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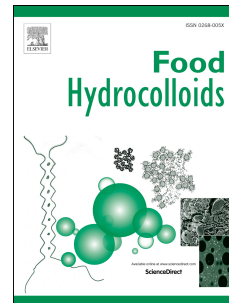
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Hydroxypropyl methylcellulose and hydroxypropyl starch: Rheological and gelation effects on the phase structure of their mixed hydrocolloid system

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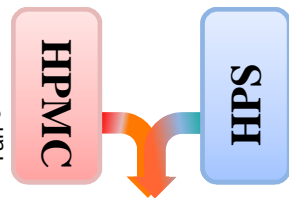
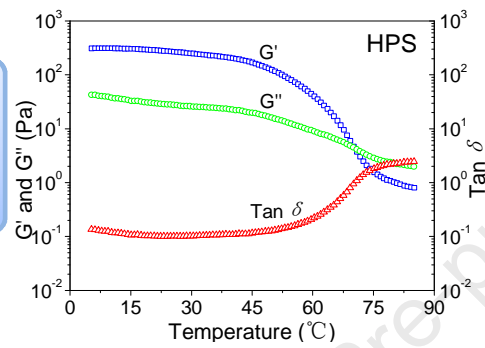
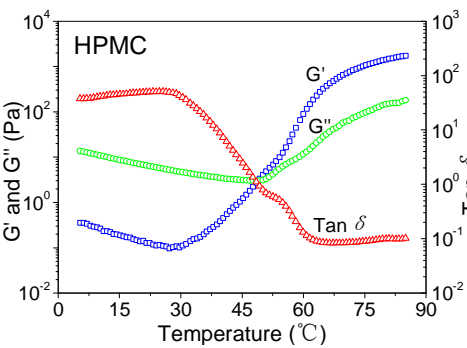
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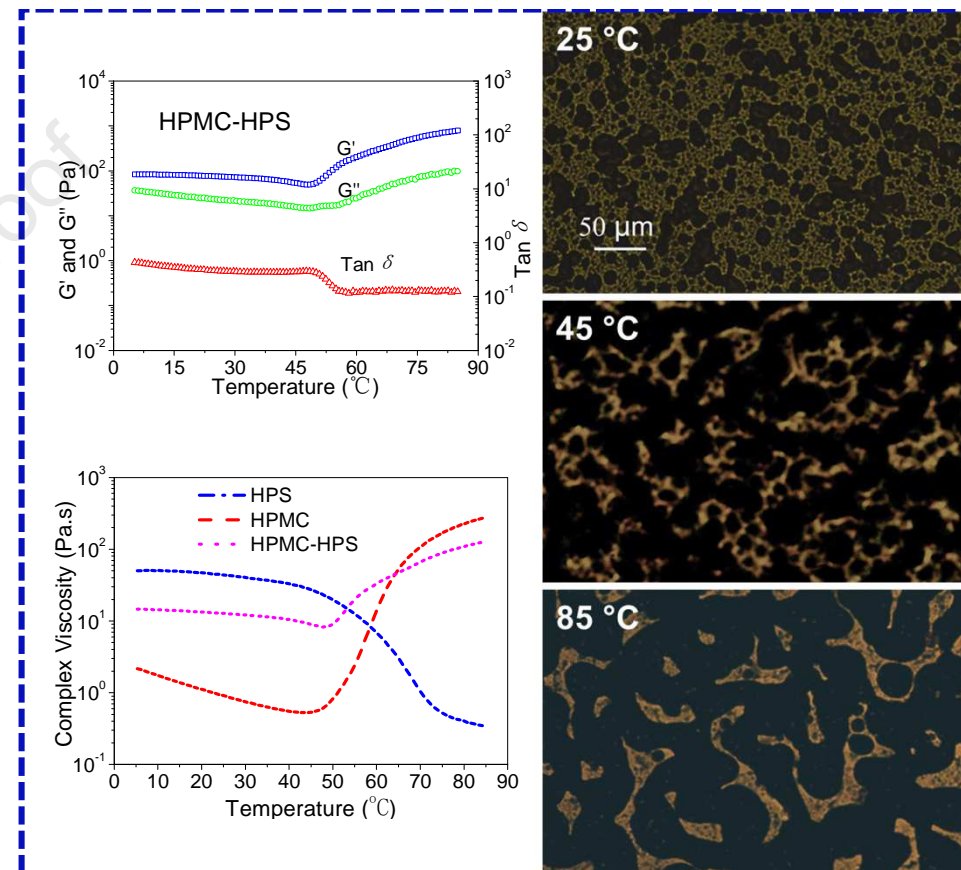
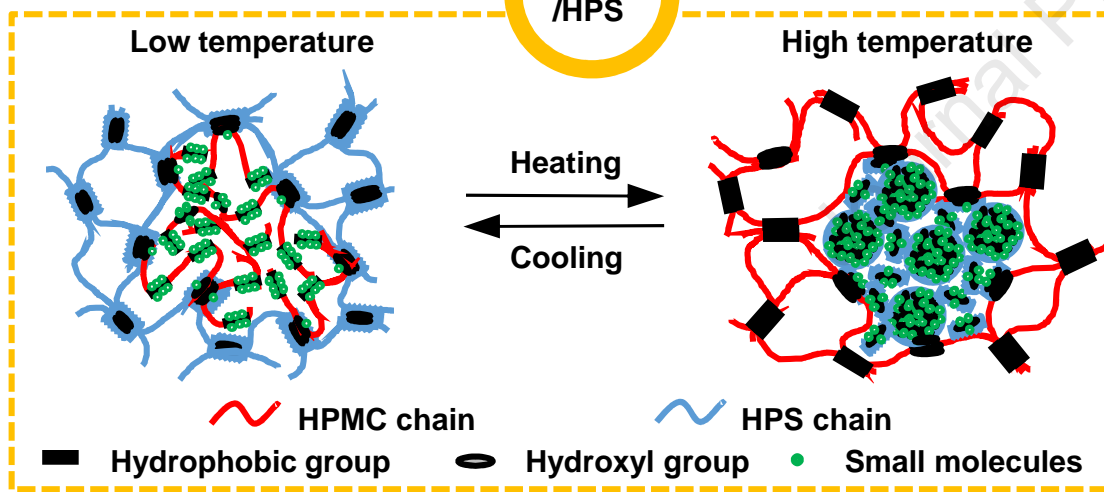
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Journal Pre-proof



HPMC /HPS



1 Hydroxypropyl methylcellulose and hydroxypropyl starch:
2 Rheological and gelation effects on the phase structure of their
3 mixed hydrocolloid system

4
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15 **Abstract**

16 It is common to hybridize biopolymers for developing materials with combined properties or
17 functionality. However, biopolymers are usually not fully compatible despite their chemical
18 similarity, posing challenges to create mixed systems. Herein, we investigated how the gelation
19 behavior and rheological properties of hydroxypropyl methylcellulose (HPMC), a thermal gel, and
20 hydroxypropyl starch (HPS), a cooling gel, affect their miscibility and the phase structure of their
21 mixed system. The dependence of the zero-shear viscosity for HPMC/HPS paste on biopolymer
22 concentration in a double-logarithmic coordinate can be divided into two parts with the slopes being
23 11.9 and 2.8 respectively, indicating different degrees of intermolecular entanglement. A typical
24 “sea-island” morphology was shown in the blends, and the phase structure (continuous or discrete)
25 changed with varying HPMC/HPS blend ratio and temperature. This phase structure change can be
26 well correlated to rheological parameters such as zero-shear viscosity, loss tangent, complex
27 viscosity, and the Arrhenius equation correction coefficient (α). Biopolymer concentration,
28 HPMC/HPS ratio, and temperature together controlled rheological properties and phase distribution
29 for the mixed system. The relationship between rheological behavior and phase structure for
30 HPMC/HPS understood from this work provides an insight into designing mixed biopolymer
31 systems with desirable processability, structure, and properties.

32 **Keywords:** Hydroxypropyl methylcellulose; Hydroxypropyl starch; Rheological properties;
33 Biopolymer phase structure; Biopolymer blends

34

35 **1 Introduction**

36 As a modified biopolymer, hydroxypropyl methylcellulose (HPMC) has been widely applied in
37 different applications such as edible packaging, medicinal capsules, and drug delivery systems due to
38 its water-solubility and biodegradability and excellent film-forming, mechanical and barrier
39 properties (Al-Tabakha, 2010; Muhammad-Javeed & Mohammed, 2018; Siepmann & Peppas, 2012).
40 However, the low oxygen-barrier property (Ghadermazi, Hamdipour, Sadeghi, Ghadermazi, & Asl,
41 2019; Hay, et al., 2018; Y. F. Wang, Yu, et al., 2016), high production energy consumption (Zhang,
42 et al., 2013), and high price of HPMC (Allenspach, Timmins, Sharif, & Minko, 2020) pose strong
43 limits for its applications. To cope with the property limitations of individual polymers, achieve
44 enhanced and/or new material properties, reduce costs, and to expand applications, mixing different
45 polymers is one of the most cost-effective methods (Aghjeh, Khonakdar, & Jafari, 2015; Botaro, de
46 Freitas, do Carmo, & Raimundo, 2020; Jéssica Bassi da Silva, Michael Thomas Cook, & Bruschi,
47 2020; Xu, Wang, & Shi, 2020). Hydroxypropyl starch (HPS), a typical chemically modified starch
48 with some original hydroxyl groups replaced with hydroxypropyl groups, is cheaper than HPMC,
49 show excellent gas barrier property, and has been widely used in the food industry, therefore being
50 an ideal substitute for part of HPMC (X. Chen, et al., 2019; J. Liu, Lai, Wang, Wang, & Liu, 2020;
51 Qin, et al., 2019; W. W. Wang, Sun, & Shi, 2019).

