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Echocardiographic assessment of aortic stenosis: a practical guideline from the
British Society of Echocardiography

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Abstract

The guideline provides a practical step-by-step guide in order to facilitate high quality echocardiographic studies of patients with aortic stenosis. In addition, it addresses commonly encountered yet challenging clinical scenarios and covers the use of advanced echocardiographic techniques, including TOE and Dobutamine stress echocardiography in the assessment of aortic stenosis.

Keywords

Aortic stenosis; guideline

Introduction.

Aortic valve stenosis is a significant health burden, particularly in older individuals, with a prevalence of up to 5% in individuals over 75 years of age¹. Aortic stenosis is the most common valve disease necessitating surgical or percutaneous intervention². Echocardiography is central in the diagnosis, assessment and management of individuals with aortic valve disease. The British Society of Echocardiography (BSE) has previously published a guideline document in order to facilitate high-quality echocardiography in the assessment of patients. This document is intended as an update to the previously published work.

This guide should be seen as supplementary to the BSE minimum dataset³. The intended benefit of this supplementary document is to:

- Support cardiologists, cardiac physiologists and clinical scientists to develop local protocols for the assessment of aortic valve disease.

- Promote quality by defining the optimal methodology in the assessment of aortic valve disease and linking this to the current evidence-base.
- Ensure that the management of patients with aortic valve disease is based around contemporary data and optimal echocardiographic assessment.

In some situations, this BSE guidance differs from the most recent European or American guidelines⁴⁻⁶. In those areas, these decisions were made in order to reflect contemporaneous data or as the result of differing interpretation. This guidance is divided into a number of subsections, which are listed in Table 1.

1. Anatomy

The aortic valve usually consists of three cusps, suspended within the aortic root, which together form a gate between the left ventricular outflow tract (LVOT) and the aorta. Each cusp is usually associated with a specific out pouching or 'sinus' of the aorta: the left and right coronary cusps (LCC; RCC) are associated with the left and right coronary sinuses respectively, which are the usual point of origin of the left and right coronary arteries. The third or 'non-coronary' cusp (NCC) is associated with a sinus from which no arteries arise. Two thirds of the circumference of the aortic root is attached to the muscular interventricular septum. One third of the aortic root, which corresponds with the majority of the non-coronary cusp and a portion of the left coronary cusp, forms a fibrous continuity with the adjacent mitral valve (called the aorto-mitral continuity)⁷. Using echocardiography, normal anatomy of the aortic valve and aortic root is depicted in Figure 1.

Variant anatomy

Bicuspid valve disease

Key points

- *The BSE recommend that bicuspid valves (BAV) be described as either 'antero-posterior (AP)' or 'right-left (RL)' orientation, with additional comment on the presence or absence of a raphe (see Figure 2)*
- *All patients with BAV should undergo a comprehensive assessment of the aorta to assess for dilatation and coarctation*
- *All patients with BAV should be offered echocardiographic surveillance*
- *Echocardiographic screening should be offered to first degree relatives of patients with BAV*

BAV has a prevalence of between 0.5-1%⁸⁻¹⁰. Identification of BAV is important as they are disproportionately responsible for more advanced valve dysfunction and are associated with aortic dilatation¹¹. The appearance and function of the valve at diagnosis are useful tools to inform discussions with the patient regarding prognosis and decisions concerning frequency of follow-up. Patients in whom the valve displays no thickening or calcification, and functions normally at baseline, have an excellent prognosis with fewer than 20% requiring aortic valve surgery over 20 years follow-up. Such individuals only require infrequent echocardiographic surveillance. Conversely, around 75% of patients with thickening, calcification or valve dysfunction will need surgery over a similar timeframe and therefore should be monitored more closely^{12,13}.

Differing classifications of BAV have been advocated in the literature, which means that comparisons and nomenclature are not standardized¹⁴⁻¹⁷. Importantly, there is no consensus as to associations between the sub-type of BAV and the pattern of valve dysfunction or aortic dilatation¹⁴⁻¹⁶.

Where there is uncertainty about the potential diagnosis of BAV, this should prompt review of any past echocardiographic images and consideration of advanced imaging techniques (i.e. TOE) to resolve the uncertainty, given the importance of the diagnosis for long-term prognosis.

Unicuspid and quadricuspid aortic valves

Key points

- *Unicuspid valves (UAV) may display advanced aortic stenosis in the absence of heavy calcification*
- *Patients with UAV and severe AS should be intervened upon according to standard indications in international guidance*

Less common anatomical variants are also recognized, which include quadricuspid or unicuspid aortic valves (QAV; UAV). Quadricuspid aortic valves are rare, with an estimated prevalence of <0.01%¹⁸. There is an association between QAV and aortic dilatation, and the predominant valve lesion is that of regurgitation, with stenosis a less frequent presentation^{18,19}.

The estimated prevalence of UAV is around 0.02%²⁰. Transthoracic (TTE) and transoesophageal echocardiography (TOE) are both highly specific for the identification of UAV, but are poorly sensitive, with unicuspid valves often mistakenly identified as bicuspid particularly in the presence of marked calcification²¹. Unicuspid valves are a disproportionate contributor to the overall burden of severe aortic stenosis, particularly in young individuals^{11,22}. An example of UAV is in Figure 3.

2. Calcification and aetiology of AS

Key points

- *Calcification is central to the development of aortic stenosis*
- *Echo studies should describe the pattern and burden of calcification*
- *Echo studies should identify thickening of cusps and restriction of motion*
- *In the absence of significant calcification, important aortic stenosis **should not** usually be considered*

There are three main aetiological factors contributing toward the development of AS within the UK. BAV is described above. Rheumatic heart valve disease is the most frequently seen worldwide but is rare in the UK. Rheumatic AS is characterized by calcification affecting the margins of the cusps and commissures, with relative sparing of the body of the cusps. Rheumatic aortic valve disease is almost never seen in the absence of mitral stenosis (MS)⁴.

The commonest cause of AS in the UK is age-related calcific degeneration of the valve, which is characterized by progressive thickening, fibrosis and calcification of

the aortic cusps. Such patients often display an abundance of calcification at the base of the cusps, whereas the commissures tend to be spared. Risk factors for calcific degenerative AS include hypertension, dyslipidaemia, smoking, diabetes and impaired renal function^{23,24}.

3. Haemodynamic principles of aortic stenosis

The normal aortic valve is compliant and opens fully, and presents almost no obstruction to blood flow out of the heart during systole. With worsening aortic stenosis, the valve becomes progressively more restricted, and consequently aortic valve maximal velocity (Vmax) and mean gradient (AVG) are correspondingly higher. Importantly, as blood approaches a fixed obstruction, it accelerates *prior* to the point of maximal obstruction, which has implications when estimating flow within the LV outflow tract (Figure 4)²⁵⁻²⁸. As blood accelerates, the jet additionally 'contracts' in order to fit through the narrowed aortic orifice²⁹. It may be assumed that once the jet has passed the valve it will immediately expand to fill the aorta, but in fact the jet continues to contract for a short distance, forming a vena contracta. This vena contracta represents the 'effective orifice area' which is always smaller than the 'anatomic' orifice area. This principle is important, as, whilst it is the *anatomical* valve area that is responsible for the flow obstruction, the *effective* orifice area is the key determinant of survival and long-term outcomes in patients with aortic stenosis (Figure 4)²⁹. Maximal AV velocity, mean gradient and the estimated aortic valve area (AVA) using the continuity equation all assess the haemodynamic impact of the *effective* orifice area and as such are useful for the determination of prognosis^{30,31}.

4. Standard echocardiographic images

In all patients with aortic valve disease, it is imperative that they undergo a complete and careful echocardiographic evaluation, according to the principles of the minimum dataset³. The specific windows and images required for the echocardiographic assessment of AS are described in Table 2 followed by a suggested reporting template in Table 3.

5. Essential parameters in the echocardiographic assessment of AS severity

Aortic valve maximal velocity and mean gradient

Key points

- *AV Vmax and mean gradient should be obtained in all patients undergoing the assessment of aortic valve stenosis*
- *The standalone or PEDOFF probe should be used in **all patients from multiple acoustic windows***
- *AV Vmax and mean gradient should be combined with the aortic valve area in order to describe AS severity*
- *BSE recommended methodology is demonstrated in Figure 5*

Maximal AV Velocity and mean gradient are both obtained using continuous wave (CW) Doppler interrogation of the aortic valve (see Figure 5)^{32,33}.

The simplified Bernoulli equation (Box 1) is a formula by which the maximal velocity across an aortic valve can be 'converted' to an equivalent pressure change. There is no specific benefit of describing a peak gradient defined using echo over and above

the maximal AV velocity, but an appreciation of the method is of value, as is an understanding of clinical scenarios in which CW Doppler may result in under- or over-estimation of AS severity.

The major challenge with CW Doppler is ensuring that the angle of insonation is fully aligned with the direction of the AS jet. A difference in alignment of more than 15-20° between the ultrasound beam and the direction of blood flow will result in significant underestimation of Doppler indices and the severity of AS^{27,32}. Sometimes this underestimation may be obvious to the sonographer, however, often traces may appear adequate only for further interrogation to demonstrate significantly higher values than first obtained (Figure 5).

Box 1

Simplified Bernoulli equation:

$$\text{Pressure difference} = 4 \times (V_2^2 - V_1^2)$$

Where V_2 is the velocity of blood flow across the obstruction, and V_1 is the velocity of blood flow prior to the level of obstruction. In most patients V_1 is relatively small ($\approx 1\text{m/s}$ or lower) and is therefore negligible in the context of high values of V_2 .

Consequently, the formula can be simplified further:

$$\text{Pressure} = 4 \times V^2$$

In circumstances where the sub-valve velocity is unexpectedly high (i.e. with small calibre LVOT dimensions or dynamic outflow tract obstruction), the longer equation (top) should be used.

Mean AVG is derived from an assessment of the average of the instantaneous velocities occurring during systole and is obtained from tracing around the CW Doppler waveform obtained through the aortic valve (see Figure 5). Calculating the mean AVG is complex and is not derived from the mean velocity, but is routinely performed by measurement packages pre-installed on imaging platforms. Deriving the mean AVG utilizes the Bernoulli equation, and as such there are two important considerations when obtaining and interpreting this parameter. Firstly, owing to the squared relationship between instantaneous velocity and gradient, any under-estimation of the CW Doppler waveform will lead to an exaggerated underestimation of the mean gradient. Secondly, in the case of sub-valve obstruction and increased LVOT velocity, both the mean gradient and maximal velocity will *overestimate* severity of valvular stenosis. Other methods to assess AS severity will need to be employed in this scenario.

Recommended methodology (Figure 5)

- **It is essential to use multiple echocardiographic windows.** Whilst in the majority of patients maximal values for AV Vmax and mean AVG are obtained from the apical window, in 20% of cases it is the suprasternal or right parasternal window that provides optimal results^{26,27}.
- The BSE recommends use of the PEDOFF or standalone probe **in all patients**.
- The traces should be optimized for gain and scale. Sweep speed should be set at 50-100mm/s.

- At least three beats should be averaged for patients in sinus rhythm with a minimum of 5-10 *consecutive* beats for patients in AF (see section 9 for details and alternative methodology).
- The dense outer edge of the spectral waveform should be traced. Transit time artefact (which appears as a spectral dispersion or ‘blurring’ at the peak of the curve) should be ignored and **not included** within the trace (Figure 5). The ‘reject’ function of the echo machine helps reduce transit time artefact and better delineate the modal signal.
- The shape of the CW waveform can provide an insight into the severity of AS. The CW curve in patients with moderate stenosis often has a rapid early peak, whereas severe AS will often display a slow acceleration with late peaking waveform⁴ (Figure 6).
- The echocardiographic report should include the AV Vmax, the mean gradient, the window and transducer with which the maximal values were obtained.

Aortic valve area

Key points

- *The effective aortic valve area, calculated using the continuity equation, should be obtained in all patients undergoing assessment of AS*
- *The AVA should be combined with the AV Vmax and mean gradient in order to describe AS severity*
- *The LVOT diameter should be measured at the **insertion point of the aortic cusps** and not below*
- *BSE recommended methodology is demonstrated in Figure 7*

The assessment of AVA is well validated using echocardiography and is an essential aspect of the comprehensive echocardiographic assessment of AS²⁵⁻²⁸. The continuity equation is used to estimate the AVA, and is outlined in Box 2.

Box 2

The continuity equation dictates that the volume of blood flowing through the LVOT *must be* the same as the volume of blood flowing through the aortic valve. We can calculate *stroke volume* in any conduit as the product of the velocity-time integral and the cross-sectional area (CSA) of the conduit. Using these two principles, we can derive the following formulae:

$$\text{Aortic valve stroke volume} = \text{LVOT stroke volume}$$

$$\text{AV VTI} \times \text{AV effective orifice area} = \text{LVOT VTI} \times \text{LVOT CSA}$$

Therefore:

$$\text{AV effective orifice area} = \frac{\text{LVOT VTI} \times \text{LVOT CSA}}{\text{AV VTI}}$$

The LVOT is assumed to be circular; therefore the LVOT CSA is replaced by:

$$\text{LVOT CSA} = \pi \times \left(\frac{\text{LVOT diameter}}{2} \right)^2$$

A 'simplified' continuity equation using velocity rather than the VTI is **not recommended** and is more prone to error, with a tendency to overestimate the calculated valve area²⁵.

Calculated AVA is useful as it is far less sensitive to alterations in transvalvular flow, and therefore will provide a more stable assessment of AS over a range of

haemodynamic states^{28,34,35}. Conversely, estimated AVA requires several detailed measurements and is therefore more susceptible to technical error.

In an ideal scenario, both the LVOT Velocity Time Integral (VTI) and the LVOT cross sectional area would be obtained *at the same anatomical level*. However, to all intents and purposes this is impossible. The two measurements are acquired from different echocardiographic windows, and so the sonographer can never be sure whether they are being obtained 'at the same point'. More importantly, there is significant axial motion (up to 1cm) of the aortic annulus during systole²⁵.

Additionally, as mentioned previously, blood flow within the LVOT accelerates prior to the stenotic valve within the zone of acceleration, which can extend up to 1cm from the anatomical annulus²⁵ (see Figure 4). As such, even if the cross-sectional area and VTI were obtained at the same anatomical level, it would not necessarily be truly representative of stroke volume.

Recommended methodology (Figure 7)

- Maximal AV velocity and mean gradient should be obtained using CW recordings as outlined in the previous section from multiple echocardiographic windows using the standalone probe. The maximal values obtained (an average of three beats) should be used in the continuity equation irrespective of which window the CW tracings were obtained from.
- The LVOT diameter should be measured **at the point of insertion of the aortic cusps**, using an inner-edge to inner-edge methodology from the parasternal long-axis window (**not** the apical windows). This recommendation differs from

historical practice whereby the LVOT has often been measured up to 1cm below the point of insertion of the cusps. This approach is no longer recommended by the BSE.

- Measuring the LVOT diameter at the point of cusp insertion improves inter-observer reproducibility, better corresponds to the 'true' AVA derived using invasive tools, and provides a more accurate assessment of the cross-sectional area, as the LVOT is usually circular at this anatomical level²⁵⁻²⁷.
- It is essential that all sonographers within a department use the same methodology to measure the LVOT diameter.
- In departments where the LVOTd was previously measured below cusp insertion, it is important to highlight to the referring clinician that the methodology has been updated. We would recommend that the report includes the following statement:
 - The AVA is now being estimated in accordance with updated BSE guidance 2021. Changes in the estimated AVA from previous studies should therefore be interpreted with caution.
- Care should be taken to exclude eccentric calcification from the measurement (see troubleshooting section below).
- The LVOT diameter **should not** be 'assumed' to be 2cm. Careful measurement of the LVOT diameter will provide a better assessment of true AS severity²⁷.
- For follow-up studies, it is important to note any changes in the measured LVOT diameter as this will dramatically impact on reported AVA. If there is a marked change in LVOT diameter, careful review of the previous and current study in

order to establish an accurate value is required. In such cases re-reporting the earlier study is essential in order to document interval change accurately.

- The PW trace should be obtained by placing the sample volume on the valve, at which point 'aliasing' will be noticed, reflecting rapid flow through the stenosed valve. The PW sample volume should then be slowly withdrawn apically until a suitable trace is obtained (Figure 7).
- The recordings should be optimized for gain and scale to improve accuracy. The sweep speed should be set between 50-100mm/s. Three consecutive waveforms should be measured and averaged for patients in sinus rhythm, with a minimum of 5-10 *consecutive* waveforms measured in AF (see section 9 for details and alternative methodology).
- LVOT waveform should have a well-demarcated, narrow band of recorded velocities throughout systole. If any spectral dispersion or transit time artefact ('blurring') of the trace is noted, the PW sample volume should be moved more apically (i.e. away from the valve).
- The process of obtaining PW traces should be repeated in both the apical 5- and 3-chamber windows. The maximal LVOT VTI obtained (as an average of three beats) should be used in the continuity equation.
- Patients in whom accurate assessment of the LVOT dimensions cannot be obtained (for example owing to poor echocardiographic windows) the calculation of AVA using the continuity equation should be abandoned, in which case other parameters should be used to determine AS severity.

Box 3: Common errors in assessment of AS

1. Failure to use PEDOFF probe from multiple acoustic windows including apex and right intercostal space.
2. Inaccurate assessment of LVOT diameter and cross sectional area
 - Calcification must be excluded
 - Measure LVOT diameter at the level of cusp insertion
 - Remember non-circular nature of LVOT
3. Poor positioning of PW sample volume.
4. Failure to image the ascending aorta and arch

Potential sources of error and troubleshooting

- Underestimation of maximal AV velocity and mean gradient owing to sub-optimal alignment of the Doppler transducer. This source of error will directly lead to an *underestimation* of AS severity.
- Underestimation of LVOT cross-sectional area. If the LVOT diameter is underestimated, this will lead to an exaggerated underestimation of the cross-sectional area owing to the squared relationship between the two. Eccentric calcification of the LVOT is a major source of error in this regard. This type of error will directly result in an *overestimation* of AS severity.

