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Effects of Sensorimotor Training Volume on Sensorimotor Function in Patients Following Lower Limb Arthroplasty

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1 **Background:** Sensorimotor function is degraded in patients after lower limb
2 arthroplasty. Sensorimotor training is thought to improve sensorimotor skills,
3 however, the optimal training stimulus with regard to volume, frequency, duration,
4 and intensity is still unknown. The aim of this study, therefore, was to firstly quantify
5 the progression of sensorimotor function after total hip (THA) or knee (TKA)
6 arthroplasty and, as second step, to evaluate effects of different sensorimotor
7 training volumes.

8 **Methods:** 58 in-patients during their rehabilitation after THA or TKA participated in
9 this prospective cohort study. Sensorimotor function was assessed using a test
10 battery including measures of stabilization capacity, static balance, proprioception,
11 and gait, along with a self-reported pain and function. All participants were randomly
12 assigned to one of three intervention groups performing sensorimotor training two,
13 four, or six times per week. Outcome measures were taken at three instances, at
14 baseline (pre), after 1.5 weeks (mid) and at the conclusion of the 3 week program
15 (post).

16 **Results:** All measurements showed significant improvements over time, with the
17 exception of proprioception and static balance during quiet bipedal stance which
18 showed no significant main effects for time or intervention. There was no significant
19 effect of sensorimotor training volume on any of the outcome measures.

20 **Conclusion:** We were able to quantify improvements in measures of dynamic, but
21 not static, sensorimotor function during the initial three weeks of rehabilitation
22 following TKA/THA. Although sensorimotor improvements were independent of the
23 training volume applied in the current study, long-term effects of sensorimotor

24 training volume need to be investigated to optimize training stimulus
25 recommendations.

26 **Clinical trial registration number:** DRKS00007894

27 **Key Words:** *balance, total knee replacement, total hip replacement, neuromuscular*
28 *training, proprioception, rehabilitation, dose-response*

29 INTRODUCTION

30 In the progression of osteoarthritis (OA), sensorimotor skills including proprioception
31 [1,2], static and dynamic balance [3], and neuromuscular control are known to
32 degrade in response to pain avoidance and advancing inactivity. These sensorimotor
33 deficiencies typically manifest as modified movement patterns and muscle weakness
34 [4,5] and have been shown to persist even after joint replacement. For instance,
35 Thewlis et al. [6] observed persistent asymmetric load distribution in TKA patients 6
36 months after surgery and Levinger et al. [2] described proprioceptive deficits that
37 remained for at least 12 months following TKA surgery. Similarly, Judd et al. [7]
38 observed sensorimotor deficits following THA, with both strength and functional
39 performance deficits persisting for at least one year after joint replacement.

40 Despite evidence that a full recovery of sensorimotor function is unlikely to occur
41 within twelve months of THA or TKA [8], there is emerging evidence that
42 sensorimotor function can be improved through dedicated sensorimotor training. For
43 instance, Zech et al. [9] found that sensorimotor training improved dynamic balance
44 in ankle sprain patients and resulted in a faster activation of hamstring muscles after
45 a sudden perturbation of stance in patients with anterior cruciate ligament rupture.
46 Similarly, sensorimotor training has been shown to produce positive effects on the
47 response of hip OA and THA patients to sudden displacements [10], improve walking
48 time and reduce knee reposition error in knee OA patients compared to strength
49 training [11].

50 Along with muscular strengthening, joint flexibility training, and pain management,
51 sensorimotor training has now become an integral part of rehabilitation guidelines
52 following THA and TKA. However, evidence-based recommendations for

53 sensorimotor training, particularly in post-operative rehabilitation programs, are
54 currently lacking. Current guidelines are based mainly on anecdotal evidence and
55 practical experience. Empirical evidence regarding the optimal sensorimotor training
56 dose and the effects of training volume, frequency, duration, and intensity are still to
57 be explored [1,12–14].

58 The first purpose of the current study, therefore, was to quantify the progression of
59 sensorimotor function during inpatient rehabilitation after THA and TKA. The second
60 purpose was to evaluate the effects of sensorimotor training volume on sensorimotor
61 function. We hypothesized that higher sensorimotor training volumes would improve
62 sensorimotor function to a larger extent than lower training volumes.

