

Tunable Carbon-Dot-Based Dual-Emission Fluorescent Nanohybrids for Ratiometric Optical Thermometry in Living Cells

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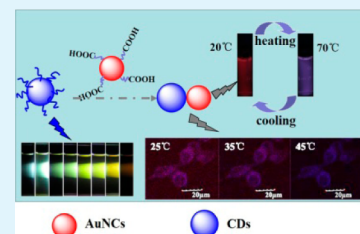
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S Supporting Information

ABSTRACT: The use of carbon-dot-based dual-emission fluorescent nanohybrids (DEFNs) as versatile nanothermometry devices for spatially resolved temperature measurements in living cells is demonstrated. The carbon dots (CDs) are prepared in the organic phase and display tunable photoluminescence (PL) across a wide visible range by adjusting the excitation wavelengths and extend of N-doping. DEFNs are formed in a straightforward fashion from CDs (emitting blue PL) and gold nanoclusters (AuNCs, emitting red PL). The DEFNs display ideal single-excitation, dual-emission with two well-resolved, intensity-comparable fluorescence peaks, and function in optical thermometry with high reliability and accuracy by exploiting the temperature sensitivity of their fluorescence intensity ratio (blue/red). Furthermore, the DEFNs have been introduced into cells, exhibiting good biocompatibility, and have facilitated physiological temperature measurements in the range of 25–45 °C; the DEFNs can therefore function as “non-contact” tools for the accurate measurement of temperature and its gradient inside a living cell.

KEYWORDS: carbon dots, tunable fluorescence, dual-emission nanohybrid, nanothermometry, living cells



1. INTRODUCTION

Temperature is one of the most frequently measured parameters that governs biological reaction within living cells.^{1–3} The accurate measurement of temperature and its gradient inside a living cell can promote advancements in cell biology and biomedicine.^{4–6} To this end, fluorescence-based temperature sensors have shown great potential since they operate as “non-contact” tools and offer the dual functions of cellular imaging and temperature sensing at the molecular level.^{7–9} Many promising fluorescent nanomaterials, such as quantum dots, carbon nanomaterials, rare earth-doped nanoparticles and copper nanoclusters, have been exploited.^{10–13} These optical temperature sensors rely on changes in luminescence intensity as the reporting mechanism (for example, an increase in nonradiative decay rate with temperature leading to decreasing luminescence).^{11,13} However, intensity-based temperature sensors are often susceptible to errors due to changes in probe concentration, the efficiency of excitation or detection, or a lack of specificity for temperature (for example, luminescence may be quenched by oxygen, sensor aggregation, or changes in pH, in addition to the aforementioned reduction due to temperature increase).^{14,15} Changes in the sensor local environment are difficult to control in complicated systems such as cells or microdevices, and can thereby cause inaccurate temperature measurement. Compared with them, dual-emitting sensors show resolvable luminescence emissions from two different excited states.^{16,17} Thus, dual-emitting temperature sensors have attracted much attention since they operate as “non-contact” tools and accurately measure temperature.¹⁸ Several dual-emitting nanomaterials,

such as CdSe/ZnS nanocrystals, rare earth-doped nanoparticles, and polymer dots have shown potential for nanothermometry in biological systems, especially living cells,^{19–21} but high toxicity or instability has limited their further application.

Carbon dots, as an important class of photoluminescence (PL) nanomaterials, have been the subject of extensive research over the past decade because of inherent advantages such as low cost, reduced toxicity, biocompatibility, and excellent photoresponse.^{22–24} Carbon dots (CDs) have been applied widely in the fields of bioimaging, printing inks, photocatalysis, and sensors.^{25–29} Thus, far, CDs have been prepared by both top-down and bottom-up strategies in the aqueous phase.^{30,31} However, such water-based syntheses may suffer from a very broad size distribution (so an additional size selection step is required) and low product yield. Although dual-emitting nanomaterials based on CDs or metal nanoclusters (NCs) have been shown to function as nanosensors for ascorbic acid, Cu²⁺, Hg²⁺, and highly reactive oxygen species,^{16,32–34} there have been no reports thus far of CD/NCs-based dual-emitting probes for ratiometric temperature detection in living cells. The emissions of most CDs are centered in the blue and green regions,^{35–38} which may be unfavorable for biological applications because of the harm that short-wavelength radiation may cause to living cells or biosystems. The synthesis of CDs with broad-range tunable fluorescence therefore remains a major challenge.