In many circumstances, the LVOT is elliptical rather than circular. The standard method of calculating the LVOT CSA will therefore significantly underestimate the true value, resulting in an *overestimation* of AS severity. On such occasions

direct planimetry of the LVOT cross-sectional area may improve accuracy (see section 12).

Examples of these sources of error are depicted in Figure 8-9.

- Positioning of PW sample volume:

The measurement of flow using PW Doppler is highly dependent on the position of the PW sample volume. If the sample volume is positioned too close to the valve, increased velocity from the zone of acceleration will be included. This will directly lead to an *underestimation* of AS severity.

Conversely, if the PW sample volume is moved too far apically (i.e. away from the valve and into the LV cavity), the obtained LVOT VTI will frequently underplay 'true' stroke volume and lead to *overestimation* of AS severity.

In cases where the LVOT is short, withdrawing the PW sample from the valve to obtain a suitable LVOT Doppler tracing may result in a rapid reduction in velocities. In this scenario, 3D imaging of the LVOT closer to the anatomical level at which the PW trace was recorded may improve accuracy (Figure 9).

6. Approach to the patient

Figure 10 describes the echocardiographic approach to classifying the severity of AS and identifying high-risk characteristics. This will allow the majority of patients to be consistently graded and ensure that important prognostic findings are highlighted to the clinician.

- The first priority in the assessment of AS is to ensure that the valve is both calcified and restricted. In the absence of either of these, significant AS is unlikely except in the (rare) circumstance of congenital AS.
- Next, ensure that a robust assessment of both maximal AV velocity and mean gradient have been obtained. If either the AV Vmax is $\geq 4\text{m/s}$ or the mean AVG is $\geq 40\text{mmHg}$, the patient should usually be considered as having severe AS. The rare exceptions to this are in circumstances in which there is temporary increase in flow such as tachy-arrhythmia or sepsis, in which case repeat assessment when the haemodynamic status has normalized should be considered.
- Once AV Vmax is noted to be $\geq 4\text{m/s}$ or the mean AVG is $\geq 40\text{mmHg}$, the focus of the study should then turn to assessing for the high-risk characteristics that define prognosis and may inform clinical decision-making (see Box 4 and section 10).
- If AV Vmax and mean AVG **do not** fulfil the criteria for severe AS, assessment of the AVA will usually confirm that the patient has non-severe AS (i.e. the AVA will be $\geq 1\text{cm}^2$). In this scenario the severity of AS should be defined using the AV Vmax or mean gradient (whichever is the greater; Table 4).
- If, however, the Vmax and/or mean AVG suggest non-severe AS but the AVA is $< 1\text{cm}^2$, further thought is required (Figure 10). It is imperative to re-check all measurements, in particular ensuring that the PEDOFF probe has been used from multiple echocardiographic windows. Assessment of the shape of the CW waveform may provide a clue as to the underlying severity (see Figure 6). For

individuals of small body habitus (i.e. a BSA $<1.7\text{m}^2$), use of the indexed AVA may confirm that the severity is moderate (see section 8 for details of indexed AVA).

- There is not a linear relationship between Doppler indices and the AVA. Often, the V_{max} or mean gradient will fall in the range of 3.5-4m/s or 35-40mmHg respectively, at which point the AVA will likely be between 0.8-1.0cm². Such patients are usually best treated as being 'moderate AS' but are often pragmatically reported as 'moderate to severe AS' to ensure that the advancing nature of the disease is highlighted to the clinician.
- If a marked disagreement between the Doppler indices and AVA remains, the next stage is to refer to 'special circumstances' (section 12). An MDT approach for challenging cases is advocated and ensures consistency within a department.

7. Grading of severity

Aortic sclerosis

Key points

- *Aortic sclerosis is defined as a thickened restricted aortic valve without significant obstruction to flow*
- *AV V_{max} is $<2.5\text{m/s}$*
- *Echocardiographic surveillance is not routinely recommended*

The prevalence of aortic sclerosis increases with age, and is associated with hypertension, renal disease, dyslipidaemia, and smoking²³. Approximately 2% of patients per year will progress from aortic sclerosis to aortic stenosis³⁶, and as such it is important to identify these patients so they can have any risk factors addressed. In some clinical scenarios surveillance may be considered, such as younger individuals with risk factors such as advanced renal dysfunction.

Mild, moderate and severe AS

Key points

- *Maximal velocity is the preferred measure with which to define AS severity*
- *The echocardiographic report should document the change in maximal velocity with time*
- *Echocardiographic surveillance is advised⁶:*
 - *Mild AS ($V_{max} < 3\text{m/s}$) repeated every 3-5 years*
 - *Moderate AS ($V_{max} 3\text{-}3.9\text{m/s}$) repeated every 1-2 years*
 - *Severe AS ($V_{max} \geq 4\text{m/s}$) repeated every 6 months*

A wealth of prospective data has demonstrated the association between AV V_{max} and cardiovascular events^{30,37-40}. Fewer than 30% of patients with an AV $V_{max} < 3\text{m/s}$ will need aortic valve intervention within 5 years of follow-up^{30,38}. If the AV V_{max} is between 3-4m/s, around half of patients will need surgery within 4 years. As the maximal velocity increases, so time-to-event decreases^{30,37,39}. AVA is a useful tool to assess AS severity, but there are relatively few studies in the literature demonstrating an independent association between adverse survival and AVA, with

most data suggesting that the AVA cut-off for predicting poorer outcomes is $0.8\text{cm}^{241,42}$.

In patients with heavily calcified valves, a change in AV Vmax of $>0.3\text{m/s/year}$ is associated with poor outcomes^{30,37}. Accordingly, the rate of change in AV Vmax should be documented in the echo report and can be calculated by dividing the AV Vmax change by the appropriate decimal (i.e. 6 months = 0.5). Changes in AV Vmax should only be interpreted if sequential studies obtained maximal velocity from similar echocardiographic windows. It is important to review previous studies and ensure that any change in AV Vmax is not related to the measurement of artefact.

Very severe AS

Key points

- *Very severe AS is defined as an AV Vmax $\geq 5\text{m/s}$ or a mean gradient $\geq 60\text{mmHg}$*
- *Patients with very severe AS have poor event-free survival even in the absence of symptoms.*
- *Such patients should be highlighted to the referring physician.*

Very severe AS describes patients who display either very high gradients or very small aortic valve areas, associated with particularly poor outcomes. Once the AV Vmax is $\geq 5\text{m/s}$, survival is reduced even in the absence of symptoms^{40,43,44}. Similarly, a mean gradient $\geq 60\text{mmHg}$ and an AVA $\leq 0.6\text{cm}^2$ are associated with extremely high event rates and largely correspond with an AV Vmax of 5m/s^{45-47} . American

guidelines advocate surgery in such patients even in the absence of symptoms (Class IIa indication)⁶.

The BSE discourages use of the term 'critical AS' as it is not clearly defined within the literature⁴⁸⁻⁵¹.

8. Additional parameters in the assessment of aortic valve stenosis

These additional parameters are not usually required in every patient, but occasionally may provide additional clues as to the severity of the AS, or may be of use in certain clinical scenarios.

Indexed aortic valve area

Key points

- *The indexed AVA (AVAi) is **not required in all patients***
- *An AVAi $<0.6\text{cm}^2/\text{m}^2$ is consistent with severe AS*
- *In individuals of small body habitus (i.e. a BSA $<1.7\text{m}^2$), the AVAi may re-classify some individuals as having moderate AS, potentially avoiding unnecessary intervention (see Figure 10)*
- *The AVAi **should be avoided** in patients who are overweight, where AVAi will overestimate AS severity*

Indexed aortic valve area was introduced in the 1960s to account for the large proportion of paediatric patients with AS⁵². AVAi is **not** superior to absolute AVA in the assessment of individuals and identification of high risk^{42,53}. Patients who are

considered to have severe AS solely on the basis of an AVAi (i.e. an AVAi of $<0.6\text{cm}^2/\text{m}^2$ but an AVA $\geq 1\text{cm}^2$) have significantly better outcomes than individuals in whom the absolute valve area is $<1\text{cm}^2$ ⁵³.

The AVAi should usually only be employed in individuals of small body habitus (i.e. a BSA $<1.7\text{m}^2$) in whom the AVA implies severe AS but where AV Vmax or mean AVG suggest the valve is non-severe (i.e. an AVA $<1\text{cm}^2$; Vmax $<4\text{m/s}$ and mean AVG $<40\text{mmHg}$): in such patients the AVAi may re-classify AS severity as moderate, thereby avoiding unnecessary intervention (see Figure 10)^{53,54}.

Dimensionless index

Key points

- *The Dimensionless Index (DI) is obtained from the ratio of LVOT: AV velocities. A value of <0.25 is consistent with severe AS*
- *The DI is useful when image quality prevents accurate assessment of the LVOT cross-sectional area*
- *If the LVOT cannot be measured accurately, DI may be used for serial studies to monitor progression of AS*

The DI removes one potential source of error (measurement of the LVOT cross-sectional area), but does not account for the true anatomy of the LVOT, and is usually less accurate than the AVA in the assessment of AS severity²⁵⁻²⁷. If parasternal windows are challenging such that accurate assessment of the LVOT

diameter cannot be obtained, the DI is useful, and may be used for surveillance.

Once the DI is <0.2 , outcomes are very poor, independent of the patient's BSA⁵⁵.

Planimetry

Key points

- *The BSE **does not recommend** routine use of planimetry*
- *If planimetry is to be pursued, TOE is the echocardiographic modality of choice, and 3D imaging improves accuracy*
- *Flow contraction means that planimetry **always underestimates AS severity** even if performed accurately (see Figure 4)*
- *Planimetry is **not reliable** in low-flow states as there is insufficient opening of the valve*

Planimetry is a technique whereby the anatomical orifice of the aortic valve is directly traced in order to provide an estimation of the AVA (Figure 11).

There are multiple pitfalls to this technique. The imaging plane must be aligned with the point of maximal stenosis of the valve. Identifying the aortic orifice is challenging in heavily calcified valves in which blooming artefact will result in potential overestimation of severity. Whilst planimetry is feasible and correlates with Doppler-based estimates of AS severity, the limits of agreement are poor which restricts the value of this technique in clinical decision-making⁵⁶⁻⁵⁸.

Energy loss index

Key points

- *The energy loss index (ELI) accounts for the pressure recovery phenomenon*
- *The BSE **does not recommend** routine use of the (ELI)*
- *An ELI $<0.6\text{cm}^2/\text{m}^2$ is consistent with severe AS*

As blood flows past an obstructed aortic valve, the velocity of blood increases, and static energy (or pressure) is converted into kinetic energy. This manifests as a pressure drop. As blood flow continues beyond the obstructed valve into the aorta, some kinetic energy is converted back into static energy and a proportion of pressure is restored. Standard echocardiographic parameters of AS severity do not incorporate the effect of the 'pressure-recovery' phenomenon.

The ELI is a way to calculate a 'corrected' valve area that accounts for pressure-recovery, which is reported after indexing for BSA⁵⁹. The ELI will only ever re-classify a valve as being *less severe* than suggested by standard Doppler indices. Use of the ELI has been validated in observational studies and a randomized trial and occasionally re-classifies the severity of observed stenosis, but overall performs no better than traditional measures of AS severity at identifying individuals at risk^{31,60,61}.

Patients with a mean AVG $>40\text{mmHg}$ should be considered as having severe AS and not re-classified as moderate AS using the ELI. The ELI may be considered in patients with low-gradient AS (i.e. an AVA $<1\text{cm}^2$; Vmax $<4\text{m/s}$ and mean AVG $<40\text{mmHg}$): in such scenarios, the ELI can identify a subset of individuals who are at lower risk and can afford to be observed^{60,61}. A worked example of the ELI is in Figure 12.

9. Other considerations

Atrial fibrillation or irregular rhythms

Key points

- *In patients with AF, average values from 5-10 **consecutive** beats are required to ensure accurate assessment of AS severity*
- *An alternative methodology is the matched R-R interval approach (Figure 13)*
- *LVOT VTI should **not be** derived from the inner envelope LVOT seen within CW tracings (Figure 13)*

For patients in AF, Doppler indices from at least 5 consecutive beats should be measured, from which the average AV maximal velocity, mean gradient and calculated AVA are derived⁴. There is mixed evidence in the literature as to the number of consecutive beats required, with some studies reporting that, on average, 13 consecutive beats are needed to approximate the true cardiac output for a patient with AF, whereas other work has demonstrated that there appears to be minimal variation of the calculated AVA in patients with varied R-R intervals^{62,63}.

An alternative method is to obtain Doppler recordings for AV VTI and LVOT VTI from matched cycle lengths. The method involves recording a single AV VTI measurement after a long R-R cycle, combined with a single LVOT VTI measurement obtained after a similar long R-R cycle length (where 'long R-R' is defined relative to the average heart rate; Figure 13). These two single measures can then be used in the continuity equation to derive the calculated AVA. This methodology has shown to correlate

highly with the traditional method of valve area calculation, with high degrees of reproducibility⁶⁴.

It is often possible to see an approximation of the LVOT trace within the continuous-wave Doppler recordings through the AV (Figure 13). These phantom tracings **should not be used** in the continuity equation as they systematically *overestimate* the calculated stroke volume as higher velocities from the flow convergence region are included within the trace, and would result in *underestimation* of severity of aortic stenosis using the continuity equation⁶³.

Blood pressure

Key points

- *Hypertension may lead to either over- or under-estimation of AS severity*
- *In challenging clinical situations AS should be re-evaluated after adequate control of BP: target of 130-140mmHg (systolic BP)*

Assessment of AS is challenging in patients with poorly controlled hypertension, owing to the complex inter-relationship between systemic BP, afterload, transvalvular flow and indices of AS severity. In one study, systemic vascular resistance was acutely increased through the use of infused adrenaline or isometric handgrip exercise, which led to a reduction in calculated aortic valve area, although mean pressure gradient was relatively unchanged⁶⁵. Conversely, an experimental study in pigs created a hypertensive state by banding the aorta, which resulted in an acute reduction in the mean pressure gradient combined with *increased* calculated

valve areas⁶⁶. Both these studies use experimental methods to mimic a hypertensive state and therefore are unlikely to reflect the vascular, morphological and haemodynamic alterations seen in patients with long-standing hypertensive heart disease. In fact, a study in which a circulatory model was used to examine the effect of blood pressure on Doppler indices of AS suggested that BP alterations *per se* did not lead to predictable changes in mean gradient or calculated valve area, but that alterations in transvalvular flow were responsible for the variations noted⁶⁷.

Poorly controlled hypertension in the context of AS is associated with worse survival⁶⁸. Historically, anti-hypertensive agents have been considered relatively contra-indicated in the presence of significant AS, but in fact most are tolerated well and appear safe⁶⁹. There is some evidence that calcium-channel blockers (CCBs) are associated with poorer outcomes and an adverse BP response to exercise^{70,71}. Therefore, it is reasonable to use alternative anti-hypertensive agents where feasible^{72,73}. In particular, ACE-inhibitors or other agents targeting the renin-aldosterone system are not only effective and well tolerated in AS, but improve long-term prognosis⁶⁹.

10. Additional prognostic markers

The following sections outline additional echocardiographic parameters that are useful in assessment of risk and clinical decision-making. These sections refer to patients in whom an **AV Vmax $\geq 4\text{m/s}$ and/or mean AVG $\geq 40\text{mmHg}$ have been obtained**. Box 4 lists the prognostic findings that should be highlighted to the referring clinician.

Box 4: Prognostic findings in severe AS (AV Vmax \geq 4m/s or mean AVG \geq 40mmHg)*Highlight to referring clinician*

1. Very high gradients (very severe AS): AV Vmax \geq 5m/s; mean gradient \geq 60mmHg
2. Rate of change of AV Vmax: heavily calcified valve with increase of $>$ 0.3m/s/year
3. Left ventricular ejection fraction $<$ 55%
4. Global longitudinal strain (GLS) $>$ -14; (GLS is encouraged but not mandated)
5. Increased indexed LV mass: $>$ 110g/m² (males) or $>$ 99g/m² (females)
6. High likelihood of pulmonary hypertension

Left ventricular ejection fraction*Key points*

- *LVEF should be assessed in all patients with aortic stenosis using quantitative methodology if possible*
- *Patients with severe AS (Vmax \geq 4m/s and/or mean gradient \geq 40mmHg) and an LVEF $<$ 55% should be reported as 'impaired LVEF' in the clinical report*
- *Patients with severe AS (Vmax \geq 4m/s and/or mean gradient \geq 40mmHg) with an LVEF \leq 35% should be reported as 'severely impaired LVEF with high likelihood of improvement after aortic valve intervention'*

Severe AS with a mean gradient \geq 40mmHg and an LVEF $<$ 50% is encountered infrequently in clinical practice^{74,75}. Usually this scenario reflects an afterload imbalance whereby inherent contractility is largely preserved, and LVEF will typically improve after aortic valve intervention^{51,76}. Such individuals are noted to have poor

outcomes without surgery and accordingly it is a Class I indication for aortic valve intervention^{5,6}.

Patients with an LVEF <55% have significant excess mortality compared to those in whom the LVEF is >60%, independent of whether surgery is undertaken⁷⁷. Outcomes for patients undergoing AVR with an LVEF between 55-60% may also be worse than those undergoing surgery with an LVEF>60%⁷⁵. Database analyses have suggested that rapid reduction in the LVEF of more than 10% per year appears to be associated with poorer survival in patients with asymptomatic severe AS⁷⁸.

Indexed LV mass

Key points

- *Indexed LV mass (LVMI) should be reported for all patients with severe AS*
- *LVMI should be estimated using the linear method from the parasternal long-axis window and indexed to BSA³*
 - *For males an LVMI >110g/m² is abnormal*
 - *For females an LVMI >99g/m² is abnormal*

Part of the adaptive mechanism of the left ventricle to an increased afterload is compensatory hypertrophy. This leads to normalization of wall stress and maintenance of cardiac output^{79,80}. Whilst there are mechanistic benefits of hypertrophy in patients with aortic stenosis, it is also recognized that excessive indexed LV mass can result in increased myocardial oxygen demand, myocardial fibrosis, and increased cardiovascular mortality^{81,82}.

