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Ontogenetic scaling patterns and functional anatomy of the pelvic limb musculature in emus (*Dromaius novaehollandiae*)

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10 Abstract

Emus (Dromaius novaehollandiae) are exclusively terrestrial, bipedal and cursorial ratites with some similar biomechanical characteristics to humans. Their growth rates are impressive as their body mass increases eighty-fold from hatching to adulthood whilst maintaining the same mode of locomotion throughout life. These ontogenetic characteristics stimulate biomechanical questions about the strategies that allow emus to cope with their rapid growth and locomotion, which can be partly addressed via scaling (allometric) analysis of morphology. In this study we have collected pelvic limb anatomical data (muscle architecture, tendon length, tendon mass and bone lengths) and calculated muscle physiological cross sectional area (PCSA) and average tendon cross sectional area from emus across three ontogenetic stages (n=17, body masses from 3.6 to 42 kg). The data were analysed by reduced major axis regression to determine how these biomechanically relevant aspects of morphology scaled with body mass. Muscle mass and PCSA showed a marked trend towards positive allometry (26 and 27 out of 34 muscles respectively) and fascicle length showed a more mixed scaling pattern. The long tendons of the main digital flexors scaled with positive allometry for all characteristics whilst other tendons demonstrated a less clear scaling pattern. Finally, the two longer bones of the limb (tibiotarsus and tarsometatarsus) also exhibited positive allometry for length and the two others (femur and first phalanx of digit III) had trends towards isometry. These results indicate that emus experience a relative increase in their muscle force-generating capacities, as well as potentially increasing the force-sustaining capacities of their tendons, as they grow. Furthermore, we have clarified anatomical descriptions and provided illustrations of the pelvic limb muscle-tendon units in emus.

31 Introduction

32 Scaling studies (relating animal body mass to other biological parameters) have broadly elucidated 33 locomotor adaptations across a wide range of body sizes. These studies have also described 34 important size-related biomechanical (Alexander et al. 1979; Bertram & Biewener 1990; Biewener 35 1982; Gatesy & Biewener 1991; LaBarbera 1989; Maloiy et al. 1979; McMahon 1975) and metabolic 36 (Gillooly et al. 2001; Hemmingsen 1960; Hokkanen 1986; Kleiber 1932; Schmidt-Nielsen 1984; Taylor 37 et al. 1981) constraints across species. Intraspecific scaling studies are less common (Allen et al. 38 2010,2014; Carrier & Leon 1990; Carrier 1983; Dial & Jackson 2011; Main & Biewener 2007; Miller et 39 al. 2008; Picasso 2012a; Smith & Wilson 2013; Young 2009, Picasso 2014) These ontogenetic 40 approaches yield valuable insights into musculoskeletal adaptations to growth and potentially to 41 identify size-related constraints on mechanical function within a species. Furthermore, studies of 42 species where the mode of locomotion and basic anatomy remains similar during development 43 contribute to the understanding of strategies and trade-offs that occur during growth. Such 44 information can, for example, be used to comprehend developmental abnormalities and study 45 intervention strategies to manage them.

Ratites are large flightless birds with cursorial morphology (e.g., Smith et al. 2010; Smith & Wilson 2013) that makes them attractive subjects for studies of terrestrial locomotion and bipedalism (Abourachid, 2000). Certain characteristics make emus (*Dromaius novaehollandiae*) particularly useful: they have some anatomical and functional similarities to other bipedal animals, including purportedly humans (Goetz et al. 2008). Compared to ostriches, they are generally easier to handle and train in experimental settings due to their smaller size and calmer temperament. Finally, their growth rate is impressive, as they multiply their body weight ~80 times in the first 18 months of life (Minnaar & Minnaar 1998) whilst maintaining the same cursorial mode of locomotion. Despite this interest there are still some discrepancies in published anatomical descriptions and depictions of the pelvic limb musculature of emus (Haughton 1867; Patak & Baldwin 1998; Vanden Berge & Zweers 1993), and clear visual anatomical aids are lacking in the literature.

57 Some of the biomechanical changes in the hindlimb occurring during the growth in emus have been 58 described . Main and Biewener (2007) measured the skeletal strain patterns on the surfaces of the 59 femur and the tibiotarsus (TBT) in running emus, demonstrating a significant increase in the 60 magnitude of cranial and caudal femoral and caudal tibiotarsal strains during ontogeny, despite the 61 enlargement and strengthening of those bones via positive allometric scaling of the second moment 62 of area. Muscles have been shown to influence the strain patterns of bones (Yoshikawa et al. 1994), 63 and although other factors are likely to be involved in the changes in peak bone strains reported 64 across ontogeny (Main & Biewener 2007), allometric scaling of the musculature could also play a 65 role in these differences in bone tissue loading. The strains induced by muscle contraction will be 66 proportional to the muscle forces acting on the bone; therefore by estimating muscle forces (e.g., 67 maximal force capacity based upon anatomy), associations between these two findings would be 68 possible.

- 69 In order to build on already available biomechanical data for emus (Goetz et al. 2008; Main &
- Biewener 2007), we aim here to quantify the ontogenetic scaling patterns of four pelvic limb bones,
 pelvic limb muscles and their tendons and in the process describe and compare the functional and
- descriptive anatomy of the pelvic limb musculature of emus. We use regression analysis to
- determine the relationship of muscle architectural properties with body mass in an ontogenetic
- 74 series of emus and then examine the implications of these findings for the locomotor ontogen of
- 75 emus, other ratites as well as extinct theropod dinosaurs.

76 Materials and methods

77 Animal subjects and care: UK group

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78 We dissected 17 emus for this study, obtained from our ongoing research examining emu 79 ontogenetic biomechanics (conducted with ethical approval under a UK Home Office license). The 80 emus were divided in three groups of animals according to their age: Group 1: Five individuals at 4-6 81 weeks old; Group 2: Six 24-28 weeks (6 months) old individuals; and Group 3: Six 64-68 weeks (16 82 months) old individuals. All birds had been used as experimental animals and kept in a small pen 83 (7x7m) for the first six weeks of life, after which they were moved to an outdoor larger enclosure 84 with grass footing (40mx15m) until they were six months old; after this they were moved to a large 85 (1.6 hectares) grass field (maximal animal density at one time was 8 birds/ha). The birds were all 86 born in three consecutive yearly breeding seasons. Only the birds in Group 3 were from the same 87 breeding season but not necessarily the same progenitors; birds from the other two Groups were 88 from two different seasons.

90 All animals were hatched at a commercial breeding farm in the UK and raised from four weeks of age 91 at the Royal Veterinary College. They were fed a commercial ostrich pelleted diet supplemented 92 with grass and from six weeks of age were kept with free access to commercial food and grass. At 24 93 weeks, their diet changed from an ostrich grower diet to adult ostrich pelleted food (Dodson and 94 Horrel Ltd., Kettering, Northamptonshire, UK). There were no restrictions or enforcements on the animals' regular exercise regime and all animals were allowed the same area and conditions to 96 exercise during their development. All animals were euthanized after other experimental procedures 97 were completed, by lethal intravenous injection of a barbiturate following induction of deep 98 terminal general anaesthesia by intramuscular injection of ketamine and xylazine. Carcasses were 99 kept frozen in a -20°C freezer for up to 2 years before dissection. Thawing was allowed at variable ambient temperatures and for variable amounts of time depending on the size of the animal, and dissection started no longer than 4 days after removal from the freezer. All dissections were performed within a six week period and led by the same individual (L.P.L.).

