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Molecular Hydrogen and Catalytic Combustion in the Production of Hyperpolarized ^{83}Kr and ^{129}Xe MRI Contrast Agents.

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Abstract.

Hyperpolarized (hp) ^{83}Kr is a promising MRI contrast agent for the diagnosis of pulmonary diseases affecting the surface of the respiratory zone. However, the distinct physical properties of ^{83}Kr that enable unique MRI contrast also complicate the production of hp ^{83}Kr . This work presents a radically new approach in the generation of hp ^{83}Kr that can likewise be utilized for the production of hp ^{129}Xe . Molecular nitrogen, typically used as buffer gas in spin exchange optical pumping (SEOP), was replaced by molecular hydrogen without penalty for the achievable hyperpolarization. In this particular study, the highest obtained nuclear spin polarizations were $P = 29\%$ for ^{83}Kr and $P = 63\%$ for ^{129}Xe . The results were reproduced over many SEOP cycles despite the laser induced on-resonance formation of rubidium hydride (RbH). Following SEOP, the H₂ was reactively removed via catalytic combustion without measurable losses in hyperpolarized spin state of either ^{83}Kr or ^{129}Xe . Highly spin polarized ^{83}Kr can now be purified for the first time to provide high signal intensity for the advancement of *in vivo* hp ^{83}Kr MRI. More generally, a chemical reaction appears as a viable alternative to the cryogenic separation process, the primary purification method of hp ^{129}Xe for the past 2 ½ decades. The inherent simplicity of the combustion process will facilitate hp ^{129}Xe production and should allow for on-demand continuous flow of purified and highly spin polarized ^{129}Xe .

Significance.

The high signal intensity associated with magnetic resonance of hyperpolarized ^{129}Xe has enabled countless applications ranging from materials science to biomedical MRI of the lung and brain. New modalities are constantly emerging, for example hyperpolarized ^{129}Xe biosensors are of potential interest for molecular imaging of biomarker distribution in organs. Hyperpolarized ^{83}Kr shows promise as novel surface sensitive contrast agent for pulmonary MRI but previous work was limited to excised lungs. This work reports a radically new approach in the generation of hyperpolarized contrast agents that makes highly concentrated hyperpolarized ^{83}Kr available for the first time. The results also provide the basis for on-demand flow production of highly concentrated hyperpolarized ^{129}Xe for *in situ* process monitoring and *in vivo* molecular imaging.

Introduction.

The development of hyperpolarized (hp) noble gas MRI has resulted in a number of excellent protocols to probe different structural and functional aspects of lungs in health and disease (1-6). Technological improvements (6-15) have enabled pulmonary hp ^{129}Xe MRI at high spatial resolution, thereby reducing the need for usage of the scarcely available ^3He isotope. Furthermore, tissue solubility, large chemical shift range, and interaction with specific sensor molecules allow for a variety of hp ^{129}Xe applications in biomedical sciences and beyond (1-6, 16, 17). Despite its nuclear electric quadrupole moment that causes rapid relaxation, the isotope ^{83}Kr (nuclear spin $I = 9/2$) can be hyperpolarized through Rb spin exchange optical pumping (SEOP) as first demonstrated by Grover (18) and explored in detail by Cates, Happer and co-worker (19). Volk and co-workers first observed ^{83}Kr quadrupolar coupling in the gas phase that originated from the surface of the SEOP cell (20) and Mehring and co-workers described T_2 relaxation as a probe for the cell surfaces (21). The intriguing properties of ^{83}Kr can be more generally utilized after the removal of the reactive Rb vapor to generate surface sensitive MRI contrast (22). Most recently, T_1 surface quadrupolar relaxation (SQUARE) MRI contrast (23) with hp ^{83}Kr in excised lungs was demonstrated to be indicative of surface to volume changes in an animal model of emphysema (24).

Although hp ^{129}Xe can be obtained through dynamic nuclear polarization (DNP) (25) with high spin polarization levels of up to $P = 30\%$ (26), at present only SEOP can produce hp ^{129}Xe with $P \geq 90\%$. Furthermore SEOP is the currently the only method to provide hp ^{83}Kr for biomedical MRI applications (24). During SEOP of ^{83}Kr or ^{129}Xe , the noble gas is diluted with a buffer gas, usually either a $^4\text{He} - \text{N}_2$ mixture or pure N_2 gas. The buffer gas serves a dual purpose as it prevents destructive

radiation trapping, originating from radiative electronic relaxation of rubidium (27, 28), but also causes pressure broadening of the Rb D₁ linewidth. Rubidium line broadening maximizes adsorption of laser light emitted by high power solid devices, even if those are line narrowed. Following SEOP, hp ¹²⁹Xe is cryogenically separated from the gas mixture under carefully chosen conditions to prevent polarization loss (29). Cryogenic separation complicates the operational procedures for clinical and pre-clinical hp ¹²⁹Xe MRI. For a number of applications a repeat noble gas delivery at high polarization and concentration levels is needed (6, 30-35). Additionally, a very constant level of spin polarization is required for the HyperCEST molecular imaging methodology with hp ¹²⁹Xe biosensors (17, 36-38). Cryogenic separation enables increased polarization in pure xenon gas but is inherently a ‘batch mode’ production process that disrupts on-demand continuous flow. While cryogenic separation may complicate and limit some hp ¹²⁹Xe applications, it is not an option at all for the hp ⁸³Kr production due to the fast quadrupolar relaxation. To avoid cryogenic separation, SEOP at a high noble gas mole fraction has been explored in the past (6, 10, 14, 39-41). Nevertheless, gas dilution is still required to ensure high spin polarization at the high production volumes required for MRI and the dilution therefore reduces MRI signal intensity per unit volume of inhaled gas. An innovative method developed by Kimura, Imai, Fujiwara, and co-workers (6, 10, 33) produces a constant stream of 70% concentrated hp ¹²⁹Xe but the polarization is typically in the P = 10% regime. In this work, ¹²⁹Xe and ⁸³Kr SEOP is attempted with mixtures containing molecular hydrogen as buffer gas and radiation quenching agent (42-46) that can subsequently be removed through catalytic combustion.

