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## Membrane Binding of Antimicrobial Peptides is Modulated by Lipid Charge Modification

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**ABSTRACT**

Peptide interactions with lipid bilayers play a key role in a range of biological processes, and depend on electrostatic interactions between charged amino acids and lipid headgroups. Antimicrobial peptides (AMPs) initiate killing of bacteria by binding to and destabilizing their membranes. The multiple peptide resistance factor (MprF) provides a defence mechanism for bacteria against a broad range of AMPs. MprF reduces the negative charge of bacterial membranes through enzymatic conversion of the anionic lipid phosphatidyl glycerol (PG) to either zwitterionic alanyl-phosphatidyl glycerol (Ala-PG) or cationic lysyl-phosphatidyl glycerol (Lys-PG). The resulting change in membrane charge is suggested to reduce binding of AMPs to membranes, thus impeding downstream AMP activity. Using coarse-grained molecular dynamics to investigate the effects of these modified lipids on AMP-binding to model membranes, we show that AMPs have substantially reduced affinity for model membranes containing Ala-PG or Lys-PG. More than 5000 simulations in total are used to define the relationship between lipid bilayer composition, peptide sequence (using 5 different membrane active peptides), and peptide binding to membranes. The degree of interaction of a peptide with a membrane correlates with the membrane surface charge density. Free energy profile (potential of mean force) calculations reveal that the lipid modifications due to MprF alter the energy barrier to peptide helix penetration of the bilayer. These results will offer a guide to design of novel peptides which addresses the issue of resistance via MprF-mediated membrane modification.

## INTRODUCTION

An increasing number of pathogenic bacterial species are developing resistance to current antibiotics, paving the way to a post-antibiotic era in which previously treatable infections cause increased mortality<sup>1,2</sup>. Antimicrobial peptides (AMPs) are found in all kingdoms of life, in humans as part of the innate immune response<sup>3,4</sup>, and thus are a potential source for the development of novel antibiotics. Thousands of naturally occurring peptides have been identified<sup>5</sup> and many synthetic ones have also been developed<sup>6</sup>. There is little sequence conservation between peptides found in different species<sup>7</sup>, thus providing a large data-set for the design of new peptides<sup>8</sup>.

AMPs have diverse sequences but are generally cationic and form an amphipathic  $\alpha$ -helix, presenting distinct regions of hydrophobic and hydrophilic residues. These cationic peptides are rich in Arginine or Lysine<sup>9</sup> and exhibit a strong correlation between charge (typically in the range of +2 to +9) and antimicrobial activity<sup>10</sup>. AMPs selectively target bacterial membranes<sup>11</sup>. Once adsorbed onto a membrane they can induce a range of effects<sup>12</sup> including membrane deformation and disruption, membrane depolarization, and clustering of charged lipids, and various modes of pore formation<sup>13</sup> alongside a detergent-like mechanism<sup>14</sup>. Many of these effects have been observed experimentally for the canonical AMP magainin (from *Xenopus laevis*)<sup>15</sup>. NMR studies have shown that at low concentrations magainin adsorbs onto lipid bilayer membranes, interacting with lipid head-groups<sup>16,17</sup> and reducing local membrane thickness<sup>18</sup>. At high Peptide/Lipid (P/L) ratios ( $> 1/30$ ), peptides move from a surface-bound to a trans-membrane orientation<sup>19</sup> and can form a toroidal pore in the bilayer<sup>20</sup>. At this P/L, dissipation of the transmembrane potential<sup>21</sup> and membrane leakage<sup>22</sup> of cell contents are observed. Mechanisms for AMPs depend not only on peptide structure and charge, but also on membrane lipid composition<sup>23,24</sup>.

Some bacteria have developed resistance to AMPs by changing their cell surface electrostatics<sup>25</sup>. Certain Gram-positive bacteria (e.g. *Staphylococcus aureus*, *Bacillus subtilis* and *Clostridium perfringens*<sup>26</sup>) can modify their lipids to change the membrane surface charge through the action of the multiple peptide resistance Factor (MprF) protein<sup>27</sup>. This mechanism also forms an additional defence mechanism in some Gram-negative bacteria (e.g. *Pseudomonas aeruginosa*<sup>28,29</sup> and *Rhizobium tropici*<sup>30</sup>) and also in *Mycobacterium tuberculosis*<sup>31</sup>.

MprF is a transmembrane protein that acts as both an enzyme (a synthase) and as a membrane transporter (a flippase) for modified phosphatidyl glycerol (PG) lipid species. PG is a major anionic lipid in bacterial membranes. MprF consists of a C-terminal enzymatic domain responsible for aminoacylating the headgroup of PG and a hydrophobic N-terminal domain responsible for flipping

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1  
2 the modified lipid to the outer leaflet of the cytoplasmic membrane <sup>32</sup>. MprF can transfer lysine  
3 obtained from Lysyl-tRNA to transform PG into a positively charged lipid Lys-PG <sup>33</sup> (SI Fig. S1).  
4 Alanine is also a common substrate used by MprF paralogs to produce zwitterionic Ala-PG <sup>34</sup>. The  
5 presence of MprF correlates with a reduction in the activity of AMPs against resistant bacteria.  
6 Incorporation of Lys-PG into artificial membranes significantly impairs the formation of membrane  
7 defects caused by AMPs <sup>35</sup>. MprF is critical for production of these modified lipids <sup>36,37</sup>, which also  
8 provides protection against peptide antibiotics such as daptomycin <sup>38-41</sup> (a lipo-peptide) and  
9 vancomycin <sup>42,43</sup> (a glyco-peptide) in addition to AMPs <sup>44,45</sup>. This is of clinical importance, as these  
10 antibiotics are reserved for combatting pathogens already resistant to many other drugs, highlighting  
11 the importance of understanding the mechanism and role of MprF.  
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21 Molecular dynamics (MD) simulations have been widely used to explore possible mechanisms of  
22 action of AMPs <sup>46-49</sup>, and in particular their interactions with lipid bilayer membranes. MD  
23 simulations have shown individual peptide molecules will rapidly adsorb onto the membrane surface  
24 <sup>50-52</sup>, interacting with the lipid head-groups and inserting into the membrane core when multiple  
25 peptides are present, with a preference for negatively charged membranes <sup>53</sup>. Further simulations  
26 supported by experiments suggested that peptides insert into membrane bilayers forming  
27 transmembrane or monolayer pores depending on their orientation in the bilayer <sup>54,55</sup>. Peptides self-  
28 inserting into the membrane have been shown to form disordered toroidal pores <sup>50,22</sup>. MD simulations  
29 have also been used to explore various other possible peptide pore structures <sup>56-58</sup>. Coarse-grained  
30 (CG) MD simulations have also shown that peptides will adsorb onto membranes <sup>59</sup> with a preference  
31 for negatively charged surfaces and that pores pre-formed in atomistic simulations remain stable  
32 when mapped to a CG representation <sup>60</sup>.  
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43 Here, we use CG MD to examine the effect of the two types of MprF-modified lipids, Ala-PG and  
44 Lys-PG, on peptide binding to bilayer membranes. We apply this methodology to five  $\alpha$ -helical  
45 peptides of varying net charge. Using CG MD we are able to screen 5 peptides vs. 37 bilayer lipid  
46 compositions (with 25 repeats per simulation yielding 4625 simulations, plus a further 2020  
47 simulations for free energy calculations; see SI Tables S1 to S3), enabling us to define quantitatively  
48 the relationship between bilayer lipid composition, peptide sequence, and AMP binding to  
49 membranes. Free energy profiles are calculated to show that MprF-mediated lipid modifications  
50 increase the energy barrier of single peptide penetration of the bilayer membrane.  
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## 59 METHODS

