

Survey on Different Image Fusion Techniques

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Abstract: In medical imaging and remote sensing, image fusion technique is a useful tool used to fuse high spatial resolution panchromatic images (PAN) with lower spatial resolution multispectral images (MS) to create a high spatial resolution multispectral of image fusion while preserving the spectral information in the multispectral image (MS). Image fusion is the process that combines information from multiple images of the same scene. The result of image fusion is a new image that retains the most desirable information and characteristics of each input image. Now-a-days, almost all areas of medical diagnosis are impacted by the digital image processing. When an image is processed for visual interpretation, the human eye is the judge of how well a particular method works. Clinical application demanding Radiotherapy plan, for instance, often benefits from the complementary information in images of different modalities. For medical diagnosis, Magnetic Resonance Image (MRI) is a medical imaging technique used in radiology to visualize internal structures of the body in detail. MRI provides better information on soft tissue with more distortion. Whereas, Computed Tomography (CT) provides the best information on denser tissue with less distortion. Wavelet transform fusion is more formally defined by considering the wavelet transforms of the two registered input images together with the fusion rule. Then, the inverse wavelet transform is computed, and the fused image is reconstructed. The wavelets used in image fusion can be classified into three categories Orthogonal, Bi-orthogonal and A' trous' wavelet. Although these wavelets share some common properties, each wavelet has a unique image decompression and reconstruction characteristics that lead to different fusion results. Since medical images have several objects and curved shapes, it is expected that the curvelet transform would be better in their fusion. In this paper the fusion results are compared visually and statistically. The simulation results show the superiority of the curvelet transform to the wavelet transform in the fusion of digital image and MR and CT images from entropy, difference entropy, quality measure, standard deviation, PSNR.

Keywords- Fusion, Wavelet transform, Curvelet Transform

I. Introduction

Image fusion has become a common term used within medical diagnostics and treatment. The term is used when multiple patient images are registered and overlaid or merged to provide additional information. Fused images may be created from multiple images from the same imaging modality,^[1] or by combining information from multiple modalities,^[2] such as magnetic resonance image (MRI), computed tomography (CT). CT images are used more often to ascertain differences in tissue density while MRI images are typically used to diagnose brain tumors.

Multisensor data fusion has become a discipline which demands more general formal solutions to a number of application cases. Several situations in image processing require both high spatial and high spectral information in a single image. This is important in remote sensing. However, the instruments are not capable of providing such information either by design or because of observational constraints. One possible solution for this is data fusion. Image fusion is the process of merging two images of the same scene to form a single image with as much information as possible. Image fusion is important in many different image processing fields such as satellite imaging, remote sensing and medical imaging [2]. Image fusion methods can be broadly classified into two groups - spatial domain fusion and transform domain fusion. The disadvantage of spatial domain approaches is that they produce spatial distortion in the fused image. Spectral distortion becomes a negative factor while we go for further processing, such as classification problem. Spatial distortion can be very well handled by frequency domain approaches on image fusion. The multiresolution analysis has become a very useful tool for analyzing remote sensing images. The discrete wavelet transform and curvelet transform based image fusion has become a very useful tool for medical and remote sensing images. These methods show a better performance in spatial and spectral quality of the fused image compared to other spatial methods of fusion. The images used in image fusion should already be registered.

Wavelet Transform has good time frequency characteristics. It was applied successfully in image processing field [3]. Nevertheless, its excellent characteristic in one-dimension can't be extended to two dimensions or multi-dimension simply. Separable wavelet which was spanning by onedimensional wavelet has limited directivity [4].

Aiming at these limitation, E. J. Candes and D. L. Donoho put forward Curvelet Transform theory in 2000 [5]. Curvelet Transform consisted of special filtering process and multi-scale Ridgelet Transform. It could fit image properties well. However, Curvelet Transform had complicated digital realization, includes sub-band division, smoothing block, normalization, Ridgelet analysis and so on. Curvelets pyramid decomposition brought immense data redundancy [6]. Then E. J. Candes put forward Fast Curvelet Transform(FCT) that was the Second Generation Curvelet Transform which was more simple and easily understanding in 2005[7]. Its fast algorithm was easily understood. Li Huihui's researched multi-focus image fusion based on the Second Generation Curvelet Transform [8]. This paper introduces the Second Generation Curvelet Transform and uses it to fuse images, different kinds of fusion methods are compared at last. The experiments show that the method could extract useful information from source images to fused images so that clear images are obtained.

