Effect of new light curing units on microleakage and microhardness of resin sealants

Mehmet BANI1 and Resmiye Ebru TIRALI2

¹ Department of Pediatric Dentistry, Faculty of Dentistry, Gazi University, Emek, Ankara, Turkey

To determine new developed light curing units with shorter curing times effects on microleakage and microhardness values for resin fissure sealants. Resin filled sealant (UltraSeal-XT), resin unfilled sealant (Delton Type-II) and ormocer-based sealant (Admira-Seal) were light cured with a quartz-tungsten-halogen (QTH), two LED light and a high power LED. Two hundred and forty extracted human molars were randomly allocated into four groups according to used light-curing unit and three subgroups were formed for three different fissure sealant materials. Specimens were immersed in 0.5% basic fuchsin for 24 h, sectioned and examined under a stereomicroscope, and scored for marginal microleakage. Knoop hardness number (KHN) readings were measured after 48 h. Statistical analyses of test were found in significant difference both microleakage and microhardness values between the various light curing units. The time saving approaches in the curing light were determined higher microhardness, although it was found in higher microleakage.

Keywords: Microleakage, Microhardness, Fissure sealant, Light curing unit

INTRODUCTION

Preventive measures, use of fluoride agents and improvement of oral hygiene, have verified effective in reducing caries prevalence. However, posterior teeth have not uniform tooth surfaces as pit and fissure surfaces. The morphology of the occlusal surface in posterior teeth obstructs the mechanical cleaning and reduces the effects of preventive measures. Studies have demonstrated that the use of pit and fissure sealants is an effective way for preventing caries¹⁻⁶.

Light-cured resin sealants used the most common and conventionally. The polymerization of light-cured sealants can be achieved with many light sources (e.g. quartz tungsten halogen, plasma arc and light emitting diode (LED)). Current sealants are most commonly cured with a quartz tungsten halogen curing lights (QTHs), which has a peak absorption at a maximum of 465 nm. QTHs have some limitations, such as relatively short working life span, high operating temperatures and decreased light output over time^{3,7,8)}. LEDs can be operated for thousands of hours without a significant reduction in light output. The reduced temperature associated with LEDs also can prevent degradation of light guides and does not pose a threat to the pulpal tissue. Several studies, however, have shown that LEDs with relatively low irradiances may result in insufficiently cured composites and, therefore, adversely effects mechanical properties of the restorations. The light output of the first-generation LEDs required improvement to match with the cure produced by QTHs.

A number of second-generation LEDs with high power light sources are now available. The results of studies have shown that these are capable of curing CPQ-initiated composites in half the radiation time of their predecessor. The curing kinetics of photo polymerized dental sealants using LEDs showed that the second-generation LEDs reached conversion similar to control in only 10 s^{2,3,8)}. The third-generation of LED curing units contains multiple diodes (violet/blue diodes, polywave), and recently a third-generation LED curing unit was marketed (Valo, Ultradent, South Jordan, UT, USA), which is claimed to reach irradiances of up to 3,200 mW/cm² depending on the chosen mode.

These time saving approaches could have significant clinical implications, provided that there is no adverse effect on the fissure sealant's marginal integrity. The purpose of this *in vitro* study was to evaluate the effect of different generation light emitting diodes and quartz tungsten halogen curing units used for various sealants curing on the microleakage and microhardness values.

MATERIALS AND METHODS

Microleakage section

Sample size calculations were performed using PASS software (NCSS, LLC, Kaysville, UT, USA). It is estimated at about 180 teeth with a 90% confidence interval level and a standard error of 5%. Caries-free, extracted for orthodontic reasons human mandibular third molars were collected from healthy children ages 15–20. Participants signed the informed consent form. Each tooth was stored in 0.12% thymol solution immediately after extraction and for the same amount of time. Organic remnants were removed off of teeth,

² Department of Pediatric Dentistry, Faculty of Dentistry, Başkent University, Bahçelievler, Ankara, Turkey Corresponding author, Mehmet BANI; E-mail: mehmetbani@hotmail.com

Color figures can be viewed in the online issue, which is available at J-STAGE.

and the occlusal surfaces were cleaned with a slow speed bristle brush with a continuous irrigation of water coolant. The teeth were then examined under a dissecting microscope to discard those with caries, any visible hypoplasia, extraction damage, or microcracks. Teeth with irregular occlusal morphology were also excluded. The condition laboratory was under the daylight 63% relative humidity at room temperature. In the study, three various fissure sealant materials and four curing units were used (Tables 1 and 2).