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2 For the peptides assumed to be fully  $\alpha$ -helical when bound to a membrane (nAMP, cp5, cp7, Amh),  
3 the peptides were initially generated in a  $\alpha$ -helical (atomistic) conformation using PyMOL <sup>61</sup>.  
4  
5 Martinize (<http://cgmartini.nl/index.php/tools2/proteins-and-bilayers/204-martinize>)  
6 was then used  
7 to obtain a coarse-grained Martini 3 representation of the peptides. Backbone restraints were added  
8 to preserve the secondary structure. The atomistic coordinates for the Mgn2 peptide were initially  
9 taken from the protein data bank (PDB ID: 2LSA) before undergoing the same coarse-graining  
10 process. MprF-modified lipids were generated initially in an atomistic resolution using a combination  
11 of parameters already established for lipids and proteins. This atomistic representation was then used  
12 as a basis for parameterising the coarse-grained Ala-PG and Lys-PG (see SI Fig S1 for details).  
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19 Simulations were carried out using the molecular dynamics package GROMACS 2018.6 <sup>62, 63</sup> using  
20 the coarse-grained Martini 3 force field <sup>64, 65</sup>. Membrane models were generated using the INSANE  
21 <sup>66</sup> methodology (<http://www.cgmartini.nl/images/tools/insane/insane.py>), which was modified to  
22 incorporate the Ala-PG and Lys-PG lipids. After initial setup, all systems were energy minimised  
23 using the steepest descents approach. Ions (sodium and chloride) were added to neutralize the system,  
24 and in the majority of the simulations they were added to a final concentration of  $\sim 0.15$  M.  
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31 All unbiased simulations underwent 5 ns of NVT and 10 ns of NPT equilibration with the peptide  
32 restrained in its initial position before launching a 1  $\mu$ s unrestrained production run. All simulations  
33 were run with a timestep of 20 fs. Temperature was coupled at 310 K using a velocity rescale  
34 thermostat <sup>67</sup> with a coupling time constant of 1 ps. Pressure coupling was carried out by a semi-  
35 isotropic Parrinello-Rahman barostat <sup>68</sup> at a reference pressure of 1 bar, compressibility at  $3 \times 10^{-4}$  bar<sup>-1</sup>  
36 with a coupling time of 12 ps. Electrostatic interactions were calculated using a reaction field potential  
37 with a cut-off of 1.1 nm. Van der Waals interactions were calculated using a Verlet cut-off scheme  
38 for beads within 1.1 nm of each other and the potential switched from 0.9 nm.  
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47 Free energy landscapes were determined by calculation of potentials of mean force (PMFs) with a  
48 collective variable (i.e. reaction coordinate) generated by pulling a peptide across the membrane.  
49 Bilayers were generated with  $\sim 170$  lipids (of a single species – see below and SI Table S3) in each  
50 leaflet in a  $10 \times 10 \times 25$  nm<sup>3</sup> box. The peptide was pulled through the membrane with the N terminus  
51 first, with the  $z$  coordinate of the peptide ranging from -5 nm to +5 nm from the bilayer centre.  
52 Peptides were pulled through the membrane N terminus first, as this has been suggested to be a  
53 preferred binding pose <sup>69, 70</sup>. Starting conformations were generated from the pull every 0.1 nm and  
54 simulated for 1  $\mu$ s. <sup>69, 70</sup>A restraining force of 1000 kJ mol<sup>-1</sup> nm<sup>-2</sup> was employed in the  $z$  direction  
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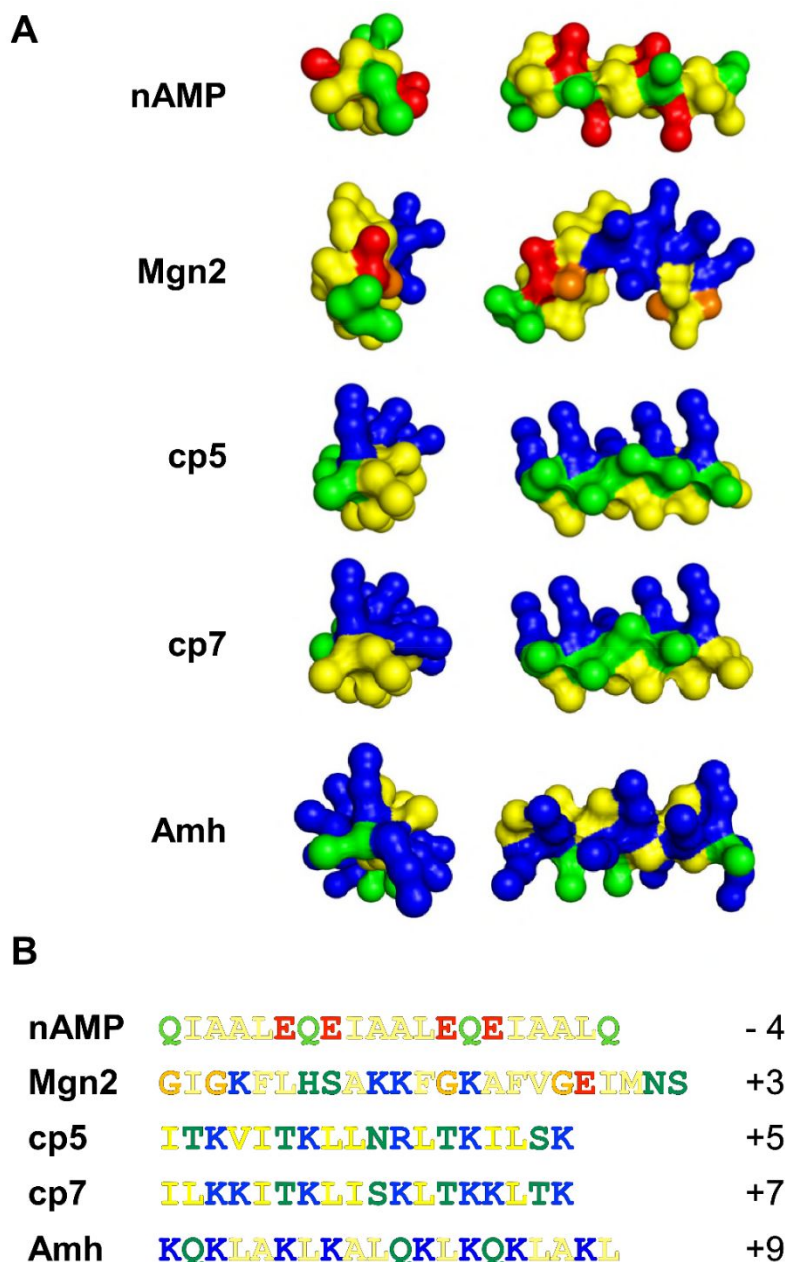
1 during each simulation window. Free energy landscapes were built using the weighted histogram  
2 analysis method <sup>71</sup>.