Results and Discussions.

Fig. 1a shows the ^{129}Xe nuclear spin polarization, P , as function of gas pressure after 6 min of SEOP of a mixture of 5% Xe and 95% Kr at an external cell temperature of 378 K. The spin polarization is similar to data produced previously with a 5% Xe – 95% N₂ mixture under almost identical conditions described and analyzed in detail in ref. (39), also shown in Fig. 1a for comparison. Using H₂ buffer gas, hp ^{129}Xe with up to $P = 63\%$ was generated within 6 min of SEOP at 70 kPa total gas pressure. Using 5% krypton in 95% buffer gas, the highest ^{83}Kr polarization of $P = 29\%$, obtained with H₂ after 11 min of SEOP at 440 K, is comparable to that obtained previously with N₂ under similar conditions (39).

On-resonance rubidium hydride formation. The high spin polarization values for ^{83}Kr with the H₂ in Fig. 1a were achieved repeatedly for more than 30 h of SEOP over a time span of about a week and for ^{129}Xe over a duration of at least 6 h of continuous SEOP despite the formation of rubidium hydrides (RbH) during on-resonance D₁ laser irradiation (47). Over time, a white RbH deposition was observed on all SEOP cell surfaces but to a lesser extent at the laser entry window. Furthermore, SEOP cell recycling, causing substantial removal of the RbH, was possible by increasing the temperature to 480 K for about 30 min with ongoing laser irradiation while the cell was connected, via a Rb trap, to a vacuum pump. Although excessive RbH build up on the cell entry window will reduce laser irradiation, deposition on other cell surfaces may not necessarily adversely affect the achievable noble gas spin polarization. Previous work demonstrated that the ^{131}Xe T₁ relaxation time increases for this spin $I = 3/2$ isotope because of RbH buildup (48-50). RbH surface coating may therefore also reduce the ^{83}Kr T₁ relaxation rates and improve SEOP. A detailed study by Cates and co-workers explored the effect of RbH surface

deposition on the T_1 relaxation of ^{129}Xe as a function of field strength (≥ 0.08 T) and temperature (≤ 340 K) in a spherical 25 mm diameter cell (51). Based on the results one may interpolate ^{129}Xe T_1 times in excess of 400 s at the conditions used in the current work, causing little interference during rapid SEOP.

H₂ as radiation quenching agent. The high polarization values obtained with H₂ in Fig. 1a, i.e. in the absence of any N₂, are remarkable. Depending on SEOP temperature, the gas mixtures usually contain at least a partial pressure of 5 kPa of molecular nitrogen for radiation quenching to prevent radiation trapping of arbitrarily polarized fluorescence photons that severely reduce Rb polarization (27, 28). Previous work, investigating the efficacy of H₂ to quench Rb radiation found that the effective cross sections for quenching of the D₁ and D₂ transitions are about 1 order of magnitude smaller for H₂ than for N₂ (42). An empirical model of radiation quenching with H₂ is reported in ref. (52) but is limited to buffer gas pressures below 7 kPa. Generally, H₂ has found little consideration as quenching agent at high gas density and temperature conditions typically employed for SEOP production of hp ^{129}Xe or hp ^{83}Kr for MRI applications.

The measurement of D₁ fluorescence at 795 nm, obscured by high power laser radiation, is experimentally very demanding. Instead, the Rb D₂ fluorescence during SEOP was straightforwardly monitored in this work. The mixing cross sections between the electronic states Rb $^*5^2\text{P}_{1/2}$ and Rb $^*5^2\text{P}_{3/2}$ are comparable for H₂ and N₂ (42) and the D₂ fluorescence should therefore provide at least qualitative insights into D₁ radiation quenching efficiency of the molecular hydrogen. Fig 1b demonstrates that H₂ serves as a remarkably efficient radiation quenching agent at partial pressures above approximately 40 – 60 kPa where little fluorescence was detected during SEOP even at the very high temperature of 433 K. Therefore, H₂ can be used as radiation

quenching agent during SEOP but the required partial pressure is about 10 times higher than that for N₂, in agreement with previous measurements of quenching cross section in ref. (42). Below this critical partial pressure, radiation quenching is largely incomplete and a substantial difference in the D₂ fluorescence is observed between SEOP of ¹²⁹Xe and ⁸³Kr. Fig. 1b depicts a higher fluorescence count at the elevated temperature used for ⁸³Kr SEOP (in the 433 – 440 K range) where the Rb density is almost 20 fold increased compared to that for ¹²⁹Xe SEOP at 378 K. At low buffer gas pressure, where radiation quenching is incomplete, the high Rb density for ⁸³Kr SEOP produces significantly more radiation trapping. The consequences of the increased radiation trapping can be observed in Fig. 1a where, at buffer gas pressures below approximately 50 kPa, the noble gas polarization obtained through SEOP with H₂ falls short compared to that with N₂. The effect of Rb density on radiation trapping was previously studied at extremely low H₂ partial pressure (< 0.1 Pa) for the purpose of SEOP of dissociated atomic hydrogen (43-46). Under these conditions, radiation quenching is effectively non-existent and radiation trapping can be limited only by keeping the Rb densities very low through SEOP temperatures around or below 318 K. In the current work, no adverse effect of H₂ as buffer gas at SEOP pressures above 40 – 50 kPa (with the exception of reversible RbH formation, discussed above) was found compared to SEOP with N₂ under otherwise identical conditions, regardless of the temperature. Note that the high IR quenching cross section of H₂ is a rare exception among small molecules without chemical double or triple bonds and Fig. 1 includes data obtained with CH₄ as buffer gas for comparison. The inefficient small quenching cross section of CH₄ (53) causes a high IR count (Fig. 1b) and a correspondingly low ¹²⁹Xe spin polarization below that of hp ⁸³Kr (Fig. 1a), a problem

that was previously solved using a ternary mixture of 5% Xe, 85% CH₄, and 10% N₂ (54).

