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Cell therapies in hypoparathyroidism

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Summary

Identification of a biocompatible i munch or ster ive membrane to prevent graft rejection re ha ne double' until the development of microcaperities trim lat double' until the developro parathyroid holds in the science of the s

KEY WORDS: parathyroid tissue, parathyroid cells, hypoparathyroidism, al ginate, cell therapies.

Introduction

Attempts to transplant parathyroid glands began almost a century ago, only two decades after the organ had been discovered, with the demonstration by histologic means that canine parathyroid autografts survived (1). Graft function was assessed only fifty years later, with the demonstration that parathyroid transplanted tissue in rodents functions sufficiently to maintain the host in a normocalcemic state (2). However, parathyroid allografts were successful only in immunosuppressed canine and human recipients (3,4).

Indications for parathyroid allotransplantation are rare, as hypoparathyroid patients who cannot be controlled on a medical regimen are also unusual. In these subjects the symptoms and associated complications of hypoparathyroidism cannot be controlled sufficiently with oral calcium and vitamin D. Due to these problems, alternate treatment modalities, involving more

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physiological and longer-acting systems for parathyroid hormone (PTH) delivery, needs to be pursued.

Various methods of immunomanipulation have been proposed to overcome allograft rejection, which include immunosuppression, immunomodulation and immunoisolation. By using the immunoisolation concept the transplant is enclosed in a biocompatible material to immobilize the transplant and at the same time preventing an immune response of the recipient. In 1964, T.M.S. Chang proposed the idea of using ultrathin polymer membrane microcapsules for the immunoprotection of transplanted tissues and cells (5). When implanted into rats, the microencapsulated pancreatic islets corrected the diabetic state for several weeks (6). Since then, bioencapsulation has provided a range of promising therapeutic treatments for diabetes, hemophilia, cancer and renal failure (7-10). In addition, the applicability of cell encapsulation in humans has also been reported in several clinical trials (11,12). Indeed, cell encapsulation in biocompatible and semipermeable polymeric memoranes as been an effective method for immunoprotect on, rehardly ss of the type of recipient (13), as encap ulated cells can maintain heir via ility while allowing or the sourcis or desired thera-teutic agents, eithe continious or in response to specific pnysiologic stil rulations.

Also or the treatment of refractory hypoparathyroidism, imn choic olated all geneic transplantation of parathyroid tissue is revared as a promising therapy concept (14), which has been uccessfully applied in iso-, allo-, and xeno-transplantations in animals by using purified alginates (15-17). Alternatively, isolated parathyroid cells are under investigation (18,19).

Up to now, a substantial challenge has been the lack of clinical grade polymers and the demanding task is to accomplish specific material requirements of high quality standards. By using homogeneous raw material and a standardized purification protocol a new class of clinical grade biopolymers was developed which establish the basis for the clinical application of encapsulation technology (20). The batches of the purified alginate have to be standardized as for the endotoxin, protein and phenolic content and also for the physical properties such as the distribution of the molar mass and the viscosity.

In the present study, we report *in vitro* data for the use of clinically suitable alginate-encapsulated human parathyroid tissue microspheres as a novel allo- and xeno-transplantation method for the delivery of PTH.

Materials and methods

Quality control of the biopolymer and cytotoxicity testing

Three different batches (a-c) of biocompatible alginate isolated from freshly collected *Laminaria pallida* (20) were tested in eight replicates, using three different cell lines (mouse, ape, human): L-929 (DSMZ # ACC 2), VERO-B4 (DSMZ ACC # 33) and NHDF (CellSystems, St. Katharinen, Germany). Experiments were repeated five times.

