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## Synthesis, characterisation and application of inherently conducting polymer nanoparticles

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# SYNTHESIS, CHARACTERISATION AND APPLICATION OF INHERENTLY CONDUCTING POLYMER NANOPARTICLES

A thesis submitted in fulfilment of the requirements for the award of the degree

#### **DOCTOR OF PHILOSOPHY**

from the

#### UNIVERSITY OF WOLLONGONG

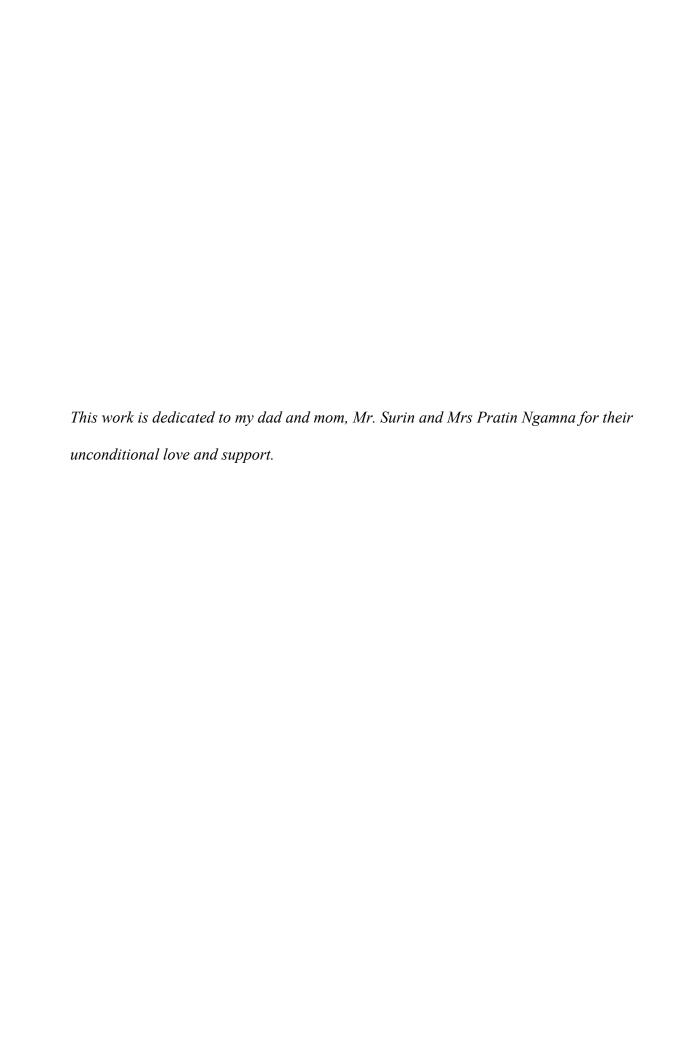
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ORAWAN NGAMNA, B.Sc.(Food Technology)

INTELLIGENT POLYMER RESEARCH INSTITUTE

DEPARTMENT OF CHEMISTRY

February 2006



#### **CERTIFICATION**

I, Orawan Ngamna, declare that this thesis, submitted in fulfilment of the requirements for the award of Doctor of Philosophy, in the Department of Chemistry, University of Wollongong, is wholly my own work unless otherwise referenced or acknowledged. The document has not been submitted for qualifications at any other academic institution.

Orawan Ngamna

February 2006

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#### **PUBLICATIONS**

- 1. S.E. Moulton\*, P.C. Innis, L.A.P. Kane-Maguire, O. Ngamna, and G.G. Wallace, "Polymerisation and characterisation of conducting polyaniline nanoparticle dispersions", *Current Applied Physics*, 2004, **4** (2-4), 402-406.
- A. Morrin, O. Ngamna, A.J. Killard, S.E. Moulton, M.R. Smyth\*, and G.G. Wallace\*, "An Amperometric Enzyme Biosensor Fabricated from Polyaniline Nanoparticles", *Electroanalysis*, 2005, 17 (5-6), 423-430.
- 3. O. Ngamna, A. Morrin, S.E. Moulton, A.J. Killard, M.R. Smyth, and G.G. Wallace\*, "An HRP based biosensor using sulphonated polyaniline", *Synthetic Metals*, 2005, **153** (1-3), 185-188.
- 4. A. Morrin, F. Wilbeer, O. Ngamna, S.E. Moulton, A.J. Killard, G.G. Wallace, and M.R. Smyth\*, "Novel biosensor fabrication methodology based on processable conducting polyaniline nanoparticles", *Electrochemistry Communications*, 2005, 7 (3), 317-322.
- 5. J.M. Pringle\*, O. Ngamna, J. Chen, G.G. Wallace, M. Forsyth and D.R. MacFarlane, "Conducting Polymer Nanoparticles Synthesized in an Ionic Liquid by Chemical Polymerisation", *Synthetic Metals*, in press.