Accordingly, 240 teeth were selected and assigned randomly into 1 of 4 experimental groups:

In group 1 (Hilux), pits and fissures were etched with 37% phosphoric acid (Vococid, Voco, Cuxhaven, Germany) for 30 s, rinsed with air-water spray for 15 s, and air-dried for 10 s. A bonding resin (Clearfil SE Bond, Kuraray, Okayama, Japan) was applied on the fissures

according to the manufacturer's instructions and light with a conventional QTH curing unit (Hilux, Benlioğlu Dental, Ankara, Turkey). A radiometer was utilized for detecting the curing unit's performance. Thereafter, three subgroup was formed by 20 teeth according to applied different fissure sealants mentioned in Table 2. Light curing was performed for 30 s with the same QTH curing unit, and kept distance standard 2 mm.

In group 2 (Elipar) acid-etch and bonding procedures were performed as in group 1, with the adhesive resin being light cured for 10 s with another LED curing unit (Elipar Free Light 2, 3M ESPE, St. Paul, MN, USA). Three subgroups were formed as with group 1 and light cured with the Elipar curing unit for 10 s, and kept distance standard 2 mm.

In group 3 (Valo SP), acid-etch and bonding procedures were performed as in groups 1 and 2, with

Table 1 Light curing used in the study

Light curing	Curing unit	Curing time	Manufacturer	Intensity (mW/cm²)	Peak Wavelength (nm)
Hilux	QTH	20 s	Benlioğlu Dental, Ankara, Turkey	600	410–500
Elipar Free Light 2	LED	10 s	3M ESPE, St Paul, MN, USA	1,000	430–480
Valo Standart Power mode (SP)	LED	10 s	Ultradent, South Jordan, UT, USA	1,000	440–480
Valo Xtra Power mode (XP)	Plasma LED	3 s	Ultradent	3,200	440–480

Table 2 Fissure sealant used in the study

Fissure Sealant	Structure	Manufacturer	Composition	Function	
UltraSeal XT	aSeal Resin Ultradent, South Jorda Filled UT, USA		Diurethane dimethacrylate Bisphenol A dimethacrylate Sodium monofluorophosphate Titanium dioxide Resin fillers (57%) Light activators	Monomer Monomer Fluoride Opaquer Fillers Photoinitator	
Delton Type II	Resin Unfilled	Dentsply, York, PA, USA	Triethylene glycol dimetharcylate Bisphenol A dimethacrylate Barium alumino fluroboro silicate glass (55%) Titanium dioxide (opaque) Sodium Fluoride Ethyl p-dimethylaminobenzoate	Monomer Monomer Fillers Opaquer Fluoride Photoinitator	
Admira Seal	Ormocer- based	Voco, Cuxhaven, Germany	Hydroxyethyl dimethacrylate Bisphenol A dimethacrylate Ormocers Silicate and glass ceramic Inorganic/organic co-polymers Light activators	Monomer Monomer Fillers Fillers Co-polymers Photoinitator	

the adhesive resin being light cured for 10 s with another LED curing unit (Valo Standart Power, Ultradent). Three subgroups were formed as with groups 1 and 2 and light cured with the Valo SP curing unit for 10 s, and kept distance standard 2 mm.

In group 4 (Valo XP), acid-etch and bonding procedures were performed as in groups 1, 2 and 3, with the adhesive resin being light cured for 3 s with another LED curing unit (Valo Xtra Power, Ultradent). Three different fissure sealants were applied as with groups 1, 2 and 3 and light cured with the Valo XP curing unit for 3 s, and kept distance standard 2 mm.

