

Faculty of Manufacturing Engineering

AUTOMATED POSTURAL ANGLE CLASSIFICATION USING MICROSOFT KINECT FOR ERGONOMICS ASSESSMENT

Tarek Mhd Moataz Albawab

Master of Science in Manufacturing Engineering

AUTOMATED POSTURAL ANGLE CLASSIFICATION USING MICROSOFT KINECT FOR ERGONOMICS ASSESSMENT

TAREK MHD MOATAZ ALBAWAB

A thesis submitted in fulfillment of the requirements for the degree of Master of Science in Manufacturing Engineering

Faculty of Manufacturing Engineering

UNIVERSITI TEKNIKAL MALAYSIA MELAKA

DECLARATION

I declare that this thesis entitled "Automated Postural Angle Classification Using Microsoft Kinect for Ergonomics Assessment" is the result of my own research except as cited in the references. The thesis has not been accepted for any degree and is not concurrently submitted in candidature of any other degree.

Signature	:	
Name	:	TAREK MHD MOATAZ ALBAWAB
Date	:	

C Universiti Teknikal Malaysia Melaka

APPROVAL

I hereby declare that I have read this thesis and in my opinion this thesis is sufficient in terms of scope and quality for the award of Master of Science in Manufacturing Engineering.

Signature	:	
Supervisor Name	:	DR. NADIAH BINTI AHMAD
Date	:	

C Universiti Teknikal Malaysia Melaka

DEDICATION

I would like to present my work to those who did not stop their daily support since I was born, my dear Father, my kindness Mother, and my treasured brothers and sister they never hesitate to provide me all the facilities to push me forward as much as they can. This work is a simple and a humble reply to their much goodness. I would like to take this opportunity to express my gratefulness to my uncle Ghassan and his children who believed in me and supported me at my most difficult time to get my degrees and achieve the best in my career. Last but not least, I would like to express the gratitude to all of my teachers, lecturers, and friends who advised me and gave me the courage to drive my career the perfect way it should be. Thanks to you all, much love.

ABSTRACT

Musculoskeletal injury is a common cause in manual material handling activities, where workers are exposed to repetitive picking and placing of materials, that therefore may lead to dangerous injuries if incorrect postures are made. It is the duty of factories to take care of the health conditions of their employees, and ensure the workplace is ergonomically designed. However, it is a difficult task to assess the work postures in a large number of employees all the time due to cost, lack of equipment, and lack of experience. The aim of this study is to formulate an ergonomic model to identify and classify body part motion angle ranges for upper limb postural analysis, to develop an automated real-time upper limb postural angle and classification system, and to evaluate the developed postural angle classification system using 30 participants in a lab setting and five ergonomic experts opinions. The chosen experts are individuals with experiences in ergonomics field working as academic researchers, consultancy agents, and industry management positions in Malaysia. Formulating the postural classification model applied the concepts of traffic light to categorise the work postures, where upper limb postures were classified into three classifications with mathematical models to count the number and percentage of each classification occurrence for each posture. The postural classification model was then integrated with a developed C# based software and a Microsoft Kinect sensor using heuristic approaches to do an automated real-time upper limb postural angle classification system. The developed postural classification was validated for 12 static postures, and 4 dynamic postures among 30 participants in a lab setting using Jamar goniometer (Sammons Preston Roylan, USA), a computerised protractor tool in ErgoFellow v3.0, and the statistical analysis used the root mean square error (RMSE). The evaluation was further explored by taking the ergonomic experts' opinions through semi-structured interviews to note the needful, usefulness, applicability, effectiveness, and the details provided for the workplace. The results of validation revealed that the static postures was 7.52 RMSE, dynamic postures was 21.93 RMSE, and combined static and dynamic results was 14.48 RMSE. The study shows better mean RMSE results than Plantard et al. (2017) study by 15.6% in static phase analysis, but larger mean RMSE in dynamic analysis which might be due to the method of capturing the reference angles. The study concluded that despite the acceptable RMSE results presented by the developed system, the software architecture and detection techniques require further improvement and development for better angle measurement accuracy with added parameters for ergonomics assessment.

