. <u>Materials and Methods</u>

Two hundred and seven (207) recently extracted molar teeth (maxillary and mandibular) were obtained from the teeth Databank at Nova Southeastern University College of Dental Medicine. The inclusion criteria included teeth with: intact coronal structure, no evidence of previous root canal therapy, no signs for any internal, external or cervical resorption, no restorations or carious lesions and single canal roots with a curvature of 30° or more. The angle of curvature was selected according to Schneider's method. In this method, first point was marked at the middle of a file at the level of the canal orifice, a straight line was drawn parallel to the file image from the first point to the level where the file starts to deviate from this line, this will represent the second point. The third point was marked at the apical foramen of the root and another line was drawn from this point to the second point. The angle formed by the intersection of the lines represents the canal curvature (248).

Only fifty-one roots of the two hundred and seven molars met the criteria.

The teeth were decoronated to obtain a standardized root length of 12 mm (261). After decoronation, patency and working length were verified by placing a number 10 K-file into the canal. A Global Endodontic Microscope (Global Surgical Corporation - St. Louis, MO, U.S.A) at 2.00x magnification power was utilized to visualize the file at the apex. The working length (WL) was determined by subtracting 0.5 mm from the canal length (249) as determined by the #10 K-file.

Before the instrumentation, root tips were sealed with hot glue and roots were embedded into silicone mold.

Instrumentation:

Instrumentation was performed by using NiTi rotary instruments (ProTaper system, Dentsply-Sirona). The sequence of the rotary files: SX, S1, S2, F1. The apical preparation was performed by using ProFile #25/.04, #30/.04 and finally #35/.04 hand files (ProFile system, Dentsply-Sirona). Between each instrument, canals were irrigated with 1 ml of 6% NaOCI solution using a syringe and a 30-gauge needle (Max-I-Probe needle, Dentsply-Sirona) (n= 39). For EndoVac group (n=12); the pulp chamber was flushed with 1 ml of 6% NaOCI solution using MDT (Master delivery tip).

To maintain irrigation consistency, a programmable syringe pump (PSP) (Alladin, AL 1000; World Precision Instruments, Inc, Sarasota, FL) set to deliver 3.0 ml / min was connected to each system.

After finishing the cleaning and shaping, the teeth were randomly distributed to the following groups (Figure 1);

- Traditional irrigation with a 30-gauge needle (Max-I-Probe needle, Dentsply Tulsa Dental). (Max-I-Probe needle, Dentsply Tulsa Dental).
 Needle tip will be positioned at Working Length– 2 mm. (n=12)
- a. 6% NaOCI application for 30 secs, followed by a passive wait of 60 secs,

- b. 17% EDTA for 30 secs, followed by a passive wait of 60 sec
- c. Final irrigation with 6% NaOCI for 30 secs, followed by a passive wait of 60 sec.
- EndoActivator and a 30-gauge needle (Max-I-Probe needle, Dentsply Tulsa Dental). Needle tip will be positioned at working Length – 2 mm. (n=12)
- a. 6% NaOCI application for 30 secs, followed by an activation for 60 sec
- b. 17% EDTA application for 30 secs, followed by an activation for 60 sec
- c. Final irrigation with 6% NaOCI for 30 secs, followed by a passive wait of
 60 seconds.
- 3. PUI (Passive Ultrasonic Irrigation)

Needle tip will be positioned at working Length -2 mm. (n=12)

- a. 6% NaOCI application for 30 secs, followed by a PUI activation for 60 seconds
- b. 17% EDTA application for 30 secs, followed by an activation for 60 seconds
- c. Final irrigation with 6% NaOCI for 30 secs, followed by an activation for 60 seconds.

4. EndoVac irrigation. (n=12)

a. Macro Cycle - 20 seconds of rapid apical/coronal movement from as

deep as the macro will go apically to the pulp chamber floor.

- **b.** Micro Cycle
- I. 6% NaOCI for 30 secs, followed by a passive wait for 60 seconds.
- **II.** 17% EDTA application for 30 secs, followed by a passive wait for 60 seconds
- III. Final irrigation with 6% NaOCI for 30 secs, followed by a passive wait for 60 seconds.
- **5. Saline irrigation** with the same protocol as group 1 with a 30-gauge needle. (n=3)

After the final irrigation, teeth were removed from the silicone mold and fixed by submerging in a 10 percent neutral-buffered formalin solution at 18°C for 24 hours. After the fixation, the teeth were dehydrated and bisected longitudinally in a buccolingual direction. A chisel was used to expose the root interiors. One half of each root was coated with sputter coat 2X 30sec under argon gas using a gold target with Cressington 108 sputter coater. After this process those specimens were imaged under low vacuum conditions with the FEI Quanta 200 SEM. The root halves (n=102) were evaluated under Scanning Electron Microscope (SEM) (Figure 2).

Scanning electron microscope was introduced by McMullan. This type of electron microscope scans the sample with a focused beam and creates an image

for it. Different signals, which carry information about the sample's surface structure and composition, will be produced when the electron interacts with atoms at different levels within the sample (250,251). Ardenne in 1937 was the first to invent a true microscope with high magnification (252). SEM micrograph has the ability to produce a three-dimensional appearance due to the large depth of field produced by the very narrow electron beam.

The amount of smear layer presents on the surfaces of the root canal wall at the coronal, middle, and apical portion was scored according to Nova Grid System (Nova Southeastern University-College of Dental Medicine Scoring System) (Figure 3). This system permits random scoring from 3 calibrated, independent Board C ertified Endodontists in order to provide a fair and reliable evaluation of each system used.

The scoring system for the amount of dentinal tubules opened, will be as follows (Figure 4):

Score 1- All dentinal tubules visible. Score 2- More than 50% of the tubules visible (>50%). Score 3-Less than 50% of the tubules visible (<50%). Score 4-No tubules visible.

For smear layer removal the results will be recorded as follows (Figure 2): Score 1- No smear layer present. Score 2- Less than 50% of the surface covered with smear layer (<50%). Score 3- More than 50% of the surface covered with smear layer (>50%). Score 4- All surface covered with smear layer.

For the amount of debris and canal cleanliness the scale will consist of the following:

Score 1- No debris present.

Score 2- Less than 50% of the surface covered with debris (>50%).

Score 3- More than 50% of the surface covered with debris (>50%).

