INVITED ARTICLE



In situ magnetorheological SANS setup at Institut Laue-Langevin

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Abstract

A magnetorheological sample environment is presented that allows for in situ magnetic field and shear flow during small-angle neutron scattering (SANS) measurements and is now available at the Institut Laue-Langevin (ILL). The setup allows performing simultaneous magnetorheological measurements together with the investigation of structural and magnetic changes on the nanometer length scale underlying the rheological response of ferrofluids. We describe the setup consisting of a commercial rheometer and a custom-made set of Helmholtz coils and show exemplarily data on the field and shear flow alignment of a dispersion of hematite nanospindles in water.

Keywords Small-angle neutron scattering · Magnetorheology · Rheology · Magnetoviscous effect · Magnetic nanoparticles

Introduction

Recent progress toward magnetic soft matter combines the unique properties of soft matter and magnetic materials into complex magnetic fluids, such as original or inverse ferrofluids, ferrogels, and ferroelastomers [1–9]. Complex magnetic fluids find technological application in vibro-protection, lubrication, and for the precise control of polishing processes [10, 11], actuators and sensors such as shape-programmable matter [12], as well as the field-controlled release of incorporated drugs [13–15]. Ferromagnetic liquid crystals combine nematic order as well as ferromagnetic order and show non-Newtonian behavior in flow field [16–19]. Magnetic nanorod dispersions have been further demonstrated as in situ and non-contact viscosity gauges,

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being suitable probes for active microrheology [20]. The rotational friction of magnetic nanorods is sensitive to the stiffness of hydrogels [21] or the viscosity of liquid samples [22]. Recording the concomitant orientational redistribution with AC susceptibility, optical transmission spectroscopy [23], depolarized dynamic light scattering [24], SAXS [25], or SANS [26] enables to extract hydrodynamic properties of the carrier medium.

Magnetic fluids consist of magnetic particles suspended in a non-magnetic carrier liquid. With the assistance of a magnetic field, the dynamics and hence the flow properties of the dispersion can be tuned. The fluid-mechanical properties are determined by the particle orientation and the potential creation of clusters, where the interparticle arrangement is governed by the competition of attractive magnetic dipolar and disruptive shear forces. The knowledge of such flowand field-induced microstructural changes is important to understand the origin of the magnetorheological properties, including the magnetoviscous effect and shear-thinning and shear-thickening behaviors.

For dilute ferrofluids consisting of spherical particles, the magnetoviscous effect is understood as the field-induced hindrance of the free particle rotation in a shear flow leading to a small increase in viscosity [27]. This effect is enhanced for dilute, elongated nanoparticles in the liquid carrier. In the absence of magnetic field and neglecting Brownian thermal fluctuations, the motion of spheroidal particles in shear flow was solved analytically by Jeffery [28]. Particles suspended in a viscous fluid rotate about the flow vorticity vector. In shear



flow, prolate spheroids will tumble and in the absence of inertial effects the rotation will follow so-called Jeffery orbits.

When a magnetic field is applied, anisometric magnetic nanoparticles align with their magnetic easy axis along the field [29–36]. If the long nanoparticle axis aligns perpendicular to the flow direction, the aligned nanoparticles oppose resistance to the flow resulting in an increase fluid viscosity. In contrast to common ferromagnetic nanorods, the easy magnetic axis of hematite spindles lies in the basal plane (i.e., the equatorial direction) such that the particles typically orient with their long axis perpendicular to an applied field [30, 32–34] with the peculiar results that a negative magnetorheological effect is observed in a magnetic field oriented perpendicular to the shear direction [37]. Hence, the application of magnetic field allows either enhancing alignment or overcoming shear alignment of magnetic fibers during sheardominated processing techniques [38].