Global longitudinal strain

Key points

- *Global longitudinal strain (GLS) may identify patients who are at an increased risk of cardiovascular events*
- *The BSE encourages the assessment of GLS in patients with AS where image quality allows*
- *Significant inter-vendor variability exists for GLS, but a value more positive than -14% is very likely indicative of LV dysfunction*

Early changes in LV performance may not result in reduction in measured LVEF, and yet will confer worse prognosis on such patients. Global longitudinal strain (GLS) derived using speckle tracking is a surrogate for the burden of LV fibrosis, and may allow the identification of early LV dysfunction^{83,84}.

GLS values are progressively more positive (i.e. less normal) as aortic stenosis severity worsens and are a strong predictor of cardiovascular mortality in patients with moderate or severe AS even after surgical intervention^{83,85-87}. A recent participant-level meta-analysis including over 1000 patients with significant AS and an LVEF >50% demonstrated that a GLS >-14.7% predicted poor survival in the overall cohort and amongst those individuals with an LVEF >60%⁸⁸.

Pulmonary hypertension

Key points

- *The echo report should include an assessment of the probability of pulmonary hypertension (PH) according to BSE guidelines⁹⁷*
- *A high likelihood of PH should be highlighted to the referring clinician*

There are relatively few published series in which echo-estimated pulmonary pressures have been examined in a cohort of patients with severe AS⁸⁹⁻⁹⁴. All are retrospective analyses, and deriving guidance is challenging, as a heterogeneous group of patients were included, many of who were already symptomatic or had other indications for intervention at the point of inclusion. Additionally, the echocardiographic methodology and threshold for defining important PH differed between reports, with some defining severe PH as an estimated PAP >50mmHg⁹¹⁻⁹³, whereas others considered the threshold of severe PH as a PAP >60mmHg^{89,90}. The most recent study used a methodology that attempts to reflect the current approach of estimating the probability of PH rather than directly estimating PAP⁹⁴. All reports are consistent in that higher values of PAP are associated with poorer long-term survival, but the threshold that should trigger intervention remains unclear. Consequently, the BSE approach of assessing the probability of PH is appropriate for the AS cohort, and those individuals with a high probability of PH should be highlighted to the referring clinician⁹⁵.

11. Additional echocardiographic imaging modalities

Trans-oesophageal echocardiography

Key points

- *TOE is rarely required for the assessment of AS*

- *If TTE is insufficient, Doppler interrogation using TOE may confirm the severity of AS*

TOE imaging windows are shown in Table 5.

TOE is rarely required to assess aortic stenosis, but has use in the assessment of patients for TAVI. 3D TOE can facilitate accurate measurements of the aortic valve annulus and important characteristics such as proximity of the left main stem, combined with an assessment of calcification, and has been shown to provide equivalent information to that obtained by cardiac CT^{4,96-99}. 2D TOE is not adequate for TAVI assessment as it may lead to undersizing of the TAVI implant owing to the elliptical nature of the LVOT and annulus^{99,100}.

Exercise stress echocardiography

Key points

- *The BSE does **not recommend** the routine use of exercise stress echocardiography for the assessment of AS*

Exercise testing (without echocardiography) is advocated in international guidance to unmask symptoms and identify patients with severe AS who may benefit from early intervention⁵. The value of exercise stress echocardiography is less clear-cut. Increases in the mean AVG and/or pulmonary pressures with exercise have both been examined in the context of severe AS, but there are contradictory reports as to whether they can identify patients at risk¹⁰¹⁻¹⁰⁴. Consequently, the use of exercise

stress echocardiography in asymptomatic severe AS is no longer recommended in international guidance^{5,6}.

12. Special circumstances

Low-gradient AS

Most of the time, the clinical approach outlined in Figure 10 and Section 6, will allow the sonographer to classify the severity of AS and identify and highlight any high risk features to aid decision-making.

However, in a significant minority of cases, the indices of aortic stenosis do not agree, which can present a challenge to the sonographer. There are several different reasons for this apparent disagreement (or *discordance*). The first is measurement error, and a priority when faced with such a scenario is to re-check all measurements and indices to ensure that accurate information has been obtained.

The second explanation is that there is not a linear relationship between AV Vmax, mean gradient and AVA (see below).

The final explanation relates to alterations in *flow*. Patients with reduced transvalvular flow will generate lower than expected Doppler indices for the observed severity of valve stenosis. The usual clinical example of this phenomenon is in the context of impaired LVEF, where poor systolic function means that gradients will be relatively low despite small aortic valve areas. This is *low-gradient AS with impaired LVEF*. In more recent times, it has been widely accepted that reduced

transvalvular flow can occur in patients with relatively normal LVEF (or at least an LVEF $\geq 50\%$). This scenario is *low-gradient AS with LVEF $\geq 50\%$* . The echocardiographic approach to patients is very different when the LVEF is impaired compared to when it is $\geq 50\%$, and therefore it makes sense to address these patient groups separately.

Low-gradient AS with LVEF $\geq 50\%$:

Key points

- *This is defined as an AVA $< 1\text{cm}^2$; an AVAi $< 0.6\text{cm}^2/\text{m}^2$; a mean AVG $< 40\text{mmHg}$ and an AV Vmax $< 4\text{m/s}$*
- *The BSE approach is summarized in Figure 14*
- *Technical error explains a significant proportion of such findings. Optimal assessment of CW Doppler, LVOT flow and LVOT cross-sectional area will lead to many patients being re-classified as moderate AS*
- *Adverse outcomes are related to the presence of higher mean gradients, lower absolute AVA, increased indexed LV mass and low stroke volume*
- *An MDT approach to resolve challenging cases is advocated*

Relationship between Doppler indices and AVA

There is not a linear relationship between AV Max, mean AVG and aortic valve area. The decision to make an AVA $< 1\text{cm}^2$ the cut-off for severe AS was largely arbitrary, and has led to a significant proportion of patients in whom the indices for severe AS apparently do not agree: prospective studies and large database analyses have shown that at least 25% of patients will have an AVA $< 1\text{cm}^2$, but a maximal AV

velocity (or mean AVG) that do not fulfil the criteria for severe AS. In fact, an AVA of 0.8cm^2 corresponds much better to the Doppler threshold of severe AS^{105,106}.

Given this knowledge, many 'challenging cases' can be resolved in a relatively straightforward manner. Very often the Vmax or mean gradient will fall in the range of 3.5-4m/s or 35-40mmHg respectively, at which point the AVA will likely be between $0.8\text{-}1.0\text{cm}^2$. In this scenario, the best study data supports such individuals as being labelled and treated as moderate AS^{5,30,38,41,42,107,108}. Pragmatically such patients are often reported as 'moderate to severe' AS which is reasonable as they are approaching the point at which intervention may be considered, and this terminology helps to identify the advancing nature of the disease to the clinician.

Where the apparent discrepancy is more overt: for example, if the mean AVG is $<35\text{mmHg}$ or AV Vmax is $<3.5\text{m/s}$ in the context of an AVA $<1\text{cm}^2$, more consideration is required.

Recommended approach (Figure 14)

- The first priority is to ensure that the valve is both heavily calcified and restricted. In the absence of these, significant AS is unlikely.
- Re-evaluation of CW Doppler indices is essential. A common error is failing to insonate using the PEDOFF or standalone probe from multiple acoustic windows, at the very least from both the apex and the right parasternal window. See section 5 for the optimal methodology for obtaining CW traces.

- The CW waveform can sometimes provide clues as to the severity of the AS. A late peak of the CW trace with slow upstroke may indicate that the valve is truly severely stenosed (Figure 6).
- Optimal assessment of the PW trace is essential. Subtle changes in the positioning of the PW sample volume can make a dramatic difference in the assessment of the AVA (see Figure 15).
- Consideration should be given to 3D planimetry of the LVOT cross-sectional area. The LVOT is often elliptical and the standard methodology of estimating the LVOT cross-sectional area will lead to an *underestimation* of stroke volume and an *overestimation* of AS severity using the continuity equation. Obtaining a 3D-image of the LVOT and directly tracing the LVOT cross-sectional area results in a substantial proportion of low-gradient severe AS patients being re-classified as moderate AS¹⁰⁹ (see Figure 9).
- If the above does not resolve the apparent discrepancy, the next stage is to evaluate the stroke volume index (SVi).
- An SVi $\geq 35 \text{ ml/m}^2$ is considered 'normal', whereas an SVi $< 35 \text{ ml/m}^2$ is considered 'low'¹¹⁰.
- Patients with low-gradient AS and **normal SVI** ($\geq 35 \text{ ml/m}^2$) have a prognosis similar to conventional 'moderate AS' and can usually be safely observed¹⁰⁸. Prospective studies have shown that even in the presence of minor symptoms, such patients can have aortic valve intervention safely deferred until the mean AVG exceeds 40 mmHg ¹⁰⁹.

- With **low SVi** ($<35\text{ml/m}^2$), it is considerably more challenging to differentiate patients with truly-severe AS from those with non-severe AS. Additional 'clues' need to be obtained from the echocardiographic study in order to inform decision-making as to whether such patients are at lower or higher risk (Figure 14).
 - - The presence of very low mean AVG ($<30\text{mmHg}$ and certainly $<25\text{mmHg}$) makes severe AS unlikely¹¹¹⁻¹¹³.
 - - A mean gradient $>30\text{mmHg}$ and certainly $>35\text{mmHg}$ makes severe AS likely^{114,115}.
 - The presence of increased indexed LV mass makes AS more likely¹¹⁵.
 - An AVA $<0.8\text{cm}^2$ makes severe AS more likely¹¹⁵.
 - Clinical interpretation is important amongst this cohort. The presence of additional valve lesions, the presence of intrusive symptoms, clinical examination and co-existent coronary disease may influence decision-making.
 - An MDT approach should be considered for challenging cases.
 - Although there are no prospective studies using CT calcium scoring to help identify true-severe AS amongst this cohort, CT may provide complimentary data to support clinical decision-making.
- Some studies have supported the value of the valvulo-vascular impedance (Zva). Higher values of Zva are associated with poor cardiovascular outcomes, although

when co-morbidities are accounted for, the discriminatory value of Zva is limited and it is not useful in identifying patients who benefit from aortic valve intervention. Consequently, the BSE **does not recommend** Zva for routine use.

- Most patients with low-gradient AS will demonstrate progressive increase in AV Vmax and mean AVG with time and therefore warrant close clinical and echocardiographic follow-up.

Flow rate assessment

There is increasing interest in the use of flow rate (FR) in aortic valve disease. Whilst FR shows promise, the current literature is insufficient to make robust guidance regarding its use in the cohort of *low-gradient AS with LVEF $\geq 50\%$* . Assessment of FR has theoretical benefits over the assessment of static volumes (i.e. the stroke volume index), but a lack of prospective studies means that, at the moment at least, it is not clear how patients should be managed if AS severity is defined according to the FR. It is not entirely clear what threshold of FR should be considered as normal, and given that FR is a non-indexed parameter, smaller individuals will necessarily have lower FR than larger individuals. Therefore the BSE currently **does not recommend** routine use of FR although acknowledges that it is an area of increasing interest.

Complimentary imaging modalities – Cardiac CT

The use of CT in paradoxical low-gradient AS is reasonable, although there are no studies in which it has been used to guide intervention. It is important to appreciate

that significant valve obstruction may occur even in the absence of significant calcification, particularly in bicuspid or unicuspid valve disease. Finally, there is a large 'grey zone' of calcium scoring in which decision-making is not clear¹¹⁶.

Low-gradient AS with impaired LVEF:

Key points

- *This is defined as: an AVA <1.0cm²; an AVAi <0.6cm²/m²; a mean gradient <35mmHg; and an LVEF ≤40%*
- *The BSE approach is summarized in Figure 16*
- *After exclusion of technical error, such patients should be considered for dobutamine stress echocardiography (DSE)*
- *Conventional DSE and projected EOA should be combined in order to identify patients who may benefit from intervention*
- *CT calcium scoring can be considered if DSE provides an indeterminate result.*
- *An MDT approach to resolve challenging cases is advocated*

Background

In patients with a low cardiac output, recorded values for Vmax and mean gradient are lower than expected for the observed severity of AS, which could lead to individuals with severe AS being missed^{27,28,34,35}. As the continuity equation is less flow-dependent than measured Vmax and mean gradient, it may be expected that an absolute AVA <1.0cm² would reliably identify patients with severe AS^{28,34}.

Unfortunately, this is not the case. Whilst flow has minimal effect on the calculated valve area of *severely* stenotic valves, if a valve is only moderately stenotic, it retains

a considerable degree of compliance. A moderately stenotic valve will open relatively little in the presence of low stroke volume (and therefore have a small calculated valve area), but as cardiac output increases, the leaflets will open further, resulting in aortic orifice area that can be 30% larger^{34,35,117}. Therefore an AVA <1.0cm² is very sensitive but not sufficiently specific in differentiating *truly* severe aortic stenosis from a valve that is only moderately stenotic but *appears* severe owing to poor cardiac output (or *pseudo-severe*).

DSE has been widely used and validated in this scenario to identify patients who may benefit from aortic valve intervention^{50,117-121}. It is important to note exercise echocardiography **does not** elicit adequate augmentation of cardiac output and therefore **should not** be used in *low-gradient AS with impaired LVEF*¹²².

Patient selection

DSE should usually be considered in patients with an AVA <1cm²; an AVAi <0.6cm²/m²; a mean gradient <35mmHg and an LVEF ≤40%. Patients with an LVEF ≤40% but in the presence of high gradients (i.e. a mean AVG ≥35mmHg) should be considered for intervention without recourse to stress echocardiography.

The BSE has diverged from international guidance with regards patient selection for DSE. Both American and European guidance advocate the use of DSE in patients when LVEF is up to 50%, although ESC guidance includes a caveat regarding stroke volume^{4,6}. The BSE has chosen not to advocate this approach on the basis that in the

published literature essentially all patients undergoing DSE for low-gradient AS were observed to have an LVEF $\leq 40\%$ (and very often $\leq 35\%$).

Patients with an LVEF 41-49% but who do not fulfil all the criteria for severe AS therefore represent a challenging subset in which there is almost no data in the literature to provide robust guidance. The first priority is to re-evaluate the study to identify any technical error and confirm that the LVEF is not $\leq 40\%$ (in which case DSE would usually be considered). Clearly a degree of clinical pragmatism is often employed in these scenarios: if a patient has an LVEF slightly higher than 40%, with an AVA $< 1\text{cm}^2$ but low mean gradient, it may be considered reasonable to undertake DSE. Conversely, a patient with an LVEF closer to 50%, with mean gradients of nearly 40mmHg would usually be considered as having severe AS and DSE would not be warranted. Other clues such as the shape of the CW waveform may help to identify when a patient has severe vs. non-severe AS (Figure 6). There is some limited data in the literature regarding the use of flow rate (FR) in patients with an LVEF between 41-49%. FR is obtained by dividing the stroke volume by the ejection time (see Figure 17 for an example of how to calculate FR). If FR is $\geq 200\text{ml/s}$, the AVA appears to be an accurate assessment of AS severity and therefore such patients may be considered as having severe AS¹²³.

Finally, the clinical scenario may influence decision-making: for example if the patient was already being worked up for coronary revascularization, a heavily calcified aortic valve with at least moderate stenosis would usually warrant intervention thereby obviating the need for further detailed assessment of the valve.

This re-iterates the central role of the clinical MDT in decision-making for challenging or borderline cases.

Conventional Dobutamine Stress Echocardiography

Contractile reserve

Most individuals demonstrate an improvement of $\geq 20\%$ in stroke volume with DSE, in which case they are considered to have 'contractile reserve'. In these patients, repeating the assessment of the aortic valve at peak stress may demonstrate one of the following responses:

True-severe AS (TS-AS): A mean gradient that increases to $\geq 40\text{mmHg}$, combined with an aortic valve area that remains $< 1\text{cm}^2$. Such patients have improved survival with AVR, whereas medical therapy results in dismal outcomes^{50,118}.

Pseudo-severe AS (PS-AS): The largest series (still only 29 patients) defined PS-AS as patients with an AVA at peak stress of $\geq 1.2\text{cm}^2$ combined with a mean gradient $< 40\text{mmHg}$ ¹²¹. Such individuals appear to have outcomes similar to those of matched controls with LV impairment but without valve disease¹²¹. Despite being somewhat larger than the usual cut-off for severe AS, an AVA 1.2cm^2 as a threshold for defining individuals with good outcomes under medical therapy is consistent with results from the TOPAS series (see below)^{117,119}.

No contractile reserve

In around one third of patients, the stroke volume does not increase by $\geq 20\%$, i.e. there is no evidence of contractile reserve. In this circumstance, conventional DSE does not readily allow the clinician to differentiate TS-AS from PS-AS. Patients without contractile reserve demonstrate high peri-procedural mortality^{118,120,124}, but routine medical therapy in such patients results in even worse survival¹²⁰. Recent work from the TOPAS registry (see more below) indicate that individuals without contractile reserve have similar medium-term survival to those patients with contractile reserve after undergoing TAVI^{125,126}. Given the increasing use of TAVI, with its associated reduction in peri-procedural risk, there is a clinical need to improve decision making within this cohort in particular.

Very low resting mean gradient

Very low resting mean gradients are strongly associated with high peri-operative mortality and apparent lack of benefit of aortic valve intervention^{118,120}. Therefore 'truly-severe' AS should be considered very unlikely in patients with resting mean aortic valve gradients of $< 20\text{mmHg}$, and decisions to proceed to intervention made in an MDT environment.

