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## Imaging Radiation-Induced Normal Tissue Injury

Mike E. Robbins<sup>a,c,1</sup>, Judy K. Brunso-Bechtold<sup>b,c</sup>, Ann M. Peiffer<sup>a,c</sup>, Christina I. Tsien<sup>d</sup>, Janet E. Bailey<sup>e</sup>, and Lawrence B. Marks<sup>e</sup>

<sup>a</sup>Departments of Radiation Oncology, Wake Forest University School of Medicine, Winston-Salem, North Carolina

<sup>b</sup>Neurobiology & Anatomy, Wake Forest University School of Medicine, Winston-Salem, North Carolina

<sup>c</sup>Brain Tumor Center of Excellence, Wake Forest University School of Medicine, Winston-Salem, North Carolina

<sup>d</sup>Department of Radiation Oncology, University of Michigan, Ann Arbor, Michigan

<sup>e</sup>Department of Radiation Oncology, University of North Carolina Chapel Hill, Chapel Hill, North Carolina

### Abstract

Technological developments in radiation therapy and other cancer therapies have led to a progressive increase in five-year survival rates over the last few decades. Although acute effects have been largely minimized by both technical advances and medical interventions, late effects remain a concern. Indeed, the need to identify those individuals who will develop radiation-induced late effects, and to develop interventions to prevent or ameliorate these late effects is a critical area of radiobiology research. In the last two decades, preclinical studies have clearly established that late radiation injury can be prevented/ameliorated by pharmacological therapies aimed at modulating the cascade of events leading to the clinical expression of radiation-induced late effects. These insights have been accompanied by significant technological advances in imaging that are moving radiation oncology and normal tissue radiobiology from disciplines driven by anatomy and macrostructure to ones in which important quantitative functional, microstructural, and metabolic data can be noninvasively and serially determined. In the current article, we review use of positron emission tomography (PET), single photon emission tomography (SPECT), magnetic resonance (MR) imaging and MR spectroscopy to generate pathophysiological and functional data in the central nervous system, lung, and heart that offer the promise of, (1) identifying individuals who are at risk of developing radiation-induced late effects, and (2) monitoring the efficacy of interventions to prevent/ameliorate them.

### INTRODUCTION

Radiation therapy (RT) remains one of the major treatment options for cancer patients; approximately 60% of all newly-diagnosed patients will receive RT sometime during the course of their treatment (1). RT represents a targeted, noninvasive, and potentially organ-preserving therapy. However, the total dose that safely can be administered to a tumor is limited by the risk of both acute- and late-radiation-induced injury to those normal tissues unavoidably included in the treatment volume. Ongoing advancements in RT and other

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<sup>1</sup>Address for correspondence: Room 412C NRC, Department of Radiation Oncology, Wake Forest University School of Medicine, Medical Center Blvd., Winston-Salem, NC 27157; [mrobbins@wfubmc.edu](mailto:mrobbins@wfubmc.edu).

cancer therapies have resulted in a progressive increase in five-year survival rates over the last 50 years; 68% of adult and 81% of pediatric cancer patients now survive beyond five years (2). In general, acute effects have been minimized by both technical advances and medical interventions. However, for the ~12 million long-term survivors, there are no proven interventions to prevent or mitigate radiation-induced late effects. Thus, the need to, (1) identify those individuals who will develop radiation-induced late effects, and (2) develop interventions to prevent or mitigate these radiation-induced late effects is currently recognized as a critical area of radiobiology research (3).

Preclinical studies carried out over the last two decades clearly demonstrate that radiation-induced late effects arise not simply from mitotic cell death of specific target cell clonogens, but more importantly, from complex and dynamic interactions between multiple cell types within an organ (4–7). Thus, normal cells are active participants in the response to injury that is hypothesized to initiate an ongoing, chronic process that leads to progressive damage. Although the exact specific pathogenic mechanisms remain to be determined, late radiation injury can be prevented/ameliorated by pharmacological therapies focused on modulating steps in the cascade of events leading to the clinical expression of radiation-induced late effects (8).

These recent advances in our understanding of how radiation-induced late effects develop and how they can be modulated have been accompanied by significant technological advances in imaging that offer the promise of identifying individuals who are at risk for developing radiation-induced late effects. Thus, normal tissue radiobiology is moving from a discipline utilizing conventional histologic analysis of fixed tissues from many experimental groups with large numbers of animals collected over many time points, to one in which noninvasive *in vivo* imaging enables serial assessment of pathophysiological and functional processes in fewer groups with smaller numbers of animals, where each animal serves as its own control (9, 10). This process has also been facilitated by advances in clinical imaging that have shifted radiation oncology from a discipline driven by anatomy and structure to one in which important quantitative functional data can be determined (11, 12).

[<sup>18</sup>F] fluorodeoxyglucose (FDG) positron emission tomography (PET) imaging provides functional data on normal tissue metabolic activity, while other radiotracers can image physiologic parameters such as angiogenesis (13), hypoxia (14), cardiac function (15), and brain function (16). Single photon emission computed tomography (SPECT) has been used to measure perfusion (17). Magnetic resonance imaging (MRI) has become increasingly important with its ability to assess functional metrics including regional perfusion (18), lung ventilation (19), and brain structure, as well as function (20, 21); In addition, metabolic states can now be assessed with MR spectroscopy (MRS) (22). More recently, multimodality imaging with PET/CT and SPECT/CT has become commonplace in radiation oncology, and ongoing research is investigating combining PET or SPECT with MRI (23). In the current article, we review the use of pathophysiological and functional imaging that offers the promise of, (1) identifying individuals who are at risk for developing radiation-induced late effects and (2) monitoring the efficacy of interventions to prevent or mitigate them. Our focus will be on central nervous system (CNS), lung, and cardiac normal tissues, and will include discussions of opportunities for future research in this field.

## CNS Injury

Based on the time of clinical expression, radiation-induced brain injury is described in terms of acute, early-delayed, and late-delayed reactions (5). Acute injury (acute radiation encephalopathy), expressed in days to weeks after irradiation, is rare under current RT regimens. Early delayed injury occurs from 1–6 months postirradiation and can involve transient demyelination with somnolence, which is mainly seen in children but also can

affect adult patients in the first 2 months after RT. While these early injuries can result in severe reactions, they usually resolve within 1–3 months, either spontaneously or following treatment with corticosteroids and their severity is not necessarily predictive of the more devastating late effects. Late delayed effects, characterized histopathologically by demyelination, vascular abnormalities and, ultimately, white matter necrosis (24), are observed > 6 months postirradiation after relatively high doses (>60 Gy) of fractionated RT (5, 25).

There is a growing awareness of intellectual deterioration in patients receiving brain irradiation (26) that can occur with relatively low total doses and in the absence of apparent structural lesions. Although diverse in character, this often includes hippocampal-dependent functions including learning, memory, and spatial information processing. Cognitive impairment, including dementia, induced by partial- or whole-brain irradiation (WBI) is reported to occur in up to 50% of adult patients who are long-term (>6 months postirradiation) survivors (27–29). The resultant impact on quality of life (QOL) has become an extremely important concern for long-term survivors, particularly for the adult survivors of childhood cancer who present with an extraordinarily high incidence of late, and often permanent, complications, including cognitive sequelae, arising from combined RT and chemotherapy (30–33).