Buffer gas removal through catalytic combustion. Efficient SEOP of noble gases in H₂ mixtures opens the path for oxidative buffer gas elimination that produces H₂O as the only, and through condensation easily removable, reaction product. Previous work demonstrated qualitatively the feasibility of hp ¹²⁹Xe MRI (54) of a methane combustion zone. To quantify the effect of catalytic hydrogen combustion on the noble gas spin polarization, an experimental setup was devised as sketched in Fig. 2a. Shutting of hp noble gas - H₂ mixture into the reactor chamber that contained a small quantity of Pt and monitoring the signal decay over time through NMR spectroscopy at 9.4 T provided the baseline data, shown as open circles in Fig 3b, for hp ¹²⁹Xe and in Fig. 4b for hp ⁸³Kr. For oxidative H₂ removal, O₂ was added, which led to hydrogen combustion within < 100 ms due to the presence of the Pt catalyst, as depicted in Fig. 2b. The reactor pressure during this process was monitored (Figs. 3a and 4a) but potential short pressure increases during the reaction were not detected at the time resolution of the pressure gauge. Upon adding O₂, slightly above the stoichiometric ratio, the pressure decreased within 15 s as the sole reaction product, H₂O, had condensed rapidly upon cooling. The temperature increase measured outside the reactor was limited to 5 K and the final reactor pressure of 4.7±0.5 kPa was close to that expected from the combined water vapor pressure at ambient temperature (3.2 kPa at 298 K) and the noble gas partial pressure (1.2 – 1.3 kPa).

Monitoring the hp ¹²⁹Xe signal intensity (Fig. 3b), an initial signal increase was observed upon O₂ delivery, caused by hp ¹²⁹Xe influx from the connecting PFA tubing (1.6 mm inner diameter) that was pushed into the reaction chamber by the oxygen gas. Within 20 s, gas convection and diffusion returned the signal intensity

approximately to the baseline value indicating that the nuclear spin state had experienced no significant depolarization. However, after the reaction, the ^{129}Xe relaxation was accelerated due to a small excess of paramagnetic O_2 (ca. 0.7 kPa partial pressure). Increasing the O_2 excess to 7.5 ± 0.5 kPa lead to further accelerated ^{129}Xe signal decay.

The hp ^{83}Kr data in Fig. 4b demonstrates that combustion caused no signal loss and, in contrast to ^{129}Xe , the ^{83}Kr gas phase relaxation slowed down after the reaction. The decrease of the ^{83}Kr T_1 relaxation was a likely consequence of competitive co-adsorption of water molecules on the reactor surface that have been found previously to reduce krypton surface interactions (55). The very low gyromagnetic ratio makes ^{83}Kr insensitive to paramagnetic relaxation even at higher (7.5 ± 0.5 kPa) oxygen partial pressure (Fig. 4b) (40). An initial short term signal increase upon O_2 gas delivery, present in the ^{129}Xe data, was not observed because hp ^{83}Kr located in the connecting PFA tubing depolarized due to fast quadrupolar T_1 relaxation in the presence of the fluorocarbon surface (56).

Conclusion.

The capability to almost instantaneously remove a buffer gas, that serves as an efficient radiation quenching agent during SEOP, allows for the first time for the generation of purified, highly spin polarized ^{83}Kr . Furthermore, the method may be of interest for a fully automated hp ^{129}Xe production at reduced costs without the need for cryogenic operations. Because of the low total gas pressure after catalytic buffer gas removal, the hp gases will require recompression to ambient pressure for biomedical application. Recompression has previously been demonstrated with little polarization loss for hp ^{129}Xe (10, 40) and acceptable 1/4 polarization loss for hp ^{83}Kr .

(40). Based on the result in this work, this would suggest that purified hp ^{83}Kr with 21% spin polarization is now feasible, a 7 fold improvement over recent hp ^{83}Kr work with 3 % apparent polarization that already allowed for MRI with $0.795 \times 0.635 \text{ mm}^2$ resolution in *ex vivo* lungs (24).

Note that the experimental setting was for the sole purpose of proof of concept demonstration and can be substituted by combustion under continuous flow within a catalytic converter. Furthermore, direct contact between H_2 and O_2 may be avoidable through the usage of recyclable metal oxides similar to those utilized in chemical looping combustion (57). Reactive H_2 removal may take place in a small flow-through catalytic converter placed downstream from the SEOP cell that would facilitate gas transport through the generated pressure gradient. Kimura, Imai, Fujiwara and co-workers used a peristaltic pump for continuous hp ^{129}Xe recompression after continuous flow SEOP at low pressures (6, 10, 33), a concept that could be further extended by flow-through catalytic buffer gas removal before recompression. Enabling on-demand production of an uninterrupted, continuous flow of hp ^{129}Xe at high spin polarization and purity, this concept should be of high value for a variety of applications ranging from material science to biomedical MRI. If required, hp ^{129}Xe could also be stored before recompression (and even before H_2 removal), using the extraordinary slow ^{129}Xe relaxation described in the past at low xenon density (58-60). As a final note, the presented concept does not involve any toxic reagents or reaction products and the complete absence of nitrogen and carbon prevents any accidental generation of nitrogen oxides (NO_x) and carbon monoxide (CO) during combustion. Any H_2 passing through the ‘buffer gas removal step’, however unlikely, can straightforwardly be detected through reliable hydrogen microsensors.

Materials and Methods.

SEOP was conducted at 0.04 T field strength in a 75 cm³ cylindrical borosilicate cell (approximately 120 mm long, 28 mm inner diameter) using a Comet module (Spectra Physics, Santa Clara, CA, USA) laser with a 0.2 nm linewidth producing 23 W incident power at the SEOP cell entrance window under very similar conditions as described in detail in ref. (61). A mixture of 5% Xe (or 5% Kr) in H₂ was used for all experiment in this work with natural abundance noble gas isotope distribution (i.e. 26.4% ¹²⁹Xe and 11.5% ⁸³Kr). Spin polarization was determined as described in ref. (61) (see also ref. (6)) and a general expression for polarization of I ≥ ½ spin systems is discussed in ref. (62). To monitor the Rb D₂ fluorescence during SEOP at 780 nm, a HR2000+ Ocean Optics spectrometer (Dunedin, FL, USA) was used.

