

Nanoscale Horizons

Accepted Manuscript



This article can be cited before page numbers have been issued, to do this please use: K. M. Pondman, C. Salvador-Morales, B. Paudyal, R. B. Sim and U. Kishore, *Nanoscale Horiz.*, 2017, DOI: 10.1039/C6NH00227G.



This is an Accepted Manuscript, which has been through the Royal Society of Chemistry peer review process and has been accepted for publication.

Accepted Manuscripts are published online shortly after acceptance, before technical editing, formatting and proof reading. Using this free service, authors can make their results available to the community, in citable form, before we publish the edited article. We will replace this Accepted Manuscript with the edited and formatted Advance Article as soon as it is available.

You can find more information about Accepted Manuscripts in the [author guidelines](#).

Please note that technical editing may introduce minor changes to the text and/or graphics, which may alter content. The journal's standard [Terms & Conditions](#) and the ethical guidelines, outlined in our [author and reviewer resource centre](#), still apply. In no event shall the Royal Society of Chemistry be held responsible for any errors or omissions in this Accepted Manuscript or any consequences arising from the use of any information it contains.

Interactions of the innate immune system with carbon nanotubes

Kirsten M. Pondman^{a,b}, Carolina Salvador-Morales^c, Basudev Paudyal^{a,d}, Robert B. Sim^e,
Uday Kishore^{a*}

^aDepartment of Life Sciences, College of Health and Life Sciences, Heinz Wolff Building,
Brunel University London, Uxbridge UB8 3PH, UK

^bNeuro Imaging, MIRA Institute, University of Twente, Enschede, The Netherlands

^cBioengineering Department and Krasnow Institute for Advanced Study, George Mason
University, 4400 University Drive MS 1G5, Fairfax, VA 22030, USA

^dFaculty of Science, Engineering and Computing, Penrhyn Road, Kingston upon Thames,
Surrey, KT1 2EE

^dDepartment of Pharmacology, University of Oxford, Oxford, UK

*Corresponding author: Dr Uday Kishore (uday.kishore@brunel.ac.uk;
ukishore@hotmail.com)

Key words: carbon nanotubes; innate immunity; complement; cytokine; macrophage;
inflammation

Running title: CNTs and innate immune response

Abstract

The therapeutic application of nanomaterials requires that they are biocompatible and can reach the desired target. The innate immune system is likely to be the first defence machinery that would recognise the nanomaterials as 'non-self'. A number of studies have addressed the issue of how carbon nanotubes (CNTs) interact with phagocytic cells and their surface receptors that can impact on their intracellular processing and subsequent immune response. In addition, soluble innate immune factors also get involved in the recognition and clearance of CNTs. The interaction of CNTs with the complement system, the most potent and versatile innate immune mechanism, has shed interesting light on how complement activation on the surface of CNTs can modulate their phagocytosis and effector cytokine response. The charge or altered molecular pattern on the surface of CNTs due to functionalization and derivatisation can also dictate the level of complement activation and subsequent inflammatory response. It is becoming evident that complement deposition may facilitate phagocytic uptake of CNTs through receptor routes that leads to dampening of pro-inflammatory response by complement-receptor bearing macrophages and B cells. Thus, recombinant complement regulators decorated on the CNT surface can influence the therapeutic strategies involving CNTs and other nanoparticles.

Introduction

CNT characteristics and applications

Since Iijima described their synthesis in 1991¹ carbon nanotube (CNT)-based nanotechnology has rapidly emerged as a platform for a variety of uses, including many biomedical applications². CNTs can be described as cylindrical tubes, composed of rolled graphene, with the carbon atoms hybridized in hexagonal sp² arrangement and consist of honeycomb lattices and are seamless structure. Each atom is joined to three other neighbour atoms just like in graphene. The type of CNTs depends on the orientation of the rolling of graphene sheet. Based on the rolling orientation of graphene sheet, CNTs are classified as arm chair, zigzag and chiral nanotubes³. CNTs can be described as cylindrical tubes, composed of rolled graphene, with the carbon atoms hybridized in hexagonal sp² arrangement. Depending on the number of concentric carbon tubes, they can be divided into single-walled (SWNT), double-walled (DWNT) and multi-walled (MWNT) carbon nanotubes (Figure 1a-b). A principal characteristic is their high aspect ratio, resulting from their small diameter (1-3 nm for SWNT up to 2-100 nm for MWNTs) and extended length (up to 500 μ m), which arise from their method of synthesis⁴. CNTs are grown on a substrate, either with or without (metallic) catalyst particles; the preparation methods include arc discharge, laser ablation and chemical vapour deposition (Figure 1c)⁵.

Biomedical applications of CNTs include drug delivery⁶⁻¹¹, immunoassays¹² and scaffold^{13,14}. In combination with magnetic filling or particles, CNTs can be used as an MRI contrast agent¹⁵⁻²⁰, and in hyperthermia treatment^{21,22}. As their most promising application, CNTs as drug delivery platforms have been reviewed extensively elsewhere^{6,23-25}. The large surface area of CNTs offers a substantially higher drug loading capacity, compared to other nanoparticles while the dimensions of CNTs allow for entry in the smallest capillaries²⁶. Compatible with the requirement for targeted drug delivery, CNTs are able to cross the cell and nuclear membrane²⁷⁻³⁰. Drugs can be either entrapped inside the CNTs³¹, or absorbed or attached on the surface^{9,10,32}. Using these methods, CNTs have been shown to be versatile carriers for a range of drugs^{6,11,23,25,32-37}, genes³⁸, proteins³⁹ and peptides²⁸. The drugs can, in principle, be delivered to specific targets (e.g. tumours) by attaching target-specific molecules (e.g. antibodies)^{40,41}.

In order to be used for a variety of applications, CNTs have to be individually dispersed in physiological buffers. Owing to their hydrophobicity, strong π - π interactions and length, CNTs are prone to rope and cluster formation; therefore, functionalizing or coating CNTs is essential⁴². Non-covalent modifications of the CNT surfaces include pre-coating with proteins⁴³, surfactants⁴⁴, synthetic polymers⁴⁵ and nucleic acids⁴⁶. Covalent functionalization involves introducing new functional groups on the external walls, usually beginning with the oxidation of the walls creating defects and carboxyl groups⁴⁷. The biocompatibility of CNTs can only be achieved by the covalent or non-covalent functionalization of their surface^{34, 48-51}.

In all biomedical applications, permanent or transient contact between CNTs and blood, cells or tissues is unavoidable, and, hence, an encounter with the immune system. These interactions may lead to severe inflammatory responses and tissue damage⁵², which is likely to interfere with the tissue targeting or intended destination of the CNTs. It is, therefore, essential to study and understand the interactions between CNTs and all components of the immune system. In this review, we focus on the interactions of CNTs with the innate immune system, the body's first line of defence, which is likely to have the largest influence on host-CNT interaction.

The innate immune system

The immune system is responsible for protection against micro-organisms (bacteria, fungi, viruses and parasites). In addition, altered or damaged cells and tissues are also cleared via the cellular and molecular immune components. Recognition of these altered self or non-self materials (e.g. synthetic nanoparticles) is mediated by specific proteins, which bind to their targets and trigger downstream effector functions with the goal of eliminating the imminent danger to homeostasis. The human immune system consists of a complex conglomeration of interacting proteins and cells. In order to enhance short and long term efficiency of the clearance mechanisms, the immune system operates via two wings: innate immunity (rapid and broad in specificity) and adaptive immunity (slow and highly specific). The innate immune system involves proteins, always present in the blood, body fluids and tissues, while in adaptive immunity new recognition proteins (e.g. antibodies) are generated specifically towards a newly presented threat.

A major part of the innate immune system response involves opsonisation of the target (e.g., a pathogen) by proteins of the complement system, migration and activation of phagocytic cells, mainly macrophages and immature dendritic cells (DCs). The complement system consists of more than 40 soluble and cell surface proteins, working together via three activation pathways in order to recognise and opsonise foreign and altered-self components (Figure 2)⁵³. The recognition proteins of the complement system work through “multiple low-affinity binding”. A single binding between the recognition protein with its target, which can be a molecular motif such as a charge cluster, single neutral sugar, vicinal hydroxyl groups or a single acetyl group, is not strong enough to hold the target and the complement recognition protein together. Therefore, the recognition proteins have a multimeric structure with multiple contact/binding sites. The complement cascade is only activated when multiple bonds are formed allowing for a strong interaction.

The complement classical pathway is initiated by C1q (Figure 3), a charge pattern recognition protein (460 kDa), consisting of 18 homologous polypeptide chains (6A, 6B and 6C chains) each consisting of a short N-terminal region, followed by a collagen like region with repeating Gly-X-Yaa triplets, and a heterotrimeric globular head (gC1q) domain composed of C-terminal region of A, B and C chains (ghA, ghB and ghC, respectively) (Figure 3). The gC1q domain binds to charge clusters or hydrophobic patches on the targets which can be altered or non-self ligands⁵⁴. In the lectin pathway, the recognition proteins include mannan-binding lectin (MBL) that mainly binds to vicinal diols on sugars such as mannose, fucose or glucosamine; collectin 11 (CL-11) that binds to more complex glycan motifs; or one of the three ficolins (L-,H- and M-ficolin) that bind to acetyl groups and possibly other motifs⁵⁵. After C1q is bound to its targets, proteases C1r and C1s are activated (or for MBL, CL-11 and ficolins, MBL-associated serine proteases, MASP-1, 2 and 3, are activated). This then activates complement proteins C4 and C2 forming a C3 convertase (C4b2a), which cleaves C3 to form C3b that then binds to the target surface. C3b and its breakdown products, iC3b and C3dg, interact with C3 receptors on phagocytic and other cells. C3b is also a binding site for C5, which is activated by the same protease which cleaves C3, and then forms a complex with C6, C7, C8 and C9 (C5-9), called membrane attack complex (MAC), which disrupts the lipid bilayer of cells (Figure 2)⁵⁵.