Currently there are no validated diagnostic procedures for determining who will or will not develop radiation-induced brain injury, including cognitive impairment, or who will/will not respond favorably to therapies aimed at preventing or ameliorating these deficits. Radiation-induced late effects occur within the closed cranial cavity, and thus, noninvasive techniques offer the opportunity to study this significant side effect of brain tumor RT. Early studies used CT, histology and neurological changes to investigate radiation-induced late effects in the dog brain after hemibrain irradiation with large single doses (34). MRI use in the clinic has been translated into experimental studies of the effects of large single doses on the rat (35–37), cat (38, 39), dog (40, 41), and pig (42) brain as well as fractionated irradiation of the mouse brain (43). CT and MRI have enabled serial evaluation of animals over a prolonged period and identified radiation-induced brain injury as either a white matter hypodensity on CT or an increased T2 signal abnormality on MRI.

A limitation of these studies is that the primary morbidity associated with modern brain RT techniques is functional, rather than structural. For brain tumor patients, radiation-induced cognitive impairment represents a major morbidity than can markedly impact their QOL. Progressive cognitive impairment can occur without any MRI evidence of white matter necrosis (44). Similarly, fractionated (f)WBI of the rat brain leads to progressive cognitive impairment in the absence of demyelination, gliosis, and white matter necrosis (45). Cognitive impairment can also occur with no change in the number of oligodendrocytes and myelinated axons, or thickness of myelin sheaths 1 year following fWBI (46). These findings suggest that more sensitive imaging techniques that focus on microstructure [e.g., diffusion tensor imaging (DTI) (21) and metabolic changes (MRS) (22)] might detect the neurobiological changes that lead to altered neural processing following fWBI.

## MRI

MRI utilizes magnetic fields to generate tissue images by exciting protons and monitoring them as they relax. In addition to standard structural images that look at gross anatomy, DTI is capable of assessing tissue microstructure by measuring the diffusion or motion of water molecules along multiple tensors within each image voxel. DTI provides a mechanism to identify microstructural abnormalities due to radiation injury well before macrostructural changes are visible (47, 48). A minimum of six tensors need to be acquired for calculating the DTI indexes. Water diffusion along each tensor is measured for each voxel and by

averaging the diffusion in all directions, the mean diffusivity, or trace, is calculated. Areas with little structure allow water to freely diffuse and will have higher mean diffusivity values than areas with more structure, such as the white matter. The Fractional Anisotropy (FA) is determined from calculating the first, second and third eigenvalues ( $\lambda_1$ ,  $\lambda_2$  and  $\lambda_3$ ) of the tensor field, which describes whether diffusion is either elliptical or spherical. When the voxel is placed within highly-structured regions such as white matter bundles, water diffusion is restricted or anisotropic, and FA is near 1 (Fig. 1A, aqua arrow head within the anterior commissure). High FA values indicate that  $\lambda_1$  is significantly greater than the perpendicular eigenvalues  $\lambda_2$  and  $\lambda_3$ , which creates an elliptical or tube-shaped diffusion pattern. When the voxel is placed in less structured regions, such as the cerebral spinal fluid (Fig. 1A, yellow arrow head), or demyelinated white matter, water diffusion is less restricted or isotropic, and FA is closer to 0. Lower FA values indicate a smaller difference between  $\lambda_1$  and the perpendicular eigenvalues  $\lambda_2$  and  $\lambda_3$ , which creates a more spherical diffusion pattern.

Parallel diffusivity ( $\lambda_{\parallel}$ ) refers to the first eigenvalue and represents the greatest amount of diffusion in one direction, which is typically along the axons of white matter tracts. DTI processing frequently color-codes the directions of diffusion to allow greater separation of different anatomical tracts and interpretation of the direction of information flow (Fig. 1B); therefore it actually shows the movement of water in 3-dimensional (3D) space.

Perpendicular diffusivity ( $\lambda_{\perp}$ ) refers to diffusion along the second and third eigenvalues ( $\lambda_2$  and  $\lambda_3$ ) and is commonly calculated as an average between them. The second eigenvalue is the second highest value of diffusion perpendicular to  $\lambda_1$ , while  $\lambda_3$  is restricted to diffusion perpendicular to both  $\lambda_1$  and  $\lambda_2$ . Quantitative measures obtained from these DTI indices have been interpreted to distinguish between myelin loss and axonal injury. With demyelination, there is a greater increase in perpendicular diffusivity ( $\lambda_{\perp}$ ) with little or no change in parallel diffusivity ( $\lambda_{\parallel}$ ), while with axonal injury there is a decrease in  $\lambda_{\parallel}$  with little or no change in  $\lambda_{\perp}$  (49, 50). While, these interpretations are limited to white matter tracts; differences in DTI parameters are also found in cortical areas and represent alterations in how water diffuses through the extracellular matrix, synaptic field, and/or small myelinated/unmyelinated axons. These DTI indices can be compared on a voxel-by-voxel basis throughout the 3D brain space, or on a region-of-interest (ROI) basis within specific anatomical regions (Fig. 1C).

### DTI as an Imaging Biomarker of Late CNS Toxicity

DTI has been used to assess early white matter injury in both pediatric and adult patients treated with partial- and WBI (51–55). A recent, prospective DTI study was undertaken at the University of Michigan in which patients with high-grade gliomas ( $n = 19$ ), low-grade gliomas ( $n = 3$ ), and benign tumors ( $n = 3$ ) received partial brain irradiation; DTI was performed before, during, and after irradiation (51). Analyses revealed progressive changes secondary to RT in the genu (anterior portion) and splenium (posterior portion) of the corpus callosum. During the first 3 months post-RT, dose-dependent demyelination (i.e., increased  $\lambda_{\perp} > \lambda_{\parallel}$ ) was noted predominantly in regions receiving high doses of RT. However, 6 months following the start of RT, the diffuse demyelination was no longer limited to the high RT dose regions. The latency in diffuse demyelination suggests an opportunity for early intervention to avoid permanent late radiation-induced white matter damage (51). This study confirms that DTI indices have the potential to detect changes in the normal appearing white matter (NAWM) of CNS patients receiving partial brain irradiation.

Similar preclinical data are available for example, DTI of the rat brain 1 year after right hemibrain irradiation with 28 Gy of 6 MV photons revealed a significantly greater decrease in functional anisotropy (FA) in the ipsilateral fimbria of the hippocampus than in the external capsule, indicating selective vulnerability of the fimbria to irradiation (48).

Longitudinal evaluation of white matter injury in the rat brain imaged 2 to 48 weeks after 25 and 30 Gy hemibrain irradiation revealed a progressive reduction in FA, which was driven by a reduction in  $\lambda_{\parallel}$  from 4 to 40 weeks postirradiation, and an increase in  $\lambda_{\perp}$  with a return to baseline for  $\lambda_{\parallel}$  at 48 weeks postirradiation (56). Moreover, changes in  $\lambda_{\parallel}$  correlated with reactive gliosis, while  $\lambda_{\perp}$  correlated with demyelination. In middle-aged rats treated with fWBI, DTI performed 1 year postirradiation revealed no apparent changes in FA in heavily-myelinated axons (corpus callosum, cingulum, and deep cortical white matter). However, significant fWBI-induced injury was present in the superficial parietal cortex as indicated by a fWBI-induced decline in FA in the more anterior slices through the parietal cortex (57). These findings suggest that fWBI-induced changes may be more pronounced in the less myelinated/unmyelinated axons, extracellular matrix, or synaptic fields rather than in heavily-myelinated tracts.

