

# Hierarchical Nanotexturing Enables Acoustofluidics on Slippery yet Sticky, Flexible Surfaces

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Cite This: *Nano Lett.* 2020, 20, 3263–3270

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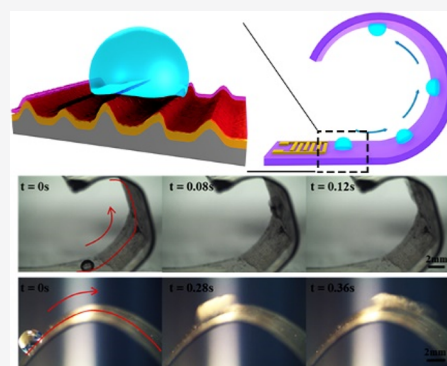
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**ABSTRACT:** The ability to actuate liquids remains a fundamental challenge in smart microsystems, such as those for soft robotics, where devices often need to conform to either natural or three-dimensional solid shapes, in various orientations. Here, we propose a hierarchical nanotexturing of piezoelectric films as active microfluidic actuators, exploiting a unique combination of both topographical and chemical properties on flexible surfaces, while also introducing design concepts of shear hydrophobicity and tensile hydrophilicity. In doing so, we create nanostructured surfaces that are, at the same time, both slippery (low in-plane pinning) and sticky (high normal-to-plane liquid adhesion). By enabling fluid transportation on such arbitrarily shaped surfaces, we demonstrate efficient fluid motions on inclined, vertical, inverted, or even flexible geometries in three dimensions. Such surfaces can also be deformed and then reformed into their original shapes, thereby paving the way for advanced microfluidic applications.

**KEYWORDS:** Hierarchical nanotexture, slippery surface, flexible devices, acoustofluidics, droplet transport



Precision control of microfluids on a small scale, particularly in a microdroplet format, underpins a range of smart microsystems, such as those for soft robotics and lab-on-chip.<sup>1–3</sup> However, a major challenge remains in the complexity of assembling all the necessary functionalities using conventional microfluidic devices which are generally based upon rigid substrates and are thus unable to conform to the flexing of natural shapes.<sup>4–7</sup> Future applications for the directional transport of fluids will require liquid actuation on flexible and deformable surfaces, on three-dimensional shapes, such as those in robotics.

Thin film piezoelectric surface acoustic wave (SAW) devices have previously been shown to enable all necessary microfluidic functions in diagnosis and sensing applications.<sup>8</sup> Material stoichiometry, texture, and crystallinity can be easily controlled, while remaining biocompatible.<sup>9–11</sup> They have previously been developed on conformable substrates and have been used for sensing and microfluidics with similar performances to their rigid counterparts.<sup>12–14</sup> However, to date, their deformability has not been exploited due to challenges both in realizing long-range wave propagation across the surfaces as well as in implementing liquid handling on curved surfaces (where gravity causes the droplet to detach).

To address these issues, we now show that we can deposit and control the surface structures of ZnO on the nanoscale, on aluminum foils (with thickness from 50 to 600  $\mu\text{m}$ ) as flexible and acoustically actuated microfluidic devices, which can be deformed (and maintain their temporal shape) before being

returned to their original shapes. Importantly, we show that the acoustic waves not only propagate over long distances of several centimeters without significant dissipation but also overcome the major challenge of enabling efficient liquid handling on curved surfaces—providing the designated slipperiness necessary for motion along the surface, while ensuring sufficient stickiness for the retention of the liquid when the surface is inclined, vertical, or even inverted.

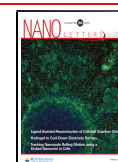
Hydrophobic coatings such as CYTOP,<sup>15</sup> or topographic structures (including roughness), have previously been combined with hydrophobic materials<sup>16–18</sup> to create surfaces with superhydrophobicity, minimizing droplet pinning forces and creating a slippery surface. However, this also minimizes the surface contact area, which itself is directly related to the quanta of energy that can be transferred from the acoustic waves into the liquid.

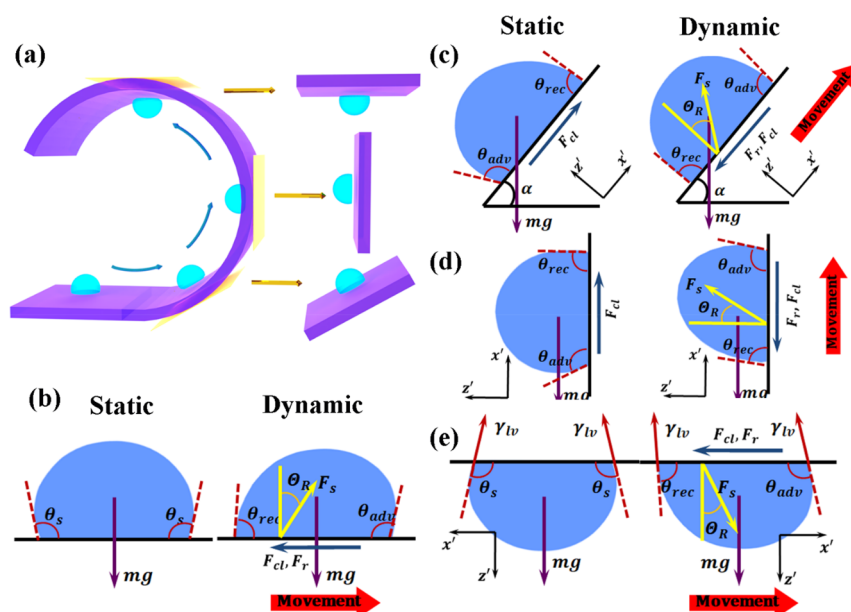
The reduced contact area for superhydrophobic surfaces also necessarily results in a reduced droplet adhesion normal to the plane (“stickiness”). Additionally, as the surface oscillates with a nanometer-scale amplitude generated by the acoustic excitation, this increases the probability that the liquid penetrates the