Score 4- All surfaces covered with debris.

The scores given to each individual square was averaged to get one score per slide. A form was provided to the evaluator for data collection (Figure 5). Data was analyzed by using the Cochran-Mantel-Haenszel method.

1	The teeth were randomly distributed to the following												
	groups:												
#	Groups												
1	Traditional irrigation with a 30-gauge needle (Max-I-Probe needle, Dentsply Tulsa Dental). (Max-I-Probe needle, Dentsply Tulsa Dental). (n=12)												
2	EndoActivator and a 30-gauge needle (Max-I-Probe needle, Dentsply Tulsa Dental). Needle tip will be positioned at working Length – 2 mm. (n=12)												
3	PUI (Passive Ultrasonic Irrigation). Needle tip will be positioned at working Length – 2 mm. (n=12)												
4	Endovac irrigation. (Discus Dental, Culver City, CA) (n=12)												
5	Saline irrigation with the same protocol as group 1 with a 30- gauge needle. (n=3)												

Figure 1. Treatment groups



Figure 2. Representative SEM micrographs taken from the coronal, middle and the apical third of the canals.



Figure 3. Sample SEM micrograph to illustrate Nova Grid Scoring System taken from one of the EndoVac specimen.

The root canals (n=102) were evaluated using a scanning electron microscope (SEM).											
Dentinal	Score 1	All dentinal tubules visible.									
tubules	Score 2	More than 50% of the tubules visible									
i di bullo b	Score 3	Less than 50% of the tubules visible									
	Score 4	No tubules visible									
Smear layer	Score 1	No smear layer present									
removal	Score 2	Less than 50% of the surface covered with smear layer.									
	Score 3	More than 50% of the surface covered with smear layer.									
	Score 4	All surface covered with smear layer.									
Debris &	Score 1	No debris present.									
canal	Score 2	Less than 50% of the surface covered with debris.									
cleanliness	Score 3	More than 50% of the surface covered with debris.									
	Score 4	All surfaces covered with debris.									

Figure 4. Scoring system

	Α		В	С	D	Е	F	G	Н		J	Κ	L	MN	0	Ρ	Q	R	S	Т	U	۷	W	Х	Υ	Ζ	A AB	ACA	D	AE /	٩F	۹G /	٩H	AI	AJ	AK	AL /	١M
1	Sample						De	entin T	Tubule	25									5	Smear	Laye	r										Deb	is					
2			1	2	3	4	5	6	7	8	9	10	11	12	1	2	3	4	5	6	7	8	9	10	11	12	1	2	3	4	5	6	7	8	9	10	11	12
3		1	1	2	- 4	- 4	2	2	3	- 4	2	2	- 4	4	1	1	- 4	4	1	1	3	- 4	1	2	- 4	- 4	2	2	3	2	2	2	2	2	2	2	2	3
4		2	3	3	3	2	- 3	3	- 4	3	2	3	3	4	3	3	3	3	3	3	3	3	3	3	- 4	- 4	4	4	4	4	4	4	4	4	- 4	4	3	3
5		3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	1	1	2	3	2	2	2	2	2
6		4	3	3	4	3	4	- 4	- 4	4	4	4	- 4	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	3	2	2	3	2	2	2	3	3
7		5	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	1	3	2	2	2	2	2	1	1
8		6	4	4	4	- 4	4	4	- 4	4	4	4	4	4	4	4	4	4	- 4	- 4	- 4	4	4	4	- 4	- 4	3	2	2	2	2	2	2	2	3	3	2	2
9		7	4	- 4	4	4	4	4	- 4	4	4	4	- 4	4	4	4	4	4	- 4	- 4	- 4	4	4	4	- 4	- 4	2	2	2	2	2	2	2	2	3	2	2	2
10		8	3	3	2	3	- 4	- 4	- 4	- 4	- 4	- 4	- 4	4	3	3	2	3	3	3	3	3	4	- 4	- 4	- 4	2	2	1	2	2	2	2	2	2	2	2	2
11		9	4	- 4	3	1	- 4	3	3	3	4	3	3	3	4	4	2	1	- 4	3	2	2	4	3	2	2	2	2	2	2	1	2	2	2	2	2	2	1
12		10	4	3	4	4	4	3	4	4	4	3	- 4	4	4	4	4	4	4	3	- 4	4	4	3	- 4	- 4	2	3	2	2	2	3	2	2	2	2	2	1
13		11	2	1	1	2	2	2	2	3	3	3	3	4	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	2	2	2	2	2	2	2	2	2
14		12	4	- 4	- 4	- 4	- 3	3	- 4	- 4	- 4	3	3	4	- 4	- 4	- 4	4	3	2	- 4	- 4	4	- 4	3	- 4	2	2	3	3	2	2	3	3	2	2	2	2
15		13	3	3	3	3	3	3	3	3	2	2	3	3	3	3	3	3	3	3	3	3	3	3	3	3	1	2	2	2	2	2	2	2	2	2	1	2
16		14	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	2	2	2	2	1	1	2	1	1
17		15	4	- 4	- 4	4	4	- 4	- 4	- 4	- 4	4	- 4	4	- 4	4	4	4	- 4	- 4	- 4	4	4	- 4	- 4	- 4	2	2	2	2	2	2	2	2	2	2	2	2
18		16	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	2	1	2	2	2	2	1	1	1
19		17	3	3	3	2	3	3	3	2	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	2	2	2	2	2	2	2	1	2
20		18	1	1	2	3	3	1	2	1	2	2	2	2	1	1	1	1	1	1	1	1	1	1	1	1	2	2	2	3	3	2	2	2	2	2	2	2
21		19	4	- 4	4	- 4	4	- 4	- 4	4	4	- 4	- 4	4	- 4	- 4	4	4	- 4	- 4	- 4	4	4	- 4	- 4	- 4	1	1	1	2	1	1	1	2	2	1	1	1
22		20	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	2	2	2	2	2	2	2	2	2	2	2	2
23		21	4	- 4	4	- 4	4	4	4	4	3	4	- 4	4	- 4	- 4	4	4	3	- 4	- 4	4	3	4	- 4	4	2	2	2	2	2	2	2	2	2	2	1	1
24		22	2	3	3	3	2	3	3	3	3	3	3	3	2	3	2	3	2	2	2	3	3	3	3	3	1	1	1	2	2	2	1	2	2	2	2	1
25		23	4	4	4	4	4	4	4	4	4	4	4	4	4	4	4	4	4	- 4	4	4	4	4	4	4	2	2	2	2	1	2	1	2	2	2	2	2
26		24	1	1	1	1	1	1	2	2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	2	2	2	1	1	1	2	2	1	1	1	1
27		25	4	3	- 4	3	3	3	- 4	1	3	4	- 4	4	3	3	3	4	3	3	- 4	4	3	3	3	- 4	2	2	2	2	2	2	2	2	2	2	2	2
28		26	3	3	3	3	3	3	2	2	2	2	3	3	3	3	3	3	3	3	3	2	3	3	3	3	2	2	2	1	2	2	2	2	2	2	2	2
29		27	1	1	2	1	1	2	1	2	2	2	3	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2	2
30		28	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	3	1	1	1	2	1	1	1	1	2	1	1	2