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#### **TABLE OF CONTENTS**

CEF	ERTIFICATION					
ACI	ACKNOWLEDGEMENTS					
PUE	BLICATI	ONS	III			
TAF	BLE OF C	CONTENTS	V			
LIS	Γ OF AB	BREVIATIONS	XVI			
ABS	STRACT		XXI			
		General Introduction and Characterisation Technique	ues			
1.1	Inhere	ntly Conducting Polymer (ICPs)	1			
	1.1.1	Polyaniline (PANI)	3			
	1.1.2	Poly (2-methoxyaniline-5-sulphonic acid)	7			
	1.1.3	Polypyrrole	10			
	1.1.4	Polythiophene	13			
1.2	Conduc	cting Polymer Nanoparticles	16			
	1.2.1	Emulsion polymerisation	18			
	1.2.2	Use of steric stabilisers	20			
1.3	Polyme	er-modified Amperometric Biosensors	21			
	1.3.1	Horseradish peroxidase and hydrogen peroxide system	22			
	1.3.2	Fabrication methods	24			
	1.3.	2.1 Electrodeposition	24			
	1.3	2.2 Evaporative casting	25			

	1.3.2	2.3 Ink-jet printing	25
1.4	Structu	re of the Thesis and the Aim of the Chapter	26
1.5	Referer	nces	29
Cha	apter 2	– Instrumental and Characterisation Techniques	
2.1.	Spectro	oscopy	37
	2.1.1.	Ultraviolet-visible (UV-visible) spectroscopy	37
	2.1.2.	Raman spectroscopy	37
2.2	Microso	copic and Light Scattering Methods	39
	2.2.1	Transmission electron microscopy (TEM)	39
	2.2.2	Atomic force microscopy (AFM)	41
	2.2.3	Light scattering	44
2.3	Electro	chemical Techniques	48
	2.3.1	Open circuit potential (OCP)	48
	2.3.2	Cyclic voltammetry (CV)	49
	2.3.3	DC amperometry	51
2.4	Conduc	ctivity Measurement	53
2.5	Contac	t Angle Measurement	54
2.6	Referer	ices	57

# PART II – Synthesis and Characterisation of Conducting Polymer Nanoparticles

#### **Chapter 3 – Synthesis and Characterisation of Polyaniline**

#### Nanoparticles

3.1	Introdu	ıction		60
3.2	Experi	mental		63
	3.2.1	Chemicals		63
	3.2.2	Equipment/in	nstrumentation	63
	3.2.3	Methods		64
	3.2.	3.1 Polyr	nerisation and purification	64
	3.2.	3.2 Chara	acterisation of PANI nanoparticles and dispersions	65
	3.2.	3.3 Stabi	lity test of nanoPANI-DBSA	65
3.3	Results	and Discussion	on	66
	3.3.1	nanoPANI-D	DBSA	66
	3.3.	1.1 Polyr	nerisation	66
		3.3.1.1.1	Open circuit potential (OCP) measurement	67
		3.3.1.1.2	UV-visible spectroscopy during polymerisation	68
		3.3.1.1.3	Particle size measurement during polymerisation	
			by DLS	69
	3.3.	1.2 Chara	acterisation of nanoparticles and dispersions	71
		3.3.1.2.1	Transmission electron microscopy (TEM),	
			mass of product and conductivity	71
		3.3.1.2.2	pH and redox switching	73

