

2007

Knee function and neuromuscular adaptations following ACL rupture and reconstruction

Adam L. Bryant
University of Wollongong

Follow this and additional works at: <https://ro.uow.edu.au/theses>

University of Wollongong

Copyright Warning

You may print or download ONE copy of this document for the purpose of your own research or study. The University does not authorise you to copy, communicate or otherwise make available electronically to any other person any copyright material contained on this site.

You are reminded of the following: This work is copyright. Apart from any use permitted under the Copyright Act 1968, no part of this work may be reproduced by any process, nor may any other exclusive right be exercised, without the permission of the author. Copyright owners are entitled to take legal action against persons who infringe their copyright. A reproduction of material that is protected by copyright may be a copyright infringement. A court may impose penalties and award damages in relation to offences and infringements relating to copyright material.

Higher penalties may apply, and higher damages may be awarded, for offences and infringements involving the conversion of material into digital or electronic form.

Unless otherwise indicated, the views expressed in this thesis are those of the author and do not necessarily represent the views of the University of Wollongong.

Recommended Citation

Bryant, Adam L, Knee function and neuromuscular adaptations following ACL rupture and reconstruction, PhD thesis, School of Health Sciences, University of Wollongong, 2007. <http://ro.uow.edu.au/theses/641>

Research Online is the open access institutional repository for the University of Wollongong. For further information contact the UOW Library: research-pubs@uow.edu.au

NOTE

This online version of the thesis may have different page formatting and pagination from the paper copy held in the University of Wollongong Library.

UNIVERSITY OF WOLLONGONG

COPYRIGHT WARNING

You may print or download ONE copy of this document for the purpose of your own research or study. The University does not authorise you to copy, communicate or otherwise make available electronically to any other person any copyright material contained on this site. You are reminded of the following:

Copyright owners are entitled to take legal action against persons who infringe their copyright. A reproduction of material that is protected by copyright may be a copyright infringement. A court may impose penalties and award damages in relation to offences and infringements relating to copyright material. Higher penalties may apply, and higher damages may be awarded, for offences and infringements involving the conversion of material into digital or electronic form.

**KNEE FUNCTION AND NEUROMUSCULAR
ADAPTATIONS FOLLOWING ACL RUPTURE AND
RECONSTRUCTION**

**A thesis submitted in fulfilment of the
requirements for the award for the degree**

Doctor of Philosophy

from

University of Wollongong

by

Adam L. Bryant

BHMS (Hons) University of New England, Northern Rivers

School of Health Sciences

2007

CERTIFICATION

I, Adam L. Bryant, declare that this thesis, submitted in fulfilment of the requirements for the award of Doctor of Philosophy, in the School of Health Sciences, University of Wollongong, is wholly my own work unless otherwise referenced or acknowledged. The document has not been submitted for qualifications at any other academic institution.

Adam L. Bryant

April 2007

DEDICATION

FOR

NATHAN

MY BROTHER & FRIEND...MY INSPIRATION

*“He who dwells in the shelter of the Most High
will rest in the shadow of the Almighty”*

(Psalm 91:1)

ACKNOWLEDGEMENTS

Sincere thanks to the following people without whose assistance; this thesis would not have been possible:

- Professors Julie Steele and Robert Newton for extending their knowledge and expertise in the formulation and refinement of this body of work. Special thanks to Julie who challenged me to bring this thesis to a higher level.
- Associate Professor Peter Reaburn, Head of School of Health and Human Performance (Central Queensland University) for his encouragement and study leave allowances which ensured that this thesis was completed.
- Professor Joan McMeekin, Professor Kim Bennell and Associate Professor Gillian Webb from the School of Physiotherapy (The University of Melbourne) who were extraordinarily generous and supportive in the late stages of the final thesis.
- my friend and colleague; Associate Professor Erik Hohmann who believed in me and has provided amazing research opportunities.
- orthopaedist Dr Ray Randle who encouraged his ACLD and ACLR patients to participate in this research.
- the numerous ACLD, ACLR and control subjects who gave up their time to participate in this study.
- Dr Lyndon Brooks for his assistance with statistical design.
- Dr Karen Gallie for her invaluable editorial advice.
- Dr Glenn Fuller whose skill, care and compassion have allowed me brighter days.
- to my friends who encouraged and supported me throughout the duration of this thesis.
- to my parents; Ross and Elizabeth, my brother and sister; Sean and Sarah and, more recently, my little niece; Hope. This has been a long and drawn-out process and I thank you for your unwavering support and love.
- Above all, I express my deepest gratitude to God; His love and faithfulness never cease to amaze me.

PUBLICATIONS

The following publications in conference proceedings have arisen directly from the work conducted for this thesis.

Bryant, A.L., Newton, R.U., Bronks, R., & Randle, R. (2000). *Isokinetic torque generated by the quadriceps muscles at increasing knee joint angles following anterior cruciate ligament reconstruction: A comparison between patella and hamstring tendon grafts*. Paper presented at the International Congress on Sport Science and Sports Medicine and Physical Education (Pre-Olympic Congress) Brisbane, Australia.

Bryant, A.L., Newton, R.U., Bronks, R., & Randle, R. (2000). *Antagonist activity of the hamstring musculature during knee extension with anterior cruciate ligament deficiency*. Paper presented at the International Congress on Sport Science and Sports Medicine and Physical Education (Pre-Olympic Congress) Brisbane, Australia.

Bryant, A.L., Newton, R.U., Bronks, R., & Randle, R. (2002). *The effects of chronic anterior cruciate ligament deficiency on ground reaction forces, tibial acceleration and length changes of the hamstring muscles during landing and deceleration from a single-legged long hop*. Paper presented at the Australian Conference of Science and Medicine in Sport Melbourne, Australia.

