

Building an *in vivo* anatomical atlas to close the phenomic gap in animal breeding

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Abstract

1 Currently, a growing gap is observed between the enormous amount of genomic
2 information generated from genotyping and sequencing and the scale and qual-
3 ity of phenotypes in animal breeding. In order to fill this gap, new technologies
4 and automated large-scale measurements are needed. Body composition is an
5 important trait in animal breeding related to growth, feed efficiency, health,
6 meat quality and market value of farmed animals. *In vivo* anatomical atlases
7 from CT will aid large-scale and high-throughput phenotyping in order to re-
8 duce some of the gap between genotyping and phenotyping in animal breeding.
9 We demonstrated that atlas segmentation was able to predict major parts and
10 organs of the pig with a numerical test applied to the primal commercial cuts.

Keywords: Computed Tomography, pig, atlas, segmentation, breeding

1. Introduction

12 Recent advances in genome sequencing technology has led to high-throughput
13 and high-density information in humans, animals and plants (Houle et al., 2010).
14 Variation in phenotypes is produced through a web of interactions between
15 genotype and environment, and there is a need for detailed phenotypic data
16 to characterize the phenomes. Measuring body composition in farmed animal
17 breeding is important in order to improve growth and feed efficiency, health,

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18 meat quality and market value of carcasses (Nissen et al., 2006; Roche et al.,
19 2009). Body composition has traditionally been assessed by a number of dif-
20 ferent means, ranging from subjective scoring (Fox & Black, 1984) or simple
21 point measurements of subcutaneous fat (Silva et al., 2005) to physical dissec-
22 tion (Nissen et al., 2006) or chemical analysis (Shields et al., 1983) of carcasses
23 or *in vivo* volume scans using Computed Tomography (CT) or Magnetic Res-
24 onance Imaging (MRI) (Szabo et al., 1999; Mitchell et al., 2001; Scholz et al.,
25 2015).

26 For pigs, the use of CT makes it possible to obtain accurate *in vivo* mea-
27 surements of body composition (Gjerlaug-Enger et al., 2012). Genetic selection
28 on body composition traits in pigs was previously done by physical dissection
29 of full-sibs and half-sibs of the selection candidates, which give much less accu-
30 rate breeding value estimations compared with measuring body composition on
31 the selection candidates themselves *in vivo*. Today, the pig breeding company
32 Topigs Norsvin uses CT to measure body composition and monitor orthopedic
33 disorders on 3.500 nucleus boars annually as an integrated part of their testing
34 system. In this paper, we present an anatomical atlas from CT, which will help
35 to close the phenomic gap in pig anatomy by giving access to high-throughput
36 and high-dimensional anatomical phenotypes.

37 Obtaining *in vivo* body composition data from CT relies on segmentation
38 of cross sectional slices. The segmentation strategies can be based on (1) in-
39 tensities, applying adaptive thresholding of different tissues like adipose (fat),
40 muscle and bone tissue (Skjervold et al., 1981), (2) shape or position using de-
41 formable models or active contours (McInerney & Terzopoulos, 1996), and (3)
42 labelled atlas (Commowick, 2007). Methods are here ranked by complexity and
43 demands of prior knowledge either from own data or literature. Automation of
44 the segmentation methods would allow for detailed population studies of body
45 composition. For atlas based segmentation, this paper shows how an atlas can
46 be constructed using a subset of animals from the population of pigs.

47 The atlas can serve as a framework for building large data sets of anatomical
48 phenotypes, paving the way to detailed and high-density phenotypic informa-

49 tion on pig anatomical traits. The number of additional variables in the breeding
50 value estimation may be a limitation in terms of speed and complexity. The
51 atlas phenotypes will be highly beneficial in terms of selection for animals with
52 competitive advantages on muscle types, compared with the current selection
53 in most breeding programs today, where results from CT are applied to muscle-
54 and fat depth only (Gjerlaug-Enger et al., 2012). Creating atlases for primal
55 cuts; "shoulder", "belly", "loin" and "ham", representing the market needs
56 around the world would also make us able to sort our genetic material of pigs
57 more efficiently in terms of different markets. Furthermore, by enhancing the
58 anatomical traits by automatic segmentation, the accuracy of genetic selection
59 for carcass traits will increase even further. The indirect effect of this is that
60 more weight can be put in the breeding goal for hard-to-measure, low-heritable
61 traits like maternal and disease-related traits, and in the end the whole breed-
62 ing goal and genetic engine towards developing a more sustainable and accurate
63 breeding program for farmed animals.