USA group of emus

104 Unpublished raw data of muscle masses from a different group of 29 emus (0.74 to 51.7 kg body 105 mass) used for similar purposes as those described for the UK group were also included in this study. 106 This group was bred and reared in the USA (Concord Field Station, Harvard University) under the 107 care of another investigator (R.P.M.) who led all dissections for this group. The size and age 108 composition for this group was more heterogeneous, and only body masses and muscle masses 109 were available for analysis. Because the purpose of the dissections in the group was not a systematic 110 ontogenetic musculoskeletal scaling study, the number of muscles dissected per animal varied. 111

112 Bone measurements

113 Maximal interarticular lengths of the femur, tibiotarsus (TBT), tarsometatarsus (TMT) and first 114 phalanx of the middle (third) digit were measured using an ordinary flexible measuring tape (±1mm) 115 once they were cleared of all soft tissues.

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117 Myology and muscle architecture

118 We identified muscles of emus using four separate literature sources (Haughton 1867; Patak &

- 119 Baldwin 1998; Smith et al. 2007; Vanden Berge & Zweers 1993); when our observations differed
- 120 from these, we described the anatomical landmarks and attachments in detail according to our
- 121 observations. General main actions of the muscle were defined based on these publications and
- 122 confirmed by identifying the muscle attachments and paths and then mimicking the muscle action
- by applying tension on the muscle during dissection. We used additional reference to a 123
- 124 biomechanical model of an ostrich (Hutchinson et al. 2014) to refine the three-dimensional actions
- 125 of the hip muscles, as those actions are difficult to accurately ascertain from visual inspection and
- 126 manipulation. Table 1 shows our simplified description of the anatomy, abbreviations used

- 127 throughout this study, and inferred muscle actions. Figures 1 to 3 show schematic anatomical 128 representations of the muscle anatomy.
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130 To avoid freeze drying of the carcasses, we ensured all animals were frozen soon after euthanasia

131 kept in sealed bags, and were not thawed and refrozen before dissection. The carcasses showed 132 minimal autolysis and therefore an easier and better dissection during which muscle actions could

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be approximated without damaging their structure and attachments.

Dissection of the right pelvic limb muscles was performed in all specimens apart from the first two 134

135 subjects in the 4-6 week old group, in which the muscles of the left limb were dissected first to

136 standardise the technique. Measurements taken from the muscles of the left limb were not used 137 (avoiding duplication of information), with the exception of when there were unidentified/damaged

138 muscles from the right limb of the same specimen, in order to create a complete set of muscles for

139 each specimen.

After identification of each muscle, we performed complete dissection and removal of it by transection at its origin and insertion(s). Next, the muscle was laid flat on a table and we took four muscle architectural measurements in a standard protocol: muscle mass (M_m), fascicle length (L_f), 143 muscle belly length and pennation angle (Θ). Muscle mass was measured on an electronic scale (± 0.01 g) after removal of tendons, fat and aponeuroses. Fascicle length was measured from at least five random sites within the muscle belly using digital callipers $(\pm 0.1 \text{ mm})$. Muscle belly length was measured as the length (± 1 mm) from the origin of the most proximal muscle fascicles to the insertion of the most distal fascicles into the distal tendon or aponeurosis. The pennation angle was measured at least five times using a goniometer $(\pm 5^{\circ})$ with the mean of the latter measurements was taken as the pennation angle for the muscle. The repeated measurements were taken from multiple cuts into the muscle to expose different anatomical orientations of the fascicles with the same muscle. This methodology minimises the differences that may be seen across an individual 152 muscle and ensures mean values used for further calculations are representative of the overall architecture of the muscle. We calculated total limb muscle mass by adding the individual masses of the muscle bellies. Our approach was straightforward for most muscles, apart from three smaller muscles of the limb: IFI, ISF and FPPDII (Table 1), where minor dissection mistakes might have 156 impaired estimates of their masses and architectural properties.

Muscle volume was calculated by dividing muscle mass by estimated muscle density of vertebrates 157 (1.06 g cm⁻³; (Brown et al. 2003; Hutchinson et al. 2014; Mendez & Keys 1960)). From these data we 158 159 calculated physiological cross-sectional area (PCSA) for each muscle via the standard formula (Powell 160 et al. 1984; Sacks & Roy 1982) (Equation 1):

$$PCSA = \left(\frac{Vmusc}{Lfasc}\right)cos\theta$$

161 When a tendon was present it was dissected down to its insertion onto the bone together with the 162 muscle. The tendon was then transected at the musculotendinous junction when a clear separation 163 became apparent and stretched on a flat surface. We then measured lengths with a standard ruler 164 or flexible measuring tape (±1mm), and tendon mass was also measured using the same 165 instrumentation as for the muscles.

166 Tendon cross-sectional area (TCSA) was calculated using tendon length (L_{ten}) ; from muscle origin to 167 bony insertion; and tendon mass (M_{ten}) as follows (Equation 2):

$$TCSA = \frac{Mten}{1120Lten}$$

168 Where 1120 kg m⁻³ is assumed as the density of tendon (Hutchinson et al. 2014; Ker 1981).

169 Statistical analysis

170 Ontogenetic scaling relationships of (non-normalized) muscle properties were analysed using 171 reduced major axis ("Model II") regression for log₁₀ of each property vs log₁₀ body mass using 172 custom-designed R software code (R Development Core Team 2010) code. A Shapiro-Wilk test was 173 performed to assess normality of distribution of the residuals, and the p value for significance was 174 set to <0.05. The inclusion criteria for data presented were: Datasets first had to have a p value 175 <0.05 in the above described Shapiro-Wilk test. If this p was >0.05, the data were then tested for the 176 presence of outliers (which were set at ±2 standard deviations [SD] from the mean) and outliers 177 removed. The RMA linear regression was performed again using this dataset and again, data were 178 only presented if the p value for distribution of residuals was <0.05. Once the datasets were defined, 179 R^2 correlation values and upper and lower bounds of the 95% confidence interval (CI) were calculated to assess the spread of data points around each regression line. 180

In order to obtain relative values to compare results from individuals of different size, muscle mass, PCSA and F_{length} were normalized to body mass (BM) by dividing each value by the subject's BM, BM^{0.67} and BM^{0.33} respectively. We used body mass (BM) as our independent variable and the target architectural parameter as our dependant variable. Overall, we followed a similar approach as that described by Allen et al. (2010,2014).

Briefly, for two objects to be considered geometrically similar (and thus for an isometric scaling pattern to be inferred), areas should scale to the square product of lengths and volumes to the cube of lengths. Because mass is a volumetric property, the dependant variable is considered to scale isometrically if the mass of the structure scales with BM¹, areal properties (PCSA, TCSA) scale to BM^{0.67} and lengths scale to BM^{0.33}, whereas angles and other non-dimensional variables should scale as BM⁰.