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7 Analysis was carried out using GROMACS tools and MDAnalysis <sup>72</sup>. VMD <sup>73</sup> and PyMOL <sup>61</sup> were  
8 used for molecular visualisation and rendering.  
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## 10 11 12 **RESULTS**

### 13 14 **Peptides and Lipid Bilayers Studied**

15 The overarching aim of this study is to test whether AMP resistance via MprF modification of  
16 bacterial membranes can be explained by a change in the electrostatic interaction of an AMP molecule  
17 with the membrane surface. To this end we selected five  $\alpha$ -helical peptides which are all amphipathic  
18 but which differ in their net charge and their antimicrobial activity (Fig. 1): magainin 2 (Mgn2) is a  
19 canonical cationic AMP <sup>15, 74</sup>; cp5 and cp7 are synthetic cationic AMPs with relatively simple  
20 sequences <sup>75</sup>}; and amhelin (Amh) is a *de novo* peptide designed to be an archetypal model of AMPs  
21 <sup>76</sup>. A negatively charged amphipathic peptide which lacks antimicrobial properties (nAMP) is  
22 included as a control. Lipid bilayer compositions were chosen to provide simple models of both  
23 unmodified bacterial membranes (PE:PG ~2:1) and models of MprF-modified membranes  
24 containing either Ala-PG or Lys-PG in place of PG. The compositions of these membranes were  
25 varied to model bacteria which different levels of MprF-mediated lipid modification (see SI Tables  
26 S1 and S2).  
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*Figure 1:*

**A** Structures of peptides shown in coarse-grained representation with cationic amino acid residues in blue, anionic residues in red, polar uncharged residues in green, and hydrophobic residues in yellow. All peptides were modelled as continuous  $\alpha$ -helices, apart from magainin 2 (Mgn2) for which the NMR structure determined in the presence of DPC micelles (PDB ID 2MAG) was employed. **B** The sequences and net charges of the peptides.

### Simulations reveal reduction of peptide binding due to lipid modifications

We first investigated whether membranes containing modified PG lipids showed reduced binding by AMPs compared to membranes in which only PG and PE lipids were present. An asymmetric lipid bilayer system was constructed. One leaflet of the bilayer contained PG, mimicking an unmodified

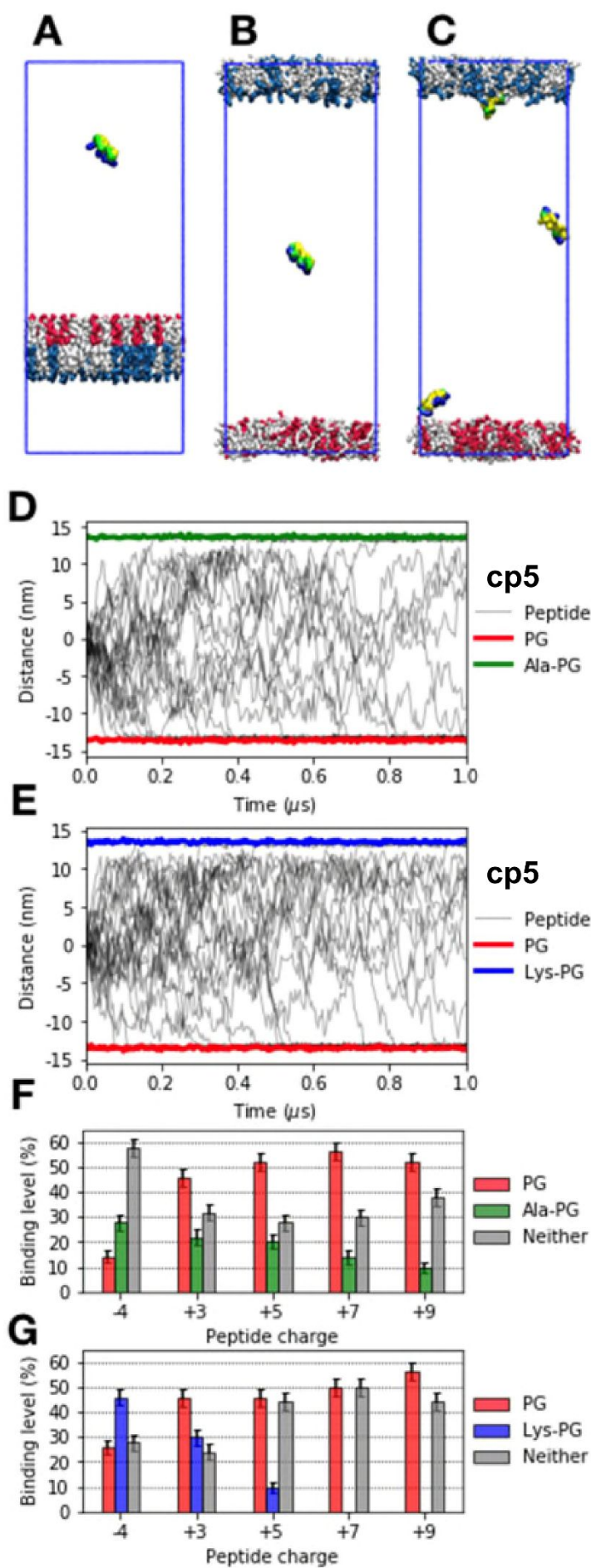


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(i.e. anionic) bacterial membrane (Fig. 2A). The other leaflet of the bilayer contained either Ala-PG or Lys-PG, representing a modified membrane. It is important to note that because of the use of periodic boundaries in the simulation, a peptide molecule initially placed in the aqueous phase about ~15 nm from the bilayer mid-plane (Fig. 2B), was able to freely access either face of the asymmetric membrane (Fig. 2C). Fifty simulations, each of a duration of 1  $\mu$ s, were run for each peptide-membrane system, and the position of the peptide relative to the two bilayer surfaces vs. time was tracked (Fig. 2D,E). Peptide binding levels to each leaflet were calculated as the percentage of simulations that resulted in the peptide interacting with a given leaflet. Binding was defined to have taken place when all peptide backbone beads remained within 0.5 nm of the closest phospholipid phosphate for over 5 ns, resulting in a peptide sitting parallel to the plane of the membrane.