64 **2. Methods**

65 *2.1. Approvement of the experiments*

66 All animals were cared for according to laws, internationally recognized
67 guidelines and regulations controlling experiments with live animals in Norway
68 (Regulation for the keeping of pigs in Norway 2003-02-18-175 (in Norwegian), 2003;
69 Animal welfare Act 2009-06-19-97 (in Norwegian), 2009); according to the rules
70 given by Norwegian Animal Research Authority. The CT scans were also used
71 in Gangsei & Kongsro (2016), which provides some more practical information
72 about the scanning.

73 *2.2. Data*

74 The intensity atlas is in principle is the average of 386 nucleus boars, in-
75 volving a total of approximately 3.4×10^{10} voxels (the 3D basic unit of the CT
76 scans). The method was motivated by methods applied to micro CT scans of

77 mice (Baiker et al., 2010; Li et al., 2008), where the skeletons were utilized as a
78 framework for conducting the transformations.

79 The raw CT scans were volume representations of the individual pigs. The
80 size of 3D data arrays (volumes) were approximately $512 \times 512 \times 1200$, where
81 the third dimension, size, varied slightly with pig length. Each data point
82 represented a voxel with size $0.9355 \text{ mm} \times 0.9355 \text{ mm} \times 1.25 \text{ mm}$. A CT intensity
83 according to the Hounsfield (HU) scale was associated with each voxel.

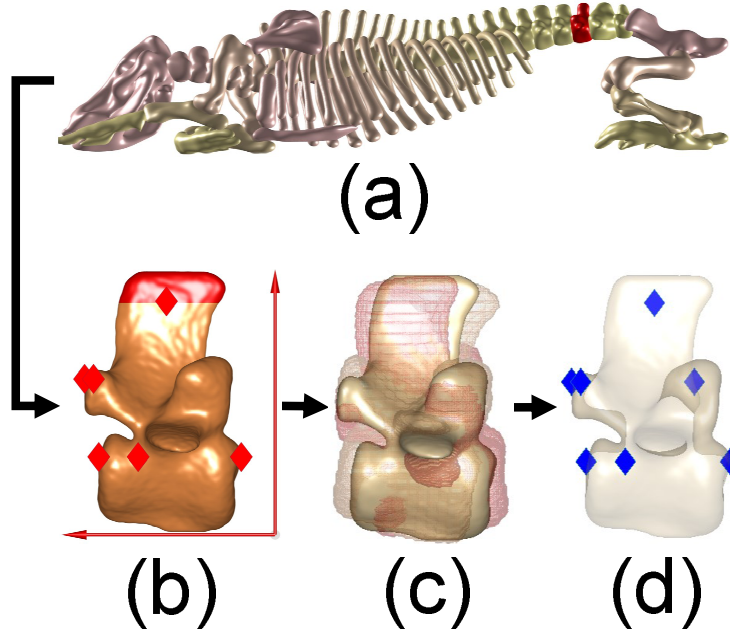
84 *2.3. Atlas*

85 The atlas represents the average pig. The atlas volume size was $500 \times 500 \times$
86 1600 , where each voxel represents a cube with a side length of 1 mm. We use the
87 expressions "intensity atlas" and "labelled atlas", where the intensities aligned
88 to each voxel might be interpreted as HU-units. In the labelled version, every
89 voxel is aligned to a specific label, i.e. organ, cut part etc.

90 Labelled and intensity volumes (3D) might be defined by a matrix repre-
91 sentation, where the $N_y \times 3$ matrix \mathbf{Y} and $N_x \times 3$ matrix \mathbf{X} , represent the
92 atlas, and a random individual pig, respectively. N_y and N_x are the number of
93 voxels in the respective images. Each row in \mathbf{Y} and \mathbf{X} defines the (Cartesian)
94 coordinates for one voxel. The atlas was constructed through successive oper-
95 ations described in the next sections. Figures are used extensively to highlight
96 important principles.