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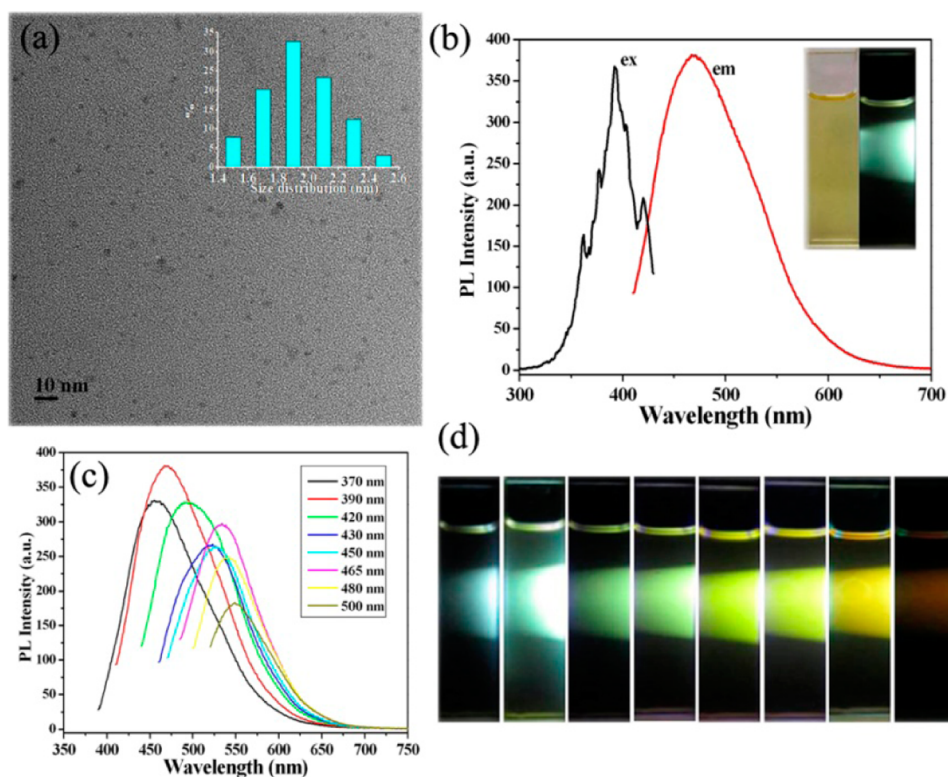


Figure 1. (a) TEM image of the CDs; (a, inset) size distribution, the average size being 1.9 ± 0.2 nm; (b) excitation (ex) and emission (em) spectra of the CDs in chloroform solution; (b, inset) photographs of solutions of the fluorescent CDs under (left) room light and (right) UV light illumination; (c) fluorescence spectra of the CDs in chloroform solution with different excitation wavelengths; (d) fluorescence images of the CDs in chloroform solution.

Herein, we report a novel colloidal synthesis of CDs capped by oleic acid (OA) and oleylamine (OLA). These CDs were dispersed in chloroform, exhibiting tunable excitation-dependent emission in the visible light region: by controlling the mole ratio of OLA to OA and thereby modifying the extent of N doping,^{39–41} the resultant CDs displayed tunable fluorescence with emission wavelengths varying from 430 to 550 nm. With the aid of cysteamine, the resultant CDs were transferred from the organic phase to the aqueous phase. Dual-emission fluorescent nanohybrids were formed by carbodiimide-activated coupling of glutathione-stabilized gold nanoclusters (GSH-AuNCs, red PL) and amino-functionalized CDs (blue PL).^{42–44} These novel DEFNs can be used as versatile nanothermometry devices, because their fluorescence intensity ratio (blue/red) correlates strongly with temperature and varies considerably over a wide temperature range (20–75 °C).