Bryant, A.L., Newton, R.U., Bronks, R., & Randle, R. (2002). *Isokinetic torque generated by the hamstring muscles at increasing knee joint flexion angles following anterior cruciate ligament rupture and reconstruction using either the patella or hamstring tendon grafts*. Paper presented at the Australian Conference of Science and Medicine in Sport Melbourne, Australia.

Bryant, A.L., Newton, R.U., Bronks, R., & Randle, R. (2002). *Activation of the quadriceps and hamstrings during isokinetic knee extension with ACL deficiency and following ACL reconstruction using either the patella or hamstring tendon grafts*. Paper presented at the Australian Conference of Science and Medicine in Sport Melbourne, Australia.

Bryant, A.L., Newton, R.U., & Steele, J.R. (2003). *Knee pain, swelling and giving way: Are these symptoms influenced by ACL reconstruction?* Paper presented at the Australian Conference of Science and Medicine in Sport Canberra, Australia.

Bryant, A.L., Newton, R.U., & Steele, J.R. (2003). *Is tibial acceleration related to knee functionality of ACL deficient and ACL reconstructed patients?* Paper presented at the Australian Conference of Science and Medicine in Sport Canberra, Australia (**British Journal of Sports Medicine Award: Best Clinical Sports Medicine Paper**).

- Bryant, A.L.,** Newton, R.U., Hohmann, E., & Steele, J.R. (2005). *Can we predict knee functionality of ACL deficient and ACL reconstructed patients using tibial acceleration profiles?* Paper presented at the 1st World Congress on Sports Injury Prevention, Oslo, Norway.
- Bryant, A.L.,** Newton, R.U., & Steele, J.R. (2005). *What is the association between knee functionality and hamstring antagonist activation in ACL deficient and ACL reconstructed patients?* Paper presented at the Australian Conference of Science and Medicine in Sport Melbourne, VIC, Australia.
- Bryant, A.L.,** Newton, R.U., Hohmann, E., & Steele, J.R. (2006). *Can we predict the knee function of ACL deficient and ACL reconstructed patients using acceleration transients derived from the proximal tibia?* Paper presented at the British Orthopaedic Association Annual Congress, Glasgow, Ireland.
- Bryant, A.L.,** Newton, R.U., Hohmann, E., & Steele, J.R. (2006). *The relationship between hamstring antagonist activation and knee function in ACL deficient and ACL reconstructed patients.* Paper presented at the British Orthopaedic Association Annual Congress, Glasgow, Ireland.

ABSTRACT

In order to alleviate symptoms associated with progressive knee dysfunction and deterioration following anterior cruciate ligament (ACL) injury, patients undergo either conservative non-operative rehabilitative regimens or early reconstructive surgery using the patella tendon (PT) or combined semitendinosus and gracilis tendon (STGT) grafts. Following treatment, ACL deficient (ACLD) and ACL reconstructed (ACLR) patients demonstrate varying levels of knee function with compensatory neuromuscular adaptations thought to be responsible for enhancing the dynamic restraint capabilities in more functional patients. Derivation of the neuromuscular factors that estimate participation restrictions could assist clinicians in developing prognoses and outcome measures for ACLD and ACLR patients. Therefore, the main aim of the present thesis was to identify neuromuscular variables, derived during open and closed kinetic chain tasks, that relate to and predict post ACL injury/ACLR functional outcome.

To achieve this, 10 male ACLD subjects together with 27 matched-males who had undergone ACLR (14 PT graft and 13 STGT graft) and 22 matched-control subjects were recruited. In Experiment 1, the Cincinnati Knee Rating System was used to assess knee symptoms and limitations associated with activities of daily living and sports. Three single-leg tests designed to replicate athletic activities were also implemented. Subjective and objective scores were combined to provide an overall knee function score for each subject. The ACLD group was significantly more symptomatic and limited in activities of daily living and sports and they also demonstrated impaired jump and hop performance. Whilst the PT and STGT subjects rated significantly higher than their ACLD counterparts, their average subjective and overall knee function scores were significantly lower compared to the control group. Importantly, graft selection did not significantly influence average subjective, objective or overall knee function scores.

In Experiment 2, the effect of ACL injury and ACLR on open kinetic chain isokinetic strength of the quadriceps and hamstrings was assessed in 10° intervals through their operational domain. Antagonist activity of the semitendinosus (ST) and biceps femoris (BF) muscles was also determined during knee extension in 10° intervals between 80 and 10° flexion. Conservatively managed subjects demonstrated significant quadriceps and hamstring weakness with involved limb quadriceps strength deficits transferred to the contralateral limb. Harvesting the central one-third of the PT as an

ACL substitute did not inhibit quadriceps strength compared those ACL-insufficient knees in which the extensor mechanism was not used in the reconstruction technique (STGT graft). In contrast, harvesting the flexor mechanism for ACLR caused significant hamstring strength deficits that were not apparent in patients having undergone ACLR using the PT graft. Relatively large amounts of hamstring antagonist activity were evident during knee extension, although ST and BF electromyographic discharge was not influenced by ACL status. Hamstring antagonist activity increased and decreased widely as a function of joint angle with the BF significantly more active than the ST in order to control internal tibial rotation. Kinesthetic joint capsule receptors were thought to be the major source dictating hamstring muscle activity in such a manner that it varied nearly inversely relative to its moment arm.