The activation of the complement alternative pathway involves a constant slow hydrolysis of C3 in solution, which forms C3(H₂O), and alters the shape of the protein. This conformational change allows the formation of a complex between factor B and C3(H₂O), which allows factor D to cleave the bound factor B into Ba, which is removed and Bb, which remains bound. C3(H₂O)Bb is a protease which cleaves more C3 to form C3b, which can bind to target surfaces, and form a complex with factor B, which is converted to C3bBb, by factor D, as above. This leads to coating of the target particle with C3bBb, which is a homologue of the classical pathway C3 convertase, C4b2a. C3bBb, the alternative pathway C3 convertase, can be further stabilized by properdin (factor P) to C3bBbP. This complex is an enzyme able to generate more C3b to bind to targets. This is an amplification mechanism in order to increase turnover of C3 and coating of targets with C3b. To avoid consuming all available C3, the amplification mechanism needs to be balanced by down regulators: Factor H binds to C3b inhibiting C3 convertase formation, and together with factor I it cleaves C3b to iC3b, which is unable to form C3bBb⁵⁵⁻⁵⁷.

After the complement proteins have tagged a particle (opsonisation), there follows interaction with cell bound receptors (e.g. red blood cells through CR1/CR35, a receptor for C3b) and phagocytosis (via CR3 and CR4, which are receptors for iC3b). These complement-receptor interactions also promote uptake of complement-activating targets by DCs. Once immature DCs ingest an antigen, they undergo a directed activation and maturation towards becoming a potent antigen presenting cell (APC), after which they migrate towards lymph nodes. This makes DCs the main link between the innate and adaptive immune system, as they provide signals for T lymphocytes with the specific receptors for the presented epitopes to become activated⁵⁸.

Interactions of CNTs with human plasma proteins

CNTs not only interact with components of the immune system but also show highly specific interactions with other soluble plasma proteins⁵⁹. The bound proteins form a corona, which plays an important role in determining the effective size, surface charge, physicochemical properties and aggregation state of the nanoparticles⁶⁰. In addition, it changes the recognition patterns, possibly presenting novel peptide or glycan motifs to the immune

system, and can therefore alter the nature of interaction with the complement system, cells and ultimately immune response and bio-distribution⁶¹⁻⁶⁴.

The composition of the protein corona changes with time, depending on the binding affinities and stoichiometry of the nanocarrier and proteins⁶⁵. Affinities can be affected by surface properties such as available functional groups, but also the surface area and curvature. In general, a nanocarrier will be first covered by the most abundant plasma proteins (e.g. albumin and fibrinogen). These proteins are then replaced by proteins with higher affinity towards the particle surface, a process called the "Vroman effect"⁶⁶⁻⁶⁸. The initial coating on the CNT can influence the binding of proteins, as some proteins have affinities towards charge, hydrophilicity, nucleic acids or carboxyl groups⁶⁶.

Oxidation of CNTs offers a more negatively charged surface, which binds more protein^{69,70}. Shannahan et al. have performed an extensive proteomics analysis to identify the proteins in the corona of SWNTs (1 nm) and MWNTs (20-30 nm) unmodified, PVP (Polyvinylpyrrolidone) coated, or oxidised⁷⁰. All CNT coronas contained 14 common proteins: serum albumin, titin, apolipoprotein-A-I, apolipoprotein A-II, α 1-anti-proteinase, α 2-HS-glycoprotein, α -S1-casein and keratin. A much larger variety of proteins was found to bind only onto specific types of CNTs. A similar binding profile was found by Salvador-Morales et al., but it was reported that more albumin bound to chemically modified MWNTs, suggesting that the plasma could enter the larger diameter MWNTs by capillary forces; these entrapped proteins are likely to be difficult to wash out^{71,72}. Cai et al. showed that larger diameter CNTs were also able to bind a wide range of proteins on their surfaces, although increasing the diameter of CNTs above 20 nm did not have any additional effect⁷³.

Complement absorption and activation

Certain components of the corona, opsonins, which include IgG, complement proteins and fibrinogen, may enhance uptake of the nanoparticles by macrophages and other cells of the reticulo-endothelial system^{48,64}. The importance of complement activation by nanoparticles used in drug targeting was highlighted by a study on liposome-encapsulated-doxorubicin. After hypersensitivity reaction was reported in clinical application of these particles, it was found that these side effects were caused due to complement activation⁷⁴.

Previous studies have shown that non-functionalized CNTs, when placed in contact with human serum, activate complement via the classical and, to a lesser extent, via the alternative pathway^{71, 75}. However, the mode of binding of the recognition proteins to the CNTs has not fully been characterised and questions remain whether complement proteins bind directly to the CNTs or bind via other deposited (serum) proteins that can act as adaptors. Complement proteins C1q and MBL, as well as C-reactive protein, an acute phase protein which itself mediates binding of C1q (an “adaptor” for C1q), are known to recognise repetitive structures or charge patterns, which are not found on pristine CNTs but commonly found on the surface of functionalized CNTs⁷⁶. Ling et al. presented evidence that C1q “crystallizes” on pristine and functionalized CNTs, but is not bound in a way that allows it to activate the next step of the complement cascade⁷⁷. Other serum proteins would thus have to form a stable layer on the CNTs for indirect C1 binding and subsequent complement activation. Others^{71, 75, 78, 79}, however, observed direct high affinity binding of C1q to CNTs by hydrophobic interactions, and concluded that direct binding of C1 would allow complement activation. Binding of C1q onto CNTs is not ionic or calcium-ion-dependent and is of high affinity since denaturation of C1q is required to remove the C1q from the CNTs⁸⁰.

Recombinant forms of individual globular head regions of C1q A, B and C chains can be bound to pristine, oxidised and carboxymethyl (CMC) cellulose coated MWNTs^{78, 79}, confirming that the binding of C1q to CNTs takes place via the gC1q domain, which is the principal ligand-recognition domain of C1q⁸¹. Binding of C1 is followed by activation of C4 and C2, but activation may not go beyond that due to the lack of suitable covalent binding (OH, NH₂ or SH) sites for C4b or C3b⁸². However, it has been shown that C3 and C5 turnover did occur with pristine and various proteins coated CNTs⁷⁹. Therefore, it is likely that C3b binds and the MAC is subsequently formed. These interactions of C3b and C4b are most likely via direct hydrophobic interactions with the surface of the CNTs⁸⁰. Similarly, another key component and up-regulator of the complement alternative pathway, properdin, which has previously been shown to bind to apoptotic T cells⁸³ and DNA exposed on apoptotic and necrotic cells⁸⁴, has recently shown pattern recognition properties and binds to both CMC-CNTs and Ox-CNTs and enhances their uptake by macrophages in a complement-independent manner. Furthermore, CNTs bound properdin still retains its C3 and C5 convertase stabilisation properties and activates the alternative pathway. However,

recombinant thrombospondin repeats (TSR) 4 and 5, the modules of human properdin that can bind C3b, acts as a potent inhibitor of the alternative pathway and also inhibit the rapid macrophage mediated clearance, raising the possibility of therapeutic use in a range of diseases, including tumour⁸⁵. CNTs, opsonised with human properdin or TSR4+5, triggered a robust pro-inflammatory response by macrophages, suggesting that local synthesis of complement proteins can alter the immune clearance of nanoparticles considerably, even when there is no complement activation involved.

Differential innate immune recognition of CNTs based on functionalisation

Several studies have shown that functionalization, and therefore, alteration in the surface properties of the CNTs, can change the extent of complement activation^{49, 52, 69, 78-80, 86, 87}. Pre-coating CNTs will increase the dispersion state, making more surface area available for complement proteins to recognise and deposit themselves. RNA and BSA, used as dispersing agents, do not uniformly coat the CNT surface, therefore, binding sites on the CNT surface are made more available and complement activation might increase compared to clustered pristine CNTs. RNA itself can interact with C1q providing an additional binding site for complement⁸⁰. Poly-ε-caprolactam (Nylon-6) and CMC-cellulose have been shown to reduce the level of complement activation via the classical pathway most efficiently, but fail to eliminate opsonisation^{52, 79}.

Until a decade ago, PEGylation (Poly ethylene glycol coating) was considered to provide a shielding surface on nanoparticles, but in 2002, it was shown that PEGylated polystyrene microspheres could activate complement, depending on the configuration of the PEG on the surface⁸⁸. The effects of PEGylation on SWNTs as well as MWNTs have been extensively studied by the Moghimi group. They showed that although PEG can reduce complement activation via both classical and alternative pathway, levels of both C4d (cleavage product of C4) and MAC significantly increased. They concluded that complement activation was likely to occur through the lectin pathway. For MWNTs, complement activation was independent of the molecular mass of PEG chains and the effect was not caused by uncoated regions of the CNTs. The surface domains of the PEG derivatives may thus act as templates for the lectin pathway activating molecules (L-ficolin and MASP-2)^{86, 89, 90}.

Complement activation can be influenced by coating specific humoral factors onto the outer walls of CNTs. For instance binding of factor H, a down-regulator of the alternative pathway, lowers the activation of the alternative pathway⁵². In contrast to full length C1q, the recombinant globular heads of C1q were shown to reduce complement activation⁷⁹. This phenomenon is likely to be caused by globular heads competing out the binding of whole C1q to CNTs, thereby diminishing complement activation. A similar technique to avoid recognition by the complement system is used by pathogenic bacteria, which have specific binding motifs on their surface to bind factor H, thus inhibiting alternative pathway activation⁹¹.

Innate immune receptors, phagocytosis and immune response

The cells of the innate immune system, including macrophages and DCs, have pattern recognition receptors (PRRs) that recognise and bind pathogens via pathogen-associated molecular patterns (PAMPs). These include toll-like receptors (TLRs), scavenger receptors, complement receptors, integrins, and lectin-like receptors, which are potentially capable of recognising nanoparticles. Once a particle is bound to receptors, the particle will be attached to the cell and taken on its path, but can also be phagocytosed and ultimately, if possible, digested internally and cleared from the system.