194 Results

We obtained 6524 measurements of seven different muscle-tendon architectural parameters from 34 pelvic limb muscles and four pelvic limb bones in 17 emus from 3.6 to 42 kg of body mass. We found strong evidence for positive allometric scaling for many of these architectural parameters, as described below. To aid interpretation of our results, we have divided the muscles of the limb into proximal (those acting mostly on the hip and knee joints) and distal (those acting on the ankle, foot and digits) groups and have used this division to compare trends between the two regions.

201 Bone lengths

The lengths of the four bones scaled with moderate positive allometry (expected slope representing isometry would be 0.33). The femur had the least marked allometric exponent (0.38), whilst the tarsometatarsus the greatest (0.44), the tibiotarsus had a slope value of 0.41 and for the 1st phalanx of the second digit (P1) the value was 0.39 (for full results see Table 2).

- 206
- 207 Myology, architectural characteristics of muscles and functional interpretation
- 208 We classified a total of 34 muscles in Table 1. As noted by Regnault et al. (2014), there is no patellar
- 209 ossification in the knee joint of emus, unlike ostriches and some other palaeognaths as well as most
- extant birds. Although muscle origins, insertions and paths were generally found to agree with
- previous publications (Haughton 1867; Patak & Baldwin 1998; Vanden Berge & Zweers 1993) and
 hence detailed re-description is unnecessary, there were a few muscles for which we have found
- some differences worth noting, or for which we needed to use methodological simplifications:
- 214

- 215 M. iliotibialis lateralis pars postacetabularis (IL): The distal fusion and similar actions of both parts of
- the IL muscle (Fig.1) meant that, in order to avoid dissection errors when finding the division
- 217 between the cranial and caudal parts of the muscle, we measured and presented them together.

M. iliotrochantericus cranialis (ITCR): Although this was a clear, separate muscle in most specimens
(Fig. 2), it was found to be fused with the ITM in two specimens of body mass ~20 kg, which is a
common finding in birds (Gangl et al. 2004)

221 M. ischiofemoralis (ISF): This small muscle is difficult to detect and dissect, which is likely to have affected the accuracy of the data obtained from it (leading to lower R² values and wider 95% CI 222 223 ranges). Its action is likely to involve fine motor control, proprioception and stabilisation of the hip 224 joint, given its very small size. Some studies have considered this muscle to be absent (or fused with 225 other muscles; e.g., CFP) in emus (Haughton 1867; Patak & Baldwin 1998), which would be unusual 226 for any birds. The origin and insertion of the muscle that we label the ISF (Fig. 3) is best interpreted 227 as a reduced -- but still present – muscle, similar to that in ostriches (Gangl et al. 2004; Zinoviev 228 2006).

M. caudofemoralis pars pelvica (CFP): We consider, contrary to other reports (Haughton 1867; Patak & Baldwin 1998), that this muscle is present in emus (Fig. 2). Prior studies classified this muscle as the "iliofemoralis" but we agree with the *Nomina Anatomica Avium* (Vanden Berge & Zweers 1993) and other reports (Gangl et al. 2004; Hutchinson 2004a; Hutchinson et al. 2014; Zinoviev 2006) that it is present in ratites, related to a reduced portion of the large caudofemoralis muscle that is ancestrally present in tailed reptiles (Gatesy 1999). There is no evidence of a caudalis part to the M. caudofemoralis in emus, unlike in ostriches (Gangl et al. 2004) and some other ratites, so this subdivision of the CFP is either fused to the CFP or lost.

M. ambiens (AMB): We found this muscle to have two insertions, previously unnoticed: a tendinous one onto the tibia and a fleshy one onto the distal femur. Unusual modifications of this muscle seem common in ratite birds (Hutchinson et al. 2014)

M. popliteus: This is a short, deeply positioned, fleshy muscle with multiple fibrous planes within it,
originating on the caudolateral, proximal aspect of the tibiotarsus and inserting onto the medial side
of the proximal fibula (Fig. 3). It is likely a stabiliser or pronator/supinator of the fibula, as in
ostriches (Fuss 1996), and may act as a proprioceptive or ligament-like structure.

244 Normalized data for individual muscles

To allow relative comparisons between muscle measurements, we normalized data from only the 16 245 246 month old (Group 3, adult birds) emus. Data are only presented for adult emus so as not to influence 247 the relative proportions due to ontogenetic allometry. The entire ontogenetic data set was analysed 248 similarly with negligible differences found, indicating that the relative patterns seen between 249 muscles for adults are present in very young birds as well. Data for muscle mass, fascicle length and 250 PCSA are presented in Figure 4. The largest relative muscles with regards to mass were three 251 proximal (ILPO, ILFB and IC) and three distal muscles (GM, FL and GL). This order changes when 252 muscles are ranked according to PCSA because parallel-fibred muscles tend to drop down the list, 253 with the large ILPO being the only parallel-fibred muscle seen in the top 10 of a list that is otherwise

- dominated by distal muscles (FL, GM, GL and FPDIII). On the other hand, when fascicle length is
 compared, the three parts of the gastrocnemius (GIM, GM and GL) are the only distal muscles listed
- amongst the 10 muscles with the longest fascicles. The four muscles with the longest fascicles are
- the FCLP, IC, ILFB and ILPO.

259 Limb muscle masses

- 260 Total mass values of the hindlimb musculature represented a mean of 13.4±3% of BM, with the
- 261 proximal limb musculature (PLM) representing 61±2% of limb muscle mass and the distal limb

- muscles (DLM) accounting for the remaining 39±2%. However, if only values for the six largest birds
 (adults) are analysed, limb muscle mass accounts for 15±1% of BM. The limb muscle mass is only
 11+2% of body mass in the five birds that were 4-6 weeks old
- 11±3% of body mass in the five birds that were 4-6 weeks old.

266 Scaling regression analysis

The slopes of the reduced major axis regression lines for muscle properties vs. body mass are shown in Tables 3 and 4, with R² and 95% CIs, as well as represented in Figures 5 (A and B) and 6. Ranges of the slope and amplitudes of the CIs referred to below are the upper and lower bounds of the 95% CIs for the regression slopes. Scaling exponents and CIs are presented in Table 3. Scaling exponents and lines representing isometry are plotted in Figure 5A and 5B (M_m, L_f and PCSA) and Figure 7 (M_{ten}, L_{ten} and TCSA). In summary, there was strong positive allometry of muscle mass and mild positive allometry or isometry of fascicle length, leading to a marked positive allometry of PCSA.

Scaling of limb muscle masses

We found limb muscle mass as well as the masses of proximal (PLM) and distal limb muscles (DLM) to be tightly correlated with body mass across all three groups. The regression slope of limb muscle mass vs. BM was 1.16 (1.05<CI<1.29, R²=0.96), whilst PLM had a value of 1.14 (1.02<CI<1.27, R²=0.96) and DLM exhibited a slope of 1.20 (1.09<CI<1.32, R²=0.97).

Consistent with the trends for the hindlimb more broadly, the individual muscles also generally showed positive ontogenetic allometry. Out of 34 muscles, 26 had slopes for M_m vs. BM with their lower CI limit >1 (consistent with positive allometry), and only eight (ITCr, ITM, IFI, ISF, FCLA, FMTL, AMB and FPPDII) had a lower CI boundary for the regression slope lower than 1 (indicating potential negative allometry). Of the 26 muscles showing positive allometry of M_m , we found strong positive allometry (regression slopes with the lower boundary of the CI greater than 1.1) in 18/34.