2. EXPERIMENTAL SECTION

2.1. Materials. Reduced glutathione (GSH, molecular weight of $307 \text{ g}\cdot\text{mol}^{-1}$), 1-octadecene (ODE, 90%), oleic acid (OA, 90%), 1-ethyl-(3-(3-dimethylamino)propyl)carboxylate hydrochloride (EDC), *N*-hydroxysuccinimide sodium (NHS), cysteamine and oleylamine (OLA, 70%) were purchased from Sigma-Aldrich. Citric acid monohydrate (CA), tetrachloroauric(III) acid (HAuCl_4), chloroform, methanol, isopropanol and acetone were purchased from Sinopharm Chemical Reagent Co., Ltd. (China). All the chemicals were used as received without further purification.

2.2. Synthesis of Organic-Soluble Carbon Dots. The mixture of CA (0.042 g, 20 mmol), OA (1 mL, 2.9 mmol), OLA (3 mL, 6.2 mmol), and ODE (6 mL, 17 mmol) was degassed at room temperature and heated up to 100 °C under vacuum for 0.5 h with stirring. The resultant homogeneous solution was placed under a dry

nitrogen atmosphere, heated to 250 °C slowly and maintained at this temperature for 1 h. The color of the solution became transparent on raising the temperature and finally became dark brown. The temperature of the solution was reduced below 100 °C. The resultant carbon dots were precipitated by addition of acetone, rinsed with methanol, and then redispersed in 20 mL of chloroform for further use. Using a similar method, other samples with different size were prepared under similar experimental conditions.

2.3. Synthesis of GSH-AuNCs. As per the previously reported method, GSH-AuNCs were prepared through reduction of $\text{HAuCl}_4 \cdot 3\text{H}_2\text{O}$ with GSH.⁶ Typically, HAuCl_4 (50 mM, 0.5 mL) and GSH (5 mM, 20 mL) were mixed in a 100 mL round-bottom flask at room temperature. The mixture was stirred at room temperature for 10 min and was heated at 100 °C for 6 h. Purification of the resultant GSH-AuNCs was effected by centrifuging at 12 000 rpm to remove large particles. The supernatants were collected and then dialyzed with deionized water and a dialysis bag (MW cutoff 1000 Da) to purify the AuNCs from unreacted species. The resultant AuNCs were stored at 4 °C for further use.

2.4. Synthesis of Dual-Emission Fluorescent Nanohybrids.

The hydrophobic CDs were further functionalized with thiol compounds, such as cysteamine, which enabled the phase transfer of CDs from hydrophobic to hydrophilic media.³⁸ In a typical process, 0.5 mL of the aforementioned CDs (3.0 mg mL^{-1}) in chloroform was added to 10 mL of cysteamine solution (5 mg mL^{-1}). A subsequent ultrasonication (~ 15 min) led to a stable white emulsion. With vigorous stirring at 60 °C for 12 h, a transparent solution was formed. After centrifugation to remove the large nanoparticles and dialysis with deionized water to remove free cysteamine, the hydrophilic CDs were collected by freeze-drying.

The dual-emission fluorescent nanohybrids (DEFNs) were built through carbodiimide-activated coupling between GSH-AuNCs and amino-functionalized CDs. In a typical process, 15 mg of EDC and 9 mg of NHS were added to 2 mL of PBS buffer (pH 6.86) containing

10 mg of GSH-AuNCs. The mixture was treated by sonication in the dark at room temperature for 30 min, and then mixed with 2 mL of an aqueous solution containing 20 mg of amino-functionalized CDs. This solution was allowed to react under magnetic stirring for 8 h. Finally, the resultant nanohybrids were precipitated by the addition of 20 mL of isopropyl alcohol, collected through centrifugation at 12 000 rpm, and then redispersed in 10 mL of aqueous solution for further application.

2.5. Temperature Measurement of Living Cells. First, 293T cells were grown on a circular coverslip (diameter 18 mm) overnight at 37 °C and 5% CO₂. Subsequently, the cells were incubated with 10 μg mL⁻¹ DEFNs in serum-free DMEM for 2 h, washed with PBS and fixed with 1 mL of 4% (by mass) paraformaldehyde in PBS for 15 min. The cells were then washed with warm PBS to remove the excess DEFNs. Prior to inspection with a confocal fluorescence microscope, the sample temperature was adjusted using a heater that controlled the in situ temperature of cells during the microscopy observation. For each point, the temperature was set and equilibrated for 5 min before the spectral measurements. The confocal microscopy images were taken using an Olympus Fluoview FV1000.