For cytotoxicity tests 100 μ l of cell suspensions were plated at a density of 2x10⁵ cells/ml in 96-well plates. Cells were incubated overnight in an incubator at 37°C in 5% CO₂/95% air hu-

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midified atmosphere. A 0.1% (w/v) suspension of the biopolymer was prepared in cell culture medium (RPMI 1640, supplemented with 2 mM L-glutamine and 10% fetal calf serum). Culture medium was used as negative control and CuSO₄ (50 ng/ml) in culture medium was used as positive control. Biopolymer suspension and control media were mixed overnight on an overhead shaker at room temperature. Cultured cells were checked for confluency and morphology after 24-hr incubation, when cell culture medium was removed and replaced by 100 µL of the biopolymer suspension. Positive and negative controls were tested in every dish. Cells were incubated for three days in the incubator. At day three 25 µL of Alamar-Blue solution (Biozol, Echingen, Germany) were added to each well and incubated. Fluorescence (excitation wavelength 535 nm, emission wavelength 590 nm) was measured after three hours. Metabolic activity of the cells was calculated versus baseline (negative controls) and expressed as percent difference.

Culture and encapsulation of human parathyroid tissue

Fresh human parathyroid tissue was obtained from six different patients undergoing surgery for parathyroid hyperplasia due to secondary hyperparathyroidism. Parathyroid tissue was transported to the laboratory under sterile conditions and then cut into fragments of about 2 mm³. Tissue particles were then kept either in RPMI 1640 medium supplemented with 2 mM L-glutamine and 10% AB-serum (17) or in serum-free culture medium in the incubator for three days with daily changes of culture medium. Thereafter, tissue particles were microencapsulated using the CellBeads[®] Biopolymer, produced according to GMP requirements (CellMed AG, Alzenau, Germany), through sus-pension in the biopolymer solution. The solution was or some through a spray nozzle and the resulting m croc psuk sides vere transferred into culture medium and with 3, cultured for .0 days.

In vitro release of PTH t or, h man en sapsulated pa at vroid tissue

In fact P Thiceles of was daily measured cuting a period varying from seven to eight day in Fo. the missurement of PTH release five microcapsul is were transferred from 5 mL of fresh serum-free meritions and incubated for two hours, when 500 μ I of the superimitant were included and immediately frozen at -20° C. After he wind human PTH 1-84 concentrations were measured by in ELISA method (DSL, Webster, USA) and the median F1H release of one capsule was derived.

Hematoxylin-eosin staining

At day seven encapsulated tissue particles were fixed in 4% formalin, Hematoxylin-Eosin (H&E) stained and histologically analyzed.

Results

Quality control of the biopolymer and cytotoxicity testing

The biopolymer used in this investigation expressed a whole set of quality control measures as it is produced under GMP conditions. The biopolymer was highly biocompatible, as demonstrated *in vitro* and *in vivo* (20). For each lot a whole set of quality controls was routinely performed, such as cytotoxicity testing in three different batches of the biopolymer using three different cell lines of diverse origin. No cytotoxic effect was observed for three different batches of the biopolymer using the three different cell lines (Fig. 1).

In vitro release of PTH from human encapsulated parathyroid tissue

The median intact PTH release per microcapsule was calculated over two hour period of incubation in serum-free medium using parathyroid tissue obtained from three different patients. At day one PTH release was below 500 pg/mL for all tissues with a constant increase in the following days (Fig. 2).

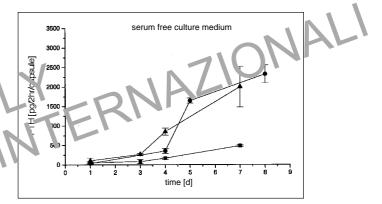


Figure 2 - PTH release from encapsulated human parathyroid tissue fragments obtained from three different donors. Intact PTH release over 2 hours of incubation in serum-free medium was evaluated for a period up to 8 days. The mean intact PTH release was elaborated from the release from 10 microcapsules and expressed as pg/2hr/capsule.

Histological examination

Microencapsulated human parathyroid tissue showed an excellent viability over 7/8 days in culture (Fig. 3).

