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Ultra-high-resolution dual-source CT for forensic dental visualization—discrimination of ceramic and composite fillings

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Abstract Dental identification is the most valuable method to identify human remains in single cases with major postmortem alterations as well as in mass casualties because of its practicability and demanding reliability. Computed tomography (CT) has been investigated as a supportive tool for forensic identification and has proven to be valuable. It can also scan the dentition of a deceased within minutes. In the present study, we investigated currently used restorative materials using ultra-high-resolution dual-source CT and the extended CT scale for the purpose of a color-encoded, in scale, and artifact-free visualization in 3D volume rendering. In 122 human molars, 220 cavities with 2-, 3-, 4- and 5-mm diameter were prepared. With presently used filling materials (different composites, temporary filling materials, ceramic, and liner), these cavities were restored in six teeth for each material and cavity size (exception amalgam n=1). The teeth were CT scanned and images reconstructed using an

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3001 Bern, Switzerland extended CT scale. Filling materials were analyzed in terms of resulting Hounsfield units (HU) and filling size representation within the images. Varying restorative materials showed distinctively differing radiopacities allowing for CT-data-based discrimination. Particularly, ceramic and composite fillings could be differentiated. The HU values were used to generate an updated volume-rendering preset for postmortem extended CT scale data of the dentition to easily visualize the position of restorations, the shape (in scale), and the material used which is color encoded in 3D. The results provide the scientific background for the application of 3D volume rendering to visualize the human dentition for forensic identification purposes.

Keywords Forensic radiology · Dental identification · Dental filling materials · Extended CT scale · Dual source CT

Introduction

In cases of single unknown bodies or multiple unknown bodies in mass fatality incidents, to accurately and rapidly identify the victims is important not only for juridical reasons. Dental identification plays a major role in the identification of corpses with postmortem alterations such as advanced stages of putrefaction or burning. On the other hand, dental identification is often used in mass casualties either from natural disasters or due to armed conflicts as it has a high reliability [1, 2].

Having already been introduced as a postmortem investigation tool, computed tomography (CT) is currently evaluated for varying purposes [3–10]. CT can also contribute to the purpose of identification manifold [11–16]. Focusing the research on the dental CT imaging for identification purposes, a few studies have already demonstrated the

feasibility of CT data [17–19]. The main problem mentioned within the published work was to overcome the well-known streak artifacts caused by the dental restorative material itself that should actually be visualized as it contains necessary individualizing characteristics.

This problem could be solved by using the extended CT scale technique for image reconstruction as it extends the radiopacity values ten times, which can be represented within the CT images by gray values [19]. Thereby, most of the filling materials lose the streak artifact as the radiopacity does not exceed the upper scale limit anymore. The first experiments investigating the CT-data-based visualization of dental restorations using the extended CT scale technique were carried out on restored teeth, which had been extracted for different reasons [19]. This first study [19] was a feasibility study lacking precise information on the filling material used in terms of composition, age of the restoration, and supplier, as well as unknown real filling dimensions. Of course, the number of investigated restorations was also too low to statistically substantiate the results [19].

Therefore, the aim of the present study was to increase the knowledge about the predominant radiopacity behavior of recently used filling materials with special focus on composite fillings. These are the materials the forensic examiners will increasingly have to deal with in the future as the formerly widespread use of amalgam will slowly disappear during the next decades. These materials will be more and more improved in terms of tooth coloration which further complicates the visual identification during an external examination of a corpse. As in the initial study, it was intended to subsequently implement the newly gained knowledge in a 3D volume-rendering (VR) algorithm for postmortem extended CT scale data that can easily visualize the dentition not only in terms of filling location but also in terms of filling material used as well as filling size and shape.

Materials and methods

Ten different materials used for restorative purposes (temporary, permanent, liner, and adhesives; displayed in Table 1) were investigated and 122 human molars were prepared with cavities of 2-, 3-, 4-, and 5-mm diameter (Fig. 1). Two cavities of either 2 and 3 or 4 and 5 mm were prepared in each tooth. For the ceramic fillings, only one cavity per tooth could be reasonably prepared as they are applied as prepared solid blocks. Knowing from the initial study that amalgam distinctively exceeds the upper 30,710 Hounsfield Unit (HU) limit of the extended CT scale (on the used Siemens CT), the amalgam fillings were limited to one in each size, respectively. This resulted in 220 restorative fillings of known restorative material and dimension to be investigated.

