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1 ***In vitro* conditions for performance evaluation of products for intravascular**
2 **administration: Developing appropriate test media using Amphotericin B as a model**
3 **drug**

4

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22

23 **Abstract**

24 Currently, there are no compendial *in vitro* release tests specifically indicated for parenteral
25 formulations. Consideration of biorelevant and clinically relevant test media represents a
26 valuable approach for the development of *in vitro* tests that ideally can provide information on
27 the formulation performance *in vivo*. The aim of this study was to investigate the effect of
28 different media components on the solubility of Amphotericin B (a poorly soluble highly
29 protein-bound drug) in order to develop biorelevant and clinically relevant media for future *in*
30 *vitro* release testing from its liposomal formulation. Three categories of media were considered
31 in the development approach: Category 1 media: effect of albumin concentration; category 2
32 media: effect of biorelevant concentrations of plasma components (bile salts, phospholipids,
33 cholesterol, albumin); category 3 media: attaining clinically relevant solubility with biorelevant
34 and synthetic surfactants with and without albumin and setting the basis for the development
35 of a simulated hypoalbuminaemic plasma medium. All the surfactants tested increased
36 Amphotericin B solubility while the simultaneous presence of albumin had a negative effect
37 on solubility. Clinically relevant media with the use of biorelevant or synthetic surfactants and
38 albumin were developed. One medium in which the solubility of Amphotericin B was reduced
39 was identified as potential candidate medium to simulate hypoalbuminaemic plasma. The
40 development of biorelevant and clinically relevant media and understanding the effect of media
41 components and their interactions, supports future development of meaningful *in vivo*
42 predictive release tests for parenteral formulations.

43

44 **Keywords:**

45 Amphotericin B; dissolution; solubility; clinically relevant; biorelevant; degradation

46

47 **1. Introduction.**

48 Recently, the development of parenteral formulations (for drugs of low aqueous solubility and
49 toxic drugs) has grown. Currently, there is no *in vitro* compendial method specifically assessing
50 how changes to a formulation might result in a change in *in vivo* performance of a parenteral
51 drug product (Allen, 2014; D'Souza and DeLuca, 2006; Seidlitz et al., 2011; Shen and Burgess,
52 2012, 2013). The *in vitro* dissolution/release testing used in quality control does not provide
53 information about the dissolution/release of the drug in the environment where the formulations
54 will be administered (such as the intravenous, intramuscular and subcutaneous routes (Allen,
55 2014)). Biorelevant dissolution testing refers to an attempt to mimic the conditions of the *in*
56 *vivo* environment in terms of the composition and physicochemical characteristics of the *in*
57 *vivo* fluids and the hydrodynamics at the site of administration (Wang et al., 2009). Recently,
58 clinically relevant dissolution testing has been defined; the term “clinically relevant” implies
59 the establishment of a link between a drug product quality attribute (e.g. solubility) and *in vivo*
60 performance (e.g. *in vivo* solubility) (Abend et al., 2018; Norris, 2016). This terminology has
61 been agreed in a workshop organised by US FDA and the International Consortium for
62 Innovation and Quality in Pharmaceutical Development (IQ) (Abend et al., 2018). A clinically
63 relevant approach to dissolution testing enables dissolution testing to establish safe boundaries
64 and reject drug product batches falling outside the established safe range (Abend et al., 2018).
65 Another aspect that is not usually covered in compendial *in vitro* release testing in terms of the
66 media composition is the variation in *in vivo* physiological conditions induced by illness. In
67 addition to simulating the fluid where the formulation will be administered, these physiological
68 changes should, when appropriate, be reflected in the test medium. From previous studies, our
69 group has developed a biorelevant test medium that simulates plasma (using Krebs Ringer
70 Buffer (KRB) (Cold Spring Harbor Protocols, 2014) for the ionic content and bovine serum
71 albumin (BSA) to represent the human serum albumin) which was used to evaluate the impact

72 of albumin concentration on the solubility and degradation of Amphotericin B (AmB) (Diaz de
73 Leon-Ortega et al., 2018). AmB, a highly protein-bound (including to albumin and lipoproteins
74 (Barwicz et al., 1998; Brajtburg et al., 1984; Ridente et al., 1999)) and poorly soluble drug
75 (Torrado et al., 2008), was selected as a model drug as it is commercially available as parenteral
76 lipid-based formulations (including Ambisome[®] and Abelcet[®]) for intravenous administration.
77 AmB formulations can be used in patients suffering from severe systemic fungal infections.
78 The presentation of sepsis in critically ill patients can include a reduced plasma albumin
79 concentration (hypoalbuminaemia), thus hypoalbuminaemia is a potential feature of the
80 vascular fluid into which AmB is administered *in vivo*. The aim of this study was to investigate
81 the impact of different media components on the solubility and degradation of AmB to develop
82 media able to target AmB plasma solubility (clinically relevant solubility) and to evaluate if
83 the composition of a medium is suitable for future compendial *in vitro* release testing. Media
84 were developed based on three categories (Figure 1). Category 1 media: biorelevant media,
85 investigating the impact of concentration of BSA. Category 2 media: Biorelevant media,
86 investigating the impact of biorelevant concentrations of plasma components to which AmB
87 binds *in vivo* [cholesterol, bile salts and phospholipids, with and without BSA]. Category 3
88 media: Clinically relevant media; category 3a media- attaining clinically relevant solubility
89 with physiological surfactants found in plasma (bile salts and phospholipids); Category 3b
90 media- attaining clinically relevant solubility with synthetic surfactants (SLS, CTAB or Tween
91 80); Category 3c media- potential for category 3b media to be used as a basis to develop media
92 for solubility and release studies simulating hypoalbuminaemic plasma. In advance of
93 performing clinically relevant release testing, the development of biorelevant and clinically
94 relevant test media (based on the active pharmaceutical ingredient (API)) is a primary step
95 towards the development of biorelevant and clinically relevant release testing of parenteral
96 formulations. Additionally, whereas API dissolution rates might not be considered directly

97 relevant to intravascular parenteral administration, API dissolution studies were performed in
98 the current work in order to identify any factors affecting the solubility behaviour of the drug
99 in the test media over time. This is an important step in the development of release testing of
100 parenteral formulations, as issues relating to API precipitation, for example, may be easier to
101 identify in a simpler API dissolution test in advance of formulation release testing.

102 **2. Materials and Methods**

103 **2.1. Materials**

104 AmB analytical standard (87.8%), methanol (MeOH) high performance liquid chromatography
105 (HPLC) grade, formic acid mass spectrometry grade, NaOH, MgCl₂, CaCl₂,
106 hexadecyltrimethylammonium bromide (CTAB), cholesterol (CH), NHCO₃ and NH₄HCO₂
107 were obtained from Sigma Aldrich (Germany); ethylenediaminetetracetic acid anhydrous
108 (EDTA) from Sigma Aldrich (USA); AmB API powder (85%) from Cayman Chemical (USA);
109 BSA protease free powder fraction V, dimethyl sulfoxide (DMSO), dextrose, sodium dodecyl
110 sulphate (SLS), Na₂HPO₄, NaH₂PO₄, KH₂PO₄, NaCl and KCl from Fisher Scientific (USA);
111 Tween 80 from Amresco (USA); phosphatidylcholine from egg from Lipoid GmbH
112 (Germany); sodium taurocholate from Prodotti Chimici e Alimentaria (Italy); GF/D (pore size
113 2.7 µm, 25 mm diameter) and GF/F (pore size 0.7 µm, 25 mm diameter) filters from Whatman
114 (UK) and regenerated cellulose (RC) filters 0.45 µm 13 mm diameter from Cronus (UK).

115 **2.1.1. Human plasma collection**

116 Blood was drawn from healthy volunteers (having given informed consent) by median cubital
117 vein venipuncture by a trained phlebotomist following local ethics committee approval
118 (EIRA1, Issue 3, 11/5/2010). To act as anticoagulant, 2 mL of an EDTA 50 mg/mL solution
119 were added to a final volume of 50 mL of blood, for a final concentration of 2 mg/mL. Plasma
120 was separated from blood cells by centrifugation for 10 min at 2000 x g (Heraeus Biofuge

121 Primo R Centrifuge, Thermo Electron LED GmbH. Osterode, Germany) and the supernatant
122 was separated into aliquots and kept at -80°C.

123 **2.2. Sample treatment of AmB in plasma and test media**

124 The sample treatment method was described previously (Diaz de Leon-Ortega et al., 2018).
125 Briefly, proteins were precipitated by adding 2 volumes of methanol to 1 volume of the sample
126 followed by mixing in a vortex mixer and centrifuged for 10 minutes at 12000 rpm at 5°C. The
127 supernatant was filtered through a 0.45 µm RC filter before injection to the HPLC.

128 **2.3. Chromatographic conditions for the analysis of AmB from plasma samples and test 129 media**

130 The chromatographic method to quantify AmB was described previously (Diaz de Leon-Ortega
131 et al., 2018). Briefly, AmB was quantified by HPLC with a C18 Waters Sunfire column
132 (Ireland) 150 x 46 mm 5 µm at 25°C. The mobile phase was formate buffer (50 mM; pH = 3.2):
133 MeOH (25:75, v/v); the flow rate was 1 mL/min and AmB was detected at $\lambda = 406$ nm. The
134 UV spectrum was recorded from 300 to 450 nm. Quantification of AmB in samples was based
135 on standard curves. Freshly prepared standard solutions (0.5 – 15 µg/mL) in the corresponding
136 medium were prepared by appropriate dilution of a 500 µg/mL stock solution of AmB
137 analytical standard in 1:1 MeOH: DMSO v/v. The limit of detection and the limit of
138 quantification were 0.12 and 0.37 µg/mL, respectively.