ABSTRAK

Gangguan pada otot berangka adalah kecederaan fizikal yang disebabkan oleh aktiviti pengendalian manual seperti mengangkat dan mencapai bahan-bahan dalam keadaan postur kerja yang tidak selamat yang boleh menyebabkan kecederaan merbahaya pada otot. Adalah menjadi tugas majikan untuk menjaga kesihatan pekerja-pekerja mereka, dan memastikan tempat kerja direka secara ergonomik. Walau bagaimanapun, adalah satu tugasan yang mencabar bagi pengamal ergonomik untuk menilai postur kerja apabila melibatkan ramai pekerja di sepanjang masa disebabkan oleh kos, kekurangan peralatan yang sesuai dan kekurangan pengalaman. Objektif kajian ini adalah untuk merangkakan satu model ergonomik untuk mengenal pasti dan mengklasifikasikan julat sudut bahagian atas badan, untuk membangunkan satu sistem penilaian dan klasifikasi postur badan yang automatik dan masa nyata, dan untuk menilai sistem penilaian dan klasifikasi postur badan yang telah dibangunkan melibatkan 30 peserta untuk eksperimen makmal dan lima pakar ergonomik. Pakar terlibat adalah individu yang berpengalaman dalam bidang ergonomik yang berkerja sebagai penyelidik akademik, ajen konsultansi, dan penjawat jawatan pengurusan dalam industri di Malaysia. Kajian ini telah merumuskan model klasifikasi postur menggunakan konsep lampu isyarat yang mengkategorikan postur bahagian atas badan dalam tiga klasifikasi menggunakan model matematik untuk mengira bilangan dan peratusan kejadian untuk setiap postur. Model klasifikasi postural kemudian diintegrasikan dengan perisian berasaskan C # dan penderia Microsoft Kinect menggunakan pendekatan heuristik untuk membangunkan sistem klasifikasi sudut postur bahagian atas otot yang automatik dan masa nyata. Sistem penilaian dan klasifikasi postur badan yang dibangunkan ini telah disahkan berdasarkan 12 postur statik, dan 4 postur dinamik di kalangan 30 peserta eksperimen di dalam makmal menggunakan Jamar goniometer (Sammons Preston Roylan, Amerika Syarikat), alat protektif berkomputer di ErgoFellow v3.0, dan analisis statistik ralat punca min kuasa dua (RMSE). Pengesahan ke atas penilaian dan klasifikasi postur badan ini terus diterokai dengan mengambil kira pendapat ahli ergonomik melalui wawancara separa berstruktur untuk menentukan keperluan, kebolehgunaan, keberkesanan, dan butiran yang diperlukan untuk penilaian ergonomik di tempat kerja. Hasil pengesahan mendedahkan bahawa postur statik adalah 7.52 RMSE, postur dinamik adalah 21.93 RMSE, dan gabungan statik dan dinamik adalah 14.48 RMSE. Kajian menunjukkan hasil RMSE lebih baik daripada kajian Plantard et al. (2017) sebanyak 15.6% dalam analisis fasa statik, tetapi lebih besar RMSE dalam analisis dinamik yang mungkin disebabkan oleh kaedah menangkap sudut rujukan. Kajian ini menyimpulkan bahawa walaupun keputusan RMSE ini berada di tahap boleh diterima, teknik dan kaedah pengesanan yang digunapakai oleh sistem penilaian dan klasifikasi postur badan yang dibangunkan ini memerlukan penyelidikan dan pembangunan yang selanjutnya untuk ketepatan pengukuran sudut yang lebih baik dengan parameter tambahan untuk penilaian ergonomik.

ACKNOWLEDGEMENTS

First praise is to Allah, the Almighty, on whom ultimately we depend for sustenance and guidance. Second, my sincere appreciation goes to my supervisors Dr. Nadiah Binti Ahmad, Dr. Isa Bin Halim, and Dr. Zaid @ Radin Zaid Bin Radin Umar for their guidance, and support all along to get this research work done. Their time and effort were much appreciated.