With increasing particle volume fraction, enhanced magnetic dipolar interparticle interactions may lead to nanoparticle arrangements, e.g., chains, rings, and hexagonal columns as observed by small-angle scattering [39, 40]. In modest magnetic fields, the (reversible) formation of superstructures gives eventually rise to a significant increase of the viscosity by several orders of magnitude [41]. This effect is based on the magnetic field-induced alignment of the superstructures perpendicular to the flow direction [42]. These superstructures collapse already at moderate shear rates, which is the cause of the commonly observed shear-thinning behavior.

These examples illustrate that the viscosity reflects an adaption in the microstructure, superstructure formation, or particle reorientation, demonstrating the importance to observe in situ microstructural changes in the dispersion under magnetic and flow fields to find correlation with the fluid-mechanical response.

Small-angle scattering techniques using X-ray and neutron radiation are versatile tools to obtain information on microstructural modifications on the nanometer length scale. Nowadays, rheometers are standard sample environments to investigate flow-induced effects on the mesoscopic scale from 1 to several hundred nanometers using small-angle scattering [43–54]. However, the combination of magnetic field and shear flow for small-angle neutron scattering is rare [53–57].

Here we present first results of a specialized sample environment for in situ MagnetoRheoSANS that is available to the wide scientific community through the user program at the Institut Laue-Langevin (ILL). It consists of an Anton Paar rheometer MCR501, which exists at the Institut Laue-Langevin to perform rheological experiments together with simultaneous SANS, and a custom made shielded magnetic coil set, which provides a static magnetic field of up to 20 mT. This setup allows investigating the structure and magnetic configuration within a ferrofluid under magnetic field and shear flows providing information on the connection between

rheological properties and the underlying microstructural response on complex magnetic fluids. As a proof of concept, MagnetoRheoSANS data of hematite nanospindles are presented.

Materials and methods

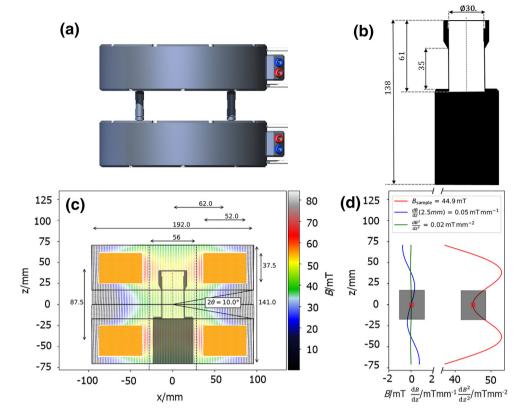
A set of Helmholtz coils was constructed to fit the existing Anton Paar rheometer MCR501 and provide a homogeneous magnetic field in the sample volume, perpendicular to the shear direction. The coil set has an outer diameter of 192 mm. The coils are made of copper wire with a diameter of 1.48 mm and 820 windings each, generating a practically usable maximum field of 20 mT in the center of the setup (Fig. 1). According to simulations (Fig. 1c-d), the field homogeneity at the sample position in the rheology cup is expected better than 0.3% over the SANS measurement position (5-mm height, red box in Fig. 1d) and better than 6% for the rheology measurement gap region (35-mm height, gray box in Fig. 1d). With a distance of 141 mm between the top and bottom of the Helmholtz coil set, an optical free distance of 35 mm in height allows for a maximum scattering angle of $2\theta = 10^{\circ}$. The coils can be cooled by water, ethylene glycol, or nitrogen stream in order to maintain a stable temperature during the measurement. A cup for Mooney Ewart rheological geometry has been specially constructed by Anton Paar made of titanium with an extended socket of 60 mm in height (Fig. 1b). The bottom of the socket is 54 mm wide and fits in the center of the magnetic coils. The measurement part has a diameter of 30 mm and a height of 35 mm, such that the measurement gap is situated in the homogeneous magnetic field between the two coils, indicated in Fig. 1c, d. Soft magnetic iron plates shield the rheometer drive against the stray field of the coils. For a bob diameter of 29 mm the shear gap of 0.5 mm, corresponding to a neutron path length of 1 mm in transmission geometry, requires a sample volume of 2.6 mL.