In Experiment 3, lower limb kinematics, kinetics and neuromuscular responses were assessed in ACLD and ACLR subjects during a closed kinetic chain task known to stress the ACL, namely abrupt deceleration when landing from a single-leg hop for distance. For the ACLD group, no significant alterations were evident in joint kinematic parameters. Biceps femoris of the involved limb of the ACLD group was activated significantly later compared to the non-involved limb, supporting the notion that after ACL injury, sensory feedback may be used to build a new internal model depicting the expected conditions during functional activities. The involved limb of the ACLD and ACLR groups demonstrated a significant reduction in vertical ground reaction force during the support phase of landing compared to the non-involved limb. Whilst the magnitude of peak tibial acceleration was not significantly different between test limbs or subject groups, it took significantly longer for the involved limb of the ACLD and ACLR groups to attain constant tibial motion compared to the non-involved limb. Subjects having undergone ACLR using the PT graft demonstrated a stiff knee strategy during landing and, whilst the STGT group also demonstrated trends towards decreased knee flexion during landing, no significant kinematic adaptations at the hip, knee or ankle were identified. Decreased knee flexion was found to significantly attenuate the mechanical advantage of the involved limb hamstrings of the ACLD, PT and STGT groups. Cumulative changes in involved limb hip and knee kinematics of the ACLD and ACLR subjects meant that the ST and BF muscles were significantly elongated when decelerating to improve dynamic restraint. Importantly, ACLR led to a restoration of normal quadriceps and hamstring electromyographic (EMG) synchrony in

the involved and contralateral limbs and there was no evidence to suggest that the ACLD subjects adopted a pattern of quadriceps-avoidance.

In Experiment 4, the strength of the associations among knee functionality of ACLD and ACLR subjects (Experiment 1) and neuromuscular variables derived from open (Experiment 2) and closed (Experiment 3) kinetic chain movements was determined. Numerous significant moderate to strong correlations were identified with determinants of knee functionality related to the type of ACL treatment and graft selection. Compensatory neuromuscular strategies that enhance function in the ACLD knee included amplified hamstring co-activation, increased hamstring preparatory activity and a greater ability to control tibial motion during dynamic deceleration. Following ACL replacement, the degree of residual strength deficit in the muscle from which the tendon graft was harvested (i.e. quadriceps or hamstrings) become an important prognosticator of knee functionality as did attenuated hamstring co-activation during knee extension within the range utilised during single-limb deceleration. More functional PT subjects demonstrated enhanced tibial control whilst superior knee functionality in STGT subjects was associated with increased preparatory activity of the quadriceps when landing on the involved limb. Furthermore, by synchronising peak hamstring muscle activity at the time when the ACL graft is most vulnerable to injury, more functional STGT subjects enhanced dynamic restraint by increasing joint compression and posterior tibial drawer. By identifying neuromuscular factors that predict function in ACLD and ACLR subjects, the results of these studies will lead to the development of more specific and effective treatment strategies.

TABLE OF CONTENTS

	Page
Certification	i
Dedication	ii
Acknowledgements	iii
Publications	iv
Abstract	vi
Table of Contents	ix
List of Tables	xiii
List of Figures	xviii
List of Abbreviations	xxiv
Chapter 1: The Problem	
1.1 Introduction	1
1.2 Statement of the Problem	6
1.3 Significance of the Study	7
Chapter 2: Review of the Literature	
2.1 Introduction	9
2.2 Treatment for the Ruptured ACL	9
2.2.1 Conservative Treatment	10
2.2.2 Surgical Treatment	11
2.2.3 ACL Graft Biomechanics and Healing	13
2.2.4 Rehabilitation Following ACLR	15
2.3 Assessment of ACLD and ACLR Patients	16
2.3.1 Subjective Assessment of Knee Functionality	16
2.3.2 Objective Assessment of Knee Functionality	20
2.3.3 Overall Knee Rating	23
2.4 The Quadriceps and ACLD/ACLR Knees	25
2.4.1 Biomechanics of Quadriceps Contraction	25
2.4.2 Quadriceps Muscle Strength Following ACL Rupture and ACLR	29
2.5 The Hamstrings and ACLD/ACLR Knees	36
2.5.1 Biomechanics of Hamstring Contraction	36
2.5.2 The ACL-Hamstring Reflex Arc	42
2.5.3 Secondary Reflex Arcs	45
2.5.4 Hamstring Muscle Strength Following ACL Rupture and ACLR	46
2.6 Cross Education of Muscle Strength	51

	Page
2.7	Compensatory Adaptations During Locomotor Tasks Following ACL Injury/ACLR..... 53
2.7.1	ACLD Involved Limb versus Non-Involved and Matched Control Limbs 54
2.7.2	ACLR Involved Limb versus Non-Involved and Matched Control Limbs 58
2.7.3	Responses of ACLD versus ACLR Patients 61
2.7.4	Responses of ACLR Patients with PT Graft versus STGT Graft Patients..... 63
2.7.5	Rationales for Adaptations Displayed by ACLR Patients..... 63
2.7.6	Rationales for Adaptations Displayed by ACLR Patients with PT Graft versus STGT Graft Patients..... 65
2.8	Tibial Acceleration, Muscle Kinematics and the ACLD/ACLR Knee..... 66
2.8.1	Tibial Acceleration During Locomotor Tasks 67
2.8.2	Muscle Kinematics During Locomotor Tasks 68
2.9	Relationships Between Knee Functionality and Variables Derived From Open and Closed Kinetic Chain Assessment 71
2.10	Summary 77
Chapter 3:	Experiment 1: Subjective and Objective Limitations in ACLD and ACLR Patients
3.1	Introduction 79
3.2	Statement of the Problem 80
3.3	Hypotheses 80
3.4	Limitations and Delimitations..... 81
3.4.1	Limitations 81
3.4.2	Delimitations 81
3.5	Methods..... 81
3.5.1	Subjects 81
3.5.2	Experimental Protocol..... 84
3.5.3	Data Analysis 86
3.5.4	Statistical Analyses 87
3.6	Results and Discussion..... 89
3.6.1	Physical Characteristics of the Subjects..... 89
3.6.2	Limb Dominance and Injury 90
3.6.3	Subjective Assessment Scores 91
3.6.4	Objective Assessment Tests 100
3.6.5	Component Averages and Overall Knee Rating Scores..... 110
3.7	Summary 113
3.8	Conclusions 114