Comparing the 5 peptides (see Fig. 1) and the two lipid modifications (Ala-PG, Fig. 2F and Lys-PG, Fig. 2G) our results demonstrate that the anionic PG leaflet is greatly preferred by all four cationic peptides relative to the zwitterionic Ala-PG and cationic Lys-PG leaflets. Furthermore, the more highly positively charged peptides show a greater preference for PG over the modified membranes, such that for peptides cp7 (charge +7) and Amh (charge +9) there were no detectable binding events with the Lys-PG leaflet. Comparison between the Ala-PG and Lys-PG systems showed that the Lys-PG modification had a more drastic effect than the Ala-PG modification. In contrast, the anionic control peptide nAMP displayed enhanced interaction with the Ala-PG and Lys-PG leaflets.



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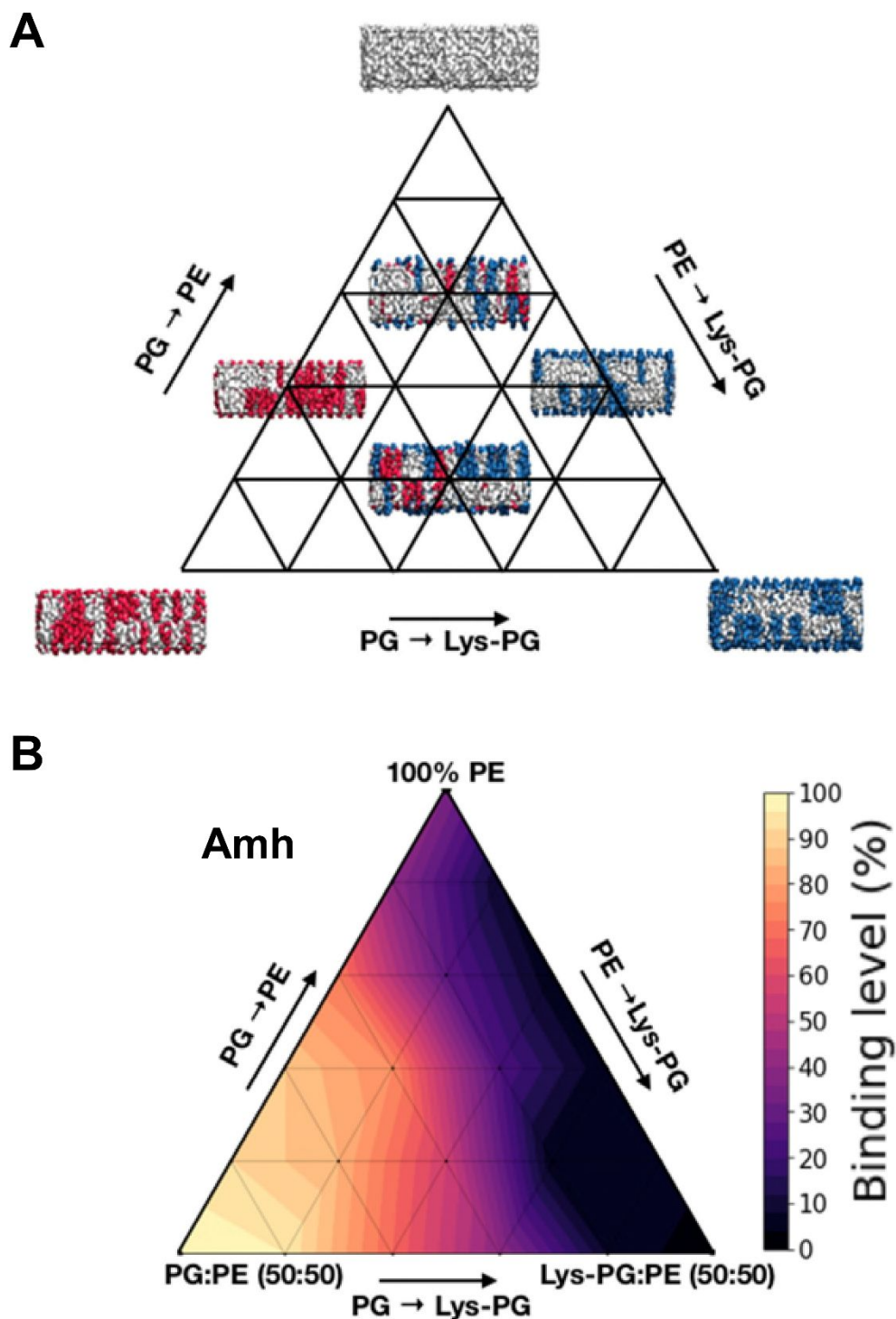
**Figure 2:**

**A** Peptides were placed in a simulation box along with a bilayer membrane with an asymmetric lipid composition. The bilayer contained ~225 lipids per leaflet in a 12 x 12 x 30 nm<sup>3</sup> box. **B** The membrane is split across periodic boundary conditions. A peptide molecule (cp5 above) was placed in the centre, ~13 nm from each leaflet surface. It should be noted that the  $z = 0$  plane in this figure corresponds to the centre of the water layer, *not* the centre of the bilayer. **C** Over 50 repeats, the cp5 peptide  $z$ -position is recorded and the binding to each leaflet is determined. Trajectories of the cp5 peptide with the **D** Ala-PG system and **E** Lys-PG systems are shown. **F** Binding levels for peptides with either the PG:PE or Ala-PG:PE leaflets. ‘Neither’ refers to a simulation in which the peptide did not bind to a membrane over the course of the simulation. **G** Binding levels for peptides with either the PG:PE, Lys-PG:PE leaflets or neither. Binding levels are defined as the percentage of simulations that result with the peptide binding to that specific leaflet. Errors are calculated through bootstrapping analysis.