		3.3.1.2.3	Raman Spectroscopy	76
		3.3.1.2.4	Cyclic voltammetry (CV)	77
		3.3.1.2.5	Stability test	79
	3.3.	1.3 Furthe	er processing and characterization	82
		3.3.1.3.1	Preparation method for the sPANI/DBSA	83
		3.3.1.3.2	UV-visible spectroscopy	83
		3.3.1.3.3	Cyclic Voltammetry (CV)	83
		3.3.1.3.4	Particle size and morphology	85
	3.3.2	PANI-DBSA	-RM	87
	3.3.2	2.1 Polym	nerisation	87
	3.3.2	2.2 Chara	cterisations of PANI-DBSA-RM nanodispersions	89
		3.3.2.2.1	UV-visible spectroscopy and redox switching	89
		3.3.2.2.2	Raman spectroscopy	91
		3.3.2.2.3	Cyclic Voltammetry (CV)	92
		3.3.2.2.4	Conductivity, particle size and morphology	93
3.4	Conclus	sions		96
3.5	Referen	ices		98
Chi	anter 4 -	– Incornora	tion of Dye into Polyaniline Nanoparticles	
4.1	Introdu	•		100
4.1	Experir			100
4.2	•			
	4.2.1	Chemicals		101
	4.2.2	Equipment/in	strumentation	101
	4.2.3	Methods		102

	4.2.	3.1	Dye purification	102
	4.2.	3.2	Polymerisation and purification	102
	4.2.	3.3	Characterisation of nanoparticles and dispersions	103
4.3	Results	and D	iscussion	104
	4.3.1	Polyn	nerisation	104
	4.3.2	Chara	ecterisations of nanoparticles and dispersions	109
	4.3.	2.1	Transmission electron microscopy (TEM), conductivity	
			and mass of product	109
	4.3.	2.2	pH switching	111
	4.3.	2.3	Redox switching	113
	4.3.	2.4	Raman spectroscopy	116
	4.3.	2.5	Cyclic voltammetry (CV)	120
	4.3.	2.6	Stability test	122
4.4	Conclu	sions		124
4.5	Refere	nces		125
Cha	apter 5	– Synt	thesis and Characterisation of Polypyrrole	
		Nano	oparticles	
5.1	Introdu	uction		127
5.2	Experi	mental		128
	5.2.1	Chem	icals	128
	5.2.2	Equip	oment/instrumentation	128
	5.2.3	Metho	ods	129
	5.2	3 1	Polymerisation and purification	129

	5.2.	3.2	Characterisation of dispersions	130
	5.2.3.3		Stability test of PPy-DS-PVA nanodispersions	130
5.3	Results and Discussion			131
	5.3.1	PPy-l	OS polymerisation	131
	5.3.2	PPy-l	OS Characterisation	132
	5.3.	2.1	UV-visible spectroscopy	132
	5.3.	2.2	Raman spectroscopy	133
	5.3.	2.3	Cyclic voltammetry (CV)	134
	5.3.	2.4	Mass of product, conductivity, particle size	
			and morphology	135
	5.3.3	PPy-l	OS polymerisation in the presence of PVA	136
	5.3.	3.1	Effect of PVA concentration on nanoparticle formation	136
	5.3.	3.2	Effect of polymerisation temperature	
			on nanoparticle formation	138
	5.3.	3.3	Effect of SDS concentration on nanoparticle formation	140
	5.3.	3.4	Effect of monomer concentration	
			on nanoparticle formation	142
	5.3.4	Chara	acterisation of PPy-DS-PVA nanodispersions	144
	5.3.	4.1	UV-visible spectroscopy	144
	5.3.	4.2	Raman spectroscopy	144
	5.3.	4.3	Cyclic voltammetry (CV)	146
	5.3.	4.4	Mass of product, conductivity,	
			particle size and morphology	146

5.4	Conclu	sions		149
5.5	Refere	nces		150
Cha	apter 6	– Synthesis	and Characterisation of	
		Polyterthi	ophene Nanoparticles	
6.1	Introd	uction		152
6.2	Experi	mental		154
	6.2.1	Chemicals		154
	6.2.2	Equipment/in	nstrumentation	155
	6.2.3	Methods		156
	6.2.	3.1 Elect	rochemical synthesis of PTTh-DBSA	156
	6.2.	3.2 Chen	nical synthesis of PTTh-DBSA nanoparticles	156
	6.2.	3.3 Chen	nical synthesis of PTTh nanoparticles in IL	156
	6.2.	3.4 Chara	acterisation of PTTh nanoparticles	157
6.3	Results	and Discussion	on	157
	6.3.1	PTTh-DBSA		157
	6.3.	1.1 Elect	rochemical synthesis of PTTh-DBSA	157
	6.3.	1.2 Chen	nical synthesis of PTTh-DBSA nanoparticles	162
		6.3.1.2.1	Effect of oxidant concentration	162
		6.3.1.2.2	Effect of surfactant concentration	168
		6.3.1.2.3	Electroactivity study	172
		6.3.1.2.4	Colloidal stability	175
		6.3.1.2.5	Size and morphology study by TEM	176
	6.3.2	PTTh nanopa	articles synthesised in IL	176