I would not have been able to complete this without amazing people for whose help I am immeasurably grateful, my deepest gratitude goes to my beloved parents; my brothers and sister; my uncle and cousins; and my lecturers and teachers for their continuous love, support, understanding and good wishes whenever I needed.

Finally, I thank all my friends who have helped me directly or indirectly in the successful completion of my thesis. Anyone missed in this acknowledgement are also thanked.

I could not have done any of this without you. Thank you all.

iii

TABLE OF CONTENTS

DEC	CLARA	ATION	
APH	ROVA	AL	
DEI	DICAT	ION	
ABS	STRAC	CT	i
ABS	STRAK	X	ii
ACI	KNOW	/LEDGEMENTS	iii
TAI	BLE O	F CONTENTS	iv
LIS	T OF 1	ΓABLES	vi
LIS	T OF F	FIGURES	ix
LIS	T OF A	APPENDICES	xii
LIS	T OF A	ABBREVIATIONS	xiii
LIS	T OF F	PUBLICATIONS	XV
CH	артеб	R	
1.	INT	FRODUCTION	1
	1.1	Background	1
	1.2	Problem statement	4
	1.3	Research objectives	6
	1.4	Research scope	6
	1.5	Methodology	8
	1.6	Thesis layout	10
2.	LIT	TERATURE REVIEW	12
	2.1	Introduction	12
	2.2	Risk factors and assessments review	12
		2.2.1 Work related musculoskeletal disorder (WMSDS) and	10
		risk factors	12
		2.2.2 Ergonomics assessment and risk factors	10
		2.2.3 Sampling and analytical tools assessments	19
	2.3	Efforts to automate the process of ergonomics assessment in	
		in the workplace	21
		2.3.1 Kinect RGB-D camera and review works	22
	2.4	2.3.2 Kinect in different methodologies	30
	2.4	I neoretical framework	33 25
	2.3	Summary	55
3.	ME	THODOLOGY	36
0	3.1	Introduction	36
	3.2	Body part motions definitions of the study	38
	3.3	Postural angle classification technique	41
	3.4	Type of sensor	45
	3.5	Position of the sensor and respective coordinates	46
	3.6	Software architecture and algorithmetic approach	47
	3.7	Mathematical modelling of postural angles measurement	49
	3.8	Mathematical modelling of the postural angle classification	53

	3.9	Softwar	re development and programming	61	
	3.10	Evaluate the RMSE values of the body part motions' angles			
		Measur	rement	69	
		3.10.1	RMSE analysis of the static standard operating procedure		
			experiment	71	
		3.10.2	RMSE analysis of the dynamic standard operating procedure		
			experiment	73	
		3.10.3	Methodology validation of angle measurement of the developed system	76	
	3.11	Evaluat	te the use of the postural angle classification system with		
		ergonoi	mics experts	78	
	3.12	Summa	ury	79	
4.	RES	ULT AN	ND DISCUSSION	80	
	4.1	Introdu	ction	80	
	4.2	The dev	veloped software	80	
	4.3	Validat	ion of angle measurement of the developed system	84	
		4.3.1	Static-motion phase experiment	86	
		4.3.2	Dynamic-motion phase experiment	90	
		4.3.3	Overall experimental results	95	
	4.4	Postura	l angle classification system	95	
		4.4.1	Application of the postural angle classification system	97	
		4.4.2	Postural angle classification system evaluation with		
		~	ergonomics experts	105	
	4.5	Summa	ıry	107	
5.	CON	CLUSI	ON AND RECOMMENDATIONS FOR FUTURE WORK	109	
	5.1	Conclu	sion	109	
	5.2	Achiev	ement of research objective	110	
	5.3	Contrib	bution of research	111	
	5.4	Signific	cance of research	111	
	5.5	Limitat	10n of research	111	
	5.6	Recom	mendations and future work	113	
REFE	REN	CES		114	
APPE	NDIC	ES		128	