All catalytic combustion experiments took place in a 1.5 mm glass wall vessel that contained 25 mg Pt/Al₂O₃ catalyst powder (i.e. 5 wt.% dry loading Pt on alumina). Standard safety precautions were followed and the H₂ - hp noble gas mixture was delivered to the reactor at pressures below 30 kPa to limit temperature and pressure bursts that could compromise reactor integrity. The reactor pressure was metered using a gas composition independent diaphragm gauge (OmegaDYNE INC, Sunbury, OH, USA).

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References.

1. Mugler JP & Altes TA (2013) Hyperpolarized ^{129}Xe MRI of the human lung. *J Magn Reson Imaging* 37(2):313-331.
2. Lilburn DML, Pavlovskaya GE, & Meersmann T (2013) Perspectives of hyperpolarized noble gas MRI beyond He-3. *J Magn Reson* 229:173-186.
3. Liu ZY, Araki T, Okajima Y, Albert M, & Hatabu H (2014) Pulmonary hyperpolarized noble gas MRI: Recent advances and perspectives in clinical application. *Eur J Radiol* 83(7):1282-1291.
4. Walkup LL & Woods JC (2014) Translational applications of hyperpolarized He-3 and Xe-129. *Nmr Biomed* 27(12):1429-1438.
5. Ruppert K (2014) Biomedical imaging with hyperpolarized noble gases. *Rep Prog Phys* 77(11).
6. Meersmann T & Brunner E eds (2015) *Hyperpolarized Xenon-129 Magnetic Resonance* (Royal Society of Chemistry).
7. Driehuys B, et al. (1996) High-volume production of laser-polarized Xe-129. *Applied Physics Letters* 69(12):1668-1670.
8. Ruset IC, Ketel S, & Hersman FW (2006) Optical pumping system design for large production of hyperpolarized Xe-129. *Phys Rev Lett* 96(5):053002.
9. Hersman FW, et al. (2008) Large production system for hyperpolarized Xe-129 for human lung imaging studies. *Academic Radiology* 15(6):683-692.
10. Imai H, Fukutomi J, Kimura A, & Fujiwara H (2008) Effect of reduced pressure on the polarization of Xe-129 in the production of hyperpolarized Xe-129 gas: Development of a simple continuous flow mode hyperpolarizing system working at pressures as low as 0.15 atm. *Concepts in Magnetic Resonance Part B-Magnetic Resonance Engineering* 33B(3):192-200.
11. Schrank G, Ma Z, Schoeck A, & Saam B (2009) Characterization of a low-pressure high-capacity ^{129}Xe flow-through polarizer. *Phys Rev A* 80(6):063424.
12. Mugler JP, et al. (2010) Simultaneous magnetic resonance imaging of ventilation distribution and gas uptake in the human lung using hyperpolarized xenon-129. *P Natl Acad Sci USA* 107(50):21707-21712.
13. Norquay G, Parnell SR, Xu XJ, Parra-Robles J, & Wild JM (2013) Optimized production of hyperpolarized Xe-129 at 2 bars for in vivo lung magnetic resonance imaging. *J Appl Phys* 113(4).
14. Nikolaou P, et al. (2013) Near-unity nuclear polarization with an open-source Xe-129 hyperpolarizer for NMR and MRI. *P Natl Acad Sci USA* 110(35):14150-14155.

15. Freeman MS, Emami K, & Driehuys B (2014) Characterizing and modeling the efficiency limits in large-scale production of hyperpolarized Xe-129. *Phys Rev A* 90(2).
16. Spence MM, et al. (2001) Functionalized xenon as a biosensor. *P Natl Acad Sci USA* 98(19):10654-10657.
17. Schroder L, Lowery TJ, Hilty C, Wemmer DE, & Pines A (2006) Molecular imaging using a targeted magnetic resonance hyperpolarized biosensor. *Science* 314(5798):446-449.
18. Grover BC (1978) Noble-Gas Nmr Detection through Noble-Gas-Rubidium Hyperfine Contact Interaction. *Phys Rev Lett* 40(6):391-392.
19. Schaefer SR, Cates GD, & Happer W (1990) Determination of Spin-Exchange Parameters between Optically Pumped Rubidium and Kr-83. *Phys Rev A* 41(11):6063-6070.
20. Volk CH, Mark JG, & Grover BC (1979) Spin Dephasing of Kr-83. *Phys Rev A* 20(6):2381-2388.
21. Butscher R, Wackerle G, & Mehring M (1996) Nuclear quadrupole surface interaction of gas phase 83Kr: comparison with 131 Xe. *Chem Phys Lett* 249:444-450.
22. Pavlovskaya GE, Cleveland ZI, Stupic KF, & Meersmann T (2005) Hyperpolarized Krypton-83 as a New Contrast Agent for Magnetic Resonance Imaging. *P Natl Acad Sci USA* 102:18275-18279.
23. Six JS, et al. (2014) Pulmonary MRI contrast using Surface Quadrupolar Relaxation (SQUARE) of hyperpolarized Kr-83. *Magnetic Resonance Imaging* 32(1):48-53.
24. Lilburn DML, et al. (2015) Hyperpolarized Kr-83 magnetic resonance imaging of alveolar degradation in a rat model of emphysema. *J R Soc Interface* 12(107).
25. Comment A, et al. (2010) Hyperpolarizing Gases via Dynamic Nuclear Polarization and Sublimation. *Phys Rev Lett* 105(1):018104.
26. Capozzi A, Roussel C, Comment A, & Hyacinthe JN (2015) Optimal Glass-Forming Solvent Brings Sublimation Dynamic Nuclear Polarization to Xe-129 Hyperpolarization Biomedical Imaging Standards. *J Phys Chem C* 119(9):5020-5025.
27. Happer W (1972) Optical-Pumping. *Reviews of Modern Physics* 44(2):169-249.
28. Wagshul ME & Chupp TE (1989) Optical-Pumping of High-Density Rb with a Broad-Band Dye-Laser and Gaalas Diode-Laser Arrays - Application to He-3 Polarization. *Phys Rev A* 40(8):4447-4454.
29. Kuzma NN, Patton B, Raman K, & Happer W (2002) Fast nuclear spin relaxation in hyperpolarized solid Xe-129. *Phys Rev Lett* 88(14):147602.
30. Baumer D, Brunner E, Blumler P, Zanker PP, & Spiess HW (2006) NMR spectroscopy of laser-polarized Xe-129 under continuous flow: A method to study aqueous solutions of biomolecules. *Angew Chem Int Edit* 45(43):7282-7284.
31. Driehuys B, Cleveland ZI, Moller HE, & Hedlund LW (2009) Continuously Infusing Hyperpolarized (129)Xe into Flowing Aqueous Solutions Using Hydrophobic Gas Exchange Membranes. *J Phys Chem B* 113(37):12489-12499.