The most important complement-derived opsonin is C3b and its breakdown product iC3b. Multiple copies of C3b bind onto the surface of the nanocarrier. C3b interacts with complement receptor 1 (CR1 or CD35) which is abundant on red blood cells. Once C3b has bound, it is gradually broken down into iC3b, which has lower affinity towards CR1, but high affinity towards CR3 and CR4, which are commonly found on phagocytic cells. Therefore, the nanoparticles will be transferred from red blood cells towards phagocytic cells, especially during the passage of the red blood cells through the liver where macrophages are present in high numbers. The iC3b will be further broken down into C3d, which can interact with CR2 (CD21) on the surface of B-lymphocytes, and therefore, interact with the adaptive immune system.

Opsonised CNTs absorb or bind onto the surface of red blood cells (Pondman et al., unpublished), indicating that C3b is bound in a conformation that allows interaction with CR1. PEGylation, which down-regulates complement activation, was shown to reduce

uptake of CNTs by monocytes, spleen and liver phagocytes that correlated with increasing molecular weight and PEG coating density⁹². Uptake of CNTs by macrophages (U937 cell line), blood monocytes and B cells (Raji cell line) is more efficient in the presence of serum; while complement inactivated (heat inactivated) serum does not enhance the phagocytosis of CNTs, indicating an important additive effect of complement^{78, 79}. Most interestingly, Jurkat T cells, which are known to express complement receptors feebly on their surface, were able to take up CNTs poorly and serum treatment did not increase uptake⁷⁸. Complement adsorption on the surface of MWNTs was shown to reduce the expression of pro-inflammatory cytokines (TNF- α , IL-6 and IL-1 β) and increase expression of anti-inflammatory cytokines (IL-10 and TGF- β) in monocytes and macrophages⁷⁹. This indicates that complement might signal the cells to silently remove the CNTs by phagocytosis, but do not give out stress signals to their microenvironment. Even when only the initial complement proteins C1q and MBL are bound on the surface of the CNT, receptor interactions are possible with calreticulin, a receptor molecule for C1q and MBL, working together with CD91 acting as a C1q receptor⁹³. These bindings are less efficient as the density of deposited C1q and MBL is far lower than C3b and for adhesion, hundreds of receptor-ligand pairs are needed. As was shown recently, pre-coating the CNTs with the recombinant globular head modules of human C1q and its full length counterpart⁸⁷ can increase the phagocytosis by macrophages. Similar properties has been shown with properdin coated CNTs⁸⁵ while factor H⁸⁷ and small fragment of properdin molecule (TSR4+5)⁸⁵ proved to be an inhibitor of phagocytosis. Recently, Meng et al. showed that after phagocytosis of ox-MWNTs, macrophages produced macrophage inflammatory proteins (MIP-1 α and MIP-2) to recruit other macrophages to the site. They also confirmed that low levels of pro-inflammatory cytokines were produced⁹⁴.

Non-complement dependent uptake of CNTs

The method of entry of CNTs into cells is a highly debated subject in the literature, complement dependent phagocytosis being one of the several mechanisms. Covalent and non-covalent modification of CNT walls can alter its interaction with immune cells. In the case of the former, that phenomenon can be caused by the chemical nature of the coating. For example, macrophages are known to interact more strongly with positively charged particles due to the presence of negatively charged sialic acid on their surface⁹⁵. However,

altered uptake and interactions can also be a direct effect of the higher dispersibility and, therefore, biocompatibility of the functionalized CNTs. In general, hydrophilic or acidic polymer coated MWNTs are more efficiently internalized by macrophages than hydrophobic polymer coated MWNTs⁹⁶. Direct penetration or “needling” through the plasma membrane is another described phenomenon^{97, 98}. Others state that absorption of albumin or other serum proteins is essential to trigger scavenger receptor-mediated uptake⁹⁹. Kam et al. found that very short SWNTS (e.g., 50-200 nm) enter cells (e.g., HeLa and H60 cell lines) through clathrin-dependent endocytosis¹⁰⁰. However, Pantarotto et al showed that slightly longer SWNTs (300-1000 nm) behave like cell penetrating peptides while entering human (3T6) and murine (3T3) fibroblasts²⁸.

After uptake by the cells, the chemically modified CNTs can be found in the cytoplasm, endosomes,^{11, 28, 98, 101, 102} and in some cases, inside the nucleus^{28, 97, 102}. These variations can be due to different functionalization^{28, 97}. Exocytosis has not been reported often and the time course for the process varies between simultaneous with endocytosis¹⁰³ and until after 5 h of incubation^{78, 79, 101}.

Cytokine, inflammation and immune responses

In their bio-persistence as well as high aspect ratio, CNTs show similarities to asbestos, and therefore, an incomplete uptake and frustrated phagocytosis with the related inflammation and granuloma formation is a risk that has to be analysed^{98, 104, 105}. Frustrated phagocytosis was analysed by Brown et al. with a variety of elongated CNTs¹⁰⁶. In their study, only individually dispersed long straight CNTs led to frustrated phagocytosis using PBMCs (peripheral blood mononuclear cells) and the THP-1 cells, (a monocyte-derived cell line), which correlated with superoxide anion and TNF- α release. The presence of CNTs interfered with the function of the macrophages as was shown by an inhibition of the ability of THP-1 cells to phagocytose *E. coli*. Clustered CNTs and nanofibers did not induce apoptotic or necrotic effects¹⁰⁶.

Exposure to long MWNTs resulted in a significant and dose-dependent release of IL-1 β , TNF- α , IL-6 and IL-8 from THP-1, but not from mesothelial cells (Met5a)¹⁰⁴. More interestingly, when cell medium from the THP-1 cells treated with long CNTs was added to Met5a cells, they too showed an increased cytokine production, indicating the essential role of

macrophages in the immune response towards CNTs. Liu et al. showed that immune response with pluronic F127 coated MWNTs in RAW (a murine macrophage cell line) and MCF-7 (a breast cancer cell line) cells was length-dependent¹⁰⁵. RAW cells showed higher internalisation, resulting in higher toxicity due to CNTs than MCF-7. Long MWNTs (3-8 μm) were more toxic than short (<1.5 μm), but short MWNTs gave more TNF- α release than long MWNTs, which could lead to a stronger inflammatory response. However, complement deposited CNTs dampened the pro-inflammatory cytokines such as IL-1 β and TNF- α despite higher internalization of these CNTs by human macrophage cell lines⁷⁹.

Besides cytokine response, indications of inflammasome formation by CNTs have been reported^{98, 107, 108}. Many carbon nanomaterials (carbon black, short, long and tangled CNTs, long needle-like MWNTs, and asbestos) induced IL-1 β secretion (indicator of inflammasome formation), but only long needle-like CNTs induced IL-1 α secretion in LPS-primed macrophages⁹⁸. DWNTs can synergize with TLR4 antagonists; when K⁺ efflux is hindered, IL-1 β secretion could be eliminated, indicating that phagocytosis was required for inflammasome activation. After phagocytosis, NF- κB (nuclear factor kappa-light-chain-enhancer of activated B cells) and NLRP3 (nucleotide-binding oligomerization domain (NOD)-like receptors family, pyrin domain containing 3) inflammasome are activated^{107, 108}

Various CNTs can modulate DC maturation¹⁰⁹. Short, purified SWNTs by an oxidation method and with free-endotoxin content induced no maturation of DC cultures and did not lead to the secretion of IL-6, TNF- α , or IL-1 β following their uptake. In comparison, incubation of DCs with LPS and CNTs induced IL-1 β secretion, which was dose and NLRP3-dependent, indicating that LPS contamination causes this effect¹¹⁰. Dumortier et al. showed that PEG₁₅₀₀-SWNTs are taken up by B- and T-cells without affecting viability of the cells or causing damage, inhibiting or stimulating their function⁵⁰. Although they found no IL-2 and IFN- α secretion (reflecting T cell activation), PEGylated SWNTs did induce IL-6 and TNF- α secretion in peritoneal macrophages *in vitro*, which the authors attributed to the formation of CNT aggregates.

Lung innate immunity and CNTs

Most likely triggered by their asbestos like appearance¹¹¹, pulmonary toxicity of CNTs is one of the most discussed aspects in the toxicology field. Disagreement started from the very

first studies published by Lam¹¹² and Warheit¹¹³ who independently concluded that CNTs were highly toxic and non-toxic to the lungs, respectively. First, they both showed that CNTs induced granulomas, but only Lam showed subsequent fibrogenesis. This effect can be explained by the fact that granuloma formation is mediated by the accumulation of alveolar macrophages at sites of CNT deposition, which become activated by the phagocytosis of the nanoparticles. The activated macrophages produce growth factors that stimulate the proliferation of fibroblasts, the collagen producing cells driving the fibrogenesis¹¹⁴. Whereas Lam found a dose- and time-dependent interstitial inflammation, Warheit did not see any inflammation and fibrosis; in addition, the granuloma formation was not dose-dependent. Warheit concluded that the toxicity of the CNTs was caused by aggregation of the CNTs due to the administration method (instillation), which also caused airway blocking. Shvedova et al. confirmed the results of Lam et al. in mice and also showed dose-dependent functional respiratory deficiencies¹¹⁵. Subsequently, Mangum et al. found no inflammation in SWNT exposed (oropharyngeal aspiration) rats, although they did find a few focal interstitial fibrotic lesions at locations with clusters of macrophages containing micron sized aggregates of SWNTs in the alveolar region. In addition, they reported, in bronchoalveolar lavage fluid (BALF), macrophages linked together with bridges of parallel bundles of SWNTs. They stated that this bridge formation is not similar to frustrated or incomplete phagocytosis seen in asbestos and other long fibres¹¹⁴. The origin in the variations of effects reported possibly owes it to a wide variation in the nanoparticles (single, double or multi-walled) with variable diameter and length, coating, aggregation states, contamination with other materials, and administration method and route¹¹⁶. By comparing well-dispersed SWNTs with aggregated SWNTs, Shvedova et al. found that poorly dispersed SWNTs formed clumps of 5 to 20 μm in the lungs, which triggered granuloma formation, whereas highly dispersed SWNTs that did not form any clumps and were found free in the tissue, gave rise to interstitial fibrosis but no granulomatous lesions¹¹⁷⁻¹¹⁹. This was confirmed by a study where well dispersed MWNTs were found in every cell and cell layer of the lung parenchyma, with signs of interstitial fibrosis of the alveolar wall but with very limited granuloma formation¹²⁰.