Pediatric studies also support the utility of DTI as a clinically-relevant tool for the assessment of treatment-related neurotoxicity, and as a potential adjunct to intelligence quotient (IQ) scores. A cross-sectional DTI study of post-treatment survivors of childhood medulloblastoma and acute lymphoblastic leukemia (ALL) was performed and compared to age-matched controls. Decreases in FA were associated with declines in IQ scores after adjusting for the effects of age, RT dose, and time interval from treatment (52). Significant decreases in FA were noted in the white matter of both frontal and parietal lobes in childhood medulloblastoma survivors compared to controls. Greater declines in FA were noted in frontal compared to parietal lobes for the same RT dose, suggesting increased radiosensitivity of the frontal lobes which are myelinated and develop throughout childhood and adolescence (53). Additionally, late structural abnormalities in normal appearing cerebral white matter were indicated by significantly-reduced FA values in the temporal lobe, hippocampus, and thalamus of adult survivors treated for ALL following WBI compared to age-matched controls (54). Although changes in structural properties of NAWM are noted postirradiation, prospective neurocognitive testing prior to RT is required to correlate these findings with late-delayed radiation-induced cognitive impairment.

Radiation-induced injury to the hippocampus region may be associated with long-term deficits in learning, memory, and executive function. Demyelination or axonal injury within this area could impact the efficiency of communication between the hippocampus and the rest of the cortex, thereby impacting learning and memory. In a preliminary study at the University of Michigan, 12 patients with brain metastases treated with fWBI with RT total doses of 30–37.5 Gy were prospectively assessed with DTI prior to RT, at the end of RT, and one month following RT. Specific ROIs included the parahippocampal cingulum, a prominent white matter fiber tract bundle of the limbic system. A decrease in FA was noted in the parahippocampal cingulum 1 month after completion of fWBI (Fig. 2) (58). More specifically, a significant increase in  $\lambda_{\perp}$  without a significant change in  $\lambda_{\parallel}$  was noted in this region, suggesting early demyelination of the white matter (Fig. 2D). These results suggest that DTI indices may be a useful noninvasive biomarker to, (1) monitor patients who are treated with hippocampal-sparing WBI regimens, and (2) for predicting cognitive performance following RT (59).

In summary, DTI is able to detect early changes in white matter integrity. These changes in the properties of NAWM may be related to late-delayed cognitive decline. Currently, ongoing studies combining DTI and neurocognitive testing are investigating longer follow-up times (up to 18 months after RT) to determine the predictive power of these MRI biomarkers. By identifying patients with early changes in white matter integrity, it may be possible to predict which patients will have greater inherent radiation sensitivity, so that interventions can begin earlier.

## MR Perfusion Imaging

Vascular damage may also play a critical role in the development of late radiation-induced injury, including radiation necrosis (60, 61). Early histopathologic changes noted in blood vessels following irradiation include vessel dilatation, endothelial cell enlargement, and perivascular astrocyte hypertrophy, which can lead to blood-brain barrier (BBB) disruption, increased permeability, and edema. Acute vascular injury following irradiation potentially can be detected prior to the development of acute demyelination and white matter necrosis (62, 63). Dynamic contrast enhanced (DCE) MRI using T1-weighted imaging allows quantitative assessment of vascular permeability by repeatedly imaging brain tissue prior to and following a short bolus injection of an MRI tracer into the blood stream. By tracking the movement of the tracer into the image volume and using compartmental modeling, a transfer constant or  $K^{\text{trans}}$  value for passive leakage of the tracer from the intravascular space to the extravascular space can be calculated (64). Areas with high  $K^{\text{trans}}$  values have a leaky vascular wall that allows movement of the tracer out of intravascular space more readily than from areas with intact vasculature. These functional characteristics of the vascular microenvironment may provide an early indication of radiation-induced changes that correlate with late cognitive impairment.

In a preliminary clinical study, changes in blood plasma volume ( $V_p$ ) and  $K^{\text{trans}}$  were evaluated in normal-appearing cerebral tissue following partial brain irradiation (65).  $K^{\text{trans}}$  was highest during the 6th week of RT and decreased in a dose-dependent manner following the conclusion of therapy; it returned to baseline levels 6 months postirradiation. Increases in  $K^{\text{trans}}$  indicate changes in BBB permeability/perfusion effects which could be related to radiation-induced cell death and apoptosis(63).  $V_p$  however, displayed a dose-dependent response with low fractionated regimens (<20 Gy) showing no significant increase in  $V_p$ . Higher-dose regimens showed a differential increase in  $V_p$  during RT with larger doses inducing faster and larger increases. Although  $V_p$  decreased after RT; this decrease was still less than baseline levels 6 months postirradiation. At 6 months postirradiation, vascular microenvironment changes evident during the 3rd week of RT within left hemisphere frontal and temporal lobes were significantly correlated with declines in verbal learning scores on the Hopkins Verbal Learning Test (HVLT). When the temporal lobe was divided into hippocampal and nonhippocampal ROIs in 12 patients,  $V_p$  at 3 weeks continued to correlate with the HVLT learning scores 6 months postirradiation for both ROIs (65). Validation studies of these initial findings are currently on-going. However, they suggest that sparing of the hippocampus alone may not be sufficient to protect memory function following WBI.

## MR Proton Spectroscopy

Proton MRS is a noninvasive technique to, (1) interrogate metabolic distributions in the brain (66, 67), (2) differentiate radiation necrosis from brain tumor progression (68, 69), and (3) serve as an indicator of neurotoxicity following experimental (48, 70) and clinical brain irradiation (71–76). Metabolites detected in brain tissue include choline-containing compounds, creatine, glutamate, lactate, *N*-acetylaspartate (NAA), myoinositol (mI) and taurine. The concentration of each of these metabolites can be mapped from 2D or 3D spectroscopic images having a voxel size of 0.7–1 cm<sup>3</sup>. The metabolite, *N*-acetylaspartate (NAA) is predominantly a neuronal marker, and decreases are associated with neuronal damage and dysfunction secondary to radiation. Choline is associated with cell membrane synthesis and/or increased metabolic turnover; it is elevated in both tumors and inflammatory processes. Creatine is a marker of energy metabolism with relatively constant concentrations throughout the brain (77), while mI is a glial cell marker and has been used as an indicator of myelin breakdown (78).

Very little preclinical data are available on MRS detection of metabolite changes in the normal brain following irradiation. Using a 4.7T MR spectrometer and a voxel size of approximately 30 mm<sup>3</sup>, Herynek *et al.* (70) observed decreases in creatine and NAA 8 and 12 months after bilateral Gamma Knife irradiation of the hippocampus of young adult male rats with 35 Gy, a dose that led to severe functional and structural impairment. Chan *et al.* (48) used a 7T MR spectrometer and a voxel size of 64 mm<sup>3</sup> to determine significant increases in choline, glutamate, lactate, and taurine levels 12 months after right hemibrain irradiation of young adult male rats with a single dose of 28 Gy of 6 MV photons. These changes in white matter were confirmed histologically. Using a similar 7T spectrometer and a larger voxel size of 125 mm<sup>3</sup> (Fig. 3), Atwood *et al.* (79) reported a potential relationship between radiation-induced changes in rat brain metabolites and cognitive impairment 52 weeks after fWBI. MRS spectra obtained 12 weeks after 40 Gy fWBI failed to show any significant differences in brain metabolites or cognitive impairment between the fWBI and sham-irradiated rats. In contrast, analysis of MR spectra obtained 52 weeks postirradiation revealed significant increases in the NAA/total creatine + phosphocreatine (tCr) and the glutamate + glutamine/tCr ratios, as well as a decrease in the mI/tCr ratio compared with age-matched sham-irradiated controls. Assessment of cognitive function in these rats 54 weeks postirradiation revealed a significant reduction in the irradiated animals. Thus, these findings suggested that MRS may be a sensitive tool to detect changes in radiation-induced brain metabolites that may be associated with radiation-induced cognitive impairment (79). However, more recent studies using this fWBI model indicated that these changes in rat brain metabolites occur after the expression of radiation-induced cognitive impairment, and do not appear to cause or predict the onset of radiation-induced cognitive impairment (45).