Specimens were stored in deionized water at 37°C for 24 h, after which thermal cycling in deionized water was performed at 5±2 to 55±2°C for 500 cycles with a dwell time of 30 s and a transfer time of 10 s. Thereafter, the teeth were kept in distilled water at 37°C for 4 weeks before dye-penetration procedures. The water (pH:7) was changed every week.

Prior to dye penetration, the apices were sealed with sticky wax and the samples were coated with 2 consecutive layers of nail varnish up to 1 mm from the sealant margins. Samples were then immersed in 0.5% basic fuchsine solution (Wako Pure Chemical Industry, Osaka, Japan) for 24 h. After thoroughly rinsing with distilled water, the samples were air-dried and embedded in epoxy resin (Struers, Copenhagen, Denmark). Five parallel longitudinal sections were made through the occlusal surfaces using a low-speed diamond saw (Isomet, Buehler, Lake Bluff, IL, USA) in the buccolingual direction. One calibrated researcher examined all sections under a stereomicroscope at ×16 magnification (Wild Type 308700, Heerbrugg, Switzerland). He was blind to the groups.

For each section, the following criteria was used to rate dye penetration scores: score 0=no dye penetration;

1=dye penetration restricted to the outer half of the sealant; 2=dye penetration into the inner half of the sealant; and 3=dye penetration into the underlying fissure. The microleakage score of each tooth was obtained by calculating the mean score of 5 slices each. Statistical evaluation of microleakage scores between the test groups was performed using the Kruskal-Wallis test with significance set at p=0.05.

Microhardness section

Three various sealant materials and above-described of the four curing units were investigated by using for each of LCU and material (Tables 1 and 2). All specimen were prepared by a single operator, with care taken to avoid bubble formation.

The sealant material was placed into a 2-mmthick silicone mold with a 4-mm internal diameter. The mold was placed between 2 glass slides. Sample size calculations were performed using PASS software (NCSS, LLC). It is estimated at about 180 specimens with a 90% confidence interval level and a standard error of 5%. One hundred eighty specimens were prepared and assigned randomly into 1 of 4 experimental groups. Each specimen was cured for the appropriate amount of time from the top surface only. The specimens were stored in the dark under 100% relative humidity at 37°C for 48 h. Five Knoop Hardness Number (KHN) readings were made at least 1 mm from the edge of each top and bottom surface after an indenter dwell time of 15 s and a load of 50 g (Microhardness Tester FM-700, Mitutoyo G3, Mitutoyo, Tokyo, Japan). A Bottom/Top (B/T) KHN ratio was calculated for each specimen. Top and bottom surface hardness and B/T KHN means were determined for each group. Microhardness scores between the test groups were performed using the Kruskal-Wallis test. The level of significance was set at p=0.05.

Table 3 Dye penetration score, percentage of microleakage and standard deviation for the various curing lights and sealant materials

	Dye penetration score $n:20$			Microlekage % (SD)		
	0	1	2	3	0	1–3
Hilux-UltraSeal XT	15	2	1	2	75	25±18.2b
Hilux-Delton Type II	15	2	2	1	75	25 ± 18.7^{b}
Hilux-Admira Seal	15	1	2	2	75	25 ± 18.3^{b}
Elipar LED-UltraSealXT	18	1	0	1	90	10±14.4a
Elipar LED-Delton Type II	18	1	1	0	90	10 ± 12.5^{a}
Elipar LED-Admira Seal	17	1	1	1	85	15±15.5a,
Valo SP-UltraSealXT	19	0	1	0	95	5±11.3a
Valo SP-Delton Type II	19	0	0	1	95	5 ± 9.5^{a}
Valo SP-Admira Seal	18	1	0	1	90	10 ± 14.2^{a}
Valo XP-UltraSealXT	12	3	2	3	60	40±30.2°
Valo XP-Delton Type II	12	2	3	3	60	$40\pm28.6^{\circ}$
Valo XP-Admira Seal	11	2	3	4	55	45 ± 32.1^{c}

a,b,c: Statistically significant differences among groups are expressed (p>0.05).