Projected flow area

In addition to the challenge of interpreting echo findings in patients without contractile reserve, a major difficulty with conventional DSE is that the contractile response of individual patients varies widely. For example: one patient may demonstrate a 50% increase in stroke volume, from 40mL to 60mL, whereas a different patient may only display a 20% increase, from 40mL to 48mL. Both would

be labelled as having 'contractile reserve', but it is obvious that the aortic Doppler indices obtained at peak stress would likely be very different, with only the first patient in the example improving stroke volume to that approaching normal.

Projected flow area (EOA-Proj) is a concept whereby the clinician can use data obtained during DSE to predict what the aortic valve area *would be* at a 'normal' transvalvular flow rate. EOA-Proj was developed to help standardize the interpretation of DSE, and improve decision-making in patients without contractile reserve^{117,119,125,126}.

Methodology

EOA-Proj relies on the fact that an increase in transvalvular *flow rate* (and not just absolute stroke volume) will lead to changes in mean gradient and valve area³⁴. If an individual undergoing DSE does not increase the transvalvular flow rate by $\geq 15\%$, the EOA-Proj is considered inaccurate and should not be used^{117,119}. See Figure 17 for a worked example.

Results of EOA-Proj

An EOA-Proj of $< 1.0\text{cm}^2$ is best at identifying TS-AS, and outperforms other resting and stress echo criteria^{117,119}. Only individuals with an EOA-Proj of $> 1.2\text{cm}^2$ performed well without AVR, consistent with the definition of PS-AS (above).

Indeterminate result

If conventional DSE does not elicit a contractile response, and the result of projected flow area is 1-1.2cm² and/or the flow-rate fails to augment by $\geq 15\%$, the DSE outcome is indeterminate. In this scenario decision-making should be made in an MDT environment and complimentary imaging should be considered (see below).

Complimentary imaging modalities – Cardiac CT

There is increasing interest in the use of cardiac CT in defining severity of AS and in particular scenarios where discordant indices are obtained^{116,127,128}. The reported experience of a CT approach in patients with *low-gradient AS with impaired LVEF* is relatively small (fewer than 100 individuals in total), and aortic valve intervention was not guided by the results of CT findings.

The value of a 'negative' CT calcium score within this cohort is not clear. CT cut-offs have been defined in order to identify patients who likely have an AVA <1cm²: However, the optimal threshold for pseudo-severe AS is 1.2cm², on the basis that this higher AVA threshold identifies patients who perform well under medical therapy alone^{117,121}. Using the standard CT threshold for severe AS therefore would risk some individuals being refused potentially beneficial intervention. As such, the BSE advises caution in the use of CT calcium scoring in the setting of *low-gradient AS with impaired LVEF*, and recommends that CT be employed only if DSE provides an indeterminate result.

High gradient high valve area

Key points

- *High gradient-high valve area (HGHA) is defined as patients with a mean gradient ≥ 40 mmHg, and an AVA ≥ 1 cm²*
- *HGHA is rarely seen in routine practice*
- *The HGHA cohort should be carefully assessed for measurement error, particularly regarding the LVOT cross-sectional area*
- *HGHA patients should be considered as having severe AS*

The clinical scenario where Vmax and mean AVG are high (implying severe stenosis) but AVA > 1 cm², consistent with only moderate AS, is seen rarely, with an estimated prevalence of 1%¹⁰⁵. To the BSE's knowledge, there has been no systematic echocardiographic analysis of such patients, with current guidance based upon findings from CT studies. All HGHA patients have high CT calcium levels, and accordingly current guidelines suggest that such patients should be treated as severe AS^{4,116,128}.

13. Combined valve disease

There is a paucity of data in the literature regarding multiple valve disease, despite the fact that the combination of one or more valve lesion occurs relatively frequently^{2,129,130}. The over-riding principle is that there should be a comprehensive assessment of all valvular lesions, evaluated according to specific guidance.

Aortic stenosis and aortic regurgitation

Key points

- *When both AS and aortic regurgitation (AR) are at least moderate in severity, the lesion should be reported as 'mixed aortic valve disease'*
- *AVA is **not a useful marker of prognosis** in mixed aortic valve disease*
- *Grading of mixed aortic valve disease should be guided by the AV Vmax:*
 - *Moderate mixed aortic valve disease (Vmax 3-3.9m/s)*
 - *Severe mixed aortic valve disease (Vmax 4-4.9m/s)*
 - *Very severe mixed aortic valve disease (Vmax \geq 5m/s)*

Mixed aortic valve disease is a commonly encountered clinical scenario, partly as the dominant causes of aortic stenosis are similarly important aetiological factors in aortic regurgitation (AR)⁴.

In the case of mixed aortic valve disease, reporting the severity is challenging. For example: the rationale for describing a valve lesion as 'moderately severe' is that it provides the clinician with information as to the likely prognosis. An echocardiographic report stating 'moderate AS and moderate AR' may be deceptive, as the prognosis of this combination of valve lesions is more in keeping with isolated severe AS¹²⁹.

Some principles are important. Mild AR does not impact upon the assessment of aortic stenosis. However, as the severity of AR increases, the stroke volume will also become larger. AV Vmax and mean gradient are proportional to stroke volume, and therefore in the presence of moderate or worse AR, higher values of AV Vmax and mean gradient will be observed relative to the aortic valve area. Given that the

assessment of AVA using the continuity equation corrects for alterations in flow, it may be assumed that AVA is a better tool in the assessment of AS in the context of co-existent AR.

In fact, the prognosis of patients with combined AS and AR is far more closely linked to the maximal AV velocity, which reflects the overall haemodynamic load on the left ventricle¹²⁹. In patients with mixed AV disease, event-free survival is the same for those individuals with a calculated AVA of $<1\text{cm}^2$ as it is for patients with an AVA between $1\text{-}1.5\text{cm}^2$, whereas there is a step-wise deterioration in outcomes as AV Vmax is seen to increase¹²⁹. The average time-to-event with mixed aortic valve disease closely resembles the event curves of lone AS when patients are divided according to AV Vmax^{30,38,39,129}. The conventional approach of intervening on the valve when the patient fulfils an accepted guideline criteria for surgery (for either AR or AS) appears appropriate and does not result in excess mortality¹²⁹.

Aortic stenosis and mitral regurgitation

Key points

- *With combined AS and mitral regurgitation (MR) a detailed assessment of both valve lesions is mandatory*
- *In the presence of severe MR, AV Vmax and mean gradient may underestimate the severity of AS*
- *AVA is a more accurate assessment of AS severity in the presence of significant MR*

- *If co-existent MR severity is more than mild, TOE is recommended to clarify the severity and mechanism of mitral regurgitation*

The combination of AS and mitral regurgitation (MR) is seen frequently, particularly in older populations¹³⁰. In the case of severe MR, forward stroke volume will be reduced. This may lead to an underestimation of AS severity when relying on the Vmax and mean gradient, whereas AVA is more reflective of true AS severity.

In such patients a comprehensive assessment of both valve lesions should be completed. Timing of intervention is informed by international guidelines^{5,6}. In particular a detailed assessment of the mechanism of mitral regurgitation should be obtained as this may provide clues as to whether the MR will improve simply by intervening on the aortic valve, or whether dual valve intervention is needed¹³⁰.

Aortic stenosis and mitral stenosis

Key points

- *Co-existent severe MS may result in an underestimation of AS severity using AV Vmax and mean gradient*
- *AVA is a more accurate assessment of AS severity in the presence of significant MS*

Patients with severe mitral stenosis will have low stroke volume, and the presence of severe MS is a well-recognised cause of low-gradient AS. The AVA provides a better assessment of true AS severity in this scenario¹³¹. In patients undergoing surgery for

MS it is recommended that detailed assessment of the aortic valve be completed to ensure that low-gradient AS is not present, which may necessitate aortic valve replacement at the time of surgery.

14. Aortic stenosis and amyloid

Key points

- *There is an important association between amyloid and advanced AS in older patients*
- *Patients with combined amyloid-severe AS still derive benefit from AV intervention*
- *Echocardiographic features of amyloid including high LV mass and changes in GLS are **not specific for amyloid** in a population of severe AS*

Recent work has demonstrated an important association between aortic stenosis and cardiac amyloid in an older population¹³²⁻¹³⁵. Whilst the overall prevalence of cardiac amyloid in individuals over 80 years of age is considered to be around 3%, in prospective studies of patients with severe AS referred for TAVI, the observed prevalence of amyloid was considerably higher, with estimates varying between 13-16% of such cases^{133,135}.

The value of echocardiography in identifying patients with combined amyloid-severe AS is not clear. GLS is frequently low in such patients but the pattern of 'apical sparing' is not specific for amyloid in this cohort and is often seen in individuals with isolated severe AS^{133,135}. Consistently, average mitral annular S' appears to be lower,

and LV mass marginally higher in patients with combined amyloid-severe AS. Non-echo findings that may hint toward the existence of amyloid include the presence of RBBB on the ECG and raised biomarkers. Owing to the prevalence of abnormal myocardial systolic and diastolic function in older patients with advancing AS, no echocardiographic or clinical feature can be considered as a reliable method to differentiate a patient with combined amyloid-severe AS from someone with isolated severe AS^{133,135}.

An early retrospective analyses suggested that patients with combined amyloid-severe AS had worse survival than equivalent patients with isolated AS¹³². However, recent prospective studies in which all participants referred for TAVI underwent diagnostic testing have shown that individuals with combined amyloid-severe AS do not have demonstrably poorer survival and derive as much benefit from aortic valve intervention as those individuals with isolated severe AS^{133,135}.

The caveat is that these recent works have only screened patients with severe AS who were referred for consideration of intervention. The prevalence, pattern, and outcomes of patients with non-severe AS combined with amyloid is not well established.

Therefore, the approach advocated throughout this guideline should be followed in all patients. The primary focus should be toward optimization of the echocardiographic assessment and classifying the severity of AS, before identifying any high-risk characteristics. All patients should undergo a comprehensive

echocardiographic assessment according to the principles of the minimum dataset³.

Whilst the classical echocardiographic features of amyloid may not be specific for the disease in patients with severe AS, when aortic stenosis is mild or even moderate, the usual echocardiographic approach for identifying infiltrative disease is appropriate.

Figure Legends:

Figure 1: Normal anatomy. Parasternal long axis window (a and b), with zoom images (c and d). M-mode recording of the aortic valve should be obtained with the cursor perpendicular to the axis of the aorta (e). Normal M-mode trace (f): note central closure line (labelled). Anatomy of the aorta (g). Image (h) marks the insertion of the cusps (red dotted line) and sino-tubular junction (green dotted line). Parasternal short axis window at the level of the aortic cusps (images i and j). Image (k) represents a zoomed image of the aortic valve during systole with the three cusps labelled. In image (l), the lines represent potential parasternal long axis imaging planes. Whilst both transect the right coronary cusp, it is evident that a subtle change in angle of the transducer will lead to inclusion of either the non-coronary cusp (red dotted line) or left coronary cusps (green dotted line).

Figure 2: Bicuspid aortic valve. In the top panes there are images of a bicuspid valve with right-left (RL) configuration (annotated; systole (a) and (b) diastole). Images (c) and (d) depict a bicuspid valve with anterior-posterior configuration (AP) with a raphe in the anterior cusps (marked with asterisk). M-mode recording of a bicuspid valve with AP configuration (e): note eccentric closure line (marked with asterisk). Image (f) depicts a calcified aortic valve obtained using TOE, which appears tricuspid. Colour Doppler is applied in image (g) and demonstrates a 'crescent-shaped' opening indicating this is a bicuspid valve (AP configuration with raphe).

Figure 3: Parasternal long axis window of a unicuspid aortic valve during diastole (a) and systole (b). Note the marked 'doming appearance' during systole. Parasternal short axis window during diastole (c) and systole (d): note how the orifice is eccentric. This valve has minimal calcification and retains mobility. Image (e) represents CW Doppler through the unicuspid valve. There is obstruction to flow despite the lack of calcification.

Figure 4: Haemodynamic considerations of AS. In a patient with severe AS, blood flow accelerates prior to the valve (flow acceleration region marked). The jet contracts in order to fit through the *anatomical orifice* and continues to contract for a short period, forming the *effective orifice*. Doppler indices of AS measure the severity of obstruction at the level of the *effective orifice*. In the ascending aorta, there is a degree of 'pressure recovery'.

Figure 5: Assessment of maximal AV velocity and mean gradient using CW Doppler. CW tracings should be obtained from multiple echocardiographic windows: suprasternal window (a), with corresponding Doppler in (b); subcostal (c) and (d); apical 5-chamber (e); and stand-alone probe from the right parasternal window (f). Note that the AV Vmax in (e) represents significant underestimation of maximal velocity when compared to that obtained using the standalone probe (f). Images (g) and (h) demonstrate spectral dispersion of the CW Doppler trace (marked with an asterisk). The mean gradient is obtained from tracing around the dense part of the CW Doppler curve. In images (i) and (j), the CW trace has been optimised: in (i) some spectral dispersion remains, but this has been completely eliminated in (j), resulting in an ideal CW trace.

Figure 6: Comparison of the shape of the CW waveform. On the left, a patient with moderate AS: note how there is a rapid acceleration and an early peak. For comparison, the patient on the right has severe AS. There is a slower acceleration with a late peak. The shape of the CW waveform is maintained irrespective of LVEF and therefore it may be useful to help identify severe AS in difficult scenarios such as low-gradient AS.

Figure 7: Optimal assessment of the LVOT Doppler. The PW Doppler sample volume should initially be placed on the aortic valve (a), which will usually result in aliasing. It should then be slowly moved apically (i.e. away from the valve; images b and c). In (c) there is a wide

area of density at the apex of the trace, evident in the zoomed image (e; marked with asterisk). This represents blood flow within the zone of acceleration immediately proximal to the valve, and **should not** be included, as it would result in an *overestimation* of LV stroke volume and an *underestimation* of AS severity. In (d), (f), (g) and (h) the trace has been optimised further and depicts ideal assessment of LVOT Doppler. When tracing the curve, any spectral dispersion should be ignored (marked in (g) with a +). Three traces should be obtained and averaged for use in the continuity equation, with sweep speed set between 50-100mm/s (h)

Figure 8: Eccentric calcification can lead to important underestimation of LVOT diameter, here demonstrated with 3D imaging. Figure (a) depicts a long-axis view obtained during TOE with LVOT diameter marked (red dotted line). Picture (b) is an image of the LVOT taken at an orthogonal plane to image (a). Note that the LVOT diameter is an underestimate owing to two areas of eccentric calcification (marked). Adjustment of the imaging plane can remove calcification from the image (c), with the optimal LVOT diameter now shown (red dotted line in images c and d).

Figure 9: Error arising from assumption of circular LVOT. Image (a) depicts a long-axis view of the aortic valve obtained using 3D TOE. The LVOT diameter has been measured 2cm proximal to the valve (red dotted line). Image (b) is a short axis image obtained at this anatomical level. Estimation of the LVOT cross-sectional area at this point calculates the area of the red dotted circle, and is a huge underestimate of the 'true' LVOT area (marked by blue dotted outline). The LVOT should be measured immediately below the insertion of the aortic cusps (c; green dotted line). Image (d) depicts the short axis view at this anatomical level: note the LVOT demonstrates a much more circular profile. Estimation of the LVOT area using $\pi (LVOTd \div 2)^2$ would calculate the area of the green dotted circle, which is much closer to

the 'true' LVOT area (blue dotted line). On occasion, direct planimetry of the LVOT cross-sectional area using 3D echo can be considered, particularly for difficult cases (see low-gradient AS, section 12).

Figure 10: Decision-aid to guide assessment of aortic stenosis.

Figure 11: Planimetry using 3D TOE. A 3D volume of the aortic valve is obtained (a). The volume can be manipulated to display orthogonal planes. Image (b) depicts a long-axis view, and the dotted red line depicts the plane from which a short axis view (c) is then shown. This plane is aligned with the point of *insertion* of the valve cusps. In (d), the image has been manipulated, and the 'plane of interest' moved further into the aorta such that it now aligns with the valve tips (dotted green line). The short axis window obtained at the level of the dotted green line is displayed in image (e). Planimetry obtained in image (c) clearly *overestimates* aortic valve orifice area when compared to the result obtained by planimetry in image (e).

Figure 12: Worked example of the energy-loss index (ELI):

- From the image (a), the LVOT cross-sectional area can be calculated:

$$LVOT\ CSA = \pi \times (LVOTd \div 2)^2 = 3.5cm^2$$

- The cross-sectional area of the ST junction (STJ) depicted in image (b) is:

$$STJ\ CSA = \pi \times (STJ\ diameter \div 2)^2 = 6.6cm^2$$

- Using the CW trace in image (c), AV Vmax is 3.1m/s; mean gradient 27mmHg; AV VTI 55cm. Using the PW trace in image (d), LVOT VTI is 14cm.

- Aortic valve area using the continuity equation is:

$$AVA = LVOT\ VTI \div AV\ VTI \times LVOT\ CSA = 14cm \div 55cm \times 3.5cm^2 = 0.9cm^2$$

- After indexing for BSA (1.7m² in this patient), the AVAi is 0.51cm²/m²

- This is an example of low-gradient AS whereby both the AVA and AVAi suggest *severe* stenosis yet the AV Vmax and mean gradient only suggest *moderate* stenosis.

- The energy-loss index is defined as:

$$ELI = (AVA \times STJ \text{ CSA}) \div (STJ \text{ CSA} - AVA)$$

$$ELI = (0.9 \times 6.6) \div (6.6 - 0.9) = 1.04 \text{ cm}^2$$

$$\text{Indexed for BSA} = 0.61 \text{ cm}^2/\text{m}^2$$

- An ELI $<0.6 \text{ cm}^2/\text{m}^2$ is consistent with severe AS, therefore this patient has been re-classified as moderate AS when accounting for the pressure-recovery phenomenon.