63

64 **METHODS**

65 **Participants**

66 Sixty-three consecutive patients presenting to an inpatient orthopaedic rehabilitation
67 clinic (Medical Park St. Hubertus, Bad Wiessee, Germany) following TKA or THA to
68 address unilateral joint disease were approached to participate in the study. Three
69 patients declined to participate and two failed to meet the study inclusion criteria,
70 which required patients to possess a minimum knee mobility of 85°/30°/0° (neutral
71 zero method: flexion/extension) [15] and to be able to fully weight-bear without aid
72 for at least 30 seconds. Consequently, fifty-eight (29 males, 29 females) patients
73 with unilateral TKA (n=21) or THA (n=37) participated in this study (**Table 1**). All
74 patients were otherwise healthy and free of gross orthopaedic conditions of the lower
75 limbs. Patients were randomly assigned to one of three groups, which differed only in

76 the volume of sensorimotor training: two sessions per week (n=20), four sessions per
77 week (n=15) and six sessions per week (n=23). Base-line (pre-training)
78 measurements took place 13.5 ± 2.8 days, on average, after surgery. All patients
79 provided written informed consent, following a verbal and written explanation of the
80 study procedures which were approved by the local ethics committee.

81

82 **Intervention**

83 All patients underwent three weeks of a standard rehabilitation protocol, which
84 included exercise training, physical therapy, seminars, and educational group
85 therapy. Within the standard rehabilitation protocol, patients also received a
86 sensorimotor training program that included supervised exercise sessions involving
87 three different therapeutic devices: (1) a balance pad (Balance Pad, Airex,
88 Germany), (2) a ball cushion (Aero-Step® XL, Togu, Germany), and (3) a Proprio-
89 Swing-System (systemreha GmbH & CO. KG, Germany). On each device, all
90 sensorimotor exercises were conducted during quiet bipedal stance but the level of
91 difficulty progressed from an 'eyes open' condition in the first week, through a
92 'forward and backward leaning' condition (within self-perceived limits of balance)
93 during the second week and concluded with an 'eyes closed' condition in the third
94 week. Sensorimotor exercises were undertaken for thirty seconds on each device,
95 and were repeated six times within each training session. A thirty second rest period
96 was provided between repetitions. Thus, in total, each sensorimotor training session
97 lasted approximately 18 minutes including rest periods. In the regular rehabilitation
98 protocol, the sensorimotor training session was scheduled six times per week. For

99 this study three groups were established by adjusting the training volume from six, to
100 four, and two sensorimotor training sessions per week.

101 **Procedure**

102 Self-reported pain and function along with measures of stabilization capacity,
103 static balance, proprioception and gait analysis were used as primary outcome
104 measures. Outcome measures were taken at baseline (pre), and repeated after 1.5
105 weeks (mid) and at the conclusion of the 3 week program (post).

106 *Gait Analysis*

107 Preferred over-ground walking speed was determined over a distance of 13
108 meters [16] using two double light barriers (TDS lightbarriers, Werthner Sport
109 Consulting KG, Austria). Step length was measured over the central 5 meters of the
110 walkway using an OptoGait System (OptoGait, Microgate, Italy) with a spatial
111 resolution of 1.04 cm and a sampling frequency of 1000 Hz. In the event, that a
112 patient was unable to walk without walkers, step length was not measured.

113 *Stabilization capacity*

114 Stabilization capacity was measured during bipedal stance on an oscillatory
115 platform (Postuomed, Haider Bioswing, Germany) [10] that incorporated a
116 provocation unit and a MicroSwing measuring system (three-dimensional
117 acceleration sensor, Haider Bioswing, Germany). The provocation unit allowed for
118 the precise displacement, fixation and the controlled release of the oscillatory
119 platform. Patients were thereby exposed to a standardized horizontal unidirectional
120 oscillatory stimulus and instructed to dampen the movement of the platform as
121 quickly as possible to return to quite standing. Acceleration of the platform was

122 measured over ten seconds and the procedure was repeated three times, with
123 oscillations independently induced in both the medio-lateral and anterior-posterior
124 directions. Proprietary software was subsequently used to calculate the stability
125 index for each trial. The dimensionless index, which reflects the patient's capacity to
126 stabilize the oscillatory platform, ranged from 0 to 1000 with higher scores
127 representing higher stabilization capacity. Average stability indices were calculated
128 from the three trials undertaken in each direction to give rise to each patients'
129 anterior-posterior and medio-lateral stabilization capacity.