Figure 5. Sample from the form that was provided to the evaluator for data collection

3. <u>Results</u>

The average scores of SEM evaluation of each group are shown in (Table 1). In the control group (Saline), smear layer covered the entire surface of the root canal dentin. There were relatively very few open dentinal tubules.

Nested-random effects model was used to look for differences by group, and to group by sections of the tooth for each dependent variable (tubules, smear layers, and remaining debris). Pairwise comparisons were conducted using Bonferroni adjustments. Consistency between raters was calculated using intra-class correlation coefficients (ICC).

The traditional irrigation group demonstrated more samples with a moderate smear layer (Fig. 2), whereas the EndoVac, EndoActivator and PUI groups demonstrated more samples with visible dentinal tubules. The EndoVac system removed significantly more smear layer and debris than other groups in every segment of the roots. There was no significant difference between EndoActivator and PUI except the debris removal in the apical third. EndoActivator removed significantly more debris compared to PUI in the apical third. The highest scores, indicating the presence of more debris and smear layer were recorded in the apical third of the canals. This was followed by the middle third, and, then the coronal third (Fig. 2, 6).

Statistical significance was found at p<0.05, and results are presented below using marginal means. Marginal means are the means for that factor averaged across all levels of the other factor.

	Tu	ıbule visibil	ity		Smear laye	r	Debris				
Group	Coronal	Middle	Apical	Coronal	Middle	Apical	Coronal	Middle	Apical		
Traditional	3.09	2.83	3.46	3.11	2.81	3.42	2.40	2.21	2.55		
Traditional	0.75	0.81	0.87	0.74	0.79	0.90	0.69	0.59	1.01		
Dessive Ultresonia	2.62	2.88	3.30	2.69	2.90	3.23	1.88	1.76	2.14		
Passive oldasonic	0.96	0.71	0.62	0.91	0.80	0.73	0.79	0.69	0.93		
Endepativator	2.46	2.64	2.73	2.51	2.74	2.92	1.79	1.75	1.87		
Endoactivator	0.83	0.94	0.96	0.71	0.82	0.82	0.72	0.81	0.81		
Endoveo	1.93	1.78	1.84	2.16	2.00	2.11	1.44	1.41	1.40		
Endovac	0.83	0.83	0.81	0.68	0.74	0.72	0.54	0.51	0.49		
Control	4.00	3.98	3.99	3.93	3.99	4.00	2.66	2.72	2.74		
	0.00	0.15	0.21	0.25	0.10	0.00	1.06	0.99	1.21		

Table 1. Average scores of SEM evaluation of tubule visibility,smear layer and remaining debris. Scores 1-2 (clean canal wall)versus 3-4.



Figure 6.1. Distribution of tubule visibility scores at coronal, middle and apical levels of all three examiners.



Figure 6.2. Distribution of smear layer scores at coronal, middle and apical levels of all three examiners.



Figure 6.3. Distribution of remaining debris scores at coronal, middle and apical levels of all three examiners.

Tubules:

Measure	Intervention Group	Coronal	Middle	Apical
	Traditional	3.09	2.83	3.46
		0.75	0.81	0.87
	Passive Ultrasonic	2.62	2.88	3.30
		0.96	0.71	0.62
Tubulaa	Endoactivator	2.46	2.64	2.73
Tubules		0.83	0.94	0.96
	Endovac	1.93	1.78	1.84
		0.83	0.83	0.81
	Control	4.00	3.98	3.99
		0.00	0.15	0.21

 Table 2. Tubules Descriptive Statistics*

Table 2.1. Tubules Intra Class Correlation Coefficient - Rater Agreement*

ICC	Measure	Lower 95% CI	Upper 95% Cl
Average	0.98	0.98	0.99

* The tables are pairwise comparisons between the means for each group. The difference is the mean difference. Significance represent a statistical difference if p < 0.05.

Table 2.1 tells us how similar the raters were in rating the measures. An ICC of .98 is excellent.

Group		Group	Differen ce	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	VS	Traditional	-0.20	-0.51	0.12	NS
Endoactivator	VS	Traditional	-0.51	-0.87	-0.15	p < 0.05
Endovac	vs	Traditional	-1.27	-1.53	-1.02	p < 0.05
Control	vs	Traditional	0.87	0.65	1.09	p < 0.05
Endoactivator	VS	Passive Ultrasonic	-0.31	-0.67	0.05	NS
Endovac	VS	Passive Ultrasonic	-1.08	-1.34	-0.82	p < 0.05
Control	VS	Passive Ultrasonic	1.07	0.84	1.29	p < 0.05
Endovac	vs	Endoactivator	-0.76	-1.08	-0.44	p < 0.05
Control	vs	Endoactivator	1.38	1.09	1.67	p < 0.05
Control	vs	Endovac	2.14	2.01	2.28	p < 0.05

Table 2.2. Tubules Pairwise Comparisons for ALL Sections*

 Table 2.3. Tubules Pairwise Comparisons for Coronal Section*

Group		Group	Differen ce	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.47	-1.04	0.10	NS
Endoactivator	vs	Traditional	-0.62	-1.09	-0.15	p < 0.05
Endovac	vs	Traditional	-1.16	-1.54	-0.78	p < 0.05
Control	vs	Traditional	0.91	0.60	1.22	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.15	-0.75	0.44	NS
Endovac	vs	Passive Ultrasonic	-0.69	-1.22	-0.16	p < 0.05
Control	vs	Passive Ultrasonic	1.38	0.90	1.86	p < 0.05
Endovac	vs	Endoactivator	-0.54	-0.94	-0.13	p < 0.05
Control	vs	Endoactivator	1.54	1.18	1.89	p < 0.05
Control	vs	Endovac	2.07	1.85	2.29	p < 0.05