52 The production of edible materials such as pre-formed films (medicinal capsules) or edible
53 coating generally relies on wet processes that are based on film-forming solutions or dispersions
54 (Cuq, Gontard, & Guilbert, 1998; Suhag, Kumar, Petkoska, & Upadhyay, 2020). Specifically,
55 polymers are first dissolved or dispersed in a liquid and then dried. The design of such processes

56 (typically comprising pumping, casting, dipping, brushing, spraying, and drying) requires accurate
57 data on the rheological properties of film-forming solutions or dispersions (Q. Wang, Yang, Chen, &
58 Shao, 2012). In turn, rheological properties also play an important role in controlling the quality of
59 coating films (Peressini, Bravin, Lapasin, Rizzotti, & Sensidoni, 2003; Xiao, Tong, & Lim, 2012).

60 For thermodynamic reasons, most polymer blends are immiscible on a molecular scale.
61 Nevertheless, immiscible blends often turn out to be useful. For example, while polypropylene and
62 polystyrene are immiscible, a polypropylene 90/polystyrene 10 blend, which showed a phase
63 separation structure where polystyrene droplets were scattered in the polypropylene matrix, showed
64 the maximum impact strength that blends at other ratios (R. Y. Chen, Liu, Han, Zhang, & Li, 2020).
65 The degree of polymer miscibility largely influences the rheological properties of the mixed systems
66 (Tanaka, Sako, Hiraoka, Yamaguchi, & Yamaguchi, 2020; Wongphan & Harnkarnsujarit, 2020).
67 And, the rheological properties of polymer blends determine material phase structure (Ilyin,
68 Makarova, Polyakova, & Kulichikhin, 2020; Xiao, Tong, Zhou, & Deng, 2015).

69 Considering that both HPMC and HPS are water-soluble polysaccharides and consist of the same
70 original repeat unit (glucose with hydroxyl groups), there should be good compatibility between
71 them. However, HPMC and HPS are hydrogels with opposite temperature-induced gelation behavior.
72 Specifically, HPMC dissolves in water at a low temperature and congeals at a high temperature,
73 whereas HPS undergoes gelation on cooling but solates upon heating (Polamapilly, et al., 2019; Qin,
74 et al., 2019; Zhong, et al., 2020). The difference in gelation behavior between HPMC and HPS
75 makes it challenging to achieve a blend of these two biopolymers with high miscibility and fine
76 phase distribution. Moreover, the phase structure of HPMC and HPS should influence the mixed gel

77 properties. The rheological properties of HPMC/HPS blends depend on several factors such as
78 biopolymer concentration, mixing ratio, temperature, and shear stress applied (Y. F. Wang, Zhang, et
79 al., 2016). The manipulation of these factors can be used to further explore the relationship between
80 microstructure and properties for thermal-/cooling-gel mixed systems.

81 In this work, the effects of solution concentration, mixing ratio, and temperature on the
82 rheological properties and morphology of HPMC/HPS blends were investigated. A schematic model
83 is proposed to describe temperature-induced phase structure changes for HPMC/HPS blends. The
84 knowledge obtained from this work could also help in understanding the relationship between
85 microstructure and processability for mixed systems based on biopolymers with different gelation
86 behavior. The results could also be insightful for the design of similar biopolymer composite
87 materials with tailored structure and properties.

88 **2 Materials and method**

89 **2.1 Materials**

90 A commercially available pharmaceutical-grade HPMC (HT-E15; viscosity at 2% concentration:
91 6.3 mPas; pH 6.0; methoxyl content on dry basis: 29%; hydroxypropyl oxygen content on dry basis
92 8.4%) was purchased from Huzhou Hopetop Pharmaceutical Co., Ltd (China). A food-grade maize
93 HPS with a degree of substitution (DS) of 0.11 was supplied by Penford (Australia).

94 **2.2 Sample preparation**

95 HPMC/HPS solutions with different total biopolymer concentration (5–20 wt%) and weight ratio
96 (0:10 to 10:0, w/w) were prepared. Specifically, HPMC and HPS in the form of dry powder were

97 firstly mixed and then dispersed in hot water (70 °C) with stirring for 30 min to ensure their proper
98 dispersion. Then, using a water bath, the solutions were heated to 95 °C and maintained for 1 h with
99 stirring to gelatinize HPS. Afterwards, the solutions were cooled to room temperature to dissolve
100 HPMC under stirring before testing.

101 **2.3 Rheological measurement**

102 The rheological properties of HPMC/HPS pastes were investigated using a Discovery HR-2
103 rheometer (TA Instruments, New Castle, DE, USA). A parallel-plate geometry (40 mm diameter)
104 with a gap of 0.5 mm was used for measurement.

105 To study the stability of HPMC/HPS pastes under shear, the samples were subjected to steady
106 shear at a constant high shear rate of 800 s⁻¹ for 2500 s at 25 °C and the change in viscosity was
107 recorded.

108 Under steady shear, the viscosity of a polymer may change with time before a stable value is
109 achieved (Tajuddin, Xie, Nicholson, Liu, & Halley, 2011). As a result, pre-shearing with a shear rate
110 of 800 s⁻¹ at room temperature (25 °C) for 1000 s was performed to ensure all samples to achieve a
111 stable rheological state before immediate measurement. Shear viscosity was measured as a function
112 of shear rate in the range of 10⁻²–10³ s.

113 Three-interval thixotropy testing was performed to investigate the stability of HPMC/HPS pastes.
114 This test was carried out at 25 °C at a low-shear stage with the shear rate kept at 1 s⁻¹ for 50 s, then a
115 high-shear stage with the shear rate kept at 1000 s⁻¹ for 20 s, and finally, a structural recovery stage
116 with the shear rate kept at 1 s⁻¹ for 250 s.

117 Temperature sweeps were carried out from 5 °C to 85 °C with a heating rate of 2 °C/min under
118 dynamic mode. The frequency was set at 1 Hz and the strain at 0.1% (to be in the linear range of
119 viscoelasticity). The sample was placed between the parallel plates, and then a small amount of
120 silicone oil was applied to the periphery of the sample to prevent moisture evaporation.

121 **2.4 Microscopy observation and method of dying HPS**

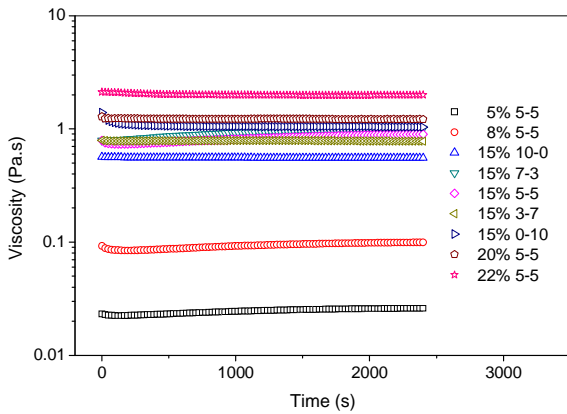
122 An Olympus BHZ-UMA optical microscope was used to image the morphology of HPMC/HPS
123 pastes. The HPMC/HPS (5:5, w/w) solution of a concentration of 3 wt% was prepared using the
124 same method mentioned above. The glass and the solution were kept at the same testing temperature
125 and then the films were prepared by casting the solutions on glass at different temperatures (25 °C,
126 45 °C, and 85 °C). HPS was dyed with 1% iodine alcohol solution (prepared by mixing 1g of iodine
127 and 10 g of potassium iodine solution in a 100 mL flask, with alcohol subsequently added) and dried
128 at the same testing temperature.

129 **3 Results and discussions**

130 **3.1 Time-dependence of HPMC/HPS paste viscosity**

131 **Fig. 1** shows the viscosity vs. time curves for HPMC/HPS blends with different selected blending
132 ratio and concentrations at a constant shear rate of 800 s⁻¹ (not all results presented here, as the trend
133 was quite similar). For all blends, the viscosity decreased with time until a stable value was achieved.
134 The time needed for achieving a stable state varied with HPMC/HPS ratio and total biopolymer
135 concentration. After 1000 s, all the samples reached constant viscosity. Therefore, pre-shearing at
136 800 s⁻¹ for 1000 s was performed for rheological tests for all the samples.

137



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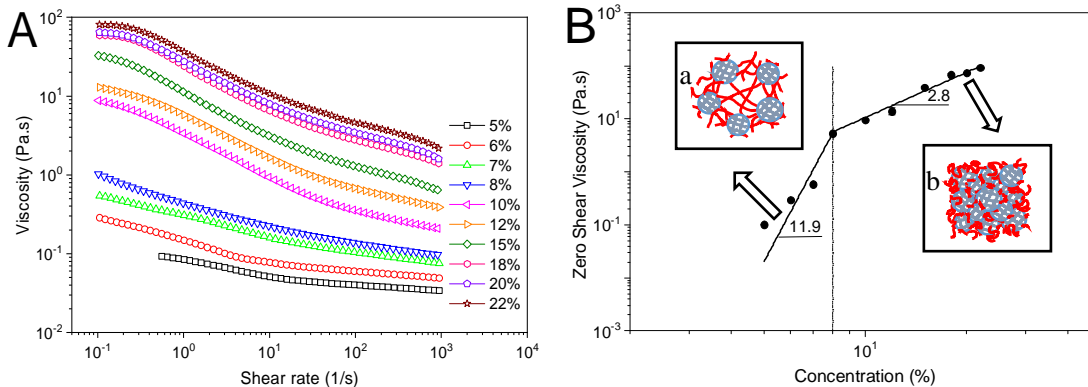
139 **Fig. 1** Viscosity as a function of time for HPMC/HPS pastes. The shear rate was fixed at 800 s^{-1} .