Figure 13: Assessment of Doppler indices and AVA in AF. Doppler traces obtained from a patient in AF (a and b): note marked beat-to-beat variations of the CW and PW waveforms. Conventionally, at least 5-10 *consecutive* CW and PW traces are obtained for assessment of valve indices (a and b). An alternative method is the ‘matched R-R interval’ approach: in image (c) the R-R interval is seen as 600ms, and the CW waveform is traced. In image (d) a comparable PW waveform is found, whereby the R-R interval is noted to be 607ms, and is therefore traced. The obtained values from these comparable CW and PW traces can be used in the continuity equation. Within CW traces it is possible to appreciate a ‘phantom’ LVOT trace (e). The true LVOT trace is displayed in image (f) for comparison. This phantom trace **should not be used** for the continuity equation, as it will directly lead to an *underestimation* of AS severity.

Figure 14: Summary of recommendations for low-gradient AS with LVEF $\geq 50\%$.

Figure 15: Example of technical error resulting in low-gradient AS. A patient was noted to have calcified restricted aortic valve. The LVOTd is 2.0cm (not shown). The LVOT cross sectional area is 3.14 cm^2 . PEDOFF values from the apical 5-chamber window demonstrate

an AV Vmax 3.5m/s; mean gradient 30mmHg; AV VTI 71cm (a). If the PW sample volume is placed as in image (b), corresponding Doppler traces are shown in (d). This leads to an estimated AVA of 0.8cm², consistent with low-gradient severe AS. In image (c), the PW sample volume has been moved closer to the valve, with corresponding Doppler trace in (e): note the amplitude of the traces is significantly larger. This leads to an estimated AVA of 1.1cm², consistent with moderate AS.

Figure 16: Summary of recommendations for DSE in low-gradient AS with impaired LVEF.

Figure 17: Worked example of the projected EOA methodology:

- A patient with severe LV impairment was noted to have calcified restricted aortic valve (a). The LVOTd is 2.2cm (b). The LVOT cross sectional area is 3.8cm².
- Optimal CW and PW recordings were obtained from the 5-chamber window (c and d). AV Vmax 2.4m/s; mean gradient 16mmHg; AV VTI 50cm (e); LVOT VTI 9cm.
- AVA at rest calculated using the continuity equation:

$$AVA_{rest} = LVOT\ VTI \div AV\ VTI \times LVOT\ CSA = 9cm \div 50cm \times 3.8cm^2 = 0.68cm^2$$

- Flow at rest (Q_{rest}) is calculated from the stroke volume and the ejection time (f):

$$Q_{rest} = stroke\ volume \div ejection\ time = 9cm \times 3.8cm^2 \div 0.36s = 95ml/s$$

- At maximal stress, CW Doppler was obtained (g): AV Vmax 3.2m/s; mean gradient 28mmHg; AV VTI 61cm. PW Doppler at peak stress (h): LVOT VTI 16cm; ejection time was 0.33ms. The LVOTd is assumed to remain unchanged with stress.

$$AVA_{peak} = LVOT\ VTI \div AV\ VTI \times LVOT\ CSA = 16cm \div 61cm \times 3.8cm^2 = 1.0cm^2$$

$$Q_{peak} = stroke\ volume \div ejection\ time = 16cm \times 3.8cm^2 \div 0.33s = 184ml/s$$

- Note that the stroke volume has increased by >20% and therefore the patient has contractile reserve.

- The mean gradient has only increased to 28mmHg, and therefore this patient **does not** fulfil the criteria for 'true-severe AS'. Equally, the patient has not fulfilled the usual criteria for 'pseudo-severe' AS, which mandates an AVA $\geq 1.2\text{cm}^2$ at peak stress.

- The projected-EOA calculates the AVA at a 'normal' transvalvular flow rate of 250ml/s:

$$\text{Projected EOA} = \text{AVA}_{\text{rest}} + ((\text{AVA}_{\text{peak}} - \text{AVA}_{\text{rest}}) \div (Q_{\text{peak}} - Q_{\text{rest}})) \times (250 - Q_{\text{rest}})$$

$$\text{Projected EOA} = 0.68 + ((1.0 - 0.68) \div (184 - 95)) \times (250 - 95) > 1.2\text{cm}^2$$

- An EOA-Proj $> 1.2\text{cm}^2$ is consistent with 'pseudo-severe AS'. This patient should therefore be treated medically.

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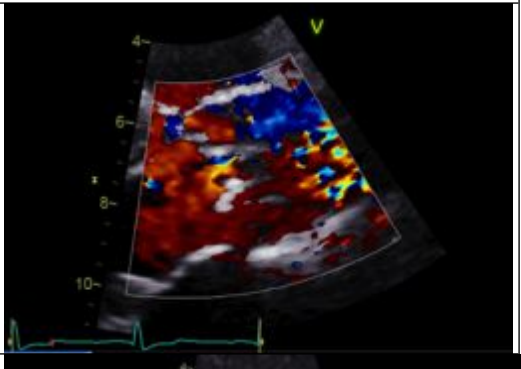
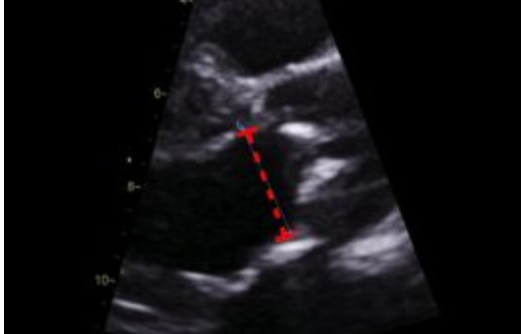
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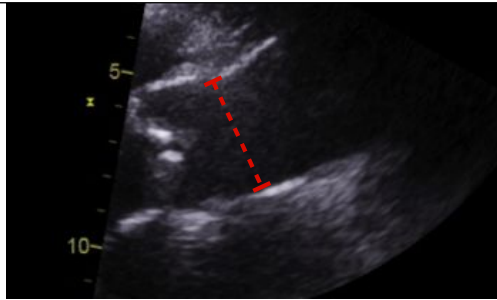


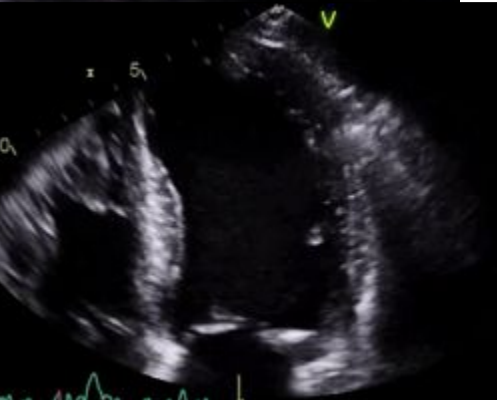

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Table 1. Subsections of the BSE aortic valve guidance

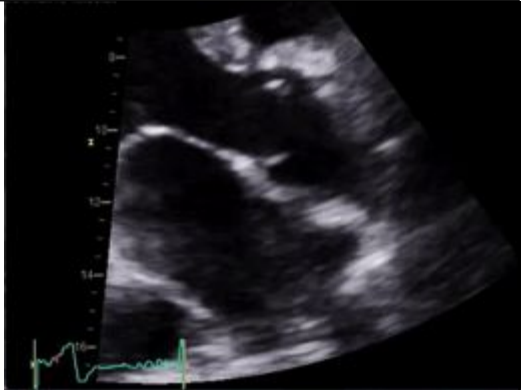
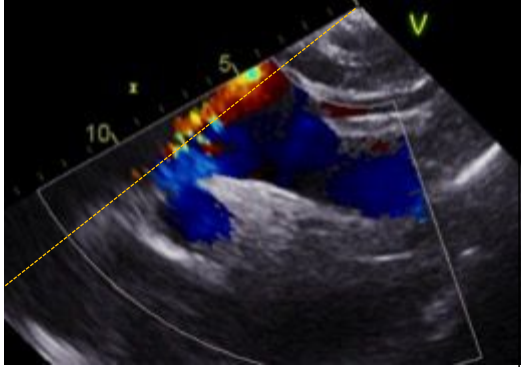
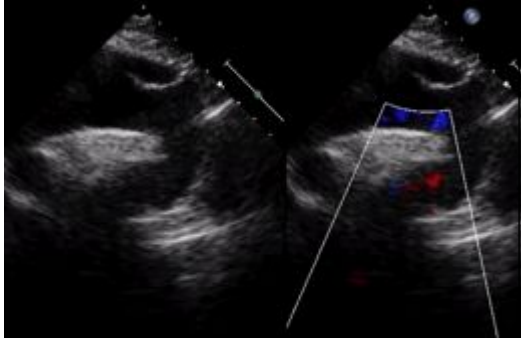
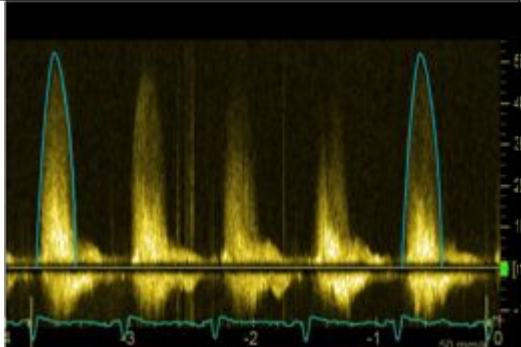
1. Anatomy
 - Standard anatomy and imaging planes
 - Variant anatomy
 2. Calcification and aetiology of AS
 3. Haemodynamic principles of AS
 4. Standard echocardiographic images
 5. Essential parameters in the echocardiographic assessment of AS severity
 - Aortic valve maximal velocity (AV Vmax)
 - Mean aortic valve gradient (mean AVG)
 - Aortic valve area (AVA)
 - Potential sources of error and troubleshooting
 6. Approach to the patient
 7. Grading of severity
 - Aortic sclerosis
 - Mild, moderate and severe AS
 - Very severe AS
 8. Additional parameters to define severity
 - Indexed aortic valve area (AVAi)
 - Dimensionless index
 - Planimetry
 - Energy loss index (ELI)
 9. Other considerations
 - Atrial fibrillation
 - Blood pressure
 10. Additional prognostic markers
 - Left ventricular ejection fraction
 - Indexed Left ventricular mass
 - Global longitudinal strain
 - Pulmonary hypertension
 11. Additional echocardiographic imaging modalities
 - Trans-oesophageal imaging
 - Exercise stress echocardiography
 12. Special circumstances
 - Low-gradient AS with LVEF \geq 50%
 - Low-gradient AS with impaired LVEF
 - High gradient high valve area
 13. Combined valve disease
 - Aortic stenosis and aortic regurgitation
 - Aortic stenosis and mitral regurgitation
 - Aortic stenosis and mitral stenosis
 14. Aortic stenosis and amyloid
-

Table 2: Standard TTE images for the assessment of AS

View (modality)	Measurement	Explanatory notes	Image
Parasternal long axis (PLAX); 2D	LV dimensions Calculate indexed LV mass using linear method	Visual assessment of wall motion. Calcification of aortic valve (see section 2) Indexed LV mass is a prognostic marker in AS (section 10)	
Parasternal long axis; zoom 2D		Assess calcification and mobility of cusps. Advanced AS unlikely without significant cusp calcification or restriction. Assess for central vs. eccentric closure line suggesting BAV (section 1)	
Parasternal long axis; zoom 2D with colour Doppler		Assess for turbulence and presence of aortic regurgitation	
Parasternal long axis; zoom 2D	LVOT dimension for assessment of AVA and stroke volume	Obtained immediately below cusp insertion Inner-edge to inner-edge in mid-systole when LVOT is at a maximum Measurement parallel to aortic valve See section 5	

Parasternal long axis; zoom 2D	Measurement of the aorta including the sino-tubular junction	Inner-edge to inner-edge method in end-diastole May be used in assessment of the energy loss index (ELI; see section 8)	
Parasternal short axis (PSAX); 2D		Overview Visual appearance of aortic valve – cusp calcification and mobility	
Parasternal short axis; zoom 2D (+ colour Doppler)		Morphology of valve Visual appearance of calcification and mobility of cusps Colour Doppler to assess for presence and origin of AR	
Apical 4-chamber view; 2D imaging optimized for LV assessment	LV volumes and LVEF using quantitative methodology Consider GLS	LVEF is a prognostic marker in AS (See section 10) GLS is a potential marker of prognosis in AS (see section 10)	
Apical 5-chamber view; 2D imaging (+ colour Doppler)		Overview Visual appearance of aortic valve – cusp calcification and mobility Colour Doppler assessment for AR	

Apical 5-chamber view; 2D imaging zoom	CW Doppler tracings for AV Vmax and mean AVG	Sweep speed 50- 100mm/s Trace around dense aspect of Doppler curve Average of three tracings in sinus rhythm (SR). See section 5 for optimization and trouble shooting	
Apical 5-chamber view; 2D imaging zoom	PW Doppler tracing in LVOT for calculation of stroke volume and AVA	Sweep speed 50- 100mm/s Trace around modal velocity Average three tracings in SR. See section 5 for optimization and trouble shooting	
Apical 2-chamber view; 2D imaging focus on LV	LV volumes and LVEF using quantitative methodology Consider assessment of GLS	LVEF is a prognostic marker in AS (See section 10) GLS is a potential marker of prognosis in AS (see section 10)	
Apical 3-chamber window; 2D imaging (+ colour Doppler)		Overview Calcification and mobility of aortic valve + colour Doppler for assessment of AR Consider GLS (see section 10)	

<p>Apical 3-chamber view; 2D imaging zoom AV</p> <p>+ repeat CW and PW Doppler</p>		<p>Mobility and calcification of valve</p> <p>Repeat Doppler tracings for assessment of severity</p>	
<p>Suprasternal notch; 2D + colour Doppler</p>	<p>Aortic arch</p>	<p>Look for turbulence and aortic pathology</p> <p>Repeat CW Doppler for AV Vmax and mean AVG (see section 5)</p>	
<p>Suprasternal notch; 2D + colour Doppler</p>		<p>Distal arch / descending aorta. Look for turbulence and pathology including coarctation</p>	
<p>PEDOFF or standalone imaging</p> <p>Try all imaging windows including right parasternal (shown)</p>	<p>AV Vmax and mean gradient</p>	<p>Repeat from all imaging windows to ensure maximal values of Vmax and mean gradient are obtained</p>	

Apical 5-chamber view; 2D imaging zoom	CW Doppler tracings for AV Vmax and mean AVG	Sweep speed 50-100mm/s Trace around dense aspect of Doppler curve Average of three tracings in SR. See section 5 for optimization and trouble shooting	
Apical 5-chamber view; 2D imaging zoom	PW Doppler tracing in LVOT for calculation of stroke volume and AVA	Sweep speed 50-100mm/s Trace around modal velocity Average three tracings in SR See section 5 for optimization and trouble shooting	
Apical 2-chamber view; 2D imaging focus on LV	LV volumes and LVEF using Simpson's biplane method Assessment of GLS	LVEF is a prognostic marker in AS (See section 10) GLS is a potential marker of prognosis in AS (see section 10)	
Apical 3-chamber window; 2D imaging (+ colour Doppler)		Overview Calcification and mobility of aortic valve + colour Doppler for assessment of AR GLS assessment (see section 10)	

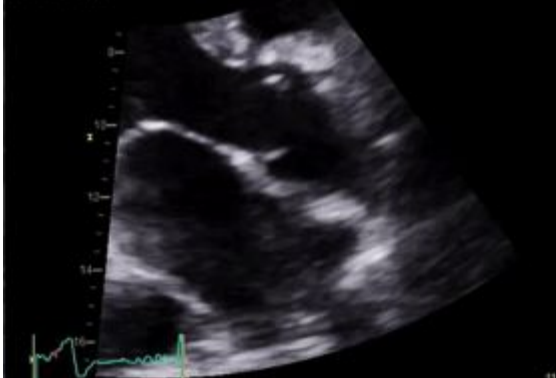
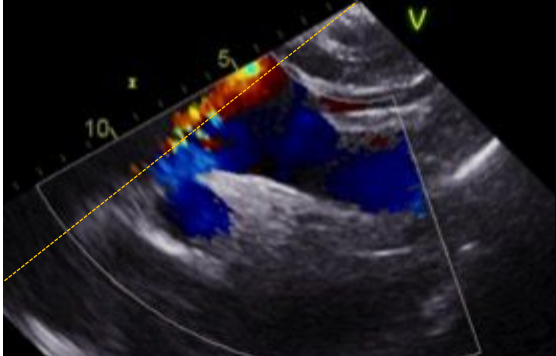
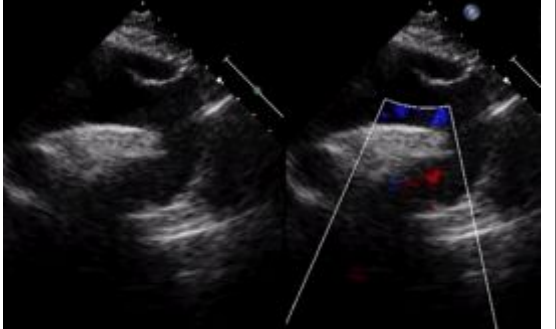
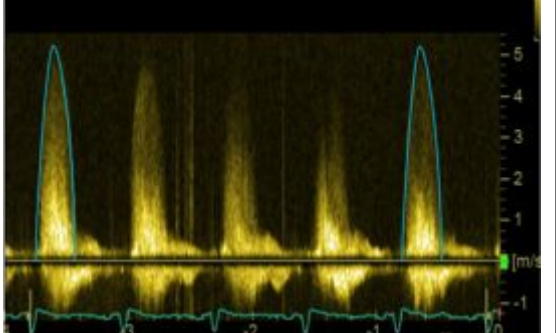
<p>Apical 3-chamber view; 2D imaging zoom AV + repeat CW and PW Doppler</p>		<p>Mobility and calcification of valve Repeat Doppler tracings for assessment of severity</p>	
<p>Suprasternal notch; 2D + colour Doppler</p>	<p>Aortic arch</p>	<p>Look for turbulence and aortic pathology Repeat CW Doppler for AV Vmax and mean AVG (see section 5)</p>	
<p>Suprasternal notch; 2D + colour Doppler</p>		<p>Distal arch / descending aorta. Look for turbulence and pathology including coarctation</p>	
<p>PEDOFF or standalone imaging Try all imaging windows including right parasternal (shown)</p>	<p>AV Vmax and mean gradient</p>	<p>Repeat from all imaging windows to ensure maximal values of Vmax and mean gradient are obtained</p>	

Table 3: Suggested reporting template for AS

Demographics

- Height, weight, body surface area (BSA).
- Blood pressure, heart rate and rhythm.