Received: January 1, 2020

Revised: February 25, 2020

Published: April 1, 2020





**Figure 1.** Principles of droplets moving on a curved surface. (a) Schematic diagram of droplet movement on a curved surface, which can be treated as a sum of movements on tangential planes. (b–e) Force analysis of the water droplet retained and moving on hydrophobic surfaces: (b) placed horizontally, (c) tilted at angle  $\alpha$ , (d) placed vertically ( $\alpha = 90^\circ$ ), and (e) placed upsidedown ( $\alpha = 180^\circ$ ) in static and dynamic (surface acoustic wave power is on) states.

surface texture, resulting in an irreversible pinning of the droplet. Such issues are counterintuitive to the key design criteria for a three-dimensional and bendable smart system for droplet transport, which critically requires retaining droplets on the surface as the physical orientation is varied (e.g., either as the angle of inclination or curvature).

We demonstrate that, by engineering the material stack and surface texture of a ZnO/Al piezoelectric flexible sheet for our SAW-based devices, we can achieve droplet manipulation on large scales and conformable shapes not previously possible, opening a new way for flexible devices to perform complex smart microfluidic systems. We combine the microscale roughness of the metal foil substrate with the nanoscale structures of ZnO film to create a hierarchically textured surface, showing not only a low contact angle hysteresis (i.e., shear hydrophobicity<sup>19</sup> allowing easy translation of droplets across the surface) but also a receding contact angle allowing droplets to be retained in a wide range of surface orientations (i.e., with sufficient tensile hydrophilicity<sup>19</sup>). Importantly, we not only demonstrate that such ZnO/Al sheets support low power wave propagation and efficiently drive liquids on horizontal, inclined, vertical, and arbitrarily shaped surfaces but also show that both the contact angle hysteresis and receding contact angle are key design parameters for requiring droplet transportation and adhesion.

**Surface Design Considerations.** Figure 1a depicts a droplet in sequential positions along a curved surface driven by SAW propagating along the surface. For microliter-sized droplets (for instance  $1 \mu\text{L}$  with a radius of  $\sim 1 \text{ mm}$ ), the radius of curvature of surfaces conforming to geometric features can be considered infinitely large ( $>10 \text{ cm}$ ) as compared to the droplet, so that we can estimate the forces applied to the droplet by considering a flat sheet tangential to the curved surface. For a droplet placed on a horizontal flat surface (see Figure 1b), the idealized static equilibrium state is described using Young's equation

$$\gamma_{sl} + \gamma_{lv} \cos \theta_Y = \gamma_{sv} \quad (1)$$

where,  $\gamma_{sl}$  is the surface tension of the liquid–solid interface,  $\gamma_{lv}$  is the liquid surface tension,  $\gamma_{sv}$  is the solid surface tension, and  $\theta_Y$  is the contact angle in the idealized equilibrium state.

When the SAW propagates, and thus moves a droplet along the horizontal surface, the advancing and receding contact angles,  $\theta_{adv}$  and  $\theta_{rec}$ , define the contact hysteresis and the pinning of the contact line.<sup>20</sup> To agitate and move the droplet, the externally applied driving force must overcome the pinning force of the droplet due to this contact angle hysteresis. Assuming there is a perfect circular contact line for the droplet, the lateral (radial) pinning force can be formulated as<sup>21,22</sup>

$$F_{cl} = \frac{24}{\pi} \gamma_{lv} D_0 (\cos \theta_{rec} - \cos \theta_{adv}) \quad (2)$$

where  $D_0$  is the equivalent base diameter in a static state.

The force can be reduced by decreasing the difference between the advancing and receding contact angles, or by tuning the surface topography and hydrophobicity, thus enabling the liquid to ball up and changing the length of the contact line (represented in eq 2 by the equivalent base diameter).