II. Image Fusion Based On Wavelet Transform

The most common form of transform type image fusion algorithms is the wavelet fusion algorithm due to its simplicity and its ability to preserve the time and frequency details of the images to be fused.

Some generic requirements can be imposed on the fusion result. a) the fused image should preserve as closely as possible all relevant information contained in the input images. b) The fusion process should not introduce any artefacts or inconsistencies which can distract or mislead the human observer or any subsequent image processing steps. c) in the fused image irrelevant features and noise should be suppressed to a maximum extent. When fusion is done at pixel level the input images are combined without any pre-processing.

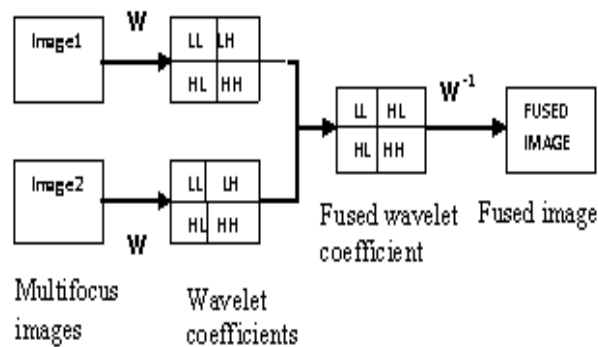


Fig.1 Block diagram of Discrete Wavelet transform

A schematic diagram of the wavelet fusion algorithm of two registered images $I_1(X_1, X_2)$ and $I_2(X_1, X_2)$ is depicted in fig.1. It can be represented by the following equation,

$$I(X_1, X_2) = W^{-1} \{ \Psi [W(I_1(X_1, X_2)), W(I_2(X_1, X_2))] \}$$

Where W , W^{-1} and ψ are the wavelet transform operator, the inverse wavelet transform operator and the fusion rule, respectively. There are several wavelet fusion rules that can be used for the selection of wavelet coefficients from the wavelet transforms of the images to be fused. The most frequently used rule is the maximum frequency rule which selects the coefficients that have the maximum absolute values. The wavelet transform concentrates on representing the image in multi-scale and it is appropriate to represent linear edges. For curved edges, the accuracy of edge localization in the wavelet transform is low. So, there is a need for an alternative approach which has a high accuracy of curve localization such as the curvelet transform.

III. Types Of Wavelet Transforms

A) Orthogonal Wavelet Transform

The dilations and translation of the scaling function $\phi_j, k(x)$ constitute a basis for V_j , and similarly $\Psi_j, k(x)$ for W_j , if the $\phi_j, k(x)$ and $\Psi_j, k(x)$ are orthonormal, they include the following property [1].

$$V_j \perp W_j$$

These results in a representation of a single image, containing multiscale detail information from all component images involved. This representation leads to multiple applications ranging from multispectral image fusion to color and multi-valued image enhancement, denoising and segmentation [9].

B) Bi-orthogonal Wavelet Transform

For biorthogonal transform, perfect reconstruction is available. Orthogonal wavelets give orthogonal matrices and unitary transforms; biorthogonal wavelets give invertible matrices and perfect reconstruction. For biorthogonal wavelet filter, the Low-pass and high-pass filters do not have the same length. The low pass and high pass filters do not have the same length. The low-pass filter is always symmetrical, while high pass filter could

be either symmetric or anti-symmetric. The method allows unusual flexibility in choosing a filter for any task involving the multiresolution analysis and synthesis. Using our method, one can choose any low-pass filter for the multiresolution filtering [1].

C) A'trous (Non-orthogonal) Wavelet Transform

A'trous is a kind of non – orthogonal wavelet that is different from orthogonal and biorthogonal. It is a stationary or redundant transform, i.e. decimation is not implemented during the process of wavelet transform, while the orthogonal or biorthogonal wavelet can be carried out using either decimation or undecimation mode [1]. The enhancement of the spatial information often leads to the distortion of the information in the spectral domain. In this paper, a spectral preserve fusion method is developed by introducing a'trous wavelet transform [10].