32. Duewel M, *et al.* (2012) Online Monitoring of Styrene Polymerization in Miniemulsion by Hyperpolarized (129)Xenon NMR Spectroscopy. *Macromolecules* 45(4):1839-1846.
33. Imai H, *et al.* (2015) Regional fractional ventilation mapping in spontaneously breathing mice using hyperpolarized Xe-129 MRI. *Nmr Biomed* 28(1):24-29.
34. Norquay G, *et al.* (2015) Relaxation and exchange dynamics of hyperpolarized Xe-129 in human blood. *Magn Reson Med* 74(2):303-311.
35. Causier A, Carret G, Boutin C, Berthelot T, & Berthault P (2015) 3D-printed system optimizing dissolution of hyperpolarized gaseous species for micro-sized NMR. *Lab Chip* 15(9):2049-2054.
36. Witte C, *et al.* (2015) Live-cell MRI with Xenon Hyper-CEST Biosensors Targeted to Metabolically Labeled Cell-Surface Glycans. *Angew Chem Int Edit* 54(9):2806-2810.
37. Wang YF & Dmochowski IJ (2015) Cucurbit[6]uril is an ultrasensitive Xe-129 NMR contrast agent. *Chem Commun* 51(43):8982-8985.
38. Tassali N, *et al.* (2014) Smart Detection of Toxic Metal Ions, Pb²⁺ and Cd²⁺, Using a Xe-129 NMR-Based Sensor. *Anal Chem* 86(3):1783-1788.
39. Six JS, Hughes-Riley T, Stupic KF, Pavlovskaya GE, & Meersmann T (2012) Pathway to Cryogen Free Production of Hyperpolarized Krypton-83 and Xenon-129. *Plos One* 7(11):e49927.
40. Hughes-Riley T, *et al.* (2013) Cryogenics free production of hyperpolarized Xe-129 and Kr-83 for biomedical MRI applications. *J Magn Reson* 237:23-33.
41. Nikolaou P, *et al.* (2014) A 3D-Printed High Power Nuclear Spin Polarizer. *J Am Chem Soc* 136(4):1636-1642.
42. Hrycyshyn ES & Krause L (1970) Inelastic Collisions between Excited Alkali Atoms and Molecules .7. Sensitized Fluorescence and Quenching in Mixtures of Rubidium with H₂, HD, N₂, CD₄, C₂H₂, and C₂H₆. *Canadian Journal of Physics* 48(22):2761-2768.
43. Young L, Holt RJ, Green MC, & Kowalczyk RS (1989) Laser-Driven Polarized Sources of Hydrogen and Deuterium. *Nucl Phys A* 497:C529-C533.
44. Redsun SG, Knize RJ, Cates GD, & Happer W (1990) Production of Highly Spin-Polarized Atomic-Hydrogen and Deuterium by Spin-Exchange Optical-Pumping. *Phys Rev A* 42(3):1293-1301.
45. Anderson LW & Walker T (1992) The Effect of Radiation Trapping on a High-Field Spin Exchange Optically Pumped Target. *Nucl Instrum Meth A* 316(2-3):123-127.
46. Anderson LW & Walker T (1995) Spin-Exchange Optical-Pumping of Hydrogen and Deuterium Nuclei. *Nucl Instrum Meth A* 357(2-3):220-224.
47. Tam A, Moe G, & Happer W (1975) Particle Formation by Resonant Laser Light in Alkali-Metal Vapor. *Phys Rev Lett* 35(24):1630-1633.
48. Volk CH, Kwon TM, Mark JG, Kim YB, & Woo JC (1980) Measurement of the Rb-Xe-131 Spin-Exchange Cross-Section in Xe-131 Relaxation Studies. *Phys Rev Lett* 44(3):136-139.
49. Kwon TM, Mark JG, & Volk CH (1981) Quadrupole Nuclear-Spin Relaxation of Xe-131 in the Presence of Rubidium Vapor. *Phys Rev A* 24(4):1894-1903.