	porary filling	materials	Permanent fillin ₈	g materials				Liner and adhe	sives	
Name IRM		Ketac Fil	Tetric Flow	Tetric Evo Ceram	Dyract eXtra	Vitablocs Mark II	Oralloy Magicap S	3M Vitrebond	Optibond	Xeno III
Characteristics Poly reii	mer vforcement	Glas-ionomer- cement	Light-curing flowable	Light-curing nanohvbrid	Fluoridated glass filler	Fine-particle feldspar	Non- gamma-2	Light cure glass	Filled, light- cure total-	Self- etching
zin	c oxide- enol		hybrid comnosite	composite	with acid- modifier	ceramic blocks	amalgam	ionomer liner/base	etch adhesive honding	dental
Sumulier DEN	TSPLY	ESPE Dental-	Ivoclar	Ivoclar	monomers DENTSPLY	VITA Zahnfahrik	Coltène /	3M Dental	system Kerr	DENTSPLY
De	Trey	Medizin Gmbh	Vivadent	Vivadent	DeTrey	H. Rauter Gmbh	Whaledent	Products,	Dentistry,	DeTrey
Gr	Jbh,	& Co. KG,	AG, Schaan,	AG, Schaan,	Gmbh,	and Co. KG, Bad	AG,	Laboratories	Orange,	Gmbh,
Dr	siech/	Seefeld,	Liechtenstein	Liechtenstein	Konstanz,	Säckingen,	Altstätten,	3M Santé,	USA	Konstanz,
Ba	ar,	Germany			Germany	Germany	Switzerland	Pithiviers,		Germany
Sw	itzerland							France		



Fig. 1 Investigated teeth. **a** Teeth were embedded in an edentulous impression system (*vellow*) that has a radiopacity comparable to bone. **b** For each investigated material six cavities of 2-, 3-, 4-, and 5-mm diameter were prepared and restored

For CT scanning, the roots of the teeth were embedded in Optosil[®] Comfort (Heraeus Kulzer, Hanau, Germany), an edentulous impression system that perfectly replaces the jaw bone in CT experiments as it shows an X-ray attenuation of 150-200 HU. This as well as immersing the teeth in artificial saliva [20] during scanning simulated enoral conditions with the aim to reduce partial volume effects at borders and to facilitate an application of the study results on whole in situ dentitions. The teeth were scanned on a dual-source CT scanner (Definition, Siemens Medical, Erlangen, Germany) using ultra-high-resolution settings (z-Sharp[™] technology). Raw data acquisition 120 kv, 182 mAs, 12×0.3-mm collimation, rotation time 1 s, pitch 0.9, and a 50 mm field of view image reconstruction in a 512 matrix resulted in a voxel size of $0.1 \times$ 0.1×0.24 mm (U70 reconstruction kernel and extended CT scale).

The maximum and minimum HU values of each filling were assessed on a radiological workstation (Leonardo, Siemens Medical, Erlangen, Germany). Furthermore, the maximum and minimum value for the dentine and the maximum value for the enamel were measured in each tooth (except for the amalgam restored teeth).

The mean values and standard deviations (SD) were calculated for every filling material and filling size as well as for every filling material including all filling sizes. The HU ranges obtained were used to redefine the preset settings for a volume-rendering software (Inspace, Syngo, Siemens Medical, Erlangen, Germany). The resulting software application was applied to a CT data set of teeth containing five different filling materials for validation.

Results

The dentine covered a range from 1,717 HU (SD 63.9 HU) to 2,130 HU (SD 72.8 HU) and the enamel reached a mean of 4,350 HU (SD 89.7 HU) as indicated in Fig. 2.

Table 2 displays the obtained mean values and standard deviations of the maximum and minimum HU measurements. Figure 2 gives an overview on the HU ranges that represent each restorative material on the extended CT scale based on our measurements and compares them to the obtained values of the tooth dentine and enamel.

Both temporary filling materials, namely IRM and Ketac Fil, showed comparable X-ray attenuation between ~6,000 and ~7,700 HU and cannot therefore be clearly differentiated from each other by their HU values. However, to separate both as temporary filling from definite restorations becomes possible as they are the only that cover this HU range.

The permanent fillings showed different radiopacities. Tetric Flow and Tetric Evo Ceram presented with the highest nonmetallic values, both covered a range of \sim 11,200 to \sim 14,000 HU. In contrast, Dyract eXtra demonstrated a range from \sim 5,000 to \sim 5,900 HU and was thereby only slightly more opaque than tooth enamel.

The ceramic fillings (Vitablocs Mark II) were difficult to assess for two reasons. They have to be embedded in a thin layer of special ceramic adhesive (Variolink 2, Ivoclar Vivadent, Schaan, Lichtenstein), which radiologically behaved like the highly opaque composites (see Table 2 and Fig. 3) and the radiopacity range of ceramic itself was within the HU range of the dentine or even lower.

Amalgam could not be represented within the 2D images by its real HU value as it exceeded the upper limit of 30,710 HU. Therefore, it was always measured as the upper scale limit value and is given as 30,710 HU within the tables.

The investigated adhesives and liner showed radiopacities comparable to enamel, slightly above enamel or comparable to bone. Knowing that none of these has a high radiopaque X-ray behavior and all of them are expected to occur only in very thin layers around definite restorations, they can be disregarded within the volume-rendering preset.