The lung innate immune defence is governed mainly by surfactant proteins A and D (SP-A and SP-D), together with lung leukocytes and the epithelial cells lining the alveolar surface. Like MBL, SP-A and SP-D are members of the collectin (collagenous lectins) family. SP-A and

SP-D have a multimeric structure similar to C1q and MBL. Among other roles, SP-A and SP-D bind to invading particles (commonly via vicinal diols) in a Ca^{2+} -dependent manner and promote their binding to receptors on alveolar macrophages¹²¹. The concentrations of SP-A and SP-D are very low, and therefore, binding of these pulmonary surfactant proteins to CNTs can cause significant depletion of the proteins and damage to the pulmonary innate immune defence mechanisms⁷².

Selective Ca^{2+} -dependent binding of BALF SP-A and SP-D to the oxygen containing functional groups on the surface of CNTs was confirmed in a study by Salvador-Morales by using acid treated (oxidized) MWNTs, which could be coated entirely with SP-A¹²². Oxidized DWNTs bound SP-A and SP-D more efficiently than non-oxidized DWNTs and purified DWNTs. Similar results were found for MWNTs and ox-MWNTs by Marchetti et al.¹²³.

SP-A-coated MWNTs were able to enter the cytoplasm and the nucleus of alveolar macrophages. Interestingly, the high nitric oxide secretion evoked by pristine MWNTs and BSA-coated MWNTs was not observed by SP-A-coated MWNTs, indicating a possible method to avoid an inflammatory response towards CNTs¹²². Allowing SWNTs to obtain a lung surfactant corona, consisting of SP-A, B and D, enhanced the *in vitro* uptake of SWNT by RAW cells (murine macrophages)¹²⁴. Gasser et al. showed that pre-coating MWNTs (pristine, oxidised and aminated) with pulmonary surfactant proteins induces clusters of coated MWNTs intracellularly in monocyte-derived macrophages, while more stable suspensions are obtained with coated MWNTs¹²⁵. It has been argued that both SP-A and phosphatidylserine might represent an “eat me” signal towards macrophages. A similar effect was seen by coating CNTs with SP-D¹²⁶. Coating the MWNTs with SP-D slightly increased apoptosis while necrosis slightly decreased¹²⁵. Interestingly, a decrease in TNF- α release was found, which might be attributed to the phosphatidylserine present in the surfactant.

Coating of CMC-MWNTs and Ox-MWNTs with recombinant SP-D (rhSP-D) increased the phagocytosis by macrophages 2-fold, at the same time enhanced the cytokine storm provoked by MWNTs (reduction of IL-12, TGF- β , IL-1 β , IL-6 and TNF- α production)¹²⁶. Interestingly, SP-D coated CNTs enhanced the complement activation and SP-D coated and

complements deposited CNTs showed the dramatic reduction of pro-inflammatory cytokines production compared to SP-D coated CNTs¹²⁶.

Conclusions

A number of studies have addressed how CNTs interact with the innate immune system including complement proteins, macrophages, dendritic cells, cell surface pattern recognition receptors and soluble factors. The results obtained thus far paint a varied and heterogeneous picture: primarily owing to the diverse range of types of CNTs and experimental *in vitro* and *in vivo* model systems used for investigation. However, it is evident that the previously suggested pro-inflammatory response to CNTs needs to be viewed in the context of complement. The recognition subcomponents of the three pathways of the complement system are fully capable of binding via patterns presented as an array over the surface of pristine or chemically-modified CNTs. This recognition can lead to complement deposition, thus enhancing phagocytosis by the immune cells bearing complement receptors such as macrophages and B cells. Complement deposition on the CNTs appears to skew the pro-inflammatory response towards an anti-inflammatory one, suggesting beneficial effects of complement. It is unclear how complement deposition enhances anti-inflammatory immune response although a link between heightened IL-10 levels and suppressed TNF- α and IL-1 β is evident in recent studies. It is worth examining how altered pattern can affect CNT engagement with TLRs with or without complement deposition. Clearly, the ability of CNTs to induce pro-inflammatory and anti-inflammatory immune response requires a comprehensive *in vivo* assessment to prove their feasibility usage as therapeutic vehicles in the long term. Thus, their potency to deposit complement on the surface is going to acquire importance. There are a number of conflicting data in the literature that have arisen out of variability of the CNTs introduced by surface coating, shapes, sizes, dispersion, and surface charge. With advancement in the production of CNTs, such issues can be resolved. It is also important to note that the ability of CNTs to activate complement has been reported consistently by a range of research groups. Thus, any clinical trials involving CNTs, or for that matter, any nanoparticle, needs to include quality control involving innate immune aspects.

Acknowledgement: We thank Valarmathy Murugaiah for drawing Figure 3.

Table 1: Differential response induced by different form of CNTs

	Pristine	Covalently functionalised CNTs	Non covalently functionalized CNTs	PEG-CNTs
Complement activation	Less Activation of both classical and alternative pathway than functionalised - CNTs. ^{71,52}	Activates both classical and alternative pathway ⁷¹	Activates both classical and alternative pathway ⁷⁹	activates all three complement pathway ^{62, 86,89}
Endocytosis (Highly dependent on size, diameter, surface modification and ability to activate complement pathways)	-	Fewer uptakes by macrophages, B-cells and T-cells compared to <i>f</i> -CNTs. Uptake highly depends on level of complement activation. ⁷⁸ .	High uptake compared to Ox-CNTs and PEG-CNTs. ⁷⁸	Pegylation decreases the uptake by macrophages and increases circulation time <i>in vivo</i> ⁹²
Cytokine response	-	Anionic functionalization decreases the production of pro-inflammatory cytokines/growth factors than cationic functionalization ¹²⁷	CMC-CNTs are Anti-inflammatory to immune cells. ⁸⁷	PEGylated CNTs decreases the production of pro-inflammatory cytokines
Cytotoxicity (Depends on impurities, functionalisation, shape and size of CNTs)	Considered more toxic than any other form of CNTs ¹²⁸ Diameter- and rigidity dependent toxicity and carcinogenicity: thin and rigid nanotubes were the most toxic and carcinogenic ¹²⁹	Based on the functional group. Oxides group presents on CNTs are less toxic than amine group. ^{38, 130}	Toxicity depend on dispersant ¹³¹	SWCNT-PEGs exhibits less cytotoxic potency ¹³² non toxicity of PEGylated CNTs on T cells. ¹³³

References:

1. S. Iijima, *Nature*, 1991, **354**, 56-58.
2. F. Liang and B. Chen, *Curr. Med. Chem.*, 2010, **17**, 10-24.
3. A. Aqel, K. M. M. A. El-Nour, R. A. A. Ammar and A. Al-Warthan, *Arabian Journal of Chemistry*, 2012, **5**, 1-23.
4. M. Keidar, *J. Phys. D*, 2007, **40**, 2388.
5. J. Prasek, J. Drbohlavova, J. Chomoucka, J. Hubalek, O. Jasek, V. Adam and R. Kizek, *J. Mater. Chem.*, 2011, **21**, 15872-15884.
6. A. Bianco, K. Kostarelos and M. Prato, *Curr. Opin. Chem. Biol.*, 2005, **9**, 674-679.
7. C. Biale, V. Mussi, U. Valbusa, S. Visentin, G. Viscardi, N. Barbero, N. Pedemonte and L. Galiotta, in *2009 9th IEEE Conference on Nanotechnology, IEEE NANO 2009*, ed. anonymous, 2009, p. 644-646.
8. J. G. Li, W. X. Li, J. Y. Xu, X. Q. Cai, R. L. Liu, Y. J. Li, Q. F. Zhao and Q. N. Li, *Environ. Toxicol.*, 2007, **22**, 415-421.
9. H. Ali-Boucetta, K. T. Al-Jamal, K. H. Muller, S. Li, A. E. Porter, A. Eddaoudi, M. Prato, A. Bianco and K. Kostarelos, *Small*, 2011, **7**, 3230-3238.
10. E. Heister, V. Neves, C. Tã®lmaciu, K. Lipert, V. S. Beltrãjn, H. M. Coley, S. R. Silva and J. McFadden, *Carbon*, 2009, **47**, 2152-2160.
11. W. Wu, S. Wieckowski, G. Pastorin, M. Benincasa, C. Klumpp, J. P. Briand, R. Gennaro, M. Prato and A. Bianco, *Angew. Chem. Int. Ed Engl.*, 2005, **44**, 6358-6362.
12. M. Yang, S. Sun, Y. Kostov and A. Rasooly, *Lab. Chip*, 2010, **10**, 1011-1017.
13. N. Aoki, T. Akasaka, F. Watari and A. Yokoyama, *Dent. Mater. J.*, 2007, **26**, 178-185.
14. X. Shi, B. Sitharaman, Q. P. Pham, F. Liang, K. Wu, W. Edward Billups, L. J. Wilson and A. G. Mikos, *Biomaterials*, 2007, **28**, 4078-4090.
15. J. H. Choi, F. T. Nguyen, P. W. Barone, D. A. Heller, A. E. Moll, D. Patel, S. A. Boppart and M. S. Strano, *Nano Lett.*, 2007, **7**, 861-867.
16. O. Vittorio, S. L. Duce, A. Pietrabissa and A. Cuschieri, *Nanotechnology*, 2011, **22**, 095706-4484/22/9/095706. Epub 2011 Jan 27.
17. P. K. Avti, Y. Talukdar, M. V. Sirotkin, K. R. Shroyer and B. Sitharaman, *J. Biomed. Mater. Res. B. Appl. Biomater.*, 2013, **101**, 1039-1049.