140

141 3.2 Effect of biopolymer concentration on HPMC/HPS paste viscosity

142 **Fig. 2(A)** shows the viscosity vs. shear rate curves for HPMC/HPS pastes of different
 143 concentration. At a certain shear rate, increasing biopolymer concentration resulted in higher
 144 viscosity, which is as expected. For all HPMC/HPS pastes, the viscosity decreased with increasing
 145 shear rate, suggesting shear-thinning behavior. Moreover, the dependence of viscosity on shear rate
 146 depended on total biopolymer concentration. The shear-thinning behavior was more evident with a
 147 higher biopolymer concentration.

148



149

150 **Fig. 2 A)** Flow curves for 50:50 (w/w) HPMC/HPS pastes of different total biopolymer
 151 concentration at 25 °C; B) Zero-shear viscosity as a function of total biopolymer concentration, with
 152 the molecular conformation of HPMC/HPS schematically shown (the HPMC/HPS ratio was 50:50
 153 (w/w), red lines represent HPMC chains and grey lines HPS).

154

155 The viscosity vs. shear rate curves for HPMC/HPS pastes were fitted with the Carreau model
 156 (Carreau, Pierre, & J., 1972) and then extrapolated to obtain zero-shear viscosity, η_0 ($0.9969 < R^2 <$
 157 0.9997). **Fig. 2(B)** shows zero-shear viscosity as a function of total biopolymer concentration. It is
 158 noticeable that η_0 had a power-law dependence on biopolymer concentration as represented by the
 159 equation below:

$$160 \quad \eta_0 = kC^m \quad (1)$$

161 Where η_0 is the zero-shear viscosity, C is the total biopolymer concentration, k and m are constants.

162 The dependence of η_0 on biopolymer concentration in a double-logarithmic coordinate can be
 163 divided into two parts with the slopes (m) being 11.9 and 2.8, respectively. The critical concentration
 164 (C^*) that divides the two regions was about 8 wt%. According to the general relationship between
 165 biopolymer concentration dependence and the polymer state in solution (Colby, 2010), the likely
 166 molecular conformation of HPMC/HPS blends was proposed schematically in the inset of **Fig. 2(B)**.

167 As the lowest concentration (5 wt%) in our work is still much higher than those used in previous
 168 studies (0.05–1.3 wt%) (Morris, Cutler, Ross-Murphy, Rees, & Price, 1981; Pakravan, Heuzey, &
 169 Ajji, 2011; Tan, Li, Chen, & Xie, 2016), likely, the samples in both regions were in a concentrated
 170 state. In the first region ($C < C^*$), gelatinized HPS thickened at a low temperature and forms
 171 microgel, which interacts with HPMC chains at the microgel particle edge. HPS microgel particles

172 and HPMC chains tended to interact or entangle with each other due to the space-block effect and
 173 hydrogen bonding (inset a of **Fig. 2B**). The η_0 of HPMC/HPS paste increased rapidly with increasing
 174 concentration. In the second region ($C > C^*$), the interactions and entanglements were already dens
 175 enough (inset b of **Fig. 2B**) and their enhancement by increasing concentration was not as effective
 176 as in the first region. Thus, the slope for the second region was not as high as the first region.

177 For a polymer solution, the relationship between shear stress (τ) and shear rate ($\dot{\gamma}$) can be
 178 described by the Ostwald-de Waele equation:

$$179 \quad \tau = K\dot{\gamma}^n \quad (2)$$

180 Where K is the fluid consistency index and n is the flow behavior index. The values of K and n
 181 calculated for HPMC/HPS pastes of different concentration are shown in **Table 1**.

182 For a Newtonian fluid, n equals 1. Pseudoplastic fluids have $n < 1$, and greater deviation of n
 183 from 1 indicates stronger pseudoplastic (shear-thinning) behavior. **Table 1** shows that for all the
 184 samples, n is less than 1, indicating they were all pseudoplastic (shear-thinning). For HPMC/HPS
 185 pastes of low concentration (e.g. 5 wt%), the n values are close to 1, meaning they were more like a
 186 Newtonian fluid as HPMC chains and HPS microgel particles are mostly separated in the solution.
 187 Increasing concentration led to lower n , suggesting stronger shear-thinning behavior. The flow
 188 behavior of high-concentration samples is attributed to the interaction and entanglement among
 189 HPMC/HPS chains.

190
 191 **Table 1** Flow behavior index (n) and fluid consistency index (K) for 50:50 (w/w) HPS/HPMC pastes
 192 of different concentration at 25 °C.

Concentration (%)	n	K (Pa·s ^{n})	R^2
-------------------	-----	---------------------------------------	-------

5	0.922±0.004 ^a	0.06±0.00	1.0000
6	0.909±0.001	0.09±0.00	1.0000
7	0.859±0.002	0.20±0.01	1.0000
8	0.842±0.001	0.28±0.01	0.9999
10	0.747±0.003	1.15±0.05	0.9981
12	0.735±0.005	2.34±0.07	0.9988
15	0.681±0.006	6.27±0.94	0.9993
18	0.678±0.006	13.37±0.88	0.9991
20	0.656±0.000	18.06±0.54	0.9984
22	0.653±0.012	24.40±2.31	0.9979

^a Mean ± standard deviation.

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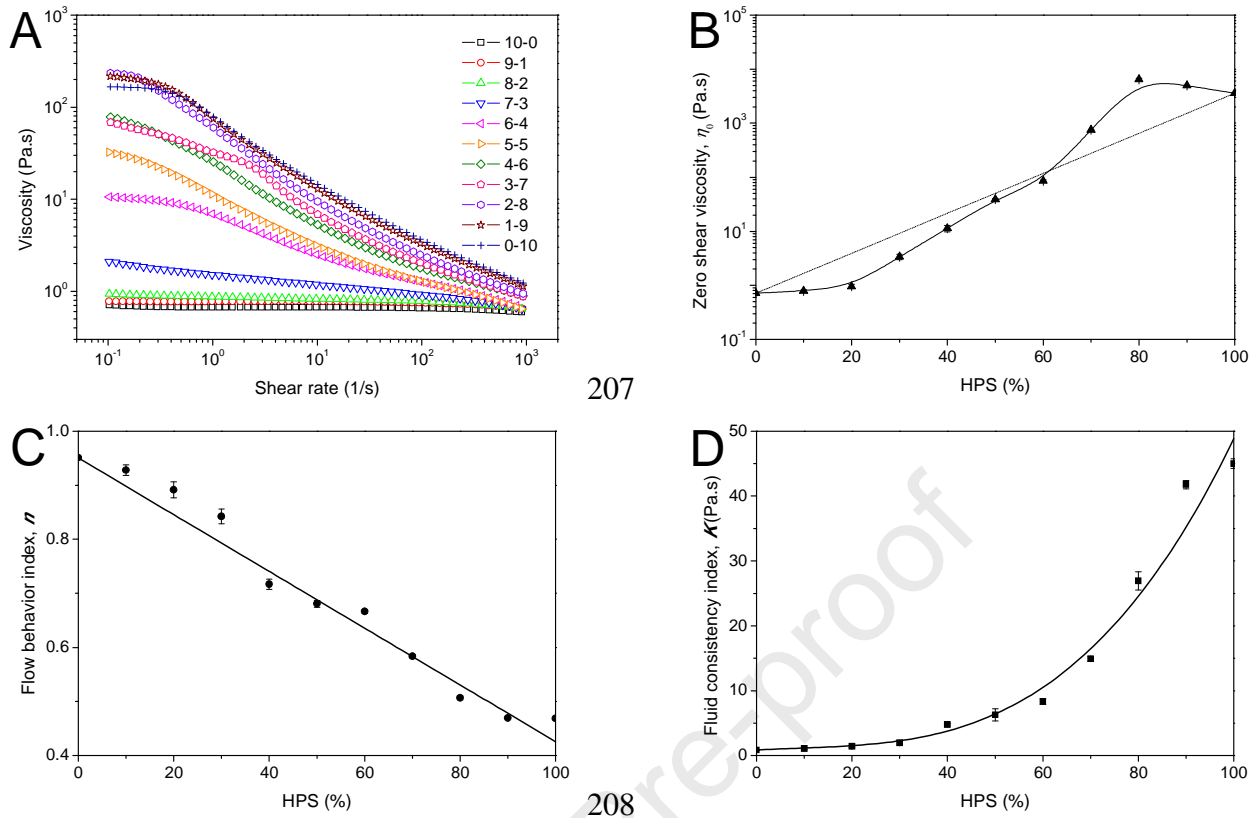
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195 For low-concentration samples, K was small. Higher concentration resulted in higher K , which
196 can be linked to higher viscosity, as expected.

197 3.3 Effect of HPMC/HPS ratio on HPMC/HPS paste viscosity

198 **Fig. 3(A)** shows the effect of HPMC/HPS ratio on the viscosity of HPMC/HPS pastes. At a low
199 HPS ratio (< 20%), the viscosity was not significantly influenced by shear rate, which could be
200 ascribed to dispersed biopolymer chains. In contrast, the samples with a high HPS ratio showed
201 significantly lower viscosity with increasing shear rate, a typical shear thinning behavior. At a certain
202 shear rate, a higher HPS ratio led to higher viscosity. This corresponds to the fact that HPS is a gel
203 with high viscosity at a low temperature (25 °C).