50. Wu Z, Happer W, Kitano M, & Daniels J (1990) Experimental Studies of Wall Interactions of Adsorbed Spin-Polarized Xe-131 Nuclei. *Phys Rev A* 42(5):2774-2784.
51. Rohrbaugh S, Wang HTJ, Singh J, Tobias WA, & Cates GD (2012) Magnetic decoupling of Xe-129 nuclear spin relaxation due to wall collisions with RbH and RbD coatings. *Phys Rev A* 86(4).
52. Rosenberry MA, Reyes JP, Tupa D, & Gay TJ (2007) Radiation trapping in rubidium optical pumping at low buffer-gas pressures. *Phys Rev A* 75(2).
53. Zameroski ND, Rudolph W, Hager GD, & Hostutler DA (2009) A study of collisional quenching and radiation-trapping kinetics for Rb(5p) in the presence of methane and ethane using time-resolved fluorescence. *Journal of Physics B-Atomic Molecular and Optical Physics* 42(24):245401.
54. Stupic KF, Six JS, Olsen MD, Pavlovskaya GE, & Meersmann T (2013) Combustion resistance of the Xe-129 hyperpolarized nuclear spin state. *Phys Chem Chem Phys* 15(1):94-97.
55. Cleveland ZI, *et al.* (2007) Hyperpolarized Kr-83 and Xe-129 NMR relaxation measurements of hydrated surfaces: Implications for materials science and pulmonary diagnostics. *J Am Chem Soc* 129(6):1784-1792.
56. Stupic KF, Cleveland ZI, Pavlovskaya GE, & Meersmann T (2006) Quadrupolar Relaxation of Hyperpolarized Krypton-83 as a Probe for Surfaces. *Solid State Nuclear Magnetic Resonance* 29:79-84.
57. Chen LM, Yang XG, Li X, Li G, & Snape C (2015) Prediction of formation of gas-phase bubbles correlated by vortices in the fuel reactor of chemical looping combustion. *Fuel Process Technol* 130:235-244.
58. Anger BC, *et al.* (2008) Gas-phase spin relaxation of Xe-129. *Phys Rev A* 78(4):043406.
59. Berry-Pusey BN, Anger BC, Laicher G, & Saam B (2006) Nuclear spin relaxation of Xe-129 due to persistent xenon dimers. *Phys Rev A* 74(6):063408.
60. Repetto M, *et al.* (2015) Systematic T-1 improvement for hyperpolarized (129)xenon. *J Magn Reson* 252:163-169.
61. Lilburn DML, *et al.* (2013) Validating Excised Rodent Lungs for Functional Hyperpolarized Xenon-129 MRI. *Plos One* 8(8).
62. Stupic KF, Cleveland ZI, Pavlovskaya GE, & Meersmann T (2011) Hyperpolarized Xe-131 NMR spectroscopy. *J Magn Reson* 208(1):58-69.

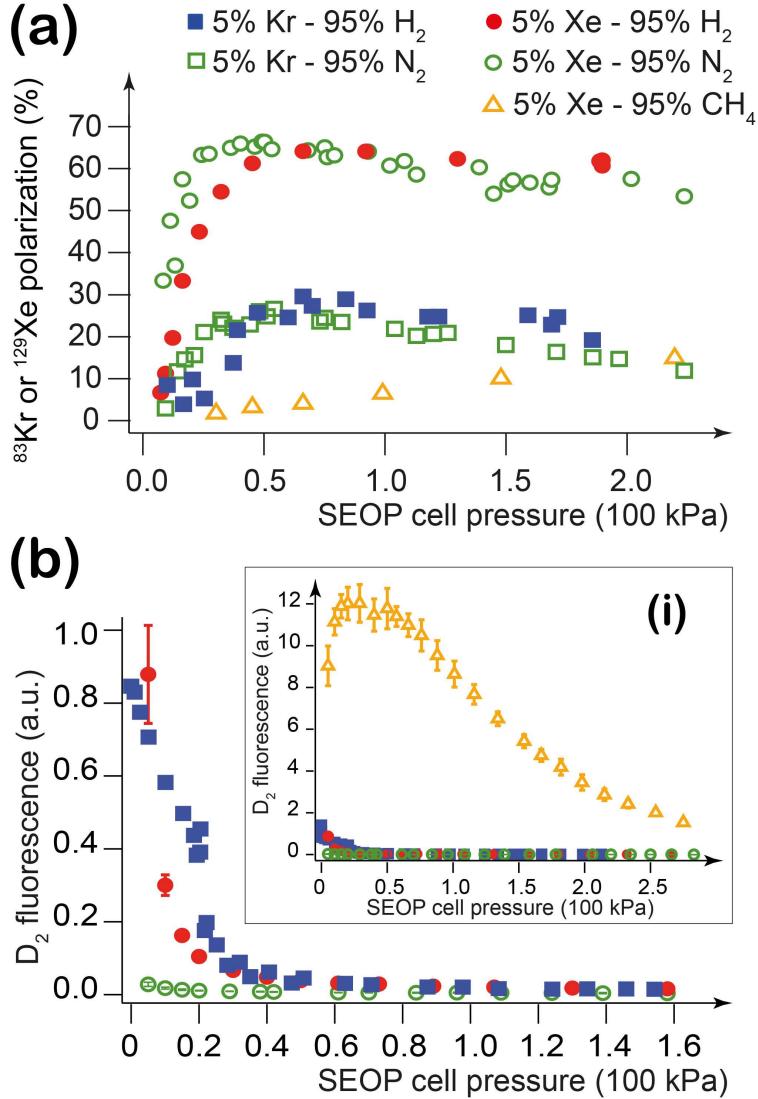


Figure 1. **(a)** SEOP generated ^{129}Xe and ^{83}Kr spin polarization in mixtures containing 5% noble gas and 95% buffer gas as a function of total SEOP gas pressure. Using H_2 as buffer gas, the ^{129}Xe spin polarization (obtained at 378 K) is shown in red filled circles and the ^{83}Kr polarization (obtained at 440 K) is displayed as blue filled squares. For comparison, previous data from ref. (39) with N_2 as buffer gas is shown for ^{129}Xe SEOP at 378 K (green open circles) and for ^{83}Kr SEOP at 433K (green open squares). In contrast, CH_4 is an inefficient buffer gas that lead to low spin polarization (orange open triangles, taken from ref. (54)). **(b)** The D_2 fluorescence at 780 nm (in arbitrary units, a.u.) measured at the front of the cell during SEOP indicates sufficient radiation quenching with H_2 at 378K (red circles) and at 433 K (blue squares) requires pressures above 50 kPa compared to N_2 that efficiently quenched D_2 radiation at pressures above approximately 5 kPa. Inset (i) shows the high D_2 fluorescence measured for Xe SOEP at 378 K with methane as a very ineffective quenching gas.