Considering the case of driving a hanging droplet, e.g., perpendicular to a surface and upward, the actuation force must overcome both the work of adhesion (given by  $\gamma_{lv}(1 + \cos \theta_{rec})$ <sup>19,23</sup>) and gravity. Use of a superhydrophobic surface is difficult to implement, because although droplets can be pushed on inclined or inverted superhydrophobic surfaces (at an angle  $\alpha$ ,  $0^\circ < \alpha \leq 180^\circ$ ), in practice, once the actuation force stops, gravity will often cause the moving liquid droplet to detach from the surface and fall off.

An alternative approach that reduces the contact line force is to reduce the contact angle hysteresis (i.e., increase shear hydrophobicity<sup>19</sup>), while retaining a receding contact angle at a value appropriate to ensure that the droplet adheres to the surface when subject to normal forces (i.e., tensile hydrophilicity<sup>19</sup>). In this approach, the reduction in contact angle hysteresis does not require the droplet to be balled-up or the contact line length to be reduced to achieve an easy droplet

transport along the surface. Moreover, since the contact line length does not have to be reduced, the droplet-surface area is large enough for the acoustic wave to interact with the liquid droplet and, hence, enable an efficient wave energy dissipation; thus, low power actuation is maintained.

Once the droplet starts moving under agitation of a SAW, the viscous resistance force becomes significant due to a strain formed along the contact line. This force,  $F_r(v)$ , can be written as<sup>24</sup>

$$F_r(v) = \int_0^{D_0/2-\varepsilon_c} \frac{3\mu v}{h(r)} (2\pi r) dr \quad (3)$$

where  $\varepsilon_c$  is the cutoff length to prevent the singularity at the contact line,  $\mu$  is the liquid viscosity,  $v$  is the droplet velocity, and  $h(r)$  is the height of the droplet at a certain position dependent on the radial coordinate  $r$ .  $F_r(v)$  is equal to zero when the droplet is immobile.

Figure 1b–e compares the total SAW streaming forces,  $F_s$ , applied to the droplet in both static and dynamic states of different substrate orientations, induced by an acoustic pressure, which is defined as<sup>25–27</sup>

$$F_s = -(1 + \theta_1^2)^{3/2} A^2 \omega^2 k_i \exp(2(k_i x + \theta_1 k_i z)) \quad (4)$$

where  $A$  is the wave amplitude,  $\omega$  is the angular velocity, and  $k_i$  is the imaginary part of  $k_i$  which is the wavenumber of the leaky surface acoustic wave.  $\theta_1 = j\theta$  (with  $j^2 = -1$ ) is the attenuation constant where  $\theta^2 = 1 - (v_{Le}/v_l)^2$ ,  $v_{Le}$  is the leaky wave velocity, while  $v_l$  is the sound velocity in liquid.

The direction of the pressure/force follows the Rayleigh angle  $\Theta_R$  which is defined by

$$\Theta_R = \sin^{-1}(v_l/v_s) \quad (5)$$

where  $v_s$  is the sound velocity in the flexible substrate. The minimum force required to move the droplet can be written as

$$F_s \sin \Theta_R - F_{cl} = 0 \quad (6)$$

The relationship among the different forces applied to the droplet which are balanced during droplet movement can be described using the following equation:

$$F_s \sin \Theta_R - F_{cl} - F_r(v) = m \frac{dv}{dt} \quad (7)$$

where  $m$  is the mass of the droplet. This relationship predicts that the projection of acoustic force will be increased with the Rayleigh angle for a given input power. If the surface is tilted at a certain inclination angle  $0^\circ < \alpha \leq 180^\circ$ , the gravitational force is involved at both static and dynamic states; thus, the force balance in both the  $z'$  and  $x'$  directions should be considered (Figure 1c–e). In the static state, the forces are balanced to keep the droplet stable in its position, and then, we have

$$\begin{cases} mg \sin \alpha - F_{cl} = 0 & 0^\circ < \alpha < 180^\circ \\ mg - \pi D \gamma_{lv} \sin \theta_{rec} = 0 & \alpha = 180^\circ \end{cases} \quad (8)$$

where  $g$  is the acceleration of gravity. Accordingly, in a dynamic state, the acoustic force needed to initiate the droplet movement is

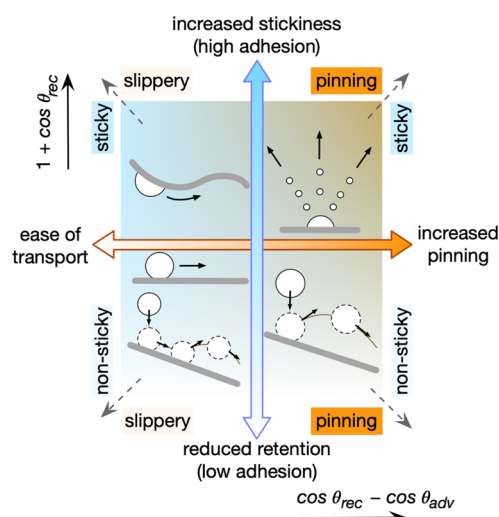
$$F_s \sin \Theta_R - F_{cl} - mg \sin \alpha = 0 \quad (9)$$

Meanwhile, eq 7, which describes the relationship between the droplet velocity and the forces, can be further modified as

$$F_s \sin \Theta_R - F_{cl} - F_r(v) - mg \sin \alpha = m \frac{dv}{dt} \quad (10)$$

Based upon the above discussion and analysis, in order to realize three-dimensional manipulations of droplets on inclined or even curved surfaces driven by SAW, the surface needs to be prepared not only with a low contact angle hysteresis for easy transportation of droplets but also with a suitable receding contact angle to retain the droplet on it.