LIST OF TABLES

TABLE	TITLE	PAGE
2.1	Various research works studies for WMSDs occurence in different industries in Malaysia	15
2.2	Various research works noting on the use of sampling methods in ergonomics	20
2.3	Definitions of postural motions with various research works with Kinect device	25
2.4	Various research works on postural angle performance measurement of Kinect	26
2.5	Various statistical analysis methodologies for Kinect performance in postural angle measurement	29
2.6	Research papers on using Kinect device with ergonomics assessment tools	31
3.1	Body part motions used for this study	41
3.2	Postural angle classification of the selected body part motions	43
3.3	Body part motions measurement reference lines	51
3.4	Mathematical equations to make the measurement of different body part motions with respect to relative motions	52
3.5	Postural angle classifications for different body part motions	56
3.6	Mathematical equations of postural angle classification evaluation for each body part motion	59
3.7	Mathematical equations of postural angle classification evaluation for the overall study	60
3.8	Kinect's (XYZ) reference lines as implemented in the developed software	63
3.9	Skeletal joints' (XYZ) vectorisation as implemented in the developed	64

software

3.10	Body part motions with respect to axes vectorisation as implemented in the developed software	65
3.11	Calibration of body part motions with respect to various laboratory experiments as implemented in the developed software	66
3.12	Heuristic approach for each postural classification as implemented in the developed software	67
3.13	Measured angles for the static postural analysis	73
3.14	Selected postural measurement angles for static and dynamic RMSE analyses	77
4.1	RMSE values of Kinect performance for each postural motions in a different pre-determined goniometer reference angles in a static analysis	88
4.2	Chosen DOE for Plantard et al. and this research for measuring the RMSE rate of static phase analysis	89
4.3	RMSE results comparison between Plantard et al. and this research in static phase analysis	89
4.4	RMSE values of Kinect performance for flexion motions of each body part motion in a different pre-determined dynamic SOP analysis	93
4.5	DOE design for Plantard et al. and this research for measuring the RMSE rate of dynamic phase analysis	94
4.6	RMSE results comparison between Plantard et al. and this research in dynamic phase analysis	94
4.7	Three testers in four phases of dynamic postural motions	100
4.8	Body part motions' angles for each tester in all tasks of the study	103
4.9	Postural classification EMN evaluation for each body part motion of each tester in the study	104
4.10	Cumulative percentage of postural classification %UIA for each body part motion of each tester in the study	104
4.11	Cumulative percentage of postural classification %UIA for each tester and overall evaluation	104
4.12	Cumulative percentage of postural classification %UIA for each sub- task of the overall study	105

LIST OF FIGURES

FIGURE	TITLE	PAGE
1.1	Flowchart of the research stages	10
2.1	Muscloskeletal disorders per 100,000 workers in UK (UK Department of Health and Safety Executive, 2017)	15
2.2	Illustration of some risk factors faced in different industries (Stack et al., 2016)	16
2.3	Features' characteristics when assessing human body with external loads (Roman-Liu, 2014)	17
2.4	Classifying assessment tools on the basis of input data (Roman- Liu, 2014)	17
2.5	Kinect RGB-D Camera external diagram (Kramer et al., 2012)	22
3.1	Flowchart process of creating the methodology for developing this research automated postural classification system	37
3.2	Body part motions' definitions of this research developed software	39
3.3	Points detected by Kinect joint tracking algorithm (Diego-Mas and Alcaide-Marzal, 2014a)	40
3.4	Planes of movement (Palma et al., 2016)	40
3.5	Various research papers reviewed on postural angle classification	44
3.6	Flowchart evaluation of choosing the suitable type of sensor for	46
	the study	