RESULTS

Microleakage section

Total 240 teeth scores were analyzed in the results, it were included to each light curing units and fissure

sealant subgroups 20 samples. The means and standard deviations of microleakage for the various light curing units and sealant materials are shown in Table 3. Also, Table 3 compares the results of the tooth scores with no microleakage (score 0) with those where microleakage

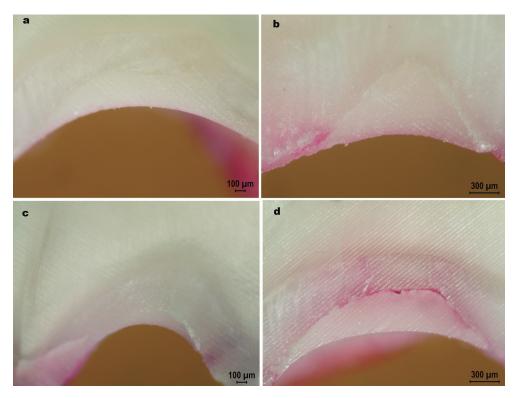


Fig. 1 View of the dye penetration scores 0, 1, 2 and 3.

a; score 0=no dye penetration, b; score 1=dye penetration restricted to the outer half of the sealant, c; score 2=dye penetration into the inner half of the sealant, d; score 3=dye penetration into the underlying fissure.

Table 4 Means and standard deviations of top (T) and bottom (B) hardness and hardness ratio (B/T) for the various curing lights and sealant materials

	Hilux	Elipar LED	Valo SP	Valo XP
UltraSeal XT				
T	23.6 ± 1.12	14.5 ± 0.76	14.1 ± 0.65	9.4 ± 0.45
В	6.5 ± 0.54	1.3 ± 0.43	0.4 ± 0.1	NA*
B/T	0.27 ± 0.07^{a}	$0.08 \pm 0.02^{\mathrm{b,c}}$	$0.02\pm0.01^{\circ}$	NA*
Delton Type II				
T	16.5 ± 0.87	12.8 ± 0.96	9.7 ± 0.78	3.8 ± 0.34
В	4.5 ± 0.39	NA*	NA*	NA*
B/T	0.27 ± 0.03^{a}	NA*	NA*	NA*
Admira Seal				
${f T}$	16.4 ± 0.77	13.1 ± 0.97	10.3±0.83	5.6 ± 0.46
В	4.8 ± 0.31	1.7 ± 0.23	0.3 ± 0.12	NA*
В/Т	0.29 ± 0.06^{a}	0.12 ± 0.03^{b}	0.02±0.01°	NA*

^{*} NA=not applicable.

a,b,c: Statistically significant differences among groups are expressed (p>0.05).

was present (scores 1, 2 and 3) (Fig. 1). The results showed that the various sealing material had not a statistically significant influence on the microleakage (p>0.05). Statistical analyses of these scores with a Kruskal-Wallis test resulted in significant difference between the various light curing units. Microleakage values demonstrated respectively the highest Valo XP, Hilux, Elipar and Valo SP groups. Valo XP exhibited statistically significantly higher microleakage, although Valo SP and Elipar were found in lowest microleakage. Valo SP had demonstrated a significantly lower leakage according to Hilux in all the sealant, however Elipar was excluding Admira Seal (p>0.05).

Microhardness section

Total 180 specimens scores were analyzed in the results, it was included to each light curing units and fissure sealant subgroups 15 samples. The means and standard deviations of microhardnes for the various light curing units and sealant materials are shown in Table 4. There was a significant difference among the groups in terms of the microhardness ratio (p<0.005). Microhardness values showed respectively the highest Valo XP, Valo SP, Elipar and Hilux group.

The results showed that the Delton Type II presented a significantly higher hardness ratio than the other fissure sealants.