MRS has also been used to assess metabolite changes in NAWM following RT (71–75). In a cross-sectional study of ALL survivors following intrathecal methotrexate and prophylactic cranial irradiation, MRS detected decreasing NAA/Cr and Cho/Cr ratios with increasing time after RT ranging from 5.6 to 19 years, suggesting long-term brain injury secondary to decreases in NAA and Cho (76).

In an initial prospective study of 11 adult patients with low-grade gliomas or benign tumors, such as pituitary adenomas and meningiomas treated with partial brain irradiation, MRS demonstrated significant alterations in brain metabolites in normal appearing brain parenchyma, both during irradiation and over a 6-month period post-RT. Similar to the previous study, decreases were also noted in both the NAA/Cr and Cho/Cr ratios starting 3 weeks following RT that persisted for up to 6 months (71).

Several small studies have demonstrated significant alterations in brain metabolites in normal appearing brain parenchyma following RT (72–75). Transient metabolic changes were noted in glioma patients 4 months following RT with increases in the Cho/NAA and Cr/NAA ratios that appeared to resolve over time (72). In a prospective study of high-grade glioma patients, similar findings were noted in normal appearing brain parenchyma following RT. Transient increases in the Cho/NAA ratios were noted 2 months following RT in NAWM regions receiving low, moderate, and high RT doses; recovery was dose-dependent (73). Similarly, in a cross-sectional adult glioma study, metabolite changes were much more pronounced in radiation-induced hyperintensity areas (RIHA) compared to NAWM. In RIHA regions, a decrease in both NAA and Cho was suggestive of myelin damage and axonal necrosis; in NAWM regions, a decrease in Cho was suggestive of membrane damage in myelin-producing oligodendrocytes that accompanies impaired tissue perfusion due to endothelial radiation effects (74).

In summary, MRS is a noninvasive imaging technique that can monitor radiation-induced changes in brain metabolites. Clinically, there are significant technical challenges that

remain in reproducibly measuring chemical metabolites near brain tumor regions. There may be signal contamination from the ROI's proximity to the ventricles, scalp and surgical clips. Normal tissues adjacent to the tumor bed may also affect local-field homogeneity and data quality (77). Ongoing studies involve the temporal dynamics of radiation-induced injury and its associated metabolite changes as well as the relationship between the detection of early tissue damage and the development of late symptomatic cognitive impairment.

## PET

The effect of fWBI on brain function has recently been investigated in nonhuman primates (NHPs) using FDG-PET imaging by determining local rates of glucose metabolism/uptake ( $CMR_{glc}$ ) during a Delayed-Match-to-Sample (DMS) cognitive function task (80). The  $CMR_{glc}$  in a brain region is an indicator of neurosynaptic activity in that region, and has become a standard technique in dementia research (81). PET scans performed 1 week prior to fWBI revealed that the brain regions activated during the DMS task were the dorsal prefrontal cortex (DPFC), the medial temporal lobe (MTL), the parietal cortex (precuneus), and dorsal striatum (DStr); areas repeatedly implicated in human and NHP cognitive function (82, 83). As anticipated, PET scans performed 9 months after fWBI, when cognitive function was significantly impaired, revealed reduced glucose metabolism in the cuneate and DPFC regions compared to pre-fWBI values (80). In contrast, glucose metabolism in the cerebellum and thalamus, regions that were not engaged during the DMS task prior to fWBI, was increased, indicating a potential imbalance in frontal subcortical circuits (Fig. 4) (84). Indeed, decreased capacity to perform higher-order executive functions has been shown to involve the DPFC, hippocampus, cuneate, and motor areas in cancer survivors following fWBI (44).

## Lung Injury

Symptomatic pulmonary injury is one of the most common side effects in patients undergoing thoracic RT (85). Noninvasive radiologic imaging techniques can be used to assess regional damage, reduced function, and potentially to predict clinically-relevant outcomes. However, radiologic evidence of pulmonary injury is not always accompanied by clinical symptoms. For example, in lung cancer patients who receive RT, 50% to 100% will develop radiologic evidence of lung injury, while only 5% to 35% develop clinical symptoms (85–87). Similarly, for breast cancer patients who receive RT, up to 63% develop radiologic evidence of lung injury, while 34% or fewer develop clinical symptoms (88–93).

The likelihood of clinical pulmonary injury is related to RT dose, irradiated volume, and fractionation schedule. Systemic therapies (e.g., chemotherapy, hormone therapy, or immunotherapy) may affect the incidence and severity of RT-induced injuries, as may patient-specific factors, such as pre-treatment pulmonary function and a history of smoking (86, 94–98).

Pulmonary injuries are typically divided into early- (or acute)-phase injuries and late- phase injuries. Radiation pneumonitis, an early-phase complication usually developing within 6 months of RT, is commonly characterized by cough and dyspnea, and typically responds well to steroids. It occasionally resolves without treatment (92, 99, 100). Fibrotic injury is a late complication, usually presenting at least 6 months post-RT and, if symptomatic, can involve progressive dyspnea and possible mortality (86, 97).

Radiologic evidence of radiation pneumonitis can be variable in appearance with increased density associated with inflammation (acute) (101), or increased density accompanied by contraction, and pleural thickening (late) (102). The frequency of detecting radiologic abnormalities depends on the sensitivity of the radiographic assessment. For example,



computed tomography (CT) is more sensitive than chest radiography because it provides 3D visualization of the lung (102).

## CT and SPECT

Preclinical studies using mouse and rat models have demonstrated that serial CT imaging can be used to demonstrate both dose-dependent increases in lung density following single-dose irradiation (103, 104), and strain-specific differences in acute- and/or late-radiation injury (105). More recently, a methodology for quantitatively measuring structural regional changes in homogeneously-irradiated rat lungs has been developed (106). Lung function has been assessed using radionuclide perfusion assays. And, it was shown that hemithoracic irradiation of the rat lung leads to decreased arterial perfusion as assessed using technetium-99m-labeled macroaggregated albumin that is evident within 4 to 6 weeks of irradiation with a single dose of 25 (107) or 28 Gy (108).

Noninvasive imaging techniques for assessing RT-induced lung injury have been previously described in detail (94, 102). CT scans provide lung tissue density information that can be associated with 3D RT dose-distribution maps. SPECT imaging is a sensitive means of assessing regional lung function such as perfusion and ventilation. RT affects both ventilation and perfusion, which is best demonstrated by the work of researchers at the Netherlands Cancer Institute (NKI; 109). Their data, and that of several others, suggest that perfusion is a more sensitive measure of normal tissue injury than is ventilation. Physiologically, the lung is better able to reduce blood flow to unventilated areas (via capillary/vascular constriction) than to reduce ventilation to unperfused areas (bronchi are less able to be constricted). Therefore, reductions in ventilation will generally also cause perfusion reductions, but the reverse is less-often true. Thus, perfusion is a more sensitive metric for assessing RT-induced lung injury.