139 **2.4. Test media for evaluation of performance of parenteral drug products**

140 Media were developed following the scheme of the 3 categories of development (Figure 1).

141 **2.4.1. Category 1 media: investigating the impact of albumin concentration**

142 Category 1 media consisted of KRB with varying biorelevant albumin concentrations and were
143 developed and characterized as previously described (Diaz de Leon-Ortega et al., 2018). BSA
144 was used as a substitute for human serum albumin as it has been reported that there is only one
145 favourable binding site for AmB in both of them (Kudva et al., 2011).

146 **2.4.2. Category 2 media: investigating the effect of biorelevant concentrations of plasma**
147 **components on AmB solubility**

148 Plasma components with the potential to affect the solubility of AmB *in vivo*, were added to
149 KRB in biorelevant concentrations: bile salts 12.0 μM (mean value of the highest
150 concentrations reported in literature (Ambros-Rudolph et al., 2007; Egan et al., 2012;
151 Hospitals, 2014)); phospholipids 2.5 mM (Salvioli et al., 1985; Schaefer et al., 1958) and CH
152 4.5 mM (Abdelmagid et al., 2015). For media preparation, bile salts [sodium taurocholate was
153 used as source of bile salts (BS)] were weighed and dissolved in KRB and then phospholipids
154 [phosphatidylcholine from egg was used as source of phospholipids (PL)] from a stock solution
155 of 100 mg/mL (dissolved in dichloromethane) were added; afterwards, where relevant, CH
156 dissolved in chloroform (3.5 mg/mL) was added to the medium. Organic solvents were
157 evaporated with a rotary evaporator consisting of a Büchi Waterbath B-480 set at 40°C and a
158 Büchi Rotovapor R-114 (Büchi Labortechnik. Flawil, Switzerland) attached to a vacuum pump
159 unit PC 2001 Vario (Vacuubrand GMBH. Wertheim, Germany). The pressure was decreased
160 from 650 mbar in steps of 70 mbar every two minutes to 100 mbar, where the pressure was
161 maintained for 10 minutes. When included in the medium, BSA (2.0% and 4.0% w/v as
162 biorelevant concentrations) was added after the evaporation of the organic solvents. A medium
163 with a high concentration (8.0% w/v) BSA was also tested. The compositions of the media are
164 listed in Table 2 (Category 2 media). Osmolality, viscosity, pH and buffer capacity of these
165 media were measured (section 2.5) and AmB solubility studies (section 2.7) were also
166 performed in these media.

167 **2.4.3. Category 3 media: investigating the impact of biorelevant and synthetic surfactants**
168 **to achieve clinically relevant AmB solubility**

169 Media were developed to achieve clinically relevant solubility values of AmB by using
170 surfactants found in plasma (BS and PL) and synthetic surfactants (SLS, CTAB, Tween 80).

171 The effect of BSA was also evaluated (media with and without BSA 4.0% w/v). Media with
172 synthetic surfactants were investigated for potential to simulate hypoalbuminaemic plasma.

173 **2.4.3.1. Category 3a: Biorelevant surfactants**

174 *Attaining clinically relevant solubility with surfactants found in plasma (BS and PL), with and*
175 *without BSA.*

176 In order to evaluate the impact of BSA concentration and biorelevant surfactants on AmB
177 solubility, media with BS, PL and BSA were prepared. The use of phosphate buffer saline
178 (PBS) (Cold Spring Harbor Protocols, 2007) as a simpler buffer solution than KRB was also
179 investigated as a basis for media development. A 2 level factorial design of experiments (DoE)
180 was used to identify which factors had a significant effect on AmB solubility. Factors
181 investigated were type of buffer: PBS or KRB; BS concentration: 3.0 or 10.0 mM; and PL
182 concentration: 0.2 or 3.0 mM. The BS concentrations were selected to represent a wide range,
183 including concentrations higher than the biorelevant concentration, with all investigated
184 concentrations being higher than the critical micelle concentration of the surfactants. The PL
185 concentration was set in order that the PL/ (BS+PL) molar fraction was lower than 0.6, which
186 is the necessary for mixed micelles formation (Moschetta et al., 2001). Eight experimental
187 setups resulted from the combination of these factors, BSA 4.0% w/v was added to all media,
188 and solubility studies were performed in the 8 media. After the identification of the statistically
189 significant factors affecting AmB solubility, the compositions of clinically relevant media were
190 predicted with a DoE (section 2.10) which targeted AmB solubility in plasma. AmB solubility
191 studies were then conducted in these predicted media for comparison with AmB plasma
192 solubility values to validate the prediction. To investigate how BSA affects AmB solubility in
193 the presence of the biorelevant surfactants, the predicted media were also prepared without
194 BSA. Media characterization, AmB degradation and solubility studies were performed in the
195 developed media with and without BSA (section 2.5, 2.6 and 2.7).

196 **2.4.3.2. Category 3b: Synthetic surfactants**

197 *Attaining clinically relevant solubility with synthetic surfactants with and without BSA.*

198 KRB and PBS were tested with 3 different types of surfactants: SLS (anionic surfactant),
199 CTAB (cationic surfactant) and Tween 80 (non-ionic surfactant). The critical micelle
200 concentration (CMC) of charged surfactants was determined in PBS and KRB by
201 conductimetry (Conductivity Meter, WPA CMD 500, Scientific Laboratory Supplies Ltd, UK)
202 to assure that the concentrations selected were above the CMC. 1 mL of a 10.0 mM solution of
203 the surfactant in the corresponding buffer was added to either 20 mL (for SLS) or 50 mL (for
204 CTAB) of the same buffer and the conductivity recorded. Conductivity was plotted against the
205 surfactant concentration and the CMC was established when there was a sudden change in the
206 slope. Measurements were performed in triplicate. Tween 80 CMC is not affected by the ionic
207 composition of the buffer and the CMC value reported in literature was used (Sigma-Aldrich,
208 2019). To study the effect of the surfactants on AmB solubility, the surfactant concentrations
209 investigated were 5.0, 50.0 and 100.0 mM with and without BSA 4.0% w/v. Single point AmB
210 solubility experiments were conducted in all the media following the procedure described in
211 section 2.7, with 1 mg of AmB API powder added in 10 mL of medium and sampling at 12 h,
212 as a solubility plateau value was reached around 12 h in previous solubility determinations
213 (Diaz de Leon-Ortega et al., 2018). The media with the surfactant resulting in an AmB
214 solubility value closest to the AmB plasma solubility, with and without BSA, were selected to
215 develop the clinically relevant media. Surfactant concentrations, in the range where media
216 demonstrated the clinically relevant AmB solubility value, were investigated in order to obtain
217 the surfactant concentration to produce clinically relevant AmB solubility by performing single
218 point solubility experiments at 12 h in those ranges. Media characterization, degradation and
219 solubility studies (section 2.5, 2.6 and 2.7) were performed in the developed media.

220 **2.4.3.3. Category 3c: Potential media to simulate hypoalbuminaemic patients.**

221 *Potential for media with synthetic surfactants and BSA, to be used as a basis to develop media*
222 *simulating hypoalbuminaemic plasma.*

223 In order to identify conditions that could direct future hypoalbuminaemic medium
224 development, clinically relevant medium in PBS from category 3b was used as a base. For
225 these studies there was no target solubility value as a reference AmB solubility in
226 hypoalbuminaemic plasma is not available. In order to mimic hypoalbuminaemic plasma, the
227 use of PBS was explored with a) 2.0% w/v BSA and the corresponding concentration of
228 surfactant developed as clinically relevant medium in category 3b, b) 2.0% w/v BSA with half
229 of the concentration of surfactant from category 3b media and c) 4.0% w/v BSA with half of
230 the concentration of surfactant from category 3b media. Media characterization, degradation
231 studies (section 2.5 and 2.6) and single point solubility studies as described in section 2.4.3.2
232 were performed in the media.

233 **2.5. Test media characterization**

234 Media characterization methodology was described previously (Diaz de Leon-Ortega et al.,
235 2018). Briefly, pH was measured in all the media following addition of all components.
236 Osmolality was measured via the freezing-point depression method with a Micro-Osmometer
237 3300 (Advanced Instruments, Massachusetts USA). Viscosity of all media was measured with
238 a Bohlin Rheometer (Germany) at 25°C in triplicate. Buffer capacity was determined by adding
239 HCl 0.1 M until there was a change of 1 unit in the pH (Equation 1).

$$240 \quad \frac{dB}{dpH} = \frac{(HCl \text{ volume } (L))([HCl])}{\left(\frac{\text{average volume of sample}}{\text{over range involved}}\right)(\Delta pH)} \quad \text{Equation 1}$$

241 where $\frac{dB}{dpH}$ is the buffer capacity, $[HCl]$ is the concentration of hydrochloric acid and ΔpH is
242 the pH increment. The measurement was performed in triplicate.

243 The media were graded based on their complexity and received values from 1 to 4, being 1 to
244 the simplest and 4 the most complex medium. The scale was based on the number of

245 components to prepare the medium (1 for PBS, 2 for KRB) and on the ease of preparation (1
246 for mixing the components, 2 for mixing components and evaporating solvents).

247 **2.6. Degradation rate constant determination of AmB in plasma and in test media**

248 The degradation rate constant determination methodology was described previously (Diaz de
249 Leon-Ortega et al., 2018). Briefly, 3 mg of AmB API powder was added to 20 mL of plasma
250 and then stirred for 1 hour at 130 rpm at 37°C. Samples were centrifuged for 5 minutes at 3000
251 rpm at 4°C and the supernatant incubated at 37°C. Samples were taken at 0.5, 1.0, 1.5, 2.0, 3.0,
252 4.0, 5.0, 6.0, 8.0 and 24.0 hours, and analysed as described in section 2.3. AmB in the samples
253 was determined. For dissolution media, the same procedure was followed with 10 mg of AmB
254 API powder added to 50 mL of dissolution media and monitored for 8 hours. All experiments
255 were performed in triplicate. A linear fit was applied to the degradation data from 4 h to the
256 last time point, after a natural logarithm transformation of the measured concentration (Excel
257 2013) and the degradation rate constant (k_{deg}) was calculated as the slope of the line.