DISCUSSION

The pit and fissure sealants' effectiveness for reducing caries risk have been demonstrated by many studies⁹⁾. Despite a lot of advantages for light cured resin sealants, gap formation between tooth and material interfaces due to polymerization shrinkage is considered one of the most important disadvantage¹⁰⁾. Various attempts have been made for reducing operating time for anxious, uncooperative patients by newly developed light curing units^{11,12)}. Although studies stated that decreasing the curing time had no effect on the microleakage of the sealants^{2,13)}, there is a scarcity of published data regarding their effects on the marginal integrity and degree of conversion.

Today, a majority of light curing units is based on the light-emitting diode (LED) technology with a single high-powered diode. Second-generation LED curing units typically reach irradiances of 1,200 to 1,500 mW/ cm². The third-generation of LED curing units contains multiple diodes, and recently a third-generation LED curing unit was marketed (VALO, Ultradent), which is claimed to reach irradiances of up to 3,200 mW/cm² depending on the chosen mode¹⁴⁾. Dental visible light curing materials generally contain a diketone-type photoinitiator that absorbs light in the 400- to 500nm range covered by the blue light from the visible spectrum. The studies showed that the emission peak of blue LED at 465 nm coincided with the absorption peak of camphoroquinone (CQ) at 467 nm^{8,15)}, but when the resin material contains new photointiators that absorb light energy in lower regions of visible spectrum

early generation LED lights failed when compared with QTH^{16} .

Interestingly, rapid cure did not have an adverse effect on Valo XP group's microleakage values. It is possible that, when upper part of the sealant polymerized adequately, it gained retention from the good adaptation. Short curing time might not allow the composite resin flow to form resin tags but this may not be valid for resin sealants. Nevertheless a higher stress level between the layers of resin material due to inadequately curing may increase the flexure under masticatory forces should not be forgotten.

For clinical success of light cured resin sealants adequate polymerization is always necessary. The higher degree of conversion for resin material provides increased mechanical properties. Knoop Hardness Number shows relative degree of conversion for resin materials¹⁷⁾. Unfilled resin sealant (Delton) showed a significant higher hardness ratio as previous studies^{2,18)} can be explained by light's more easier passage from unfilled resin material.

In the present study, the lowest micro hardness values found for Hilux group. This was an unexpected result but light units spectrum is not the only factor that effect polymerization quality of the resin fissure sealants. Different (filler/matrix) compositions of light curing dental materials may have a more pronounced influence on material properties than radiant exposure¹⁹.

Higher amount of filler particles provides less porosity²⁰, better wear resistance²¹, good shear-bond strength²² and similar retention scores as conventional ones²⁰. For the ormocer-based sealant tested, relatively high viscosity that cause greater thickness may explain the not statically significant but higher microleakage values. It is important for the clinician to understand that the polymerization process varies from different types of curing units and different resin materials. Further studies are needed to understand the nature of complex relationship between resin sealant's polymerization and different light curing technology.

CONCLUSION

Sealant microleakage and microhardness effected by the type of light curing device technology. Valo XP exhibited statistically significantly higher microhardness, although it was found in statistically significantly higher microleakage. Valo SP showed lowest microleakage and higher microhardness values. UltraSeal XT and Delton Type II were showed similar microleakage, but Delton Type II presented a significantly higher hardness ratio than the other fissure sealants. This paper adds to the literature results of an in vitro study investigating whether the microleakage and microhardness of a different sealant is influenced either a quartz-tungsten halogen (QTH), two LED light and a high power LED. This study demonstrated that sealant microleakage and microhardness were effected by the type of light curing device technology.

ACKNOWLEDGMENTS

All authors deny any conflicts of interest.