IV. Wavelet Transform Algorithm Steps

The process can be divided into four steps.

a) Histogram match

Apply the histogram match process between panchromatic image and different bands of the multispectral image respectively, and obtain three new panchromatic images PANR, PANG, PANB

b) Wavelet decomposition

Use the wavelet transform to decompose new panchromatic images and different bands of multispectral image twice, respectively.

c) Details information combination

Add the detail images of the decomposed panchromatic images at different levels to the corresponding details of different bands in the multispectral image and obtain the new details component in the different bands of the multispectral image and obtain the new details component in the different bands of the multispectral image.

d) Inverse wavelet transform

Perform the wavelet transform on the bands of multispectral images, respectively and obtain the fused image.

V. Image Fusion Based On Curvelet Transform

The curvelet transform is a multiscale directional transform that allows an almost optimal nonadaptive sparse representation of objects with edges. It has generated increasing interest in the community of applied mathematics and signal processing over the years. Most natural images/signals exhibit line-like edges, i.e., discontinuities across curves (so-called line or curve singularities). Although applications of wavelets have become increasingly popular in scientific and engineering fields, traditional wavelets perform well only at representing point singularities since they ignore the geometric properties of structures and do not exploit the regularity of edges.

The curvelet transform has evolved as a tool for the representation of curved shapes in graphical applications. Then, it was extended to the fields of edge detection and image denoising. Recently, curvelet transform used in image fusion. The algorithm of the curvelet transform of an image P can be summarized in the following steps:

A) The image P is split up into three subbands Δ_1, Δ_2 and P_3 using the additive wavelet transform.

B) Tiling is performed on the subbands Δ_1 and Δ_2 .

C) The discrete Ridgelet transform is performed on each tile of the subbands Δ_1 and Δ_2 .

A schematic diagram of the curvelet transform is shown in Fig.2

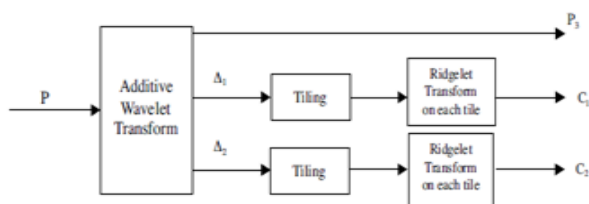


Figure 2. Discrete curvelet transform of an image P.

1. Subband Filtering:

The purpose of this step is to decompose the image into additive components; each of which is a subband of that image. This step isolates the different frequency components of the image into different planes without down sampling as in the traditional wavelet transform. Given an image P, it is possible to construct the sequence of approximations: $F_1(P)=P_1, F_2(P)=P_2, \dots, F_N(P)=P_N$. Where n is an integer which is preferred to be equal to 3. To construct this sequence, successive convolutions with a certain low pass kernel are performed. The

functions $f_1, f_2, f_3,$ and f_n mean convolutions with this kernel. The wavelet planes are computed as the differences between two consecutive approximations P_{l-1} and P_l i.e. $\Delta l = P_{l-1} - P_l$

Thus, the curvelet reconstruction formula is given by:

$$P = \sum_{l=1}^{n-1} \Delta l + P_1$$

2. Tiling:

Tiling is the process by which the image is divided into overlapping tiles. These tiles are small in dimensions to transform curved lines into small straight lines in the subbands $\Delta 1$ and $\Delta 2$. The tiling improves the ability of the curvelet transform to handle curved edges.

3. Ridgelet Transform:

The ridgelet transform belongs to the family of discrete transforms employing basis functions. To facilitate its mathematical representation, it can be viewed as a wavelet analysis in the Radon domain. The Radon transform itself is a tool of shape detection. So, the ridgelet transform is primarily a tool of ridge detection or shape detection of the objects in an image. The ridgelet basis function is given by,

$$\Psi_{a,b,\theta}(x_1,x_2) = a^{-1/2} \Psi[(x_1 \cos \theta + x_2 \sin \theta - b)/a]$$

for each $a > 0$, each $[b \in \mathbb{R}]$ and each $(\theta \in [0, 2\pi])$ this function constant along with lines $X_1 \cos \theta + X_2 \sin \theta = \text{constant}$. Thus the ridgelet coefficients of an image $f(x_1, x_2)$ are represented by:

$$R_f(a,b,\theta) = \iint_{-\infty}^{\infty} \Psi_{a,b,\theta}(x_1,x_2) f(x_1,x_2) dx_1 dx_2$$