	Page
Chapter 4: Experiment 2: Neuromuscular Responses in ACLD and ACLR Patients During an Open Kinetic Chain Movement	
4.1	Introduction 116
4.2	Statement of the Problem 118
4.3	Hypotheses 119
4.4	Limitations and Delimitations 120
	4.4.1 Limitations 120
	4.4.2 Delimitations 120
4.5	Methods 121
	4.5.1 Subjects 121
	4.5.2 Experimental Protocol 121
	4.5.3 Data Analysis 124
	4.5.4 Statistical Analyses 127
4.6	Results and Discussion 130
	4.6.1 Quadriceps and Hamstring Moment Arm Lengths 130
	4.6.2 Isokinetic Knee Extension Torque 134
	4.6.3 Isokinetic Knee Flexion Torque 149
	4.6.4 Hamstring Antagonist Muscle Activation 161
4.7	Summary 172
4.8	Conclusions 174
Chapter 5: Experiment 3: Kinematic, Kinetic and Neuromuscular Responses in ACLD and ACLR Patients During a Closed Kinetic Chain Movement	
5.1	Introduction 176
5.2	Statement of the Problem 177
5.3	Hypotheses 178
5.4	Limitations and Delimitations 179
	5.4.1 Limitations 179
	5.4.2 Delimitations 179
5.5	Methods 180
	5.5.1 Subjects 180
	5.5.2 Experimental Protocol 180
	5.5.3 Data Analyses 184
	5.5.4 Statistical Analyses 190
5.6	Results and Discussion 191
	5.6.1 Ground Reaction Forces 191
	5.6.2 Tibial Acceleration 203
	5.6.3 Joint Kinematics 208
	5.6.4 Hamstring Moment Arm Length 222
	5.6.5 Hamstring Musculotendinous Length 226
	5.6.6 Muscle Activity 234
5.7	Summary 245
5.8	Conclusions 248

	Page
Chapter 6: Experiment 4: Relationships Between Knee Functionality of ACLD and ACLR Patients and Variables Derived from Open and Closed Kinetic Chain Assessment	
6.1 Introduction	249
6.2 Statement of the Problem	250
6.3 Hypotheses	250
6.4 Limitations and Delimitations.....	251
6.4.1 Limitations	251
6.4.2 Delimitations	251
6.5 Methods.....	252
6.5.1 Subjects	252
6.5.2 Experimental Protocol.....	252
6.5.3 Data Analyses.....	252
6.5.4 Statistical Analyses	252
6.6 Results and Discussion.....	253
6.6.1 Relationships Between Knee Functionality and Variables Derived from Open Kinetic Chain Assessment	253
6.6.2 Relationships Between Knee Functionality and Variables Derived from Closed Kinetic Chain Assessment.....	262
6.7 Summary	269
6.8 Conclusions	272
Chapter 7: Summary, Conclusions and Recommendations	
7.1 Summary of the Results	273
7.1.1 Subjective and Objective Limitations	273
7.1.2 Neuromuscular Responses in an Open Kinetic Chain Movement.....	275
7.1.3 Kinematic, Kinetic and Neuromuscular Responses in a Closed Kinetic Chain Movement	279
7.1.4 Relationships Between Knee Functionality and Variables Derived From Open and Closed Kinetic Chain Tasks	282
7.2 Conclusions	285
7.3 Recommendations for Further Research.....	285
References	289
Appendix I: Human Ethics Approval	329
Appendix II: Cincinnati Knee Rating System	330
Appendix III: Technical Note: Determining sampling rates and filter cut-off frequency for a kinematic analysis of one-leg jumping	333

LIST OF TABLES

Table	Page
2.1	Knee extension strength data collected for chronic ACLD subjects (a) and ACLR subjects having undergone ACLR using either the PT (b) or STGT graft (c) 31
2.2	Knee flexion strength data collected for chronic ACLD subjects (a) and ACLR subjects having undergone ACLR using either the PT (b) or STGT graft (c) 48
2.3	Major adaptations identified for ACLD patients when the non-involved limb is compared with the involved limb and matched control subjects 55
2.4	Relationships between measures of knee functionality and quadriceps and hamstrings isokinetic torque parameters for ACLD subject groups 72
2.5	Relationships between measures of knee functionality and quadriceps and hamstrings isokinetic torque parameters for ACLR subject groups 73
3.1	Selection criteria for the ACLD, PT, STGT and control subjects 83
3.2	Mean (\pm standard deviation) of the age, height, mass and time since injury/surgery for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects, together with F-ratios and alpha levels derived for each source of variance 90
3.3	Mean (\pm standard deviation) of the ratings (0-10) for pain, swelling, full giving way and partial giving way for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects, together with F-ratios and alpha levels derived for each source of variance 92
3.4	Mean (\pm standard deviation) of the ratings (0-40) for walking, stairs and squatting/kneeling (activities of daily living) for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects, together with F-ratios and alpha levels derived for each source of variance 96
3.5	Mean (\pm standard deviation) of the ratings (0-100) of sports function for straight running, jumping/landing and hard twists/cuts/pivots for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects together with F-ratios and alpha levels derived for each source of variance 98
3.6	Mean (\pm standard deviation) single-leg performance scores for the vertical jump (VJ), long hop (LH) and timed hop (TH) for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) and control subjects (n = 22) (dominant and non-dominant limbs and the “standard” data), together with F-ratios and alpha levels derived for each source of variance 101