Similarly, scaling patterns of the muscle masses for the USA group of emus (Figure 6), showed similar scaling patterns to the UK group, with only five muscles having a lower CI boundary <1 (POP, ILPO, FPDIV, OBTII and FPDII) and the remaining having their CIs entirely within positive allometry values.

292 Scaling of muscle fascicle length

293 In general, fascicle length (L_f) was only moderately well correlated with body mass due to substantial 294 variation in the data (a combination of inevitable measurement errors, sampling bias and true biological variation, as usual for muscle fascicle measurements (e.g., Allen et al. [2010,2014]) The 295 296 datasets for four muscles (ISF, PIFLM, FPDII and FPPDII) had a p value>0.05, so these are not 297 presented (Table 3). Of the remaining 30 muscles, only 16/30 had R^2 values >0.5. Scaling of L_f vs. BM 298 showed a trend towards positive allometry for 18/30 muscles (lower limit of the slope's CI >0.33), 299 and for the remaining 12 muscles a slope of 0.33 was included in the CIs, so isometry could not be 300 ruled out.

301

302 Scaling of muscle PCSA

The lower boundary of the CIs of the scaling slope was greater than 0.66 (i.e., exhibiting positive allometry) for 27 muscles and a value <0.66 (suggesting a potential negative allometry of muscle PCSA in emus) was obtained for eight muscles (ITM, ITC, IFI, FMTL, AMB, TC and FPPDII) (Table 3).

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307 Scaling of tendon mass

308 We recorded tendon characteristics for 28 muscles (Table 4); the six muscles excluded did not have a

- discrete tendon at either of their attachments (CFP, FCLA, FCLP, IC, PIFLM, POP). We encountered
- 310 difficulties in achieving a consistent method for tendon dissection and measurement of muscles with
- thin (IFE, AMB), very short (ISF and IFI) or multiple tendons (FMTM, FMTIM), which lead us to
- exclude data from these as well. The tendon of the GIM was included with the GM tendon, and the

- FMTL tendon was not measured because the muscle was transected at the proximal aspect of the large patellar tendon for studies of patellar tendon morphology by Regnault et al. (2014). Thus data are presented for the tendons of 20 muscles. The major gastrocnemius tendon resulting from the
- fusion of the tendons of the three gastrocnemius muscles was dissected by transecting the tendon
- of the GL at the site of fusion onto the common tendon; therefore the GM remained with the
- extensive common portion of the tendon, which distally was transected at its insertion onto the
- 319 fibrous scutum at the level of the ankle joint.
- 320
- 321 The scaling slopes for tendon mass indicate positive allometry in 10 out of 20 tendons (lower CI
- boundary >1) across emu ontogeny. The masses for the remaining ten tendons scaled with isometry
 (lower Cl<1.0, upper Cl>1.2)..

324 Scaling of tendon length

We measured L_{ten} for the same 20 muscles for which we obtained tendon masses (Table 4), from the end of the muscle belly to the insertion. Statistical analysis of one muscle (ITCr) led to exclusion of this muscle because the p value was >0.05. For the other 19 tendons, the general scaling trend was towards strong positive allometry, with 16 muscles having the lower limit of the CI >0.33. In three muscles (FCM, GM, FL), the lower CI for tendon length was <0.33, indicating isometry for length in these tendons. Given these patterns, we infer a general trend for positive allometry of tendon length in growing emus.

Scaling of tendon cross-sectional area

Average TCSA was calculated for the same 20 tendons as above (Table 4). The dataset for ILPO had a *p* value >0.05 and was excluded. Of the 19 remaining tendons, 10 showed a lower CI limit of the slope consistent with positive allometry (>0.66). The remaining nine tendons showed ontogenetic isometry for TCSA.

Discussion

341 Emus, like other ratites and other precocial birds, must have locomotor independence from hatching 342 and develop into large, running adult birds within 16-18 months (Davies & Bamford 2002). Taking 343 into consideration their initial development within the egg, their ontogeny poses interesting 344 questions about their locomotor development, related to our study's aims, such as: How do muscle 345 structure and anatomy change to accommodate precocial development in emus? What are the 346 strategies that growing emus use to maintain tissue mechanical safety factors during rapid 347 development of cursorial morphology and high-speed locomotor abilities? Our data suggest some 348 answers to these questions, as follows.

349

350 Scaling patterns across ontogeny

351 We found positive allometry of emu pelvic limb muscle masses, indicating that most muscles get

become significantly more powerful (in relative and absolute terms) as the animals grow. However,

353 the functional relevance of this observation is slightly mitigated by a less marked positive allometry

- of PCSA (and therefore maximal muscle force), driven by a trend for fascicle length that is closer to isometry (i.e., preserving geometric similarity).
- In the proximal part of the pelvic limb of emus, the developmental and functional mechanics appear to rely on the arrangement of large and metabolically expensive muscles (ILPO, ILFB, IC, FCLP and FMTL) to provide the wide range of motion of the knee joint (and hip, during faster running) in combination with a relatively short femur that scales close to isometry. This arrangement also leads
- to a proximal to distal gradient of muscle mass, which has been previously reported for other birds
- 361 (Paxton et al. 2010; Smith et al. 2006) and has long been thought to favour energy-savings by

- keeping the distal end of the limb light and its muscles dependent on springy tendons. The proximaldistal gradient also concentrates large, power-generating muscles in the proximal limb (Alexander
 1974; Alexander 1991) with large moment arms (Hutchinson et al. 2014; Smith et al. 2007) and thus
 the ability to produce the considerable joint moments needed for high-speed running (Hutchinson
 2004a,b).
- The distal limb, on the other hand, is heavily dependent on the triad of M. gastrocnemius (GL, GIM and GM) along with M. fibularis longus (FL); both ankle extensors; as well as M. tibialis cranialis (TC) and M. extensor digitorum longus (EDL); both ankle flexors. Combined, these muscles constitute 80% of the muscle mass and 60% of the force-generating capacity (PCSA) of this portion of the limb. The unusual proportion of body mass taken up by the ankle extensors has been noted before (Hutchinson 2004a) and is likely an ancestral characteristic of birds (e.g., Paxton et al. 2010) but is taken to an extreme in large ratites (e.g., Smith et al. 2006).

Further distally, the long and slender tarsometatarsus bone lends itself well as a support for the long tendons of the digital flexor muscles which in turn provide essential springs used in support and propulsion of the limbs and body. The relatively small muscles and long tendons of the digital flexors make them likely to operate mainly as energy storage devices at faster speeds, as seen in other species like horses and smaller running birds (Biewener 1998; Daley & Biewener 2011). The positive allometry of many tendon properties in emus is in line with this increase in force-generating capacity seen during ontogeny. As in most other birds, the tendons running along the tarsometatarsus are almost exclusively on the cranial and caudal (dorsal/plantar) side. It would also be interesting to know the effect on bone strains from this "bow and arrow" anatomical arrangement between the tarsometatarsus and the dorsal/plantar tendons to see if it influences the predominantly torsional loads experienced by the two proximal pelvic limb bones (Main & Biewener 2007).

