



Automated fetal brain segmentation of 2D magnetic resonance images: transfer learning and 3D topology correction



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BACKGROUND

- Fetal brain extraction in MRI: first step for further processing (super-resolution reconstruction, tissue segmentation, etc.)
- Manual annotations are cumbersome and time



- Deep learning limitations:
 - Need of a large amount of labeled data
 - Highly specialized models
- Transfer learning can partially help to overcome

consuming, and hence inappropriate to automated analysis and large-scale studies.

• **Deep learning** is an *Artificial Intelligence* branch that has proven to be very successful in image processing, including fetal brain segmentation^[1-3].

Automated brain segmentation of a fetus of 26 gestational weeks

these caveats.

Aim: To evaluate transfer learning for segmenting the fetal brain from one dataset (Lausanne University Hospital, **CHUV**) using the pre-trained parameters of a larger dataset (Boston Children Hospital's, **BCH** ^[1]).

MATERIALS AND METHODS

• 2D convolutional neural network U-Net^[4].



Our dataset (CHUV)

- 39 subjects
- From 20 to 36 weeks of gestation
- Orthogonal T2-weighted HASTE at **1.5T**
- 227 series totalling **4,767 slices**
- 1.125 mm in-plane isotropic
- 3 to 5 mm slice thickness
- We evaluate three scenarios:
- a. Using BCH pre-trained parameters^[1] to test on CHUV dataset;
- b. Solely training on CHUV data, with random initialization;

BCH dataset

- 41 subjects
- From 22 to 38 weeks of gestation
- Orthogonal T2-weighted SSFSE at **3T**
- 385 series totalling ~13,000 slices
- 1 to 1.125 mm in-plane isotropic
- 2 to 3 mm slice thickness



Network

- U-Net architecture^[4] with ~8 million parameters
- Weighted-cross entropy loss function
- Trained with Adam optimiser for ~200 epochs
- Model evaluation in a leave-four-out crossvalidation using an average of *precision* and *recall*
- c. Fine-tuning the network with the pretrained parameters of [1].
- Post-processing: 3D continuity of the brain to refine the predictions by morphological operations such as closing, opening and connected components.

RESULTS

- Directly applying the pre-trained weights (a) from [1] to our dataset generated non plausible segmentations.
- The pre-trained network c significantly outperforms the randomly initialized b network in both healthy and pathological subjects (Wilcoxon test, p<0.05).
- Remaining errors: 1) at extremities of the brain, 2) slices containing the temporal lobe.
- The 3D topology correction did help qualitatively but not quantitatively.







CONCLUSION

- Feasibility of using a different scanner/magnetic field strength through transfer learning.
- Hospitals lacking of a large amount of data can benefit from pre-trained parameters from other hospitals to boost their models.

REFERENCES: [1] Salehi et al., ISBI 2018; [2] Lou et al., MLMI 2019; [3] Rutherford et al., bioRxiv 2019; [4] Ronneberger et al., MICCAI 2015. ACKNOWLEDGMENTS: This work is supported by the Swiss National Science Foundation (FNS projects 205321_141283 & 205321_182602) and the Hasler Foundation (17029).



0.4 Healthy Pathological Method Random_init_U-Net b Pre-trained_U-Net c



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