Group		Group	Differen ce	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	0.05	-0.48	0.57	NS
Endoactivator	vs	Traditional	-0.19	-0.73	0.35	NS
Endovac	vs	Traditional	-1.05	-1.53	-0.57	p < 0.05
Control	vs	Traditional	1.14	0.73	1.56	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.24	-0.72	0.25	NS
Endovac	vs	Passive Ultrasonic	-1.10	-1.51	-0.68	p < 0.05
Control	vs	Passive Ultrasonic	1.10	0.76	1.44	p < 0.05
Endovac	vs	Endoactivator	-0.86	-1.29	-0.43	p < 0.05
Control	vs	Endoactivator	1.33	0.97	1.70	p < 0.05
Control	vs	Endovac	2.19	1.94	2.45	p < 0.05

Table 2.4. Tubules Pairwise Comparisons for Middle Section*

Table 2.5. Tubules Pairwise Comparisons for Apical Section

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.16	-0.63	0.31	NS
Endoactivator	vs	Traditional	-0.73	-1.27	-0.18	p < 0.05
Endovac	vs	Traditional	-1.62	-2.11	-1.13	p < 0.05
Control	vs	Traditional	0.54	0.15	0.93	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.57	-1.04	-0.09	p < 0.06
Endovac	vs	Passive Ultrasonic	-1.46	-1.88	-1.04	p < 0.05
Control	vs	Passive Ultrasonic	0.70	0.40	1.00	p < 0.05
Endovac	vs	Endoactivator	-0.90	-1.40	-0.39	p < 0.05
Control	vs	Endoactivator	1.27	0.87	1.66	p < 0.05
Control	vs	Endovac	2.16	1.83	2.49	p < 0.05
Smear layer:

Measure	Intervention Group	Coronal	Middle	Apical	
	Traditional	3.11	2.81	3.42	
		0.74	0.79	0.90	
	Passive Ultrasonic	2.69	2.90	3.23	
		0.91	0.80	0.73	
Smoor	Endoactivator	2.51	2.74	2.92	
Sillear		0.71	0.82	0.82	
	Endovac	2.16	2.00	2.11	
		0.68	0.74	0.72	
	Control	3.93	3.99	4.00	
		0.25	0.10	0.00	

Table 3. Smear Layer Descriptive Statistics*

Table 3.1. Smear Layer Intra Class Correlation Coefficient - Rater Agreement*

ICC	Measure	Lower 95% Cl	Upper 95% Cl
Average	0.98	0.97	0.99

Table 3.2. Smear Layer Pairwise Comparisons for ALL Sections*

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.17	-0.46	0.12	NS
Endoactivator	vs	Traditional	-0.39	-0.69	-0.09	p < 0.05
Endovac	vs	Traditional	-1.02	-1.30	-0.74	p < 0.05
Control	vs	Traditional	0.87	0.66	1.08	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.21	-0.51	0.08	NS
Endovac	vs	Passive Ultrasonic	-0.85	-1.13	-0.56	p < 0.05
Control	vs	Passive Ultrasonic	1.04	0.82	1.26	p < 0.05
Endovac	vs	Endoactivator	-0.63	-0.92	-0.34	p < 0.05
Control	vs	Endoactivator	1.26	1.03	1.48	p < 0.05
Control	vs	Endovac	1.89	1.70	2.08	p < 0.05

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.42	-0.90	0.06	NS
Endoactivator	vs	Traditional	-0.60	-0.96	-0.24	p < 0.05
Endovac	vs	Traditional	-0.96	-1.28	-0.63	p < 0.05
Control	vs	Traditional	0.82	0.51	1.13	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.18	-0.65	0.30	NS
Endovac	vs	Passive Ultrasonic	-0.54	-1.00	-0.07	p < 0.05
Control	vs	Passive Ultrasonic	1.24	0.80	1.68	p < 0.05
Endovac	vs	Endoactivator	-0.36	-0.68	-0.03	p < 0.05
Control	vs	Endoactivator	1.42	1.12	1.72	p < 0.05
Control	vs	Endovac	1.78	1.53	2.02	p < 0.05

Table 3.3. Smear Layer Pairwise Comparisons for Coronal Section*

Table 3.4. Smear Layer Pairwise Comparisons for Middle Section*

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	VS	Traditional	0.09	-0.45	0.63	NS
Endoactivator	vs	Traditional	-0.07	-0.56	0.42	NS
Endovac	vs	Traditional	-0.81	-1.29	-0.32	p < 0.05
Control	vs	Traditional	1.18	0.77	1.59	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.16	-0.63	0.30	NS
Endovac	vs	Passive Ultrasonic	-0.90	-1.36	-0.44	p < 0.05
Control	vs	Passive Ultrasonic	1.09	0.70	1.47	p < 0.05
Endovac	vs	Endoactivator	-0.74	-1.13	-0.35	p < 0.05
Control	vs	Endoactivator	1.25	0.97	1.53	p < 0.05
Control	vs	Endovac	1.99	1.73	2.24	p < 0.05

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.19	-0.70	0.32	NS
Endoactivator	vs	Traditional	-0.50	-1.00	0.00	NS
Endovac	vs	Traditional	-1.31	-1.79	-0.83	p < 0.05
Control	vs	Traditional	0.59	0.18	1.00	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.31	-0.73	0.11	NS
Endovac	vs	Passive Ultrasonic	-1.12	-1.53	-0.72	p < 0.05
Control	vs	Passive Ultrasonic	0.78	0.46	1.11	p < 0.05
Endovac	vs	Endoactivator	-0.81	-1.18	-0.45	p < 0.05
Control	vs	Endoactivator	1.09	0.81	1.38	p < 0.05
Control	vs	Endovac	1.90	1.66	2.15	p < 0.05

Table 3.5. Smear Layer Pairwise Comparisons for Apical Section*

Debris:

Table 4. Debris Descriptive Statistics*

Measure	Intervention Group	Coronal	Middle	Apical
	Traditional	2.40	2.21	2.55
		0.69	0.59	1.01
	Passive Ultrasonic	1.88	1.76	2.14
		0.79	0.69	0.93
Dobric	Endoactivator	1.79	1.75	1.87
Deblis		0.72	0.81	0.81
	Endovac	1.44	1.41	1.40
		0.54	0.51	0.49
	Control	2.66	2.72	2.74
		1.06	0.99	1.21

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1 able 4.1.	Debris Intra	i Class Co	rrelation	Coefficient	- Kater .	Agreement [*]

ICC	Measure	Lower 95% Cl	Upper 95% Cl
Average	0.98	0.97	0.98

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.46	-0.74	-0.19	p < 0.05
Endoactivator	vs	Traditional	-0.58	-0.80	-0.37	p < 0.05
Endovac	vs	Traditional	-0.97	-1.16	-0.78	p < 0.05
Control	vs	Traditional	0.32	-0.17	0.80	NS
Endoactivator	vs	Passive Ultrasonic	-0.12	-0.38	0.15	NS
Endovac	vs	Passive Ultrasonic	-0.50	-0.76	-0.25	p < 0.05
Control	vs	Passive Ultrasonic	0.78	0.27	1.29	p < 0.05
Endovac	vs	Endoactivator	-0.39	-0.55	-0.22	p < 0.05
Control	vs	Endoactivator	0.90	0.42	1.38	p < 0.05
Control	vs	Endovac	1.28	0.84	1.72	p < 0.05

Table 4.2. Debris Pairwise Comparisons for ALL Sections*

 Table 4.3. Debris Pairwise Comparisons for Coronal Section*

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	vs	Traditional	-0.53	-0.92	-0.13	p < 0.05
Endoactivator	vs	Traditional	-0.61	-0.94	-0.28	p < 0.05
Endovac	vs	Traditional	-0.96	-1.24	-0.69	p < 0.05
Control	vs	Traditional	0.26	-0.22	0.74	NS
Endoactivator	vs	Passive Ultrasonic	-0.09	-0.46	0.29	NS
Endovac	vs	Passive Ultrasonic	-0.44	-0.77	-0.10	p < 0.05
Control	vs	Passive Ultrasonic	0.78	0.27	1.29	p < 0.05
Endovac	vs	Endoactivator	-0.35	-0.62	-0.08	p < 0.05
Control	vs	Endoactivator	0.87	0.40	1.34	p < 0.05
Control	vs	Endovac	1.22	0.81	1.64	p < 0.05

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	VS	Traditional	-0.45	-0.79	-0.11	p < 0.05
Endoactivator	vs	Traditional	-0.46	-0.79	-0.14	p < 0.05
Endovac	vs	Traditional	-0.80	-1.05	-0.54	p < 0.05
Control	vs	Traditional	0.51	0.02	0.99	p < 0.05
Endoactivator	vs	Passive Ultrasonic	-0.01	-0.36	0.35	NS
Endovac	vs	Passive Ultrasonic	-0.34	-0.64	-0.05	p < 0.05
Control	vs	Passive Ultrasonic	0.96	0.43	1.49	p < 0.05
Endovac	vs	Endoactivator	-0.34	-0.62	-0.05	p < 0.05
Control	vs	Endoactivator	0.97	0.45	1.49	p < 0.05
Control	vs	Endovac	1.30	0.83	1.78	p < 0.05

Table 4.4. Pairwise Comparisons for Middle Section*

Table 4.5. Debris Pairwise Comparisons for Apical Section*

Group		Group	Differenc e	Lower 95% Cl	Upper 95% Cl	Significant
Passive Ultrasonic	VS	Traditional	-0.41	-0.93	0.11	NS
Endoactivator	vs	Traditional	-0.68	-1.19	-0.16	p < 0.05
Endovac	vs	Traditional	-1.15	-1.60	-0.70	p < 0.05
Control	vs	Traditional	0.17	-0.61	0.95	NS
Endoactivator	vs	Passive Ultrasonic	-0.26	-0.75	0.22	NS
Endovac	vs	Passive Ultrasonic	-0.74	-1.13	-0.34	p < 0.05
Control	vs	Passive Ultrasonic	0.58	-0.18	1.34	NS
Endovac	vs	Endoactivator	-0.47	-0.83	-0.11	p < 0.05
Control	vs	Endoactivator	0.85	0.11	1.59	p < 0.05
Control	vs	Endovac	1.32	0.67	1.97	p < 0.05

Data were analyzed by Pairwise comparisons. EndovacTM system was significantly more effective (p<0.05) than the other groups at the apical, middle and coronal sections for elimination of smear layer as well as debris removal and improved tubule visibility. Negative pressure delivery systems may provide better cleaning in curved root canals.

4. Discussion

One of the main goals of endodontic treatment is to optimize root canal disinfection which involves a thorough chemo-mechanical debridement of pulp tissues, canals debris and eliminate infective microorganisms (1-4).

As mentioned previously, chemo-mechanical preparation combined the action of root canal instrument with the action of different irrigants in an important step to remove the smear layer and achieve optimal disinfection of the root canal system (253).

The teeth selected in this study had intact coronal structures to avoid any possible detrimental effects on: the physical properties, the composition of root canal dentin and dentinal tubules, which may cause some variations in the outcome.

The teeth that were selected were mainly molars with roots that have a curvature of 30 or more degrees, as these teeth are more challenging to instrument and clean (254,255). In addition to that, curved canals have higher risks of instrument separation due to torsional stress and cyclic fatigue (256,257). These canals are usually narrow, which make the contact angle between the file and the dentinal wall bigger and increase the fatigue of the file (258).

The degree of curvature was determined by using Schneider's method. This method as explained in materials and methods is simple, practical and has already been adopted by many studies (248).

Plastic teeth/models were avoided in this study as it was important to create an environment that is similar as much as possible to the actual challenge in the clinical setting as shown in many studies (259,260).

Decoronation of the teeth was accomplished to create a straight line access and to remove any obstacles that may interfere with the instrumentation and cleaning process. In this study, decoronation was performed to standardize root length at 12 mm as this tends to create an artificial scenario for which the access opening cannot influence the intracanal procedures and to eliminate any possible discrepancy that may affect the final results of this study.