**Peptide binding is modulated by the lipid bilayer composition**

We have seen that complete replacement of PG in a model bacterial membrane with either of the modified variants, Ala-PG or Lys-PG, leads to reduced selective binding of cationic peptides. However, *in vivo* membranes of bacteria expressing MprF are expected to contain both PG and Ala-PG and/or Lys-PG. The fractional composition of the modified lipids is believed to be dependent on bacterial strain and growth conditions, such that an acidic environment results in a larger number of modified lipids<sup>29,30</sup>. We therefore investigated peptide binding to bilayers composed of mixtures of PE and both PG and modified-PG lipids, thus defining how the bilayer composition of modified lipids affected the ability of AMPs to bind to the membrane.

Symmetric membranes of three components (PE:PG:Lys-PG or PE:PG:Ala-PG) were generated with lipid compositions ranging between PE (100%), PG:PE (50%:50%) to Lys-PG (or Ala-PG):PE (50%:50%) as defined on a triangular grid (Fig. 3A) with 10% increments in lipid composition between adjacent grid points (see also SI Table S2). This approach defined a lipid composition space for which AMP binding was investigated via 25 x 1  $\mu$ s simulations for each grid point (i.e. each lipid composition; Fig. 3B). The binding level for all 5 peptides was thus determined by the total number of interaction events with the bilayer, for both the PE:PG:Lys-PG and the PE:PG:Ala-PG systems (Fig. 4A).



*Figure 3:*

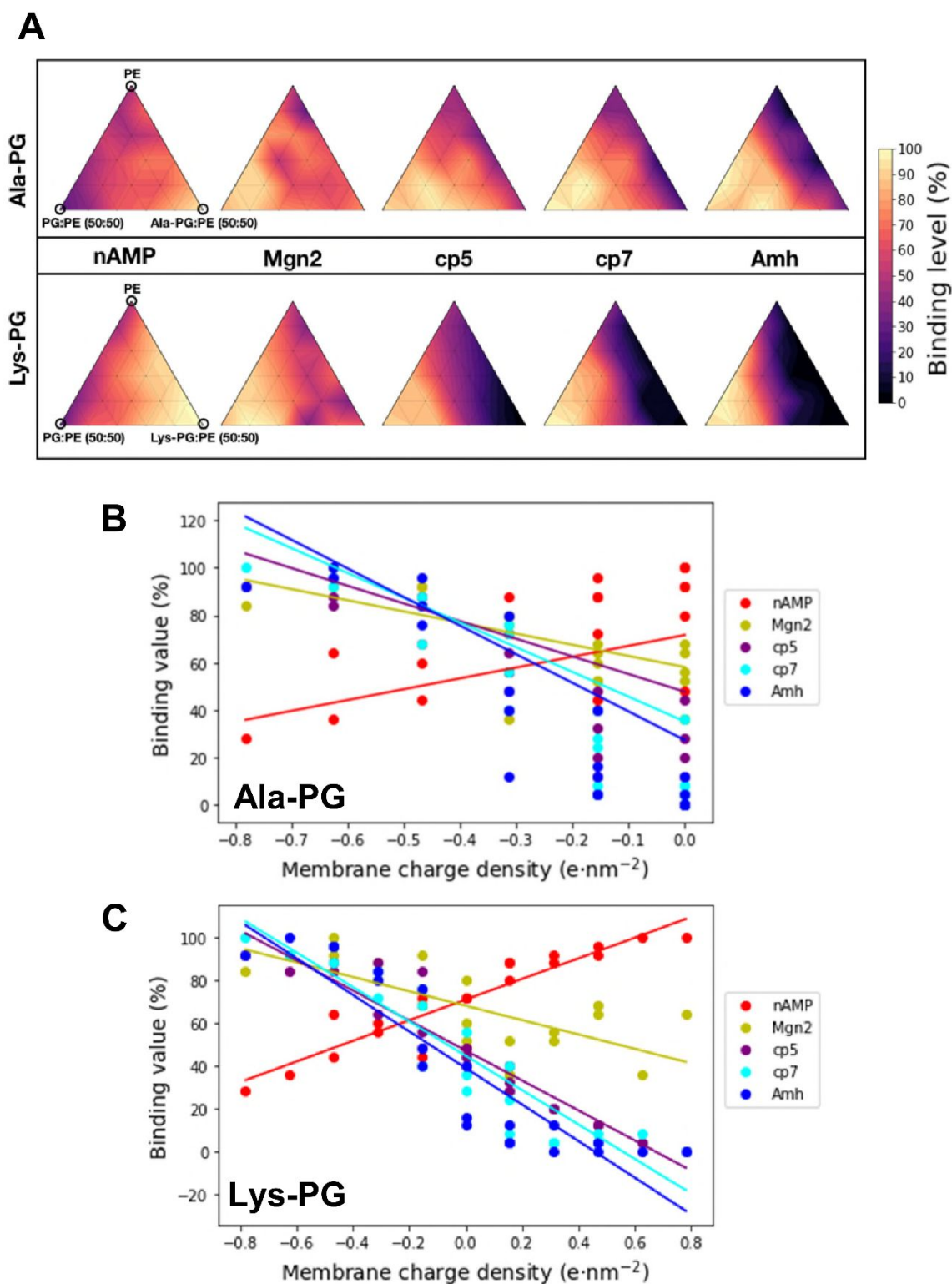
**A** Construction of lipid composition space to be investigated. Lipid compositions vary between 100 % PE, 50 % PG 50% PE and 50% Lys-PG or Ala-PG:PE. Membrane composition is varied by 10% at a time. Also see SI Table S2. **B** Peptide binding level vs. lipid composition space for a PG/PE/Lys-PG system with the Amh peptide. Binding level is calculated as the percentage of simulations in which the peptide binds to either leaflet of the membrane. A binding level of 0% (black) corresponds to no binding in any of the 25 repeats for that lipid composition, and a level of 100% (bright orange) represents every simulation resulting in binding.

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2 All of the cationic peptides exhibited greater levels of binding when PG was present in the membrane,  
3 whilst replacement of PG by Lys-PG resulted in a reduction in binding. For the most positively  
4 charged peptides, i.e. cp7 and Amh, binding decreased from ~100% to 0% when comparing  
5 membranes containing 50% PG to those containing 50% Lys-PG. The replacement of PG with Ala-  
6 PG also resulted in decreased cationic peptide binding, though this effect is less than that of Lys-PG,  
7 especially for the most positively charged peptides. In contrast, nAMP binding increased from ~30%  
8 with a 50% PG membrane to ~100% binding with the 50% Lys-PG membrane.  
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16 Broadly speaking, for any given peptide the binding level correlates with the membrane charge  
17 density, with the sign and strength of the correlation depending on the charge on the peptide (Fig.  
18 4BC). Thus, binding levels for nAMP show a positive correlation with increased (i.e. less negative,  
19 more positive) membrane surface charge density caused by lipid modification for both Ala-PG (Fig  
20 4B) and Lys-PG (Fig 4C). The three most positively charged peptides (cp5, cp7 and Amh) all show  
21 a strong negative correlation with increasing (positive) membrane charge density, whilst Mgn2 shows  
22 intermediate behaviour. Thus, whilst Mgn2 exhibits a decrease in binding upon the inclusion of Ala-  
23 PG and Lys-PG, its binding level rarely falls below 50% regardless of the lipid composition,  
24 suggesting less highly charged peptides may be more resilient to changes in the membrane  
25 electrostatic environment. We tested the robustness of our results to the concentration of ions used in  
26 the simulations (see SI Fig. S2). Doubling this from a physiological concentration of ~0.15 M to  
27 ~0.3M resulted in a small (< 10%) reduction of binding of e.g. the cp5 (+5) peptide to a PG/PE  
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**Figure 4:**