A practically usable maximal magnetic field of 20 mT was achieved at the position of the sample in the neutron beam, whereas for higher magnetic fields, we observed significant heat dissipation from the magnetic coils. Experiments using a higher field of 30 mT led to an increase of the temperature by 4 degrees (measured at the temperature sensor at the coils) within 15 min of operation, accompanied by an increased coil resistance. Whereas the sample temperature in the rheology cup may in principle be stabilized using a dried air stream (not implemented in our experiment), the increasing coil resistance will have a direct impact on the generated magnetic field. Therefore, a maximal, reliable applied field of 20 mT is recommended for our setup. The specifications of the magnetic coil set are summarized in Table 1.

As test sample, we used spindle-shaped hematite nanoparticles presented and precharacterized recently [30]. The



Fig. 1 a Design of the Helmholtz coils with $\bf b$ a technical sketch of the measurement cup and $\bf c$ - $\bf d$ simulation of the magnetic field homogeneity. Data in (d) represent the local field homogeneity at the sample position in the cup at x = 15 mm (compare with (c)) with the black and red rectangles indicating the cup and beam dimensions, respectively



known and well-defined orientation behavior in applied magnetic field makes them a suitable model sample for our MagnetoRheoSANS setup. In brief, hematite nanospindles

Table 1 Technical parameters of the Helmholtz coils used for MagnetoRheoSANS

Dimensions	
Height (mm)	141
Outer diameter (mm)	192
Inner diameter (mm)	56
Optical free distance (mm)	35
Wire diameter (mm)	1.48
Maximum scattering angle 20 (°)	10
Magnetic field	
Maximal magnetic field (mT)*	20
Field homogeneity (%)	< 6
Technical parameters of cup	
Total height (mm)	138
Height of socket (mm)	60
Diameter of the socket (mm)	54
Optically free path (mm)	35
Inner diameter (mm)	30
Bob diameter (mm)	28/29**

^{*}Where field stability is not affected by energy dissipation

were synthesized by the hydrolysis technique according to Matijević and co-workers [58]. The nanospindles are characterized by a particle length of 375(14) nm and an equatorial diameter of 56(2) nm with a lognormal size distribution in both dimensions of σ_{log} = 19%, as well as an aspect ratio of 6.7(1) [30]. The integral moment of the particle determined by magnetometry is $\mu = 6.6(1) \cdot 10^{-19} \,\mathrm{J}\,\mathrm{T}^{-1}$, equivalent to 7.1(1) $10^4 \,\mu_B$ with a spontaneous magnetization of $\sigma_S = 1.566(1) \,\mathrm{kA}$ m⁻¹. The spindles have a magnetic volume of $V_{\rm mag} = \mu/\sigma_{\rm S} =$ $4.2(1) \cdot 10^{-22}$ m³, which is slightly smaller than the structural particle volume of $V_{TEM} = 5.0(3) \cdot 10^{-22} \text{ m}^3$. For MagnetoRheoSANS experiments, the nanospindles were dispersed in water with a concentration of 3 vol%. The low concentration was chosen in order to minimize the magnetic field effect on the rheological properties of the sample and to show the individual effects of field- and shear-induced nanoparticle orientations.

The first MagnetoRheoSANS experiment using the setup was conducted at D22 instrument at ILL, Grenoble, France [59]. SANS experiments were performed with a neutron wavelength of 6 Å and a sample-to-detector distance of 17.6 m with symmetrical collimation setting. The Anton Paar MCR501 rheometer together with the Helmholtz coils was installed at the sample position (Fig. 2). The measurements were done in Mooney Ewart geometry, applying vertical magnetic fields of 0–20 mT strength and shear rates increasing stepwise from 0 to 600 s⁻¹ using the rotational mode of the rheometer. The applied magnetic field is parallel to the