258 **2.7. Solubility studies of AmB in plasma and in test media**

259 Solubility study methodology was described previously (Diaz de Leon-Ortega et al., 2018).
260 Briefly, approximately 2.5 mg of AmB API powder were placed in a 100 mL glass bottle with
261 30 mL of the corresponding dissolution media, stirred at 130 rpm and incubated at 37°C. The
262 sampling times were 0.5, 1.0, 1.5, 2.0, 3.0, 4.0, 5.0, 6.0, 8.0, 10.0, 12.0 and 24.0 hours. The
263 undissolved AmB was removed by centrifugation and after protein precipitation and samples
264 were analysed as described in section 2.3. Solubility studies in plasma were performed with
265 1.5 mg of AmB in 10 mL of plasma. Solubility studies in media with synthetic surfactants
266 (single point solubility at 12 h) were performed with ~1 mg of AmB in 10 mL of medium. The
267 AmB solubility saturation value was considered when the concentration reached a plateau
268 value. An AmB solubility value in the dissolution media similar to the AmB plasma solubility
269 was considered "clinically relevant". All experiments were performed in triplicate.

270 **2.8. Dissolution studies of AmB in clinically relevant media from category 3a and 3b, and**
271 **category 3c media, with the flow through-cell dissolution apparatus**

272 Dissolution studies were carried out in a flow-through cell dissolution apparatus (Sotax CE7
273 smart connected to a Sotax piston pump CP7, Sotax, Switzerland) operated in the closed mode
274 (Fotaki, 2011). Tests were carried in category 3 clinically relevant media (3a and 3b) and in
275 media from category 3c. A 5mm ruby glass bead was positioned at the bottom of the cell (small
276 cell: 12 mm diameter; large cell: 22.6 mm diameter). 0.5 mg of AmB API powder was weighed
277 and mixed with 6.0 g or 0.75 g of 1 mm glass beads, for the large or small cell, respectively,
278 and were placed into the cell filling the conical part. Glass fibre filters (GF/D, GF/F) were
279 positioned at the top of the cell. Two different hydrodynamic conditions were tested: i. High
280 velocity: small cell with a flow rate of 35 mL/min (average linear velocity 0.52 cm/s) and ii.
281 Low velocity: large cell with a flow rate of 16 mL/min (average linear velocity 0.07 cm/s). 50
282 mL of test medium were placed into the reservoir under constant stirring at 37°C. 0.5 mL
283 samples were collected at specific time points up to 8 hours and volume was replaced with
284 fresh medium. Dissolution studies were also performed with 5 mg (high dose) of AmB in
285 category 3b PBS medium without BSA under both velocity conditions. Samples were treated
286 and analysed as described in section 2.3 and the %AmB dissolved over time was calculated.
287 All experiments were performed in triplicate.

288 **2.9. Treatment of dissolution data**

289 Treatment of dissolution data was described previously (Diaz de Leon-Ortega et al., 2018).
290 Briefly, AmB dissolution profiles were corrected for degradation using the corresponding
291 degradation rate constants with Equation 2.

292 $C_{corrected(t)} = C_t + k_{deg} * AUC_{0-t}$ Eq 2

293 where C_t is the observed concentration at time t , AUC_{0-t} is the Area Under the Observed
294 Concentration – Time Curve from time 0 to time t and k_{deg} is the degradation rate constant
295 obtained from the degradation experiments.

296 The corrected dissolution profiles were calculated based on $C_{corrected(t)}$ and a first order curve
297 fitting (Eq 3) was performed in order to obtain the dissolution rate constant (Graph Pad Prism
298 7, Graph Pad Software, Inc., USA).

$$299 X_{corrected(t)} = X_{max} * (1 - e^{-k_{diss}t}) \quad \text{Eq 3}$$

300 where k_{diss} is the dissolution rate constant, $X_{corrected(t)}$ is the corrected percent dissolved at
301 time t and X_{max} is the maximum corrected percent dissolved.

302 **2.10. Statistical analysis**

303 Equation 4 was used to analyse the DoE of the category 3a clinically relevant media development.

$$304 y = \mu + A + B + C + A * B + A * C + B * C \quad \text{Equation 4}$$

305 where y is the response (AmB solubility), μ is the total mean; A , B and C are the main factors
306 (buffer, BS concentration and PL concentration, respectively); $A * B$, $A * C$ and $B * C$ are the
307 2 level interactions. Buffer type was represented by a value of -1 for PBS and +1 for KRB. The
308 coefficients were determined by calculating the main effects and interactions and relating them
309 to the factor tested (by least square algorithms of DoE) and the substituted equation was used
310 to calculate the composition of clinically relevant media (targeting AmB solubility plasma
311 values).

312 To evaluate the effect of surfactants and BSA on AmB solubility in the category 3a and 3b
313 clinically relevant media, the standardized effects for surfactants (BS-PL, SLS, CTAB and
314 Tween 80), BSA presence and its interaction, were calculated and used to construct a Pareto
315 chart. A factor was significant when the standardized effect (bars) was larger than the line for
316 statistical significance level ($\alpha = 0.05$) (vertical line).

317 To compare degradation rate constants, a t-test was used to compare two experimental
318 independent means and a paired t-test to compare two experimental related means (significance
319 $p < 0.05$). A multiple linear regression model was used to investigate if the solubility and the
320 degradation rate constant of AmB in any given medium could be related to any of the
321 parameters of media characterization: viscosity, pH and buffer capacity (significance $p < 0.05$).
322 Data analysis and the DoE (design and analysis) were performed with the statistical software
323 Statgraphics Centurion XVII (USA).

324 **3. Results and discussion**

325 **3.1. Determination of solubility and degradation rate constant of AmB in human plasma** 326 **from healthy volunteers**

327 AmB solubility in plasma reached a plateau between 3 – 12 h at a concentration of $32.52 \pm$
328 $0.98 \mu\text{g/mL}$ (Figure 2) and the AmB degradation rate constant in plasma was $0.033 \pm 0.002 \text{ h}^{-1}$
329 ¹ (degradation half-life ~21 h) (Table 1).

330

331 **3.2. Test media development for evaluation of performance of parenteral drug products**

332 **3.2.1. Category 1 media**

333 AmB solubility values in category 1 media, obtained in our previous study, were lower (13.03
334 $- 17.56 \mu\text{g/mL}$) than those observed in plasma and the degradation rate constants were not
335 statistically similar to those observed in plasma (Figure 2, Table 1) (Diaz de Leon-Ortega et
336 al., 2018).

337 **3.2.2. Category 2 media**

338 The osmolality of Category 2 media is similar to the osmolality of plasma. The viscosity values
339 are also similar to those of plasma using a similar method and range of shear rates, to those
340 presented by Rand et al (Rand et al., 1964) for plasma at 22°C (Table 2).

341 On the other hand pH is only similar to plasma in the media with BSA but the buffer capacity
342 was not as high as in plasma. BSA increased the osmolality and the buffer capacity, and kept
343 the pH at ~7.5. However, when any other component apart from BSA was added, an increase
344 in the pH and a decrease in the buffer capacity were observed (Table 2).

345 Addition of BSA, in a concentration range from 1.5 to 4.0% w/v in KRB buffer (category 1
346 biorelevant media), was reported to increase AmB solubility (Diaz de Leon-Ortega et al.,
347 2018). The addition of biorelevant plasma components, to which AmB is bound *in vivo*, to the
348 medium would be expected to increase AmB solubility bringing it closer to its plasma
349 solubility. AmB concentration profiles in category 2 media show a decrease in AmB solubility
350 compared to its solubility in KRB BSA 4.0% w/v (category 1 media) and plasma (Figure 2).

351 In the concentrations utilized for media development, PL and CH are not soluble (NCBI, 2019;
352 Sigma-Aldrich, 2019); this might be counterproductive to AmB solubilisation, as the
353 components need to be in solution in order to dissolve AmB. When CH or BS-PL are present
354 in the media without BSA the AmB solubility values are the lowest of all the values measured
355 in all the tested media (Figure 2). In the media where BSA is present along with BS-PL or BS-
356 PL CH, regardless of its concentration, AmB solubility is slightly higher than in these media
357 without BSA, but lower than the solubility values measured in media with only BSA (Figure
358 2). It has been reported that BSA is capable of binding bile salts (Farruggia and Picó, 1999;
359 Green et al., 1971; Pico and Houssier, 1989), cholesterol (Sankaranarayanan et al., 2013; Zhao
360 and Marcel, 1996) and phospholipids (Jonas, 1976). The results suggest that, rather than CH
361 or BS-PL having an additive effect to BSA on the solubility of AmB, BSA is hindering
362 solubilisation by the biorelevant components added to the medium, while at the same time the
363 biorelevant components are reducing the solubilising effect of BSA on AmB. Only in the
364 medium with the highest BSA concentration (KRB BS PL BSA 8.0% w/v) AmB solubility was
365 increased, but still it was lower than in the medium with only BSA 4.0% w/v (category 1

366 biorelevant medium). As category 2 media failed to produce better solubility values than
367 category 1 media, no further studies were performed with these media.

368 **3.2.3.1. Category 3a media**

369 The concentrations of BS and PL in the medium were the only significant factors identified in
370 the analysis of AmB solubility for the development of category 3a media (Figure 3).