viii

3.7	A person standing in front of Kinect camera with upper arms 90° abducted (T-Pose) 4			
3.8	Process flowchart of the software development and validation			
3.9	Process flowchart of the user interaction with the software	49		
3.10	Postural joints of a human standing in the frontal view as detected by Kinect			
3.11	Relative angle of Elbow Flexion/Extension (Souza and Stemmer,	52		
	2018)			
3.12	Flowchart of the postural classification technique	54		
3.13	Joints and motions sampling selection from the software	55		
3.14	Pseudocode of postural angle measurement algorithm	62		
3.15	Pseudocode of postural angle classification algorithm	63		
3.16	Flowchart of the entire developed software 6			
3.17	Flowchart thinking process of developing the analysis methods			
	for the study	70		
3.18	Setup experiment for static postural validation	71		
3.19	Measurement taken from the goniometer for various body part motions 7			
3.20	Side-orthogonal view of the dynamic SOP 74			
3.21	Phases of motions of the dynamic experimental analysis 7			
3.22	Dynamic postural validation study (Albawab et al., 2019) 7			
3.23	Flowchart thinking process on developing the experts' evaluations on the developed postural classification technique 79			
4.1	Developed user interface showing a human posture in the frontal view of Kinect device	81		
4.2	Postural motion plotted angles data for upper arm flexion/extension as detected by Kinect	82		

4.3	Postural motion plotted categorisation data for upper arm flexion/extension as detected by Kinect	82
4.4	Overall quantitative and qualitative results of the designed research study	83
4.5	Flowchart of the overall developed software	83
4.6	A pre-measured motion angle by Jamar goniometer for upper arm flexion (Static-Motion Analysis)	85
4.7	Measuring Upper Arm Flexion/Extension using computerized protractor tool in ErgoFellow v3.0 software (Dynamic-Motion Analysis)	
4.8	RMSE value of the Kinect developed software in static postural measurement	87
4.9	RMSE values of the Kinect developed software in dynamic phase for each postural motions	92
4.10	RMSE values of the Kinect developed software in each phase in the dynamic phase	92
4.11	Overall RMSE performance of the Kinect developed software in static and dynamic phases	95
4.12	Flowchart of the process to use the developed postural angle classification method	96
4.13	Postural classification for various body part motions	97
4.14	EMN and UIA classification for each body part motion of participant 1	101
4.15	EMN and UIA classification for each body part motion of participant 2	101
4.16	EMN and UIA classification for each body part motion of participant 3	102
4.17	UIA classification for overall study of each participant and overall experimental study	102
4.18	UIA classification for each sub-task of the study	103

LIST OF APPENDICES

APPENDIX	TITLE	PAGE
А	Data collection among 30 participants performing static postures in a lab setting	128
В	Data collection among 30 participants performing dynamic postures in a lab setting	132
С	Data collection from Plantard et al. (2017) research study	136
D	Privacy statement and consent form	138
Е	Survey sheets for ergonomics experts evaluation on the developed system	140

LIST OF ABBREVIATIONS

А	-	Acceptable postural angle classification
AoM	-	Angle of Motion
CMC	-	Coefficient of Multiple Correlation
CV	-	Coefficient of Variation
CVME	-	Coefficient of Variation of Method Error
DOE	-	Design of Experiment
Е	-	Excessive postural angle classification
EF	-	Elbow Flexion
eq.	-	Mathematical Equation
Ι	-	Investigate postural angle classification
IR	-	Infrared sensor
ICC	-	Intraclass correlation coefficient
IMU	-	Inertial Measurement Unit
j	-	joint or body part motion
K	-	Kinect
LEF	-	Left Elbow Flexion
LOA	-	Limit of Agreement
LUAA	-	Left Upper Arm Abduction
LUAF	-	Left Upper Arm Flexion

xii

М	-	Moderate postural angle classification
MBS	-	Marker Based System
MIS	-	Minimally Invasive Surgery
MLS	-	Marker-Less System
MoCAP	-	Motion Capturing System
Ν	-	Neutral postural angle classification
NF	-	Neck Flexion
NLLF	-	Neck Left Lateral Flexion
NRLF	-	Neck Right Lateral Flexion
OLP	-	Ordinary Least Product
REF	-	Right Elbow Flexion
RGB-D	-	RGB camera with Depth sensing
RMSE	-	Root Mean Square Error
ROM	-	Range of Motion
RUAA	-	Right Upper Arm Abduction
RUAF	-	Right Upper Arm Flexion
SOP	-	Standard Operating Procedure
TF	-	Trunk Flexion
TLLF	-	Trunk Left Lateral Flexion
TRLF	-	Trunk Right Lateral Flexion
U	-	Urgent postural angle classification
UAF	-	Upper Arm Flexion
UI	-	User Interface
WMSD	-	Work related Musculoskeletal Disorder