130 *Static balance*

131 Static balance was assessed using previously published methods[17]. In brief,
132 displacement of the centre of pressure was recorded while patients stood as still as
133 possible on a pressure platform (footscan® USB plate, RSscan International,
134 Belgium) under four sequential experimental conditions; (1) bipedal stance with eyes
135 open, (2) bipedal stance with eyes closed, (3) semi-tandem stance with the operated
136 leg positioned anteriorly, and (4) semi-tandem stance with the operated leg
137 positioned posteriorly. Balance data for each experimental condition were collected
138 for 20 seconds at a sampling rate of 43.3 Hz [3]. For each trial, the root mean square
139 (RMS) of the displacement of the centre of pressure (COP) was calculated in both
140 the medio-lateral and anterior-posterior directions and used in subsequent analysis.

141 *Proprioception*

142 Knee joint proprioception was assessed using the passive-active angle-
143 reproduction test [18], conducted at target angles of 40° and 60° of knee flexion.
144 Patients were seated on a height adjustable therapy chair with the knee of the
145 operated leg positioned at 90 degrees of flexion. The foot was positioned on a low

146 friction linear bearing, so that active and passive movement of the knee could be
147 accomplished with minimal effort. A digital goniometer (accuracy: 0.1°, digital angle
148 rule 200mm, Trend, United Kingdom) was attached to the lateral aspect of the knee
149 using Velcro straps with the angular point device positioned over the estimated joint
150 centre. Patients were instructed to close their eyes throughout proprioception
151 measurement. From the initial position of 90 degrees of flexion, the knee was then
152 passively moved to a target angle of either 40 or 60 degrees. The target angle was
153 maintained for four seconds before the knee was passively returned to the initial
154 position. Patients were then requested to actively move their leg to reproduce the
155 target angle. The absolute difference between the actively reproduced angle and the
156 target angle was subsequently calculated and used for further analysis.

157 *Functional Assessment*

158 The German adaptation of the Lequesne Algofunctional Questionnaire[19] was used
159 to assess self-perceived functional impairment, stiffness, and pain during activities of
160 daily living. The questionnaire consisted of 11 items analysing pain (5 items),
161 maximum walking distance (2 items) and activities of daily living (4 items). Scores
162 can range from 0 to 24 and were subclassified according to the criteria of Nilsdoter,
163 where a score of 0 represents “no handicap”, 1 – 4 reflects “mild handicap”, 5 - 7
164 represents “moderate handicap”, 8 – 10 reflects “severe handicap”, 11 – 13
165 represents “very severe handicap”, and a score ≥ 14 indicates an “extremely severe
166 handicap” [20]. The questionnaire takes approximately two minutes, on average, to
167 complete and has been shown to have good acceptance among patients [19]. The
168 use of pain-modifying medication was recorded as a dichotomous variable prior to
169 each measurement.

170 *Statistical Analysis*

171 The Statistical Package for the Social Sciences (version 21, IBM, USA) was used for
172 all statistical procedures. Kolmogorov–Smirnov tests were used to evaluate data for
173 underlying assumptions of normality. Outcome variables were determined to be
174 normally distributed, and consequently means and standard deviations have been
175 used as summary statistics. Between–group differences in age and body
176 anthropometry were investigated using one-way analysis of variance (ANOVA). The
177 effect of time (pre, mid, post) and training volume (2, 4 or 6 sessions per week) on
178 measures of static balance, proprioception and basic gait parameters were
179 evaluated using two–way repeated measures ANOVA in which time (pre, mid, post)
180 was treated as a within–subject factor. Significant effects for time were evaluated
181 using *post hoc* paired t-tests. Partial effect size (η_p^2) was calculated as an estimate of
182 effect size. An alpha level of .05 was used for all univariate tests of significance.

183

184 **RESULTS**

185 One-way ANOVA demonstrated no difference between the three groups with respect
186 to age, height and body weight at baseline (**Table 1**).

187 *Gait Analysis*

188 Walking velocity significantly increased over time ($p < .001$; $\eta_p^2 = .670$), but did not
189 differ between training volumes ($p = .481$) (**Figure 1**). Similarly, step length
190 increased in the operated ($p < .001$, $\eta_p^2 = 0.549$) and non-operated leg ($p < .001$, $\eta_p^2 =$
191 0.630) over time, but was not significantly different between training volumes
192 (operated leg, $p = .497$; not operated leg, $p = .559$).

193 *Stabilization Capacity*

194 Although the stability index significantly increased over time in both the anterior-
195 posterior ($p < .001$, $\eta_p^2 = 0.184$) and medio-lateral ($p < .001$, $\eta_p^2 = 0.203$) directions
196 (**Figure 2**), there was no significant difference between training volumes (anterior-
197 posterior $p = .942$; medio-lateral $p = .845$).