371 Equation 5 was obtained from the DoE analysis and was used to predict the concentrations of
372 BS and PL in both KRB and PBS to produce AmB solubility values similar to those observed
373 in plasma (clinically relevant).

$$374 \text{ Solubility } (\mu\text{g/mL}) = 5.56 - 2.09 * \text{Buffer} + 0.33 * \text{BS(mM)} + 0.04 * \text{PL(mM)} + \\ 375 0.29 * \text{Buffer} * \text{BS(mM)} + 0.81 * \text{Buffer} * \text{PL(mM)} + 0.18 * \text{BS(mM)} * \text{PL(mM)} \quad (\text{Eq} \\ 376 5).$$

377 The predicted concentrations of BS and PL were BS 20.0 mM PL 4.0 mM for KRB BSA 4.0%
378 w/v and BS 19.7 mM PL 7.9 mM for PBS BSA 4.0% w/v. The media characterization showed
379 that the presence of BSA increases the buffer capacity, the osmolality and the pH (in KRB);
380 similar to the effects noted in category 2 media (Table 2). Osmolality was similar to that of
381 plasma only for the media prepared without BSA (the concentration of BS-PL had a high
382 impact on the osmolality and when BSA was added, osmolality increased up to 425 mOsm/L).
383 The pH value was only similar to that of plasma for the medium prepared in PBS, with the
384 buffer capacity being only statistically similar to the plasma value in PBS BS 19.8 mM PL 7.9
385 mM BSA 4.0% w/v. Degradation rate constants were not statistically similar to that observed
386 in plasma except in the KRB BS 20.0 mM PL 4.0 mM medium (Table 1). In both buffers, the
387 presence of BSA resulted in faster degradation of AmB than in the media without BSA. The
388 higher AmB degradation rate constant values in these media could potentially be due to the
389 absence of plasma components which could reduce the AmB degradation.

390 AmB solubility values in the media with BSA were lower than those observed in plasma, but
391 in the media without BSA, AmB solubility values were similar to those observed in plasma
392 (clinically relevant) (Figure 4).

393 The predicted BS and PL concentrations to attain clinically relevant solubility were much
394 higher than the initial exploration ranges. Thus the effects of BS - PL on the solubilising
395 potential of BSA and vice versa were not captured in the predicted media compositions as the
396 equation was not validated outside of these exploration ranges. However, the effect of BSA in
397 the first place seems to have been immaterial in equation 3.5, as clinically relevant solubility
398 was achieved without inclusion of BSA in the media.

399 **3.2.3.2. Category 3b: clinically relevant media**

400 The CMC of SLS and CTAB in water is 8.1 mM and 1.0 mM, respectively (Attwood and
401 Florence, 1983). The CMC of charged surfactants tends to decrease in a medium where the
402 ionic strength is high, such as in saline buffers like PBS and KRB (Thongngam and
403 McClements, 2005). The CMC of SLS in PBS and KRB was 1.3 ± 0.0 mM and 1.4 ± 0.2 mM,
404 respectively and the CMC of CTAB in PBS and KRB was 0.9 ± 0.0 mM and 0.2 ± 0.0 mM,
405 respectively. The surfactant concentrations selected for the solubility studies were above their
406 CMC. CTAB was not soluble at 100.0 mM and KRB CTAB 50.0 mM BSA 4.0% w/v medium
407 gelatinized, thus, AmB solubility could not be measured in these media. Figure 5 shows the
408 AmB solubility in the various category 3b media with and without BSA.

409 The apparent AmB concentration, even with the highest surfactant concentration, was limited
410 by the AmB amount added ~ 1.0 mg, hence, the concentration could not be higher than ~100.0
411 $\mu\text{g/mL}$. The charged surfactants (anionic and cationic) solubilised more AmB than the non-
412 ionic surfactant despite the fact that AmB is a hydrophobic molecule ($\log P$ 0.8 (Sigma-Aldrich,
413 2015)). AmB, as an amphoteric molecule with two pKa values ($\text{pKa}_1 = 5.5$, $\text{pKa}_2 = 10.0$) will
414 be charged at pH 7, thus, the interaction between its charges and those of the surfactant would

415 promote contact of the molecules leading to solubilisation of the drug. Similar to category 2
416 and 3a media observations, BSA presence in the media decreased AmB solubility. It has been
417 reported that BSA binds to SLS, CTAB and Triton X-100 (non-ionic surfactant) with with the
418 weakest binding observed for Triton X-100 (De et al., 2005; Gull et al., 2009; Valstar et al.,
419 2000). Figure 6 shows the effect of surfactants (in both category 3a and 3b media) and BSA on
420 AmB solubility.

421 The surfactant presence has a statistically significant positive effect on AmB solubility,
422 whereas BSA and the interaction between BSA and surfactant have a negative effect. The
423 results suggest that the presence of BSA and the surfactant alone in the medium, solubilise
424 AmB (Diaz de Leon-Ortega et al., 2018), but when both are in the medium, they interfere with
425 each other preventing AmB solubilisation and leading to a decrease in the solubility compared
426 to the solubility reached in the medium with the surfactant alone. The ability of BSA to interfere
427 with several types of molecules (BS, PL, CH, SLS, CTAB, Tween 80, as found in this study)
428 has to be taken into account when a biorelevant or clinically relevant medium, incorporating
429 BSA, is developed. The required concentration of other components with surfactant/solubilising
430 activity could be under-estimated due to protein-surfactant interactions, leading to an
431 unintended reduction in API solubility. Among the media with the different surfactants tested,
432 only media which included SLS resulted in clinically relevant solubility values of AmB in KRB
433 and PBS either with or without BSA.

434 The compositions of media based on either KRB or PBS with BSA were calculated to target
435 an AmB clinically relevant solubility value (based on the single point solubility studies). The
436 calculated compositions of the media to reach AmB solubility values similar to the observed
437 plasma value were KRB SLS 30.0 mM BSA 4.0% w/v and PBS 60.0 mM BSA 4.0% w/v. The
438 media composition without BSA could not be obtained directly by just removing BSA from
439 the media as AmB solubility would be extremely high (Figure 5). Therefore, lower

440 concentrations of SLS (0.1 – 4.0 mM) were tested in PBS and KRB to find the appropriate
441 concentration for clinically relevant AmB solubility values without BSA. The SLS
442 concentrations where the AmB solubility was similar to that observed in plasma were 1.5 mM
443 for KRB and 1.4 mM for PBS. In the clinically relevant media developed with SLS, the
444 presence of BSA did not affect the viscosity but increased the buffer capacity and the
445 osmolality as in category 3a media (Table 2). AmB degradation rate constants were not
446 statistically similar to that observed in plasma, and were lowest in media composed of SLS
447 alone in buffer solution, which can be considered minimal (Table 1). The AmB degradation
448 rate constants in media with BSA were significantly higher than in the media without BSA.
449 This effect could be related to observations found in category 1 media (Table 1) where an
450 increasing BSA concentration had a positive effect on the degradation rate constant. The results
451 of the solubility studies in the developed category 3b media with and without BSA are
452 presented in Figure 7. It can be observed that the AmB concentration profiles in the category
453 3b media are similar to that observed in plasma.

454 **3.2.3.3. Category 3c media**

455 As solubility data in plasma was only available from plasma obtained from healthy subjects, a
456 target solubility value for hypoalbuminaemic plasma was not available. This section therefore
457 represents characterisation of media evolved from category 3b as potential candidates for
458 further patient-centric media development. The composition of the media was as follows: a)
459 PBS SLS 60.0 mM BSA 2.0% w/v, b) PBS SLS 30.0 mM BSA 2.0% w/v to reflect a reduction
460 of the inhibition of BSA on SLS solubilisation of AmB (observed during category 2 and 3a and
461 3b media development) when the lower BSA concentration was used and c) PBS SLS 30.0 mM
462 BSA 4.0% w/v to explore the reduced potential for SLS solubilisation which might better
463 reflect a potentially lower solubility in hypoalbuminaemic plasma. These 3 media had
464 characteristics similar to healthy plasma (Table 2) apart from a reduced buffer capacity ($p <$

465 0.05) and slightly lower pH. The AmB degradation rate constants in media with BSA 2.0% w/v
466 are apparently lower than those obtained in media with BSA 4.0% w/v (category 3b and 3c)
467 but the difference was not statistically significant. Only the degradation rate constant in PBS
468 SLS 60.0 mM BSA 2.0% w/v was statistically similar to that observed in plasma. The results
469 of the single point (12h) AmB solubility studies in these media were: a) PBS SLS 60.0 mM
470 BSA 2.0% w/v = 65.57 ± 4.98 $\mu\text{g/mL}$, b) PBS SLS 30.0 mM BSA 2.0% w/v = 25.84 ± 0.97
471 $\mu\text{g/mL}$, c) PBS SLS 30.0 mM BSA 4.0% w/v = 19.77 ± 0.29 $\mu\text{g/mL}$. This supports the
472 hypothesis that BSA interferes with the action of the surfactants, in this case SLS, with the 12
473 h concentrations highest and lowest in the media with SLS 60.0 mM and BSA 2.0% w/v and
474 SLS 30.0 mM and BSA 4.0% w/v, respectively.

475 **3.2.4. Summary and evaluation of the test media**

476 Table 3 presents a summary and an evaluation of solubility, degradation rate constant and
477 media characterization in comparison with the parameters obtained/reported in plasma.
478 Although category 1 media (Diaz de Leon-Ortega et al., 2018) was not clinically relevant for
479 solubility or degradation, this media could be useful to investigate the impact of albumin
480 concentration on poorly soluble and highly – protein bound drugs as demonstrated for AmB in
481 terms of solubility, degradation and pharmacological activity (Diaz de Leon-Ortega et al.,
482 2018). Clinically relevant AmB solubility values are achieved by using biorelevant surfactants
483 in category 3a media without BSA. These media could be used for *in vitro* release tests of AmB
484 lipid-based formulations and also, these media with BSA could be used in order to explore
485 effects of BSA on release from the formulation. Clinically relevant AmB solubility values were
486 achieved in all the category 3b media developed. Category 3b media without BSA could be
487 proposed as a basis for the development of appropriate media for compendial release tests, as
488 they easier to prepare and the degradation of the drug is minimal (Table 1). For category 3c
489 media, there were no reference values for solubility, degradation and media characterization

490 due to the lack of availability of hypoalbuminaemic plasma. Assuming that AmB solubility
491 will be lower in hypoalbuminaemic plasma compared to healthy plasma, PBS SLS 30.0 mM
492 BSA 4.0% w/v is a good candidate for the development of simulated hypoalbuminaemic
493 plasma as the AmB solubility at 12 h in this medium was lower than the clinically relevant
494 value.