Table	Page
3.7	Mean (\pm standard deviation) vertical jump, long hop and timed hop symmetry indexes for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects, together with F-ratios and alpha levels derived for each source of variance 108
3.8	Subjective (0-20), activity (0-15), functional tests (0-10) and overall scores (0-100) for the Cincinnati Knee Rating System for the ACLD (n = 10), PT (n = 14), STGT (n = 13) and control (n = 22) subjects, together with F-ratios and alpha levels derived for each source of variance 111
4.1	Isokinetic knee extension torque (N•m) at knee angular position intervals Ext45, Ext35, Ext25 and Ext15 at $180^{\circ}\cdot s^{-1}$ for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 135
4.2	F-ratios and alpha levels derived for each source of variance for extension torque 136
4.3	Isokinetic knee flexion torque (N•m) at knee angular position intervals Flex45, Flex55, Flex65 and Flex75 at $180^{\circ}\cdot s^{-1}$ for the non-involved and involved limbs of the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 150
4.4	F-ratios and alpha levels derived for each source of variance for flexion torque 151
4.5	Antagonist muscle activation (%) of the ST during isokinetic knee extension at $180^{\circ}\cdot s^{-1}$ for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 162
4.6	Antagonist muscle activation (%) of the BF during isokinetic knee extension at $180^{\circ}\cdot s^{-1}$ for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with dominant and non-dominant limbs and the “average limb” data for the control group (n = 22)..... 163
4.7	F-ratios and alpha levels derived for each source of variance for antagonist activation of the ST muscle 164
4.8	F-ratios and alpha levels derived for each source of variance for antagonist activation of the BF muscle 164
4.9	F-ratios and alpha levels derived for each source of variance for antagonist activation of the ST and BF muscles 170
5.1	Magnitude and timing of vertical GRF (F_{v1} and F_{v2}) relative to IC generated during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22)..... 192

Table	Page
5.2	F-ratios and alpha levels derived for each source of variance for the magnitude and timing of F_{v1} and F_{v2} relative to IC..... 193
5.3	Magnitude and timing of braking GRF (F_{Br}) relative to IC during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 200
5.4	F-ratios and alpha levels derived for each source of variance for the magnitude and timing of F_{Br} relative to IC..... 201
5.5	Magnitude and timing of TA_p relative to IC and timing of TA_0 relative to IC during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 204
5.6	F-ratios and alpha levels derived for each source of variance for the magnitude of TA_p and timing of TA_p and TA_0 relative to IC.... 205
5.7	Hip flexion angles ($^{\circ}$) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 209
5.8	F-ratios and alpha levels derived for each source of variance for hip flexion 210
5.9	Knee flexion angles ($^{\circ}$) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 214
5.10	F-ratios and alpha levels derived for each source of variance for knee flexion..... 215
5.11	Ankle flexion angles ($^{\circ}$) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 221
5.12	F-ratios and alpha levels derived for each source of variance for ankle flexion..... 222

Table	Page
5.13	Hamstring moment arm length at the knee (mm) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 223
5.14	F-ratios and alpha levels derived for each source of variance for hamstring moment arm length..... 224
5.15	ST muscle length (mm) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 227
5.16	F-ratios and alpha levels derived for each source of variance for ST muscle length 228
5.17	BF muscle length (mm) at selected kinetic and acceleration events during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 231
5.18	F-ratios and alpha levels derived for each source of variance for BF muscle length 232
5.19	Timing of quadriceps muscle burst onset relative to IC and normalised to the time from IC to TA _p during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 235
5.20	Timing of peak quadriceps muscle activity relative to IC and normalised to the time from IC to TA _p during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 236
5.21	F-ratios and alpha levels derived for each source of variance for the timing of quadriceps muscle burst onset relative to IC and normalised to the time from IC to TA _p 237
5.22	F-ratios and alpha levels derived for each source of variance for the timing of peak quadriceps muscle activity relative to IC and normalised to the time from IC to TA _p 237
5.23	Timing of hamstring muscle burst onset relative to IC and normalised to the time from IC to TA _p during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22) 239

Table	Page
5.24	Timing of peak hamstring muscle activity relative to IC and normalised to the time from IC to TA _p during landing from a single-leg long hop for the non-involved and involved limbs for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups together with the dominant and non-dominant limbs and the “average limb” data for the control group (n = 22)..... 240
5.25	F-ratios and alpha levels derived for each source of variance for the timing of hamstring muscle burst onset relative to IC and normalised to the time from IC to TA _p 241
5.26	F-ratios and alpha levels derived for each source of variance for the timing of peak hamstring muscle activity relative to IC and normalised to the time from IC to TA _p 241
6.1	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and isokinetic knee extension and flexion torque values generated at 180•s ⁻¹ for the involved limb relative to the non-involved limbs for the ACLD (n=10), PT (n=14) and STGT (n=13) groups..... 254
6.2	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and ST antagonist activity generated during knee extension at 180•s ⁻¹ for the involved limb of the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups..... 258
6.3	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and BF antagonist activity generated during knee extension at 180•s ⁻¹ for the involved limb of the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups..... 259
6.4	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and timing of muscle onset (quadriceps and hamstrings) during involved limb landing for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups 263
6.5	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and peak muscle activity (quadriceps and hamstrings) during involved limb landing for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups 264
6.6	Correlation coefficients between overall knee rating scores derived from the Cincinnati Knee Rating System (1995) and magnitude and timing of tibial acceleration during involved limb landing for the ACLD (n = 10), PT (n = 14) and STGT (n = 13) groups 268