For both CT and SPECT, pre- and post-RT images can be compared to the 3D dose distribution to study the dose-dependent nature of RT-induced regional lung injury. Perfusion defects are more common than ventilation defects, and both are more common than changes in CT (94). Investigators from Duke University, the NKI, and the Princess Margaret Hospital (PMH) have reported prospective data relating lung RT dose to CT-defined lung injury (100, 109, 110). In a study of 25 patients irradiated for malignant lymphoma, Boersma *et al.* at the NKI observed dose-dependent increases in CT density 3 to 4 months post-RT (109). Mah *et al.* at the PMH studied changes in CT density up to 6 months following lung irradiation for 54 patients; dose-dependent increases in the frequency of CT-defined lung injury were observed (110). At Duke, Levinson *et al.* studied changes in local CT density for 13 patients with lung cancer (100). Significant increases in CT density were observed for regions of lung receiving >60 Gy; smaller increases were observed for regions receiving smaller doses. The pre- and post-RT CT images, for a typical irradiated lung cancer patient, are shown in Fig. 5A and B. Increased density is seen on the post-RT CT image (indicated by an arrow in Fig. 5B) and is associated with inflammation.

Similar to CT images, pre- and post-RT SPECT images can be compared to the 3D dose distribution to study the dose-dependent nature of regional RT-induced lung injury. Pre- and post-RT SPECT perfusion images, including the isodose distributions, for an irradiated lung cancer patient are shown in Fig. 6A and B; the dose-response curve for RT-induced reductions in regional perfusion are shown in Fig. 6C. Using 3D image-fusion techniques, investigators at Duke and NKI have related changes in pre- and post-RT CT density, SPECT ventilation, and SPECT perfusion to the 3D regional dose distribution (Fig. 7) (100, 109, 111–114).

Several investigators have established a connection between the extent of radiologic evidence of pulmonary injury and clinically-relevant symptoms (110, 115, 116). Fan *et al.* at Duke, and Theuws *et al.* at NKI, showed a correlation between reductions in pulmonary function tests (PFTs) and integrated changes in regional perfusion, i.e., the integrated response (116–118). Although statistically significant, the relatively weak correlation between reduced PFT performance and integrated response suggests the existence of additional factors to explain post-RT changes in PFT. A stronger association between pulmonary symptoms (Grade 2) and the estimated sum of regional functional changes has been shown by Gopal *et al.* (119).

Recent reports have focused on radiation-induced lung injury after stereotactic radiosurgery. In a study of 31 patients receiving stereotactic radiosurgery for primary or metastatic lung lesions, Aoki *et al.* noted asymptomatic increases in CT density 2 to 6 months post-RT, and later fibrotic reactions at 6 and 15 months post-RT (120). While all 31 patients developed radiographic changes, no patients developed severe symptoms (e.g., Grade 2 or requiring steroids). When follow-up CTs were compared to the dose distribution on the treatment planning CT, investigators observed that the minimal dose for the development of CT-defined changes in lung tissue density ranged from 16 to 36 Gy.

## MRI

Contrast-enhanced MRI may also be used to describe perfusion characteristics of various phases of RT-induced lung injury. Japanese studies suggest that MRI can also detect radiation-induced lung injury in animal models. Shioya *et al.* used MR techniques to determine the extent of radiation-induced lung tissue damage in rats within 2 weeks of a 20 Gy single fraction to the hemithorax. They found that MRI was more sensitive than conventional imaging techniques for detecting early effects on normal tissue (121). Ogaswara *et al.* also suggested that contrast-enhanced perfusion MRI may be helpful in differentiating acute pneumonitis from late fibrosis in dogs (122).

Similar results using contrast-enhanced perfusion MRI for distinguishing acute pneumonitis from late fibrosis have been reported in the clinical setting (122, 123). A recent study by Muryama *et al.* suggested that pulmonary hypertension, detected by velocity-encoded cine (VEC) MRI, may be used as a predictor of radiation pneumonitis (124). MRI has also been suggested to be potentially useful to detect differences in tumor response during treatment, with the potential to guide adaptive changes in treatment plans (123).

## PET

FDG-PET imaging provides regional functional information that has potential for assessing RT-induced lung injury. A recent study by Hart *et al.* at MD Anderson Cancer Center, noted dose-dependent increases in regional FDG-PET activity in 101 esophageal cancer patients assessed 3 to 12 weeks post-RT (125). Further, the severity of the regional inflammatory changes appeared to be significantly correlated with the probability of symptoms. Data from several studies using SPECT, CT, MRI, and PET to detect changes in the lung following thoracic RT are summarized in Table 1. In some of the studies, the rate of symptomatic shortness of breath is also noted. These data are included in the table and illustrate that imaging is more sensitive than clinical symptoms as a marker of RT-induced lung injury.

In summary, several investigators have used a variety of imaging tools to study RT-induced regional injury/changes. For some, there is a reasonable dose-response relationship. The association between the extent/severity of regional imaging changes and changes in global function is less well-defined. Additional work is needed to better clarify the relationship between changes in regional imaging and changes in global function.

## HEART INJURY

RT to the thorax may induce both early and late cardiac effects if portions of the heart are included in the radiation field. Patients with breast cancer and Hodgkin's disease are particularly at risk for developing late myocardial damage, due to their longevity and possibly to the frequent use of anthracycline-containing chemotherapy. In general, one has to wait at least 10 years post-treatment to see these effects manifest clinically (131). The use of radiologic methods may allow for the early detection of treatment-associated dysfunction. The vast majority of the available data on RT-induced heart injury use SPECT myocardial perfusion imaging in breast cancer and Hodgkin's disease patients. Recent studies have also investigated the incidence of the cardiac effects of RT in lung and esophageal cancer patients. Finally, preliminary data are available on newer imaging technologies, such as cardiac MRI and PET, for assessing RT-induced cardiac injury in patients with thoracic cancers. However, to our knowledge, there are no published reports using imaging techniques to noninvasively assess radiation-induced cardiotoxicity in preclinical models. Nevertheless, this is likely to become a fruitful area of research in the near future.

### Scintigraphy and SPECT

Nuclear medicine imaging provides both qualitative and quantitative information about regional and global cardiac function (132), and has been suggested to be a sensitive means to assess myocardial injury in patients with coronary artery disease (133). Cardiac SPECT techniques that produce 3D images are currently applied more frequently than are planar scintigraphic techniques; they provide a noninvasive assessment of left ventricular myocardial perfusion and function, such as changes in wall motion and left ventricular ejection fraction. Scans taken in the early years following RT may be useful for estimating subclinical damage. The incidence of perfusion defects appears to be related to the irradiated volume of the left ventricle and largely persists for up to 6 years after RT in breast cancer patients (134, 135).

Gyenes *et al.* conducted a prospective study and performed Tc-99m Sestamibi scintigraphy prior to and ~1 year after left breast/chest wall RT in 12 patients. Six of the 12 patients (50%) with some portion of the left ventricle within the radiation field exhibited a new perfusion defect. Again, the location of the defects corresponded with the irradiated volume of the left ventricle. Interestingly, neither electrocardiographic (ECG) changes nor left ventricular segmental wall motion abnormalities were detected by echocardiography (136). Seddon *et al.* performed SPECT myocardial perfusion imaging in 24 patients with left breast tumors, and 12 control patients with right breast tumors, who had undergone RT at least 5 years previously. Myocardial perfusion defects were found in 17/24 (70.8%) of left breast patients compared to 2/12 (16.7%) of right breast patients. Almost all myocardial defects in left breast patients were located in the cardiac apex, the portion of heart that is incidentally included within the RT fields (137). In a prospective study at Duke, new RT-associated perfusion defects were detected in 16/55 (29%) of breast cancer patients 6–12 months post-RT (Fig. 8). The incidence of perfusion deficits was related to the irradiated volume of the left ventricle, with new defects occurring in approximately 10–20% and 50–60% of patients with <5% and >5% of their left ventricle included within the RT fields, respectively (134). These studies used SPECT images generated without attenuation correction. However, the same technique was used to generate the pre- and post-RT images, and these images were compared to each other. All of the data presented are based on comparisons of pre- vs. post-RT images. Thus, the lack of attenuation correction does not explain these findings. For patients who do not experience significant anatomic changes between pre- and post-RT images, attenuation correction does not influence the validity of the results. The accuracy of these studies is dependent on the assumption that there are not meaningful changes in the patient's anatomy in between the pre- and post-RT scans.