Aortic valve morphology

- Tricuspid / bicuspid / unicuspid
- Severity and extent of calcification

LVOT

- Dimensions and VTI
- Report any change in the LVOTd from previous studies

Aortic stenosis severity

- Aortic valve Vmax; mean gradient: include window from which maximal values were obtained
- Change in AV Vmax from previous echo study
- Aortic valve area
- Description of severity (mild / moderate / severe / very severe)

Additional prognostic markers

- Left ventricular ejection fraction
- Global longitudinal strain
- Indexed LV mass
- High probability of pulmonary hypertension (see specific BSE guidance)

Aortic regurgitation – note presence and severity (see specific BSE guidance)

Aorta – measure size (see specific BSE guidance and reference intervals)

Table 4: Grading of aortic stenosis

Grading of severity	Echocardiographic indices		
	AV Vmax (m/s)	Mean gradient (mmHg)	AVA (cm ²)
Aortic sclerosis	<2.5 m/s	-	-
Mild	2.5-2.9m/s	<20 mmHg	>1.5 cm ²
Moderate	3-3.9m/s	20-39 mmHg	1-1.5 cm ²
Severe	4-4.9m/s	40-59 mmHg	<1 cm ²
Very severe	≥5m/s	≥60 mmHg	≤0.6 cm ²

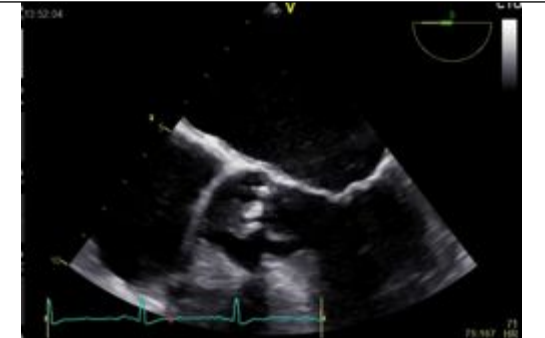
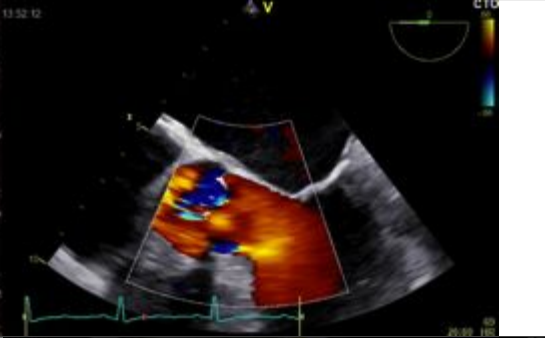




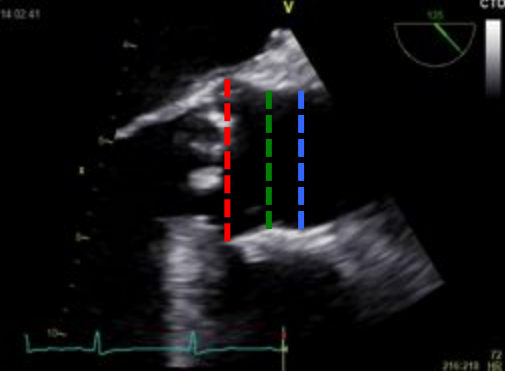

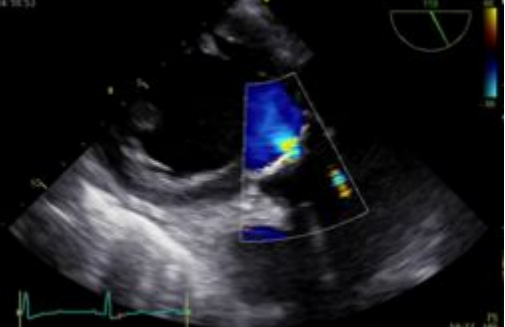
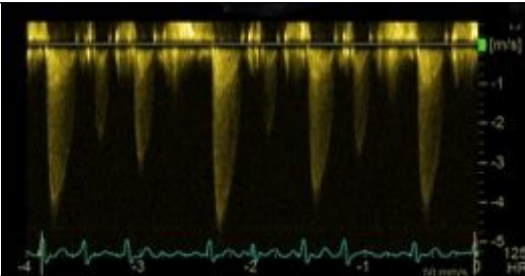
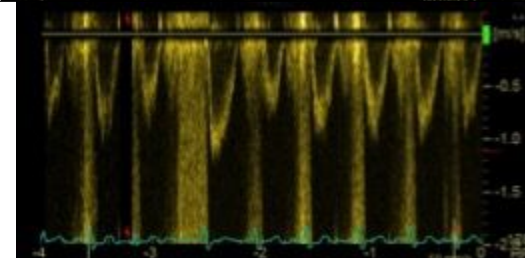
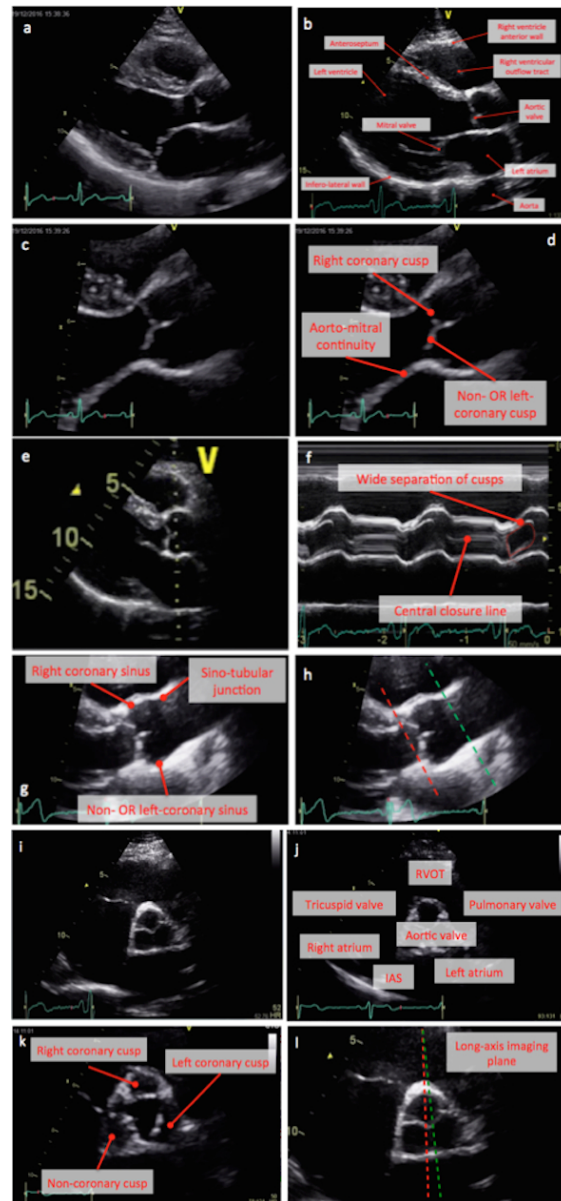
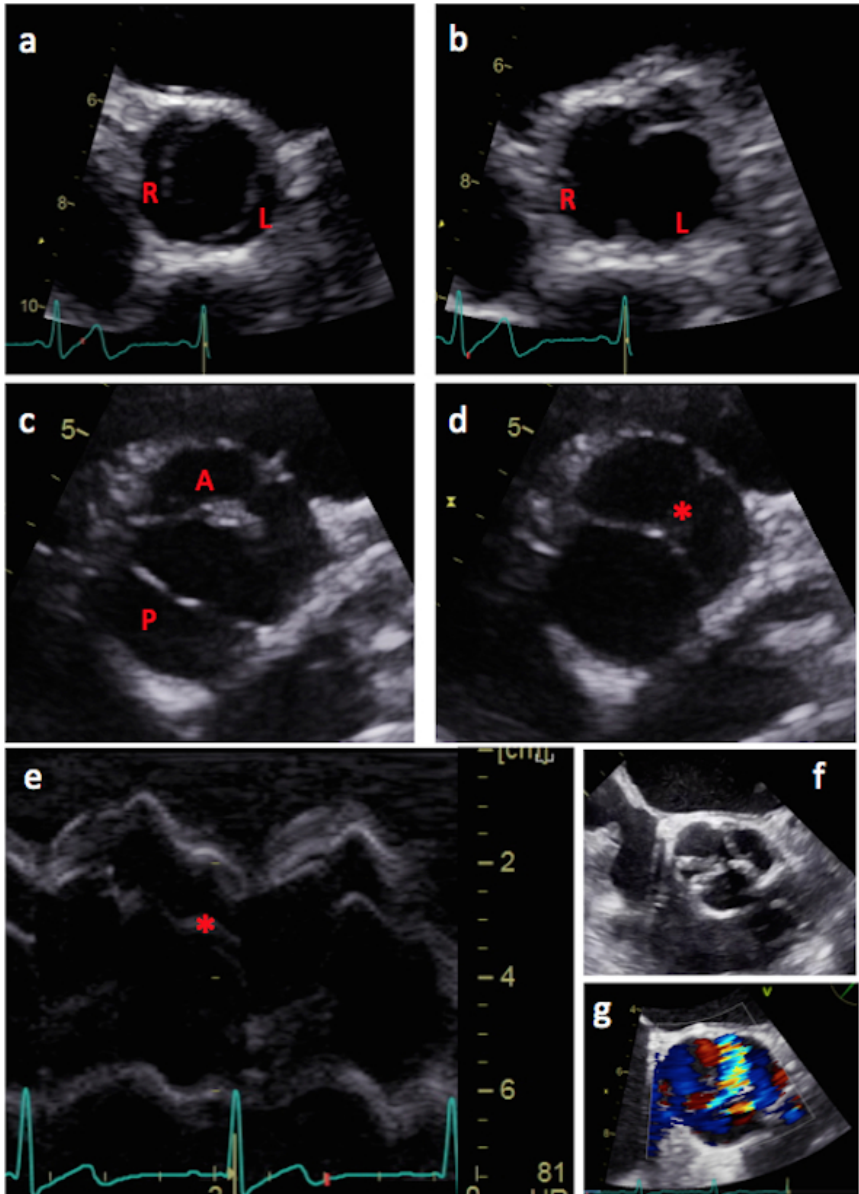
View (modality)	Measurement	Explanatory notes	Image
5-chamber view; mid-oesophageal window; 0°; zoom 2D		Observe calcification and mobility of the cusps.	
5-chamber view; mid-oesophageal window; 0°; zoom 2D + colour Doppler		Colour Doppler imaging to assess for turbulence and valve regurgitation.	
Short-axis view; mid-oesophageal window; 40-60°; the level of the aortic cusps 2D		Assess for valve morphology, cusp mobility and calcification	
Short-axis view; mid-oesophageal window; 40-60°; at the level of the aortic cusps 2D zoom + colour Doppler		Assess for AR Colour Doppler may help identify morphology (shown is tricuspid valve; see section 1)	

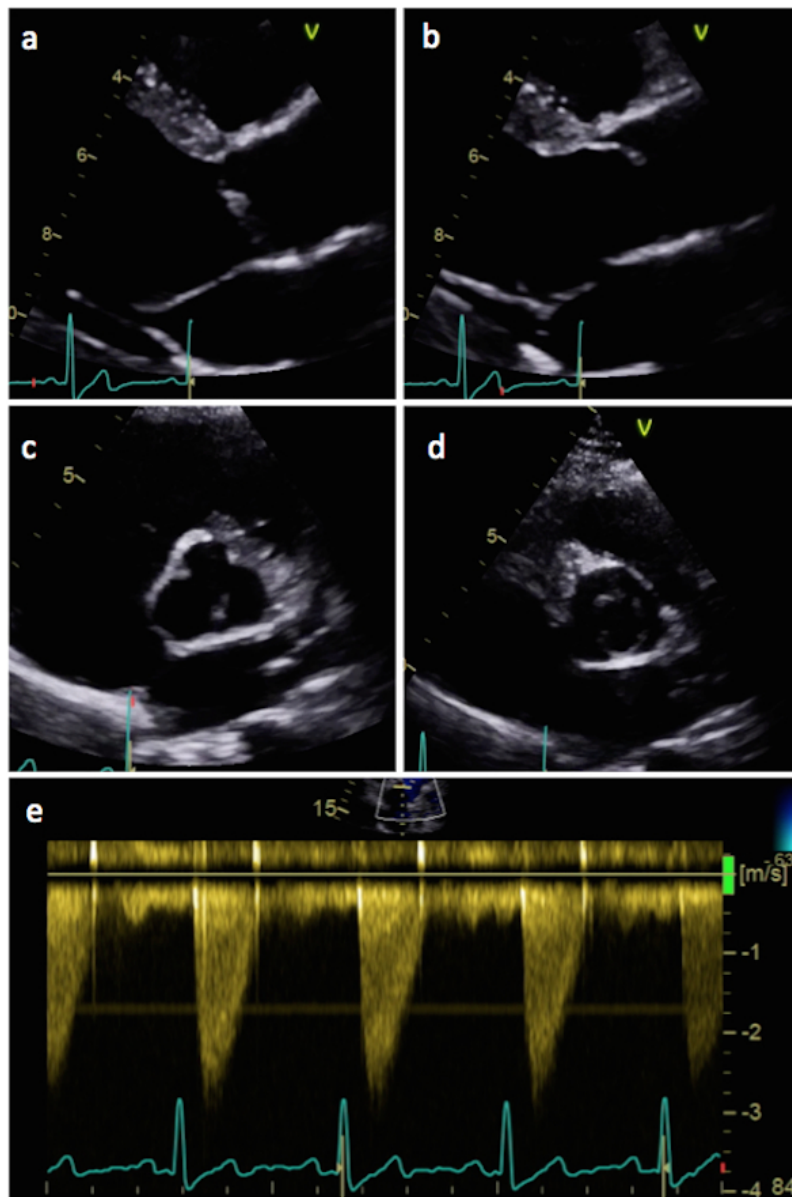
Table 5: TOE imaging in aortic stenosis

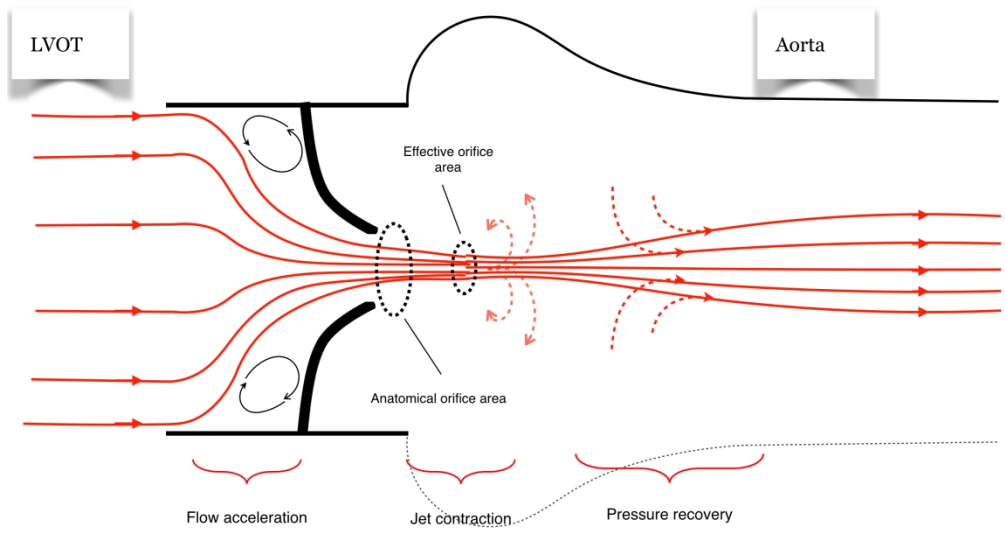
3D dataset	Consider planimetry	Overview and optimized images for planimetry	
Long-axis view; mid-oesophageal window; 120-140°; 2D imaging	Measurement of LV size and wall thickness Indexed LV mass calculation	Observe calcification and mobility of the cusps. LV size and function Indexed LV mass is a prognostic sign	
Long-axis view; mid-oesophageal window; 120-140°; 2D imaging zoom	LVOT dimension (not shown) Measurement of aorta	Inner-edge to inner edge method; end-diastole Red = Sinus of Valsalva Green = ST junction Blue = Ascending	
Short-axis view; trans-gastric window; 0°; at the level of the aortic cusps 2D + colour Doppler		Manipulation of probe to 'open' aortic valve (marked with 'A') Assessment of turbulence and the presence of AR	
Long-axis view; trans-gastric window; 120-140°; 2D imaging + colour Doppler		Assess for AR Colour Doppler may help identify morphology (shown is tricuspid valve; see section 1)	