		6.3.2.1	.1 Effect of oxidant concentration	176
		6.3.2.1	.2 Effect of solvent	179
		6.3.2.1	.3 Electroactivity study	181
		6.3.2.1	.4 Colloidal stability	184
		6.3.2.1	.5 Size and morphology study by TEM	184
6.4	Conclu	sions		185
6.5	Referei	nces		186
PA]	RT III -	– Applic	ations of Conducting Polymer Nanodispersio	ns
Cha	apter 7	– Polyan	niline-Dedecylbenzene Sulphonic acid-	
		Horser	adish Peroxidase Biosensors	
7.1	Introdu	ıction		188
7.2	Experi	mental		189
	7.2.1	Chemica	als	189
	7.2.2	Equipme	ent/instrumentation	190
	7.2.3	Methods	S	190
	7.2.	3.1 P	Preparation of <i>nano</i> PANI-DBSA modified electrodes	190
	7.2.	3.2	Characterisations of the polymer modified electrodes	192
	7.2.	3.3	Colorimetric enzyme assay	192
				400
7.3	Results	and Disc	ussion	193
7.3	<b>Results</b> 7.3.1		ion of nanoPANI-DBSA films	193

Chemical synthesis of PTTh nanoparticles in emiTFSA

6.3.2.1

176

	7.3.2	Characterisations of electrodeposited nanoPANI-DBSA	films 196
	7.3.3	Optimisation of the mass of HRP on the electrode surface	ce 200
	7.3.4	Optimisation of electrodeposition	204
	7.3.5	Colorimetric enzyme assay	205
7.4	Conclu	asions	206
7.5	Referei	nces	207
Cha	apter 8	- Poly(2-methoxyaniline-5-sulphonic acid)-	
		Horseradish Peroxidase-Poly(L-lysine) Biose	nsors
8.1	Introdu	uction	208
8.2	Experi	mental	210
	8.2.1	Chemicals	210
	8.2.2	Equipment/instrumentation	211
	8.2.3	Methods	211
	8.2.	Preparation of polymer modified electrodes	211
	8.2.	.3.2 Characterisation of polymer modified electrodes	212
8.3	Results	s and Discussion	213
	8.3.1	Complexation and fabrication methods	213
	8.3.2	Optimisation of PMAS concentration	215
	8.3.3	Optimisation of PLL concentration	216
	8.3.4	Optimisation of the mass of HRP on the electrode surface	ce 219
	8.3.5	Characterisations of the PMAS-HRP-PLL sensors	221
	8.3.	Sensor response to various applied potentials	
		and huffer nH	221

	8.3.5	5.2	Linearity and sensitivity	223
	8.3.5	5.3	Interferent test	224
	8.3.5	5.4	Long-term stability test	225
8.4	Conclus	sions		226
8.5	Referen	ces		227
Cha	apter 9 -	- Inhe	erently Conducting Polymer Nanodispersion	
		Ink-j	et Printed Biosensors	
9.1	Introdu	ction		228
9.2	Experin	nental		232
	9.2.1	Chem	icals	232
	9.2.2	Subst	rate	233
	9.2.3	Equip	ment/instrumentation	233
	9.2.4	Metho	ods	233
	9.2.4	l.1	Viscosity measurements and pH adjustment	
			of the ICPs nanoparticles	233
	9.2.4	1.2	Printing method for Epson C45 printer	234
	9.2.4	1.3	Film preparation	235
	9.2.4	1.4	Real-time monitoring of enzyme/substrate interactions	
			in a batch cell	235
9.3	Results	and Di	iscussion	235
	9.3.1	Instru	mentation	235
	9.3.2	Substi	rate characterisation	236
	932	) 1	Flectrochemistry	236

PA]	RT IV -	- Conc	clusions and Future Studies	261
9.5	Referei	nces		260
9.4	Conclu	sions		258
	9.3.	4.4	Printing the PANI-DBSA-RM nanodispersions	254
	9.3.	4.3	Printing the sPANI-DBSA	251
	9.3.	4.2	Printing the PMAS and PLL solutions	244
	9.3.	4.1	Printing the PPy-DS-PVA nanodispersions	243
	9.3.4	Ink-je	t printing of ICP nanoparticles	243
	9.3.	3.2	Wetting ability and viscosity	242
	9.3.	3.1	Particle size in concentrated solution	239
	9.3.3	Prope	rties of ICP nanoparticles	239
	9.3.	2.2	Hydrophilicity of substrates	238