The contact angle hysteresis and receding contact angle can be regarded as two key parameters describing a design space, with the first parameter controlling whether a droplet is pinned (thus preventing motion along it), and the second parameter controlling how strongly a droplet adheres in the direction perpendicular to the surface. Figure 2 summarizes these four

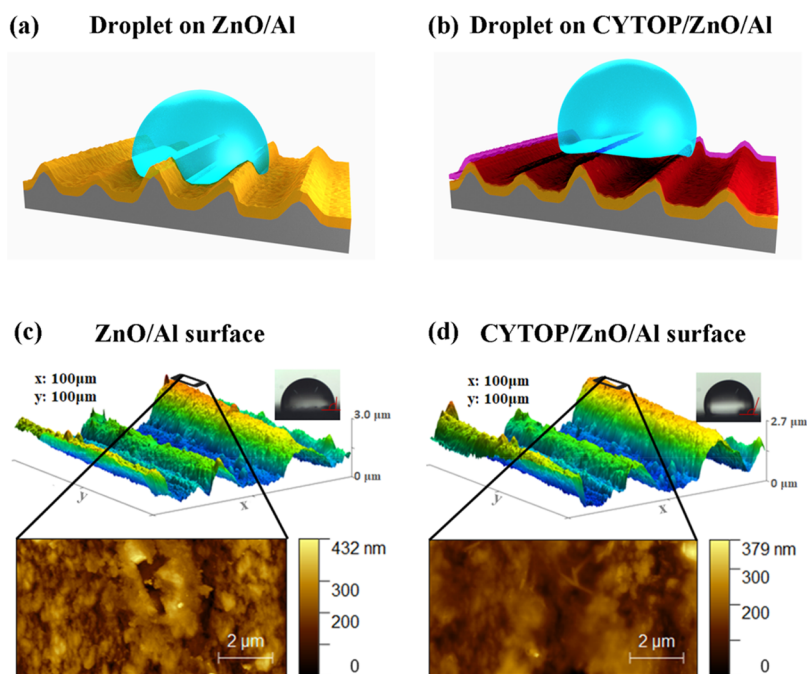


**Figure 2.** Combinations of four different surface types arising from contact angle hysteresis and receding contact angle. Scheme defining the design space of slippery/nonsticky,<sup>28</sup> pinning/nonsticky,<sup>29</sup> pinning/sticky,<sup>30</sup> and slippery/sticky surface types with exemplars of possible applications.

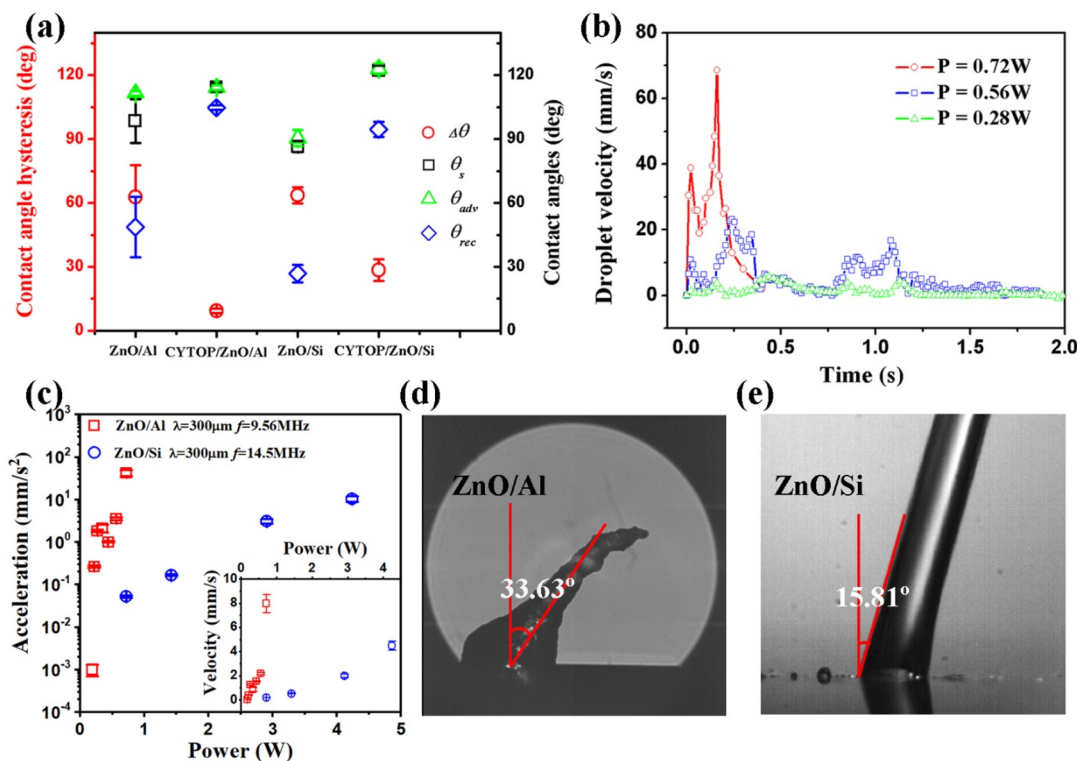
fundamental combinations of slipperiness and stickiness (e.g., showing low/high pinning and low/high adhesion) and provides exemplars of potential applications.<sup>28–30</sup> For our application in this study requiring droplet motion along a surface that can have multiple orientations including vertical and inverted, the surface wettability design requires ease of transport and sufficient adhesion, and this was achieved by creating a hierarchical texture of nano- and microscale features, as shown in Figure 3a,b.