In addition to that, it has been shown that the average molar root length from cervical line to apex is about 12-13 mm (261).

As part of the chemo-mechanical preparation, the root canals in the present study were instrumented with ProTaper and ProFile rotary system up to size #35/.04 at the apical portion of the canal. These instruments have been shown to remove significantly more smear and debris than hand instrumentation (262). However, the efficacy of the irrigation delivery systems also depends on the root canal preparation size and taper. It is an ongoing debate that while some studies report that larger apical preparation sizes reduce the bacterial population (263,264), others indicate the risk of perforations or possible root fractures (265,266).

Many studies have showed the importance of the depth of the needle insertion and how far the irrigant can penetrate apically. These studies were also conducted to determine the ideal size for the root canal preparation and how the

canal enlargement will improve the access of the irrigant to the microorganism that have penetrated deeply into the dentin.

Studies by Ørstavik et al (267,268) and Matsumiya and Kitamura (269) concluded that the size of apical instrumentation may play an important role in removal of canal bacteria. They also reported that with larger instrumentation, fewer bacteria remained in the canal and the healing was more rapid. Recently, Wu and Wesselink (179) concluded that instrumentation of the molar canals to size #45 apical file with 0.02 taper will result in a much cleaner canals (270).

In addition to that, for the needle tip to function efficiently, a proper enlargement of the root canal is recommended. Ram et al recommended preparation of the canal up to size #40 /.02 taper for effective delivery of the irrigant (271). Other study by Salzgeber and Brilliant et al. showed that the irrigant can reach to the root canal apex when the canal was instrumented to file size #30 /.02 taper (272). Even though larger preparation sizes with large tapers provide a constant increase in hydrodynamic flow during irrigation, in this study, the apical preparation size was limited to #35 /.04 mm taper in order to conserve radicular dentin, to minimize the risk of procedural errors and to establish a path for the irrigants to reach into the most infected areas of the root canal (14). This will ensure adequate apical flushing and proper chemical disinfection.

The largest irrigation needle in the present study was the stainless steel micro-cannula for EndoVac system, which has an external diameter size of 0.32mm with 0.04mm taper. This tip can be used in the canals that are enlarged

to size #35 and is responsible for the irrigation of the apical part of the canal by placing it close to working length to suction irrigant and debris (239).

Therefore, it was important to make sure all the tips were able to move loosely in the canal systems (245), to avoid insufficient preparation and enlargement of the root canal. This will restrict the activation of the ultrasonic irrigant and limit the free oscillation of the file, which can limit the cleaning efficacy of the root canal irrigant (202,226).

Many studies also showed that a canal preparation to size #30-35/.04 taper is required for NaOCI to be effective (276-275), and an apical preparation to ISO size 0.35 or larger is recommended (276).

The depth of the activator tip or the irrigation needle and the size of the canal preparation influence the cleaning and shaping process. This plays an important role on the extent of irrigant replacement and the amount of pressure at the apical part of the root canal (277).

Nielsen and Baumgartner reported that the needle depth in the standard irrigation technique should be limited to 2 mm from WL (245). This measurement was applied in the present study. This depth was also applied to the PUI and EndoActivator, while the EndoVac system was positioned to WL (280,246) Moreover, the rate of irrigation solution delivery into the canal system was set at 3.0 ml / min for each irrigation group except EndoVac. The EndoVac system delivers more irrigant into the root canal system. Unfortunately, there was no plausible means to measure the rate of irrigant delivery for the EndoVac group (278).

For this study, a 30-guage side vented (Max-I-Probe needle, Dentsply-Sirona) needle was used. Studies have shown that the 30G needles were more efficient in cleaning the apical part of the root canal (176,279). The needle has a luer lock connector to provide a secure attachment and better removal from any disposable syringe.

Manufacturer claimed that the rounded tip reduces the chance of perforating the apex and the side-port in the cannula allows a unique upward turbulent flow which reduces the chance of the irrigant from passing through the apical foramen. This needle has a tip size of 0.3mm, which allows deeper penetration of the needle inside the root canal and its side vented design allows a more effective flow for the irrigant (279). This needle size is convenient for a canal space prepared up to size #35/.04 apical size to allow the needle to get into the last 2 mm of working length (181,280).

The needle allows a decent control of the depth of penetration of the irrigant. However, the delivery of the irrigant was restricted to only 1mm deeper from the tip and the flushing mechanism is relatively weak with limited ability to access isthmuses and lateral accessary canals (175,271).

A study by Dalton et al. showed that 72% of instrumented teeth still contain a positive culture (11) and instrumentation only eliminates 20-30% of bacteria (15). Therefore, the introduction and the use of different chemicals is a very critical part in cleaning and disinfecting root canal systems.

In this study, NaOCI was used, as it is the most common Endodontic irrigant with a superior tissue dissolution property and a well-documented antimicrobial, sporicidal and virucidal characteristic (23,280).

As earlier explained, the antimicrobial effectiveness of NaOCI depends on its high pH value and the potency of hypochlorous acid, which is a strong nonradical oxidant. When hypochlorous acid get in contact with the organic tissues, chlorine will be released. This chlorine will interfere with the DNA synthesis and cause the cell proliferation to cease (101,131).

Giardino et al showed that 5.25% NaOCI was the only irrigant to remove and desegregate E. faecalis biofilm generated on cellulose nitrate membrane filters compared to BioPure MTAD (Dentsply Tulsa Dental, Johnson City, TN) and Tetraclean (Ogna Laboratori Farmaceutici, Milano, Italy) (115). Luis E. Chavez et al exposed biofilms of E. faecalis, Lactobacillus paracasei, S. anginosus, and S. gordonii isolated from the infected root canals after 5 min exposure to the following: alkali (pH=12), 2.5% chlorhexidine digluconate, EDTA, and 1% NaOCI. The results showed that 1% NaOCI affected the membrane integrity of all organisms and removed most biofilm cells while the 2.5% CHX had a mild effect and removed only 50% of its biofilm cells (281).

A SEM and biofilm assay was used in another study to show that biofilm grown on dentin harbored more cells than polystyrene. The study also showed that biofilms of starved E. faecalis cells were more resistant to 5.25% NaOCI than in stationary cells and the effect of 5.25% NaOCI will decrease as the biofilm mature. This may contribute to the predominant role of E. faecalis in persistent periapical

infections (282). Ozdemir et al. showed that the combination of 2.5% NaOCI and 17% EDTA significantly reduced intracanal E. faecalis biofilm in young and old individuals however, the bacterial count in the old group were higher (283).