97 *2.4. Skeleton atlas – image moments invariants*

104 The first step was to identify the major bones in all pigs (Gangsei & Kongsro,
105 2016) (Fig. 1a). We calculated basic features for each bone, often referred to
106 as image moments invariants (Hu, 1962): Center of mass (COM or $\bar{\mathbf{x}}$), the
107 orthonormal basis of the bone (\mathbf{R}), volume ($v = n_\delta \times 0.9355^2 \times 1.25$, where n_δ
108 is number of voxels) and length (l), that is, the Euclidian distance spanned by
109 the bone along the first orthogonal basis vector. Left side bones were treated
110 as right side bones by mirroring them over the sagittal plane before calculating
111 the image moments invariants. The coordinates of each bone were represented



98

99 Figure 1: Construction of average bone by image moment invariants. (a) Segmented skeleton
 100 in a random pig; the vertebra illustrated in panels b–d is highlighted in red. (b) A vertebra with
 101 its orthonormal basis (arrows), landmarks, and the area where extra weight for orientation is
 102 added (red at top). (c) Construction of the average shape by rotating and scaling bones from
 103 all pigs to a common formwork. (d) Landmarks (blue) on the average vertebrae.

112 by the $n_\delta \times 3$ matrix \mathbf{X}_δ . Furthermore, the diagonal weight matrix \mathbf{W} assigned
 113 a specific weight to each voxel for the purpose of controlling the main directions
 114 of the orthonormal basis. The mathematical expressions for the COM and
 115 orthonormal basis were:

$$\bar{\mathbf{x}} = (1/n_\delta) \mathbf{X}_\delta^t \mathbf{1}_{n_\delta}, \quad \mathbf{R} = \text{Eig} \left\{ (\mathbf{X}_\delta - \mathbf{1}_{n_\delta} \bar{\mathbf{x}}^t)^t \mathbf{W}^2 (\mathbf{X}_\delta - \mathbf{1}_{n_\delta} \bar{\mathbf{x}}^t) \right\}, \quad (1)$$

116 where the notation $\text{Eig} \{ \mathbf{A} \}$ denotes the eigenvectors of the matrix \mathbf{A} scaled to
 117 unit length.

118 The concept of the weighting of voxels is shown in Fig. 1b, where the voxels
 119 in the red area, i.e. the voxels within a distance less than $1/10$ of the total length
 120 (l) from the top, were given heavy weights (100). Thus, the first column in \mathbf{R} ,

121 i.e. the eigenvector having the largest corresponding eigenvalue, points approx-
 122 imately perpendicular to the coronal plane (upwards), the second eigenvector
 123 points approximately perpendicular to the transverse plane (forwards) and the
 124 third eigenvector points approximately perpendicular to the sagittal plane (to
 125 the left). For other bones, different parts were assigned additional weights, but
 126 the basic principle remains unchanged.

127 Based on the features of the individual bones we constructed atlas bones,
 128 i.e. templates for every bone in a pig (Fig. 1d). To every atlas bone, COM,
 129 volume, length, a common orthonormal basis and a shape, was applied. The
 130 COM ($\bar{\mathbf{x}}_T$), volume (v_T) and length (l_T) was just the average for all bones. For
 131 all bones in the spine and sternum, the COM value for the direction perpendic-
 132 ular to the sagittal plane (i.e. sideways), was set to 250 (mm). The common
 133 orthonormal basis, \mathbf{R}_T , was set to the individual orthonormal basis closest to
 134 the geometrically average orthonormal basis. Hence, by letting r_{ij} denote the
 135 element of the i th row and j th column of \mathbf{R} , and letting \bar{r}_{ij} denote the average
 136 of the same element in all pigs, the \mathbf{R} for which $\sum_{i=1}^3 \sum_{j=1}^3 (r_{ij} - \bar{r}_{ij})^2$ had the
 137 minimum value was chosen as the common orthonormal basis for the bone in
 138 question.