This transform is invertible and the reconstruction formula is given by:

$$f(x_1,x_2) = \frac{\int_0^{2\pi} \int_{-\infty}^{\infty} R_f(a,b,\theta) \Psi_{a,b,\theta}(x_1,x_2) da db d\theta}{4\pi a}$$

The radon transform for an object F is the collection of line integrals indexed by $(\theta, t) \in [0, 2\pi] \times \mathbb{R}$ and is given by:

$$R_f(\theta, t) = \iint_{-\infty}^{\infty} f(x_1,x_2) \delta(x_1 \cos \theta + x_2 \sin \theta - t) dx_1 dx_2$$

Thus for ridgelet transform can be represented in terms of the radon transform as follows:

$$R_f(a,b,\theta) = \int_{-\infty}^{\infty} R_f(\theta, t) a^{-1/2} [(t-b)/a] dt$$

Hence, the ridgelet transform is the application of the 1-D wavelet transform to the slices of the Radon transform where the angular variable θ is constant and it is varying. To make the ridgelet transform discrete, both the Radon transform and the wavelet transform have to be discrete. It is known that different imaging modalities are employed to depict different anatomical morphologies. CT images are mainly employed to visualize dense structures such as bones. So, they give the general shapes of objects and few details. On the other hand, MR images are used to depict the morphology of soft tissues. So, they are rich in details. Since these two modalities are of a complementary nature, our objective is to merge both images to obtain as much information as possible.

VI. Wavelet And Curvelet Based Image Fusion Algorithm

1. First, we need pre-processing, and then cut the same scale from awaiting fused images according to selected region. Subsequently, we divide images into sub-images which are different scales by Wavelet Transform. Afterwards, local Curvelet Transform of every sub-image should be taken. Its sub-blocks are different from each others on account of scales' change.

2. Resample and registration of original images, we can correct original images and distortion so that both of them have similar probability distribution. Then Wavelet coefficient of similar component will stay in the same magnitude.

3. Using Wavelet Transform to decompose original images into proper levels. One low-frequency approximate component and three high-frequency detail components will be acquired in each level.

4. Curvelet Transform of individual acquired low frequency approximate component and high frequency detail components from both of images, neighborhood interpolation method is used and the details of gray can't be changed.

5. According to definite standard to fuse images, local area variance is chose to measure definition for low frequency component. First, divide low-frequency coefficients $C_{j_0}(k_1, k_2)$ into individual four square

subblocks which are $N1 \times M2$ (3×3 or 5×5), then calculate Standard deviation(STD) of the current sub-block and other statistical parameters.

VII. Results

In medicine, CT and MRI image both are tomography scanning images. They have different features. Fig. 3 shows CT image, in which image brightness related to tissue density, brightness of bones is higher, and some soft tissue can't be seen images. Fig. 4 shows MRI image, here image brightness related to an amount of hydrogen atom in tissue, thus brightness of soft tissue is higher, and bones can't be seen. There is complementary information in these images.