385 For these spring-like tendons, a trade-off between muscle force and tendon elasticity does not seem 386 to occur in emus. This lack of a trade-off is indicated by the similar scaling patterns of the cross-387 sectional areas of the digital flexor muscles and tendons, both of which trend towards positive 388 allometry across emu ontogeny. As seen in other species (Ker et al. 1988), the relative increases in 389 the cross-sectional areas of tendons might maintain tendon safety factors (maximal stresses before 390 failure vs. in vivo maximal stress) as emus increase in size. However, tendons might also change their 391 biomechanical properties (Young's modulus) with age, as seen in other species (Shadwick 1990; 392 Thorpe et al. 2014), therefore influencing biomechanical interpretations of the data presented here. 393 Without measuring tendon elastic modulus with age, it is difficult to interpret how tendon stiffness 394 and safety factor might change with age in emus.

395 To complement data from a prior study showing the scaling patterns of the cross-sectional areas of 396 the femur and tibiotarsus of emus to be close to isometry (Main & Biewener 2007), here we 397 analysed the scaling patterns of the lengths of the three longest limb bones and the first phalanx of 398 the third toe. Our data indicate positive allometry of the two longer bones, the tibiotarsus (lower CI 399 limit=0.37) and tarsometatarsus (lower CI limit=0.39), but a less marked positively allometric scaling 400 trend for the femur (lower limit of CI=0.34) and for the first phalanx of digit III (lower CI limit=0.33). 401 These results differ from those reported for another ratite, the greater rhea (*Rhea americana*), in 402 which only the tarsometarsus showed positive allometry (Picasso 2012a) but interestingly are in line 403 with general interspecific scaling exponents found for pelvic limb bone lengths across different 404 species of palaeognaths (Cubo & Casinos, 1996). Considering our results, if similar cross-sectional 405 geometry is assumed along the length of the bone shafts, this would lead to an increase in strains (at 406 least in bending, due to larger moments) at the mid-shaft with increasing body mass. However, 407 changes in cross-sectional areal geometry have been shown to lead to slight positive allometry of 408 the cross-sectional geometry of avian limb bones across species (Doube et al. 2012) and 409 ontogenetically (Main & Biewener 2007). As these geometrical changes might not suffice to explain

- 410 the increases in strain magnitudes seen during ontogeny, they leave unexplained the role of internal
- 411 forces (of soft tissues) on bone mechanics and consequently their influence on bone morphology
- 412 during growth.

413 Although there are very limited data on the ontogeny of skeletal muscle physiology, experiments in 414 mice and cats (Close 1964; Close & Hoh 1967) demonstrate that although muscle force: velocity 415 parameters change from newborns to adults, these changes appear to occur in a relatively short 416 period and therefore newborn muscle, after the first few days of life, becomes similar to that of 417 adults. However, mice and cats, like many other mammals, are born with neuromotor immaturity 418 (Muir 2000), in contrast to emus. It is therefore reasonable to speculate that, like other birds (Gaunt 419 & Gans 1990), emus are unlikely to have appreciable changes in muscle physiology during growth. 420 Thus changes in functional (e.g., maximal force-generating capacity) and biomechanical parameters 421 should be detectable by anatomical studies such as ours.

Few studies have quantified the ontogenetic scaling patterns of limb musculature in birds (Carrier & Leon 1990; Dial & Carrier 2012; Paxton et al. 2014; 2012b; Picasso 2014), but positive allometry predominates in the muscle masses involved in the major adult mode of locomotion (flying vs. cursorial). In the Californian gull, the M. gastrocnemius scaled isometrically but the M. pectoralis had strong positive allometry with an inflection point when the fledglings started exercising their wings (Carrier & Leon 1990). Paxton et al. (2014; also 2010) recently reported the ontogenetic scaling patterns of the musculature of a highly modified galliform, the broiler chicken. These birds, unsurprisingly due to their selective breeding, were found to have positive allometry of muscle masses of the main pelvic limb muscles but isometry of the fascicle lengths (Paxton et al. 2014), a pattern that is nonetheless similar to our findings. Picasso et al. (2012b) found quite similar scaling patterns across rhea ontogeny: an average 64-fold increase in pelvic limb muscle mass from 1 month of age to adulthood whilst only a 34-fold increase in body mass. In a later study, where scaling exponents were calculated, a more generalised positively allometric scaling was found in these South American ratites compared to emus: with all muscle masses but two (where isometry was evident) scaling with positive allometry (slopes ~1.3). Total limb muscle mass of rheas scaled with an exponent of 1.18 (Picasso 2014), which is similar to our value of 1.16 .Together, these data suggest 438 that positive allometry prevails across ontogeny for leg muscles in extant birds with precocial 439 development; potentially a homologous feature of their development that is quite unlike the 440 isometry prevailing in their closest extant relatives, Crocodylia (Allen et al., 2010,2014).

441 Dial and Carrier (2012) suggested that birds must optimise their energy consumption to achieve their 442 ultimate functional gait whilst channelling resources to their precocial gait (Dial & Carrier 2012) 443 (running vs. swimming or flying). Ratites are unusual for birds in that they solely have terrestrial gaits 444 throughout their life and, in the case of emus, their wings have atrophied to such an extent that they 445 should not present much metabolic competition to hindlimb development. Considering the 446 approximately isometric overall scaling of kinematic parameters (e.g., stride lengths, stride 447 frequencies, duty factors) seen in ratites (Main & Biewener 2007; Smith et al. 2010), it is likely that 448 this increase in muscle masses will lead to a limb that is adapted for power production and perhaps 449 (considering our less allometric tendon results) elastic energy storage/return. The former is also 450 supported by metabolic studies which found a predominance of fast fibres in the M. gastrocnemius 451 of adult emus (Patak 1993), although more studies of muscle physiology in emus and other ratites 452 would be valuable.

The need for locomotor independence and high performance in vulnerable, young, precocial and cursorial birds might favour allometry of muscle architecture (Carrier 1996). If so, could adult muscle phenotypes be a reflection of the locomotor needs during early development and therefore be overdesigned for their demands? Alternatively, negative allometric scaling in the musculoskeletal system may occur as seen in goats (Main & Biewener 2004) and jackrabbits (Carrier 1983). It is hard

- to draw an inference from our data, because the overall positive allometry seen in the pelvic limb
 musculature could indicate a necessity to grow faster and stronger to adulthood to compensate for a
 juvenile disadvantage or could reflect selective pressures on the locomotor ontogeny of emus in
 which muscles congenitally primed for fast growth during adolescence could lead to continued
 growth past an optimum in adulthood. Although direct measurements of maximal performance of
 complex locomotor systems is problematic, a modelling approach using the data presented here
 could be a valid approach to answer this question.

465 How well are farmed emus representative of the species overall?

466 Although emu farming is relatively common, its goal is to extract meat, oil and skin and therefore 467 these birds are not bred in captivity for their locomotor behaviour, nor do they suffer strong 468 predatory pressures on it. The diet of captive bred birds as well as their relative sedentary regime 469 when compared to wild animals is likely to influence tissue development and distribution. However, 470 as farming of these birds is a recent activity and it is not a highly specialised or intense process as 471 with other domesticated species (Goonewardene et al. 2003), it is unlikely that heritable traits of the 472 emu musculoskeletal system have been significantly altered. Therefore, we expect the muscle 473 distribution and scaling patterns of our emus to be similar to wild emus.