Discussion

The present study aimed at a reevaluation of the results from a feasibility study published in 2006 [19]. The cited study showed promising results but was lacking in various aspects, such as insufficient information about the used Fig. 2 Graphical HU range delineation based on the values obtained in the investigated restorative materials. a With amalgam. Note that the lower and upper limit of amalgam's radiopacity cannot reliably be assessed. Within the images, it is given with the upper limit of the actual extended CT scale. But it is likely that it distinctively exceeds this value. b Without amalgam. Note that only Vitablocks (ceramic), liner, and an adhesive have radiopacities that are at the level of teeth or lower



filling materials and exact filling size. Furthermore, the number of investigated teeth was also low; therefore, a prospective study that would provide the background for a further implementation of the extended CT scale for the purpose of dental visualization became necessary.

When planning the study, restorative materials were chosen that are the most widely used at least in central Europe (in the authors' experiences). Of course, it was impossible to include every material that has been used or is used around the world. As it was expected that most of

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the material groups differed only slightly with different suppliers, the study concentrated on imaging the material groups. Materials that are used during the restorative process to prepare the cavity for the filling and act as a glue for a filling were also included because they could remain visible as thin layers around the filling when having distinctively differing HU values. Fortunately, the measurements showed that both of the adhesives and also the Vitrebond as a liner have radiopacities which do not differ greatly from normal teeth. Therefore, and as they are only

Table 2 Investigated materials and maximal and minimal HU values that were obtained instead of the mean as they are needed to reasonably set the borders of the HU trapezoids within the VR presets for discrimination

	Temporary fi	ling materials		Liner and adhesives						
Name	IRM	Ketac Fil	Tetric Flow	Tetric Evo Ceram	Dyract eXtra	Vitablocs Mark II	Oralloy Magicap S	3M Vitrebond	Optibond	Xeno III
Mean of max HU values	7693.3	7654.2	14015.4	13899.6	5883.8	2428.8	30710.0	3516.3	5465.4	606.7
Standard deviation of max HU values	307.2	267.3	430.5	437.4	209.9	134.5	0.0	355.9	213.7	48.5
Mean of min HU Values	6177.9	6055.0	11224.6	11538.8	4997.5	1544.2	30710.0	2976.7	4840.0	277.1
Standard deviation of min HU values	310.7	174.7	396.7	372.4	271.6	143.9	0.0	449.8	181.0	55.6
Reformatted 2D example images	W		7	27	Ø			7	7	1

Note at the example images below that the radiopacity of the ceramic (Vitablocs Mark II) filling itself is comparable to the dentine. However, there is a thin margin of very dense material around the ceramic, which indicates a radiopaque adhesive as bonding substance

occurring as thin layers around the filling, the results justify that they can be ignored within the VR preset.

To compare a view on a volume-rendered 3D model to a conventional radiograph of the dentition for the purpose of identification, it is important that not only the location of the restoration but also the filling shape is correctly displayed within the VR image. To address this requirement, it was indispensable to investigate fillings with at least one known filling diameter. Therefore, the teeth were prepared with cavities of known width in four different sizes. This was intended to rule out or recognize and further investigate size-dependent visualization errors. Fortunately, there was no obvious size-dependent change in radiopacity. Tests of the preset showed also that all four filling sizes were displayed correctly within the 3D images (see Fig. 3).

There are two permanent filling materials that do challenge imaging by CT. First of all and already known from the feasibility study, the amalgam needs to be discussed. Being a composition of different metals such as



Fig. 3 Preset tested on a data set including five different study teeth in lateral and cranio-caudal view (temporary filling 4+5 mm [IRM]— *green*, high radiopaque definite filling 4+5 mm [Tetric Flow Cavifil]— *red*, low radiopaque definite filling 4+5 mm [Dyract eXtra]—*yellow*, Ceramic 5 mm—*black* with *yellow* and *red* surrounding *circle* and amalgam 4+5 mm—*blue*). For an initial overview, all trapezoids have to be "on," which results in *thin red* (blooming caused) and *yellow*

(streak caused) margins on the amalgam filling. However, when the low radiopaque fillings have been assessed their trapezoids can be set "off" and the amalgam fillings regain their optimal solely blue visualization. *a* All trapezoids "on" with enamel at 30 % opacity. *b* All trapezoids "on" with enamel at 5 % opacity. *c* Only the teeth trapezoids and the amalgam ramp "on"

silver, copper, stannous, and predominantly mercury, its strong radiopacity is explained by the high mass number of mercury, which is close to lead that is used for radiation protection because of its strong X-ray attenuation. So it is a very hostile composition for CT visualization. However, there is no need to look "into" the filling for its characterization. For dental identification, it is the real visualization of its shape that matters. This could be distinctively improved with the adaptation of its HU ramp settings within the VR preset (Fig. 3). This might also improve the visualization of more metallic restorations such as implants or bridges, although not investigated within the present study. However, in 2D images amalgam remains a problem but it is expected to be mostly replaced within the forthcoming decades by more radiolucent materials.