139 In order to construct the average shape, all bones were transformed to a 3D
 140 image, \mathbf{B} , of predefined size, $m_1 \times m_2 \times m_3$, (Fig. 1c). The coordinates for the
 141 individual bones in these 3D images, denoted \mathbf{Z}_δ , were given by rounded and
 142 scaled values of $(m_1/l) \mathbf{X}_\delta \mathbf{R}$. The scaling of \mathbf{Z}_δ was done by subtracting column
 143 means and adding column minimum values. Thus, every bone spanned the first
 144 dimension of \mathbf{B} completely and was centred according to the two remaining
 145 dimensions. The final intensities of \mathbf{B} equalled the sum of all bones transformed
 146 into it. The average shape was constructed by setting a threshold making sure
 147 that the volume of voxels in \mathbf{B} having higher intensity than this threshold, was
 148 equal to the average volume of the bone (v_T).

149 *2.5. Corresponding landmarks*

150 The crucial steps of the method involved constructing corresponding land-
 151 marks between the volumes of the individual pigs (Fig. 2a–c). The initial step
 152 (Fig. 1d), was to set landmarks at approximately every 20mm along the main
 153 direction of the orthonormal basis of the average shaped bone. The landmarks
 154 were set either at the top, bottom, right and left side of the surface or in the cen-
 155 tre of the bone (typically for ribs, hand and foot). In total approximately 1200
 156 landmarks on the skeleton were identified (Fig.2a), varying with the number of
 157 vertebrae and ribs in the individual pigs. The coordinates of the landmarks in
 158 the common orthogonal basis, \mathbf{R}_T , are denoted \mathbf{Z}_l , and the corresponding COM
 159 is denoted $\bar{\mathbf{z}}$.

160 These landmarks were transformed back to the basis of the individual pigs
 161 and the atlas by reversing the transformations based on image moments invari-
 162 ants. The common averages were used for the transformation to the atlas space
 163 resulting in a pattern symmetric over the sagittal plane (Fig. 2b). Individ-
 164 ual image moments invariants were used for the individual pigs; consequently
 165 there was no symmetric pattern for these points (Fig. 2a). The mathematical
 166 expressions for the reverse transformations are given by:

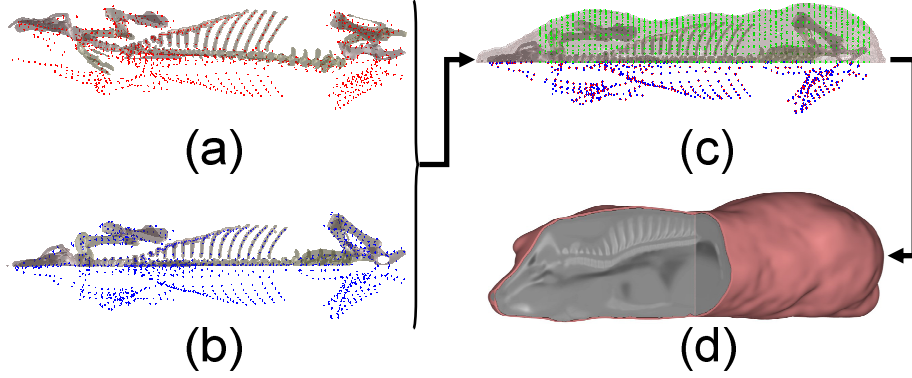
$$\begin{aligned} \mathbf{Y}_l &= (l_T/m_1) (\mathbf{Z}_l - \mathbf{1}_{n_l}\bar{\mathbf{z}}) \mathbf{R}_T^{-1} + \mathbf{1}_{n_l}\bar{\mathbf{x}}_T \\ \mathbf{X}_l &= (l_T/m_1) (v/v_T)^{1/3} (\mathbf{Z}_l - \mathbf{1}_{n_l}\bar{\mathbf{z}}) \mathbf{R}^{-1} + \mathbf{1}_{n_l}\bar{\mathbf{x}} \end{aligned} \quad (2)$$

167 , where the landmarks in the atlas and individual pigs are denoted \mathbf{Y}_l and \mathbf{X}_l ,
 168 respectively.