2.6. Characterization. Photoluminescence experiments were performed with a Shimadzu RF-5301 PC spectrofluorimeter (Shimadzu, Japan). UV-vis absorption spectra were obtained using a TU-1991 UV-vis spectrophotometer. X-ray photoelectron spectroscopy (XPS) with Mg K α excitation (1253.6 eV) was collected using a VG ES-CALAB MKII spectrometer (ThermoFisher Scientific, USA); the binding energy was calibrated with C 1s at 284.6 eV. Fourier transform infrared spectroscopy (FTIR) was measured in the range of 500–4000 cm⁻¹ using a Nicolet 6700 FTIR spectrophotometer. Transmission electron microscopy analyses to study the morphology and mean diameter of the resultant samples were carried out on a JEM-2100F (FEI, USA), operating at an accelerating voltage of 200 kV. Dynamic light scattering (DLS) and Zeta potential measurements were performed using a Zetasizer NanoZS (Malvern Instruments). The confocal microscopy images were observed under a confocal fluorescence microscope (FV1000, Olympus).

3. RESULTS AND DISCUSSION

The carbon dots (CDs) were prepared by the colloidal synthesis method described in the [Experimental Section](#). Citric acid (CA) was adopted as the C source and was carbonized at high temperature. The resultant CDs were stabilized in situ by OA and OLA. The morphology and structure of the CDs were confirmed by various analyses. [Figure 1a](#) shows a transmission electron microscopy (TEM) image of the CDs, revealing that the CDs are distributed without apparent aggregation, and that the diameters of the particles are ca. 1.5–2.5 nm, with the average value being 1.9 ± 0.2 nm (inset of [Figure 1a](#)). The surface groups were also investigated by X-ray photoelectron spectroscopy (XPS) ([Figure S1](#)). A high-resolution XPS spectrum in the C 1s window ([Figure S1](#)) revealed the presence of C–C or C=C, C=O, and C–N bonds, which mostly stem from carbogenic cores, surface carbonyl groups, and surface-bound oleylamine molecules, respectively.^{39,45} In chloroform, the optimal excitation and emission wavelengths of the CDs are 390 and 470 nm, respectively ([Figure 1b](#)). A diluted solution of the as-prepared CDs in chloroform appeared pale yellow under visible light (inset of [Figure 1b](#)), while emitting blue-green fluorescence under UV light illumination (inset of [Figure 1b](#)). The as-prepared CDs in the present studies also exhibited excitation-dependent emission behavior without an accompanying significant decrease in fluorescence emission intensity, due to the size distribution (1.5–2.5 nm) and the novel colloidal method. As shown in [Figure 1c](#), when the CDs were excited at wavelengths progressing from 370 to 500 nm, the corresponding emission peaks shifted concom-

itantly from 456 to 550 nm while maintaining comparable intensities. The strongest photoluminescence (PL) peak appeared at 470 nm upon 390 nm excitation, which is consistent with the photoluminescence excitation (PLE) and PL spectra shown in [Figure 1b](#). The as-prepared CDs exhibited selective emission across a broad color range from blue to orange ([Figure 1c,d](#)); such excitation-dependent PL behavior is common for fluorescent CDs and useful in multicolor imaging applications.^{46–50}

The PL properties of CDs can be influenced by quantum size effects, surface states, zigzag sites, and so on.^{51–53} Previous reports had ascertained that CDs possessing tunable emission wavelengths could be prepared by adjusting the extent of N, S or P doping.⁴³ In the present study, we modified the ratios of OA/OLA to vary the N amount on the surface of the resultant CDs. As shown in [Figure S2](#), upon increasing the amount of OLA, the room temperature PL emission exhibited a significant red shift, from 430 to 550 nm. The emission wavelengths of the samples span blue, cyan, and yellow, with the emission sufficiently bright that it can be readily detected with the naked eye (inset of [Figure S2](#)). TEM images are shown in [Figure S3](#), demonstrating that the as-prepared CDs were well-dispersed, and with an average size that decreased with increasing content of OLA, and thereby N content, the latter being confirmed by XPS ([Figure S4](#)); the extent of N doping correlates with the redshift of the emission of the CDs (i.e., the fluorescence is tunable).^{51–53}

The organic solvent-soluble CDs can be easily transferred to the aqueous phase by using thiol compounds, such as cysteamine.^{39–41} In aqueous solution, the cysteamine-CDs were well dispersed, emitting blue light ([Figure S5](#)). Fourier transform infrared (FTIR) spectroscopy ([Figure S6](#)) was employed to identify the functional groups present on the surfaces of the CDs in aqueous solution; while the intensity of the characteristic S–H stretching band decreased, the bands characteristic of the other functional groups of cysteamine were still present, supporting the proposed formation of amino-functionalized CDs ([Figure S6](#)).