REFERENCES

- Shah S, Roebuck EM, Nugent Z, Deery C. In vitro microleakage of a fissure sealant polymerized by either a quartz tungsten halogen curing light or a plasma arc curing light. Int J Paediatr Dent 2007; 17: 371-377.
- Duangthip D, Ballungpattama S, Sitthisettapong T. Effect of light curing methods on microleakage and microhardness of different resin sealants. J Dent Child (Chic) 2011; 78: 88-95.
- Cehreli SB, Arikan S, Gulsahi K, Arhun N, Arman A, Sargon M. Effect of LED curing on marginal integrity of an ormocerbased sealant. J Dent Child (Chic) 2009; 76: 53-57.
- Bohanan HM, Bader JD. Future impact of public health and preventive methods on the incidence of dental decay. J Can Dent Assoc 1984; 50: 229-233.
- Ripa LW. Sealants revisited: An update of the effectiveness of pit and fissure sealants. Caries Res 1993; 27: 77-82.
- Rethman J. Trends in preventive care: Caries risk assessment and indications for sealants. J Am Dent Assoc 2000; 131: 85-115
- Tarle Z, Meniga A, Knezevic A, Sutalo J, Ristic M, Pichler G. Composite conversion and temperature rise using a conventional, plasma arc, and experimental blue LED curing unit. J Oral Rehabil 2002; 29: 662-667.
- Jandt KD, Mills RW, Blackwell GB, Ashworth SH. Depth of cure and compressive strength of dental composites cured with blue light emitting diodes (LEDs). Dent Mater 2000; 16: 41-47
- Ahovuo-Saloranta A, Hiiri A, Nordblad A, Worthington H, Makela M. Pit and fissure sealants for preventing dental decay in the permanent teeth of children and adolescents. Cochrane Database Syst Rev 2004; 3: CD001830.
- Yap AU, Wang HB, Siow KS, Gan LM. Polymerization shrinkage of visible light cured composites. Oper Dent 2000; 25: 98-103.
- Frost T, Norevall LI, Persson M. Bond strengt hand clinical efficiency for two light guide sizes in orthodontic bracket bonding. Br J Orthod 1997; 24: 35-40.

- 12) James JW, Miller BH, English JD, Tadlock LP, Buschang PH. Effects of high-speed curing devices on shear bond strength and microleakage of orthodontic brackets. Am J Orthod Dentofacial Orthop 2003; 123: 555-561.
- Bodrumlu E, Topuz O, Uzun Ö. Comparison of halogen versus LED light-cured temporary endodontic filling materials for sealing. Minerva Stamatol 2013; 62: 193-198.
- 14) Flury S, Lussi A, Hickel R, Ilie N. Light curing through glass ceramics with a second- and a third-generation LED curing unit: effect of curing mode on the degree of conversion of dual-curing resin cements. Clin Oral Investig 2013; 17: 2127-2137.
- 15) Mills RW, Uhl A, Jandt KD. Optical power outputs, spectra and dental composite depths of cure, obtained with blue light emitting diode (LED) and halogen light curing units (LCUs). Br Dent J 2002; 193: 459-463.
- 16) Ikemura K, Endo T. A review of the development of radical photopolymerization initiators used for designing light-curing dental adhesives and resin composites. Dent Mater J 2010; 29: 481-501.
- Pilo R, Cardash HS. Post-irradiation polymerization of different anterior and posterior visible light activated resin composites. Dent Mater 1992; 8: 299-304.
- 18) Mills RW, Jandt KD, Ashworth SH. Dental composite depth of cure with halogen and blue light emitting diode technology. Br Dent J 1999; 186: 388-391.
- Hadis M, Leprince JG, Shortall AC, Devaux J, Leloup G, Palin WM. High irradiance curing and anomalies of exposure reciprocity law in resin-based materials. J Dent 2011; 39: 549-557
- 20) Oba AA, Sönmez IŞ, Ercan E, Dülgergil T. Comparison of retention rates of fissure sealants using two flowable restorative materials and a conventional resin sealant: twoyear follow-up. Med Princ Pract 2012; 21: 234-237.
- 21) Ciamponi AL. Assessment "in vitro" of the microleakage in enamel/sealant interface: Influence of contamination, using the primer, and different sealants [thesis]. Sao Paulo, Brazil: School of Dentistry, University of Sao Paulo; 1995.
- 22) Eminkahyagil N, Gokalp S, Baseren M, Korkmaz Y, Karabulut E. Sealant and composite bond strength to enamel with antibacterial/self-etching adhesives. Int J Pediatr Dent 2005; 15: 274-281.