204



205

207

206

208

209 **Fig. 3** A) Viscosity vs. shear rate curves for HPMC/HPS pastes with different HPS ratio at 25 °C; B)
 210 Zero-shear viscosity η_0 , with the solid line indicating measured values and the dashed line predicted
 211 values; C) Flow behavior index n ; and D) flow consistency index K for HPMC/HPS pastes with
 212 different HPS ratio. The total concentration of HPMC/HPS was 15 wt%.

213

214 **Table 2** lists the n and K values for HPS/HPMC pastes with different mixing ratio. With
 215 increasing HPS ratio, n reduced gradually, while K showed a rising trend, implying that the addition
 216 of HPS made the HPMC paste more viscous and difficult to flow. This result is consistent with a
 217 previous study (Zhang, et al., 2015).

218

219 **Table 2** Flow behavior index (n) and fluid consistency index (K) of HPS/HPMC solutions with
 220 different HPS/HPMC ratio at 25 °C. The total biopolymer concentration was fixed at 15 wt%.

HPMC/HPS	n	K (Pa·s ^{n})	R^2
10:0	0.9511±0.0023	0.84±0.01	0.9999
9:1	0.9280±0.0096	1.09±0.10	0.9998
8:2	0.8915±0.0146	1.41±0.16	0.9994
7:3	0.8423±0.0135	1.94±0.31	0.9998
6:4	0.7170±0.0094	4.76±0.20	0.9996
5:5	0.6807±0.0063	6.27±0.94	0.9993
4:6	0.6666±0.0032	8.33±0.41	0.9969
3:7	0.5835±0.0028	14.91±0.40	0.9942
2:8	0.5068±0.0037	26.93±1.39	0.9869
1:9	0.4694±0.0008	41.76±0.64	0.9897
0:10	0.4687±0.0019	45.01±0.72	0.9935

221

222 For a homogeneous system, the relationship among the rheological properties of the blend and its
 223 individual components follow a logarithmic sum rule (Utracki, 1983). For a binary system, this rule
 224 can be expressed as:

$$225 \quad \log F = \phi_1 \log F_1 + \phi_2 \log F_2 \quad (3)$$

226 where F , F_1 , and F_2 are the rheological parameter of the mixture, component 1, and component 2,
 227 respectively; ϕ_1 and ϕ_2 are the mass fractions of component 1 and component 2, respectively,
 228 with $\phi_1 + \phi_2 = 1$.

229 The measured and predicted curves of η_0 as a function of HPS ratio are shown in **Fig. 3(B)**. The
 230 zero-shear viscosity increased with HPS ratio and their relationship generally follows the log-

231 additivity rule, implying good compatibility of this system. Nonetheless, the measured values deviate
232 from the mixing rule either positively or negatively, depending on HPS ratio. This suggests the
233 mixed system had a continuous-discrete type of phase structure and the change of continuous phase
234 occurred (Yao, Mukuze, Zhang, & Wang, 2013) at an HPS ratio of 60%. Regarding the negative
235 deviation at a low HPS ratio, HPMC chain existed as a continuous phase in which HPS microgel was
236 scattered. Regarding positive deviation at a high HPS ratio, HPMC became a separated phase
237 scattered in the HPS continuous phase. These results are confirmed by microscopy observation with
238 a previous study (Y. F. Wang, Zhang, et al., 2016).

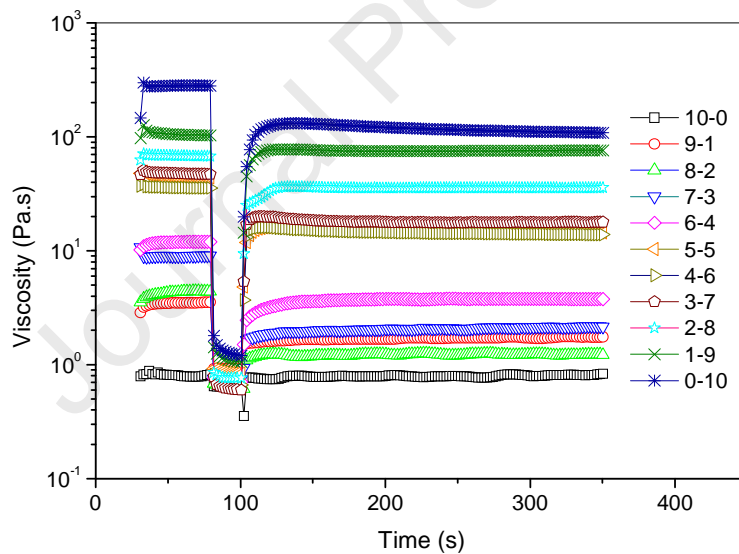
239 **Fig. 3(C)** shows that n decreased progressively with increasing HPS ratio and the relationship
240 between n and HPS ratio follows the linear-additivity rule. This suggests that addition of HPS to
241 HPMC imparts stronger pseudoplastic (shear-thinning) behavior. The linear regression analysis was
242 achieved with $R^2 = 0.98062$, denoting good compatibility between the two biopolymers.

243 **Fig. 3(D)** shows that increasing HPS ratio resulted in higher K , related to the gelation behavior of
244 HPS at a low temperature. For HPMC/HPS pastes with an extreme blend ratio (HPS ratio < 20 wt%
245 or > 70 wt%), the K value for a blend paste is closer to that for the biopolymer with a high ratio in
246 that mixture. In this regard, the viscosity of a mixture paste is mainly determined by the continuous
247 phase. On the other hand, for HPMC/HPS pastes with an intermediate ratio (20 wt% $<$ HPS ratio $<$
248 70 wt%), although HPMC with low viscosity still existed as a continuous phase, K rose rapidly with
249 increasing HPS ratio, indicating that HPS as the separated phase made a major contribution to the
250 viscosity of the blends. This implies that the continuous phase and the separated phase make
251 different contributions to the viscosity of a blend depending on the ratio of the two components.

252 3.4 Thixotropic behavior of HPMC/HPS pastes

253 Thixotropy describes the structural stability of a material against shear applied (Krystyjan, et al.,
 254 2016; Shakeel, Kirichek, & Chassagne, 2020; Marek Sikora, Adamczyk, & Krystyjan, 2011).
 255 Thixotropy can be linked to time and the history of shearing that results in microstructural changes
 256 (Czaikoski, da Cunha, & Menegalli, 2020; Mewis & Wagner, 2009; M. Sikora, et al., 2015). **Fig. 4**
 257 shows the results of the three-interval thixotropic behavior of HPMC/HPS pastes with different
 258 mixing ratio. All the samples were thixotropic. The viscosity at a low shear rate (1 s^{-1} , in the first and
 259 third stages) increased significantly with a higher HPS ratio.

260



261

262 **Fig. 4** Three-interval thixotropic curves for HPMC/HPS pastes with different HPMC/HPS ratio at 25
 263 °C. The total biopolymer concentration was 15 wt%.

264

265 The structural recovery ratio (DSR) can be defined by the equation:

$$266 \text{ DSR} = \frac{\eta_t}{\eta} \times 100\% \quad (4)$$

267 where η_t is the viscosity in the structural recovery stage (the third stage) at a certain time (t) and η is
 268 the final viscosity in the first stage (Mewis & Wagner, 2011; Toker, Karasu, Yilmaz, & Karaman,
 269 2015).

270 With $DSR < 100\%$, it can be assumed that the recovered paste was less resistant to shear and the
 271 material is thixotropic. In contrast, $DSR > 100\%$ indicates that the sample is anti-thixotropic. In a
 272 word, for thixotropic material, a higher DSR value means weaker thixotropic behavior (higher
 273 shear-resistance) and higher rheological stability.

274 The DSR data from three-interval thixotropic tests were listed in **Table 3**. The pure-HPMC
 275 solution showed a very high DSR value, close to 100%. In this regard, HPMC chains are rigid with a
 276 short relaxation time, which means the structure can recover quickly. In contrast, the pure-HPS
 277 solution presented a low DSR value. This indicates that the structural recovery of HPS is slow and
 278 can be explained by HPS chains being flexible and their long relaxation time.

279

280 **Table 3** Degree of structure recovery (DSR) at certain recovery time for HPMC/HPS solutions with
 281 different HPMC/HPS ratio at 25 °C. The total biopolymer content was 15 wt%.

HPMC/HPS ratio	DSR (%)		
	10 s	60 s	250 s
10:0	91.29±1.70 ^a	93.57±0.65	98.98±0.37
9:1	63.26±2.12	66.67±2.18	71.66±1.66
8:2	39.32±0.95	42.94±0.95	45.78±1.30
7:3	20.43±0.62	22.87±0.75	24.76±0.77
6:4	24.68±0.43	30.81±0.27	31.83±0.53

5:5	37.00±1.44	36.97±1.03	34.03±0.91
4:6	44.19±0.90	41.75±0.78	38.98±0.81
3:7	59.98±1.90	53.23±1.84	50.36±1.67
2:8	57.58±0.97	58.86±0.98	59.40±0.59
1:9	67.60±0.16	72.78±0.76	72.74±1.01
0:10	38.29±0.34	45.31±0.45	38.65±0.19

282 ^a Mean ± standard deviation

283

284 While the DSR values for mixture pastes were lower than that for the pure-HPMC sample but
 285 higher than that for the pure-HPS sample, the change in DSR did not follow a consistent trend. For
 286 mixtures with a low HPS ratio (< 30 wt%), DSR decreased with increasing HPS ratio, indicating
 287 enhanced thixotropic behavior. In this regard, flexible HPS chains in the system counteracted the
 288 effect of rigid HPMC chains to some extent, thus decreasing the capability of the structure to recover
 289 rapidly from shear-induced deformation and prolonging the relaxation time. However, further
 290 increasing HPS content (> 30 wt%) led to an increase in DSR, suggesting weakened thixotropic
 291 behavior. In this regard, the interaction between HPMC and HPS chains might result in improvement
 292 in overall chain rigidity and thus a reduction in relaxation time.