Glutathione-stabilized gold nanoclusters (GSH-AuNCs) were then prepared, displaying red fluorescence centered at 605 nm. The as-prepared GSH-AuNCs were well-dispersed in aqueous solution, with an average size of ca. 2.4 nm ([Figure S7](#)),⁵⁴ due to the presence of GSH on the surface of the AuNCs, the surface modification being beneficial for subsequent applications.^{55–57} Our DEFN-based temperature sensor was then assembled through carbodiimide-activated coupling of the GSH-AuNCs and the amino-functionalized CDs ([Figure 2a](#)).^{42,43} A typical TEM image ([Figure 2b](#)) revealed peanut-like and monodisperse nanohybrids. The average size of the nanohybrids was ca. 5 nm, which is consistent with CD-AuNC addition. The CD and AuNC content in the peanut-like nanostructure was clearly seen by high resolution TEM (HRTEM; inset of [Figure 2b](#)). Dynamic light scattering measurements confirmed the size of the DEFNs, with a number-averaged diameter of ~ 4.8 nm, which is in agreement with the results from TEM ([Figure S8](#)). As shown in [Figure S9](#), the maximum absorption peaks of the CDs and AuNCs are in the UV region. Therefore, a 365 nm wavelength laser could excite both materials in the hybrid sensor, and indeed under 365 nm excitation, the nanohybrid system exhibited two well-resolved emission peaks at 430 and 605 nm ([Figure 2c](#)). There is a narrow overlap between the absorption spectrum of the AuNCs and the PL spectrum of the

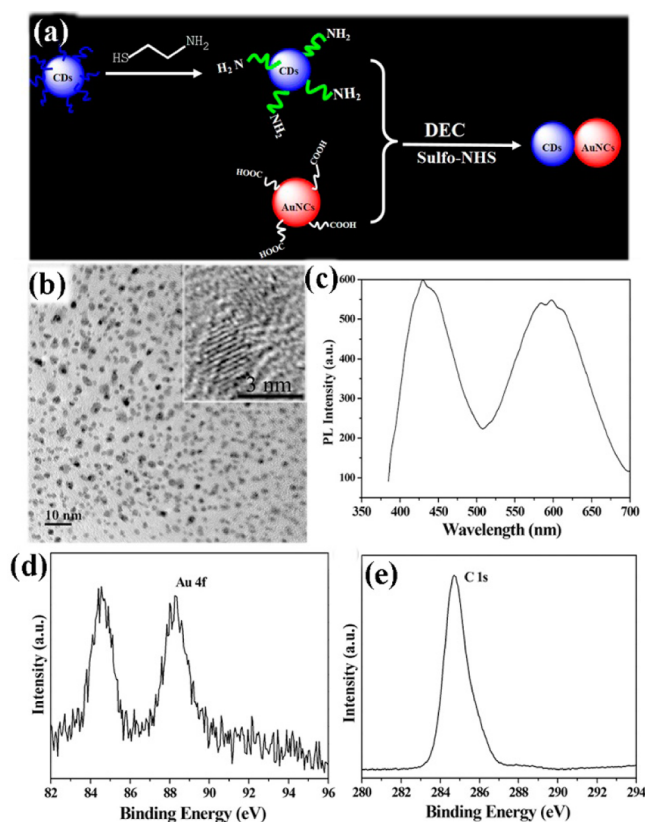


Figure 2. (a) Schematic illustration of the synthesis of the DEFNs from CDs and GSH-AuNCs; (b) TEM and (inset) HRTEM images of the DEFNs; (c) fluorescence spectrum of the DEFNs in aqueous solution; (d) Au 4f XPS spectrum of the DEFNs; and (e) C 1s XPS spectrum of the DEFNs.