**Hierarchically Textured Surface with Shear Hydrophobicity and Tensile Hydrophilicity.** Here, we used Al sheets with a thickness of 600  $\mu\text{m}$  as the underlying substrates. There are surface grooves with microscale roughness on the surface, generated by cold rolling manufacturing processes (Figure S1), and the root-mean-square roughness of grooved surfaces is in the range  $0.72 \pm 0.05 \mu\text{m}$ , measured using a profilometer. ZnO thin film was deposited on top of the microstructure, providing a hierarchical and fractal surface with an average roughness value of 73.6 nm (shown in Figure 3c—AFM image,  $5 \mu\text{m} \times 8 \mu\text{m}$ ).

Sputtered ZnO thin films have a relatively low surface energy, and contact angles of a water droplet on such a surface vary between  $70^\circ$  and  $100^\circ$ .<sup>31</sup> When the droplet is located on the



**Figure 3.** Surface morphology of hierarchical textures. (a) 3D schematic diagram of the bilayer structure composed of the Al substrate (gray) and ZnO thin film (orange). (b) 3D scheme of the trilayer structure composed of the Al substrate, ZnO thin film, and CYTOP coating (red). AFM images showing the root-mean-square (RMS) roughness of the hierarchical structure (c) before and (d) after CYTOP coating.



**Figure 4.** Contact angle measurements and pumping experiments on horizontal surfaces. (a) Comparison of the static contact angle  $\theta_s$ , the receding contact angle  $\theta_{rec}$ , and the advancing contact angle  $\theta_{adv}$ , and hence the contact angle hysteresis,  $\Delta\theta = \theta_{adv} - \theta_{rec}$  of water droplets ( $1 \mu\text{L}$ ) on ZnO/Si and ZnO/Al surfaces before and after CYTOP coating. (b) Pumping velocity as a function of time with different input powers when the water droplet is driven by an acoustic wave on a  $600 \mu\text{m}$  thick horizontal Al plate. (c) Average acceleration calculated from videos of horizontal pumping on ZnO coated  $600 \mu\text{m}$  thick Al plates and ZnO coated Si wafer increasing with the input power. The inset figure shows the average velocity (over time). Rayleigh angles of the surface acoustic wave can be observed from the jetting trajectory of  $2 \mu\text{L}$  water droplets on (d) the ZnO/Al device (jetted at 8 W) and (e) the ZnO/Si device (jetted at 14 W).

ZnO/Al sheet structure, a Wenzel state is formed on the surface as shown in Figure 3a. This Wenzel state could be transformed

into a Wenzel/Cassie–Baxter mixed state by coating the ZnO surface with a thin hydrophobic layer (300–500 nm thick) of

CYTOP, an amorphous fluoropolymer with high transparency and water and oil repellency. Figure 3c,d shows that the nanoscale roughness is reduced after the surface is coated with CYTOP. For a comparison, we also measured the surface roughness of a ZnO film deposited onto a standard polished (100) Si wafer using the AFM and obtained a homogeneous and smooth surface with an average roughness of  $15.05 \pm 4.58$  nm over an area of  $100 \mu\text{m} \times 100 \mu\text{m}$ , which is much smaller than those on the foil substrates.