293 The DSR values with different recover time are also listed in **Table 3**. HPMC/HPS pastes almost
 294 finished the structural recovery within 10 s as the DSR were very close to the final DSR (at 250 s).
 295 For some samples, the DSR values at 60 s were even high than the final DSR. Given this, these
 296 samples were more unstable as their structure could be destroyed even at very low shear rate.

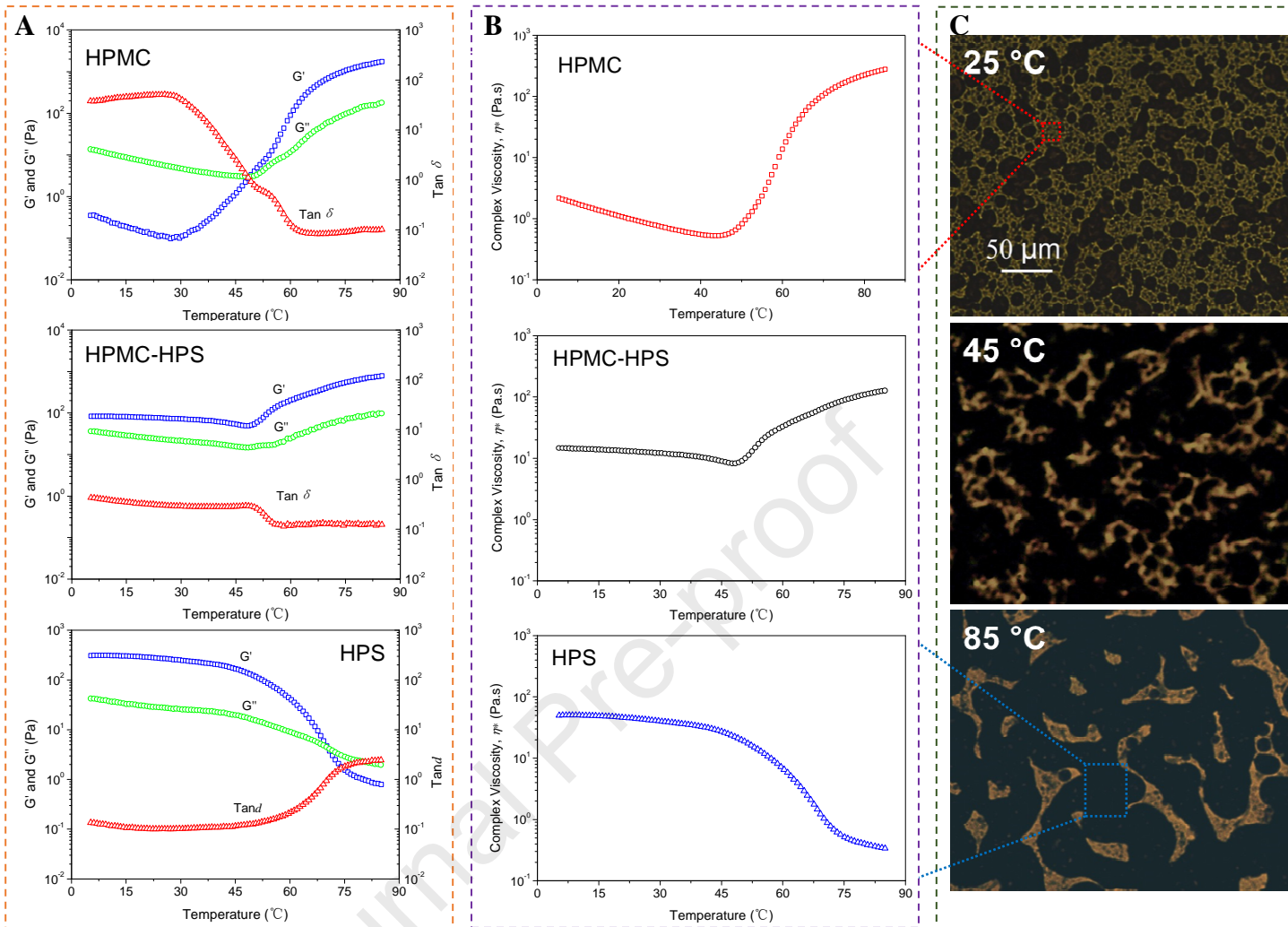
297 **3.5 Effect of temperature on the dynamic rheological properties and phase structure of**
298 **HPMC/HPS pastes**

299 As a wide range of temperature could be applied during the processing and storage of
300 biopolymers, it is important to understand the effect of temperature on rheological properties (Park,
301 Chung, & Yoo, 2004; Rao, 2014). Both HPMC and HPS are temperature-sensitive hydrogels and
302 their opposite gelling behavior make it difficult to achieve a blend with high miscibility, despite
303 these polysaccharides are chemically akin. Nevertheless, at a suitable mixing ratio and under a
304 certain temperature, HPMC and HPS could interact with each other to the maximum extent.

305 **3.5.1 Gelation behavior of HPMC/HPS pastes studied by dynamic viscoelasticity**

306 The viscoelastic properties of HPMC/HPS pastes with different mixing ratio are shown in **Fig. 5**
307 **(A)**. The pure-HPMC paste showed liquid-like behavior at a low temperature as G' was below G'' ,
308 while it congealed at a high temperature with G' surpassing G'' . For the pure-HPS sample, the three-
309 dimensional gel network at a low temperature solated at a high temperature, inferred from $G' < G''$.
310 The cross point of G' and G'' was at about 49 °C for the pure-HPMC sample and 70 °C for the
311 pure-HPS sample, confirming HPMC being a thermal gel and HPS being a cooling-gel.

312



313

314 **Fig. 5** A) Storage modulus (G'), loss modulus (G'') and loss tangent ($\tan \delta$) vs. temperature curves for
 315 the pure-HPMC paste, the 5:5 (w/w) HPMC/HPS paste, and the HPS paste, respectively, all having a
 316 total biopolymer concentration of 15 wt%; B) Complex viscosity vs. temperature curves for the
 317 HPMC paste, the 5:5 (w/w) HPMC/HPS paste, and the HPS paste, respectively, all having a total
 318 biopolymer concentration of 15 wt%; C) Light-microscopic images of the dyed 5:5 (w/w)
 319 HPMC/HPS paste of 3 wt% total biopolymer concentration at 25 $^{\circ}\text{C}$, 45 $^{\circ}\text{C}$, and 85 $^{\circ}\text{C}$, respectively.

320

321 For the 5:5 (w/w) HPMC/HPS paste, the G' and G'' curves were roughly parallel to those for the
 322 pure-HPS paste at a low temperature and to those for the pure-HPMC paste at a high temperature.

323 Given this, HPS had a major influence on the viscoelastic properties of the mixture at a low
324 temperature because HPS mainly contributed to the gelation at a low temperature, whereas HPMC
325 dominated the mixture behavior at a high temperature when HPMC was responsible for gelation. The
326 blend had intermediate moduli between those for individual HPS and HPMC. Besides, G' was
327 always higher than G'' during the whole temperature range, indicating solid-like behavior contributed
328 by biopolymer chain interactions. Furthermore, the 5:5 (w/w) HPMC/HPS paste showed a $\tan \delta$ peak
329 at about 45 °C, at which point a change of the continuous phase occurred.

330 **3.5.2 Effect of temperature on the complex viscosity of HPMC/HPS pastes**

331 For mixed systems, the viscosity of individual components is important. Normally, when two
332 components with largely different viscosity were mixed, the component with a higher viscosity tends
333 to form a scattered phase in the continuous phase of the lower-viscosity component.

334 **Fig. 5(B)** shows the effect of temperature on the complex viscosity (η^*) in the range of 5–85 °C
335 of HPMC/HPS pastes. With increasing temperature, the η^* of the pure-HPS sample showed a slight
336 decrease followed by a sharp decrease. However, the η^* of the pure-HPMC sample first experienced
337 a slight decline and then a strong rise starting at 45 °C. For the 5:5 (w/w) HPMC/HPS paste, η^* first
338 decreased slightly and then increased moderately, a changing pattern close to that for HPS at a low
339 temperature but similar to that for HPMC at a high temperature. This result should be ascribed to the
340 different gelation behavior of HPS (cooling gel) and HPMC (thermal gel). The rapid change in η^* of
341 the 5:5 (w/w) mixture at about 45 °C might be due to the change in the phase distribution of
342 HPMC/HPS.

343 The temperature dependence of η^* for HPMC/HPS pastes at a certain temperature can be
344 evaluated using an Arrhenius-type equation:

$$\eta^* = \eta_i \exp\left(\alpha \frac{E}{RT}\right) \quad (5)$$

where η^* is complex viscosity, η_i is a constant describing the viscosity coefficient at a reference temperature (Pa·s) (Laity & Holland, 2017; Qing, Jinsong, Changjiang, Jianpeng, & Shouqin, 2014a), T is the absolute temperature (K), R is the gas constant ($8.3144 \text{ J}\cdot\text{mol}^{-1}\cdot\text{K}^{-1}$), α is the correction coefficient (± 1), and E is the activation energy ($\text{J}\cdot\text{mol}^{-1}$).