CDs, but in the overlap range, the PL of the CDs was rather weak. Moreover, the PL quantum yields (QYs) of the AuNCs and the CDs were found to be 5.5% and 3.8% using quinine sulfate (0.1 M H_2SO_4 as solvent; QY = 0.54) as a reference. After forming the DEFNs, the QYs were 5.8% (AuNCs) and 3.3% (CDs), respectively, so the energy transfer between the AuNCs and the CDs in the DEFNs was trivial. The elemental composition of the nanohybrids was confirmed by XPS. The Au 4f binding energies (88.1 and 84.3 eV; Figure 2d) are consistent with the electronic structure of AuNCs,^{58,59} while the C 1s binding energy matched those of previously reported CDs (Figure 2e).^{41,45} The purity of the DEFNs was confirmed by gel electrophoresis (Figure S10). It was possible to track the movement of the nanomaterials along the gel due to their different Zeta potentials, particle size and so on. The GSH-AuNCs did not move at all since their Zeta potential was about 0 mV (Figure S10a). Instead, the movement of NH_2 -CDs (belt b) and DEFNs (belt a) were observed under UV light. The speed of the DEFNs (belt a) was less than that of the NH_2 -CDs (belt b) along the gel, which was consistent with the results of Zeta potentials (Figure S10). The bright and narrow signal of the DEFNs (belt a in lane 3) clearly indicated that the nanohybrids were highly pure and uniform, while only a weak NH_2 -CDs signal (belt b in lane 3) was observed (Figure S10b). The CD-AuNCs therefore preserved the composition and structure of the constituent CDs and AuNCs, confirming the successful synthesis of the dual-emission nanohybrids.

To explore the potential applications of the DEFNs in intracellular nanothermometry, we investigated their temper-

ature-dependent response. The PL spectra of the DEFNs were measured at temperatures ranging from 20 to 75 °C. The measurements were conducted with both increasing and decreasing temperature to ensure reproducibility, the resulting PL spectra being shown in Figure 3a and Figure S11a. GSH-AuNCs have been used as nanothermometry devices because of the temperature sensitivity of their fluorescence lifetime and emission intensity;⁶ the nonradiative recombination of electrons and holes increases as the temperature increases, whereas the radiative transition rate remains constant, reducing the fluorescence intensity corresponding to emission from the excited state.^{13,60} Thus, upon increasing the temperature, we observed a concomitant decrease in intensity of red emission from the GSH-AuNCs, while the blue emission from the CDs changed little (Figure 3a and Figure S11a). Although the fluorescence of the CDs in the DEFNs differed little with temperature change, the fluorescence of the AuNCs decreased rapidly with increasing temperature. A linear relationship was observed between the ratios of emission intensities at the two emission wavelengths (I_{430}/I_{605}) and the temperature (Figure 3b). Thus, the varying fluorescence of the CDs with temperature changes did not affect the efficient function of the DEFNs as a ratiometric temperature sensor. Unlike semiconductor QDs,^{10,61} which display remarkable temperature-dependent spectral shifts, the emission spectra of CDs and NCs do not shift within the investigated temperature window. The changes in the intensities of the two emission peaks resulted in a continuous fluorescence color variation (inset of Figure 3b). The fluorescence at 605 nm decreased with increasing temperature, and was accompanied by a distinguishable fluorescence color change from red to violet. To obtain sensitivity information, the blue bands at 430 nm were normalized, the resultant PL spectra being shown in Figure S12. For the red band, the PL intensity decreased by 99.0% with a temperature variation of 75 °C, indicating a sensitivity of approximately $1.8\% \text{ } ^\circ\text{C}^{-1}$, which is competitive with previous reports.^{9,21,62–64} The fluorescent nanosensor therefore functioned as an ideal ratiometric temperature sensor with high reliability and accuracy. A Commission Internationale de L'Eclairage (CIE) 1931 chromaticity diagram in the temperature range of 20–70 °C showed that the system color shifts between red and violet (Figure 3c), consistent with the PL spectra of Figure 3a. The reproducibility of the emission intensity measurements at the different temperatures indicated that the DEFNs have excellent stability over the temperature range. The luminescence switching operations were repeated for six consecutive heating and cooling cycles between 20 and 60 °C (Figure 3d; see corresponding spectra in Figure S13). This fatigue-resistant performance suggests that the DEFNs may be applicable as PL thermometers and biosensors in cell monitoring.