169 *2.6. Non-rigid transformation*

177 The stacked matrices of \mathbf{Y}_l -s and \mathbf{X}_l -s (all bones), are denoted \mathbf{Y}_1 and \mathbf{X}_1 .
 178 These matrices were used to construct a cubic B-spline based transformation of
 179 \mathbf{X}_1 to \mathbf{Y}_1 . The underlying model for the transformation is:

$$\mathbf{Y}_1 = \mathbf{Q}_{1X}\beta_1 + \mathbf{E}_1, \quad (3)$$



170

171 Figure 2: Construction of corresponding landmarks and the intensity atlas. (a) Landmarks for
 172 all bones transformed back to the original space of the pig. (b) Landmarks of all average bones
 173 transformed to the atlas space. (c) Non-rigid transformation based on the skeleton landmarks
 174 applied to the skeleton (blue/ red) and surface (skin). A secondary set of landmarks on the
 175 pig surfaces (green). (d) The intensity atlas. I.e. average HU-units after all voxels of all pigs
 176 are transformed to the atlas space.

180 , where \mathbf{Q}_{1X} denotes a matrix of size $n_1 \times p_L$ the elements of which were calcu-
 181 lated by tensor (cubic) B-spline functions using \mathbf{X}_1 as input. The parameter β_1
 182 denotes the regression parameters and \mathbf{E}_1 random noise. We utilized existing
 183 software (Kroon, 2011a,b) for the implementation of all B-spline based transfor-
 184 mations. The software automatically calculated \mathbf{Q}_{1X} including optimizing the
 185 knot grid used in the cubic B-spline functions, and provided estimates, $\hat{\beta}_1$, of
 186 β_1 for all pigs based on the input \mathbf{X}_1 and \mathbf{Y}_1 .

187 For all pigs the surface voxels (skin) were identified, with coordinates denoted
 188 \mathbf{X}_S . The surface points from all 386 pigs were transformed to a common 3D
 189 image, \mathbf{S} , with the same dimensions as the atlas, by applying the transformation
 190 based on skeleton landmarks. The mathematical formula for this transformation
 191 is written as $\hat{\mathbf{Y}}_S = \mathbf{Q}_{SX}\hat{\beta}_1$ where the rounded values of $\hat{\mathbf{Y}}_S$ gave the coordinates
 192 of the surface voxels \mathbf{X}_S transformed to \mathbf{S} . In order to get a symmetric surface,
 193 \mathbf{S} was mirrored over the sagittal plane. The final atlas surface was defined as the
 194 voxels in \mathbf{S} having maximum intensity and composing a continuous, connected
 195 surface.

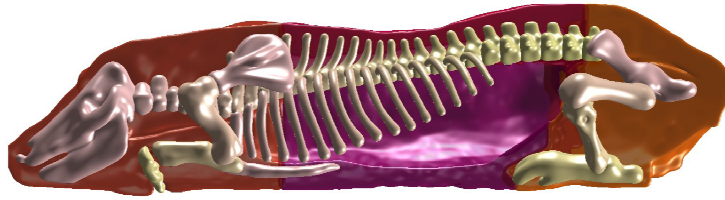
196 For every 20 mm, on the interval from 200mm to 1400mm, along the lon-
 197 gitudinal axis of the atlas surface, 34 new landmarks were set on the average
 198 surface (Fig. 2c). These points were set at a fixed set of angles around the cen-
 199 tre of the slice in question. The coordinates of these landmarks are denoted \mathbf{Y}_2 .
 200 Corresponding points for individual pigs, \mathbf{X}_2 , were set as the surface points in
 201 \mathbf{X}_S of which the corresponding transformed points, i.e. $\hat{\mathbf{Y}}_S$, had the minimum
 202 Euclidian distance to the points in \mathbf{Y}_2 .

203 The motivation for constructing the corresponding points on the surface, i.e.
 204 \mathbf{Y}_2 and \mathbf{X}_2 , was to increase the precision of the final B-spline transformations
 205 that were applied to the full volumes of the original pigs. Hence, the coordinates
 206 of the full volumes were the rounded values of $\hat{\mathbf{Y}} = \mathbf{Q}_{12X}\hat{\beta}_{12}$, where the basic
 207 functions of \mathbf{Q}_{12X} and $\hat{\beta}_{12}$ were calculated using the stacked matrices of \mathbf{Y}_1
 208 and \mathbf{Y}_2 , and \mathbf{X}_1 and \mathbf{X}_2 . The final intensity-based result is illustrated in Fig.
 209 2d. The intensities of the voxels in the intensity atlas are simply the average
 210 HU-unit after the final transformation of all voxels in all pigs.