18. E. Fidiani, P. M. F. J. Costa, A. U. B. Wolter, D. Maier, B. Buechner and S. Hampel, *J. Phys. Chem. C*, 2013, **117**, 16725-16733.
19. J. T. Wang, L. Cabana, M. Bourgognon, H. Kafa, A. Protti, K. Venner, A. M. Shah, J. K. Sosabowski, S. J. Mather, A. Roig, X. Ke, G. Van Tendeloo, R. T. M. de Rosales, G. Tobias and K. T. Al-Jamal, *Advanced Functional Materials*, 2014, **24**, 1880-1894.
20. B. Chen, H. Zhang, C. Zhai, N. Du, C. Sun, J. Xue, D. Yang, H. Huang, B. Zhang, Q. Xie and Y. Wu, *J. Mater. Chem.*, 2010, **20**, 9895-9902.
21. R. Klingeler, S. Hampel and B. Buchner, *Int. J. Hyperthermia*, 2008, **24**, 496-505.
22. I. Moench, A. Meye and A. Leonhardt, 2007, .
23. M. Foldvari and M. Bagonluri, *Nanomedicine*, 2008, **4**, 173-182.
24. Z. Liu, S. Tabakman, K. Welsher and H. Dai, *Nano Res.*, 2009, **2**, 85-120.
25. M. Foldvari and M. Bagonluri, *Nanomedicine*, 2008, **4**, 183-200.
26. N. A. Monteiro-Riviere and A. O. Inman, *Carbon*, 2006, **44**, 1070-1078.
27. M. VanHandel, D. Alizadeh, L. Zhang, B. Kateb, M. Bronikowski, H. Manohara and B. Badie, *J. Neuroimmunol.*, 2009, **208**, 3-9.
28. D. Pantarotto, J. P. Briand, M. Prato and A. Bianco, *Chem. Commun. (Camb)*, 2004, **(1)**, 16-17.
29. N. A. Monteiro-Riviere, R. J. Nemanich, A. O. Inman, Y. Y. Wang and J. E. Riviere, *Toxicol. Lett.*, 2005, **155**, 377-384.
30. A. E. Porter, M. Gass, K. Muller, J. N. Skepper, P. A. Midgley and M. Welland, *Nanotechnol*, 2007, **2**, 713-717.
31. S. Hampel, D. Kunze, D. Haase, K. Kramer, M. Rauschenbach, M. Ritschel, A. Leonhardt, J. Thomas, S. Oswald, V. Hoffmann and B. Buchner, *Nanomedicine (Lond)*, 2008, **3**, 175-182.
32. Z. Liu, X. Sun, N. Nakayama-Ratchford and H. Dai, *ACS Nano*, 2007, **1**, 50-56.
33. Z. Liu, W. Cai, L. He, N. Nakayama, K. Chen, X. Sun, X. Chen and H. Dai, *Nat. Nanotechnol*, 2007, **2**, 47-52.
34. A. Bianco, K. Kostarelos, C. D. Partidos and M. Prato, *Chem. Commun. (Camb)*, 2005, **(5)**, 571-577.
35. L. Lacerda, A. Bianco, M. Prato and K. Kostarelos, *Adv. Drug Deliv. Rev.*, 2006, **58**, 1460-1470.

36. N. Sinha and J. T. Yeow, *IEEE Trans. Nanobioscience*, 2005, **4**, 180-195.
37. T. L. Moore, S. W. Grimes, R. L. Lewis and F. Alexis, *Mol. Pharm.*, 2014, **11**, 276-282.
38. D. Pantarotto, R. Singh, D. McCarthy, M. Erhardt, J. P. Briand, M. Prato, K. Kostarelos and A. Bianco, *Angew. Chem. Int. Ed Engl.*, 2004, **43**, 5242-5246.
39. R. A. Graff, T. M. Swanson and M. S. Strano, *Chemistry of Materials*, 2008, **20**, 1824-1829.
40. S. K. Smart, A. I. Cassady, G. Q. Lu and D. J. Martin, *Carbon*, 2006, **44**, 1034.
41. M. R. McDevitt, D. Chattopadhyay, B. J. Kappel, J. S. Jaggi, S. R. Schiffman, C. Antczak, J. T. Njardarson, R. Brentjens and D. A. Scheinberg, *J. Nucl. Med.*, 2007, **48**, 1180-1189.
42. R. Bandyopadhyaya, E. Nativ-Roth, O. Regev and R. Yerushalmi-Rozen, *Nano Letters*, 2002, **2**, 25-28.
43. C. Bertulli, H. J. Beeson, T. Hasan and Y. Y. Huang, *Nanotechnology*, 2013, **24**, 265102.
44. M. F. Islam, E. Rojas, D. M. Bergey, A. T. Johnson and A. G. Yodh, *Nano Letters*, 2003, **3**, 269-273.
45. N. Hadidi, F. Kobarfard, N. Nafissi-Varcheh and R. Aboofazeli, *Int. J. Nanomedicine*, 2011, **6**, 737-746.
46. M. Zheng, A. Jagota, E. D. Semke, B. A. Diner, R. S. McLean, S. R. Lustig, R. E. Richardson and N. G. Tassi, *Nat. Mater.*, 2003, **2**, 338-342.
47. Y. Li, X. Zhang, J. Luo, W. Huang, J. Cheng, Z. Luo, T. Li, F. Liu, G. Xu, X. Ke, L. Li and H. J. Geise, *Nanotechnology*, 2004, **15**, 1645.
48. K. Bhattacharya, F. T. Andon, R. El-Sayed and B. Fadeel, *Adv. Drug Deliv. Rev.*, 2013, **65**, 2087-2097.
49. V. A. Basiuk, C. Salvador-Morales, E. V. Basiuk, R. M. J. Jacobs, M. Ward, B. T. Chu, R. B. Sim and M. L. H. Green, *J. Mater. Chem.*, 2006, **16**, 4420-4426.
50. H. Dumortier, S. Lacotte, G. Pastorin, R. Marega, W. Wu, D. Bonifazi, J. P. Briand, M. Prato, S. Muller and A. Bianco, *Nano Lett.*, 2006, **6**, 1522-1528.
51. M. Shim, N. W. Shi Kam, R. J. Chen, Y. Li and H. Dai, *Nano Letters*, 2002, **2**, 285-288.
52. C. Salvador-Morales, E. V. Basiuk, V. A. Basiuk, M. L. Green and R. B. Sim, *J. Nanosci Nanotechnol*, 2008, **8**, 2347-2356.
53. Y. H. Kang, L. A. Tan, M. V. Carroll, M. E. Gentle and R. B. Sim, *Adv. Exp. Med. Biol.*, 2009, **653**, 117-128.

54. U. Kishore and K. B. Reid, *Immunopharmacology*, 1999, **42**, 15-21.
55. M. V. Carroll and R. B. Sim, *Adv. Drug Deliv. Rev.*, 2011, **63**, 965-975.
56. L. Kouser, M. Abdul-Aziz, A. Nayak, C. M. Stover, R. B. Sim and U. Kishore, *Frontiers in Immunology*, 2013, **4**, 93.
57. U. Kishore and R. B. Sim, *Immunobiology*, 2012, **217**, 162-168.
58. J. Leleux and K. Roy, *Adv. Healthc. Mater.*, 2013, **2**, 72-94.
59. C. Salvador-Morales, E. Flahaut, E. Sim, J. Sloan, M. L. Green and R. B. Sim, *Mol. Immunol.*, 2006, **43**, 193-201.
60. C. Gräfe, A. Weidner, M. v. d. Lühe, C. Bergemann, F. H. Schacher, J. H. Clement and S. Dutz, *Int. J. Biochem. Cell Biol.*, 2016, **75**, 196-202.
61. G. Maiorano, S. Sabella, B. Sorce, V. Brunetti, M. A. Malvindi, R. Cingolani and P. P. Pompa, *ACS Nano*, 2010, **4**, 7481-7491.
62. C. Sacchetti, K. Motamedchaboki, A. Magrini, G. Palmieri, M. Mattei, S. Bernardini, N. Rosato, N. Bottini and M. Bottini, *ACS Nano*, 2013, **7**, 1974-1989.
63. A. Gustafsson, E. Lindstedt, L. S. Elfsmark and A. Bucht, *J. Immunotoxicol.*, 2011, **8**, 111-121.
64. Y. K. Lee, E. J. Choi, T. J. Webster, S. H. Kim and D. Khang, *Int. J. Nanomedicine*, 2014, **10**, 97-113.
65. T. Cedervall, I. Lynch, S. Lindman, T. Berggard, E. Thulin, H. Nilsson, K. A. Dawson and S. Linse, *Proc. Natl. Acad. Sci. U. S. A.*, 2007, **104**, 2050-2055.
66. P. Aggarwal, J. B. Hall, C. B. McLeland, M. A. Dobrovolskaia and S. E. McNeil, *Adv. Drug Deliv. Rev.*, 2009, **61**, 428-437.
67. M. Rahman, S. Laurent, N. Tawil, L. Yahia and M. Mahmoudi, in *Protein-Nanoparticle interactions*, ed. nonymous, Springer, 2013, p. 21-44.
68. M. Lundqvist, J. Stigler, G. Elia, I. Lynch, T. Cedervall and K. A. Dawson, *Proc. Natl. Acad. Sci. U. S. A.*, 2008, **105**, 14265-14270.
69. M. Rybak-Smith, K. M. Pondman, E. Flahaut, C. Salvador-Morales and R. B. Sim, in *Carbon Nanotubes for Biomedical Applications*, ed. R. Klingeler and B. R. Sim, Springer Berlin Heidelberg, Berlin, Heidelberg, 2011, p. 183-210.
70. J. H. Shannahan, J. M. Brown, R. Chen, P. C. Ke, X. Lai, S. Mitra and F. A. Witzmann, *Small*, 2013, **9**, 2171-2181.