As has been previously reported, the fluorescence of CDs and GSH-AuNCs show high stability.^{11,58} After forming the DEFNs, the dual fluorescence and the fluorescent intensity ratios did not change over the entire physiologically relevant pH range of 4–9 (Figure S14a), in the presence of the physiological ionic strength (Figure S14b), in the presence of biomolecules (Figure S14c) and after exposing the DEFNs to a 500 W Xe lamp for 150 min (Figure S14d). Therefore, the as-prepared DEFNs from the present study possess high stability and are particularly appropriate for practical applications. This dual-emission fluorescent temperature sensor was also assayed in 10 mM phosphate-buffered saline (PBS) solution (pH 7.4,

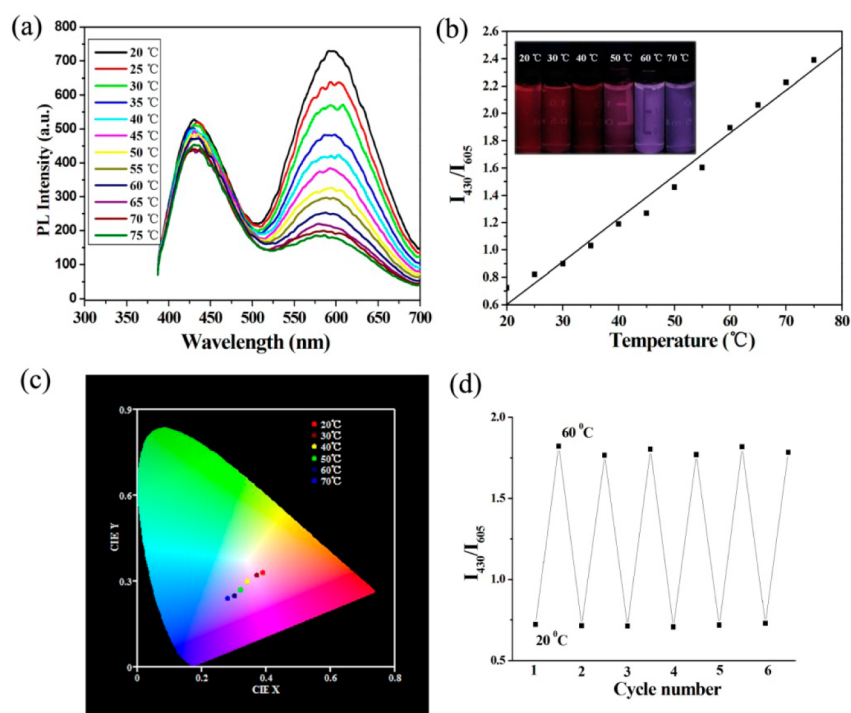


Figure 3. (a) Fluorescence spectra (excitation 367 nm) of DEFNs with an increase of temperature from 20 to 75 °C (top to bottom); (b) the ratios of the emission intensities at 430 and 605 nm (I_{430}/I_{605}) versus temperature; (inset) photographs of DEFNs at various temperatures under a UV lamp with an excitation wavelength at 365 nm; (c) CIE chromaticity diagram showing the temperature dependence of the (x,y) color coordinates of the DEFNs; (d) temperature-induced switching of the emission intensities ratio of the DEFNs (alternating between 20 and 60 °C).