#### **ABBREVIATIONS**

μ micro

 $\mu$  viscosity

 $\lambda \qquad \qquad wavelength$ 

*k*<sub>B</sub> Boltzman's constant

γ surface tension

 $\Omega$  Ohm

v frequency

°C degree Celsius

 $\Theta$  angle

η refractive index

σ conductivity

 $\rho$  resistivity

υ scan rate

A ampere

Å angstrom

A anion

 $A_{\rm i}$  acivity of species i

ABTS 2,2'-azino-bis(3-ethylbenzthiazoline-6-sulphonic acid)

AFM atomic force microscopy

Ag/AgCl silver/silver chloride reference electrode

Ag/Ag<sup>+</sup> silver/silver ion reference electrode

APS ammonium peroxydisulphate

BSA bovine serum albumin

BFEE boron-fluoride ethyl ether

C Cunningham slip correction factor

ca. approximately

CB Carbolan Blue

CCD charge-coupled device

cm centrimeter

cm<sup>-1</sup> wave number

CMC critical micelle concentration

CV cyclic voltammetry

d diameter

Da dalton

D<sub>AB</sub> diffusion coefficient

DBSA dodecylbenzene sulphonic acid

DLS dynamic light scattering

E potential

E<sup>0</sup> standard reduction potential

EB emeraldine base

emiTFSA 1-ethyl-3-methylimidazolium-

bis(trifluoromethane-sulfonyl)amide

ES emeraldine salt

F Faraday constant

g gram

GC glassy carbon

HCSA camphorsulphonic acid

HPLC high performance liquid chromatography

HRP horseradish peroxidase

h hour

ICP inherently conducting polymer

IL ionic liquid

ITO indium tin oxide

k thousand

L litre

LB leucoemeraldine base

m metre

M molar

MAS 2-methoxyaniline-5-sulphonic acid

mg milligram

min minute

ml millilitre

mM millimolar

MoAb monoclonal antibody

mS millisiemen

Mw molecular weight

nm nanometre

OCP open circuit potential

PANI polyaniline

PB perniganiline base

PBS phosphate buffer saline

PEI poly(ethyleneimine)

PLL poly(L-lysine)

PMAS poly(2-methoxyaniline-5-sulphonic acid)

PPy polypyrrole

PS perniganiline salt

PSS poly(sodium 4-styrene sulfonate)

Pt platinum

PTh polythiophene

PTTh polyterthiophene

PVA poly(vinyl alcohol)

PVP poly(4-vinylpyridine)

PVS polyvinylsulphonate

Py pyrrole

r radius

RM rapid mixing

RMS root mean square

rpm round per minute

S siemen

SCE saturated calomel electrode

SDS sodium dodecylsulfate

SEM scanning electron microscopy

SHE standard hydrogen electrode

SPM scanning probe microscopy

T temperature

TBAP tetrabutylammonium perchlorate

TEM transmission electron microscopy

Th thiophene

TTh terthiophene

V volt

vs. versus

w/v weight by volume

w/w weight by weight

#### **ABSTRACT**

Synthesis of inherently conducting polymers (ICPs) nanoparticles is an option to improve the processability and conductivity of ICPs. In this thesis, the synthesis and application of ICPs nanoparticles has been demonstrated. Various polymerisation methods, such as emulsion polymerisation, use of steric stabiliser and synthesis in ionic liquid (IL) media, have been used to synthesise polymer nanoparticles. These synthesis methods render the ICPs nanoparticles stable as dispersions which are more processable and contain peculiar and fascinating properties superior to their bulk counterparts. These nanoparticles are further applied as mediators for biosensors. They have been fabricated into sensors using electrodeposition, evaporative casting, or ink-jet printing methods. Electrodeposition method results in formation of ultra thin nanostructured polymeric films that enhance sensor performance. Evaporative casting method is an easy one-step method, but precision is hard to achieve and dense films with rough morphology are formed. Ink-jet printing can be used to produce precise and accurate patterns and also this approach is amenable to mass production.