LIST OF FIGURES

Figure		Page
2.1	Intra-articular ACLR using the PT graft (Laxdal <i>et al.</i> , 2005, p. 35)	12
2.2	Intra-articular ACLR using the combined STGT graft (Laxdal <i>et al.</i> , 2005, p. 36).....	13
2.3	Maximum isometric knee-extensor torque-angle curves for the model (thick solid line) and for human subjects (shaded region). The thin solid line is the mean of all the experimental measurements. The shaded region represents ± 1 standard deviation of the total extensor torques measured for the subjects during maximum, voluntary, isometric contractions of the quadriceps (Shelburne & Pandy, 1997, p. 171)	28
2.4	Definition of patella tendon tibial shaft angle (α), knee flexion angle (θ), and the anterior shear force vector ($F_{Q,x}$). F_Q is the total quadriceps muscle force applied to the patella tendon (DeMorat <i>et al.</i> , 2004, p. 478).....	29
2.5	Maximum isometric knee-flexor torque-angle curves for the model (thick solid line) and for human subjects (shaded region). The thin solid line is the mean of all the experimental measurements. The shaded region represents ± 1 standard deviation of the total flexor torques measured for the subjects during maximum, voluntary, isometric contractions of the hamstrings and gastrocnemius muscles (Shelburne & Pandy, 1997, p. 172).....	38
2.6	(A) Relationship between cruciate-ligament forces, hamstrings activation and knee-flexion angle during simultaneous contractions of the extensor and flexor muscles. At each knee-flexion angle, the quadriceps are fully activated and the activation of gastrocnemius and each hamstrings muscle is varied from 0 to 100%. (B) Relationship between hamstrings co-contraction force and the resultant ACL force at various knee-flexion angles during simultaneous contractions of the extensor and flexor muscles. The resultant ACL force is plotted only against hamstrings force since activation of gastrocnemius has a negligible effect on ACL force in the model (Pandy & Shelburne, 1997, p. 1020)	39
2.7	Anterior tibial translation versus flexion angle for the intact, ACLD (sectioned), and ACLR knee. (A) shows the results with no hamstrings activation, and (B) is with 90 N hamstrings load (More <i>et al.</i> , 1993, p. 235)	40

Figure	Page
2.8	Muscle inhibition of the knee extensors in unilateral knee patients (n = 88) with anterior knee pain (AP), anterior cruciate ligament deficiency (ACL-D), and anterior cruciate ligament reconstruction (ACL-R). The average muscle inhibition in the knee extensors for healthy people (no knee injuries) is 9.7% (horizontal line). Note that all patient groups have significantly elevated muscle inhibition in the affected leg (as expected) and in the “normal” unaffected contralateral leg (unexpected); therefore, in a clinical test in which the left-to-right differences are assessed, muscle inhibition would be greatly underestimated (Herzog <i>et al.</i> , 2003, p. 311)..... 52
2.9	Kinematic mechanisms of avoiding excessive ATT in ACLD patients. Increased knee flexion (a) reduces ATT (b) (from Papadonikolakis <i>et al.</i> , 2003, p. 238)..... 55
2.10	Neuromuscular (quadriceps) mechanisms of avoiding excessive ATT in ACLD patients. Decreasing quadriceps activity (a) reduces quadriceps force (b) (from Papadonikolakis <i>et al.</i> , 2003, p. 238)..... 56
2.11	Neuromuscular (hamstrings) mechanisms of avoiding excessive ATT in ACLD patients. Hamstring activity (a) increases posterior tibial draw (b) and reduces and ATT (from Papadonikolakis <i>et al.</i> , 2003, p. 238)..... 57
3.1	Test limb effect for single-leg vertical jump height for the ACLD, PT, STGT and control groups. * indicates a significant difference between the non-involved and involved limbs 102
3.2	Test limb effect for single-leg long hop distance for the ACLD, PT, STGT and control groups. * indicates a significant difference between the non-involved and involved limbs 103
3.3	Subject group effect for the single-leg long hop distance for the ACLD, PT, STGT and control groups. + indicates a significant difference between subject groups 104
3.4	Subject group × test limb interaction for the single-leg timed hop for the ACLD, PT, STGT and control [‡] groups. <i>Between test limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs. <i>Between subject group contrasts</i> : + indicates a significant difference between the non-involved limbs and involved limbs of the ACLD and control groups; ++ indicates a significant difference between the non-involved and involved limbs of the ACLD and STGT groups ([‡] <i>Note</i> : Control group data is the average of the dominant and non-dominant limbs) 106
4.1	Raw rectified and linear envelopes for a representative EMG signal created using f_c ‘s of 10, 20, 30 and 40 Hz..... 126
4.2	Moment arm length (mm) of the quadriceps during knee extension between 90° of flexion and full extension (0° flexion)..... 131
4.3	Moment arm length (mm) of the hamstrings during knee flexion between 90° of flexion and full extension (0° flexion) 132