By presenting muscle mass data from two distinct groups of birds (UK and USA groups), we established that these groups at least have similar scaling patterns, ruling out any potential bias imposed by different breeding regimes. With regards to diet, it was apparent that our birds were carrying a significant amount of subcutaneous and peritoneal fat; likely encouraged by their *ad libitum* access to a commercial pelleted diet. The influence of body fat on our scaling results is hard to test with the available data, but Hutchinson et al. (2014) noted a possible reduction in relative muscle masses in wild vs. captive bred ostriches, which could also apply to emus. Regardless, it is less certain that the scaling patterns for muscle/tendon architecture observed here would differ in wild vs. captive emus.

485 Conclusions

486 We have provided a new dataset on the ontogenetic scaling of pelvic limb anatomy and muscle 487 architectural properties of a cursorial bird (the first complete architectural dataset of its kind), and 488 we have done this using a group of 17 emus across a tenfold increase in body mass. A marked trend 489 of positive allometry of muscle masses and PCSAs is accompanied by less marked positive allometry 490 of fascicle lengths. Tendons, specially the long digital flexors, also demonstrate positive allometry of 491 their lengths, as do the two longer limb bones (tibiotarsus and tarsometatarsus). We have 492 illuminated the ontogenetic adaptation of the musculoskeletal system in an extreme example of size 493 variation during rapid growth. Our dissections refined the myology of the pelvic limb in emus (Table 494 1 and Figures 1-3) and found some anatomical aspects that were previously misunderstood. This is 495 important, as functional studies depending on inaccurate anatomical accounts of the myology could 496 obtain unrealistic results from biomechanical models using such data (Goetz et al. 2008; Hutchinson 497 et al. 2014). This work should be a valuable resource for future functional, comparative and 498 evolutionary studies of emus, other birds and extinct related animals.

499

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Tables and table captions

Table 1. Pelvic limb muscles of emus and their apparent actions.

Muscle	Abbreviation	Origin	Insertion	Action	
M. iliotibialis cranialis	IC	Dorsal edge of preacetabular ilium	Insertion on the medial aspect of the proximal	Main: Hip flexion; knee extension/flexion	
			tibiotarsus	Other: Hip medial rotation, adduction	
M. iliotibialis lateralis	() ILPO	Lateral edge of acetabular ala	Craniolateral proximal tibiotarsus (cranial and	Main: Hip extension, abduction; knee extension	
(cranial and caudal portions)			lateral cristae cnemiales) via aponeurosis	Other: Hip medial/lateral rotation	
			(combined with FMTL)		
M. iliotrochantericus cranialis	ITCr	Cranial surface of preacetabular ilium	Lateral aspect of the femoral trochanteric crest	Main: Hip flexion, medial rotation	
	Q		(distal to IFE insertion)	Other: Hip abduction/adduction	
M. iliotrochantericus medialis	П ІТМ	Craniodorsal surface of preacetabular ilium	Lateral aspect of the femoral trochanteric crest	Main: Hip flexion, medial rotation	
	$\overline{}$		(proximal to IFE insertion)	Other: Hip abduction/adduction	
M. iliotrochantericus caudalis	ІТС	Ala preacetabularis ilii: fossa iliaca dorsalis	Lateral aspect of the femoral trochanteric crest	Main: Hip flexion, medial rotation	
	U			Other: Hip abduction/adduction	
M. iliofibularis	ILFB	Ala postacetabularis ilii: facies lateralis	Proximal third of the corpus fibulae	Main: Knee flexion;, hip extension	
	n			Other: Hip abduction	
M. iliofemoralis externus	IFE	Crista iliaca dorsalis, dorsal to foramen acetabulum	Lateral side of femoral trochanteric crest	Main: Hip flexion, abduction	
			(between ITC and ITM insertions)	Other: Hip medial/lateral rotation	
M. iliofemoralis internus	IFI	Ventral preacetabular ilium	Medial side of proximal femoral shaft; tubercle	Main: Hip flexion, adduction	
				Other: Hip medial/lateral rotation	
M. ischiofemoralis	ISF	Cranial margin of the foramen ilioischiadicum	Proximal caudal femur under origin of FMTL	Main: Hip abduction, lateral rotation	
				Other: Hip flexion/extension	
M. caudofemoralis p. pelvica	CFP	Caudolateral ilium and ischium	Proximal caudomedial femur	Main: Hip extension	
				Other: Hip lateral rotation, abduction	
M. flexor cruris lateralis pars pelvica	FCLP	Caudolateral corner of pelvis	Proximal craniomedial tibiotarsus	Main: Hip extension, abduction	
				Other: Medial rotation of hip and knee; knee	
				flexion	
M. flexor cruris lateralis pars accessoria	FCLA	By a raphe from the distal third of the FCLP	Caudomedial femoral shaft	Main: Hip extension, abduction	
				Other: Hip medial rotation	
M. flexor cruris medialis	FCM	Caudolateral extremes of ischium and pubis	Via split cranial aponeurosis: on the caudal	Main: Hip extension, abduction; knee flexion	
			femoral shaft, and on the caudoproximal	Other: Hip medial rotation	

			tibiotarsus, caudodistally to the insertion of the			
			FCLP.			
M. puboischiofemoralis p. lateralis and p.	PIFLM	Along the length of the lateral ischium	Via thin tendinous insertion onto the caudal	Main: Hip extension, abduction		
medialis			aspect of the femoral shaft	Other: Hip lateral rotation		
M. femorotibialis lateralis	FMTL	Caudolateral surface of femoral shaft. With 3 fused	Crista cnemalis of tibiotarsus via a thick	Knee extension		
(Cranial, intermediate and caudal portions)		parts: cranial, intermediate and caudal	patellar tendon (no ossified patella) with ILPO			
M. femorotibialis intermedialis FMTIM		Cranial surface of the proximal femoral shaft	Medial side of crista cnemalis cranialis of tibiotarsus	Knee extension		
M. femorotibialis medialis	FMTM	3 distinct heads originating from the medial surface	Proximo-medial extremity of tibiotarsus	Knee flexion, adduction		
	, ,	of the femur, cranial and caudal portions on the				
		proximal third and distal portion on the distal third				
M. obturatorius medialis (Ilium – Ischium part)	OMII	Surface of fenestra ilioischium	Long tendon that passes through the foramen	Main: Hip lateral rotation		
<u>O</u>			ilioischiadicum and inserts onto the lateral side	Other: Hip flexion, adduction		
			of the femoral trochanteric crest			
M. obturatorius medialis (Ischium – pubis part)	ΟΜΙΡ	Surface of fenestra ischiopubica	As OMII	Main: Hip lateral rotation		
)			Other: Hip flexion, adduction		
M. ambiens	AMB	Cranial pubic rim (preacetabular process)	Two insertions on the medial knee ligaments,	Main: Hip adduction; knee flexion		
			one tendinous and the other one fleshy	Other: Hip medial rotation		
M. gastrocnemius lateralis	GL	Lateral condyle of femur, aponeurosis of M.	Tendons fusing to form a thick fibrous	Main: Ankle extension; knee flexion		
	I.	lliotibialis and tendon from cranial fibula	calcaneal pad, onto caudal side of			
			tarsometatarsus (Calcaneal scutum)			
M. gastrocnemius medialis	GM	Aponeurosis of M. Iliotibialis and facies	As GL	Main: Ankle extension; knee flexion		
		gastrocnemialis, connecting to the medial surface of				
		the proximal tibia				
M. gastrocnemius Intermedius	GIM	Craniolateral femur, adjacent of the origin of FHL	As GL and GIM	Main: Ankle extension; knee flexion		
		muscle				
M. fibularis longus	FL	Proximal origin from medial distal patellar ligament	Two tendinous insertions: Plantar calcaneal	Main: Ankle extension		
		and craniolaterally onto proximal tibiotarsus.	scutum and joining the tendon of FPDIII	Other: Knee flexion; toe flexion via FPDIII		
				tendon		
M. tibialis cranialis c. tibiale and c. femorale	тс	2 heads: A fleshy one onto the proximal cranial	Cranial side of proximal tarsometatarsus	Main: Ankle flexion		
		tibiotarsus, and via a thick tendon onto the cranial		Other: Knee extension (femoral head)		
		aspect of the lateral trochlear ridge of the femur				
M. popliteus	POP	Medial side of proximal fibula	Caudal side of proximal tibiotarsus	Main: Fibular rotation		
M. flexor perforatus digiti II	FPDII	Via origin of FPDIII	Splits into 2 branches at level of proximal	Main: Digit II flexion		
			phalanx to insert on either side of middle	Other: Ankle extension		