For fitting using **Eq.(5)**, the curves need to be divided into two sections before and after $45 \text{ }^\circ\text{C}$ according to viscosity curves shown in **Fig. 5(B)**. **Table 4** presents the values of E , α , and η_i calculated based on **Eq.(5)** for the temperature ranges of $10\text{--}45 \text{ }^\circ\text{C}$ and $45\text{--}85 \text{ }^\circ\text{C}$ ($R^2 > 0.90$). It can be seen that the η_i value for the pure-HPMC sample was very small ($1.31 \times 10^{-5} \text{ Pa}\cdot\text{s}$) at a low temperature but high ($1.99 \times 10^{28} \text{ Pa}\cdot\text{s}$) at a high temperature. In contrast, for the pure-HPS sample, the η_i value at a low temperature ($0.56 \text{ Pa}\cdot\text{s}$) was much higher than that at a high temperature ($1.78 \times 10^{-19} \text{ Pa}\cdot\text{s}$). This difference in η_i between the two biopolymers could be ascribed to their different gelation behavior, namely, HPS is a cooling-gel and HPMC is a thermal-gel. For the 5:5 (w/w) blend, the η_i value was similar to that for the pure-HPS paste and much higher than that for the pure-HPMC at a low temperature, and between that for the pure-HPS sample and that for the pure-HPMC sample at a high temperature. This implies that HPS played a dominant role in the blend at a low temperature, while HPMC had a much stronger effect at a high temperature.

Table 4 Arrhenius equation parameters (correction coefficient, α ; activation energy, E ; constant, η_i ; and determination coefficient, R^2) for the HPS paste, the 5:5 (w/w) HPS/HPMC paste, and the HPMC paste. The total biopolymer content is 15 wt%.

Sample	5–45 °C	45–85 °C
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	η_i (Pa·s)	α	E (kJ·mol ⁻¹)	R^2	η_i (Pa·s)	α	E (kJ·mol ⁻¹)	R^2
HPMC	1.31×10^{-5}	+1	27.7	0.9917	1.99×10^{28}	-1	174	0.9441
HPMC-HPS	0.47	+1	8.09	0.9219	5.67×10^{12}	-1	72	0.9688
HPS	0.56	+1	10.7	0.9071	1.78×10^{-19}	+1	124	0.9744

366

367 The temperature affects biopolymer paste viscosity in different ways:

368 a) It is known that a higher temperature leads to greater chain mobility and lower viscosity.

369 Based on this effect (effect A), the viscosity is inversely proportional to temperature and α is
370 a negative value.

371 b) For a thermal gel like HPMC, increasing temperature is favorable for greater interaction
372 between hydrophobic groups and that between hydrophilic hydroxyl groups, thus enhancing
373 the three-dimensional network and increasing the viscosity. Based on this effect (effect B),
374 the viscosity is proportional to temperature and α is a positive value (Qing, Jinsong,
375 Changjiang, Jianpeng, & Shouqin, 2014b).

376 c) For a cooling gel like HPS, a higher temperature causes the breakage of intermolecular
377 hydrogen bonds and thus the three-dimensional network, leading to declined viscosity. Based
378 on this effect (effect C), the viscosity is inversely proportional to temperature and α is a
379 negative value.

380 In the low-temperature region (5–45 °C), only effect A existed for the pure-HPMC paste since it
381 was in a liquid-like state and therefore, E was high and $\alpha = +1$. For the pure-HPS paste, which was a
382 solid-like gel, there were both effects A and C, while effect A was greater than effect C; thus, $\alpha = +1$
383 and E was lower than that for the pure-HPMC sample. For the 5:5 (w/w) HPMC/HPS paste, both

384 effects A and C presented here, but effect C was weakened by HPMC due to its liquid-like state and
385 thus, $\alpha = +1$ and E was lower than that for the pure-HPMC sample. In a word, HPS played the
386 dominant role in controlling the phase structure and rheological behavior at a low temperature.

387 In the high-temperature region (45–85 °C), both effects A and B existed for HPMC since HPMC
388 underwent gelation at a high temperature, with effect A \ll effect B; thus, E was very high and $\alpha =$
389 -1 . For HPS, there was only effect A as HPS solates at a high temperature and therefore, E was very
390 high and $\alpha = +1$. For the 5:5 (w/w) mixture paste, there were both effects A and B but effect B was
391 lessened by HPS which was liquid-like; therefore, $\alpha = -1$ and E was lower than that for the pure-
392 HPMC sample. These results indicate that HPMC played the leading role in controlling the structure
393 and rheological behavior of the blend at a high temperature.

394 3.5.3 *Effect of temperature on the phase structure of HPMC/HPS pastes*

395 **Fig. 5(C)** shows the morphologies of the 5:5 (w/w) HPMC/HPS blends at 25 °C, 45 °C, and
396 85 °C observed using an optical microscope. Two phases could be identified, the HPMC phase in
397 light and the HPS phase in dark. Under light microscopy, HPS becomes dark after being dyed with
398 iodine (Y. F. Wang, Zhang, et al., 2016). Increasing temperature resulted in an increased dark area
399 (HPS phase) but a reduced light area (HPMC phase). At 25 °C, HPMC (in light color) was shown to
400 be a continuous phase, with the scattering of small spherical HPS domains (dark). In contrast, at
401 85 °C, the HPMC phase became quite small and scattered in the HPS continuous phase.

402 There should be a certain temperature at which the viscosity of HPMC and HPS became similar,
403 thus leading to a change in the phase distribution (continuous or discrete) of the two biopolymers.
404 We observed this transition at 45 °C (**Fig. 5C**) when the typical “sea-island” morphology in the
405 blend was not shown but a pattern with two continuous phases was observable. The observation

406 agrees with the transition indicated by the $\tan \delta$ peak and the rapid change in viscosity for the 5:5
407 (w/w) mixture at 45 °C.

408 **3.6 Temperature-induced structural changes of HPMC/HPS solutions**

409 Based on the comparison of HPMC/HPS blends discussed above in the context of the classic
410 rheological behavior of polymer solution and hybrid gels (Ford, 1999; Rachmawati, Woortman, &
411 Loos, 2013; Zhang, et al., 2015), we propose a schematic representation of the temperature-induced
412 conformational change of HPMC/HPS pastes, as shown in **Fig. 6**.

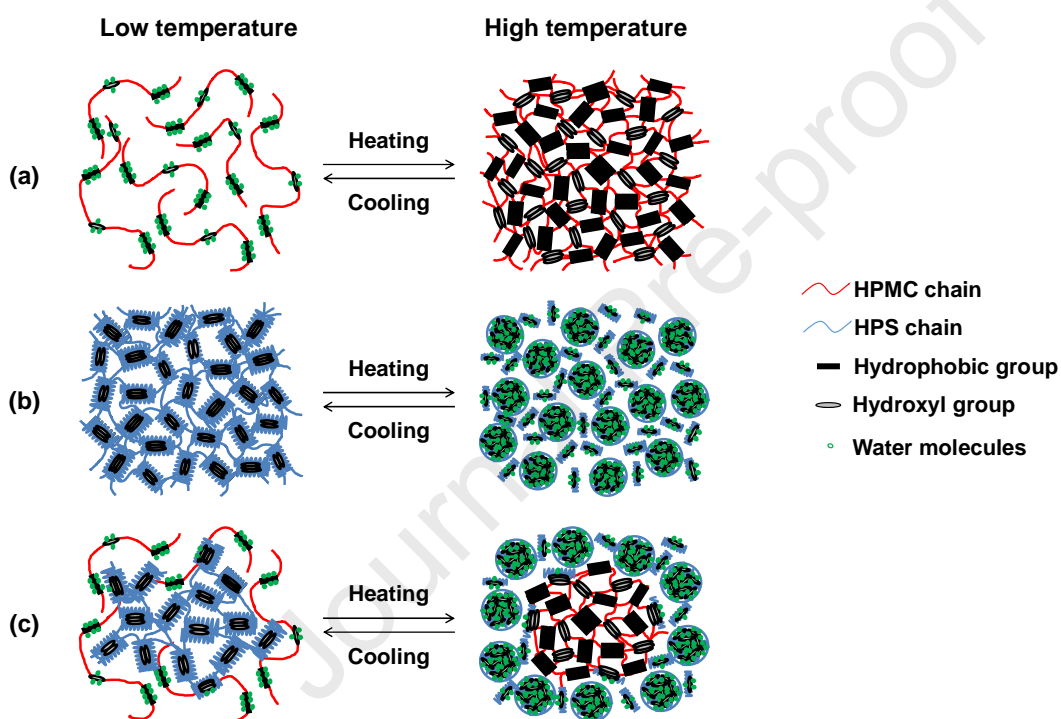
413 The gelation behavior of HPMC has been reported and the related mechanism has been discussed
414 (Haque & Morris, 1993; Haque, Richardson, Morris, Gidley, & Caswell, 1993; S. Q. Liu, Joshi, Lam,
415 & Tam, 2008; Viriden, Larsson, Schagerlof, & Wittgren, 2010; Y. F. Wang, et al., 2018).

416 Specifically, it is recognized that HPMC chains exist in solution as aggregated bundles. These
417 bundles are held together by the packing of the un-substituted or the sparingly soluble regions of the
418 cellulosic structure and by the hydrophobic clustering of methyl groups and hydroxyl groups in
419 regions with denser substitution. These packings and clusters are the so-called water cages and shells,
420 preventing the formation of inter-chain hydrogen bonding at a low temperature. The absorption of
421 heat can break the water cages and shells, which is kinetic of the sol-gel transition. The breakage of
422 the water cages and shells exposes methyl and hydroxyl groups to the surrounding water and causes
423 a significant increase in volume. At a higher temperature, due to both the interaction among
424 hydrophobic groups and that among hydroxyl groups, a cross-linked network is formed (**Fig. 6a**).