Figure	Page
4.4	Test limb effect for extension torque for the ACLD group. <i>Between test limb contrasts:</i> * indicates significant difference between the non-involved and involved limbs..... 137
4.5	Test limb × knee flexion interval interaction for extension torque for the PT group. <i>Between limb contrasts:</i> * indicates a significant difference between the non-involved and involved limbs .. 139
4.6	Test limb effect for extension torque for the STGT group. <i>Between test limb contrasts:</i> * indicates a significant difference between the non-involved and involved limbs..... 141
4.7	Knee flexion interval × subject group interaction for extension torque for the non-involved limb of the ACLD, PT, STGT and control [‡] groups. <i>Between limb contrasts:</i> * indicates a significant difference between the ACLD and PT groups; ** indicates a significant difference between the ACLD and STGT groups; *** indicates a significant difference between the ACLD and control groups. <i>Within group contrasts:</i> + indicates a significant difference between knee flexion intervals for all subject groups ([‡] Note: Control group data is the average of the dominant and non-dominant limbs)..... 144
4.8	Subject group effect for extension torque for the involved limb of the ACLD, PT, STGT and control [‡] groups. <i>Between subject group contrasts:</i> + indicates a significant difference subject groups ([‡] Note: data for the control group data is the average of the dominant and non-dominant limbs)..... 146
4.9	Knee flexion interval effect for extension torque for the involved limb of the ACLD, PT, STGT and control [‡] groups. <i>Between knee flexion interval contrasts:</i> + indicates a significant difference between knee flexion intervals ([‡] Note: data for the control group data is the average of the dominant and non-dominant limbs) 148
4.10	Test limb × knee flexion interval interaction for flexion torque for the STGT group. <i>Between limb contrasts:</i> * indicates a significant difference between the non-involved and involved limbs..... 154
4.11	Knee flexion interval effect for flexion torque for the non-involved limb of the ACLD, PT, STGT and control [‡] groups. <i>Between flexion interval contrasts:</i> + indicates a significant difference between knee flexion intervals ([‡] Note: Control group data is the average of the dominant and non-dominant limbs)..... 155

Figure	Page
4.12	Subject group \times knee flexion interval interaction for flexion torque for the involved limb of the ACLD, PT, STGT and control [‡] groups (A) <i>Between subject group contrasts</i> : indicates a significant difference between the ACLD and PT groups and the ACLD and control groups; ** indicates a significant difference between the PT and STGT groups; *** indicates a significant difference between the STGT and control groups (B) <i>Within ACLD group contrasts</i> : + indicates a significant difference between flexion intervals (C) <i>Within PT group contrasts</i> : + indicates a significant difference between flexion intervals (D) <i>Within STGT group contrasts</i> : + indicates a significant difference between flexion intervals (E) <i>Within control group contrasts</i> : + indicates a significant difference between flexion intervals ([‡] Note: Control group data is the average of the dominant and non-dominant limbs) 158
4.13	Average hamstring moment arm length and antagonist activation of the ST and BF muscles during maximal effort isokinetic knee extension at 180°•s ⁻¹ 167
4.14	Knee flexion interval effect for ST antagonist EMG activity for the ACLD, PT, STGT and control groups. <i>Between flexion interval contrasts</i> : + indicates a significant difference between flexion intervals..... 168
4.15	Knee flexion interval effect for BF antagonist EMG activity for the ACLD, PT, STGT and control groups. <i>Between flexion interval contrasts</i> : + indicates a significant difference between flexion intervals..... 168
4.16	Test muscle \times knee flexion interval interaction for hamstring antagonist EMG activity for the ACLD, PT, STGT and control groups. <i>Between muscle contrasts</i> : * indicates a significant difference between the ST and BF muscles 171
5.1	Experimental arrangement including; (A) reflective markers, (B) EMG electrodes (only VL and BF displayed), (C) accelerometer, and (D) force plate (<i>Note</i> : an elastic bandage was wrapped around the thigh during testing to secure the EMG electrodes and leads but has been excluded from this photograph) 182
5.2	Typical GRF-time curves generated during landing from a single-leg long hop for distance. Variables obtained from vertical (top) and braking (bottom) GRF: (A) magnitude of F _{v1} , (B) time from IC to F _{v1} , (C) magnitude of F _{v2} , (D) time from IC to F _{v2} , (E) magnitude of F _{Br} and, (F) time from IC to F _{Br} 185
5.3	Typical tibial acceleration-time curve generated during landing from a single-leg long hop for distance. Variables obtained from tibial acceleration: (A) magnitude of TA _p , (B) time from IC to TA _p , and (C) time to from IC to TA ₀ 186

Figure	Page
5.4	Definition of (i) hip, knee and ankle joint angles in the neutral standing position, and (ii) the angle of HF = $A - \alpha$; Angle of KF = $B - \beta$, and; Angle of DF = $C - \gamma$ 187
5.5	Subject group \times test limb interaction for F_{v1} for the ACLD, PT, STGT and control [‡] groups (A) <i>Between test limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs for the ACLD group; ** indicates a significant difference between the non-involved and involved limbs for the STGT group (B) <i>Between subject group contrasts for the non-involved limb</i> : + indicates a significant difference between subject groups (C) <i>Between subject group contrasts for the involved limb</i> : + indicates a significant difference between subject groups ([‡] Note: Control group data is the average of the dominant and non-dominant limbs) 194
5.6	Test limb effect for F_{v2} force for the ACLD, PT, STGT and control groups. <i>Between test limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs .. 197
5.7	Subject group effect for F_{v2} force for the non-involved and involved limbs of the ACLD, PT, STGT and control [‡] groups. <i>Between subject group contrasts</i> : + indicates a significant difference between subject groups ([‡] Note: Control group data is the average of the dominant and non-dominant limbs)..... 198
5.8	Subject group effect for F_{Br} force for the non-involved and involved limbs of the ACLD, PT, STGT and control [‡] groups. <i>Between subject group contrasts</i> : + indicates a significant difference between subject groups ([‡] Note: Control group data is the average of the dominant and non-dominant limbs)..... 202
5.9	Test limb effect for the duration of positive tibial acceleration for the ACLD, PT, STGT and control groups. <i>Between test limb contrast</i> : * indicates a significant difference between the non-involved and involved limbs..... 207
5.10	Test limb \times event interaction for hip flexion for the STGT group. <i>Between test limb contrasts</i> : No contrasts reached statistical significance..... 212
5.11	Test limb \times event interaction for knee flexion for the PT group. <i>Between limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs..... 216
5.12	Test limb \times event interaction for hamstring moment arm length for the ACLD, PT, STGT and control groups. <i>Between test limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs..... 225
5.13	Test limb \times event interaction for ST muscle length for the ACLD, PT, STGT and control groups. <i>Between limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs..... 229