495 The multiple linear regression analysis showed that neither the solubility nor the degradation
496 rate constant could be related to any of the properties of media characterization shown in Table
497 2 ($p > 0.05$).

498 **3.4. Dissolution studies of AmB with the flow through cell apparatus in clinically relevant** 499 **media**

500 Dissolution studies were performed in media with clinically relevant AmB solubility from
501 category 3a and 3b, and in each of the media explored in category 3c (Figure 8).

502 Clinically relevant AmB solubility values were obtained in PBS and in KRB, but the media
503 with PBS were selected for dissolution studies due to their reduced medium complexity
504 (compared to KRB). First order equation parameters of AmB, for dissolution profiles
505 (corrected for degradation) fitted to Eq 3, are listed in Table 4.

506 Dissolution profiles in PBS BS 19.8 mM PL 7.9 mM could not be modeled using Eq 3 in either
507 low or high velocity conditions. In the low velocity environment, the %AmB dissolved reached
508 a maximum value of $44.93 \pm 2.89\%$ at 3.0 h and then started to decrease until the end of the
509 experiment (8 h). This could indicate that mixed micelles of BS – PL need a stronger agitation
510 (as in the bottle/stirrer setup used in the solubility and degradation studies) for a notable,
511 durable effect on AmB dissolution. There was no reduction over time of the AmB percent
512 dissolved when the test was conducted at high velocity, however in this situation there was no
513 discernible plateau and rather a very gradual increase in % dissolved over time, prohibiting

514 fitting of Eq 3 to the data. In summary, AmB dissolution is greater under the high velocity
515 conditions in the clinically relevant category 3a medium (Figure 8).

516 There was a statistically significant negative effect of velocity on the dissolution rate constant
517 for the 0.5 mg dose and a positive effect on maximum % dissolved on the 5 mg dose; however,
518 these differences were of low practical significance and possibly reflect process variability.

519 The %AmB dissolved in the experiment with the high dose of AmB reached a plateau value of
520 around 20%, due to the solubility of AmB in this medium ($\sim 30 \mu\text{g/mL}$), (Figure 8). In category
521 3b medium with BSA, with respect to velocity, the low and high velocity conditions had little
522 effect on AmB dissolution in comparison to medium composition.

523 The velocity regimes in the flow through apparatus (average velocities: low velocity: 0.07 cm/s,
524 high velocity: 0.52 cm/s), are low overall in comparison to the bottle/stirrer set up. A faster
525 dissolution and a higher %AmB dissolved is observed in the category 3b medium with BSA
526 compared to that observed in the medium without BSA. This could be attributed to increased
527 wetting/dispersion from either the BSA or the SLS. PBS SLS 1.4 mM is therefore suggested
528 as a simplified medium that could be used in compendial dissolution testing of AmB parenteral
529 formulations, as clinically relevant AmB solubility values were obtained in this medium.

530 In category 3c media, the %AmB dissolved in PBS SLS 60.0 mM BSA 2.0% w/v started to
531 decrease before the 1.5 h sample in the low velocity conditions. The results suggest that the
532 agitation required to keep SLS, BSA and AmB in solution at these concentrations was higher
533 as the decrease was not observed when the high velocity conditions were used. The highest
534 %AmB dissolved was observed in PBS SLS 60.0 mM BSA 2.0% w/v and the lowest in PBS
535 SLS 30 mM BSA 4.0% w/v, again supporting the hypothesis that BSA binds the surfactants
536 and prevents their interaction with AmB. The AmB dissolution profiles in PBS SLS 30.0 mM
537 BSA 2.0% w/v and PBS SLS 60 mM BSA 4.0% w/v were similar, probably due to the same
538 ratio of SLS/BSA in these two media. Velocity had a negative effect only on the dissolution

539 rate of AmB in PBS SLS 30.0 mM BSA 2.0% w/v whereas this was not observed in the AmB
540 dissolution in the other category 3c media. Based on the presumption of lower AmB solubility
541 in hypoalbuminaemic plasma, the results suggest that the most suitable clinically relevant
542 medium to simulate hypoalbuminaemic conditions is PBS SLS 30 mM BSA 4.0% w/v;
543 confirmation with solubility studies in plasma from hypoalbuminaemic patients would be
544 needed. As the dissolution profiles were calculated based on concentrations corrected
545 accounting for AmB degradation, the degradation rate constant was not a factor to be
546 considered in the analysis, as it was already taken into account in the profiles.

547 The dissolution studies provided information on which test media would be suitable for
548 formulation release studies. For example, some test media were not able to keep AmB
549 solubilized for the duration of an 8 h test, even after correcting for degradation, despite being
550 designed to produce clinically relevant solubility values. Furthermore, there is scope for further
551 exploration of dissolution test conditions in terms of apparatus and hydrodynamic environment
552 to determine suitably discriminating conditions for dissolution/release testing of parenteral
553 formulations.

554 Summarizing, in order to develop a clinically relevant test for a poorly soluble, degradation-
555 susceptible and highly protein-bound drug for parenteral administration, based on the current
556 work focussed on AmB, the following steps are proposed:

- 557 1. Determine API solubility in the target fluid, in this case plasma
- 558 2. If the API is highly protein-bound, a suitable protein should be incorporated in the medium
559 or a surfactant able to match the desired solubility; and if both are going to be incorporated,
560 investigate the effect of any interaction between them on the solubility of the drug
- 561 3. Determine the degradation rate of the API in the media investigated for further correction of
562 dissolution/release profiles

563 4. Test the API dissolution/solubility behaviour in the test media and hydrodynamic conditions
564 that will be used in the formulation dissolution/release testing, as stability/solubility problems
565 will be easier to be identified using the API alone before the drug dissolution/ release testing
566 from the formulation.

567

568 **4. Conclusions**

569 AmB is an antifungal drug that is highly bound to plasma proteins, including albumin and
570 lipoproteins. It is administered to patients intravenously as lipid-based formulations. Therefore,
571 a test medium to assess the release profile of the drug from its lipid-based parenteral
572 formulations that can provide clinically relevant results is desirable.

573 In this study we have developed biorelevant media based on plasma composition and clinically
574 relevant dissolution media based on the solubility of AmB in plasma. This was achieved by
575 using saline buffers, surfactants (biorelevant and synthetic) and BSA. Clinically relevant AmB
576 solubility was not achieved in the biorelevant media. It was shown that addition of BSA in the
577 medium generally induces a faster degradation of AmB. Another role of BSA in the media is
578 the capability to interfere with the solubilizing activity of almost all of the components that
579 were added to the media. Instead of resulting in an improved AmB solubility by combining
580 surfactants with BSA, the opposite effect was observed. This has to be taken into consideration
581 for development of *in vitro* test media where the protein binding is an important feature. Based
582 on the dissolution study results, medium complexity and minimal degradation, PBS SLS 1.4
583 mM is suggested as an option for development of release tests for AmB formulations. For the
584 simulated hypoalbuminaemic media, PBS SLS 30 mM BSA 4.0% w/v is suggested as a
585 potential candidate medium for further (patient centric) medium development, although future
586 experiments with hypoalbuminaemic plasma are needed to confirm the effect of
587 hypoalbuminaemia on solubility. Guidance is given for the initial stages of the development of

588 a clinically relevant *in vitro* dissolution/release test for parenteral formulations. Development
589 of clinically relevant media is a first step for developing clinically relevant dissolution/ release
590 tests with a view to obtaining *in vitro* data predictive of the *in vivo* behaviour of the formulation
591 and the drug.

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599

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711

712 **Tables**

713 Table 1. Degradation rate constants of AmB in plasma, category 1 and 3 media. (Mean \pm SD;
 714 n = 3).

Type of medium	Medium	k_{deg} (h^{-1})	
Plasma	Plasma	0.033 \pm 0.002	
Category 1	KRB BSA 1.5% w/v	0.026 \pm 0.000 (Diaz de Leon-Ortega et al., 2018)	
	KRB BSA 2.0% w/v	0.065 \pm 0.005 (Diaz de Leon-Ortega et al., 2018)	
	KRB BSA 3.0% w/v	0.065 \pm 0.021 (Diaz de Leon-Ortega et al., 2018)	
	KRB BSA 4.0% w/v	0.095 \pm 0.003 (Diaz de Leon-Ortega et al., 2018)	
Category 3	3a	KRB BS 20.0 mM PL 4.0mM	0.023 \pm 0.010
		KRB BS 20.0 mM PL 4.0 mM BSA 4.0% w/v	0.060 \pm 0.008
		PBS BS 19.8 mM PL 7.9 mM	0.048 \pm 0.006
		PBS BS 19.8 mM PL 7.9 mM BSA 4.0% w/v	0.097 \pm 0.021

	3b	KRB SLS 1.5mM	0.009 ± 0.007
		KRB SLS 30.0mM BSA 4.0% w/v	0.038 ± 0.001
		PBS SLS 1.4 mM	0.005 ± 0.003
		PBS SLS 60.0 mM BSA 4.0% w/v	0.052 ± 0.015
	3c	PBS SLS 30.0 mM BSA 2.0% w/v	0.062 ± 0.014
		PBS SLS 30.0 mM BSA 4.0% w/v	0.082 ± 0.015
		PBS SLS 60.0 mM BSA 2.0% w/v	0.041 ± 0.013

715

716

717 Table 2. Media composition and media characterization. Plasma characterization is included (Mean \pm SD; n = 3 for Vis and BC HCl).