^{**}In our experiment, a bob with 29 mm diameter was used

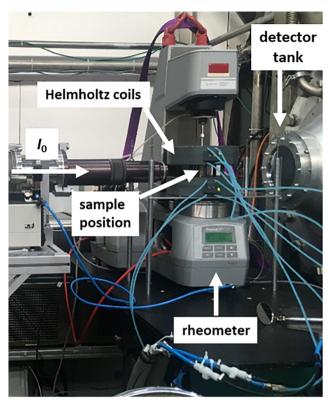


Fig. 2 MagnetoRheoSANS setup at D22 instrument at ILL

rotation axis of the rheometer head. To reach a steady state, the sample was equilibrated for 90 s at the given shear rate before the shear viscosity and the scattering pattern were recorded using nonpolarized SANS over an exposure time of 10 min. The SANS data were corrected to the transmission, blocked beam, and background of the solvent and empty cup and converted into absolute scale using Grasp [60]. The dependence of the intensity on the azimuthal angle was extracted over a momentum transfer range of $Q = 0.019-0.026 \,\text{\AA}^{-1}$.

Results and discussion

In radial beam configuration with the incident beam parallel to the flow velocity gradient, we observe the shear flow- and magnetic field-induced order-disorder transitions of spindle-shaped hematite nanoparticles. The 2D SANS scattering patterns (Figs. 3 and 4) change from an isotropic, circular shape in the absence of magnetic field and shear flow, indicating random orientation of the particles, to a vertically elongated pattern under strong enough fields or shear rates. The magnetic field-dependent SANS in the absence of shear flow is presented in Fig. 3a. In general, a magnetic scattering contribution arising from the nanoparticle magnetization is accessible using magnetic SANS [61]. In the case of the only very weakly ferromagnetic hematite nanospindles, however, the magnetic signal is too small to be detectable by our nonpolarized

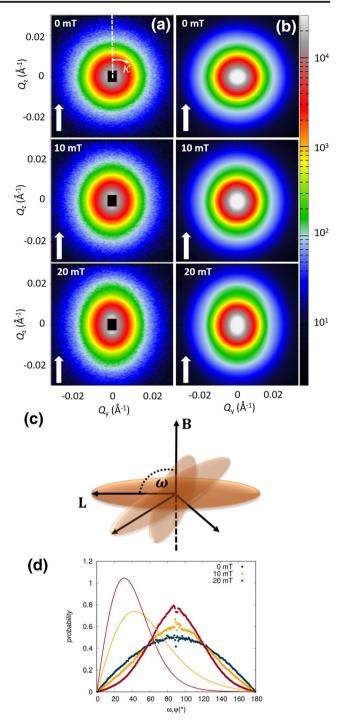


Fig. 3 a 2D scattering cross sections of 3 vol% of hematite nanospindles under various applied magnetic fields (white arrow indicating the magnetic field direction) and **b** simulated 2D scattering cross sections of rotational ellipsoid. **c** Sketch of an oriented ellipsoid with length **L** free to rotate in the plane perpendicular to the field direction **B**. **d** Orientation distribution of the easy axis (ψ , lines) and the resulting orientation distribution of the long spindle axes **L** (ω , points) towards the applied magnetic field. Noise observed near $\omega = 90^{\circ}$ results from numerical artifacts

setup and is therefore disregarded in this study. The elongation of the scattering cross section in the field direction indicates the preferred orientation of the nanospindles perpendicular to