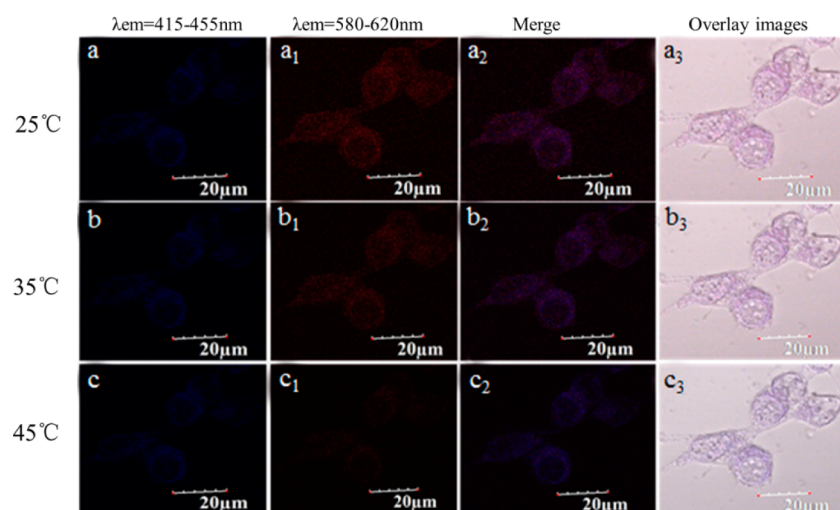


Figure 4. Confocal fluorescence microscopy images of 293T cells with internalized DEFNs at three different temperatures: (a) 25, (b) 35, and (c) 45 °C. Fluorescence images at (1) the blue channel and (2) the red channel; (3) overlap of the fluorescence images; and (4) corresponding bright field images.

Figure S15a), with the ratios of fluorescence intensities showing a linear relationship with increasing temperature over the range 20 to 45 °C (Figure S15b). This temperature range is larger than the physiological temperature range, suggesting that the DEFNs have considerable potential for in vivo temperature sensing applications. Toxicity is a major factor that needs consideration in the design of an intracellular sensor system for subsequent biological applications. To evaluate the cytotoxicity of the DEFNs, we conducted a thiazolyl blue tetrazolium bromide (MTT) assay on cells loaded with DEFNs.^{65,66} As shown in Figure S16, the viability of the 293T cells remained

above 80% following incubation with the DEFNs, even at a concentration of 100 μg/mL for 24 h, considerably more forcing conditions than those used for cell incubation and imaging. The results confirm that the as-prepared nanohybrids are biocompatible and have low toxicity and can therefore be used in optical thermometry in living cells.

The utility of the DEFN thermometers in monitoring intracellular temperature was investigated using confocal fluorescence microscopy; 293T cells were selected as a model system, and three samples under different environmental temperatures were tested, as shown in Figure 4. After

incubating with the DEFNs, the 293T cells maintained their normal morphology, consistent with good biocompatibility of the DEFNs. The blue and red channels both displayed fluorescence signals with typical cytosolic colocalization. The DEFNs were therefore delivered rapidly into the cytoplasm and maintained their dual-emission characteristics. Upon increasing the temperature, the fluorescence emission color of the probe changed from red (Figure 4a₃) to violet (Figure 4c₃), consistent with the changes in the fluorescence spectra observed in aqueous solution and PBS solution. These changes were clearly observed in the separate channels in Figure 4; upon increasing the temperature, the red fluorescence image from the AuNCs became dimmer whereas the blue reference channel showed almost no change. The results confirmed the potential of carbon-dot-based dual emission nanohybrid systems in sensing temperature profiles at the subcellular level and, more broadly, highlight their potential in fundamental biology research.

4. CONCLUSION

In summary, fluorescent CDs were prepared in the organic phase. These CDs exhibited excitation-dependent emission behavior, with PL peaks varying from 456 to 550 nm, and N-doping-dependent tunable PL emission in the range of 430–550 nm. Carbon-dot-based DEFNs were fabricated through condensation between carbodiimide-activated GSH-AuNCs and amino-functionalized CDs. The DEFNs displayed ideal single-excitation, dual-emission behavior with two well-resolved, intensity-comparable fluorescence peaks. These features render the DEFNs very attractive due to their capacity to enhance imaging contrast and accuracy. The DEFNs are sensitive sensors for quantitative ratiometric detection of external environmental temperature with good reproducibility. The DEFNs were also employed to monitor intracellular temperature differences (25–45 °C) in living cells. Because of their facile synthesis, attractive fluorescence properties, and excellent biocompatibility, the DEFNs are promising candidates for cellular imaging and temperature sensing at the molecular level.

■ ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsami.5b11317.

Additional emission spectra, FTIR spectra, XPS analysis results, UV–vis spectra, TEM images, DLS, Zeta potentials, and MTT results. (PDF)

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Notes

The authors declare no competing financial interest.

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