Other research study demonstrated that 2% CHX does not improve the biofilm dissolution or increase the cleaning of the dentin and 30 min application of NaOCI is necessary to achieve a higher value of cleaning and biofilm dissolution independent of the concentration (284). A study by Seet et al. showed that sonic or laser activation of 4% NaOCI resulted in greater E. faecalis reduction compared with syringe irrigation (285).

In this study 6% concentration of NaOCI was used. Previous studies have shown that dilution of NaOCI will significantly lower its tissue dissolution ability and the 6% concentration has more effective antimicrobial properties and better debridement quality compared to lower concentrations (137,286,287). As discussed, Clegg el al showed that 6% NaOCI was the only irrigant to remove biofilm compared to 1%, 3% NaOCI and 2% CHX (288).

Due to the limitation of NaOCI to act on the inorganic particles of the smear layer after instrumentation, EDTA was used as another main chemical and powerful chelating agent. This approach was justified by the recommendation of Yamada et al. when they set up the gold standard of the irrigation protocol and showed the necessity to use a chelating agent (17% EDTA) in combination with a tissue solvent irrigant (5.25% NaOCI) to remove both superficial debris and smear layer more efficiently (44).

Ethylenediaminetetraacetic Acid reacts with calcium ions in the hydroxyapatite crystal and removes them from the dentin matrix. It may also detach biofilm from the walls of the root canal (156).

The antimicrobial activity of EDTA is very limited and some studies related this activity to the chelation of cations from the bacteria outer membrane (155). A study by Ballal NV. et al. to evaluate the antimicrobial efficacy of 7% maleic acid and 17% EDTA against E. faecalis and Staphylococcus. No significant different were found (289). Ordinola-Zapata et al. reported in their study that a contact time of 5 min of 17% EDTA and 10% citric acid had no effect on the biofilm viability (290). These finding were similar to study by Arias-Moliz et al that showed EDTA has no effect on the E. faecalis even after 60 min (291).

Urea peroxide was introduced by Stewart et al. and showed the ability of urea peroxide solution to retain it is antimicrobial effect in the presence of blood. They also advocated the addition of EDTA to RC-Prep (15% EDTA, 10% urea peroxide and carbowax) to combine the chelating and the antimicrobial actions together (292).

EDTA was used at a concentration of 17% as many articles demonstrated its effectiveness at this level (44,293). In addition, a 1 min EDTA application with ultrasonic activation found to be very effective on smear layer removal at the apical area of the root canal (294).

Besides that, EDTA can cause erosion of the dentin structure with a significant reduction in the microhardness if left more than 3 min. For this reason, irrigation with EDTA was done for 30 secs with passive wait of no more than 1 min

to limit the amount of dentin destruction and according to other studies, EDTA has the ability to remove smear layer if applied for one min (295).

Another chelating agent known as EDTAC is produced by adding quaternary ammonium bromide (Cetavlon or Cetrimide) to EDTA to reduce its surface tension. Although, it has been shown no significant difference in the effectiveness between EDTA and EDTAC in removing smear layer, other studies have showed significantly lower efficacy of EDTAC than that of EDTA with reduced ability to remove calcium ions from dentin. Also, reducing the surface tension of EDTA did not significantly improve its effectiveness (296,297,298). Based on these facts, a decision was made to use EDTA in this study.

The method of delivery of the irrigant solutions also play an important part in root canal disinfection. Many studies have shown that traditional needle irrigation was insufficient to clean and reach all the anatomical complexities of the root canals (22,20) and the necessity to activate the endodontic irrigant appears to be an important approach to achieve a better cleaning and disinfection of the root canal system (194).

As mentioned earlier in this study, the main advantage of using ultrasonic in cleaning and shaping along with root canal irrigation is the acoustic streaming (209). This is a state of steady streaming patterns in a rapid vortex-like motion associated with a vibrating file. The agitation of the irrigant, by this method, has the advantage of increasing the penetration and the effectiveness of the irrigant through hydrodynamic shear stress (219,299,300). By taking the 6% NaOCI solution as an example , this irrigant has 300 μ m maximum depth of penetration

after 20 min of application (301) whereas E. faecalis can go up to 800-1000 μ m inside dentinal tubules (7).

The other physical effect that can be observed in the irrigant with free ultrasonic vibration is cavitation. This term reflects the growth and the collapse of gas bubbles due to rapid changes in pressure during oscillation in the fluid (302). A forced collapse in these bubbles creates some structure deformity in the surface due to the heavy impact which can be helpful in the endodontic application to disrupt bacterial biofilm and remove smear layer debris (303).

Under usual clinical conditions, the power of dental ultrasonic units is too low to produce significant cavitation effects on the dentinal walls (229).

EndoActivator is a sonically driven root canal irrigation system, which can produce a strong hydrodynamic phenomenon and vigorously agitate the irrigant once activated. This system operates at a lower frequency and produces less shear stresses compare to ultrasonic irrigation (209). Numerous researches have shown its effectiveness in removing the smear layer and displacing the clumps of simulated biofilm in curved canals (184,196).

In the current study, and specially at the coronal and apical thirds of the canal, our results agreed with the numerous researchers that have shown the effectiveness of EndoActivator in removing smear layer (184,195,196). This could be related to the improved flow rate and to the acoustic streaming action in creating implosions that radiates miniature tsunamis or shockwaves that dissipate at 25,000-30,000 times per second (195). The oscillation of the file shows large

displacement amplitudes and is unaffected by loading (when the file contacts the walls) (185).

As previously discussed, PUI depends on the transmission of the acoustic energy by means of ultrasonic waves from an oscillating file to the irrigant inside the root canal (220,209). This action improved the irrigant flow into the irregularities of the root canal and increased its volume (204).

Couple of studies have demonstrated that the ultrasonic activation method of the irrigant is more effective than traditional needle irrigation against canal debris and smear layer (194,304,305). This could be related to the cavitation effect and the increase in the irrigant temperature which improved the dissolution action of NaOCI inside the canal (209). This is in accordance with the results of the current study.