Perfusion defects have been associated with episodes of chest pain and wall motion abnormalities, but their clinical implications are not well understood (134, 135, 137, 138). Further, relatively large perfusion defects appear to cause reductions in the ejection fraction (130), although the data on this point are limited. Abnormalities detected by SPECT have been suggested to be due to attenuation artifacts related to RT-induced pericardial scarring of the breast or chest wall. These artifacts may be misinterpreted as defects in the anterior myocardium (134); however, recent analyses suggest that this is unlikely (139) and that the perfusion changes seen post-RT are “real.” Data from several studies relating SPECT changes in the heart of breast cancer and Hodgkin’s disease patients, and preliminary data from studies in esophageal and lung cancer patients are shown in Table 2.

## MRI

MRI allows the determination of myocardial wall thickness and, with delayed hyper-enhancement, direct visualization of myocardial injury or fibrosis; it is more sensitive than SPECT in assessing sub-endocardial injury. Both MRI and SPECT provide information regarding wall motion and ejection fraction, but MRI has better spatial resolution and thus may be more accurate (153, 154). Presently, quantification of myocardial perfusion is better developed with SPECT than with MRI (154).

While MRI provides the ability to globally assess the heart, at this time MRI has only been used to study RT-induced cardiac disease for a small number of lung cancer patients. In pilot studies from MD Anderson Cancer Center and Duke University, no apparent cardiac MRI changes have been observed in a small number of evaluable patients (151, 152).

## PET

There is increased interest in the use of PET to provide a map of regional myocardial perfusion because of its improved resolution and accuracy when compared to SPECT. PET has an advantage of possibly shorter exam times than SPECT, but is similarly limited to imaging only the left ventricle (155). A recent case report noted increased FDG uptake within cardiac regions receiving 25 Gy ~ 4 years earlier; the patient was asymptomatic and had a normal ECG (156).

In summary, imaging has been used to define RT-induced changes in regional perfusion and function in the left ventricle, largely relying on SPECT. Some newer imaging methods may be better able to study RT-induced changes in imaging and function throughout the entire heart. This is critical to better understand the cardiac effects of RT given the multiple cardiac sub-regions and their functional interrelationship/dependency.

## SUMMARY

Technological advances in biomedical imaging have enabled preclinical and clinical studies of radiation-induced normal tissue injury to move from assessing simply anatomical changes to generating functional, microstructural, and metabolic data. Moreover, noninvasive approaches allow the longitudinal determination of the extent and severity of radiation-induced normal tissue injury on an individual basis. Molecular imaging, including MR, SPECT, and PET, holds the promise of identifying the specific targets and biological processes that precede or underlie anatomical and functional changes (157). Recent studies demonstrating, (1) the ability to monitor disease progression and therapy response in neurodegenerative disorders by imaging of peripheral benzodiazepine receptors with PET (158), (2) SPECT imaging of serotonin and dopamine receptors (159), (3) PET and MR imaging of neuroinflammation (160–162), and (4) cardiovascular disease with MR, SPECT, and fluorescent-tagged molecules (163), suggest that applying these techniques to radiation biology/oncology will greatly advance our understanding of the molecular mechanisms

underlying the development and progression of radiation-induced normal tissue injury. These mechanistic insights will enable radiation oncologists to plan RT regimens more rationally to minimize treatment-related morbidities, as well as intervene to improve the outcome and QOL of their patients.

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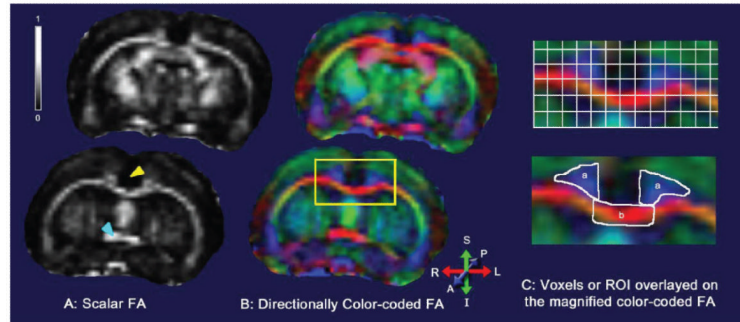
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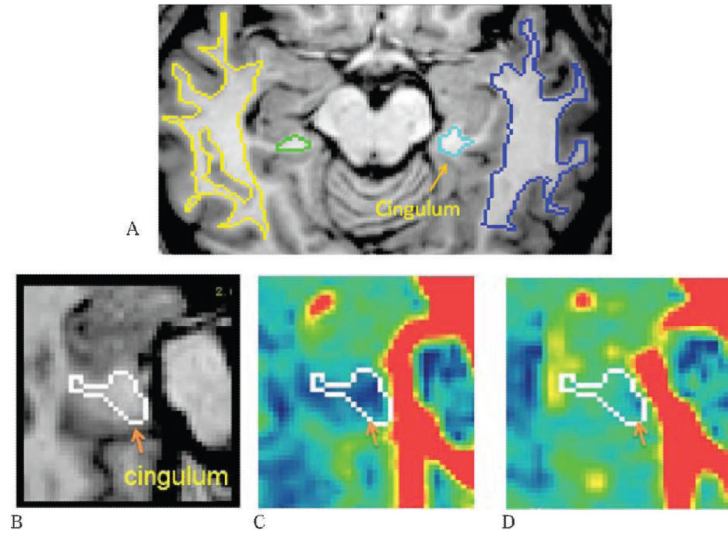
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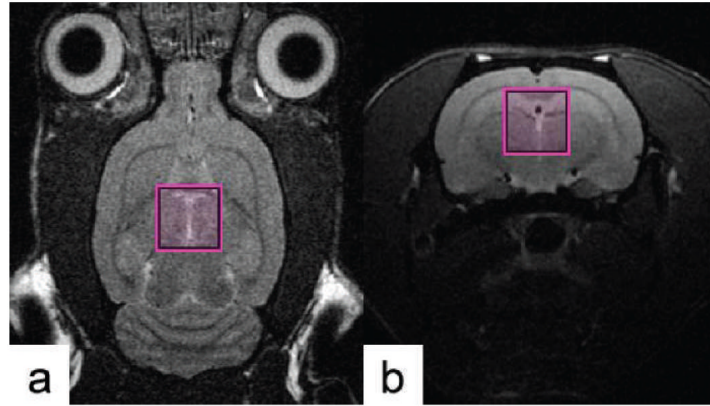
**FIG. 1.**

Coronal brain slices of a male Fischer 344  $\times$  Brown Norway rat. Panel A: Fractional Anisotropy (FA) indicates the directional water diffusion within a voxel. Fractional anisotropy values approaching 1 (aqua arrowhead) have high directional flow and can be seen within white matter tracts throughout the rat brain. Panel B: Fractional anisotropy can be colored to represent the direction of flow throughout the 3D image. In this example, blue defines flow between anterior (A) and posterior (P), red defines flow between left (L) and right (R), and green defines flow between superior (S) and inferior (I). Colors in between these axes represent the entire color spectrum applied in 360°. Panel C: To compare voxel-wise and region of interest (ROI) analysis, a medial region of the lower panel from part B has been magnified. Voxel analysis will compare across individuals the area of tissue that is contained within each voxel and relies on voxels being in the same region across all subjects. As can be seen, structures are split across voxels creating partial volumes, which contain two or more tissue types or anatomical regions. ROI analysis relies on an individual or automated segmentation to delineate particular structures such as the cingulum bundles (a) or corpus callosum (b). Both methods have limitations and benefits, and should be used with a clear understanding of the assumptions of the methodology whether alone or in combination.