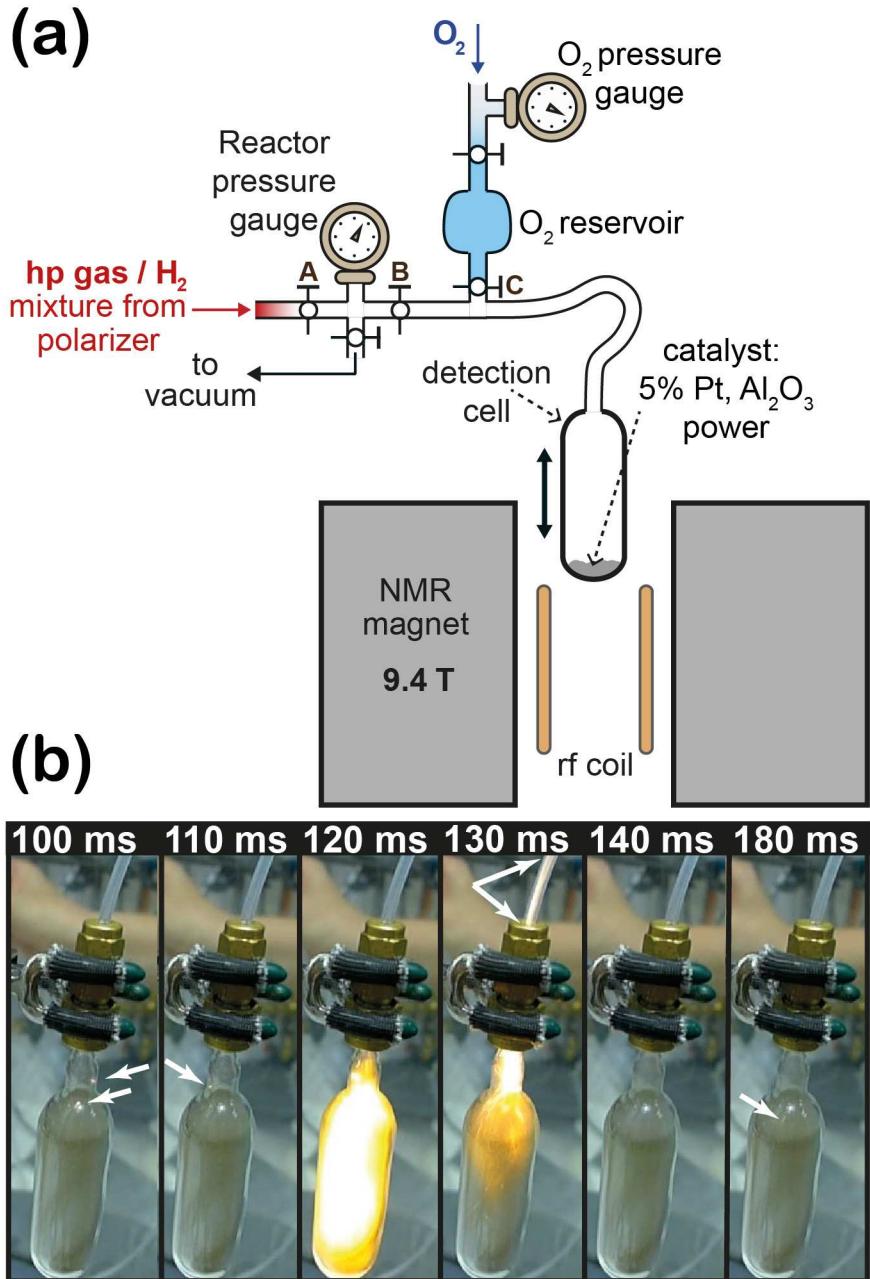


Figure 2. (a) Experimental setup used for combustion experiments. Using pressure equalization, the hp gas/H₂ mixture was shuttled to the reactor /detection cell containing the Pt catalyst. Oxygen was then injected from the reservoir. (b) Exported pictures from 100 frame/s video of the reactor upon O₂ delivery. Approximately 100 ms after opening of valve C, minor combustion zones became visible (indicated by white arrows) indicating that the catalytic oxidation of the H₂ gas had commenced. The major combustion event took place 20 – 30 ms thereafter and the combustion appeared to be largely completed within 80 ms. The reactor outside temperature increase was approximately 5K.