However, One of the PUI drawback in the present study, is the limited ability to show its effectiveness at the apical part of the root canal compared to the EndoVac system. Similar findings applied to the EndoActivator groups. This could be related to the present findings, such as the difficulty to standardize the position of the ultrasonically activated file in the middle of the canal and the vapor lock effect with air entrapment at the apical area of the root canal. This may prevent the adequate contact of the irrigant to this inaccessible are, and thus limit its effectiveness (237,238,235).

The present results did not agree with previous studies that have shown no significant differences in the removal of dentin debris between syringe irrigation and PUI (223,226,306).

Martin and Cunningham introduced Cavi-Endo as an untrasonic endodontic device. They conducted couple of studies on using ultrasound in root canal treatment. In these studies, they showed the efficacy of endosonic in root canal preparation and disinfection with the ability of ultrasonically activated irrigant to improve the cleaning of these canals. Martin and Cunningham also related the success of ultrasonic instrument to the synergistic effect which combine the ultrasonic energy with the irrigation solution (199-202).

The amount of time required to activate the irrigant is another critical factor in achieving the optimal cleaning results. A study was performed by Cameron et al. to compare different ultrasonic irrigation periods on smear layer removal. They illustrated that both 3 and 5 min ultrasonic irrigation produced smear free canals, while the 1 min irrigation was not effective. Other studies found the ultrasonic irrigation was ineffective against smear layer (307,308).

When the ultrasonic debridement efficacy in vital mandibular molar was compared histologically, the results showed significantly cleaner isthmuses and canals after only 1 min application of ultrasonic needle with no larger than a size #30 file compared to 3 min application in previous studies (309).

Similar results to the previous in vivo study were reported in necrotic human mandibular molars, as ultrasonic application for 1 min after hand/rotary preparation of the root canal showed significantly cleaner isthmuses and improved biofilm removal at the apical part of the root canal (310).

Ultrasonic was also promising in curved canals. Blank-Goncalves et al. reported a better removal of the smear layer in the apical third of curved root canals

when sonic and ultrasonic irrigation were used (311). According to Ahmad et al., better results can be achieved by pre-bending the file (217,220,312).

Other studies reported significantly cleaner isthmuses when PUI was used compared to syringe irrigation and PUI was able to remove debris in areas untouched by endodontic instruments (221,224).

On the other hand, Siqueira et al. tested the effectiveness of 4% NaOCI used in three irrigation methods in eliminating E. faecalis from the root canals, the results showed no significant differences between hand files and ultrasonic agitation (313).

Due to the limitation of conventional needle irrigation to replenish and exchange the irrigant (especially at the apical part of the root canal and the vapor lock effect that results in trapped air), the debridement efficiency of the irrigant and its ability to get in direct contact with the canal walls will be restricted (181,314). Therefore, a new system with different mechanism was introduced by Schoeffel GJ (239).

The EndoVac system is a root canal irrigation device which utilize an apical negative pressure (ANP) mechanism to deliver the irrigant with higher flow as close as 1 mm from working length, with the ability to suction out the canal debris with lower risk of irrigant extrusion accident (239,245,246).

In fact, the negative apical pressure system showed significantly less tendency for apical extrusion of the irrigant compared to the side vented needle (Max-I-Probe), whereas the size of the apical enlargement did not significantly affect the apical extrusion of the root canal irrigant (315).

The effectiveness of EndoVac system in cleaning canal debris is well documented (246). A study by Nielsen et al. showed a significant better debridement of EndoVac system compared with needle irrigation at 1 mm from working length using a 30-guage irrigation needle and canal enlargement to ISO size 36/.04 taper or larger (245). EndoVac system also achieved better control against E. faecalis than traditional positive pressure with no relation to the size of the canal preparation (#35 or #45), nor to the taper of the preparation (316). This system was also very successful in reducing intracanal levels of Candida Albicans (317).

In contrast, an in-vitro study by Townsend et al. compared the effect of different agitation techniques against E. faecalis. Their results showed that the ultrasonic agitation was significantly better than EndoVac and needle irrigation against intra-canal bacteria (196). Our study did not agree with their findings as these results could be related to the use of plastic simulated canals which do not have any actual similarities to natural teeth in the clinical setting. In addition, the present results did not agree with Brito et al findings either. These findings reported no significant differences between conventional irrigation with: NaviTip needles inserted up to 3 mm short of working length, EndoActivator and EndoVac system as they reported that all of these techniques showed a highly significant reduction in bacterial population (318).

A recent micro computed tomography analysis showed that EndoVac was not very successful in eliminating hard tissues debris from the isthmus area in the

mesial root of the mandibular molars. However, the apical negative pressure approach showed a much lower percentage of debris compare to conventional irrigation (319).

In this study, EndoVac[™] system was significantly more effective (p<0.05) than the other groups at the apical, middle and coronal sections for elimination of smear layer, debris removal and improved tubule visibility.

Although Uroz-Torrez et al. did not find any significant difference between the EndoActivator system and standard irrigation protocols (320), the current results demonstrated that the use of sonic and ultrasonic activation methods were actually more efficient in cleaning the root canal system compared to conventional irrigation. This is in agreement with other studies (294,321). In the recent study there was no significant difference between PUI and EndoActivator systems in curved canals. Jensen et al. confirmed these findings in their study comparing PUI to sonic activation (312).

In summary, Negative pressure delivery systems appears to provide better cleaning in curved root canals. Introducing the micro-cannula to the working length, the irrigant was able to reach safely to the complex anatomy of the root canal system in adequate volume and flow and suctioned out with canal debris to achieve excellent results in removing smear layer from dentinal walls.

5. <u>Conclusions:</u>

Irrigation regimes play an important role in the success of endodontic treatment. Up to date, no single irrigant protocol could achieve all the tasks required by irrigation. The advances in technology like positive and negative irrigation techniques have brought to fruition new devices that depend on different mechanism of irrigant delivery to the most apical part of the root canal system, tissue debridement and removal of both debris and smear layer.

The Endovac[™] apical negative pressure irrigation system was found to clean the root canal systems significantly better in all of the root canal sections we observed. This system was also superior to positive pressure devices in preventing apical extrusion of the irrigant, eliminating vapor lock effect, and providing adequate irrigant volume.

We recommend the use of the negative pressure irrigation system to improve the removal of smear layer and debris from root canals without the risk of irrigant extrusion.

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