71. C. Salvador-Morales, E. Flahaut, E. Sim, J. Sloan, M. L. Green and R. B. Sim, *Mol. Immunol.*, 2006, **43**, 193-201.
72. C. Salvador-Morales, P. Townsend, E. Flahaut, C. Vénien-Bryan, A. Vlandas, M. L. H. Green and R. B. Sim, *Carbon*, 2007, **45**, 607-617.
73. X. Cai, R. Ramalingam, H. S. Wong, J. Cheng, P. Ajuh, S. H. Cheng and Y. W. Lam, *Nanomedicine*, 2013, **9**, 583-593.
74. A. Chanan-Khan, J. Szebeni, S. Savay, L. Liebes, N. M. Rafique, C. R. Alving and F. M. Muggia, *Ann. Oncol.*, 2003, **14**, 1430-1437.
75. C. Salvador-Morales, M. L. H. Green and R. B. Sim, in *Chemistry of carbon nanotubes*, ed. Basiuk, E. V, Basiuk, V.A, American Scientific Publishers, 2007.
76. S. M. Moghimi, A. J. Andersen, D. Ahmadvand, P. P. Wibroe, T. L. Andresen and A. C. Hunter, *Adv. Drug Deliv. Rev.*, 2011, **63**, 1000-1007.
77. W. L. Ling, A. Biro, I. Bally, P. Tacnet, A. Deniaud, E. Doris, P. Frachet, G. Schoehn, E. Pebay-Peyroula and G. J. Arlaud, *ACS Nano*, 2011, **5**, 730-737.
78. K. M. Pondman, A. G. Tsolaki, B. Paudyal, M. H. Shamji, A. Switzer, A. A. Pathan, S. M. Abozaid, B. Ten Haken, G. Stenbeck, R. B. Sim and U. Kishore, *J. Biomed. Nanotechnol*, 2016, **12**, 197-216.
79. K. M. Pondman, M. Sobik, A. Nayak, A. G. Tsolaki, A. Jakel, E. Flahaut, S. Hampel, B. Ten Haken, R. B. Sim and U. Kishore, *Nanomedicine*, 2014, **10**, 1287-1299.
80. M. J. Rybak-Smith and R. B. Sim, *Adv. Drug Deliv. Rev.*, 2011, **63**, 1031-1041.
81. U. Kishore, R. Ghai, T. J. Greenhough, A. K. Shrive, D. M. Bonifati, M. G. Gadjeva, P. Waters, M. S. Kojouharova, T. Chakraborty and A. Agrawal, *Immunol Lett*, 2004, **95**, 113-128.
82. C. Salvador-Morales, E. Flahaut, E. Sim, J. Sloan, M. L. Green and R. B. Sim, *Mol. Immunol.*, 2006, **43**, 193-201.
83. C. Kemper, L. M. Mitchell, L. Zhang and D. E. Hourcade, *Proc. Natl. Acad. Sci. U. S. A.*, 2008, **105**, 9023-9028.
84. W. Xu, S. P. Berger, L. A. Trouw, H. C. de Boer, N. Schlagwein, C. Mutsaers, M. R. Daha and C. van Kooten, *J. Immunol.*, 2008, **180**, 7613-7621.
85. L. Kouser, B. Paudyal, A. Kaur, E. Flauhat, H. A. Khan, C. M. Stover, R. B. Sim and U. Kishore, *Biomaterials*, 2016, **submitted**.
86. I. Hamad, A. Christy Hunter, K. J. Rutt, Z. Liu, H. Dai and S. Moein Moghimi, *Mol. Immunol.*, 2008, **45**, 3797-3803.

87. K. M. Pondman, L. Pednekar, B. Paudyal, A. G. Tsolaki, L. Kouser, H. A. Khan, M. H. Shamji, B. Ten Haken, G. Stenbeck, R. B. Sim and U. Kishore, *Nanomedicine*, 2015, **11**, 2109-2118.
88. J. K. Gbadamosi, A. C. Hunter and S. M. Moghimi, *FEBS Lett.*, 2002, **532**, 338-344.
89. A. J. Andersen, J. T. Robinson, H. Dai, A. C. Hunter, T. L. Andresen and S. M. Moghimi, *ACS Nano*, 2013, **7**, 1108-1119.
90. A. J. Andersen, B. Windschiegl, S. Ilbasimis-Tamer, I. T. Degim, A. C. Hunter, T. L. Andresen and S. M. Moghimi, *Nanomedicine*, 2013, **9**, 469-473.
91. J. Hellwage, T. Meri, T. Heikkila, A. Alitalo, J. Panelius, P. Lahdenne, I. J. Seppala and S. Meri, *J. Biol. Chem.*, 2001, **276**, 8427-8435.
92. R. Gref, M. Luck, P. Quellec, M. Marchand, E. Dellacherie, S. Harnisch, T. Blunk and R. H. Muller, *Colloids Surf. B Biointerfaces*, 2000, **18**, 301-313.
93. C. A. Ogden, A. deCathelineau, P. R. Hoffmann, D. Bratton, B. Ghebrehiwet, V. A. Fadok and P. M. Henson, *J. Exp. Med.*, 2001, **194**, 781-795.
94. J. Meng, X. Li, C. Wang, H. Guo, J. Liu and H. Xu, *ACS Applied Materials & Interfaces*, 2015, **7**, 3180-3188.
95. S. Hussain, J. A. Vanoirbeek and P. H. Hoet, *Wiley Interdiscip. Rev. Nanomed Nanobiotechnol*, 2012, **4**, 169-183.
96. L. Tabet, C. Bussy, A. Setyan, A. Simon-Deckers, M. J. Rossi, J. Boczkowski and S. Lanone, *Part Fibre Toxicol.*, 2011, **8**, 3-8977-8-3.
97. K. Kostarelos, L. Lacerda, G. Pastorin, W. Wu, WieckowskiSebastien, J. Luangsivilay, S. Godefroy, D. Pantarotto, J. Briand, S. Muller, M. Prato and A. Bianco, *Nat Nano*, 2007, **2**, 108-113.
98. J. Palomaki, E. Valimaki, J. Sund, M. Vippola, P. A. Clausen, K. A. Jensen, K. Savolainen, S. Matikainen and H. Alenius, *ACS Nano*, 2011, **5**, 6861-6870.
99. G. Laverny, A. Casset, A. Purohit, E. Schaeffer, C. Spiegelhalter, F. de Blay and F. Pons, *Toxicol. Lett.*, 2013, **217**, 91-101.
100. N. W. Kam, Z. Liu and H. Dai, *Angew. Chem. Int. Ed Engl.*, 2006, **45**, 577-581.
101. B. Kang, D. C. Yu, S. Q. Chang, D. Chen, Y. D. Dai and Y. Ding, *Nanotechnology*, 2008, **19**, 375103-4484/19/37/375103. Epub 2008 Aug 1.
102. Q. Mu, D. L. Broughton and B. Yan, *Nano Lett.*, 2009, **9**, 4370-4375.
103. H. Jin, D. A. Heller and M. S. Strano, *Nano Lett.*, 2008, **8**, 1577-1585.

104. F. A. Murphy, A. Schinwald, C. A. Poland and K. Donaldson, *Part Fibre Toxicol.*, 2012, **9**, 8-8977-9-8.
105. D. Liu, L. Wang, Z. Wang and A. Cuschieri, *Nanoscale Res. Lett.*, 2012, **7**, 361-276X-7-361.
106. D. M. Brown, I. A. Kinloch, U. Bangert, A. H. Windle, D. M. Walter, G. S. Walker, C. A. Scotchford, K. Donaldson and V. Stone, *Carbon*, 2007, **45**, 1743.
107. C. P. Chio, S. C. Chen, K. C. Chiang, W. C. Chou and C. M. Liao, *Sci. Total Environ.*, 2007, **387**, 113-127.
108. E. Meunier, A. Coste, D. Olagnier, H. Authier, L. Lefevre, C. Dardenne, J. Bernad, M. Beraud, E. Flahaut and B. Pipy, *Nanomedicine*, 2012, **8**, 987-995.
109. E. Koike, H. Takano, K. Inoue, R. Yanagisawa and T. Kobayashi, *Chemosphere*, 2008, **73**, 371-376.
110. M. Yang, K. Flavin, I. Kopf, G. Radics, C. H. Hearnden, G. J. McManus, B. Moran, A. Villalta-Cerdas, L. A. Echegoyen, S. Giordani and E. C. Lavelle, *Small*, 2013, **9**, 4194-4206.
111. V. C. Sanchez, J. R. Pietruska, N. R. Miselis, R. H. Hurt and A. B. Kane, *Wiley Interdiscip. Rev. Nanomed Nanobiotechnol*, 2009, **1**, 511-529.
112. C. W. Lam, J. T. James, R. McCluskey and R. L. Hunter, *Toxicol. Sci.*, 2004, **77**, 126-134.
113. D. B. Warheit, B. R. Laurence, K. L. Reed, D. H. Roach, G. A. Reynolds and T. R. Webb, *Toxicol. Sci.*, 2004, **77**, 117-125.
114. J. B. Mangum, E. A. Turpin, A. Antao-Menezes, M. F. Cesta, E. Bermudez and J. C. Bonner, *Part Fibre Toxicol.*, 2006, **3**, 15.
115. A. A. Shvedova, E. R. Kisin, R. Mercer, A. R. Murray, V. J. Johnson, A. I. Potapovich, Y. Y. Tyurina, O. Gorelik, S. Arepalli, D. Schwegler-Berry, A. F. Hubbs, J. Antonini, D. E. Evans, B. K. Ku, D. Ramsey, A. Maynard, V. E. Kagan, V. Castranova and P. Baron, *Am. J. Physiol. Lung Cell. Mol. Physiol.*, 2005, **289**, L698-708.
116. A. R. Murray, E. R. Kisin, A. V. Tkach, N. Yanamala, R. Mercer, S. H. Young, B. Fadeel, V. E. Kagan and A. A. Shvedova, *Part Fibre Toxicol.*, 2012, **9**, 10-8977-9-10.
117. A. A. Shvedova, J. P. Fabisiak, E. R. Kisin, A. R. Murray, J. R. Roberts, Y. Y. Tyurina, J. M. Antonini, W. H. Feng, C. Kommineni, J. Reynolds, A. Barchowsky, V. Castranova and V. E. Kagan, *Am. J. Respir. Cell Mol. Biol.*, 2008, **38**, 579-590.
118. A. A. Shvedova, E. Kisin, A. R. Murray, V. J. Johnson, O. Gorelik, S. Arepalli, A. F. Hubbs, R. R. Mercer, P. Keohavong, N. Sussman, J. Jin, J. Yin, S. Stone, B. T. Chen, G. Deye, A. Maynard, V. Castranova, P. A. Baron and V. E. Kagan, *Am. J. Physiol. Lung Cell. Mol. Physiol.*, 2008, **295**, L552-65.