**A** Peptide binding level maps for peptides in membranes of varying lipid compositions. The binding in lipid composition is for each peptide is determined from  $900 \times 1 \mu\text{s}$  simulations. This data together represents 4.5 ms of data. **B,C** Correlation between the level of binding and the charge density of the bilayer for **B** Ala-PG containing bilayers and **C** Lys-PG containing bilayers, corresponding to the binding level maps shown in **A**.

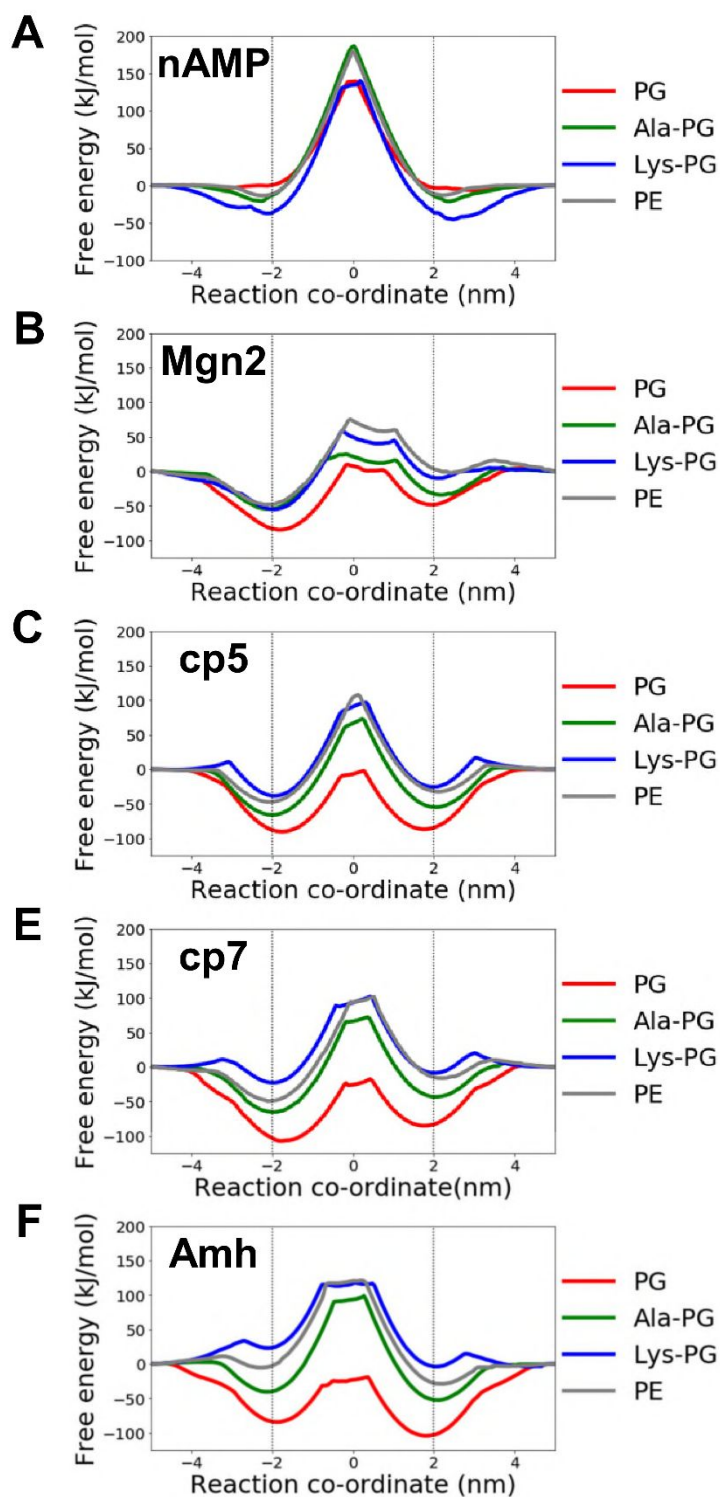
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**Free energy landscapes for single peptide molecule interactions with lipid bilayers**

Free energy landscapes for the interaction of single peptide molecules with bilayers of differing lipid compositions can provide a mechanistic understanding of the trends analysed above. To this end free energy landscapes were calculated using Potential of Mean Force (PMF) calculations with a reaction coordinate corresponding to the distance between the centre of mass of a single peptide molecule and the centre of mass of the lipid bilayer. For every position along this reaction coordinate the peptide was allowed to rotate relative to the bilayer normal so as to fully sample all possible orientations relative to the membrane.

PMFs were generated for the interaction of the five different peptides with lipid bilayers containing a single species of lipid (i.e. PE, PG, Lys-PG or Ala-PG; see SI Table S3). Thus, a total of 20 PMFs were estimated, as shown in Fig. 5. In these PMFs the initial position of the peptide was with its N terminus oriented towards the bilayer. The peptides were otherwise free to rotate. Analysis of the tilt angle between the peptide helix axis and the bilayer normal (SI Fig. S3) shows that the peptides rotate freely whilst in the aqueous region outside the bilayer, adopt a tilt angle of  $\sim 90^\circ$  (corresponding to parallel to the bilayer surface) when at the water/bilayer interface, before switching to the  $\sim 180^\circ$  whilst the helix spans the bilayer (centred around a reaction coordinate value of  $\sim 0$  nm). The two halves of the PMF are approximately equivalent, with the difference between the two corresponding to whether the N terminus or the C terminus of the peptide is approaching and/or penetrating the bilayer surface (i.e. the system and reaction coordinate is asymmetric so the PMF is expected to be asymmetric, as shown in SI Fig. S4).



*Figure 5:*

Potentials of mean force (PMFs) for single peptide helices with bilayers composed on PG (red), Ala-PG (green) Lys-PG (blue) or PE (grey). A reaction coordinate of 0 corresponds to the centre of the lipid bilayer. See text for further details.