425 Amylose, exuded from starch granules after gelatinization, tended to coil to form hollow, left-
426 handed single helices coaxially twisting along the chains. These helices feature a hydrophobic cavity
427 inside and a hydrophilic surface outside. This compact structure of starch affords higher stability

428 (Lopez, de Vries, & Marrink, 2012; Rachmawati, et al., 2013; Zhou, et al., 2016). Therefore, HPS
 429 behaves as flexible random coils with stretches of helical segments in an aqueous solution at a high
 430 temperature. With reducing temperature, the hydrogen bonds between starch chains and water were
 431 broken, releasing the structured water, and inter-chain hydrogen bonding is enhanced, leading a
 432 three-dimensional gel network (**Fig. 6b**).

433



434

435 **Fig.6** Schematic representation of the sol-gel transition of HPMC (a), HPS (b), and HPMC/HPS (c)
 436 pastes.

437

438 For the mixture pastes, at a low temperature, HPMC has a lower viscosity than HPS and thus
 439 HPMC forms a continuous phase encompassing discrete domains of higher-viscosity HPS gel. At the
 440 edge of the two phases, the hydroxyl groups of HPMC chains can lose the structured water and form
 441 hydrogen bonding with HPS chains. Upon heating, HPS may receive enough energy to form

442 hydrogen bonding with water, resulting in the gradual disintegration of the gel network. Meanwhile,
443 the shells and water cages of HPMC chains are disrupted and even broken to expose hydroxyl groups
444 and hydrophobic clusters. At a high temperature, HPMC forms a gel network due to the inter-chain
445 hydrogen bonding and hydrophobic interaction and becomes a high-viscosity phase scattered in the
446 continuous phase of HPS coils (**Fig. 6c**). Therefore, HPS at a low temperature, or HPMC at a high
447 temperature, plays a dominant role in viscoelastic properties, gelation behavior, and phase structure
448 for HPMC/HPS pastes.

449 **4 Conclusion**

450 This work reveals how the phase structure of HPMC/HPS pastes was influenced by the gelation
451 behavior and rheological properties of individual biopolymers. And, we have established new links
452 between rheological parameters and phase structure for such systems.

453 The HPMC/HPS mixture showed a typical “sea-island” phase structure. The variation in this
454 phase conformation was significantly influenced by the viscosity of individual biopolymer, blending
455 ratio, and temperature. With increasing HPS ratio, the continuous phase of the blend changed from
456 HPMC to HPS at an HPS ratio of 60%. We found that this phase structure change can be well
457 correlated to the positive or negative deviation of η_0 from the log-additivity rule.

458 At a low temperature, HPMC, with low viscosity, was the continuous phase, and so was HPS at a
459 high temperature. Moreover, HPS at a low temperature, or HPMC at a high temperature, plays the
460 dominant role in controlling the viscoelastic properties and gelation behavior. With increasing
461 temperature, the continuous phase changed from HPS to HPMC at a critical point of 45 °C. We
462 introduced a modified Arrhenius-type equation with correction coefficient α (± 1) to explore the
463 effect of temperature on the continuous-phase change. This phase structure change can be well

464 correlated to rheological indicators such as the presence of a $\tan \delta$ peak, a sudden change in η^* , and
465 the positive-negative change in α .

466 The results from this work led a schematic model to describe the temperature-induced
467 conformational change of HPMC/HPS pastes, which may provide an insight into the understanding
468 of the gelling mechanism for other temperature-sensitive multi-phasic systems.

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475 **Conflicts of interest**

476 There are no conflicts of interest to declare.

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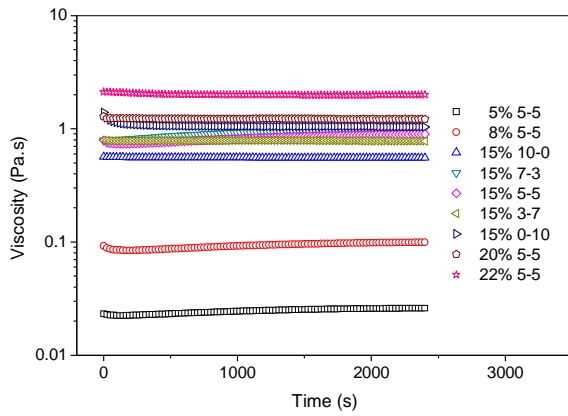


Fig. 1 Viscosity as a function of time for HPMC/HPS pastes. The shear rate was fixed at 800 s^{-1} .

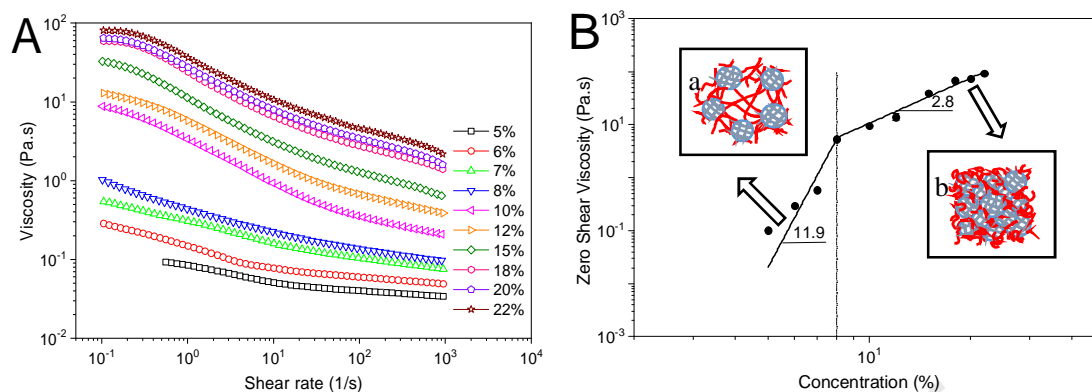


Fig. 2 A) Flow curves for 50:50 (w/w) HPMC/HPS pastes of different total biopolymer concentration at 25 °C; B) Zero-shear viscosity as a function of total biopolymer concentration, with the molecular conformation of HPMC/HPS schematically shown (the HPMC/HPS ratio was 50:50 (w/w), red lines represent HPMC chains and grey lines HPS).

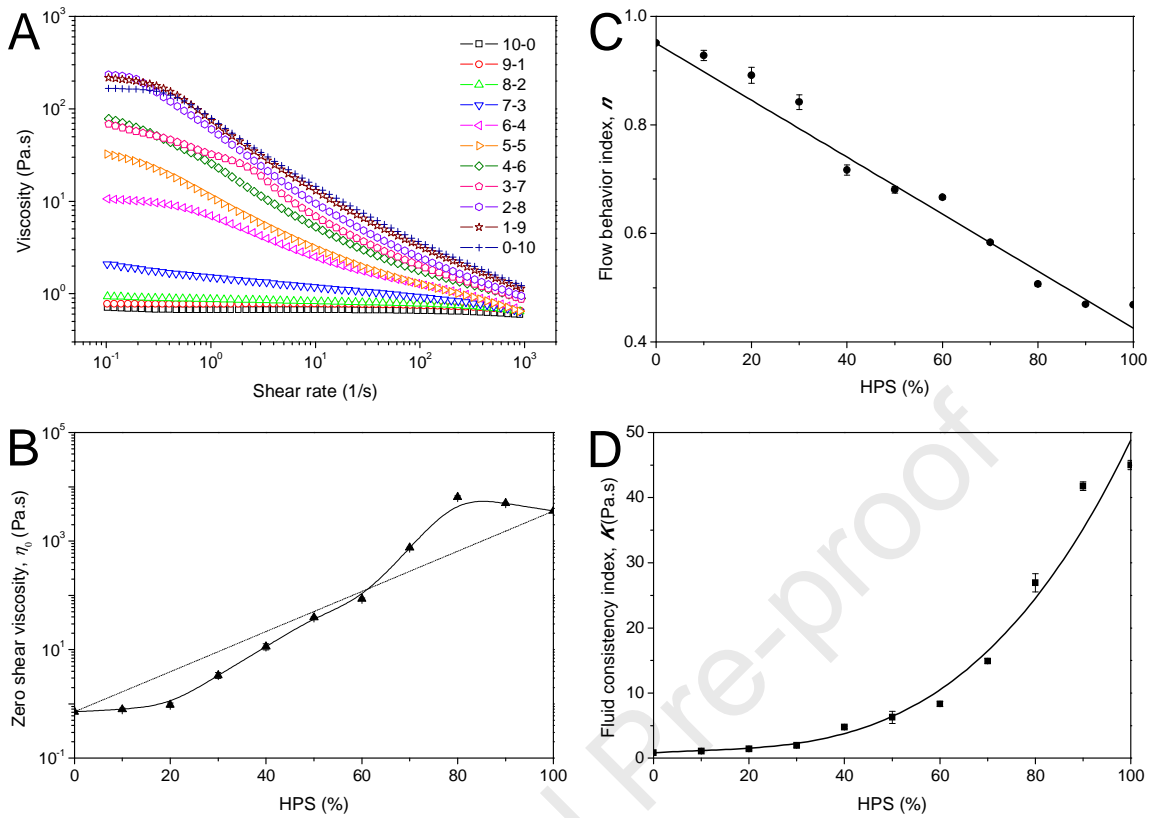


Fig.3 A) Viscosity vs. shear rate curves for HPMC/HPS pastes with different HPS ratio at 25 °C; B) Zero-shear viscosity η_0 , with the solid line indicating measured values and the dashed line predicted values; C) Flow behavior index n ; and D) flow consistency index K for HPMC/HPS pastes with different HPS ratio. The total concentration of HPMC/HPS was 15 wt%.