198 *Static Balance*

199 There were no significant main effects of time or training volume on two of the
200 four static balance conditions. There was a non-systematic though significant
201 interaction between time and training volume in the RMS of the anterior-posterior
202 displacement of the COP during the eyes closed condition ($p = .033$; $\eta_p^2 = 0.093$,
203 **Figure 3**). In semi-tandem stance conditions, the RMS decreased significantly over
204 time in both the anterior-posterior and medio-lateral directions when the operated leg
205 was positioned anteriorly (anterior-posterior: $p = .003$, $\eta_p^2 = 0.119$; medio-lateral: $p =$
206 $.03$, $\eta_p^2 = 0.074$) but decreased only in the anterior-posterior direction when the
207 operated leg was positioned behind the non-operated leg ($p = .009$, $\eta_p^2 = 0.011$,
208 **Figure 4**).

209 *Proprioception*

210 There was no significant difference in the angle reproduction test at either
211 target angle over time or between training volumes (**Figure 5**).

212 *Functional Assessment*

213 Self-reported function scores improved significantly over time ($p < .001$, $\eta_p^2 =$
214 0.584) but did not differ between training volumes ($p = .458$) (**Figure 6**).

215

216

217 **DISCUSSION**

218 The first purpose of the study was to quantify the progression of sensorimotor
219 function during inpatient rehabilitation using a test battery that included static and
220 dynamic measures of sensorimotor function. We could observe improvements in gait
221 parameters, postural stability and in self-reported function during the three week
222 period of early recovery in THA and TKA patients. The improvements in walking
223 velocity (for all groups $\Delta_{T3-T1} > +0.25$ m/s) are considered to reflect a clinically
224 meaningful change [21].

225 We observed significant improvements in stabilization capacity over the three week
226 rehabilitation period. As sensorimotor training is known to improve the reaction of
227 individuals to sudden disturbances of the support surface [10], we attribute a major
228 contribution to the improved stabilization capacity of our patients to sensorimotor
229 training but recognise potential time or learning effects may also play a role. While
230 our results are consistent with those reported by Boer et al. [22], we evaluated
231 stabilization capacity during bipedal, rather than unipedal, stance since the majority
232 of participants in our study were unable to stand on one leg without aid.

233 In contrast to the improvements in stabilization capacity, static balance improved
234 only in the more challenging semi-tandem stance conditions (operated leg in front or
235 behind). While the present experimental setup did not allow for a mechanistic
236 explanation as to why control of quiet bipedal stance did not improve during
237 rehabilitation periods, asymmetric load distribution is known to increase COP

238 displacement during quiet stance and has been shown persist in TKA patients for at
239 least six months following surgery [6,23]. In light of the magnitude of load asymmetry
240 that occurs following THA [24], however, this effect is likely too low to explain the
241 impairment in postural control observed in the current study [25]. Thus, our findings
242 suggest that recovery of normal bipedal stance control is not improved with
243 sensorimotor training and likely needs substantial time for recovery to occur, if at all.
244 Semi-tandem stance conditions cause between 258% to 319% (anterior-posterior)
245 and 350% to 355 % (medio-lateral) more postural sway as compared to bipedal
246 stance with open eyes at baseline. It remains questionable, whether improvements
247 in these more challenging balance conditions are achieved through improved intra-
248 and inter-muscular coordination or better sensorimotor control in general.

249 Proprioception, as defined by the angle reproduction measurement, showed no
250 significant changes in any group over time. A trend towards an improvement can be
251 seen at a target angle of 60°, however this was not statistically significant. For most
252 of the TKA patients, particularly at baseline, replication of the 40° target angle was
253 close to the upper limit of the available range of motion of the knee and was often
254 coupled with pain. Thus, pain may have confounded measurements of
255 proprioception in the current study and may also, in part, account for the inconsistent
256 findings reported elsewhere in the recovery of joint-position sense in THA and TKA
257 patients following surgery [26, 28]. While improvements have been reported by some
258 studies following TKA [26], others have observed persistent deficits for up to twelve
259 months following TKA [8].

260 The second purpose of the study was to evaluate the effects of sensorimotor training
261 volume on sensorimotor function. In contrast to our hypothesis, we found that
262 decreasing the training volume of sensorimotor training to fewer than six sessions

263 per week had no significant effect on sensorimotor function in our cohort. There are
264 several possible explanations for this observation.