The general shape of the PMFs is as anticipated (Fig. 5), with a central barrier corresponding to a transmembrane orientation of the peptide helix, with free energy wells either side of this



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2 corresponding to the peptide lying at the bilayer/water interface, partially penetrating the bilayer  
3 surface (SI Fig. S5) and interacting extensively with the lipid headgroups. The depth of the free  
4 energy well for each peptide, corresponding to the free energy difference for transfer of the peptide  
5 from the aqueous phase to the peptide bound at the water/membrane interface, can be seen to depend  
6 on both the lipid species and the charge on the peptide Fig. 6A). From these data we may calculate  
7  $\Delta\Delta G_{WELL}$  (PG-KPG or PG-APG) which corresponds to the change in well depth when a PG membrane  
8 is changed to either Lys-PG or Ala-PG. Plotting  $\Delta\Delta G_{WELL}$  as a function of peptide charge reveals a  
9 linear relationship for Lys-PG and for Ala-PG, in both cases passing through the (0,0) origin (Fig. 6B).  
10 This demonstrates the importance of peptide charge and the stronger effect of PG being replaced by  
11 Lys-PG than by Ala-PG. Note that these graphs show the effect on the free energy of peptide binding  
12 of complete replacement of a PG membrane by either Lys-PG or Ala-PG.

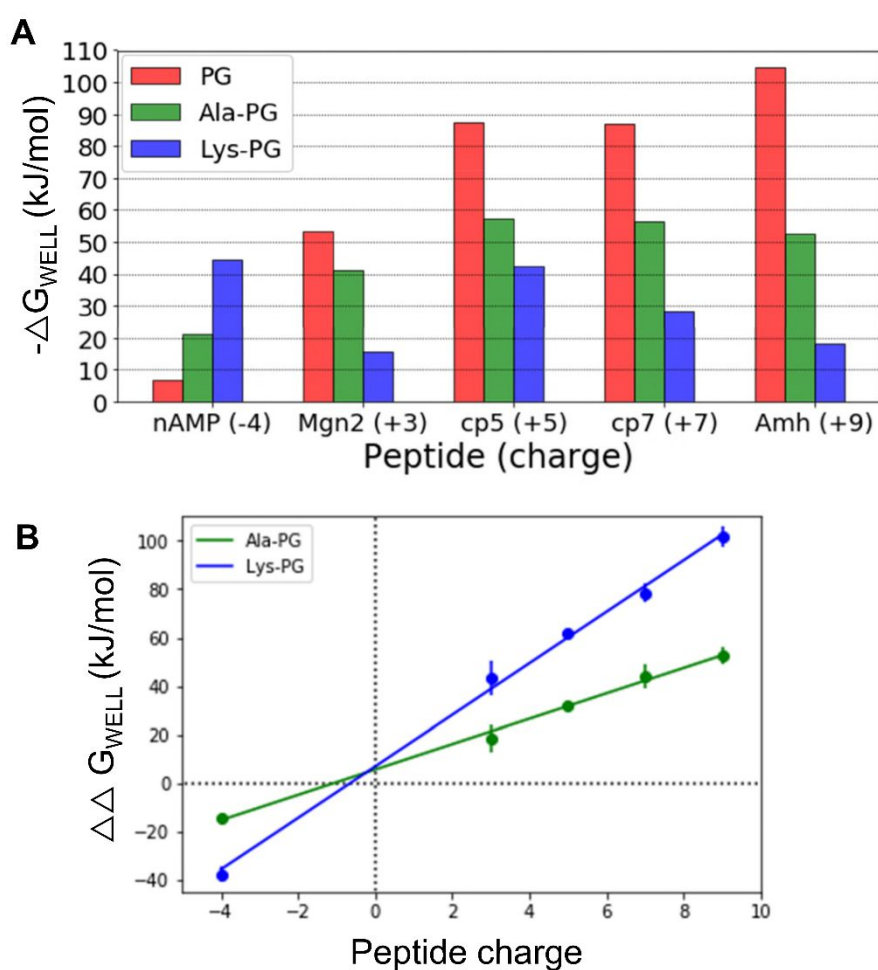


Figure 6:

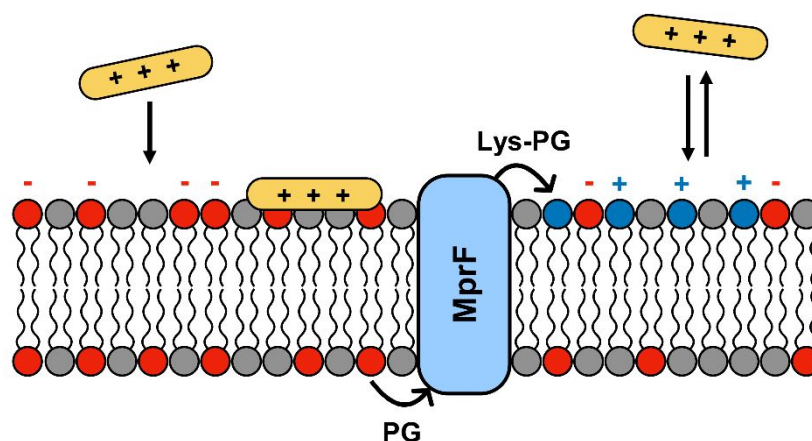
Depths of the free energy wells for peptide binding to the membrane surface derived from the PMFs shown in Fig. 5. **A** Depth of interfacial free energy wells for each peptide/membrane combination derived from the PMFs in Fig. 5. These correspond to the energy required to leave the membrane-water interface when the peptide is bound. They are determined only for the N-terminal approach to the membrane (i.e. the right-hand side in Fig. 5), as this is the suggested approach path for binding. **B** Change in free energy well depth when a PG membrane is changed to either Lys-PG or Ala-PG.

Graphs of data derived from **A**, showing  $\Delta\Delta G_{WELL}$ (PG-KPG or PG-APG) as a function of peptide charge with corresponding best linear fits. If  $\Delta\Delta G_{WELL}$  is positive that correspond to the modification of the lipid resulting in stronger binding of the peptide compared to a pure PG membrane.

All peptides show a large free energy barrier corresponding to the shift from an interfacial location to a membrane-spanning orientation. As suggested elsewhere<sup>77</sup>, this indicates that spontaneous insertion of single peptide molecules is unlikely to occur. However, cooperative insertion of multiple peptide molecules is likely to favour insertion and subsequent pore formation and/or membrane disruption<sup>78</sup>. Such peptide insertion may also be sensitive to lipid acyl tail species<sup>79</sup>.