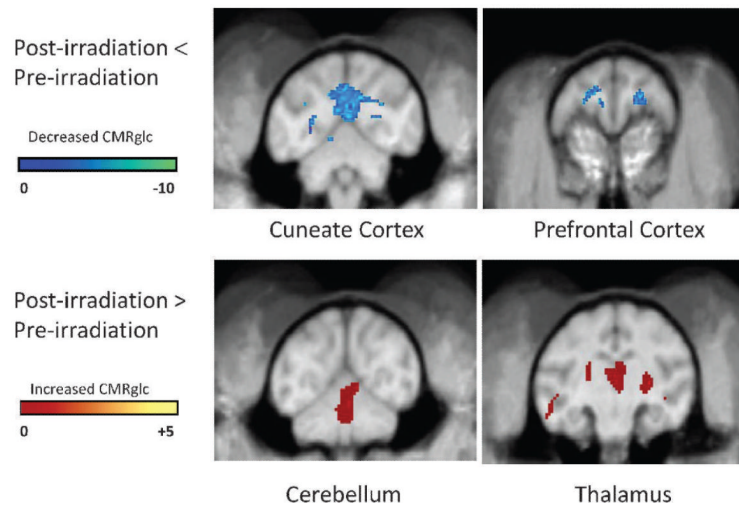


**FIG. 2.** Prospective human MR DTI study to assess changes in normal appearing white matter following whole-brain radiation therapy (WBRT). Panel A shows an MR T1-weighted axial slice illustrating the different regions of interest defined for each patient including parahippocampal cingulum outlined in green (right hemisphere) and light blue (left hemisphere). Temporal lobe white matter (yellow and blue) regions are also shown. Panel B shows an MRI T1-weighted MR axial slice obtained at baseline prior to WBRT; the parahippocampal cingulum is outlined in white. In panel C, a calculated MR DTI map of  $\lambda_{\perp}$  is shown. Parahippocampal white matter prior to WBRT appears dark on  $\lambda_{\perp}$  images indicating greater diffusion in the direction parallel to the white matter fiber tracts. However, 1 month following 30 Gy WBRT, there is a significant increase in  $\lambda_{\perp}$  indicating early demyelination in the region of the parahippocampal cingulum (panel D).

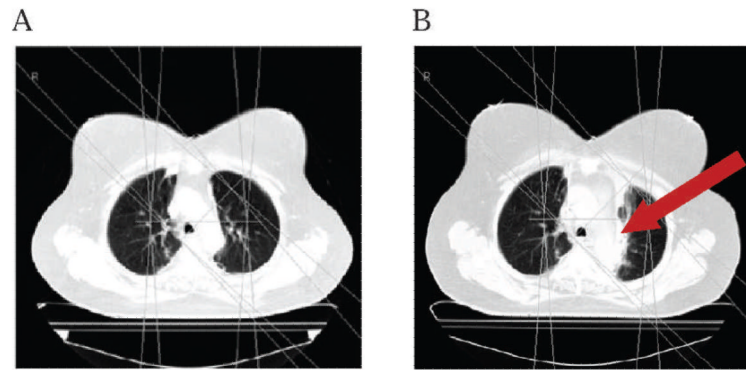




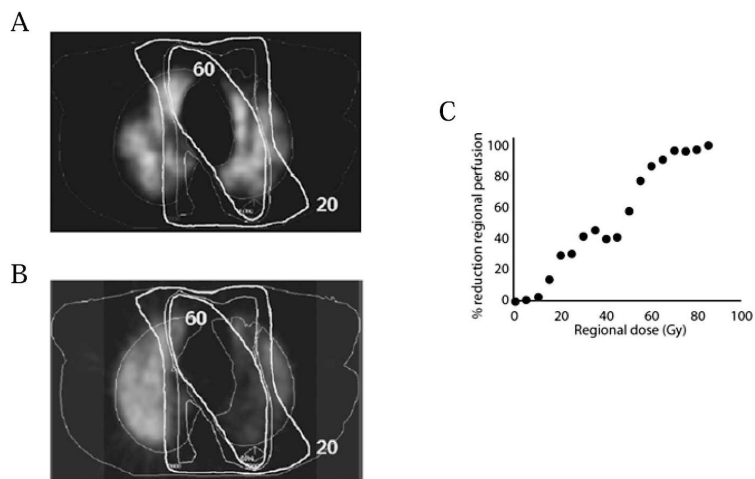
**FIG. 3.** High-resolution T<sub>2</sub>-weighted control (panel a) and axial (panel b) images illustrating the location of the 5 × 5 × 5 mm voxel used to obtain the MR spectra in the fWBI rat brain (79).



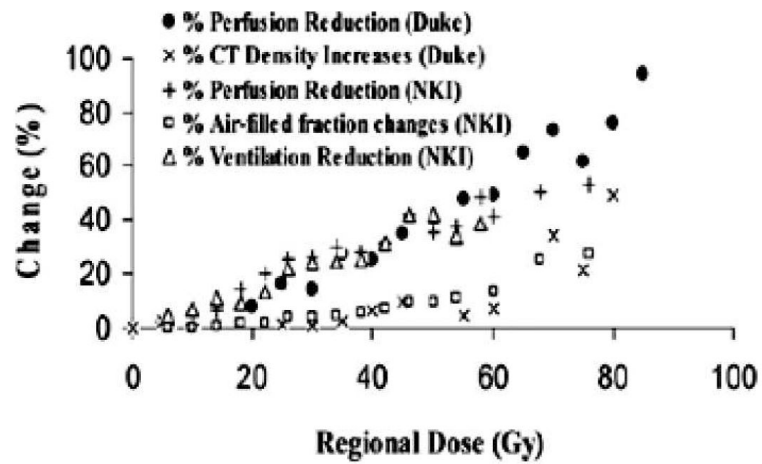
**FIG. 4.**  $[^{18}\text{F}]$ FDG-PET scans of cerebral glucose metabolism 9 months after fWBI. Upper panel: post-irradiation < pre-irradiation. Blue areas in the cuneate cortex and prefrontal cortex exhibited less metabolic activity in fWBI scans obtained 9 months after fWBI than in the scans prior to fWBI. Lower panel: post-irradiation > pre-irradiation: The red areas in the cerebellum and thalamus showed greater metabolic activity in the fWBI scans obtained 9 months after fWBI than in the scans prior to fWBI. The color bar is the degree of intensity difference shown as a scale of t values with  $P < 0.001$  (80).



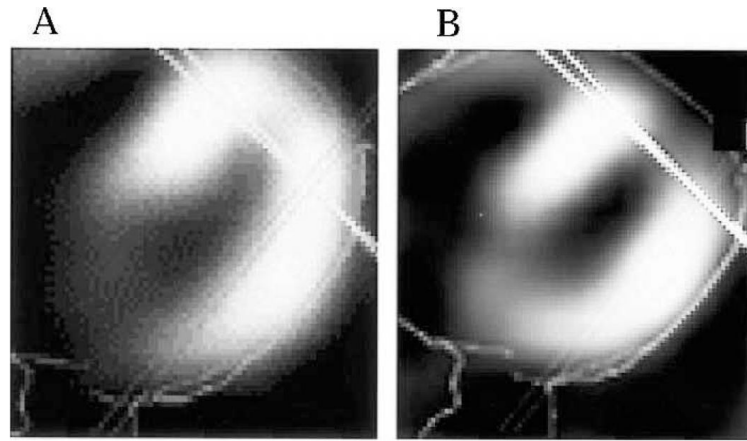
**FIG. 5.** Shows the (panel A) pre- and (panel B) 12-month post-radiation therapy (RT) computed tomography images from an irradiated lung cancer patient. The beam paths are shown (anterior, posterior, oblique). The arrow indicates the region of increased CT density in the irradiated medial left lung following RT. [Adapted from Kocak (102) with permission.]