Figure		Page
5.14	Test limb × event interaction for BF muscle length for the ACLD, PT, STGT and control groups. <i>Between limb contrasts</i> : * indicates a significant difference between the non-involved and involved limbs.....	233
5.15	Test limb × subject group interaction for the onset of BF activity relative to IC (IC-onset) for the non-involved and involved limbs of the ACLD, PT, STGT and control [‡] groups. <i>Within Subject Group Between Test Limb Contrasts</i> : * indicates a significant difference between the non-involved and involved limbs for the ACLD group. <i>Between Subject Group Within Test Limb Contrasts</i> : + indicates a significant difference between the ACLD and PT groups for the non-involved limb ([‡] Note: control group data is the average of the dominant and non-dominant limbs)	243
5.16	Test limb × subject group interaction for the onset of BF activity relative to IC (IC-onset/IC-TA _p (%)) for the non-involved and involved limbs of the ACLD, PT, STGT and control [‡] groups. <i>Within Subject Group Between Test Limb Contrasts</i> : indicates a significant difference between the non-involved and involved limbs for the ACLD group. <i>Between Subject Group Within Test Limb Contrasts</i> : + indicates a significant difference between the ACLD and PT groups for the non-involved limb ([‡] Note: Control group data is the average of the dominant and non-dominant limbs)	244

LIST OF ABBREVIATIONS AND NOTATIONS

Abbreviations and notations used in the text of this thesis are defined below. Abbreviations used in tables are defined within the relevant tables. Symbols used in equations are defined below each equation.

Notation	Definition	Notation	Definition
ACL	Anterior cruciate ligament	IC	Initial contact
ACLD	Anterior cruciate ligament deficient/deficiency	IKDC	International Knee Documentation Committee
ACLR	Anterior cruciate ligament reconstruction/reconstructed	Int15	Interval between 20-10° knee flexion
A/C	Alternating current	Int25	Interval between 30-20° knee flexion
A/D	Analog-to-digital	Int35	Interval between 40-30° knee flexion
ATT	Anterior tibial translation	Int45	Interval between 50-40° knee flexion
CNS	Central nervous system	Int55	Interval between 60-50° knee flexion
BF	Biceps femoris	Int65	Interval between 70-60° knee flexion
BF15	Biceps femoris antagonist activity between 20-10° knee flexion	Int75	Interval between 80-70° knee flexion
BF25	Biceps femoris antagonist activity between 30-20° knee flexion	LH	Lateral hamstring
BF35	Biceps femoris antagonist activity between 40-30° knee flexion	MH	Medial hamstring
BF45	Biceps femoris antagonist activity between 50-40° knee flexion	PT	Patella tendon
BF55	Biceps femoris antagonist activity between 60-50° knee flexion	RF	Rectus femoris
BF65	Biceps femoris antagonist activity between 70-60° knee flexion	ROM	Range of motion
BF75	Biceps femoris antagonist activity between 80-70° knee flexion	S	Soleus
EMG	Electromyography	SM	Semimembranosus
EMD	Electromechanical delay	ST	Semitendinosus
Ext15	Extension torque between 20-10° knee flexion	ST15	Semitendinosus antagonist activity between 20-10° knee flexion
Ext25	Extension torque between 30-20° knee flexion	ST25	Semitendinosus antagonist activity between 30-20° knee flexion
Ext35	Extension torque between 40-30° knee flexion	ST35	Semitendinosus antagonist activity between 40-30° knee flexion
Ext45	Extension torque between 50-40° knee flexion	ST45	Semitendinosus antagonist activity between 50-40° knee flexion
F_{Br}	Peak braking ground reaction force	ST55	Semitendinosus antagonist activity between 60-50° knee flexion
f_c	Filter cut-off frequency	ST65	Semitendinosus antagonist activity between 70-60° knee flexion
Flex45	Flexion torque between 40-50° knee flexion	ST75	Semitendinosus antagonist activity between 80-70° knee flexion
Flex55	Flexion torque between 50-60° knee flexion	STGT	Combined semitendinosus and gracilis tendon
Flex65	Flexion torque between 60-70° knee flexion	TA	Tibialis anterior
Flex75	Flexion torque between 70-80° knee flexion	TA_0	Zero tibial acceleration
F_{v1}	Peak vertical ground reaction force	TA_p	Peak tibial acceleration
F_{v2}	Peak vertical ground reaction force during stabilisation	VL	Vastus lateralis
G	Gracilis	VM	Vastus medialis
GA	Gastrocnemius	VMO	Vastus medialis oblique
GRF	Ground reaction force		