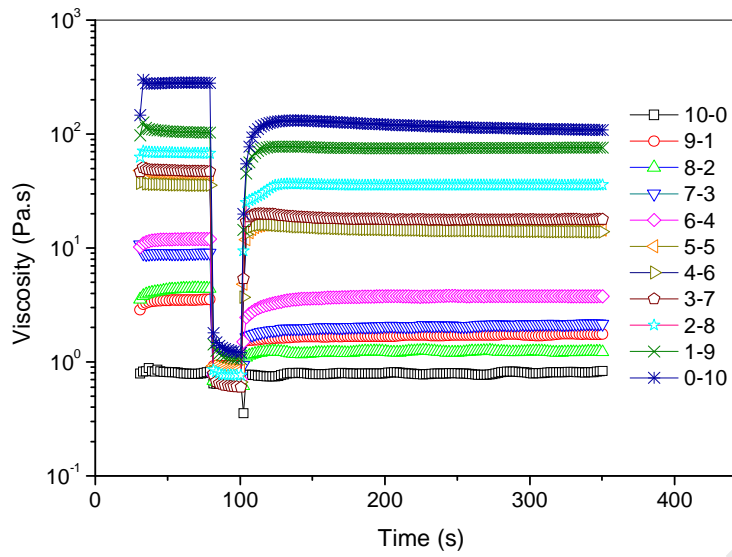


Fig. 4 Three-interval thixotropic curves for HPMC/HPS pastes with different HPMC/HPS ratio at 25 °C. The total biopolymer concentration was 15 wt%.

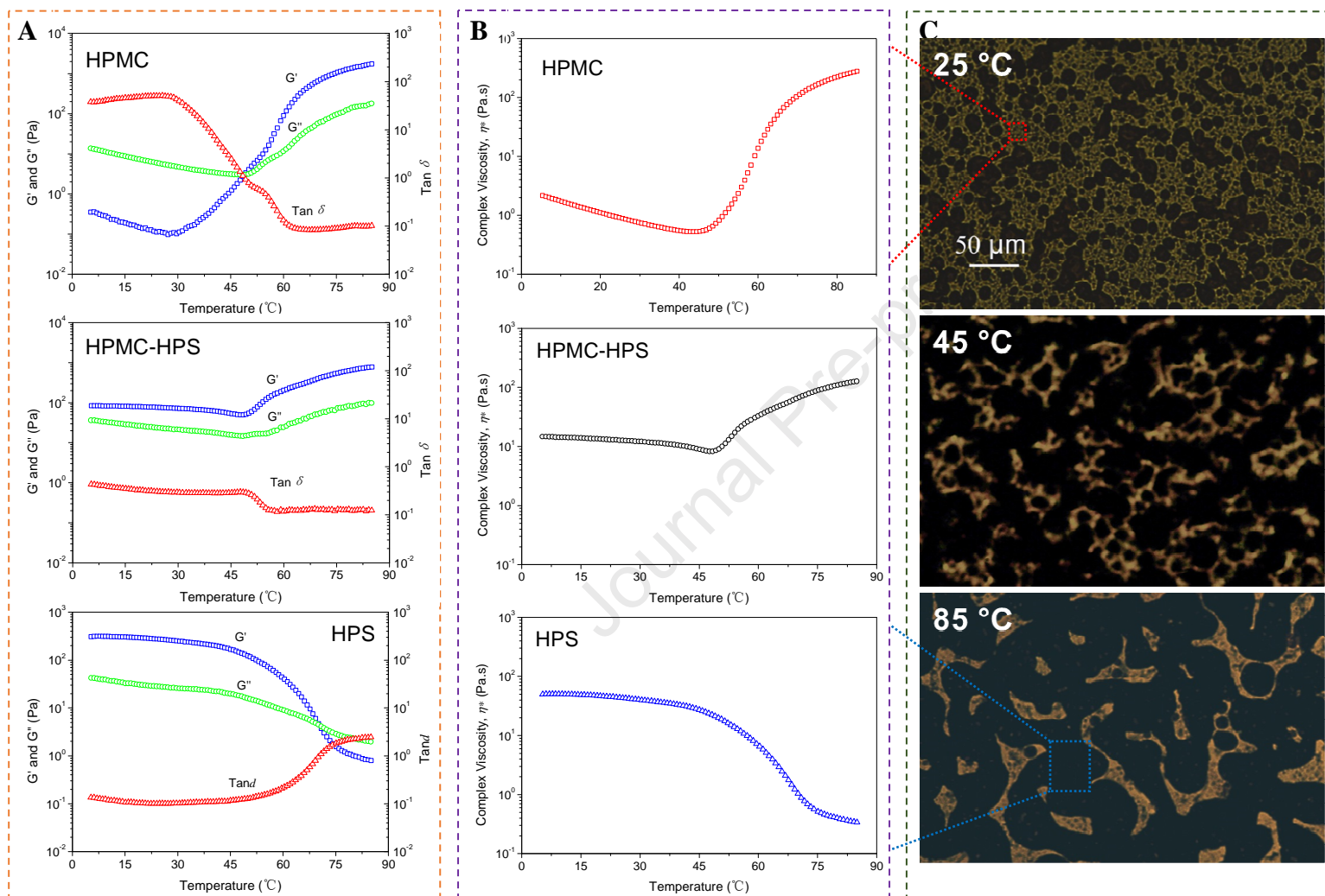


Fig.5. A) Storage modulus (G'), loss modulus (G'') and loss tangent ($\tan \delta$) vs. temperature curves for the pure-HPMC paste, the 5:5 (w/w) HPMC/HPS paste, and the HPS paste, respectively, all having a total biopolymer concentration of 15 wt%; B) Complex viscosity vs. temperature curves for the HPMC paste, the 5:5 (w/w) HPMC/HPS paste, and the HPS paste, respectively, all having a total biopolymer concentration of 15 wt%; C) Light-microscopic images of the dyed 5:5 (w/w) HPMC/HPS paste of 3 wt% total biopolymer concentration at 25 °C, 45 °C, and 85 °C, respectively.

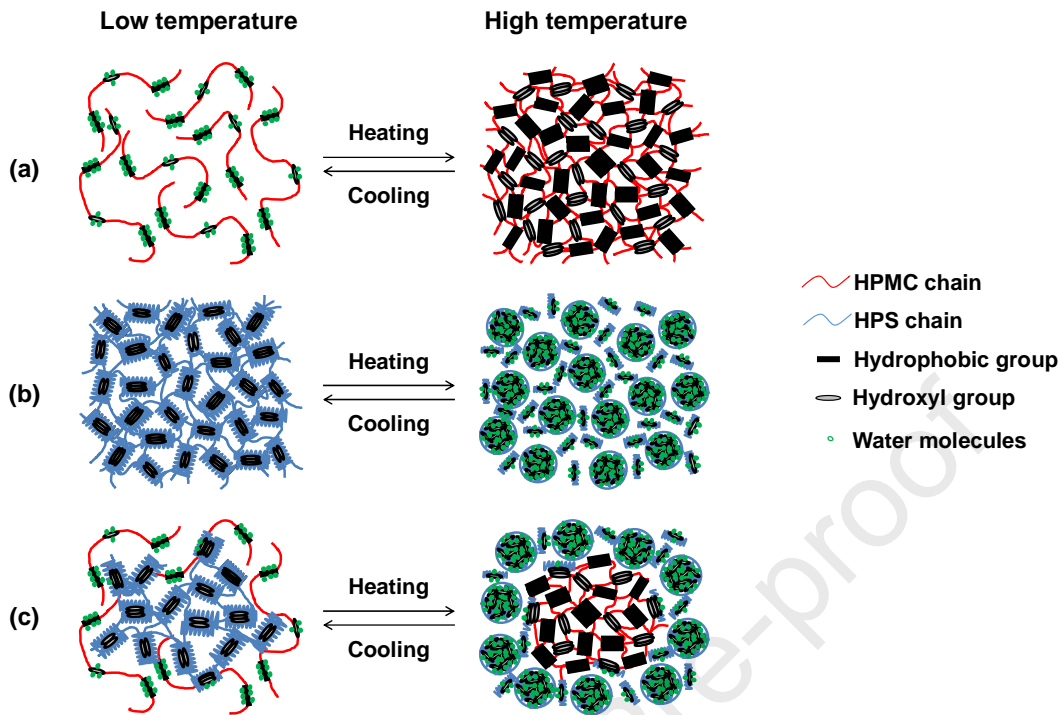


Fig. 6 Schematic representation of the sol-gel transition of HPMC (a), HPS (b), and HPMC/HPS (c) pastes.

Highlights:

- ✓ Hydroxypropyl methylcellulose (HPMC) and hydroxypropyl starch (HPS) mixture studied
- ✓ Strong rheological and gelation effects on the phase structure of HPMC/HPS shown
- ✓ HPMC/HPS blend ratio and temperature controls continuous/discrete phase change
- ✓ Phase structure correlated to zero-shear viscosity and Arrhenius coefficient α
- ✓ A schematic model to describe the temperature-induced conformational change

– Declaration of Interest –

Hydroxypropyl methylcellulose and hydroxypropyl starch:
Rheological and gelation effects on the phase structure of their
mixed hydrocolloid system

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The authors declare that there is no conflict of interest regarding the publication of this article.