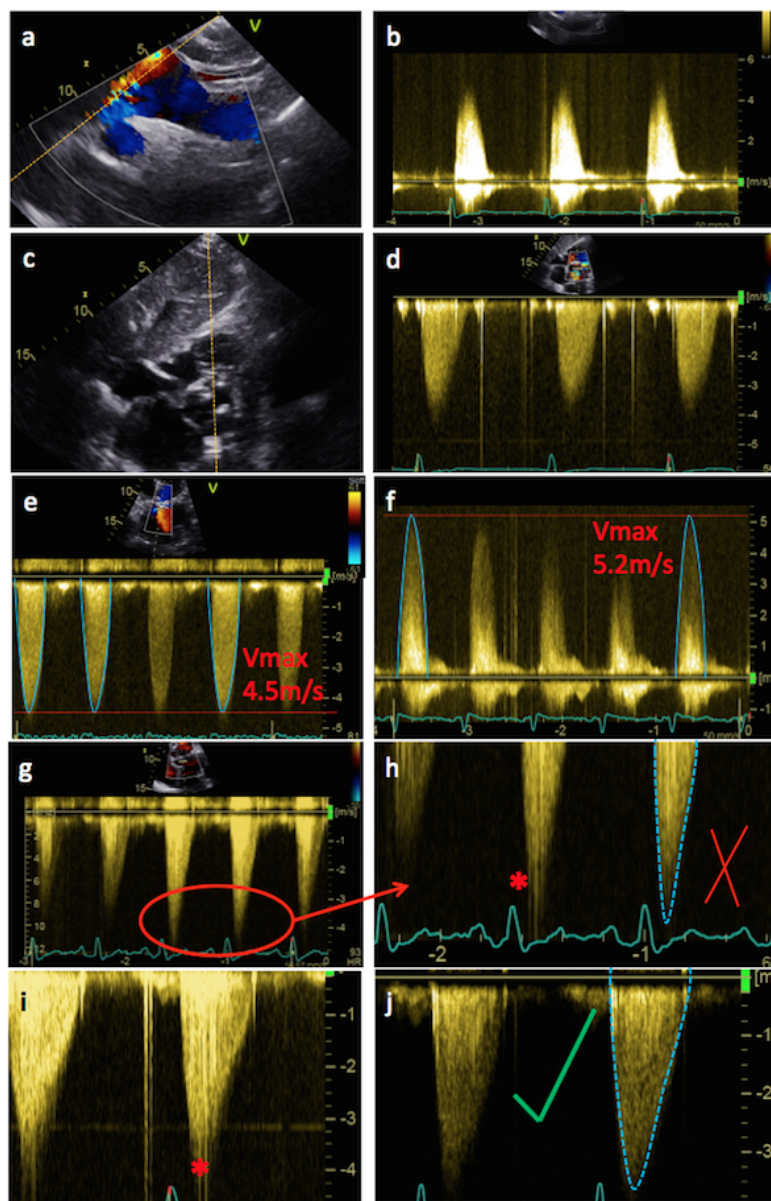
<p>Transgastric windows (re-attempt at all angles); CW Doppler</p>	<p>AV Vmax and mean gradient</p>	<p>Trace round modal velocity See section 5 for details</p>	
<p>Transgastric windows (re-attempt at all angles); PW Doppler</p>	<p>LVOT VTI for stroke volume and AVA assessment</p>	<p>Trace round modal velocity See section 5 for details</p>	

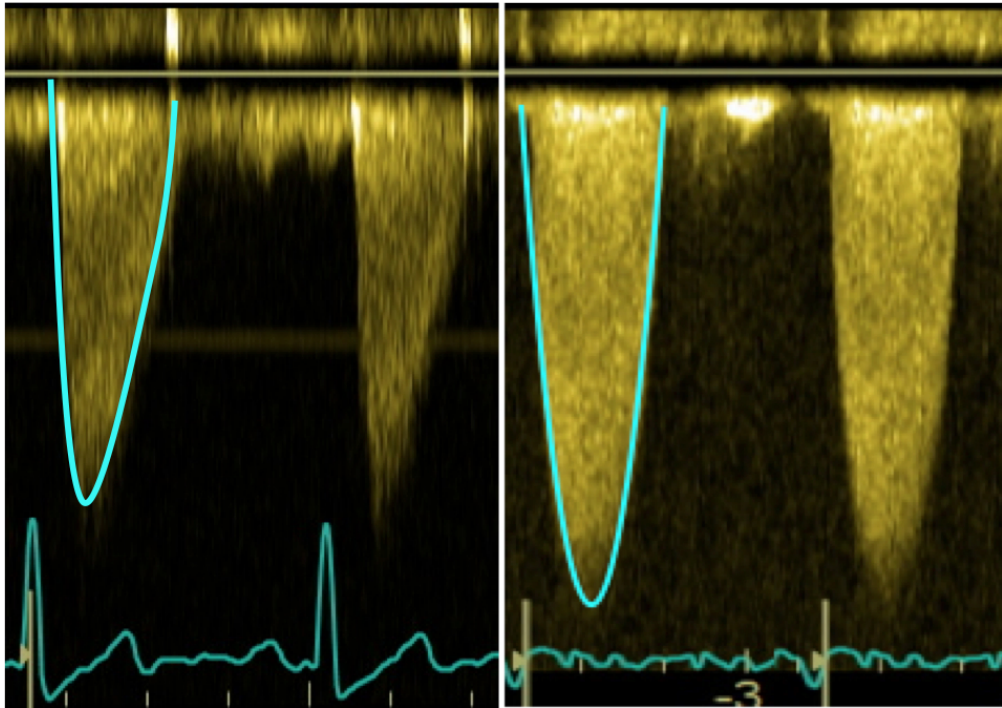




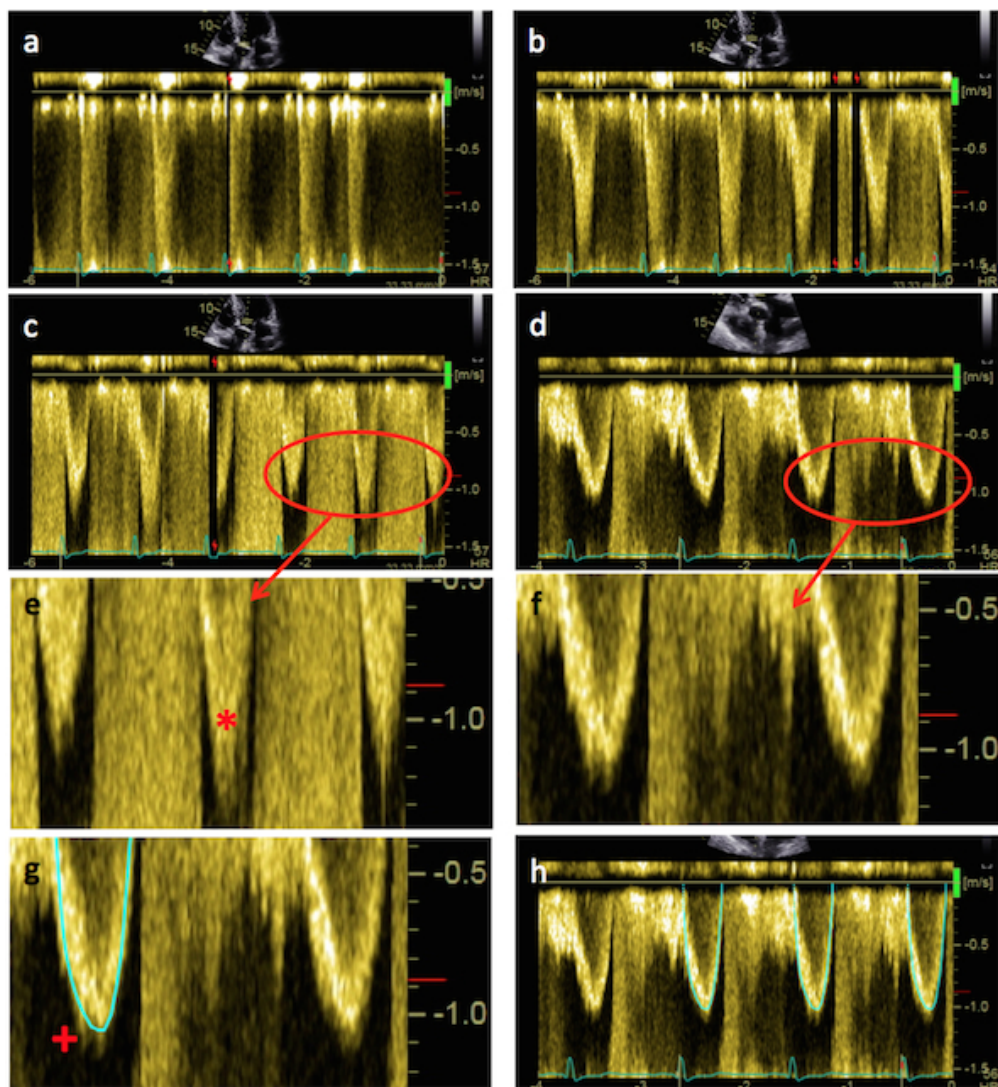


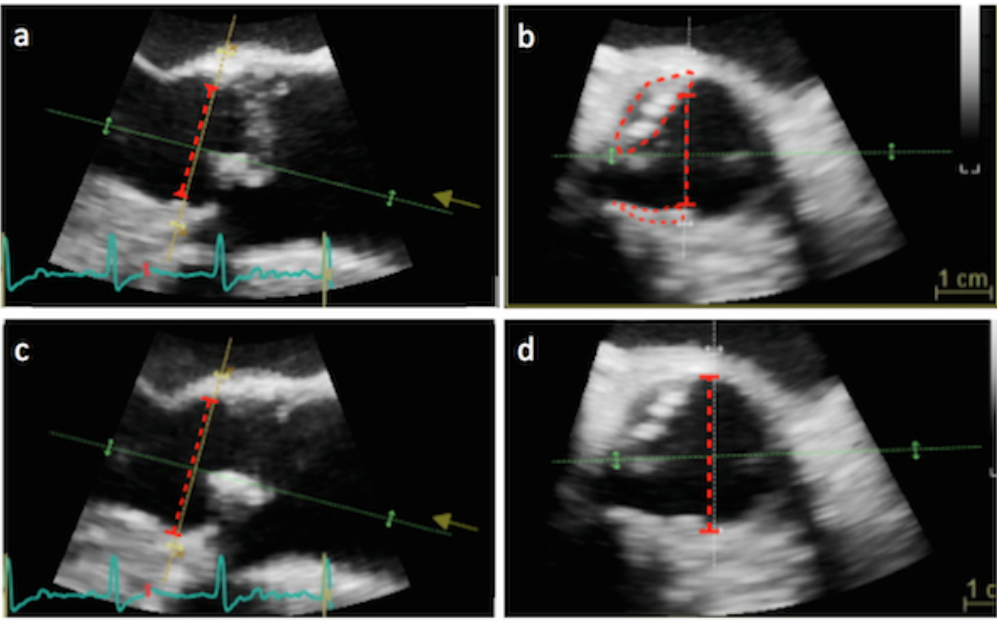


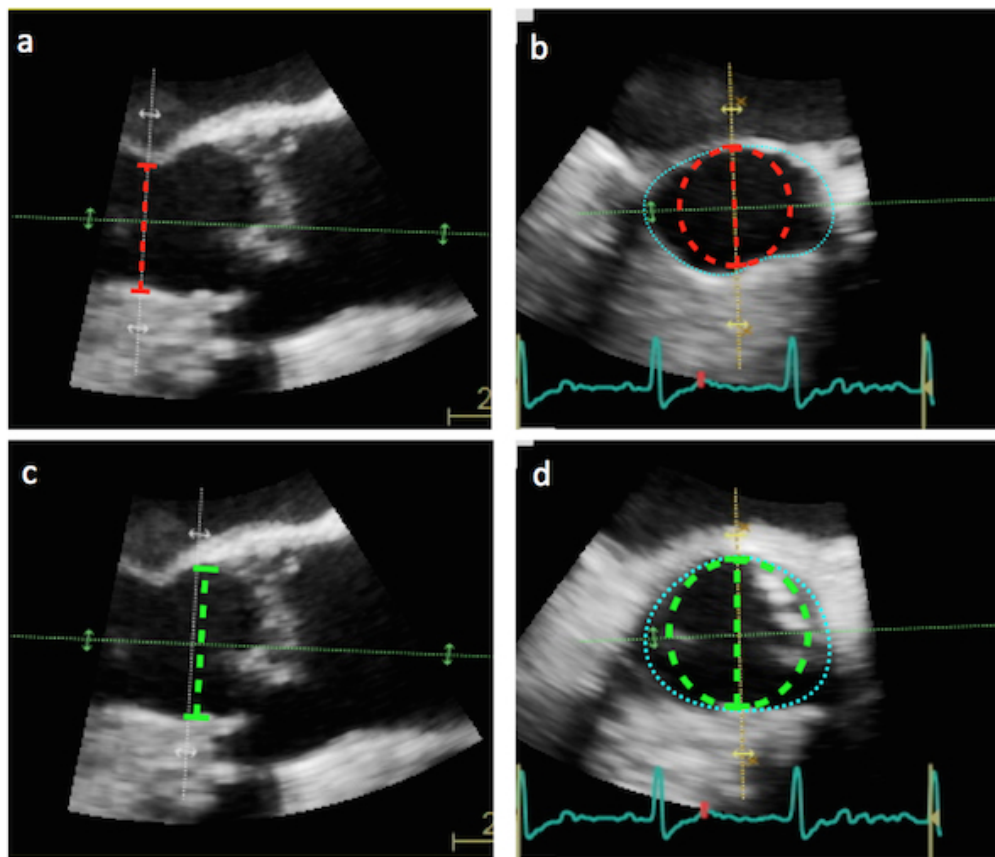




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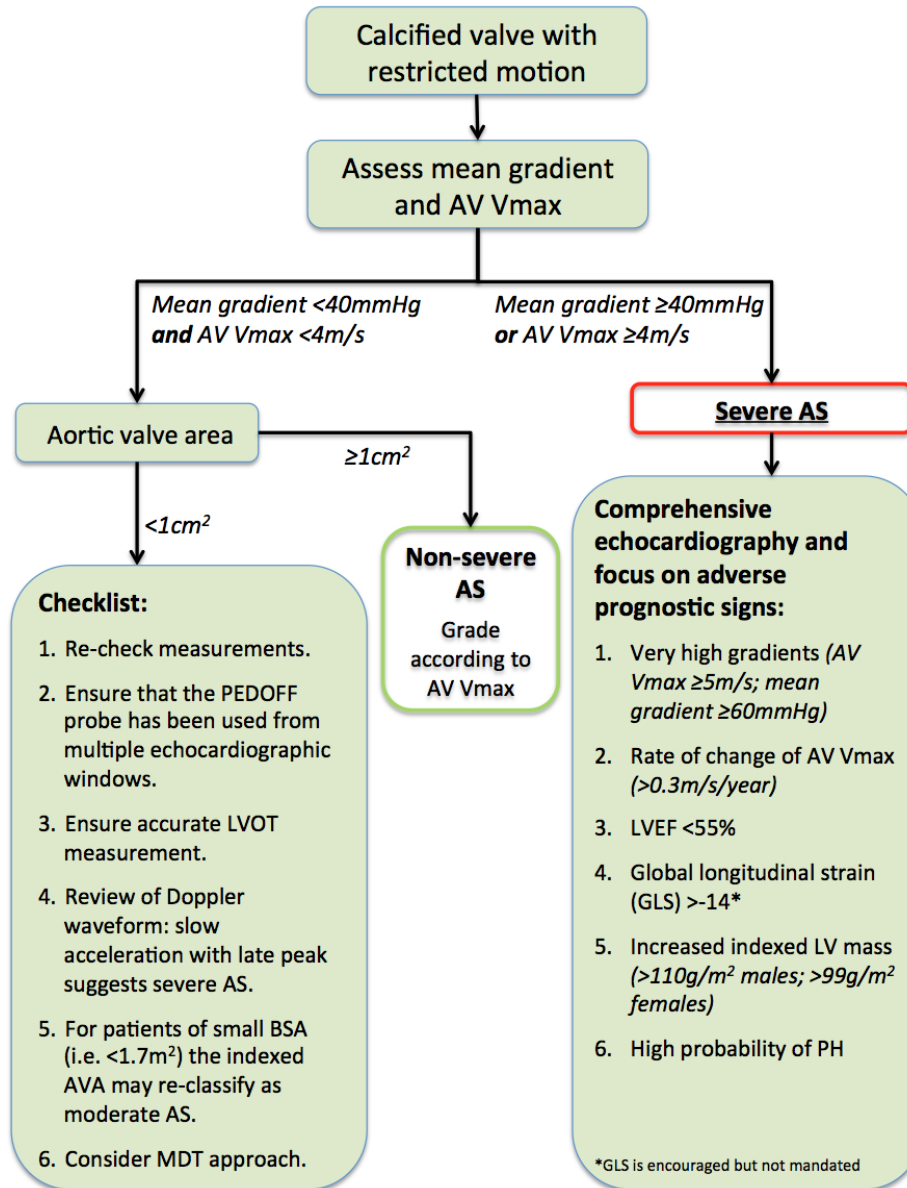
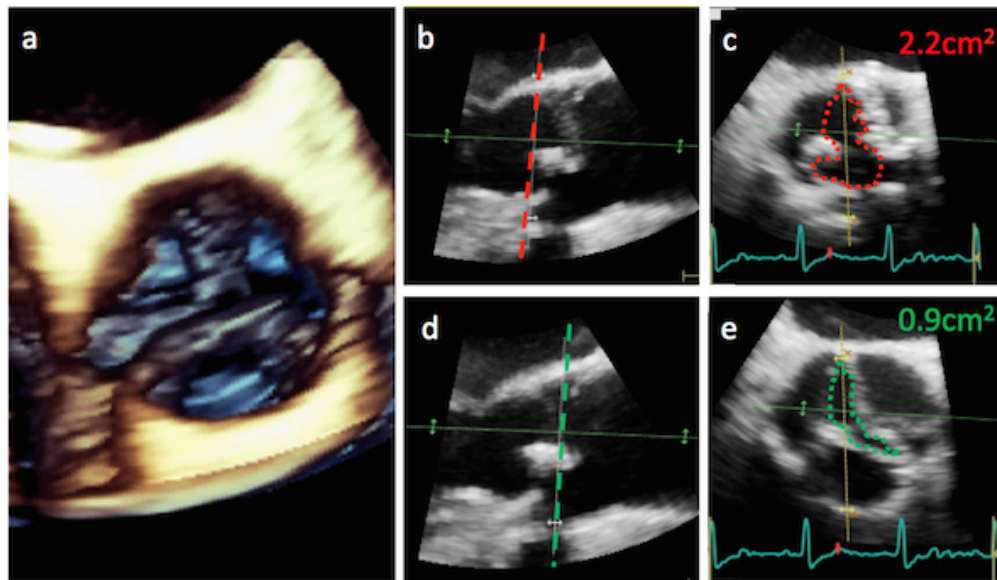
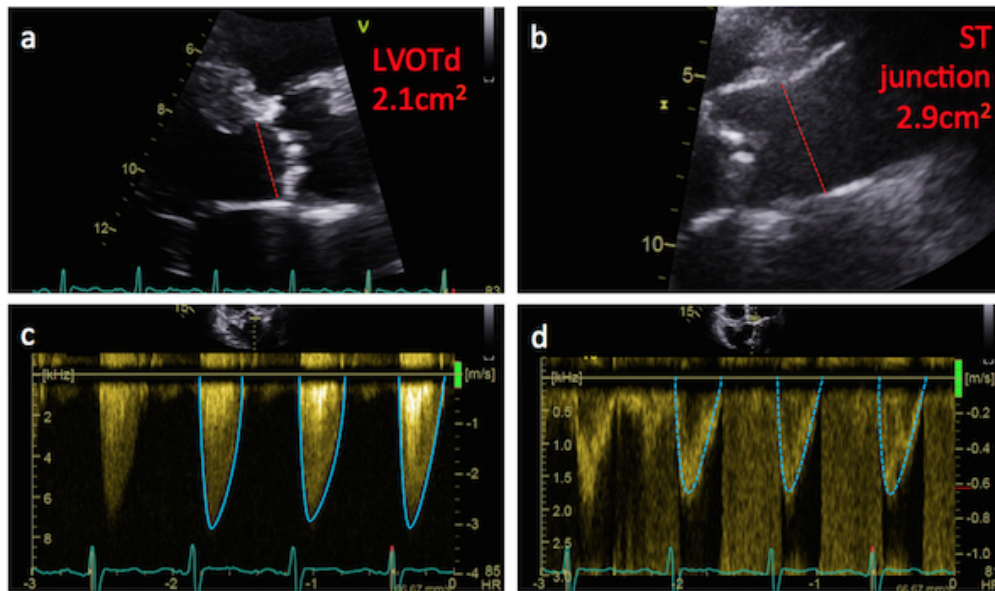
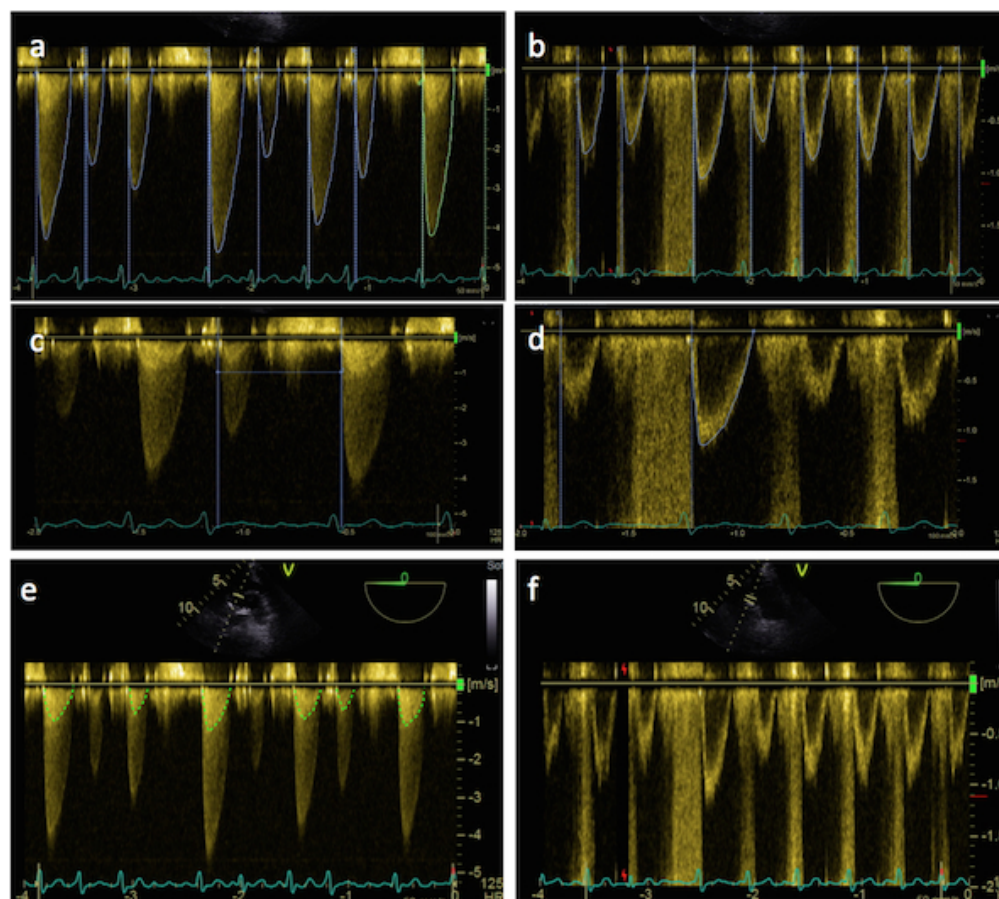