Category	Medium	Osm (mOsm/L)	Vis (cPs)	pH	BC HCl (mEq/L/pH)
Plasma	Plasma	275 - 300 (Dasgupta and Wahed, 2014)	3.5 (Rand et al., 1964)	7.34 \pm 0.04 (Shepherd, 1979)	16.1 \pm 0.9 (Ellison et al., 1958)
Category 1	KRB BSA 4.0% w/v	308 (Diaz de Leon-Ortega et al., 2018)	4.0 \pm 0.0 (Diaz de Leon-Ortega et al., 2018)	7.36 (Diaz de Leon-Ortega et al., 2018)	12.0 \pm 1.2
Category 2	KRB BS 12.0 μ M PL 2.5 mM	278	5.0 \pm 0.1	8.64	1.5 \pm 0.0
	KRB BS 12.0 μ M PL 2.5 mM CH 4.5 mM	273	5.0 \pm 0.1	8.79	1.5 \pm 0.1
	KRB BS 12.0 μ M PL 2.5 mM BSA 2.0% w/v	314	5.2 \pm 0.1	7.79	7.8 \pm 0.0
	KRB BS 12.0 μ M PL 2.5 mM CH 4.5 mM BSA 4.0% w/v	306	5.0 \pm 0.1	7.80	7.5 \pm 0.2

		KRB BS 12.0 μ M PL 2.5 mM BSA 8.0% w/v	351	5.2 \pm 0.0	7.65	7.7 \pm 0.0
Category 3	3a	KRB BS 20.0 mM PL 4.0 mM	310	4.8 \pm 0.1	8.25	1.7 \pm 0.0
		PBS BS 19.8 mM PL 7.9 mM	330	4.7 \pm 0.1	7.36	6.1 \pm 0.1
		KRB BS 20.0 mM PL 4.0 mM BSA 4.0% w/v	415	5.0 \pm 0.1	8.50	5.2 \pm 0.1
		PBS BS 19.8 mM PL 7.9 mM BSA 4.0% w/v	425	4.9 \pm 0.1	7.18	14.2 \pm 0.8
	3b	KRB SLS 1.5 mM	289	4.6 \pm 0.1	8.54	1.2 \pm 0.0
		PBS SLS 1.4 mM	280	4.4 \pm 0.1	7.43	5.6 \pm 0.1
		KRB SLS 30.0 mM BSA 4.0% w/v	350	5.0 \pm 0.1	7.84	7.9 \pm 0.1
		PBS SLS 60.0 mM BSA 4.0% w/v	325	5.2 \pm 0.1	7.56	10.3 \pm 0.2
	3c	PBS SLS 30.0 mM BSA 2.0% w/v	300	4.8 \pm 0.0	7.10	9.3 \pm 0.2
		PBS SLS 30.0 mM BSA 4.0% w/v	297	4.6 \pm 0.0	7.18	9.6 \pm 0.6
		PBS SLS 60.0 mM BSA 2.0% w/v	302	4.9 \pm 0.1	7.04	11.6 \pm 0.3

718 Osm: Osmolality, Vis: Viscosity, BC HCl: buffer capacity determined with HCl.

719 Table 3. Evaluation of solubility, degradation rate constant and media characterization in comparison with the parameters obtained/reported in
 720 plasma. ND = not determined due to data unavailable for comparison, ✖ = not biorelevant, ✓ = biorelevant.

Category	Medium	CRS	CRD	Osm	Vis	pH	BC HCl	Medium Complexity
Category 1	KRB BSA 4.0% w/v (Diaz de Leon-Ortega et al., 2018)	No	No	✖	✖	✓	✖	1
Category 3a	KRB BS 20.0 mM PL 4.0 mM	Yes	Yes	✖	✖	✖	✖	4
	PBS BS 19.8 mM PL 7.9 mM	Yes	No	✖	✖	✓	✖	3
	KRB BS 20.0 mM PL 4.0 mM BSA 4.0% w/v	No	No	✖	✖	✖	✖	4
	PBS BS 19.8 mM PL 7.9 mM BSA 4.0% w/v	No	No	✖	✖	✖	✓	3
Category 3b	KRB SLS 1.5 mM	Yes	No	✓	✖	✖	✖	2
	PBS SLS 1.4 mM	Yes	No	✓	✖	✓	✖	1
	KRB SLS 30.0 mM BSA 4.0% w/v	Yes	No	✖	✖	✖	✖	2
	PBS SLS 60.0 mM BSA 4.0% w/v	Yes	No	✖	✖	✖	✖	1
Category 3c	PBS SLS 30.0 mM BSA 2.0% w/v	ND	ND	ND	ND	ND	ND	1
	PBS SLS 30.0 mM BSA 4.0% w/v	ND	ND	ND	ND	ND	ND	1

	PBS SLS 60.0 mM BSA 2.0% w/v	ND	ND	ND	ND	ND	ND	1
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721 CRS: AmB clinically relevant solubility, CRD: AmB clinically relevant degradation rate constant, Osm: osmolality, Vis: viscosity, BC HCl: buffer

722 capacity determined with HCl, MC: medium characterisation score

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724 Table 4. Parameters obtained after fitting (Eq 3) of %AmB dissolution profiles in category 3b clinically relevant media and 3c media with the flow
 725 through cell apparatus (Mean \pm SD, n = 3).

Type of medium	Medium	Flow/velocity	k_{diss} (h ⁻¹)	X_{max} (%)	R ²	AIC
Category 3b	PBS SLS 1.4 mM Low dose	Low	2.39 \pm 0.13	36.28 \pm 0.59	0.94 \pm 0.00	50.03 \pm 0.29
	PBS SLS 1.4 mM High dose	Low	2.98 \pm 0.74	16.75 \pm 1.16	0.91 \pm 0.01	38.77 \pm 2.28
	PBS SLS 60.0 mM BSA 4.0% w/v	Low	3.65 \pm 1.59	52.79 \pm 5.52	0.91 \pm 0.05	63.05 \pm 3.77
	PBS SLS 1.4 mM Low dose	High	1.88 \pm 0.26	38.66 \pm 2.08	0.93 \pm 0.02	53.94 \pm 4.06
	PBS SLS 1.4 mM High dose	High	2.50 \pm 0.40	19.47 \pm 0.81	0.92 \pm 0.01	40.40 \pm 1.32
	PBS SLS 60.0 mM BSA 4.0% w/v	High	5.60 \pm 1.30	62.86 \pm 5.22	0.91 \pm 0.10	63.03 \pm 12.28

Category 3c	PBS SLS 30.0 mM BSA 2.0% w/v	Low	4.21 ± 0.96	53.38 ± 9.94	0.96 ± 0.05	50.47 ± 9.28
	PBS SLS 30.0 mM BSA 2.0% w/v	High	2.33 ± 0.35	63.07 ± 3.48	0.94 ± 0.01	63.20 ± 1.21
	PBS SLS 30.0 mM BSA 4.0% w/v	High	7.66 ± 5.39	37.22 ± 8.20	0.89 ± 0.04	57.06 ± 3.45
	PBS SLS 60.0 mM BSA 2.0% w/v	High	6.43 ± 2.87	78.38 ± 0.50	0.96 ± 0.01	63.08 ± 3.31

726

727 R²: correlation coefficient, AIC: Akaike Information Criterion.

728 **Figures' captions**

729

730 **Figure 1.** Categories of media development for evaluation of performance of parenteral drug
731 products.

732 **Figure 2.** Solubility study of AmB in category 2 media: AmB concentration as a function of
733 time in plasma and category 2 media (Mean \pm SD; n= 3). KRB BSA 4.0% w/v solubility
734 (category 1 medium) and KRB BS 12.0 μ M PL 2.5 mM BSA 8.0% w/v were added for
735 comparison purposes (Diaz de Leon-Ortega et al., 2018). BSA concentration is in % w/v units.

736 **Figure 3.** Pareto chart for the standardized effects of the main factors and 2 level interactions
737 of the analysis of AmB solubility in media with BS, PL and different types of buffer. The black
738 horizontal line represents the significance threshold for the effects. The factors with an effect
739 (bar) larger than the threshold are statistically significant.

740 **Figure 4.** Solubility study of AmB in category 3a media: AmB concentration as a function of
741 time in category 3a media with and without BSA (Mean \pm SD; n= 3). BSA concentration is in
742 % w/v units. AmB plasma solubility was added for comparison purposes [solid lines represent
743 the media with BSA 4.0% w/v; dashed lines represent the media without BSA].

744 **Figure 5.** Solubility study of AmB in media with surfactants for the development of category
745 3b media: AmB concentration in PBS or KRB with 5.0, 50.0 and 100.0 mM concentrations of
746 SLS, CTAB or Tween with and without BSA 4.0% w/v at 12 h (Mean \pm SD; n= 3). Black
747 horizontal line represents the AmB solubility value in human plasma from healthy subjects.

748 **Figure 6.** Pareto charts for the standardized effects of the main factors and 2 level interactions
749 of the analysis of AmB solubility in media with surfactants and BSA 4.0% w/v. The black
750 horizontal line represents the significance threshold for the effects. The factors with an effect
751 (bar) larger than the threshold are statistically significant.