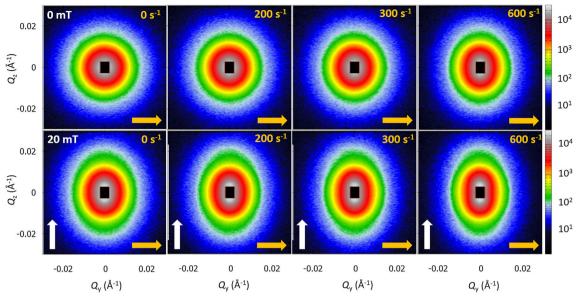


Fig. 4 Evolution of the anisometric 2D scattering at different applied shear rates in applied magnetic fields of 0 mT (top row) and 20 mT (bottom row). Direction and value of shear rates and magnetic field are indicated in orange and white color, respectively

the applied magnetic field. This is in line with our previous studies [30] and is expected as hematite nanospindles are known to bear their magnetic easy axis in the equatorial direction and therefore orient with their principal axis perpendicular to any applied field. If only a magnetic field is applied, the orientation within the normal plane is expected isotropic. Simulations of the field-dependent 2D scattering cross section according to an ellipsoidal form factor with orientation distribution given by Boltzmann statistics [30] are displayed for comparison in Fig. 3b. For the simulation, all morphological (radius, length, and size distribution of length) and magnetic parameters (magnetic particle moment) were fixed as given by the precharacterization. A magnetic field of 20 mT is far below a nominal saturation field, and from magnetization measurements, an average orientation of the magnetic easy axis of $\psi = 46.3^{\circ}$ toward the applied magnetic field is expected according to the Langevin function $\mathcal{L}(\xi) = \langle \cos \psi \rangle$ with the Langevin parameter $\xi = \frac{\mu \mu_0 H}{k_{\rm B} T} = 3.1992$. As a result, the orientation of the long spindle axes is distributed fairly broad

around the horizontal plane perpendicular to the field direction ($\omega = 90^{\circ}$, Fig. 3d). The excellent agreement between the measured data and simulations confirms that the coil set provides a homogeneous magnetic field, suitable for SANS measurements in combined magnetic field and shear flow.

In shear flow, an anisometric particle in dispersion rotates and tumbles as it travels in the suspending medium, and in the steady state, a preferred orientation will develop giving rise to scattering anisotropy. Zero-field SANS measurements performed in shear flow reveal increasing scattering anisotropy perpendicular to the shear direction (Fig. 4, top). This feature is attributed to the continuous alignment of the long particle axis in the direction of shear flow.

The application of either magnetic field or shear flow has a very similar effect on the 2D scattering anisotropy, illustrating that the short nanospindle dimension preferentially orients along the vertical direction for both cases. For simultaneous application of flow and magnetic field, an enhanced scattering anisotropy is observed with shear rate, exceeding the

Fig. 5 Field- and shear-dependent azimuthal scattering intensity in a Q range of 0.019–0.026 Å⁻¹. **a** Field-dependence without applied shear. **b** Shear-dependence in zero magnetic field. **c** Shear-dependence in 20 mT applied field

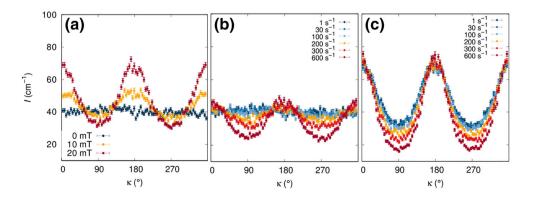
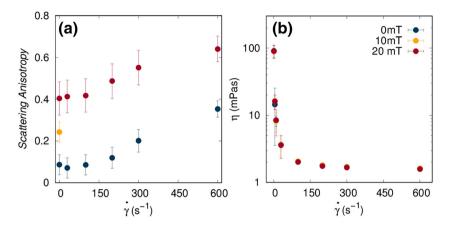




Fig. 6 a Field- and sheardependent scattering anisotropy parameters as extracted from Fig. 5a-c. b Simultaneously measured shear viscosity of the 3 vol% nanospindles dispersion in water depending on the applied magnetic field



scattering anisotropy observed for field or flow only. The vertical elongation of the scattering cross section is hardly affected, whereas the scattering intensity shifts to lower Q in the horizontal direction indicating a further alignment of the nanospindles (Fig. 4, bottom).