119. A. A. Shvedova, E. R. Kisin, A. R. Murray, C. Kommineni, V. Castranova, B. Fadeel and V. E. Kagan, *Toxicol. Appl. Pharmacol.*, 2008, **231**, 235-240.
120. D. W. Porter, A. F. Hubbs, R. R. Mercer, N. Wu, M. G. Wolfarth, K. Sriram, S. Leonard, L. Battelli, D. Schwegler-Berry, S. Friend, M. Andrew, B. T. Chen, S. Tsuruoka, M. Endo and V. Castranova, *Toxicology*, 2010, **269**, 136-147.
121. U. Kishore, T. J. Greenhough, P. Waters, A. K. Shrive, R. Ghai, M. F. Kamran, A. L. Bernal, K. B. Reid, T. Madan and T. Chakraborty, *Mol. Immunol.*, 2006, **43**, 1293-1315.
122. C. Salvador-Morales, Z. Khan, J. Zamory, V. Tran, A. Cedeno, J. Umanzor-Alvarez, U. Kishore and R. B. Sim, *Journal of Advanced Microscopy Research*, 2013, **8**, 93-99.
123. M. Marchetti, M. S. Shaffer, M. Zambianchi, S. Chen, F. Superti, S. Schwander, A. Gow, J. J. Zhang, K. F. Chung, M. P. Ryan, A. E. Porter and T. D. Tetley, *Philos. Trans. R. Soc. Lond. B. Biol. Sci.*, 2015, **370**, 20140038.
124. A. A. Kapralov, W. H. Feng, A. A. Amoscato, N. Yanamala, K. Balasubramanian, D. E. Winnica, E. R. Kisin, G. P. Kotchey, P. Gou, L. J. Sparvero, P. Ray, R. K. Mallampalli, J. Klein-Seetharaman, B. Fadeel, A. Star, A. A. Shvedova and V. E. Kagan, *ACS Nano*, 2012, **6**, 4147-4156.
125. M. Gasser, P. Wick, M. J. Clift, F. Blank, L. Diener, B. Yan, P. Gehr, H. F. Krug and B. Rothen-Rutishauser, *Part Fibre Toxicol.*, 2012, **9**, 17-8977-9-17.
126. K. M. Pondman, B. Paudyal, R. B. Sim, A. Kaur, L. Kouser, A. G. Tsolaki, A. L. Jones, S. Khan C., A. H. Khan, B. Ten Haken, G. Stenbeck and U. Kishore, *Nanomedicine*, 2017, **9**, 1097-1109.
127. R. Li, X. Wang, Z. Ji, B. Sun, H. Zhang, C. H. Chang, S. Lin, H. Meng, Y. P. Liao, M. Wang, Z. Li, A. A. Hwang, T. B. Song, R. Xu, Y. Yang, J. I. Zink, A. E. Nel and T. Xia, *ACS Nano*, 2013, **7**, 2352-2368.
128. S. Jain, V. S. Thakare, M. Das, C. Godugu, A. K. Jain, R. Mathur, K. Chuttani and A. K. Mishra, *Chem. Res. Toxicol.*, 2011, **24**, 2028-2039.
129. H. Nagai, Y. Okazaki, S. H. Chew, N. Misawa, Y. Yamashita, S. Akatsuka, T. Ishihara, K. Yamashita, Y. Yoshikawa, H. Yasui, L. Jiang, H. Ohara, T. Takahashi, G. Ichihara, K. Kostarelos, Y. Miyata, H. Shinohara and S. Toyokuni, *Proc. Natl. Acad. Sci. U. S. A.*, 2011, **108**, E1330-8.
130. B. Kang, S. Chang, Y. Dai, D. Yu and D. Chen, *Small*, 2010, **6**, 2362-2366.
131. H. Haniu, N. Saito, Y. Matsuda, Y. A. Kim, K. C. Park, T. Tsukahara, Y. Usui, K. Aoki, M. Shimizu, N. Ogihara, K. Hara, S. Takanashi, M. Okamoto, N. Ishigaki, K. Nakamura and H. Kato, *Int. J. Nanomedicine*, 2011, **6**, 3295-3307.
132. Y. Zhang, Y. Xu, Z. Li, T. Chen, S. M. Lantz, P. C. Howard, M. G. Paule, W. Slikker Jr, F. Watanabe, T. Mustafa, A. S. Biris and S. F. Ali, *ACS Nano*, 2011, **5**, 7020-7033.

133. M. H. Cato, F. D'Annibale, D. M. Mills, F. Cerignoli, M. I. Dawson, E. Bergamaschi, N. Bottini, A. Magrini, A. Bergamaschi, N. Rosato, R. C. Rickert, T. Mustelin and M. Bottini, *J. Nanosci Nanotechnol*, 2008, **8**, 2259-2269.

Figure legends

Figure 1 (A) TEM micrograph of MWNTs, clearly showing the high number of concentric carbon sidewalls and a 5 nm inner tube diameter. The outer walls of the MWNT are undamaged. **(B). SEM micrograph** of “as grown” MWNTs on a surface, also known as nanotube forest grown by chemical vapour deposition. These MWNTs are approximately 300 μm in length and 50 nm in diameter. On the top, remainder of the catalyst layer can be seen. **(C)** Sketch of the structure of carbon nanotubes showing different number of concentric carbon sidewalls

Figure 2. The three complement pathways: Classical, lectin and alternative pathways, have different recognition strategies. The classical pathway is activated by recognition and binding of antigen-antibody complexes binding via C1q, which in turn activates C1r and C1s. C1a, cleaves inactive C4 and C2 in sequence to form active C3 convertase, C4b2a. The lectin pathway is initiated by binding of mannose or carbohydrate moieties with MBL or ficolins activating membrane associated serine proteases (MASPs), which cleave C4 and C2 to form common C3 convertase (C4b2a). The alternative pathway is spontaneously activated by spontaneous lysis of C3 to C3b. Factor D cleaves factor B and forms C3 convertase (C3bBb) which in turn cleaves C3 leading to amplification of C3b formation and C5 convertase (C3bBbC3b). C3 convertase is stabilized by properdin while Factor H acts as an antagonist. Factor H inactivates C3b to form inactive iC3B. C5 convertase cleaves C5 forming C5B which combines with C6, C7, C8 and C9 to form membrane attack complex (MAC) leading to cell lysis. C3b acts as an opsonin and facilitates rapid macrophage mediated clearance of foreign particles. C4a, C3a and C5a acts as anaphylatoxins and enhance the inflammation

Figure 3. Overall structure of C1q and surfactant protein SP-D. (a) C1q is a charge pattern recognition protein (460 kDa), consisting of 18 homologous polypeptide chains (6A, 6B and 6C chains) with by a collagen like region (N terminal) with repeating Gly-X-Yaa triplets, and a globular head domain (C terminal), which bind to charge clusters or hydrophobic patches on targets. Each trimeric subunit has three globular head domains, called ghA, ghB, ghC. (b) SP-D has an N-terminal triple-helical collagen region, followed by a trimerising α -helical coiled-coil neck region, and C-terminal homotrimeric carbohydrate recognition domain (CRD). This

primary subunit structure can associate further to yield a cruciform tetrameric supramolecule.

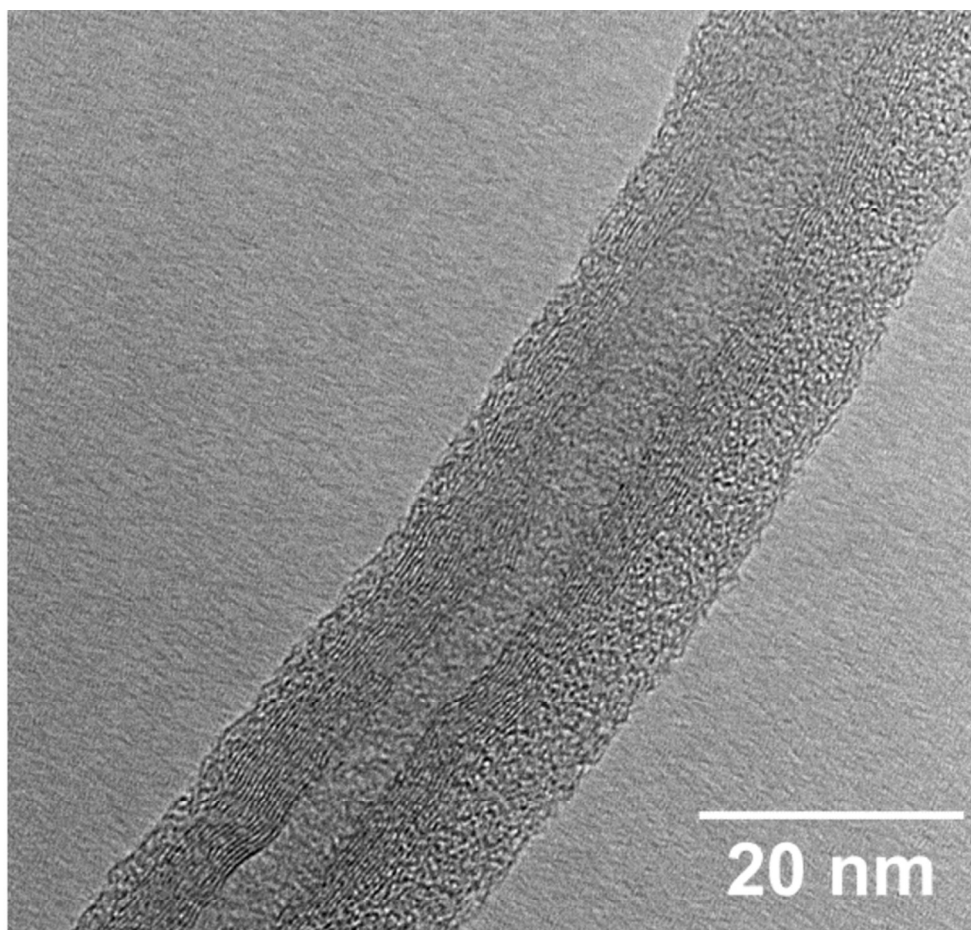


Fig1a

Figure 1a

77x84mm (300 x 300 DPI)