Polyaniline (PANI) nanoparticles; *nano*PANI-dodecylbenzene sulphonic acid (DBSA) have been synthesised using emulsion polymerisation (Chapter 3). The *nano*PANI-DBSA obtained has a conductivity of 34±7 S/cm with particle size in the range of 10±2 nm. The *nano*PANI-DBSA has been used as a mediator layer in biosensor applications as demonstrated in Chapter 7. These nanoparticles were fabricated onto the conductive electrode using an electrodeposition method with subsequent immobilisation of the enzyme horseradish peroxidase (HRP). Sensor performance was examined using

amperometric method and HRP/hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) configuration as a model system. The nanodomain of the *nano*PANI-DBSA particles contributed to highly ordered nanostructure patterning on the electrode surface. This uniform surface showed improved enzyme deposition characteristics, a lower background signal and better sensor performance at a lower HRP loading when compared to the sensors fabricated from electropolymerisation of the bulk monomer.

NanoPANI-DBSA particles aggregate at high concentrations; hence they are not amenable to ink-jet printing. sPANI-DBSA was prepared from centrifugation of the nanoPANI-DBSA dispersions and used as a material for ink-jet printing. HRP was premixed with the sPANI-DBSA nanodispersions before fabrication onto ITO-coated mylar using ink-jet printing. The print quality from the sPANI-DBSA nanodispersions was inconsistent and the catalytic signal of this biosensor was very low. These resulted in no further ink-jet printing work for this material.

The PANI-DBSA-rapid mixing (RM) nanodispersions were synthesised using a RM method. These dispersions contained nanometre size PANI particles dispersed in aqueous media. These nanoparticles have been successfully printed using ink-jet printing as outline in Chapter 9. This work has demonstrated the ink-jet printability of conducting polymer nanoparticles and their use as working electrodes for biosensors. The sensor response from these ink-jet printed PANI-DBSA-RM was higher than the sensor response from evaporative casting of poly(2-methoxyaniline-5-sulphonic acid) (PMAS) in Chapter 8.

The addition of functional group into PANI nanoparticles was also investigated. Carbolan Blue (CB) dye was incorporated into the PANI backbone using emulsion polymerisation method as demonstrated in Chapter 4. The dye was proved to have strong interaction with PANI backbone using Raman spectroscopy and centrifugation test. The

distinct solution colour after a reduction process could lead the PANI-DBSA-CB to be a potential candidate of the material for electrochromic devices.

Synthesis of polypyrrole (PPy) nanoparticles is demonstrated in Chapter 5. Poly(vinyl alcohol) (PVA) was used as the steric stabiliser to produce PPy-DS-PVA nanoparticles. These nanoparticles were well dispersed in water with particle size in the order of 52±5 nm. Aggregation was obvious in concentrated solutions and leaded to poor ink-jet printed quality of the PPy-DS-PVA nanoparticles.

The water soluble polymer, PMAS, was also used to fabricate biosensors using evaporative casting method in Chapter 8 and ink-jet printing in Chapter 9. In chapter 8, its solubility enabled PMAS to pre-mix with the HRP enzyme prior to complexing with the polycations poly(L-lysine) hydrochloride (PLL) and subsequently casting onto ITO coated mylar substrate. This biosensor format has proven ability to easily fabricate the conducting polymer nanoparticles by one-step evaporative casting. The optimised sensors exhibited good sensor response, high selectivity and very good long-term stability. The ink-jet printed films from PMAS and PLL solutions (Chapter 9) showed better electroactivity compared to the evaporative cast films which could lead to better sensor performance. However, the problem of PLL blocking the print head resulted in the discontinuation of its use.

The polyterthiophene (PTTh) aqueous dispersed nanoparticles were also successfully synthesised in the presence of surfactant (DBSA) and in ionic liquid; 1-ethyl-3-methylimidazolium bis(trifluoromethane-sulfonyl)amide (emiTFSA) as demonstrated in Chapter 6. The dispersion of PTTh-DBSA nanoparticles has shown poor colloidal stability and poor electroactivity. Although the PTTh nanoparticles synthesised in emiTFSA needed

2-3 minutes sonication to be dispersed in water, they have shown good electrochemistry and being test in another study in our laboratories for its use in photovoltaic devices.

These processable ICPs nanoparticles are promising materials for biosensor applications, electrochromic devices and solar cells. Assembly of these nanoparticles on to conductive substrates leads to highly ordered nanostructured ICPs on the surface and improves the biosensor performances. Also these nanoparticles prove their ability to be processable in mass production scale.