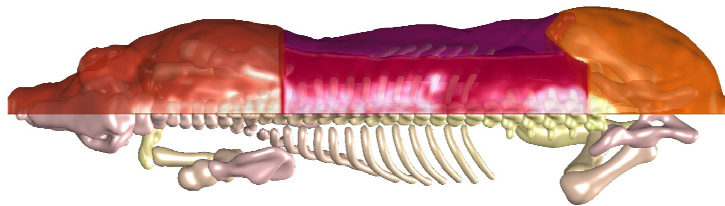
211 2.7. Labelled atlas – atlas segmentation

217 A labelled version of the atlas (Fig. 3a–b), was constructed by manual seg-
 218 mentation of the intensity atlas. The final step was to transform the labels onto
 219 the individual pigs, or eventually, onto new pigs registered to the atlas. Since
 220 every voxel in the individuals transformed to the (labelled) atlas corresponds to
 221 exactly one voxel in the atlas, the label of all voxels in individual pigs are easily
 222 defined (Fig. 4a–d).

223 The inner organs were segmented out by methods combining thresholds (HU-
 224 units) in the intensity atlas, and manual segmentation. The commercial cuts
 225 were set by segmenting the shoulder, which also includes the head, from loin
 226 and belly by a cut exactly in the transverse plane of the atlas. The ham and
 227 loin were also segmented by a cut in the transverse plane. Belly was segmented
 228 from ham and loin by manual segmentation based on the intensity atlas.



(a)



(b)

212

213 Figure 3: The labelled atlas. (a) View perpendicular to the sagittal plane. (b) View perpen-
 214 dicular to the coronal plane. In both panels ham is shown with orange color, belly with violet
 215 color, loin with clear red color and shoulder with red/ brown color. The major bones in the
 216 skeleton are shown with different shades in gray/ yellow/ pink colors.

229 *2.8. Validation*

230 First and foremost the method was validated by visual inspection of the
 231 segmentation applied to the individual pigs.

232 In order to conduct a numerical test of the method, we applied atlas seg-
 233 mentation to the primal cuts of 52 headless carcasses (left half) (Fig. 4). We
 234 predicted the weights of all voxels by applying a simple regression equation
 235 for voxel density (kg/m^3) using the intensities, measured as Hounsfield units
 236 (HU), as predictor variable. The regression parameters were calculated by or-
 237 dinary least squares regression using the registered weights of all 52 carcasses
 238 as response.

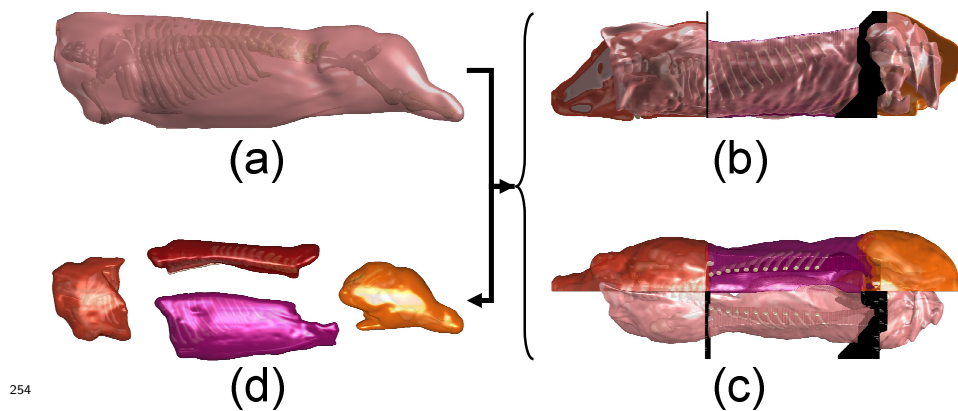
239 The corresponding cut weights (kg) and their proportions (% of carcass
 240 weight) (carcass right half) were registered by butchers at the Norwegian Meat
 241 and Poultry Research Center (Animalia) pilot plant. Thus we were able to cal-

242 culate the correlations between cut weights and cut proportions based on two
 243 independent methods, i.e. atlas segmentation and manual butchering. Vari-
 244 ances in cut proportions are, unlike variances in the cut weights, independent
 245 of total carcass weight. Thus, an eventual significant positive correlation for
 246 cut proportions, as opposed to the correlation between cut weights, might be
 247 viewed as a strong indication of the validity of the atlas segmentation method.