LIST OF PUBLICATIONS

JOURNAL:

 Albawab, T. M. M., Halim, I., Ahmad, N., Umar, R.Z.R., Mohamed, M.S.S., Abdullais, F., Basari, A.S.H., Bakar, M., Saptari, A., 2019, 'Upper Limb Joints and Motions Sampling System Using Kinect Camera', *Journal* of Advanced Manufacturing Technology, 12(2), pp. 147–158.

CHAPTER 1

INTRODUCTION

1.1 Background

Work-related musculoskeletal disorders (WMSDs) are common injuries in a workplace environment which affect the various anatomical sites of the human body including muscles, joints, and nerves. As stated in the annual report of 2017 in Health and Safety Executive (HSE) in the UK, a total of 45% of disorders are from upper limbs or neck, followed by 38% from backs, and 17% from lower limbs' joints. Awkward postures are one of the risk factors that mostly cause WMSDs. It is highlighted that manual materials handling, repetitive motion in awkward or strenuous postures are the main causes of these disorders (UK Department of Health and Safety Executive, 2017). Marcum et al. (2017) reported the WMSDs from the year 1999 to 2013 in different sectors of the industry, and it is found that overexertion due to manual handling and poor postures are the most prevalent causes of these WMSDs. Lifting, pulling and repetitive works were the highest proportion of the overall overexertion reported. Wang et al. (2016) did a review on WMSDs among workers in construction sites in the US from the year 1992 to 2014, and it is noted that the US managed to reduce the WMSDs by 60% in 2014 as compared to the past historical data, and the most musculoskeletal injuries were due to overexertion, poor postures, and repetitive motions.

Wilson et al. (2000) stated ergonomics is the only science that ensures the technology and workplace are suited for human performance. The paper further

emphasised the importance of ergonomics science in our daily life and defined how ergonomics would enhance the quality of work and human development.

From the point of human care and development, various assessment models and tools have been developed to assess the exposure of workers to injury risks with the goal of preventing WMSDs. And perhaps one of the very first assessment tools that are made as a measure for human development at work is the work done by Karhu et al. (1977) with his paper "Correcting working postures in industry: A practical method for analysis". The paper introduced a practical reference for future assessments called the Ovako Working Posture Analysing System (OWAS).

Karhu et al. (1977) made the assessment to be as an observational method to evaluate the human postural working performance in industry and set the measures to know which and what to redesign and enhance in the workplace. This tool was the inspiration for future assessment tools, and one of it was the work done by Mcatamney et al. (1993) in his assessment tool called Rapid Upper Limb Assessment (RULA).

RULA is designed to assess the human upper limb postures by making two categorisations "A" and "B" for postural angles, postural support, muscle use, and force or load exertion. The two categorisations "A" and "B" seperate arm and wrist from the neck, trunk, and leg analysis. And the final results of both category assessment are tabulated in "C" category, and combined to make an abstracted decision for the whole work done in four categorial scoring as: "acceptable", "further investigation and change may be needed", "further investigation and change soon", and "investigate and implement change". With the clarity that the assessment gave, it became so popular in the 21st century, and many trials were made to implement this assessment with computerised methods. However, the identification of postural movement is very challenging, since human posture is very dynamic with high movement degrees of freedom, and various body types and topologies.

Moreover, the traditional practices usually only consider the worst case postural scenario in the ergonomics assessment, in which it reduces the quality of ergonomics effectiveness in industry.