To further understand the wettability of the ZnO/Al sheet surface, we measured the static contact angle  $\theta_s$ , and the advancing and receding contact angles, giving us a contact angle hysteresis,  $\Delta\theta = \theta_{\text{adv}} - \theta_{\text{rec}}$  for  $1 \mu\text{L}$  water droplets with and without CYTOP treatment as shown in Figure 4a (values are tabulated in Table S1 in the Supporting Information). The untreated ZnO/Al sheet delivered good tensile hydrophilicity with a receding contact angle of  $49^\circ \pm 14^\circ$  retaining the droplet against any normal force. However, the droplet on such a surface is also pinned in the direction of movement due to the large contact angle hysteresis of  $63^\circ \pm 15^\circ$  and, hence, poor shear hydrophobicity. Similarly, the untreated ZnO/Si surface provides a smaller receding contact angle ( $27^\circ \pm 4^\circ$ ), indicating a better tensile hydrophilicity, while having poor shear hydrophobicity due to the contact angle hysteresis staying the same as the untreated ZnO/Al surface. After the surface was coated with CYTOP, the surface wetting properties were modified, and the shear hydrophobicity was enhanced with a decreased contact angle hysteresis of  $28^\circ \pm 6^\circ$ . The receding contact angle of the CYTOP/ZnO/Si surface increased to  $95^\circ \pm 4^\circ$  but was still able to prevent the droplet from being detached perpendicularly providing acceptable tensile hydrophilicity (adhesion) compared to superhydrophobic surfaces. By using the ZnO/Al surface, we could further optimize the shear hydrophobicity and reduce the contact angle hysteresis to  $9^\circ \pm 2^\circ$  while achieving a receding contact angle of  $105^\circ \pm 1^\circ$ , thus creating a surface that simultaneously has excellent shear hydrophobicity (slipperiness) and sufficient tensile hydrophilicity (adhesiveness). In such cases, the surface acoustic wave actuation force required to transport a droplet along a surface, which is proportional to  $\gamma_{\text{lv}}(\cos \theta_{\text{rec}} - \cos \theta_{\text{adv}})$ , is reduced, while the force normal to the surface required to remove a droplet, which is proportional to  $\gamma_{\text{lv}}(1 + \cos \theta_{\text{rec}})$ , remains sufficiently large to prevent droplet detachment.

**Droplet Transport Enhanced on Horizontal and Tilted Flat Surfaces.** The input power determines the displacement amplitude of the Rayleigh wave and, thus, the streaming force  $F_s$ . According to eq 9, when  $F_s \sin \Theta_R$  is larger than the lateral pinning force  $F_{\text{cl}}$  ( $mg \sin \alpha = 0$  applied for a horizontal surface), the droplet starts to move forward. During the movement, eq 10 can be used to explain the behavior of the droplet shown in Figure 3b, where the instant velocity presents multiple peak values. The streaming force  $F_s$  decreases exponentially as the droplet moves away from the wave source due to its attenuation in the substrate. Meanwhile, the viscous resistance force  $F_r(v)$  is proportional to the instant velocity. At the starting point,  $F_s \sin \Theta_R$  is much larger than the sum of  $F_{\text{cl}}$ ,  $F_r$ , and  $mg \sin \alpha$ , creating a positive acceleration  $dv/dt$ . The instant velocity increases accordingly while  $F_s \sin \Theta_R$  decreases, and  $F_r$  increases until the forces reach their first balance point, where  $dv/dt = 0$ . Afterward, the instant velocity decreases rapidly due to the negative acceleration, causing the fast decrease of  $F_r$  until once again  $F_s \sin \Theta_R$  is dominant. This process would repeat several

times before the droplet moves to the position where the damped acoustic wave cannot initiate the movement.

We also investigated the droplet transport characteristics of the hydrophobically treated ZnO/Al SAW devices by measuring average moving velocities and accelerations at different power levels (Figure 4c) and compared them with those on a ZnO/Si surface. The average accelerations on both the CYTOP/ZnO/Al and CYTOP/ZnO/Si surfaces are increased with the input power, reaching  $42.1 \pm 7.1$  and  $0.05 \pm 0.003$   $\text{mm/s}^2$ , respectively, for an applied power of 0.72 W, corresponding to average velocities (averaged over time) of  $8.0 \pm 0.8$  and  $0.2 \pm 0.01$   $\text{mm/s}$ . Importantly, the threshold power to initiate droplet movement on the CYTOP/ZnO/Al surface is much smaller than that on the CYTOP/ZnO/Si device. In addition, the droplet average velocities are higher on the CYTOP/ZnO/Al surface than that on the CYTOP/ZnO/Si device at the same power, indicating that the acoustic devices on the ZnO/Al with a hierarchically textured surface are more efficient for droplet transport.

This enhanced performance can, in the first instance, be attributed to the hierarchical CYTOP/ZnO/Al surface, which reduces the contact angle hysteresis to  $9^\circ$ , significantly smaller than on the CYTOP/ZnO/Si surface at  $28^\circ$ , decreasing the threshold power required to initiate the droplet movement along the surface, and also reducing the power needed to overcome the lateral pinning force which could restrict the droplet movement. The surfaces also retained a receding contact angle of  $105^\circ$ , ensuring that droplets do not detach from the surface when curved/bent.