			phalanx, ventrally		
M. flexor perforatus digiti III	FPDIII	2 tendons: Cranial fibula and medial side of the	Proximal phalanx, small portion fused to FPPDII	Main: Digit III flexion	
		medial condyle of the femur	tendon in some specimens, ventrally	Other: Ankle extension	
M. flexor perforans et perforatuss digiti II	FPPDII	Deep fibular tendon of GL muscle	Middle phalanx of digit II, ventrally	Main: Digit II flexion	
				Other: Ankle extension	
M. flexor perforans et perforatus digiti III	FPPDIII	Lateral knee ligaments and FPDIV origin	Middle phalanx of digit III, ventrally	Main: Digit III flexion	
				Other: Ankle extension	
M. flexor perforatus digiti IV	FPDIV	Superficial side of FPDIII origin	Proximal and middle phalanges of digit IV,	Main: Digit IV flexion	
	()		ventrally	Other: Ankle extension	
M. flexor hallucis longus	FHL	2 heads: lateral and caudal aspects of distal femur	Fuses with FDL tendon	Main: Ankle extension; knee flexion	
		near condyles			
M. flexor digitorum longus	FDL	2 heads: proximal tibiotarsus and distal third of	Splits into 3 parts above MTP joint to insert	Main: Digits II, III and IV flexion	
	Û	fibula (3/4 of length)	onto the distal, ventral phalanx of each toe	Other: Ankle extension	
M. extensor digitorum longus	EDL	Cranial proximal tibiotarsus	Dorsal surface of each phalanx	Main: Digits II, III and IV extension; ankle	
				flexion	
	Ō				
	ñ				

Bone	Scaling exponent	Lower 95% Cl	Upper 95% Cl	R ²
Femur	0.38	0.34	0.42	0.96
Tibiotarsus	0.41	0.38	0.45	0.97
Tarsometatarsus	0.44	0.39	0.49	0.96
First Phalanx (Dig III)	0.39	0.33	0.46	0.91

511 **Table 2.** Regression analysis results for the lengths of the four limb bones. The lower 95% boundary

512 (>0.33) demonstrates positive allometry of the tibiotarsus and the tarsometatarsus but results are

513 closer to isometry for the femur and first phalanx of digit III.

M_m vs BM					$L_{f} vs BM$					PCSA vs BM					
Muscle	Outliers	Slope	Lower 95% Cl	Upper 95% Cl	R^2	Outliers	Slope	Lower 95% Cl	Upper 95% Cl	R^2	Outliers	Slope	Lower 95% Cl	Upper 95% Cl	R ²
AMB	0	1.08	0.96	1.21	0.96	0	0.42	0.31	0.57	0.67	0	0.81	0.64	1.03	0.81
CFP	0	1.18	1.09	1.28	0.98	0	0.48	0.31	0.73	0.36	0	0.94	0.78	1.13	0.89
EDL	0	1.25	1.10	1.41	0.95	0	0.54	0.39	0.75	0.64	0	0.82	0.67	1.01	0.86
FCLA	1	1.16	0.95	1.43	0.87	1	0.36	0.24	0.53	0.51	1	0.89	0.73	1.09	0.87
FCLP	0	1.26	1.16	1.36	0.98	0	0.33	0.24	0.44	0.69	0	0.99	0.89	1.09	0.97
FCM	1	1.31	1.16	1.48	0.95	1	0.60	0.39	0.91	0.42	1	0.95	0.75	1.20	0.83
FDL	1	1.29	1.15	1.44	0.96	1	0.58	0.37	0.90	0.36	1	0.93	0.76	1.15	0.86
FHL	1	1.22	1.04	1.42	0.93	1	0.66	0.42	1.04	0.34	1	0.98	0.70	1.37	0.64
FL	0	1.32	1.23	1.42	0.98	0	0.44	0.33	0.58	0.73	0	0.98	0.84	1.16	0.91
FMTIM	0	1.24	1.05	1.48	0.90	0	0.64	0.43	0.97	0.40	0	0.99	0.70	1.41	0.57
FMTL	0	1.19	0.95	1.49	0.83	0	0.43	0.31	0.60	0.64	0	0.86	0.65	1.14	0.73
FMTM	0	1.29	1.05	1.59	0.86	0	0.45	0.29	0.70	0.31	0	0.99	0.80	1.22	0.85
FPDII	0	1.45	1.26	1.67	0.93		-	-	-	-	0	1.40	1.06	1.84	0.74
FPDIII	0	1.34	1.19	1.51	0.95	0	0.60	0.41	0.88	0.47	0	1.03	0.78	1.36	0.74
FPDIV	0	1.20	1.09	1.32	0.97	0	0.43	0.28	0.65	0.38	0	0.99	0.80	1.22	0.85
FPPDII	0	0.75	0.59	0.95	0.81	0	0.74	0.49	1.14	0.37	0	0.68	0.44	1.07	0.29
FPPDIII	0	1.29	1.15	1.45	0.96		-	-	-	-	0	0.98	0.72	1.34	0.67
GIM	0	1.32	1.01	1.73	0.75	0	0.46	0.34	0.63	0.69	0	1.03	0.72	1.48	0.54
GL	0	1.30	1.19	1.43	0.97	0	0.51	0.40	0.67	0.77	0	0.88	0.76	1.01	0.93
GM	0	1.24	1.14	1.33	0.98	0	0.34	0.26	0.43	0.77	0	0.93	0.82	1.06	0.95
IC	0	1.27	1.15	1.40	0.97	0	0.31	0.24	0.39	0.81	0	1.00	0.88	1.13	0.95
IFE	0	1.26	1.11	1.42	0.95	0	0.56	0.42	0.75	0.72	0	0.79	0.66	0.93	0.91
IFI	2	1.22	0.97	1.54	0.85	2	0.49	0.33	0.72	0.57	2	0.92	0.66	1.28	0.68
IB	0	1.32	1.22	1.42	0.98	0	0.36	0.30	0.44	0.89	0	0.98	0.89	1.07	0.97
ILPO	0	1.29	1.16	1.43	0.96	0	0.31	0.21	0.46	0.50	0	1.08	0.92	1.26	0.92
ISF	3	1.10	0.93	1.32	0.92	-	-	-	-		3	1.06	0.73	1.54	0.63
ΙΤϹ	2	1.26	1.14	1.39	0.97	2	0.76	0.61	0.95	0.86	2	0.64	0.50	0.81	0.84
ITCr	0	1.16	0.99	1.36	0.92	0	0.37	0.27	0.50	0.68	0	0.89	0.70	1.13	0.80
ITM	2	1.12	0.83	1.51	0.75	2	0.78	0.49	1.23	0.39	2	0.89	0.55	1.45	0.29
OMII	0	1.23	1.10	1.39	0.95	0	0.73	0.46	1.15	0.27	0	1.05	0.76	1.45	0.65
OMIP	0	1.23	1.11	1.36	0.97	0	0.53	0.36	0.77	0.49	0	0.94	0.77	1.15	0.87
PIFLM	0	1.24	1.13	1.36	0.97	-	-	-	-	-	0	1.11	0.89	1.39	0.83
POP	2	1.44	1.17	1.76	0.88	2	0.68	0.41	1.13	0.22	2	1.15	0.88	1.51	0.79
ТС	0	1.20	1.08	1.33	0.97	0	0.68	0.50	0.93	0.67	0	0.77	0.55	1.07	0.63