The variation of the scattering intensity with azimuthal angle κ illustrates the evolution of the scattering anisotropy with magnetic field and shear flow (Fig. 5). The clearly different effect of magnetic field and shear flow on the scattering anisotropy results from the different orientation behavior induced. Whereas the vertical magnetic field accumulates the spindles in the horizontal plane, the shear deformation takes place mainly within the horizontal plane and aligns the particles with the horizontal shear flow direction. To quantify the scattering anisotropy from the scattering pattern, we determine the anisotropy factor by

$$A(Q) = \frac{I(Q, 90^{\circ}) - I(Q, 180^{\circ})}{I(Q, 90^{\circ}) + I(Q, 180^{\circ})},$$

which varies from A(Q) = 0 for isotropic orientation to A(Q) = 01 for complete alignment of the major axis perpendicular to the magnetic field direction. The anisotropy factor of the SANS pattern increases with magnetic field as well as shear rate (Fig. 6a). Variation of the shear rate for different applied magnetic fields (0 mT and 20 mT shown here) leads to a very similar slope of the scattering anisotropy, suggesting a nearly field-independent effect of shear flow on the particle alignment. This is reasonable considering that the modest magnetic field is sufficiently far from saturating the sample and the magnetic torque and the shear flow torque act independently on the particle. Whereas the spindle orientation in the horizontal plane is isotropic in applied magnetic field, shear flow directs the particle orientation into the shear direction and therefore additionally acts on the orientation distribution within the horizontal plane.

The shear viscosity measured simultaneously to the SANS experiment is presented in Fig. 6b. In contrast to the SANS experiment, it does not exhibit a significant magnetic field dependence. A shear thinning effect is observed for small

shear rates that might be related to initial orientation of the spindles in the dilute dispersion. With increasing shear rate, only the behavior of the solvent contributes to the viscosity. This observation is in line with expectations for a dilute nanospindle dispersion far below the critical interaction concentration, where field- and shear-induced orientations of the nanoparticles have no significant effect on the shear viscosity. The absence of a visible magnetic field effect confirms in this case the successful shielding of the rheometer against the imposed magnetic field. At the same time, SANS is very sensitive to the nanoparticle orientation even if a rheological effect is absent.

The combination of rheology in applied magnetic field and SANS to MagnetoRheoSANS thus gives access to clearly distinguishable effects of magnetic field and shear flow on the nanoparticle orientation behavior. A more detailed, quantitative description will require in-depth simulation and modeling of the field- and shear flow-induced orientation distributions, which is beyond the scope of this paper.

Conclusion

Small-angle scattering is a valuable tool for studying flowing systems of dispersed nanoparticles to reveal the collective orientation distribution of particles and the relation between microscopic organization and macroscopic rheological properties. In this work, a magnetorheology setup available for SANS is presented, which extends the available RheoSANS suite at the ILL toward the application of magnetic field and gives the opportunity of polarized neutron scattering. Measurements in radial and tangential scattering geometry through the rheology setup allow reconstructing the 3D orientational distribution and intraparticle arrangement. It opens the opportunity to investigate the magnetic field- and flowinduced structure formations, and hence the microscopic origin of magnetoviscous effects in magnetically functionalized soft matter systems. The sample environment is available for the user community of ILL and is of interest for the study of



complex magnetic fluids like magnetic gels, elastomers, and ferromagnetic liquid crystals.

As a model system, the alignment of anisometric particles within the fluid under the influence of shear and magnetic field is presented. A detailed determination of the order parameter and the use of a dedicated particle model in the future will be necessary for a quantitative description of the particle orientation dynamics under combined shear and magnetic field.

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Availability of data The SANS data is stored and will be available based on the ILL data policy (https://doi.ill.fr/10.5291/ILL-DATA.5-32-785).

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Compliance with ethical standards

Conflict of interest The authors declare that they have no conflict of interest.

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