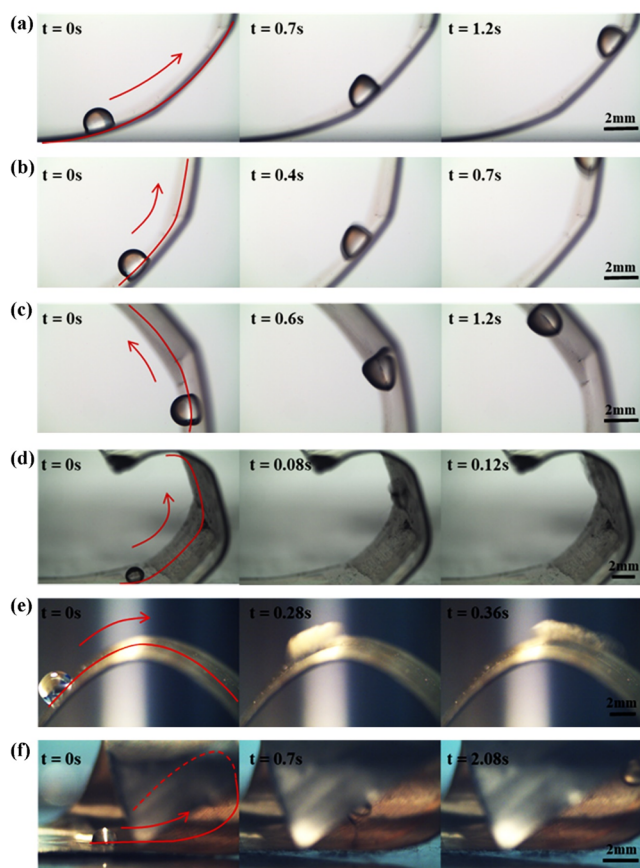
For completeness, the Rayleigh angle also plays an important part in the enhanced performance. We calculated it as  $30.8^\circ$  on ZnO/Al, as opposed to  $19.7^\circ$  on ZnO/Si (using phase velocities of 2868 m/s on the ZnO/Al sheet, 4351 m/s on ZnO/Si, and 1468 m/s in water) and verified experimentally (e.g.,  $33.6^\circ$  and  $15.8^\circ$  as shown in Figure 4d,e). As predicted by eq 10, the driving force is the projection of the streaming force on the moving surface, which can be calculated by  $F_s \sin \Theta_R$ . For ZnO/Al,  $\sin \Theta_R$  is around 0.55, while it is around 0.27 for ZnO/Si. Therefore, given the same input power (same  $F_s$ ), the driving force of ZnO/Al devices is twice that of ZnO/Si devices along the moving direction and, thus, is more efficient for droplet transport.

Furthermore, the enhanced actuation of the liquid can be attributed to the different ways in which the droplets interact with the substrate surface. For the droplet on the CYTOP/ZnO/Al substrate, assuming it is in a mixed Wenzel/Cassie–Baxter state, the entrapped air prevents the droplet from flowing into the surface's topology and reduces the contact area between the liquid and the solid surface, thus lowering the friction and causing efficient transport. In contrast, there is little air entrapped under the droplet on the silicon substrates with smooth surfaces. The larger Rayleigh angle and smaller contact angle hysteresis for the CYTOP/ZnO/Al device during movement imply that liquid droplets move using a combination of rolling and sliding (Figure S2a). On the contrary, the droplet movement is dominated by sliding and jumping modes on the CYTOP/ZnO/Si surface (Figure S2b).

This mechanism enables us to demonstrate movement on inclined surfaces (Figure S3) by tilting the device plate into different orientations, e.g., inclined angled slopes, vertical, and upsidedown positions. Here, an important consideration is the droplet size, as it has a significant influence on pumping at different inclination angles due to the effect of gravity. This is

especially important at inclination angles around  $90^\circ$ , and we experimentally determined a maximum volume for our device to be  $3 \mu\text{L}$ . Larger droplets cannot be pumped upward but move downward due to gravity.

**Demonstration of Programmable, Flexible, and Bendable Acoustofluidics.** To demonstrate the concept of programmable, flexible, and bendable three-dimensional acoustofluidics using hierarchical CYTOP/ZnO/Al nanostructured surfaces, we deformed the CYTOP/ZnO/Al ( $600 \mu\text{m}$  thick) device into a circle (see schematic illustration in Figure 1a). Figure 5a–c shows that a water droplet could be efficiently pumped forward on different segments of its surface with a curvature varying from  $54.5$  to  $85.7 \text{ m}^{-1}$ .



**Figure 5.** Experimental demonstration of 3D pumping driven by the ZnO-based acoustic wave on bendable substrates. (a–c)  $1 \mu\text{L}$  droplets moving at different stages on curved surfaces ( $P = 15 \text{ W}$ ). (d)  $0.5 \mu\text{L}$  droplet moving on a “roller coaster” formed by curled acoustic wave devices ( $P = 20 \text{ W}$ ). (e)  $2 \mu\text{L}$  droplet moving past a hilly surface ( $P = 6 \text{ W}$ ). (f)  $0.5 \mu\text{L}$  droplet moving on a twisted surface ( $P = 3 \text{ W}$ ).

To further extend the flexibility of our platform, we reduced the thickness of Al sheets with the corresponding acoustic wave modes changing from those associated with Rayleigh waves to Lamb waves. Acoustic wave devices were designed and fabricated on  $200 \mu\text{m}$  thick ZnO/Al sheets and deformed in shapes of a “roller coaster” (Figure 5d,e, and Movies S1 and S2). Finally, we also show that the droplet can be easily pumped along arbitrary topographies using a randomly twisted CYTOP/ZnO/Al ( $50 \mu\text{m}$  thick) sample (Figure 5f and Movie S3).