The second problematic restorative material was ceramic which behaved radiologically like dentine. Thereby, it would be almost impossible to even recognize it within the teeth. But there are two findings that can strongly indicate a ceramic filling. The ceramic blocks are always embedded in a thin layer of a special adhesive which results in a highly radiopaque layer between ceramic and dentine. Therefore, a huge area of the enamel behaving like dentine in the CT images combined with a thin radiopaque layer surrounding it is a strong hint for a ceramic filling (Table 2 and Fig. 3).

As the data interpretation will always be based on the available antemortem data parts of the study results might be of limited value for identification purposes. Although the study shows that even different manufacturers could theoretically be differentiated, its value for dental identification is the differentiation of different filling materials in general as most antemortem documents of treating dentists only include information on the filling material used but not about the manufacturer. The greatest progress is the easy discrimination between ceramic and different composite fillings that can contribute to the task of dental identification. As demonstrated in Fig. 3, the power of CT scanning of dentitions is the documentation of the teeth and the fillings. Every filling is visualized at its location (occlusal, distal, palatinal, buccal, lingual, or mesial) and also in its shape to be compared to antemortem radiographs if available. And this documentation is fast. Combined with a whole-body scan, the scanning time does not exceed 3-4 min. The dentition alone can be scanned within 1 min. However, interpretation of the dental CT data will not be sped up but facilitated. Every wished view on the dentition is possible and the fillings will lighten up at their locations with different colors that indicate the materials used. In case of mass fatalities, the data can be distributed to odontologists around the world and consulted again. However, as identification itself does not need to be fast but has to be the most reliable, interpretation must remain efficient and thorough whether on the corpse itself or on its CT data.

Updated VR preset

The obtained radiopacity values were implemented in a VR preset as described in Table 3. Besides the actual data of the measurements, the following main considerations have been applied within the preset.

The opacity of the materials should increase with their radiopacity resulting in less opaque visualization of low radiopaque material within the VR model. This reduces blooming and discoloration caused by streaks around highly radiopaque filling materials.

The colors that are used will go from brighter colors such as yellow or light green for low radiopaque materials via red to blue as darker colors for more radiopaque materials. Thereby, the optical difference to the white teeth is greatest for dense materials and the highly radiopaque fillings are surrounded by margin due to blooming that is closer to the bright teeth than if handled the opposite way.

To reduce the influence of partial volume effects at the border between filling and tooth and between filling and

	HU	HU	Lower	Upper			
	ramp	trapezoid	HU limit	HU limit	Opacity	Color	Shape
Bone + dentine		x	800	2300	10%	White	\frown
Enamel		x	2200	4500	5% ^a	White	\sim
Low radiopaque definite fillings		x	4800	6000	15%	Yellow	П
Temporary fillings		x	6000	8000	20%	Green	
High radiopaque definite fillings		x	11000	14100	40%	Red	
Amalgam	x		~20000	တ	100%	Blue	r

Table 3 Preset suggestion based on the results of the measurements

Also different shading and surface enhancement applications may be used to enhance the image quality to the demand of the actual user ^a One may set the enamel to 30% opacity for a first overview as the dental anatomy is better displayed thereby

oral cavity, the lower limit of the representing HU trapezoid was chosen slightly lower than the measured minimal value if possible. However, due to the high spatial resolution (voxel size of $0.1 \times 0.1 \times 0.24$ mm) and the U70 kernel used, the expected partial volume errors could be reduced distinctively in advance at the time of CT image generation.

The opacity of the dentine was kept very low and was only allowed to outline the shape of the teeth to optimize the visibility of the restorative materials.

Fillings with increased radiopacity such as amalgam will still be displayed with a thin layer of the color of lower radiopacity materials when all trapezoids encoding the different materials are set "on." As already discussed in detail within the initial study, this is caused by partial volume effects at the border of the filling and the distinctively reduced but still partly remaining streak artifacts within the 2D images. If a detailed shape of a high-density filling is aimed for, it can be achieved by turning off the lower HU trapezoids (Fig. 3).

Conclusions

In conclusion, the presented study provides the scientific background to implement the suggested VR preset in routine postmortem investigation by CT. Thereby, the advantages of an easy, fast and observer independent postmortem documentation of the dentition can be used for the purpose of forensic identification as it allows for a very quick overview on the dental status. Especially ceramic and composite fillings can be differentiated. This can facilitate daily forensic routine work and especially support disaster victim identification teams in their work when CT-based whole-body documentation is applied to the victims after a mass fatality.

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