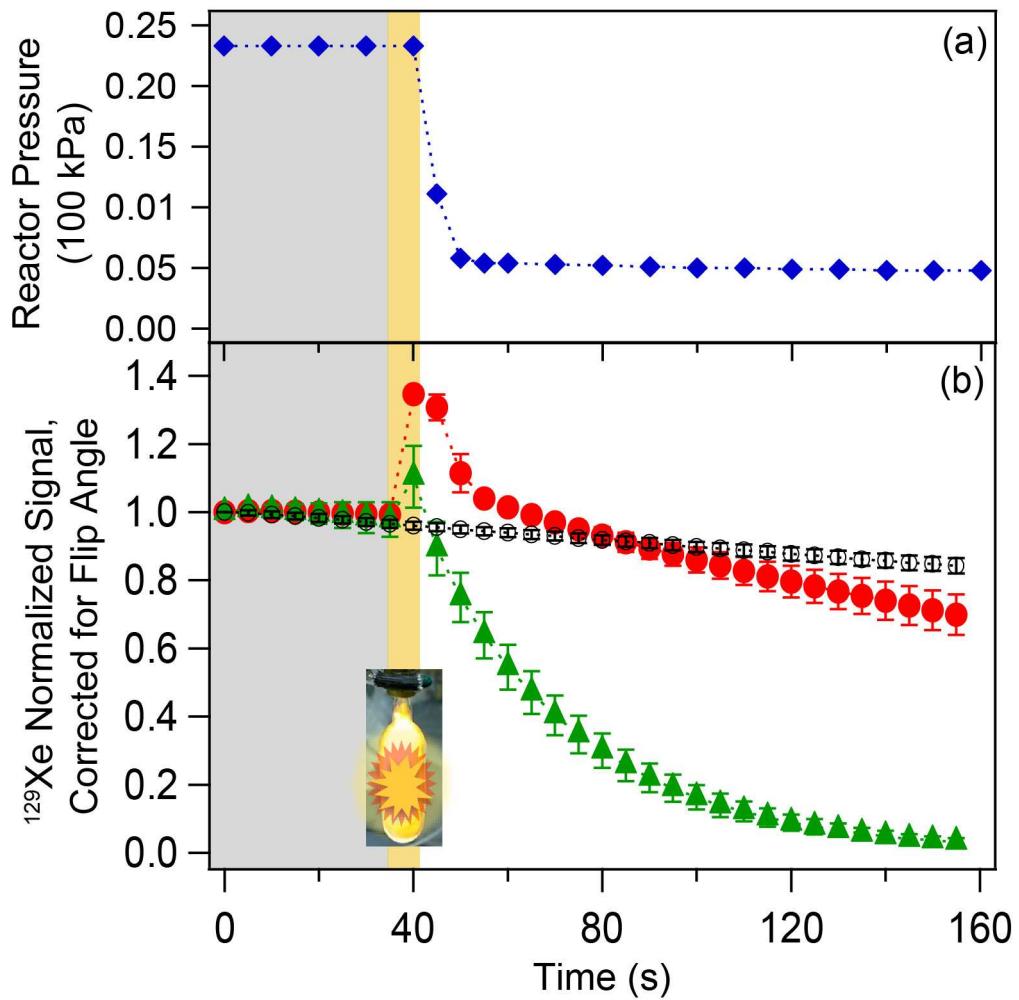


Figure 3. (a) *In situ* reactor pressure measurements (blue diamonds) during the combustion reaction of a 5% Xe / 95% H₂ gas mixture, with oxygen reservoir tap (tap C, Fig. 2a) opened at t=40 s adding 11.2 ± 0.4 kPa partial pressure of O₂. Average initial partial pressure of H₂ = 22.0 ± 1 kPa. **(b)** Normalized integrated hp ^{129}Xe NMR signals following a 9° pulse during the catalytic oxidation with 13.4 ± 0.4 kPa oxygen (red circles) or 20.5 ± 0.5 kPa (green triangles) added at t=40 s. Note that tap B (Fig. 2a) was kept shut, to reduce the dead volume of the reactor system. Average initial partial pressure of H₂ = 25.5 ± 1 kPa. Control signals with no oxygen / combustion (tap C, Fig. 2a, remained closed) shown as black open circles. Signal intensity data were corrected for flip angle attenuation and are the average from 3 repeat measurements.

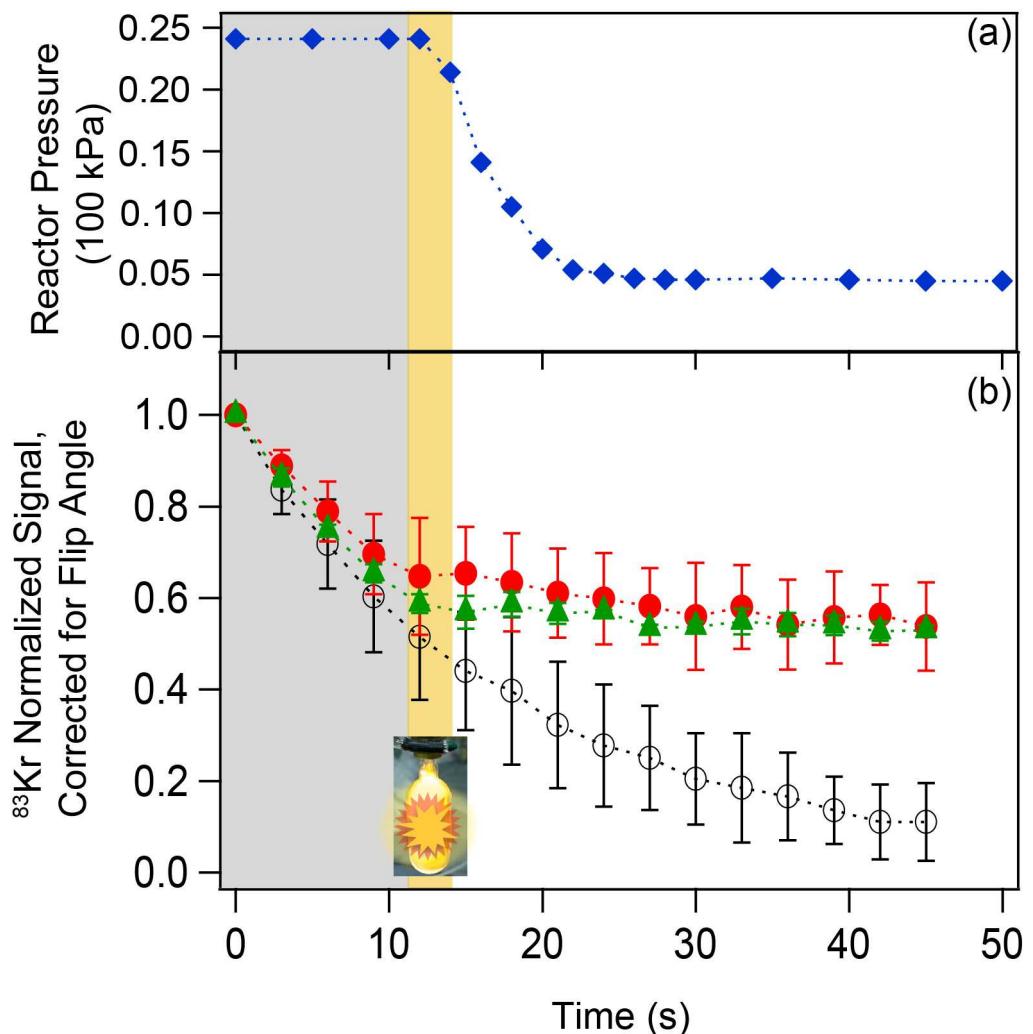


Figure 4 (a) Pressure curve of combustion reaction of a 5% Kr / 95% H₂ gas mixture after adding 11.2 ± 4 kPa O₂. Average initial partial pressure of H₂ = 23.5 ± 1 kPa. **(b)** Normalized integrated hp ⁸³Kr NMR signals following a 12° pulse during the combustion reaction adding 13.4 ± 0.4 kPa (red circles) and 20.5 ± 0.5 kPa (green triangles) partial pressure of oxygen. Average initial partial pressure of H₂ = 27.5 ± 2.5 kPa. Black open circles show control signals for a 5% Kr / 95% H₂ gas mixture with no combustion. Signal intensity data were corrected for flip angle attenuation and are the average from 3 repeat measurements.