**FIG. 6.** Shows the (panel A) pre- and (panel B) 6-month post-radiation therapy (RT) transverse SPECT perfusion images from an irradiated lung cancer patient. The RT dose distribution, relative to isodose contours, is also shown. Panel C shows the dose-response curve for RT-induced reductions in regional perfusion from the patient's SPECT scans; post-RT perfusion defects are seen most predominantly within regions of the lung receiving >60 Gy. [Adapted from Kocak (102) with permission.]



**FIG. 7.** Dose-dependent reductions in regional SPECT perfusion and ventilation, as well as increases in CT density in patients receiving lung irradiation. [Adapted from Marks (114) with permission; data from Netherlands Cancer Institute (109, 111, 112) and Duke (100, 113).]



**FIG. 8.** Cardiac SPECT scans showing representative axial images obtained (panel A) pre-RT and (panel B) post-RT. The deep tangent border is shown as the solid line. A new perfusion defect after irradiation is seen in the anterior left ventricle. [Adapted from Marks *et al.* (134) with permission.]

TABLE 1  
 Compared Frequencies of Radiographic and Symptomatic Pulmonary Changes after Thoracic Irradiation [Adapted from Hubbs (126) with permission]

Reference, author, year	No. of cases	Disease site(s)	Radiographic follow-up	Radiologic endpoint	Rate (%)	Clinical endpoint	Rate
Radiography/CT							
Polansky, 1980 (127)	37	Breast	0.7–10 years	increased radiopacity	16/37 (43%)	-	0/37 (0%)
Mah, 1987 (110)	54	Lung, breast, Hodgkin's disease	6 months	increased radiopacity	36/54 (67%)	radiation pneumonitis	10/54 (19%)
Rotstein, 1990 (91)	33	Breast	9 months	increased radiopacity	24/33 (73%)	cough/dyspnea	13/33 (39%)
Seppenwoolde, 2000 (111)	106	Lung	3 months	increased radiopacity	25/25 (100%)	-	-
Marks, 2000 (85)	184	Lung breast, lymphoma	24 months	increased radiopacity	162/259 (63%)	dyspnea	34/175 (19%)
Scintigraphy/SPECT							
Allavena, 1992 (128)	75	Hodgkin's disease	3–10 years	decreased perfusion	29/45 (100%)	radiation pneumonitis	4/25 (16%)
Boersma, 1996 (109)	25	Lymphoma	18 months	decreased perfusion, decreased ventilation	110/110 (100%)	-	-
Theuws, 2000 (112)	110	Breast, lymphoma	48 months	decreased perfusion, decreased ventilation	25/25 (100%)	-	-
Seppenwoolde, 2000 (111)	106	Lung	3 months	decreased perfusion	168/230 (81%)	dyspnea	34/175 (19%)
Marks, 2000 (85)	184	Lung, breast lymphoma	24 months	decreased perfusion	79/79 (100%)	-	-
Woel, 2002 (113)	79	Lung, lymphoma, breast, other thoracic tumors	5 years or more	decreased perfusion	-	-	-
Tokatli, 2005 (95)	20	Breast	1 year	decreased lung clearance	10/10 (100%)	mild radiation pneumonitis	2/20 (19%)
MRI							
Yankelevitz, 1994 (123)	10	Lung	3.5 years	increased lung density	10/10 (100%)	-	-
Ogasawara, 2002 (122)	9	Lung	0.5–7 months	Asymmetric enhancement on dynamic perfusion MR	9/9 (100%)	acute radiation pneumonitis/RT fibrosis	-
Muryama, 2004 (124)	40	Lung, esophagus	none (pre-RT image)	increased lung density	-	radiation pneumonitis	-
PET							
Hicks, 2004 (129)	73	Lung	38 months	increased FDG <sup>1</sup> uptake	55/73 (75%)	-	-
Guerrero, 2007 (130)	36	Esophagus	1–3 months	increased FDG <sup>1</sup> uptake	36/36 (100%)	-	-
Hart, 2008 (125)	101	Esophagus	3–12 weeks	increased FDG <sup>1</sup> uptake	-	NCI Common Toxicity Criteria (CTC) Grade 2	-

Note. Some data estimated from published reports.

<sup>18</sup>F-FDG; fluorodeoxyglucose.

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TABLE 2

Compared Frequencies of Radiographic and Symptomatic Cardiac Changes after Thoracic Irradiation  
[Adapted from Hubbs (126) with permission]

Reference, author, year	Years of RT	No. of cases	Median radiographic follow-up	Subgroup	Rate of perfusion defects
Breast cancer – retrospective					
Gyenes, 1994 (140)	1971–1976	37	18.4 years	Left-sided photons or electrons	25% (5/20)
			19 years	Right-sided photons or electrons	0% (0/17)
Gustavsson, 1999 (141)	1978–1983	90	13 years	Left-sided RT	12% (4/34)
				Right-sided or no RT	4% (2/56)
Højris, 2000 (142)	1982–1990	16	7.9 years	Left-sided electrons	44% (4/9)
				No RT	57% (4/7)
Cowen, 1998 (143)	1987–1993	17	8.4 years	Left-sided photons	0% (0/17)
Girinsky, 2000 (144)	1987–1995	36	6.7 years	Left-sided photons	71% (17/24)
			8.3 years	Right-sided photons	17% (2/12)
Breast cancer – prospective					
Gyenes, 1996 (136)	1993–1994	12	1.1 year	Left-sided photons	100% (4/4)
				Left-sided electrons	25% (2/8)
Marks, 2005 (134)	1998–2001	114	0.5 year	Left-sided photons	27% (21/77)
			1 year	Left-sided photons	29% (16/55)
			1.5 years	Left-sided photons	38% (13/34)
			2 years	Left-sided photons	42% (11/26)
Prosnitz, 2007 (135)	1998–2006	44	3 years	Left-sided photons	38% (3/8)
			4 years	Left-sided photons	58% (7/12)
			5 years	Left-sided photons	67% (4/6)
			6 years	Left-sided photons	67% (2/3)
Other disease sites					
Savage, 1990 (145)	1967–1985	16	9.3 (2.5–21.5) years	Hodgkin's disease	0% (0/16)
Gustavsson, 1990 (146)		26	15 (4–20) years	Hodgkin's disease	61% (14/23)
Maunoury, 1992 (147)	1978–1988	31	7 (3–11) years	Hodgkin's disease	84% (21/25)
Glanzmann, 1998 (148)	1964–1992	112	11.2 (1.0–31.5) years	Hodgkin's disease	7% (7/100)
Girinsky, 2000 (144)		49	75 (28–208) months	Hodgkin's disease	78% (32/41)
Heidenreich, 2007 (149)	1964–1994	294	6.5 (4.0–8.4) years	Hodgkin's disease	12% (32/274)
Gayed, 2006 (150)	2005–2006	51	3 months	Esophageal cancer	54% (14/26)
Lind, 2006 (151)		13	2 months, 6 months	Lung cancer	
Hubbs, 2008 (152)	2006–2007	12	3, 6, 12, and 18 months	Lung cancer, Mesothelioma	50% (6/12)