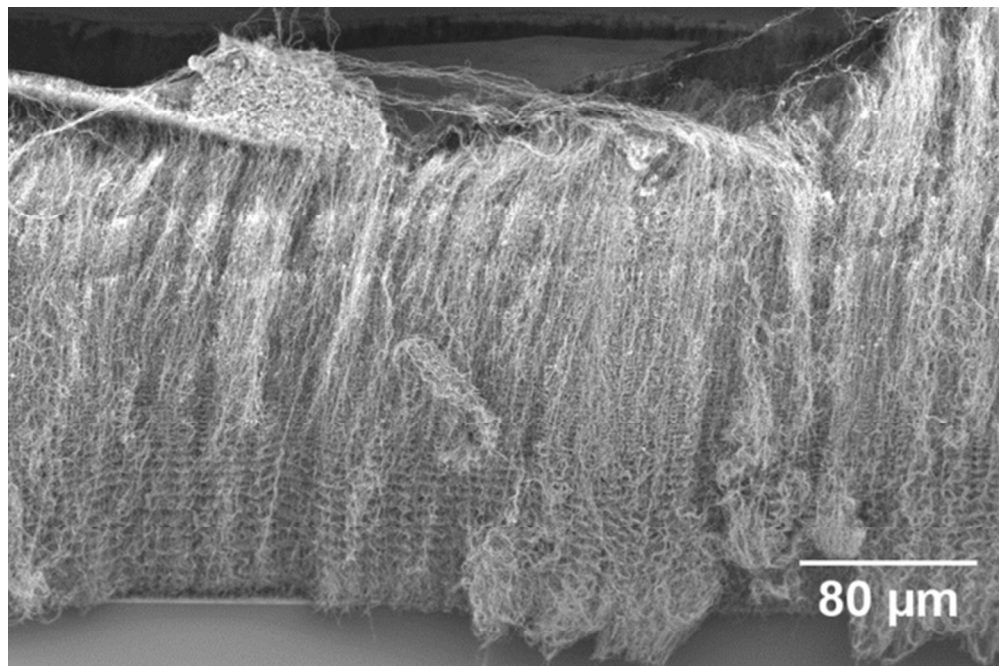


Fig1b

Figure 1b

57x47mm (300 x 300 DPI)

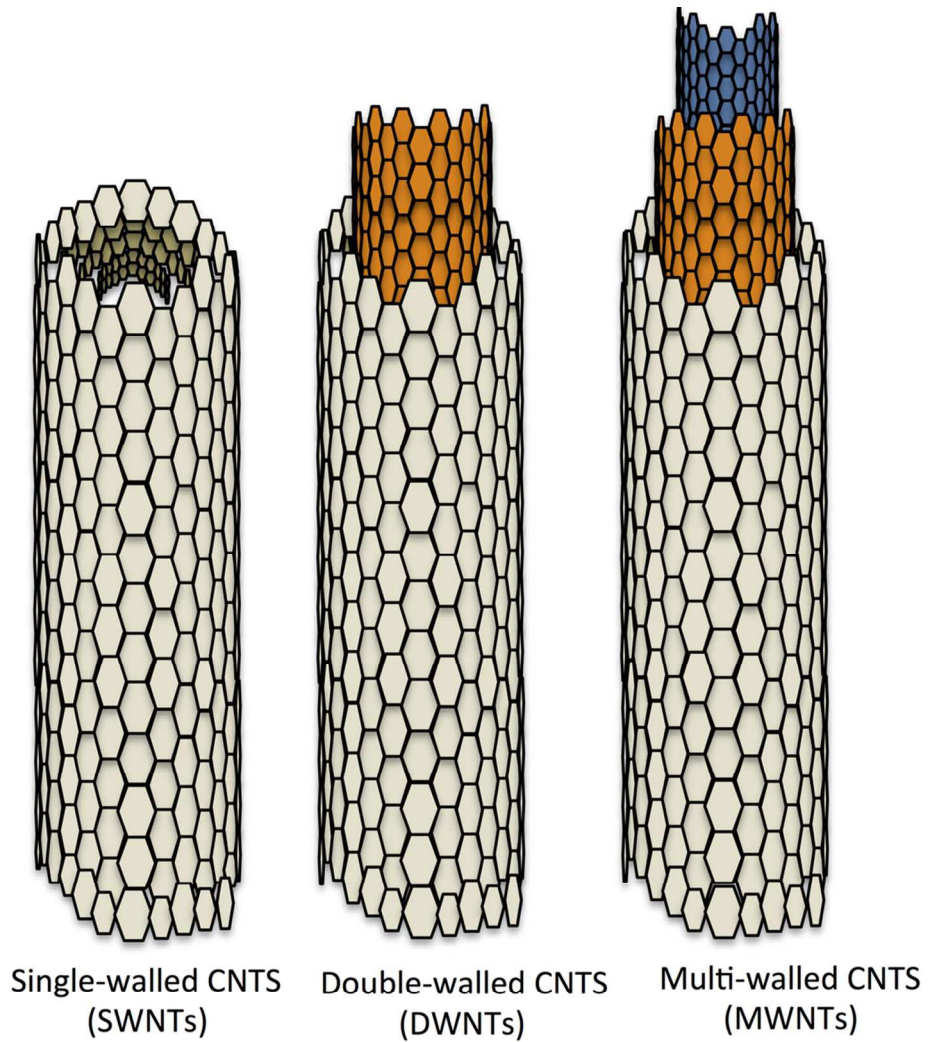


Fig1c

Figure 1c

94x122mm (300 x 300 DPI)

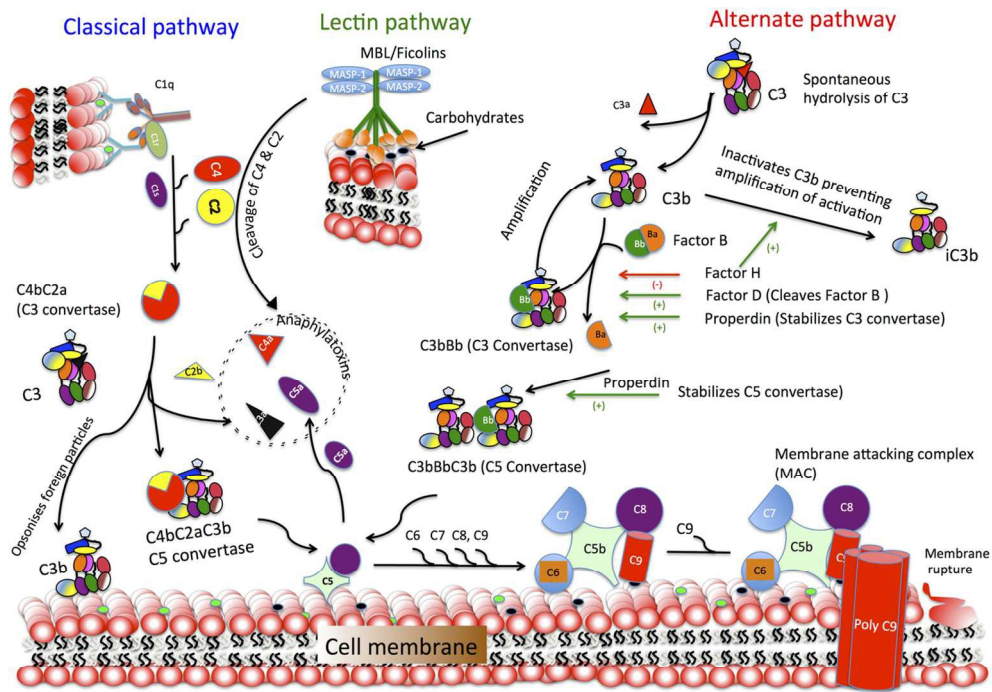


Fig 2

Figure 2

121x92mm (300 x 300 DPI)

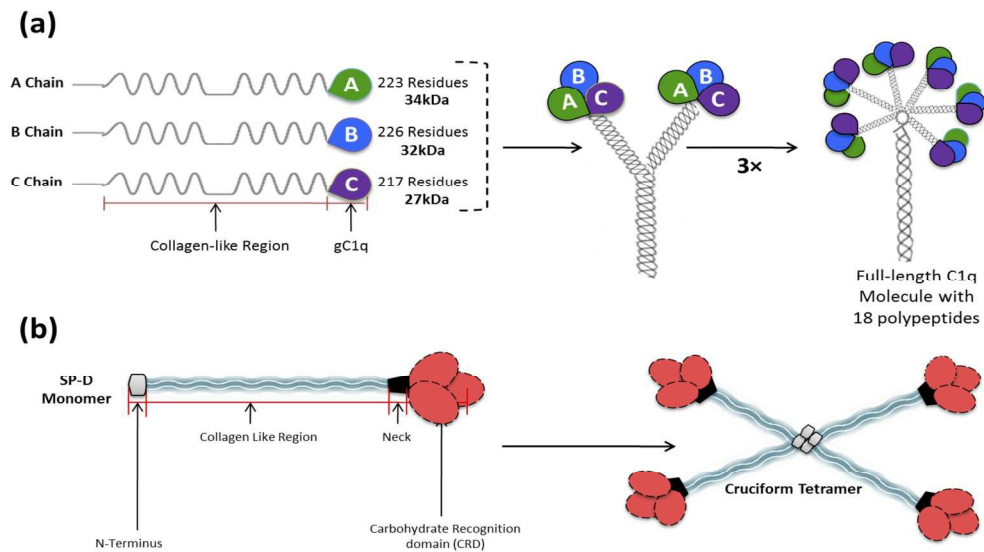


Fig 3

Figure 3

170x113mm (300 x 300 DPI)