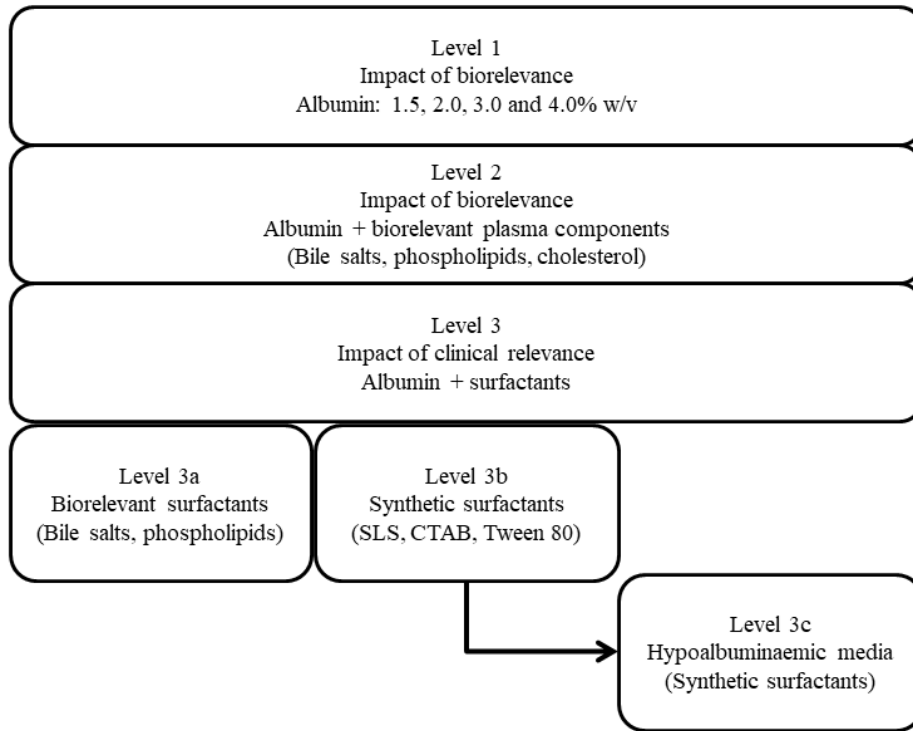
752 **Figure 7.** Solubility study of AmB in category 3b media: AmB concentration as a function of
753 time in the category 3b clinically relevant media with and without BSA (mean \pm SD; n= 3).
754 AmB plasma solubility was added for comparison purposes. The BSA concentration is in %
755 w/v units.

756 **Figure 8.** %AmB dissolved as a function of time in the category 3a and 3b clinically relevant
757 media and in category 3c media with the flow through cell apparatus at 37°C (mean \pm SD; n=
758 3). High dose = 5 mg of AmB. BSA concentration is in % w/v units. Points represent observed
759 data and the lines the first order (Eq 3) equation fittings.

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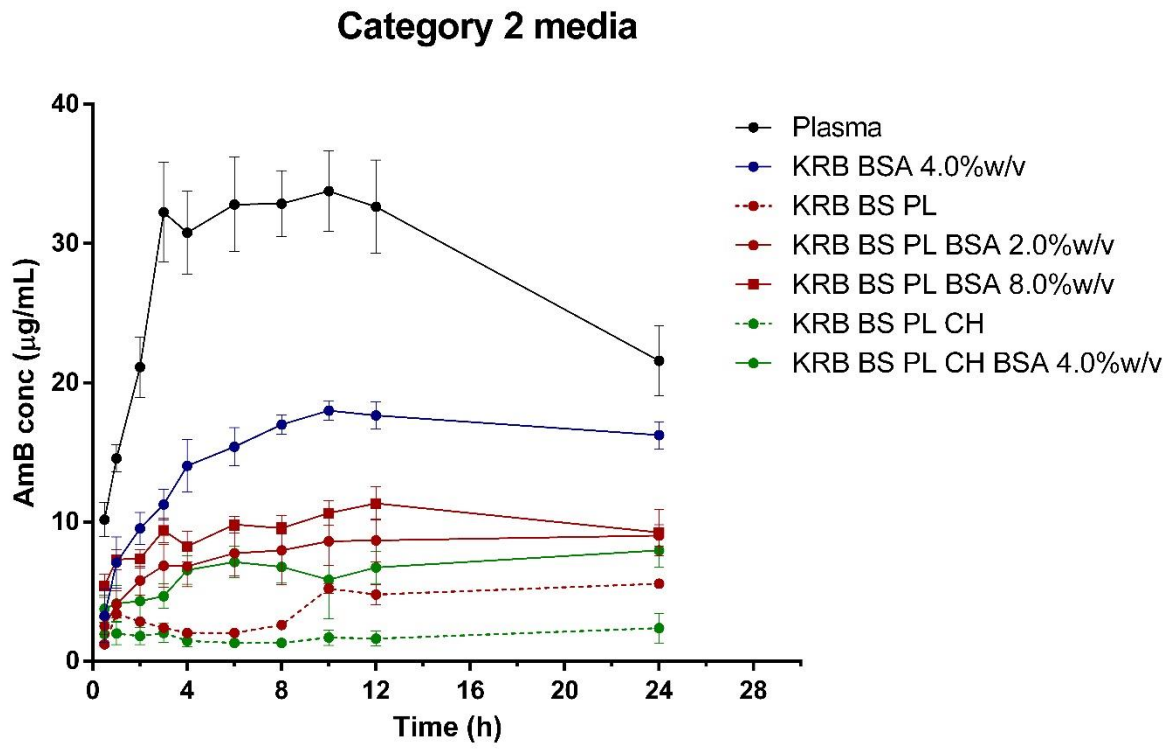
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764 **Figure 1**

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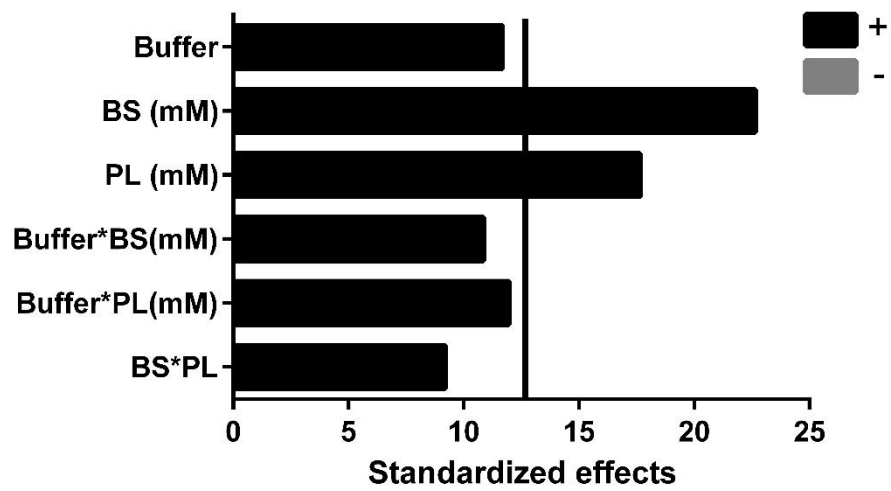
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770 **Figure 2**

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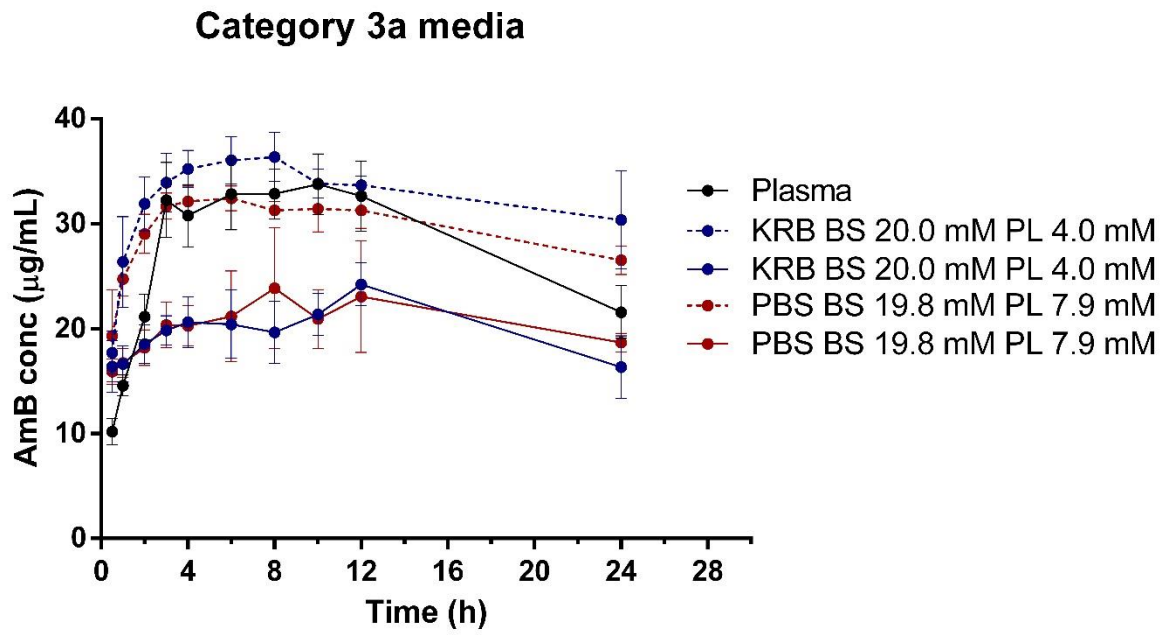


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774 **Figure 3**

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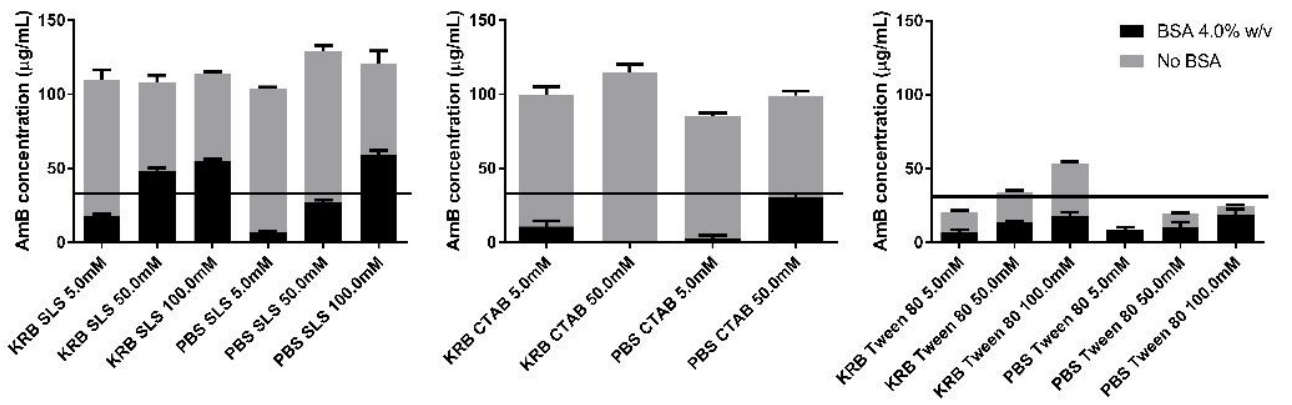
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778 **Figure 4**