515 **Table 3.** Results of RMA linear regression of muscle architecture vs. body mass (BM) for the pelvic limb of *Dromaius novaehollandiae*, across ontogeny. *M_m*,

516 muscle mass (kg); *L*_f, fascicle length (m), *PCSA*, physiological cross-sectional area (m²).

M _{ten} vs BM					L_{ten} vs BM					TCSA vs BM					
Tendon	Outliers	Slope	Lower	Upper	R^2	Outliers	Slope	Lower	Upper	R^2	Outliers	Slope	Lower	Upper	R^2
			95% CI	95% CI				95% CI	95% CI				95% CI	95% CI	
EDL	0	1.26	1.10	1.44	0.94	1	-0.81	-1.07	-0.61	0.75	0	0.86	0.61	1.22	0.58
FCM	0	1.31	1.01	1.69	0.86	0	0.46	0.27	0.79	0.34	0	1.05	0.78	1.43	0.81
FDL	1	1.22	1.08	1.39	0.95	1	0.43	0.36	0.51	0.91	1	0.81	0.70	0.93	0.94
FHL	1	1.29	1.09	1.53	0.91	1	0.45	0.34	0.60	0.74	1	0.87	0.75	1.01	0.93
FL	0	1.33	1.15	1.52	0.94	0	0.39	0.31	0.50	0.81	0	0.99	0.82	1.20	0.88
FPDII	0	1.26	1.03	1.53	0.87	0	0.63	0.40	0.97	0.32	0	1.09	0.76	1.57	0.56
FPDIII	0	1.38	(1)21	1.58	0.94	0	0.43	0.36	0.52	0.88	0	1.01	0.82	1.24	0.86
FPDIV	0	1.17	1.05	1.31	0.96	0	0.42	0.37	0.48	0.95	0	0.76	0.67	0.86	0.95
FPPDII	0	1.34	0.95	1.88	0.60	0	0.78	0.58	1.06	0.69	0	0.80	0.50	1.27	0.24
FPPDIII	0	1.24	1.06	1.44	0.92	0	0.43	0.38	0.49	0.95	0	0.83	0.68	1.03	0.85
GL	0	1.63	(1)19	2.23	0.66	0	0.89	0.59	1.36	0.38	0	0.95	0.69	1.30	0.66
GM	0	0.98	0.78	1.23	0.83	0	0.28	0.18	0.43	0.37	0	0.79	0.64	0.97	0.85
IB	1	1.03	0.79	1.33	0.79	1	0.51	0.35	0.73	0.57	1	0.81	0.53	1.23	0.43
ILPO	2	1.38	0.99	1.93	0.68	2	1.04	0.69	1.56	0.51	-	-	-	-	-
ΙΤϹ	3	1.04	0.81	1.33	0.84	3	0.61	0.44	0.83	0.74	3	0.75	0.46	1.22	0.34
ITCr	1	1.02	0.76	1.36	0.73	-	-	-	-	-	1	1.18	0.80	1.74	0.52
ITM	7	1.37	0.76	2.46	0.43	6	0.72	0.37	1.42	0.09	7	1.19	0.61	2.33	0.21
OMII	0	1.26	0.98	1.62	0.79	0	0.71	0.53	0.94	0.72	0	0.75	0.51	1.10	0.48
OMIP	0	0.99	0.74	1.33	0.70	1	0.48	0.36	0.65	0.71	1	0.67	0.44	1.02	0.43
ТС	0	1.06	0.85	1.30	0.85	0	0.50	0.34	0.73	0.47	0	0.75	0.56	1.00	0.71

Table 4. Results of RMA linear regression of tendon dimensions vs. body mass (BM) for the pelvic limb of *Dromaius novaehollandiae*, across ontogeny. *M*_{ten},

519 tendon mass (kg); *L*_{ten}, tendon length (m); *TCSA*, tendon cross-sectional area (m²).



Figure 1 Schematic anatomical representation of the most superficial layer of muscles, in lateral
 view, of the pelvic limb of an adult emu.

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Figure 2. Schematic anatomical representation of the intermediate layer of muscles, from a lateral
 view, of the pelvic limb of an adult emu.



533 **Figure 3.** Schematic anatomical representation of the deeper layer of muscles, from a lateral view, of

the pelvic limb of an adult emu.



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Figure 4. Normalized relative muscle parameters for individual muscles in emu pelvic limbs of the 16
month old birds only (Group 3; mean body mass 38.5 kg); mean values (error bars showing ±1 S.D.)
are shown. Abbreviations for muscles are in Table 1. The key on the right side of the figure shows
how muscle mass (M_m), physiological cross-sectional area (PCSA), and fascicle length (L_f) were
normalized. L_f values were adjusted to be 1/10 of the actual results in order to be of similar
magnitude to the others. Muscles are organised from top to bottom in decreasing order of muscle

542 mass.

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Figure 5. Ontogenetic scaling exponents and 95% confidence intervals (shown as error bars around 547 548 mean exponent) for muscle mass (red), PCSA (blue) and fascicle length (green) for individual muscles in emu pelvic limbs. Abbreviations for muscles are in Table 1. Dashed lines indicate the expected 549 550 isometric scaling exponent for each parameter. Data are for A) proximal limb muscles and B) distal 551 limb muscles.

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Figure 6. Ontogenetic scaling exponents and 95% confidence intervals for masses of individual muscles in emu pelvic limbs, from the USA group. Abbreviations for muscles are in Table 1. Dashed line indicates the expected isometric scaling exponent (1.0), and the number above each parameter indicates the number of muscles included in each regression analysis.



Figure 7. Ontogenetic scaling exponents and 95% confidence intervals for tendon mass (red),
 average cross-sectional area (blue) and length (green) for 20 individual muscles in emu pelvic limbs.
 Abbreviations for muscles are in Table 1. Dashed lines indicate the expected isometric scaling
 exponent for each parameter.

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