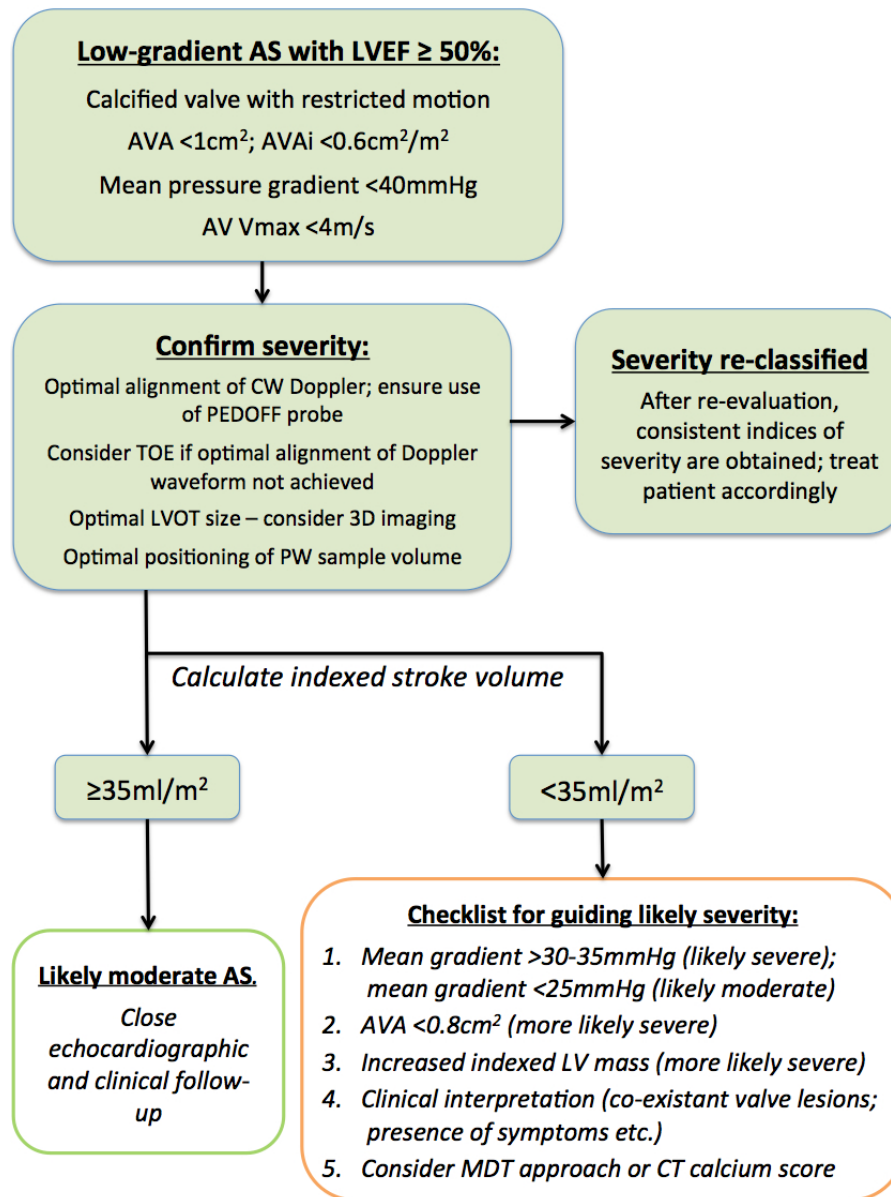
Figure 10

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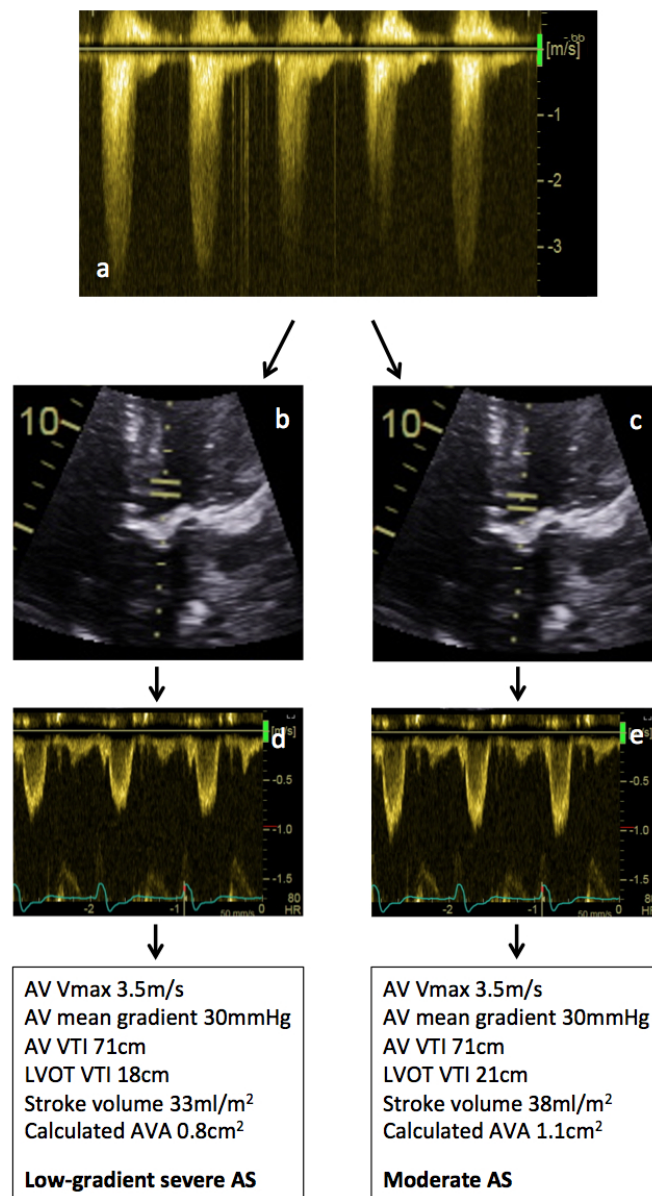




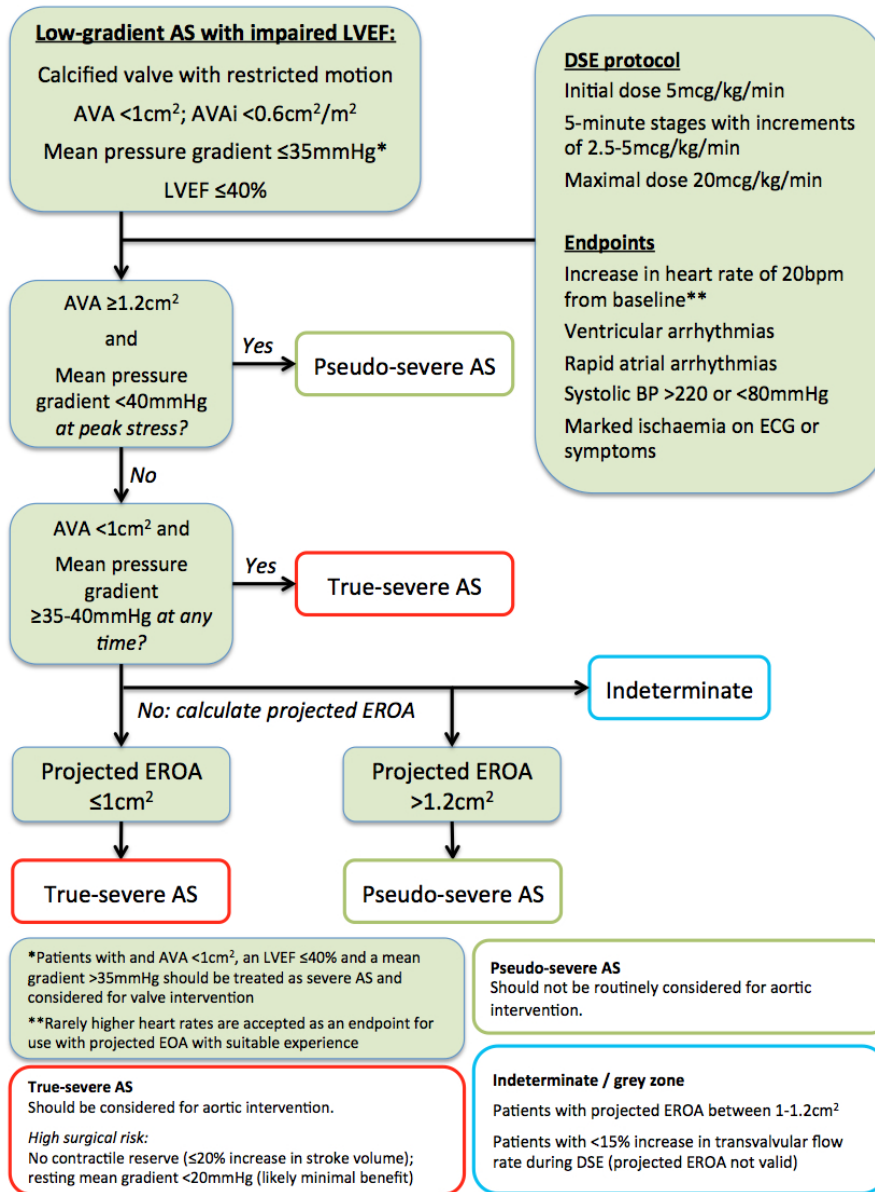




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225x406mm (72 x 72 DPI)



293x392mm (72 x 72 DPI)

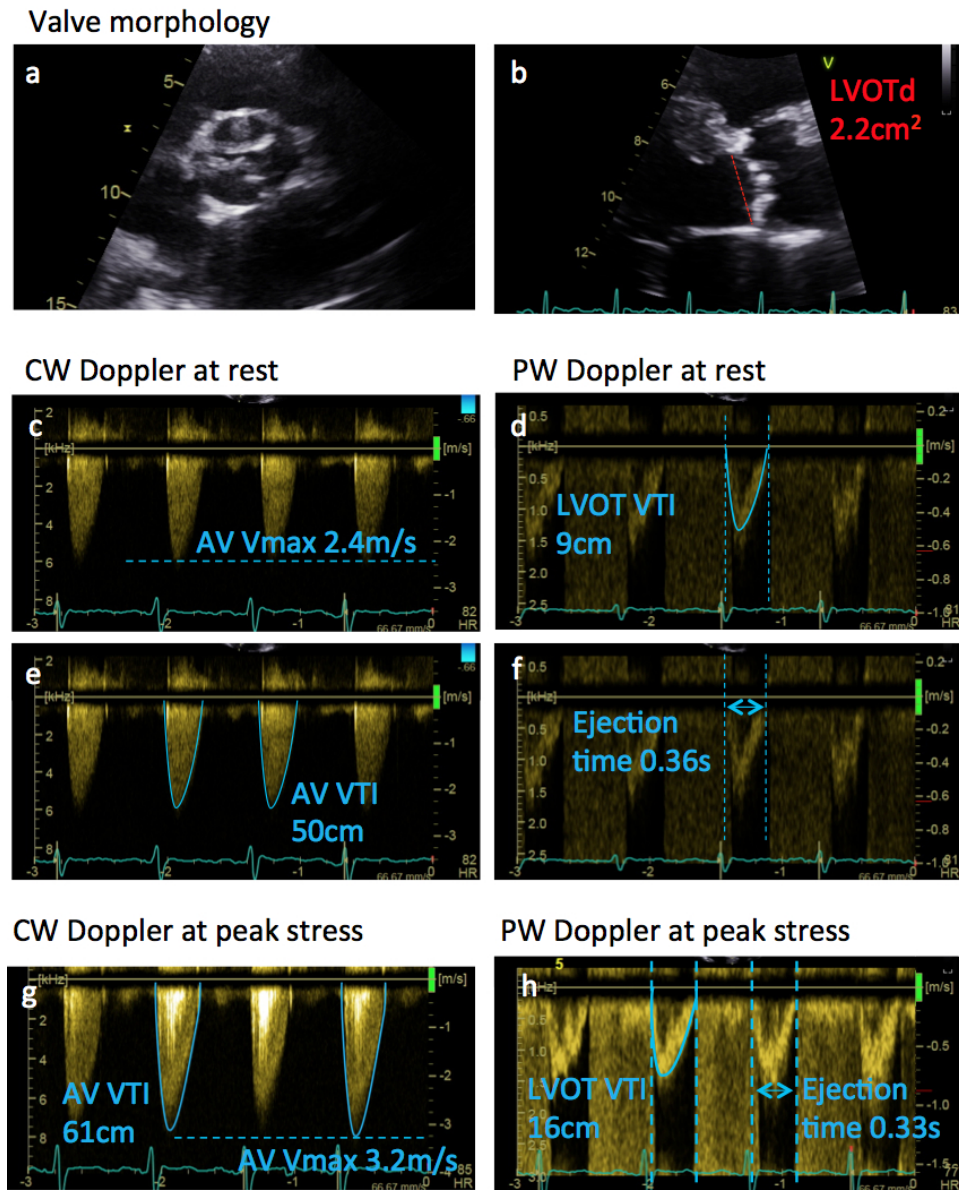


Figure 17

299x374mm (72 x 72 DPI)