**Conclusions.** In summary, we designed nanostructured surfaces using hierarchical textures to optimize shear hydrophobicity and tensile hydrophilicity to tune droplet transport

and adhesion on arbitrarily oriented devices. We demonstrated that the CYTOP/ZnO/Al sheets enabled a significantly better actuation performance when compared to conventional ZnO/Si acoustic wave devices. These CYTOP/ZnO/Al sheets were uniquely capable of efficiently driving droplets across a wide range of inclination angles ( $0^\circ < \alpha \leq 180^\circ$ ). Our designed devices can be flexibly deformed and then maintain their shape, while enabling efficient liquid pumping. We envisage that the surface design principles and demonstrated devices/applications will be pivotal for liquid sampling for smart diagnostic systems within mobile and disposable settings.

**Methods. Sample Preparation.** ZnO/Al and ZnO/Si substrates were prepared using magnetron sputtering (NS3750, Nordiko). ZnO films with thicknesses of  $5 \mu\text{m}$  were deposited on  $50 \mu\text{m}$  thick Al foils,  $200$  and  $600 \mu\text{m}$  thick Al thin plates, and  $500 \mu\text{m}$  thick  $4 \text{ in. (100)}$  Si wafers in vacuum with a pressure of  $0.65 \text{ Pa}$ . A  $99.99\%$  pure Zn target was used while Ar/ $\text{O}_2$  gases with flow rates of  $10/13 \text{ sccm}$  were introduced to form a plasma and to provide oxygen ions (power,  $400 \text{ W}$ ).

The acoustic wave devices included interdigital transducers (IDTs) on top of the ZnO thin films, fabricated through photolithography and lift-off processes. The Cr/Au electrodes with a thickness of  $20 \text{ nm}/100 \text{ nm}$  were deposited using a thermal evaporator. For hydrophobic surface treatment,  $1\%$  CYTOP solution (L-809A) was dip-coated on the ZnO surface and heated to  $180^\circ \text{C}$  for  $1 \text{ min}$ .

**Experimental Methods.** The surface roughness of all samples was characterized using an interferometer (Bruker Contour GT-K) and an AFM (Veeco Dimension 3100). The static, advancing, and receding contact angles were measured using sessile droplets and volume addition and withdrawal on a droplet shape analyzer (Kruss DSA30S). In the acoustofluidic experiments, the acoustic wave devices were connected to an RF signal generator ( $9 \text{ kHz}–2.4 \text{ GHz}$  2024, Marconi Instruments) through a power amplifier (model 75A250, Amplifier Research). The movements of water droplets were imaged by both a high-speed camera (Phantom V2511,  $3000 \text{ FPS}$ ) and a standard CMOS camera.

## ■ ASSOCIATED CONTENT

### SI Supporting Information

The Supporting Information is available free of charge at <https://pubs.acs.org/doi/10.1021/acs.nanolett.0c00005>.

Additional data and figures including surface morphology of the  $600 \mu\text{m}$  thick Al substrate, deformation of a  $1 \mu\text{L}$  droplet in the movement driven by acoustic waves, droplets moving on various tilted flat surfaces, and contact angle hysteresis measurements (PDF)

Movie S1: droplet moving on a “roller coaster” (AVI)

Movie S2: droplet moving past a hilly surface (AVI)

Movie S3: droplet moving on a twisted surface (AVI)

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### Author Contributions

Y.Q.F., G.M., J.R., and J.M.C. proposed the idea. R.T., Y.Q.F., J.T.L., and P.C.-P. performed the experimental work. R.T. and Y.Q.F. wrote the manuscript and performed analyses. G.M., J.R., H.T., Q.W., J.L., X.Y., J.Z., and J.M.C. were involved in writing, discussions, and modifications of the paper.

### Notes

The authors declare no competing financial interest.

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### ACKNOWLEDGMENTS

We gratefully acknowledge the microfluidic platforms in Northumbria University and the James Watt Nanofabrication Centre at the University of Glasgow. The work is also supported by the Special Interests Group for Acoustofluidics under the UK Fluids Network. We also acknowledge Mr. Yong Wang and Mr. Xiang Tao for their support in experiments. This work was financially supported by Research and Development Program of China (Grant 2016YFB0402705), the UK Engineering and Physical Sciences Research Council (EPSRC) grants, EP/P018998/1 and EP/K027611/1, Shenzhen Key Lab Fund (ZDSYS20170228105421966), Shenzhen Science & Technology Project (Grant JCYJ20170817100658231), the National Natural Science Foundation of China (51605485), as well as by the European Research Council Advanced Investigator Award

340117 (BioPhononics). All data needed to evaluate the conclusions in the paper are present in the paper and/or the Supporting Information. Additional data related to this paper may be requested from the authors.

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