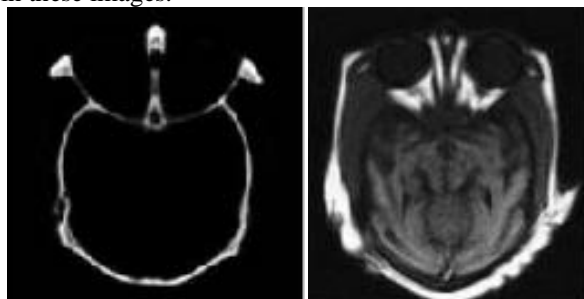


Fig. 3 CT Image of brain

Fig. 4 MRI Image of brain

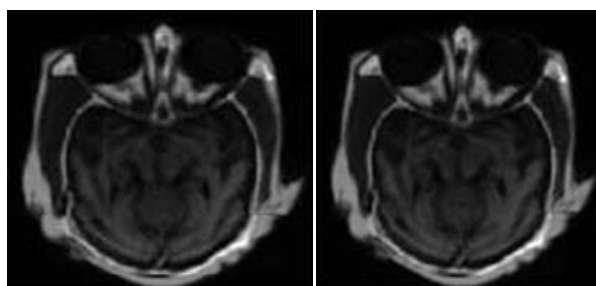


Fig.5a) Orthogonal Fused Image

Fig.5b) Biorthogonal Fused Image

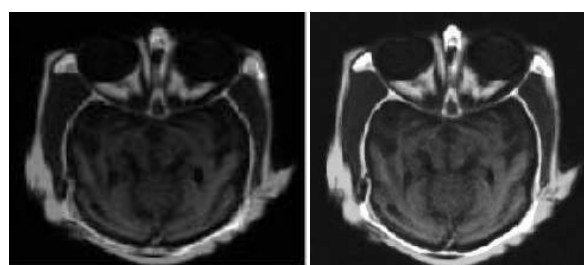


Fig. 5c) A' trous fused image

Fig.6 Fused Image of Wavelet Transform

Fig. 3 and fig. 4 represents the MRI and CT images of brain of same person respectively. In the MRI image the inner contour missing but it provides better information on soft tissue. In the CT image it provides the best information on denser tissue with less distortion, but it misses the soft tissue information. The fig. 5a image is the result of orthogonal wavelet fusion technique which is by combining of MRI and CT images. The orthogonal wavelet fused image have information of both images but have more aliasing effect. The fig. 5b image is the result of Biorthogonal wavelet fusion technique. When compare Biorthogonal wavelet with orthogonal wavelet it shows soft tissues information which are not shown in above figure i.e at the left and right side of the inner part. The fig. 5c image is the result of 'A trous' wavelet (non-orthogonal wavelet) based fusion. The fusion results of non-orthogonal wavelet have information on soft tissues and denser tissues.



Fig.7 Fused Image of Curvelet Transform

Since the curvelet transform is well-adapted to represent panchromatic image containing edges as shown in fig.7 and the wavelet transform preserves spectral information of original multispectral images as shown in fig.6, the fused image has high spatial and spectral resolution simultaneously. In addition to the visual analysis, we extended our investigation to a quantitative analysis. The experimental result was analyzed based on the combination entropy, standard deviation, quality measure as shown in table 1.

VIII. Quantitative Analysis

In order to compare the wavelet and curvelet based approaches; apart from visual appearance quantitative analysis is done over the fused images. For the visual evaluation, the following criterion is considered: natural appearance, brilliance contrast, presence of complementary features, enhancement of common features etc. The quantitative criterion [11] includes three parameters namely Entropy, Difference Entropy and Standard deviation. Each has its importance in evaluating the image quality.

1. Entropy: The entropy of an image is a measure of information content. The estimate assumes a statistically independent source characterized by the relative frequency of occurrence of the elements in X , which is its histogram. For a better fused image, the entropy should have a larger value.

2. Difference Entropy: It is calculated from taking the entropy of the image obtained from subtracting a source image from the fused image and the input source image.

Example: Fused image – CT Image = MRI Image Entropy [obtained MRI Image – Input MRI] gives Difference Entropy. The difference entropy between two images reflects the difference between the average amounts of information they contained. Minimum difference is expected for a better fusion.

3. Standard deviation: The standard deviation (SD), which is the square root of variance, reflects the spread in the data. Thus, a high contrast image will have a larger variance, and a low contrast image will have a low variance.

Table 1: Statistical parameters of Wavelet and Curvelet transform

FUSION METHODS	WAVELET TRANSFORM	CURVELET TRANSFORM
Entropy	5.05	5.823
Difference entropy	5.40	5.361
Standard deviation	62.03	69.29
Quality measure Q	0.891	0.90
RMSE	2.392	1.530

Quantitative analysis of the fused images indicates better results for curvelet transform based fusion with greater entropy, larger standard deviation and lower difference entropy than their wavelet equivalents. And among the curvelets, addition gives a better result. Moreover, compared with the fused results obtained by the wavelet and the curvelet, the curvelet based fusion result has a better visual effect, such as contrast enhancement.

IX. Conclusion

A comparison study has been made between the traditional wavelet fusion algorithm and the proposed curvelet fusion algorithm. The experimental study shows that the application of the curvelet transform in the fusion of MR and CT images is superior to the application of the traditional wavelet transform. In many important imaging applications, images exhibit edges and discontinuities across curves. In biological imagery, this occurs whenever two organs or tissue structures meet. Especially in image fusion, the edge preservation is important in obtaining the complementary details of the input images. As edge representation in Curvelet is better, Curvelet based image fusion is best suited for medical images.

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