## DISCUSSION

Our simulations clearly demonstrate that the conversion of PG into either Ala-PG or Lys-PG leads to electrostatic repulsion of positively charged peptides and a reduction in the binding of these peptides to the membrane (Figure 7). This effect is more dramatic for membrane systems containing Lys-PG, as this lipid has a greater effect on the change in the surface electrostatics of the membrane. Increasing the charge of the peptide compounds the reduction in binding. In contrast, the negatively charged peptide nAMP shows a greater binding preference for modified lipid membranes. Thus it is expected that the activity of MprF would correlate with an increase in binding of anionic peptides. However, nAMP is not a pore-forming peptide and has no antimicrobial action. However, it may provide a template for the design of peptides that can bind to and disrupt MprF-modified bacterial membranes.



*Figure 7:*

Cationic peptides (orange) bind to a negatively charged membrane. The action of the MprF protein (blue) modifies the electrostatics of the membrane via the conversion of PG lipids into Ala-PG (zwitterionic) or Lys-PG (cationic). The altered surface charge prevents peptides from binding to the membrane.

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Our results from varying the bilayer compositions suggest a substantial fraction of the membrane has to be composed of Lys-PG to have a notable effect on peptide binding. From our lipid composition diagrams (Fig 4C) we see that compared to a ‘wild type-like’ membrane composed of 50:50 PG:PE, ~40% conversion (corresponding to reduction in membrane charge density below  $0.5 e\text{-nm}^{-2}$ ; Fig 4D), is required to observe the beginning of a substantive drop-off in binding of cp5, cp7 and Amh. Lipid composition is variable between different species and strains of bacteria and also dependent on environmental conditions, for example Lys-PG content has been shown to increase during the growth phase<sup>80</sup>. Furthermore, *S. aureus* membranes can contain ~35% Lys-PG during the growth phase<sup>32</sup>, at which level we would predict there should be a reduction in AMP binding. At this lipid composition the MIC of the human AMP, LL-37<sup>81</sup> is  $>300 \mu\text{g/ml}$ , compared with a *S. aureus* mutant with 0% Lys-PG in its membranes which has a MIC of  $\sim 75 \mu\text{g/ml}$ .

It is useful to reflect critically upon the methodology employed. Given the importance of electrostatic interactions between membrane and peptides<sup>82-85</sup> we considered an approach based on combining Poisson-Boltzmann calculations and Brownian dynamics (BD), as has been used previously to model e.g. PH domain binding to anionic membranes<sup>86</sup>. However, whilst such an approach offers a number of advantages (e.g. estimation of rate constants for association<sup>87, 88</sup>) it has the limitation that the bilayer surface is described by a fixed surface charge density, which does not respond to the proximity of a charged peptide<sup>89</sup> during e.g. a BD simulation, and cannot allow the peptide to partially penetrate the surface of the bilayer. Given previous studies of PH domains have shown that anionic lipids can cluster around a bound cationic protein<sup>90</sup> we were concerned to allow this interplay between peptide interaction and lipid redistribution to take place during our simulations, and hence adopted a CG-MD approach to characterise peptide/bilayer interactions. Comparison of lipid radial distribution functions derived from such simulations in the presence vs. absence of bound peptide molecules (see e.g. SI Fig. S6) confirmed effects of peptide interaction on lipid distribution. It could be interesting in a future study to use our CG-MD simulations to optimize PB/BD parameters (perhaps also using constant-pH BD<sup>91</sup>) and to compare the two simulation approaches (i.e. CG-MD and BD) for high throughput screening of peptides.

One limitation of the CG method as applied is the approximate treatment of ions. However, increasing the concentration of ions from a physiological concentration of  $\sim 0.15 \text{ M}$  to  $\sim 0.3 \text{ M}$  resulted in only a small ( $< 10\%$ ) reduction of binding of e.g. the cp5 (+5) peptide to a PG/PE membrane (see SI Fig. S2). In calculating PMFs for the interaction of peptides with different membranes, we have so far restricted ourselves to single lipid species in the bilayer. This could in principle be extended to more complex mixed bilayer compositions (as in the unrestrained simulations), although the relatively slow

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2 relaxation of lipids around an interacting peptide would mean that careful monitoring of convergence  
3 would be essential. A further limitation of the CG-MD approach is that the secondary structure of the  
4 peptides is restrained during the simulations. These restraints are somewhat weaker at the helix  
5 termini, thus allowing a degree of the local distortion of the termini of the otherwise stable helices  
6 (SI Fig. S7A). To explore further the behaviour of a peptide when bound to the surface of a bilayer,  
7 we have in a number of cases taken final snapshots from CG simulations of a peptide bound at the  
8 bilayer surface, and used these as the starting point for all atom (3 x 300 ns) simulations (SI Fig.  
9 S7B). Over the duration of these (short) AT MD simulations, the overall helicity of the bound peptide  
10 is maintained whilst a degree of flexibility at the termini is observed.  
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19 Undoubtedly, the mechanism of action of AMPs is much more complicated than simply binding of  
20 peptides to a bilayer. However, it is clear that if lipid modification reduces the affinity of a peptide  
21 for a bacterial membrane, then the downstream efficacy of that peptide will also be substantially  
22 reduced. It is also important to note that we investigated peptide binding to the membrane, not folding  
23 of the peptide at or close to the membrane surface. It is known that AMPs adopt their preferred  
24 secondary structure upon association with a membrane or membrane-like surface<sup>92</sup>. The folding  
25 process may affect how peptides penetrate the membrane and may provide a partial explanation as to  
26 why the free energy of peptides spanning the hydrophobic core is so large. This question may be  
27 addressed further using all-atom simulations<sup>51</sup>.  
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36 Based on the results presented here we conclude that MprF brings about resistance by reducing  
37 peptide binding to the membrane *prior* to subsequent aggregation of peptides and pore formation.  
38 This would correspond to a resistance mechanism against a broad range of cationic AMPs as it would  
39 be expected to lead to resistance, independent of the exact mechanism of subsequent pore formation  
40 and/or peptide internalization for downstream metabolic effects<sup>13</sup>.  
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47 We can use our simulations to address the functionally relevant question of what percentage of lipid  
48 modification has to occur for AMP binding to be substantially decreased. From considerations of the  
49 computational biophysics of peptide/bilayer interactions it would seem that >40% modification may  
50 be required. As we continue to explore and design peptides with different modes of action<sup>93-95</sup> in  
51 order to address antimicrobial resistance, it will become increasingly important to take account of the  
52 quantitative effects of changes in lipid composition on interactions with these peptides<sup>96</sup>. From a  
53 methodological perspective, our studies indicate the CG MD simulations allow us to explore the  
54 interplay of peptide sequence and lipid bilayer composition in a computationally efficient manner  
55 which lends itself to machine learning approaches to molecular design<sup>97</sup>.  
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## SUPPORTING INFORMATION

A supporting information file containing seven figures and three tables is available. This information is available free of charge via the Internet at <http://pubs.acs.org>.

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