There have been efforts to do detection of human postural motions using computerised methods to facilitate the analysis of human postures and get as much information as possible on the effect of workplace design on human postures, despite the observation challenges such as occlusion and environmental effects on electronics (Karhu et al., 1977; Mcatamney et al., 1993; Lehrmann et al., 2014; Mohamed, 2015). The interest of studying human postural motions appeared since ages, and perhaps it starts to be a highly researched topic when the power of computers started to exist in human life. Since the late 1970s, researchers have set their lives to find optimised ways to study the human motions in a real-time using computerised methods (Mohamed, 2015; Elmadany et al., 2018; Negin et al., 2018). Cristani et al. (2013) discussed the aspects of the analysis of human activity for computer vision based systems. Aspects can be concluded as physical, poses and postures, and environmental characteristics. Designing an automated real-time postural analysis system contributes to agile decision making for workplace assessment to reduce the human risk factors, and it provides a better electronic documentation of each individual to monitor performances over time (Wilson, 2000; Mohamed, 2015).

In 2010, a new, innovative, and cost-effective technology came into sight, with its ability to do high-speed human motion analysis. This technology combines the power of depth sensing with the two-dimensional RGB cameras to create a three-dimensional spatial analysis of the scenes. This RGB-D camera is called Kinect. And since its release, researchers showed a significant interest to use it for solving the dream of a real-time human motion analysis (Han et al., 2013; Shotton et al., 2013). Kinect provides a simplified tool to enable a software developer to track the skeletal motions related to its

joints (Cruz et al., 2012). According to author's reviews of various usage of Kinect with ergonomics assessments, it is found that papers experimented on ergonomics assessment tools with Kinect were: Rapid Upper Limb Assessment (RULA), Ovako Workplace Assessment (OWAS), and Rapid Entire Body Assessment (REBA).

The focus of this research is to provide a software design model to study the kinematics of human motion in industry. This research then apply the ergonomics assessment principles to evaluate the postural movement of workers in the industry for the purpose of determining the risk level exposed in the workplace. The study evaluates the upper limb postural analysis, by categorising sets of angle ranges for the upper limb on the basis of earlier published research studies, especially the researches done by Bao et al. (2009) and Juul-Kristesen et al. (1997). In order to study the human postural movement, first, it is important to set the definition of body part motions in relation to body joints for this software development. Providing an abstracted definition of body part motions relation will enable a better understanding of the human postural motion and better integration and implementation with other assessment tools. The scope of this study is more to action recognition and analysis for ergonomics science.

1.2 Problem statement

WMSDs are still presenting a significant negative effect on industries and countries Marcum et al. (2017). The negative effects as reported by the latest UK's HSE for 2017/18 show that 14.9 billion euros were wasted for work-related injuries, 0.5 million people suffer from WMSDs, and 31.2 million days were wasted due to working days lost (UK Department of Health and Safety Executive, 2018). Making the working environment fit the human body needs changes in system designs and approaches, together with developing profession and discipline. System designs and approaches should not only be based on financial costs, but also on how to boost the safety and health of the human body in the workplace. Giving the care on human development in the industry will contribute to a better image of companies, and boost the performance and productivity (Dul et al., 2012).

Despite the movement towards Industry 4.0 that emphasises automation, the human workers existence is still vital as most mass production industries are assembly workbased, and in this, the human is still more capable than any machine (Hecklau et al., 2016; Pfeiffer, 2016). Ergonomics has to be at the center of any design or development involving human, and it is the role of ergonomics scientists to provide a tool that will empower the use of the ergonomics science in the industry. Finding solutions to empower ergonomists to do assessments in a more feasible and economical way is needed.

Ergonomists encounter challenges in assessing the workplace design and workers' performance. The challenges include not being able to make detailed reports of the whole work duration, all population in the industry, and the full working postures with all of its dimensions. Current assessments tend to make use of only a sample of working time and worker population which only gives abstracted knowledge of the scenes, while depending on observational methods for making decisions. These abstracted observational methods lacks of detailed reports on what body part motions are most affected, as the current assessment tool. Moreover, the tools used are tedious and time-consuming, as they are done manually with a specified time and workers' population in the industry (Kilbom, 1994; Bao et al., 2009; Takala et al., 2010; Abd Rahman, 2011).

Therefore, there is a need for a tool that allows for a more comprehensive analysis of postures and can present the distribution of postural dynamics throughout the work duration. There is a research gap of having a computerised system that is able to be used