265 First, it is possible that the sensorimotor training program may not affect the recovery
266 of sensorimotor function during in-patient rehabilitation. However, other studies have
267 shown that sensorimotor function improves with sensorimotor training during
268 recovery from ankle sprain [9], following anterior cruciate ligament rupture [9], with
269 knee osteoarthritis [27], TKA [13], and following THA [10].

270 Second, the training volume employed in the current study may not have been
271 sufficient to induce neuromuscular adaptation. In the absence of recommendations
272 on the intensity of sensorimotor training, however, the duration of the training
273 program employed in the current study was designed to fall within the range that has
274 been previously shown to have beneficial effects [28,29].

275 Finally, while there is some evidence that increasing training to more than one
276 session per week invokes additional sensorimotor benefit [29], it is possible that
277 there is a ceiling effect, in which there is no additional benefit beyond two
278 sensorimotor training sessions per week. It remains to be shown whether, in the
279 course of further rehabilitation of THA or TKA, a higher training frequency leads to
280 greater improvement in sensorimotor function.

281 This study has several limitations which should be considered when interpreting the
282 results. First, pain sensation is known to influence proprioception [30], and by the
283 patients' general pain sensitivity, surgical outcome, and level of pain medication.
284 During the course of our study, pain medication was reduced progressively on an
285 individual basis, and hence might have influenced the sensorimotor function at
286 different time points. Evidence of an effect of pain on sensorimotor function,

287 however, is contradictory [30] and we observed no differences in the use of pain
288 medication between groups. Moreover, despite a reduction in self-reported pain in
289 our cohort over time, we observed no significant change in proprioception
290 performance. Second, repeated measurements carry the risk of potential learning
291 effects. To keep potential learning effects to a minimum, patients were exposed to
292 the measurement devices for as short as possible and were not permitted to use the
293 devices between measurements. Finally, there may be a temporal delay in the
294 effects of training on sensorimotor performance. Previous research, however, has
295 shown improvements in dynamic balance tasks and structural reorganization of grey
296 and white matter after as little as two 45-minute training session within two weeks
297 [31]. Despite these limitations, we believe this study provides clinically relevant
298 insights into the progress of sensorimotor function and the effects of sensorimotor
299 training volume during the early recovery following total hip or knee arthroplasty.
300 Further research investigating potential differential effects of sensorimotor training on
301 TKA and THA patients over a longer duration of recovery is warranted.

302

303 **Conclusion**

304 We were able to quantify improvements in measures of dynamic, but not static,
305 sensorimotor function during the initial three weeks of recovery from TKA or THA.
306 Sensorimotor improvements were independent of sensorimotor training volume, as
307 sensorimotor performance did not differ with weekly training volumes of two, four or
308 six sessions. Thus, in contrast to common clinical practise, greater volume of
309 sensorimotor training during rehabilitation does not necessarily lead to better
310 sensorimotor function. Further research investigating the effect of training volume

311 and its long-term effects are needed, however, before definitive recommendations
312 regarding optimal training stimulus (magnitude, frequency, duration) can be
313 formulated.

314 **Competing interests**

315 The authors declare that they have no competing interests.

316 **Author's contributions**

317 TP, TB, KS and TH designed the study. TP and TB developed the study protocol
318 methods and were responsible for statistical analyses. KS and TH reviewed the
319 study protocol methods and SW reviewed the statistical analyses. TP, KS and TH
320 were involved in participant recruitment. TP performed the measurements and
321 drafted the manuscript which was revised by TB and SW. All authors read and
322 approved the final manuscript.

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TABLES:**Table 1. Demographic data of the treatment groups**

Training volume	two sessions	four sessions	six sessions
n	20	15	23
Age (years)	63.3 ± 10.3	61.1 ± 9.7	57.5 ± 15.2
Height (cm)	171.6 ± 10.7	174.5 ± 10.3	172.5 ± 7.5
Weight (kg)	79.2 ± 16.2	82.5 ± 18.8	86.4 ± 16.8
Days post op (days)	14.0 ± 2.4	13.3 ± 2.1	13.2 ± 3.5
Male/Female (%)	50 / 50	60 / 40	44 / 56
TKA/THA (%)	40 / 60	27 / 73	39 / 61

Between-group analysis (ANOVA) showed no significant differences ($p > .05$). TKA = total knee arthroplasty, THA = total hip arthroplasty