248 2.9. Code availability

249 All computations were conducted using the software MATLAB (MATLAB,
 250 2015). A demonstration of the central parts of the computer code applied to
 251 data from parts of a random pig is included as supplementary material in the
 252 zipped folder "Code_and_Data.zip".

253 3. Results



255 Figure 4: Atlas segmentation applied to a carcass (left half). (a) An untransformed carcass.
 256 (b–c) The carcass (left hand side) registered (transformed) to the atlas (right hand side). The
 257 loin cut is removed to increase visibility. The other cuts are illustrated as black surfaces. (d)
 258 The final segmentation for the carcass in its four major cuts.

259 Visual inspection of the individual carcasses after transformation show that
 260 the method has an acceptable accuracy for atlas segmentation of the major
 261 parts, for an example see supplementary Video 1. The accuracy is best close

262 to the skeleton structure, where the density of landmark is huge, whereas the
263 accuracy declines in areas where landmarks are scarce, typically in the back
264 part of the belly.

265 The correlations between cut weight measured by atlas segmentation and
266 manual butchering were 0.95, 0.91, 0.87 and 0.95 for shoulder-, belly-, loin- and
267 ham weights, respectively. For the cut proportions the corresponding correla-
268 tions were 0.60, 0.38, 0.36 and 0.47, all significantly different from 0 ($p < 0.01$).
269 The variation in cut proportions between individuals were small, i.e. standard
270 deviation at approximately 1 % unit.

271 4. Discussion

272 Differences in predicted cut weights between left and right sides might be
273 substantial due to morphological differences, butcher effects and inaccurate
274 splitting of carcasses. For shoulder and belly weights, differences between butch-
275 ers are reported as high as 6–10% (Nissen et al., 2006). Thus, the correlation
276 between the cut weights registered by butchers and by atlas segmentation was
277 not expected to be extremely high even with a perfect atlas segmentation. For
278 the cut proportions the *a priori* expected correlation between the two methods
279 were substantially lower, due to the small variation in cut proportions between
280 individuals. Thus, the highly significant positive correlations is a strong support
281 for the usefulness of atlas segmentation.

282 The transformations were solely based on corresponding landmarks. The
283 state-of-the-art methods in medical image analysis, see Sotiras et al. (2013)
284 for an overview, would generally include an extra step involving fine tuning of
285 the transformation based on image intensities, typically based on the Gauss-
286 Newton algorithm (Gill & Murray, 1978). This step aims at minimizing the
287 cost based on a similarity measure between individual pigs and the intensity
288 atlas (reference and template), utilizing the intensities of all data points. The
289 transformations and intensity atlas described in this paper would constitute a
290 natural starting point for such an algorithm. If successful, the result would be

291 an even finer tuned intensity atlas, which in turn enables construction of a more
292 detailed labelled atlas. However, there is a substantial risk associated with such
293 methods as they may result in convergence to local optima, or yield over-fitted
294 solutions, i.e. applying too much non-rigid deformation.

295 The full set of landmarks is the joint set of the original skeleton-landmarks
296 and the surface-landmarks. The surface-landmarks are set based on a provi-
297 sional transformation of the full surface, based on the skeleton-landmarks. We
298 applied a simple method based on euclidian distances to define the surface land-
299 marks. As part of our further work we would like to evaluate 3D point matching
300 algorithms (Tam et al., 2013) as an alternative for defining these landmarks. We
301 would also like to evaluate the possibility for identifying more landmarks prior
302 to the final transformation. In particular landmarks defining the surface sepa-
303 rating the internal organs from the commercial cuts would have been valuable.

304 For a whole-body analysis, the corresponding landmarks are sufficient to
305 obtain a satisfactory level of accuracy. As the method is automatic and robust,
306 it offers a potential of multiplying the level of registered phenotypic variation for
307 the full parental lines of breeding pigs. Thus it might constitute the foundation
308 for the next generation of high-throughput and high-density phenotyping in
309 animal breeding.

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