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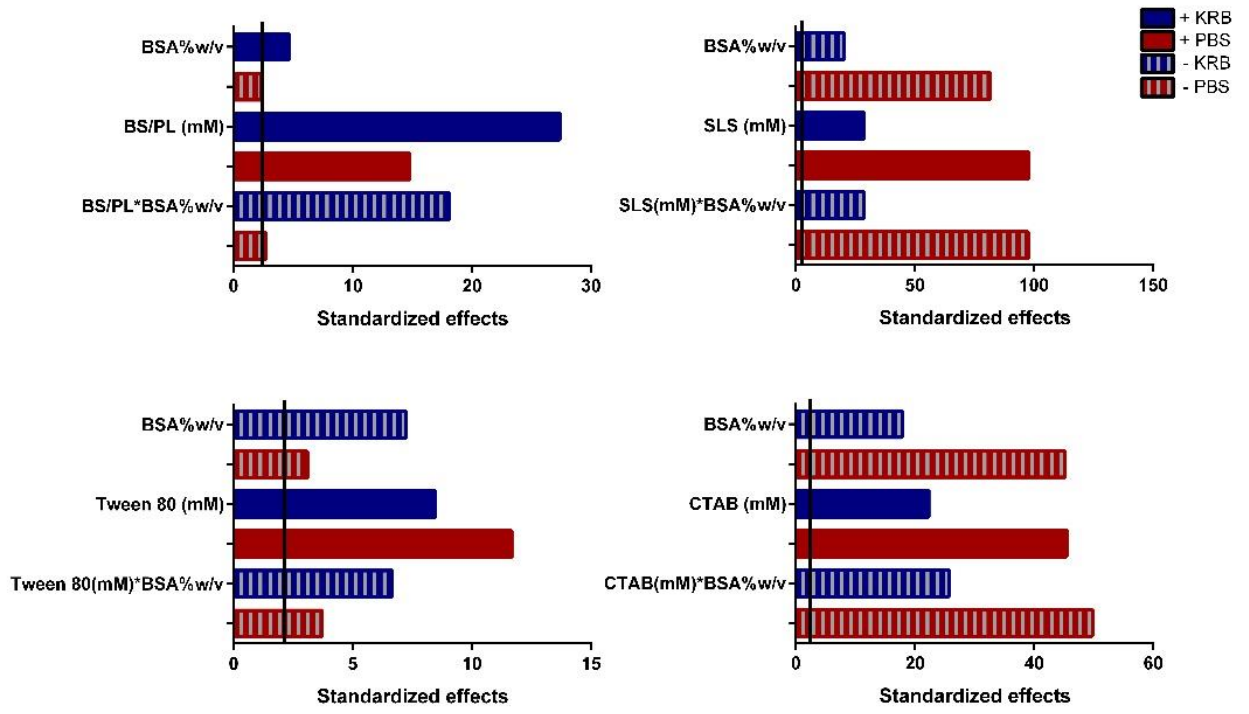
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784 **Figure 5**

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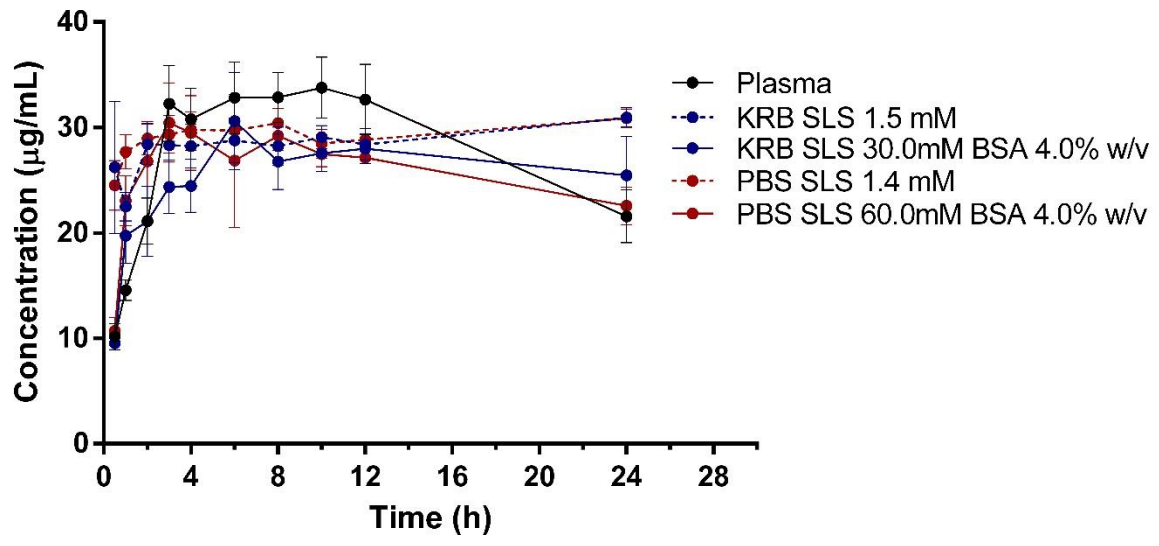


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788 **Figure 6**

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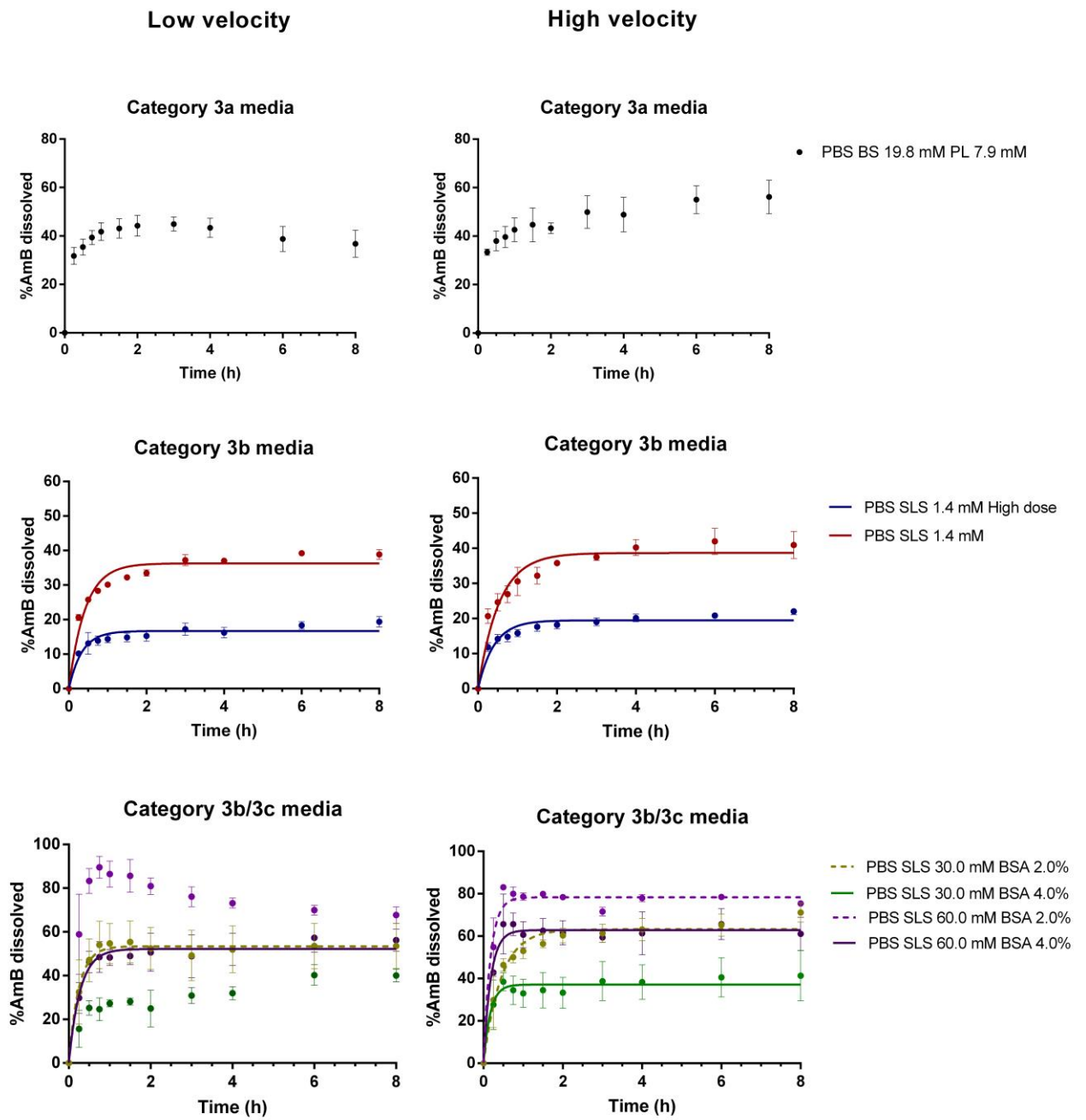
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792 **Figure 7**

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796 **Figure 8**