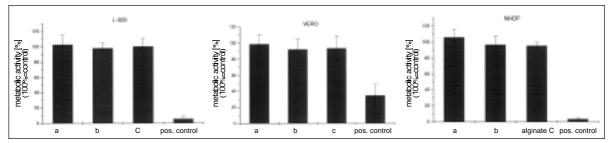


Figure 1. Cytotoxicity testing was performed for three biopolymer solutions (a-c) using three different cell lines (L-929, VERO, and NHDF). The metabolic activity of the cell lines is expressed as percentage on negative controls. The positive control (pos. control) is represented by RPMI 1640 culture medium containing 50 ng/mL CuSO₄.

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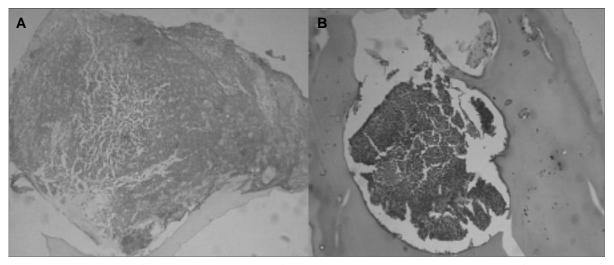


Figure 3 - Histological sections of encapsulated human parathyroid fragments. H&E staining showed a conserved morphology after 7 days in culture with serum-free culture medium.

Discussion

Secondary hypoparathyroidism with permanent hypocalcemia is a well recognized complication after thyroid surgery, reaching up to 30% after total thyroidectomy (21, 22). More rarely, hypoparathyroidism can occur as a congenital primer, disc der, characterized by genetic heterogeneity (23,24. Per ha nent hypoparathyroidism is one of the mon diricult of all endocrine disorders to treat medical'y. This is part cularly true for subjects who do not respond to n suical to srapy with calhiuin and vitamin D3 (ranactory hy pop ar, +, yroidism) (25). . or ran transplant tion is proption or permanent or and stinct in the med for parath read allotransplantation or uld be justified. E aceuse hy, oparathyroidismua, aly is vi al thi at to the patient, systen is post-transtiant in mun is prossion is not justified. The applicability of biochcap up ion to immunoisolate parathyroid tiss te or cells has provided a range of encouraging results ir in vitro ar.1 in ivo experimental models (14-19).

V hile a large number of synthetic, semi-synthetic and natural water soluble polymers have been evaluated as potential materials for cell and tissue encapsulation (26, 27), the most promising approach are hydrogel- and particularly alginatebased microcapsules, as these materials meet best the requirements for long-term immunoisolation and simultaneous maintenance of transplant function (28). However, a consistent and standardized quality of the material which is a pre-requisite for biomedical applications has not been provided so far. Other challenges involve the production of uniform capsules through automated machines, the suitability of cell or tissue types for immobilization, and the transplantation site. For all these reasons allotransplantation of parathyroid tissue is still in its experimental stage, with the exception of isolated attempts in humans (15, 29). Moreover, the variability of the materials used in different investigations accounts for the poor comparability of results

In a stepwise analysis of the essential obstacles, we have developed a clinical grade biomaterial. Indeed, the purified biopolymer used in this investigation was produced under GMP conditions, encompassing several quality control measures, such as cytotoxicity testing. This material made possible the *in vitro* maintenance of both morphological and functional features of human parathyroid tissue, as shown through histologi-

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cal examination and measurement of PTH release. In add, i.m, the lack of need for fetal calf serum in the culture measures is another interesting characteristic of our million napsulation model. Lecause potential sources is dise ase transmission, such as additives of animal is hun ar ong in could be avoided. The results of this study, toge the virin those of previous *in vivo* studies using united uncertain of encapsulation technology in the results of parathyroid patients refractory to medic. I the apy. The use of parathyroid cell suspension may proide an additional opportunity to further improve this therapy option.

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